Neuroimaging data analysis Classical Statistical Inference in SPM12

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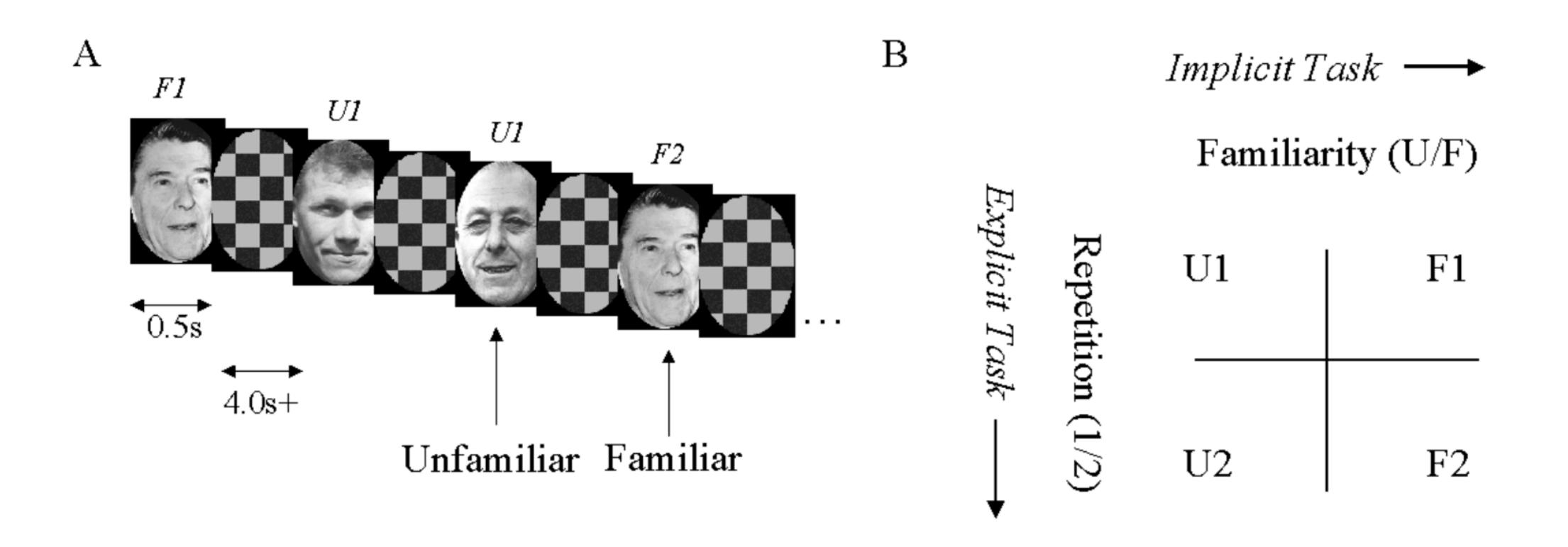
실습 데이터 다운로드

download:

http://www.fil.ion.ucl.ac.uk/spm/download/data/face_rep/face_rep.zip

어떤 데이터 일까?

Face repetition fMRI task



Reference) Henson, R.N.A., Shallice, T., Gorno-Tempini, M.-L. and Dolan, R.J. (2002), Face repetition effects in implicit and explicit memory tests as measured by fMRI. Cerebral Cortex, 12, 178-186.

점화현상

Priming effects

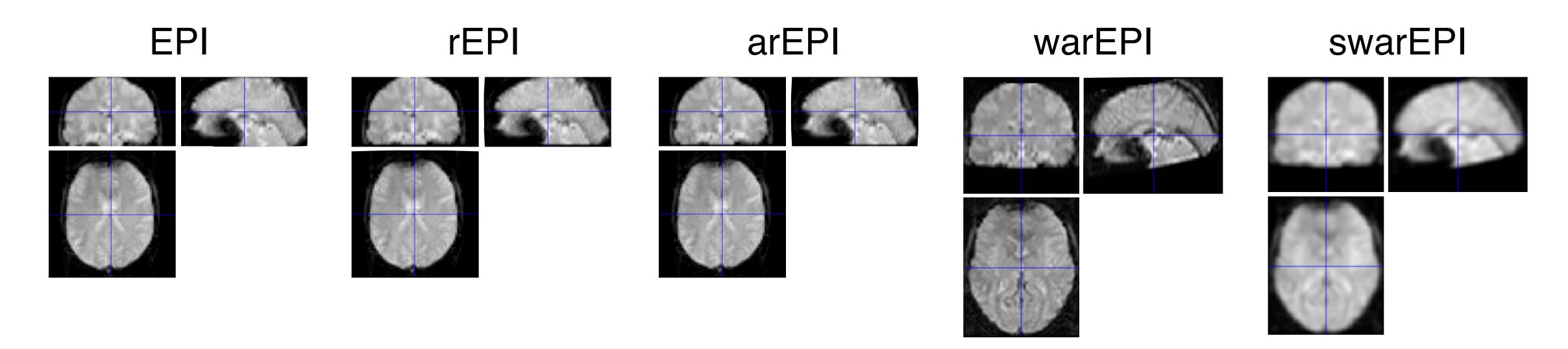
'먼저 본 정보에 의해 떠올려진 개념으로 인해 이후에 접한 정보를 해석할 때 영향'을 받게 되는 현상.

Experiment Information

- 2x2 factorial event-related fMRI
- One session (one subject)
- (Famous vs. Nonfamous) x (1st vs 2nd presentation) of faces against baseline of chequerboard
- 2 presentations of 26 Famous and 26 Nonfamous Greyscale photographs, for 0.5s, randomly intermixed, for fame judgment task (one of two right finger key presses).
- Parameteric factor "lag" = number of faces intervening between repetition of a specific face
- Minimal SOA=4.5s, with probability 2/3 (ie 1/3 null events)
- Continuous EPI (TE=40ms,TR=2s), 24 descending slices (64x64 3x3mm²), 3mm thick, 1.5mm gap

Reference) http://www.fil.ion.ucl.ac.uk/spm/data/face_rep/

Summary of Preprocessing



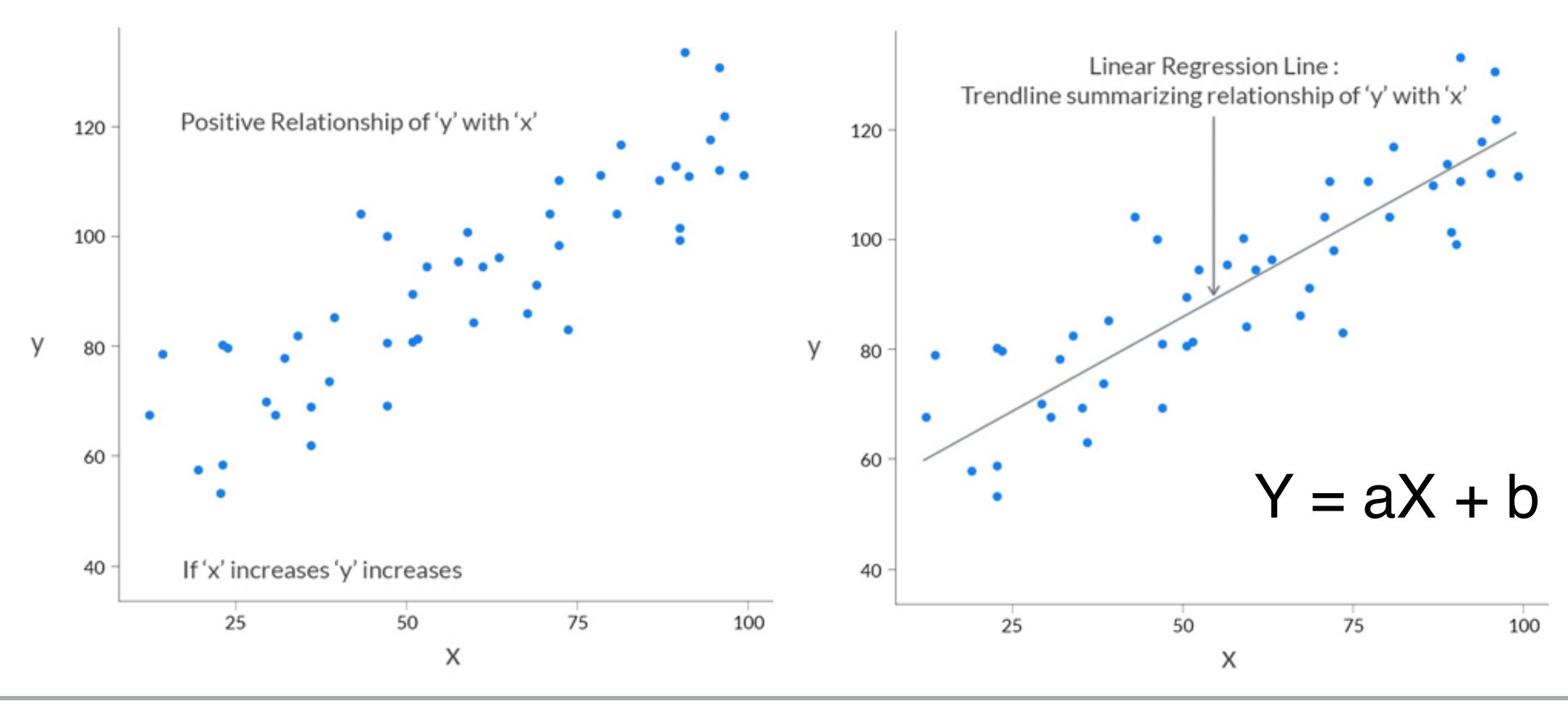
File: ./sM03953_0005_0100.img	File:./rsM03953_0005_0100.img	File:./arsM03953_0005_0100.img	File:arsM03953_0005_0100.img	File:arsM03953_0005_0100.img	
Dimensions: 64 x 64 x 24	Dimensions: 64 x 64 x 24	Dimensions: 64 x 64 x 24	Dimensions: 79 x 95 x 79	Dimensions: 79 x 95 x 79	
Datatype:int16	Datatype:int16	Datatype:int16	Datatype:int16	Datatype:int16	
Intensity: Y = 0.050325 X	Intensity: Y = 0.050325 X	Intensity: Y = 0.050325 X	Intensity: Y = 0.050325 X	Intensity: Y = 0.050325 X	
SPM compatible	spm - realigned	spm - realigned acq-fix ref-slice 14	Warped	Warped - conv(6,6,6)	
Vox size:-3 x 3 x 4.5	Vox size:-3 x 3 x 4.5	Vox size:-3 x 3 x 4.5	Vox size:-2 x 2 x 2	Vox size: -2 x 2 x 2	
Origin: 32.6 32.3 12.5	Origin: 32.5 32.3 12.5	Origin: 32.5 32.3 12.5	Origin: 40 57 36	Origin: 40 57 36	
Dir Cos: 1.000 -0.003 0.005	Dir Cos: 1.000 0.000 0.000	Dir Cos: 1,000 0,000 0,000	Dir Cos: 1,000 0,000 0,000	Dir Cos: 1,000 0,000 0,000	
0.003 1.000 -0.001	0.000 1.000 0.000	0.000 1.000 0.000	0.000 1.000 0.000	0.000 1.000 0.000	
-0.005 0.001 1.000	0.000 0.000 1.000	0.000 0.000 1.000	0.000 0.000 1.000	0.000 0.000 1.000	

In this tutorial,

we need 351 swar*.img files and rp_motion.txt

회귀분석

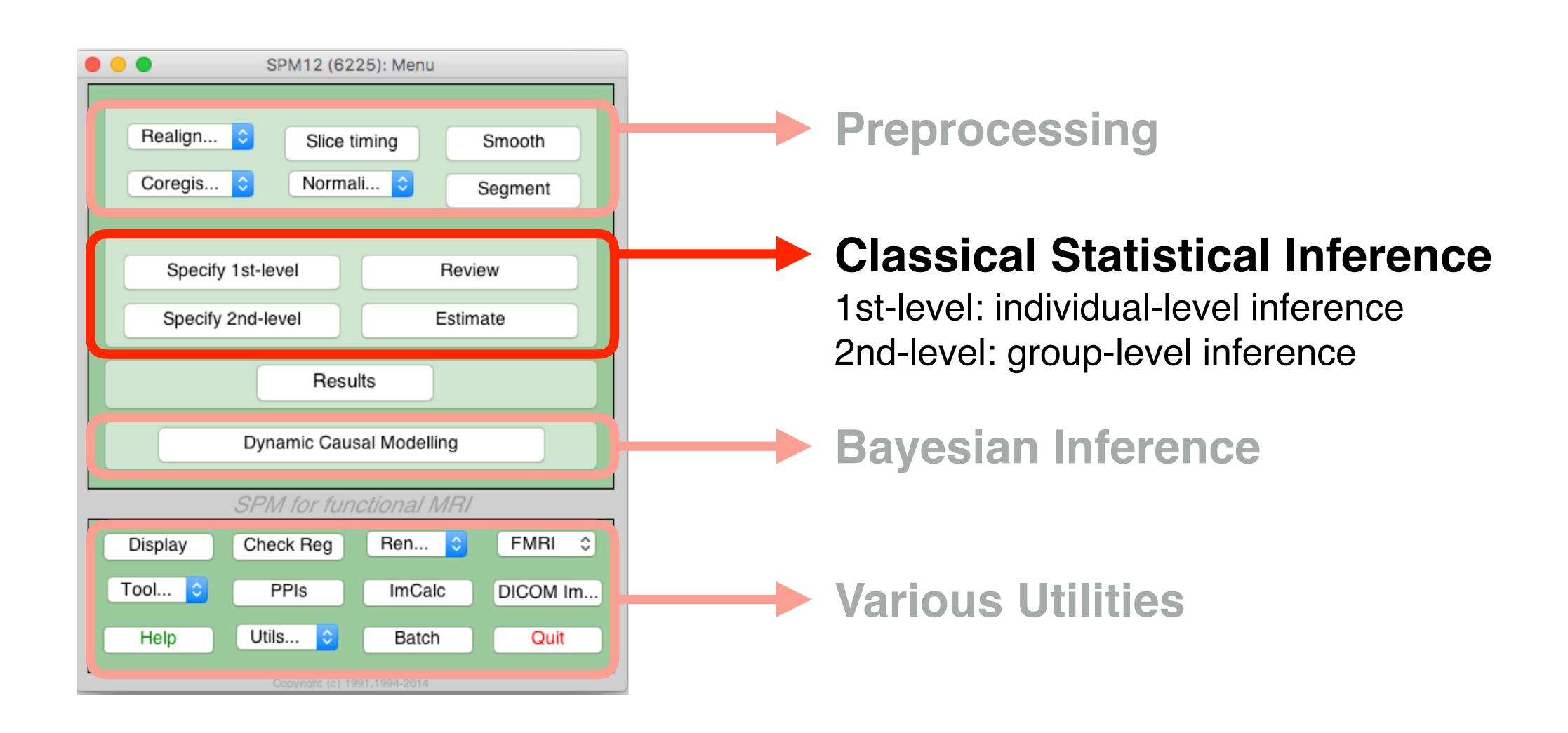
회귀분석은 과학적인 체계로 Quantities 사이의 관계에 대하여 추론을 내리는데 사용되는 통계기술의 집합을 뜻함.



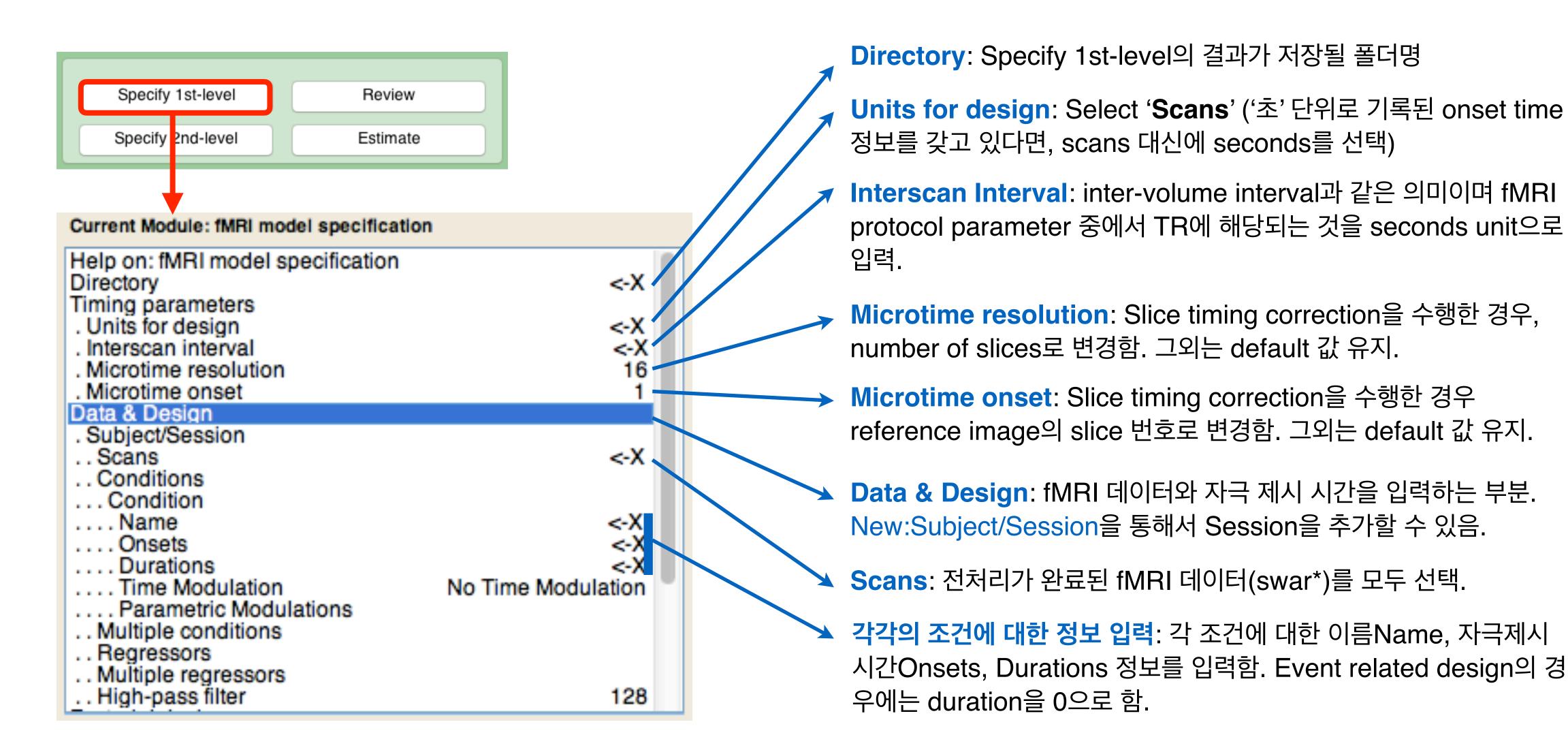


Modelling categorical responses
Reference) Chapter 31.2 in SPM12 manual

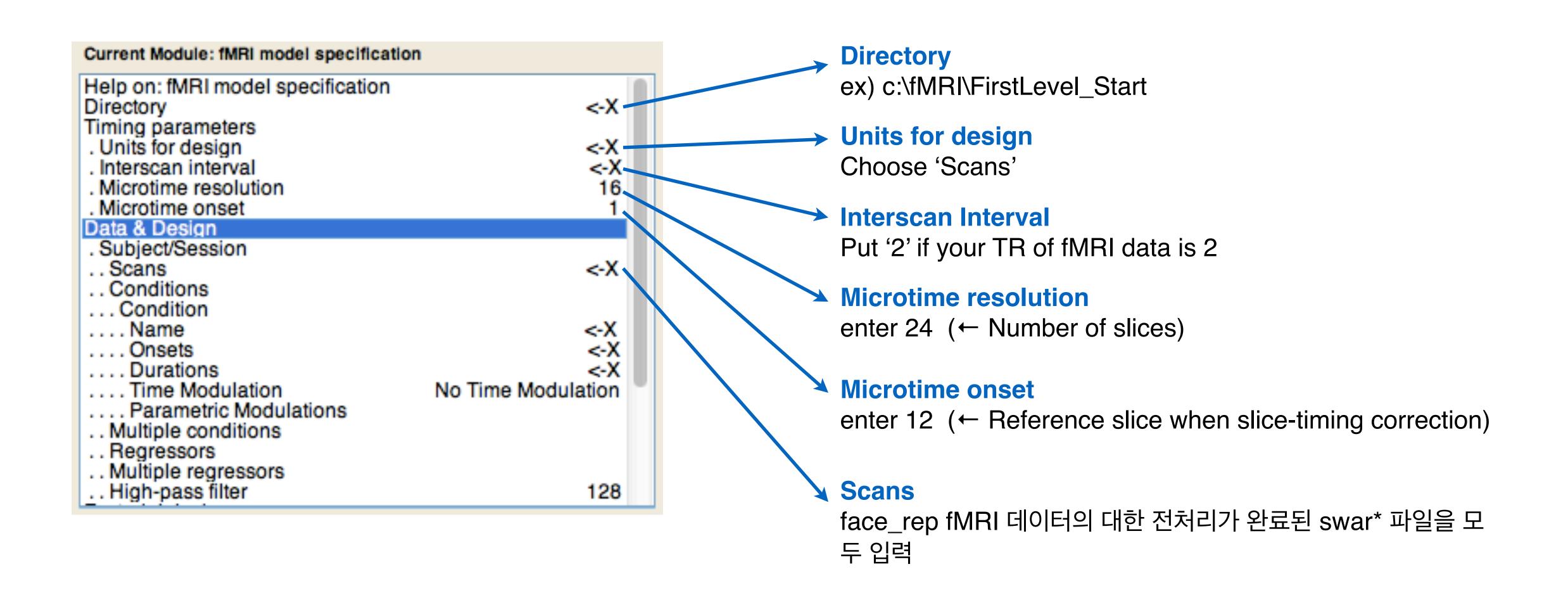
Exploring SPM12 Manu



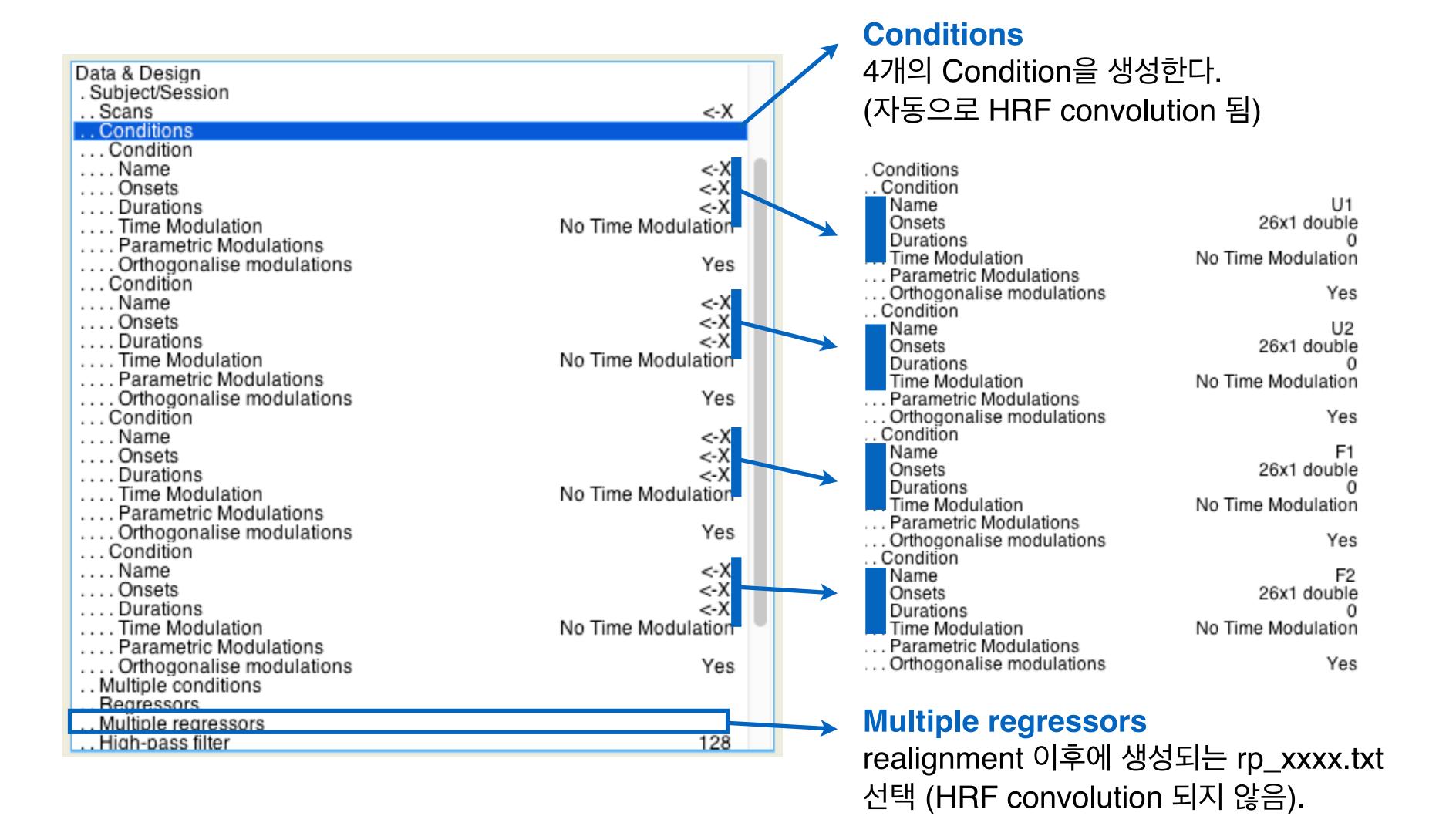
1st-level UI 설명



실습 - Specify 1st-level (1/3)



실습 - Specify 1st-level (2/3)

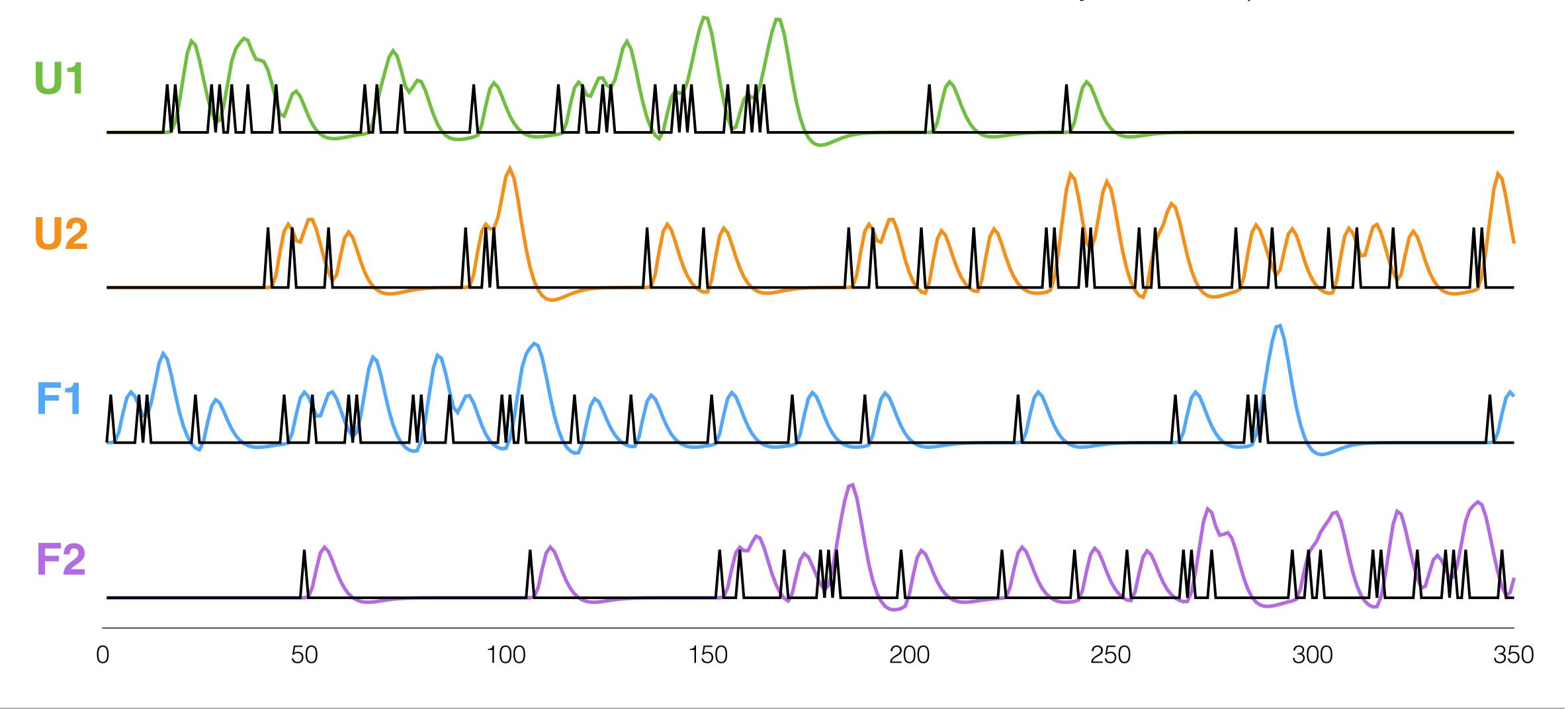


TriallD	U1	U2	F1	F2
1	6.75	13.5	0	33.75
2	15.75	40.5	2.25	49.5
3	18	47.25	9	105.75
4	27	56.25	11.25	153
5	29.25	90	22.5	157.5
6	31.5	94.5	45	168.75
7	36	96.75	51.75	177.75
8	42.75	135	60.75	180
9	65.25	148.5	63	182.25
10	67.5	184.5	76.5	198
11	74.25	191.25	78.75	222.75
12	92.25	202.5	85.5	240.75
13	112.5	216	99	254.25
14	119.25	234	101.25	267.75
15	123.75	236.25	103.5	270
16	126	243	117	274.5
17	137.25	245.25	130.5	294.75
18	141.75	256.5	150.75	299.25
19	144	261	171	301.5
20	146.25	281.25	189	315
21	155.25	290.25	227.25	317.25
22	159.75	303.75	265.5	326.25
23	162	310.5	283.5	333
24	164.25	319.5	285.75	335.25
25	204.75	339.75	288	337.5
26	238.5	342	344.25	346.5

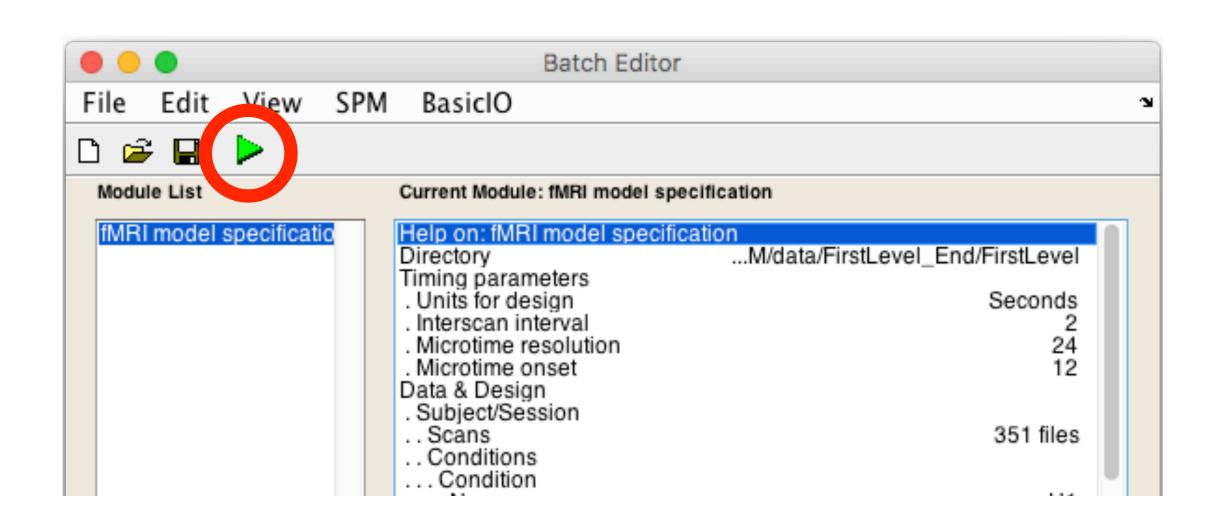
<Onset 정보가 있는 엑셀 파일>

Stimulus Convolved with HRF

Hemodynamic response function



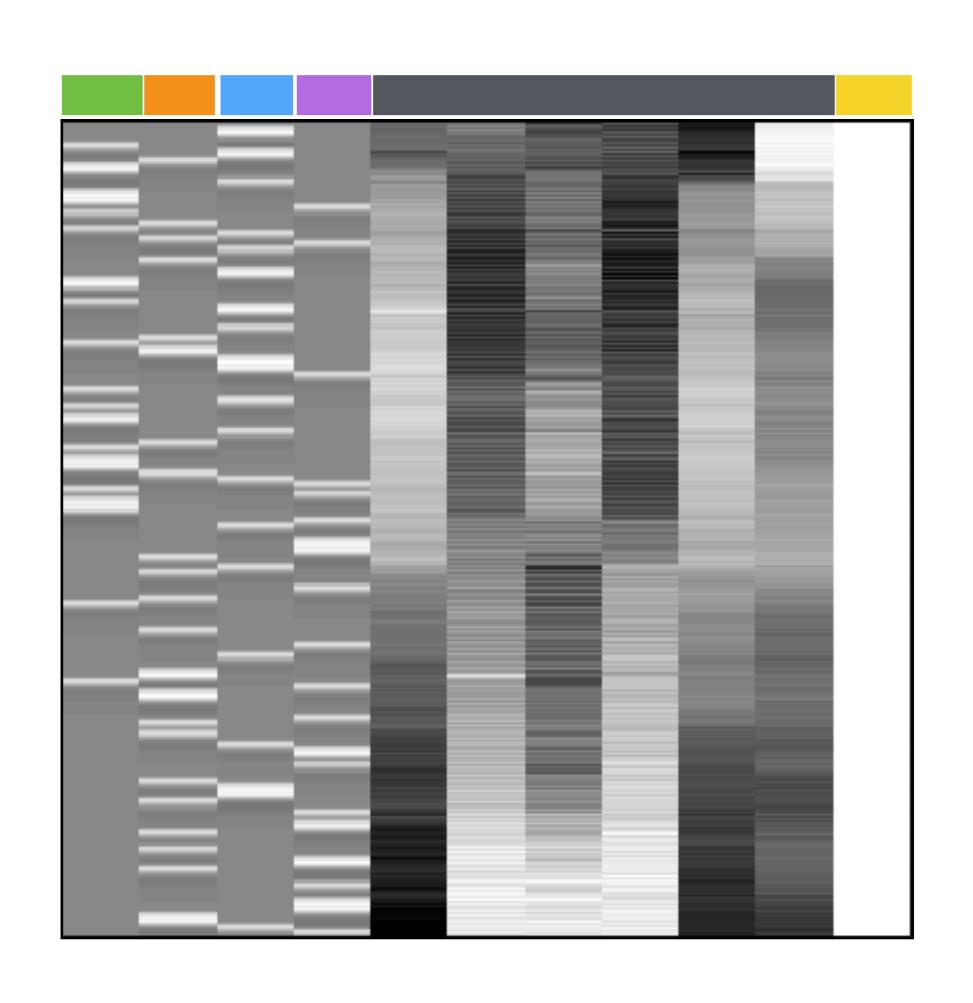
실습 - Specify 1st-level (3/3)



- 1st-level 분석에 필요한 모든 정보가 입력 되었으면 "▶Run Batch" 버튼이 활성화됨.
- 버튼을 클릭하여 개별 fMRI 데이터의 General Linear Model을 만든다.
- Specify 1st-level은 뇌영상 데이터를 다음의 모델로 분석하 겠다고, 정의 하는 과정임.

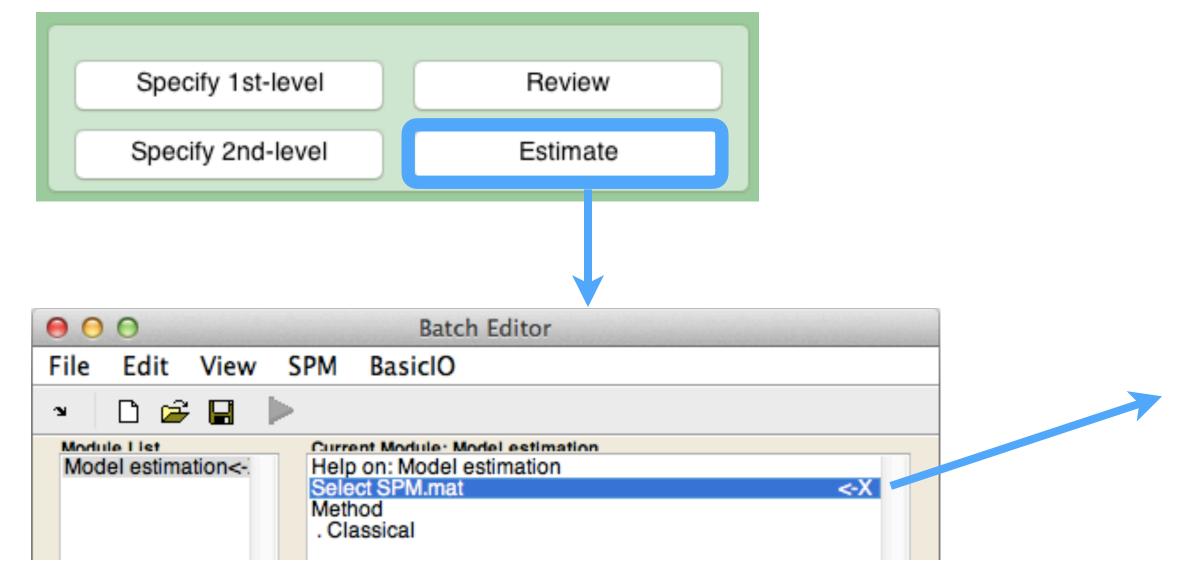
$$Y=\beta_0+\beta_{\rm U1}X_{\rm U1}+\beta_{\rm U2}X_{\rm U2}+\beta_{\rm F1}X_{\rm F1}+\beta_{\rm F2}X_{\rm F2}$$
 unknown parameters: β_i onset vectors: X_i

Voxel-wise 1st-level model



- **U1**: HRF convolved U1 condition
- **U2**: HRF convolved U2 condition
- **F1**: HRF convolved F1 condition
- **F2**: HRF convolved F2 condition
- Head motion parameters (HRF convolution 되지 않음.)
- Constant term: 상수항!

실습 - (Parameter) Estimation



Estimate

Specify 1st-level 을 통해서 구성한 General Linear Model의 unknown parameters의 값을 추정(계산)함.

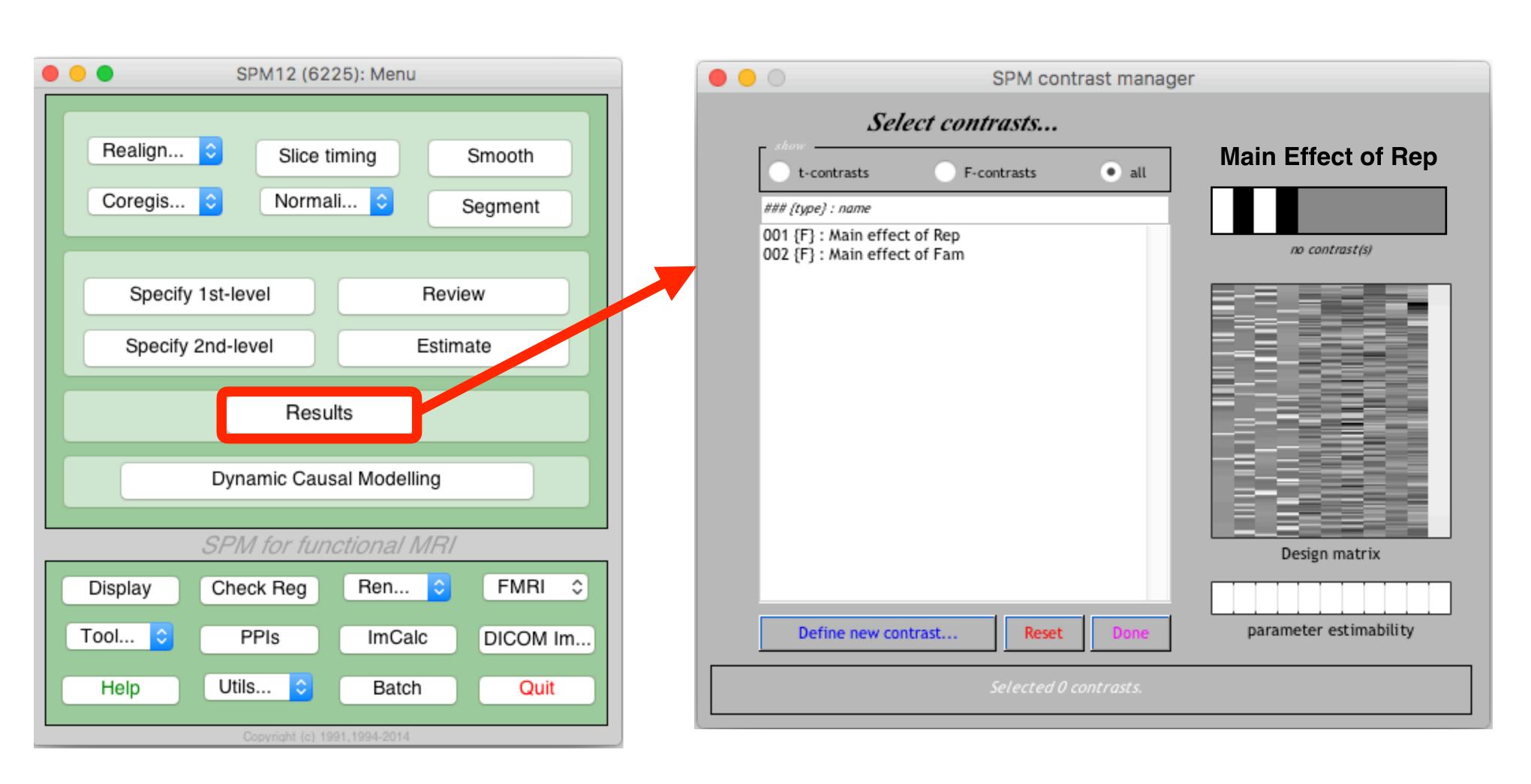
Select SPM.mat

Slide의 11페이지에서 지정했던 Directory에 생성된 SPM.mat 파일을 선택함.

$$Y=\beta_0+\beta_{\rm U1}X_{\rm U1}+\beta_{\rm U2}X_{\rm U2}+\beta_{\rm F1}X_{\rm F1}+\beta_{\rm F2}X_{\rm F2}+\sum\beta_kX_k$$
 unknown parameters: β_i onset vectors: X_i

Regressors of no interest

실습 - Results (Create F-contrasts)



Main Effect of Rep



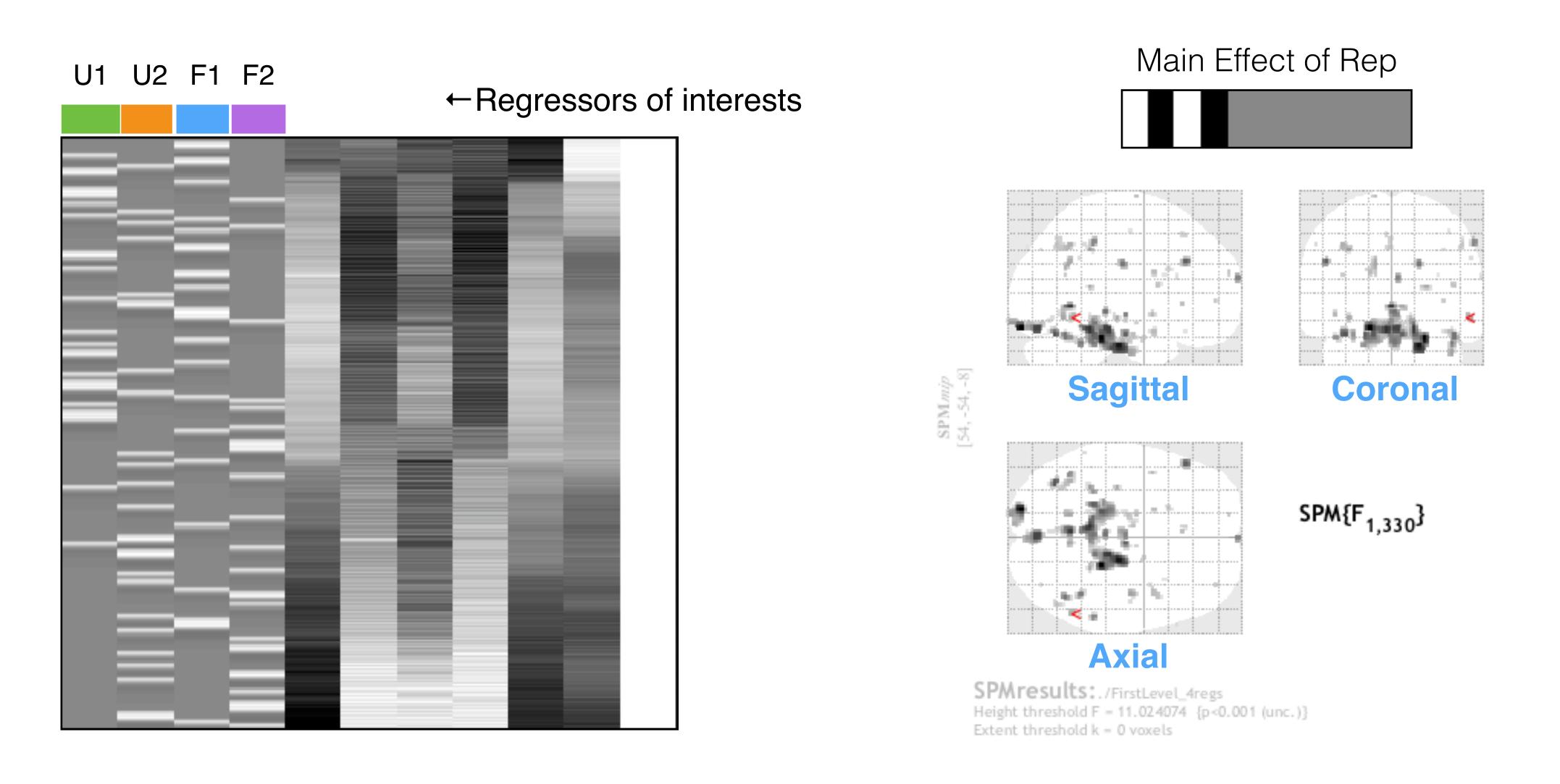
[1-11-1000000]or [-11-11000000]

Main Effect of Fam



[11-1-1000000][-1 -1 1 1 0 0 0 0 0 0]

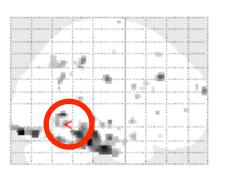
실습 - Visualization

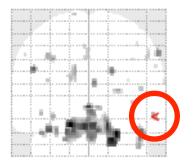


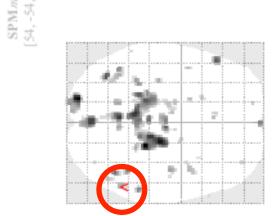
실습 - Plotting Time-courses

Ventral temporal cortex

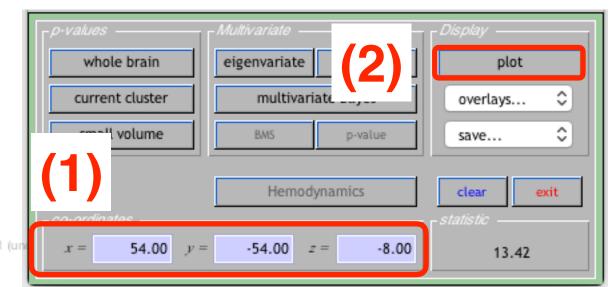
MNI: [54, -54, -8]



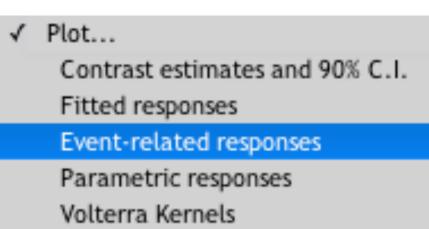


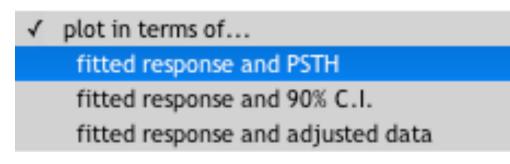






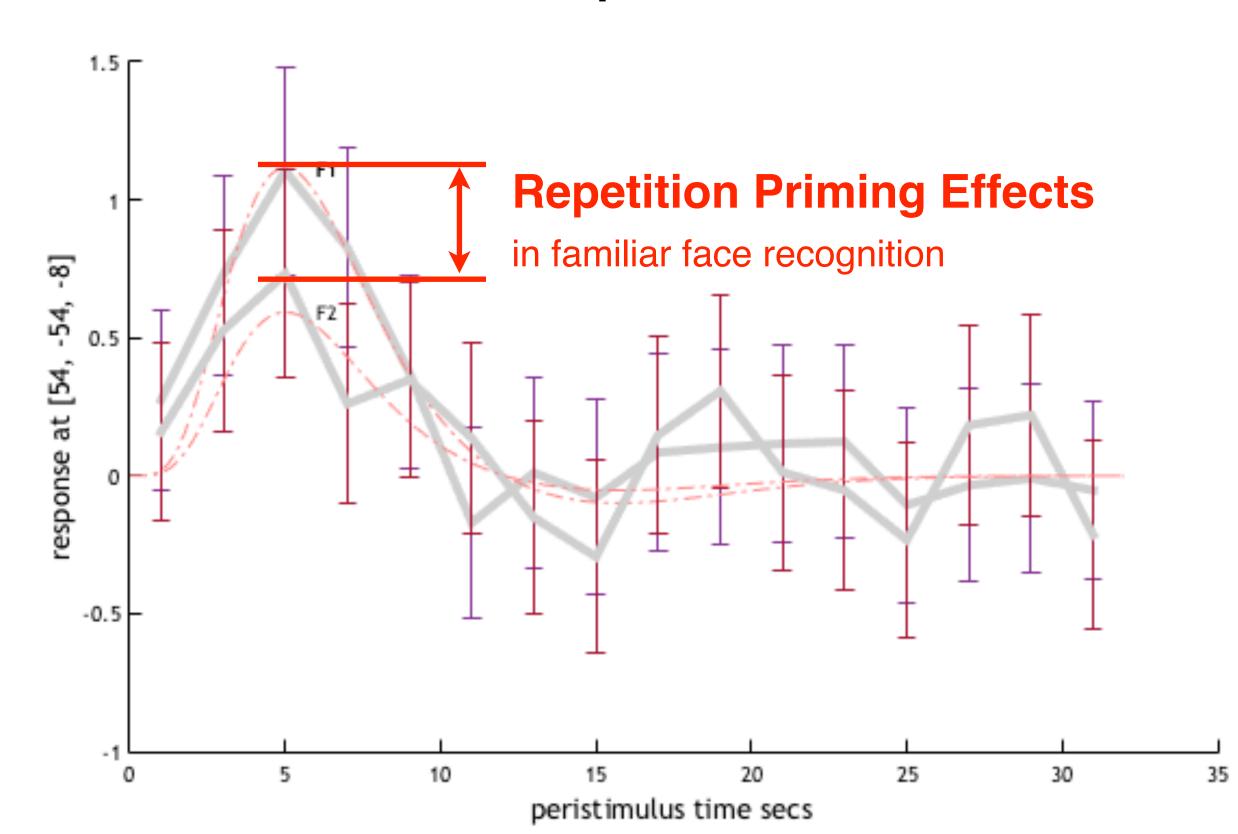




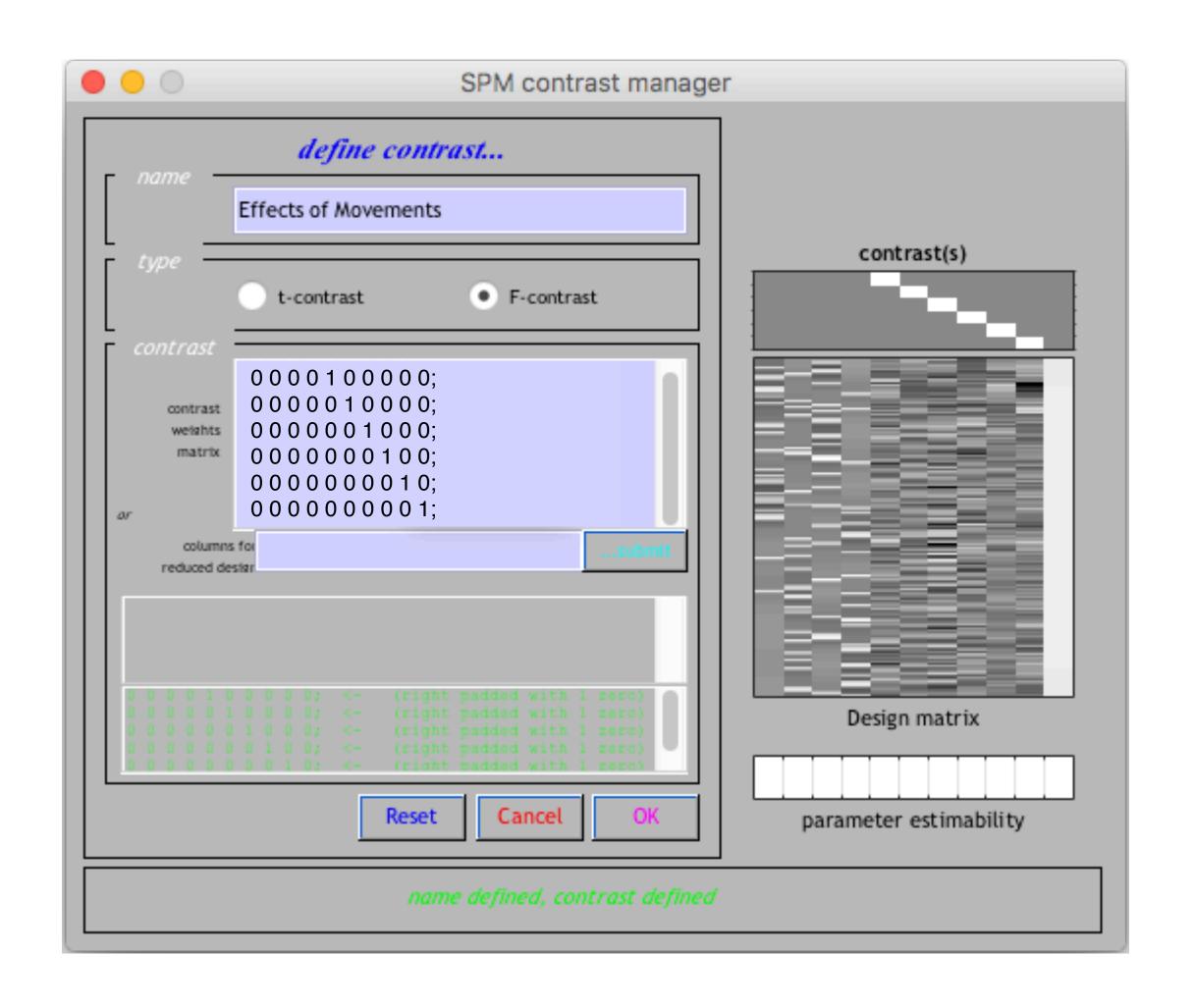


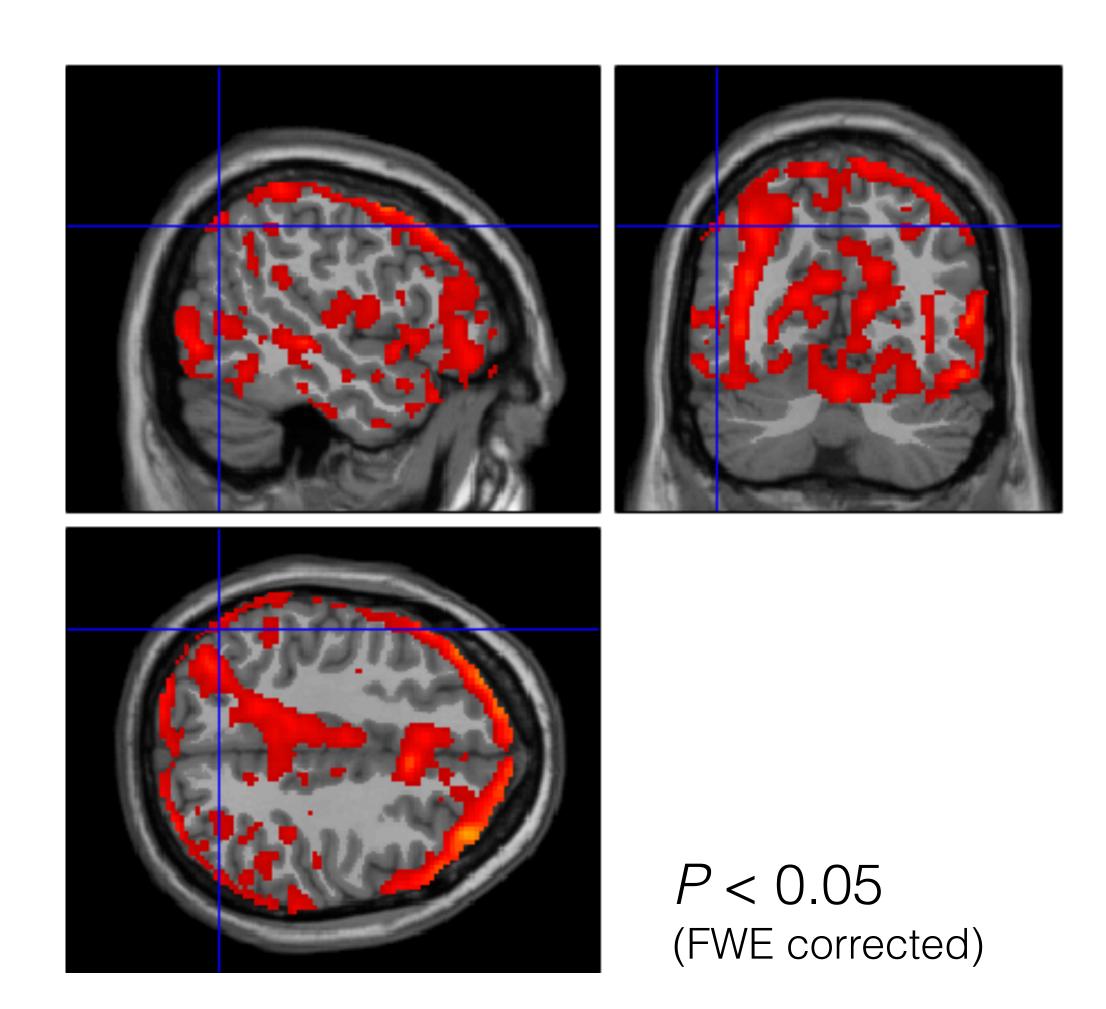
where, **PSTH** indicates peristimulus histogram.

Fitted response and PSTH



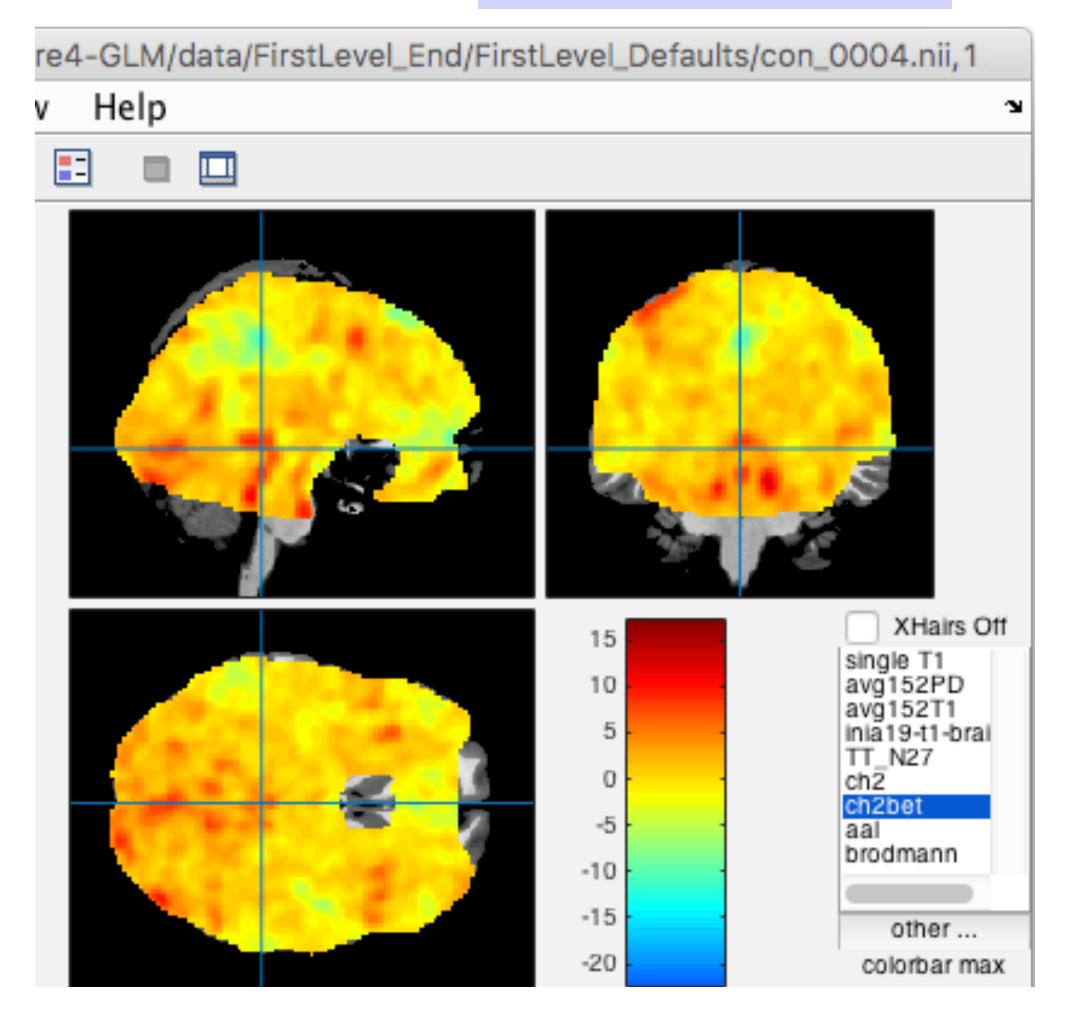
F-contrasts for testing effects of movement



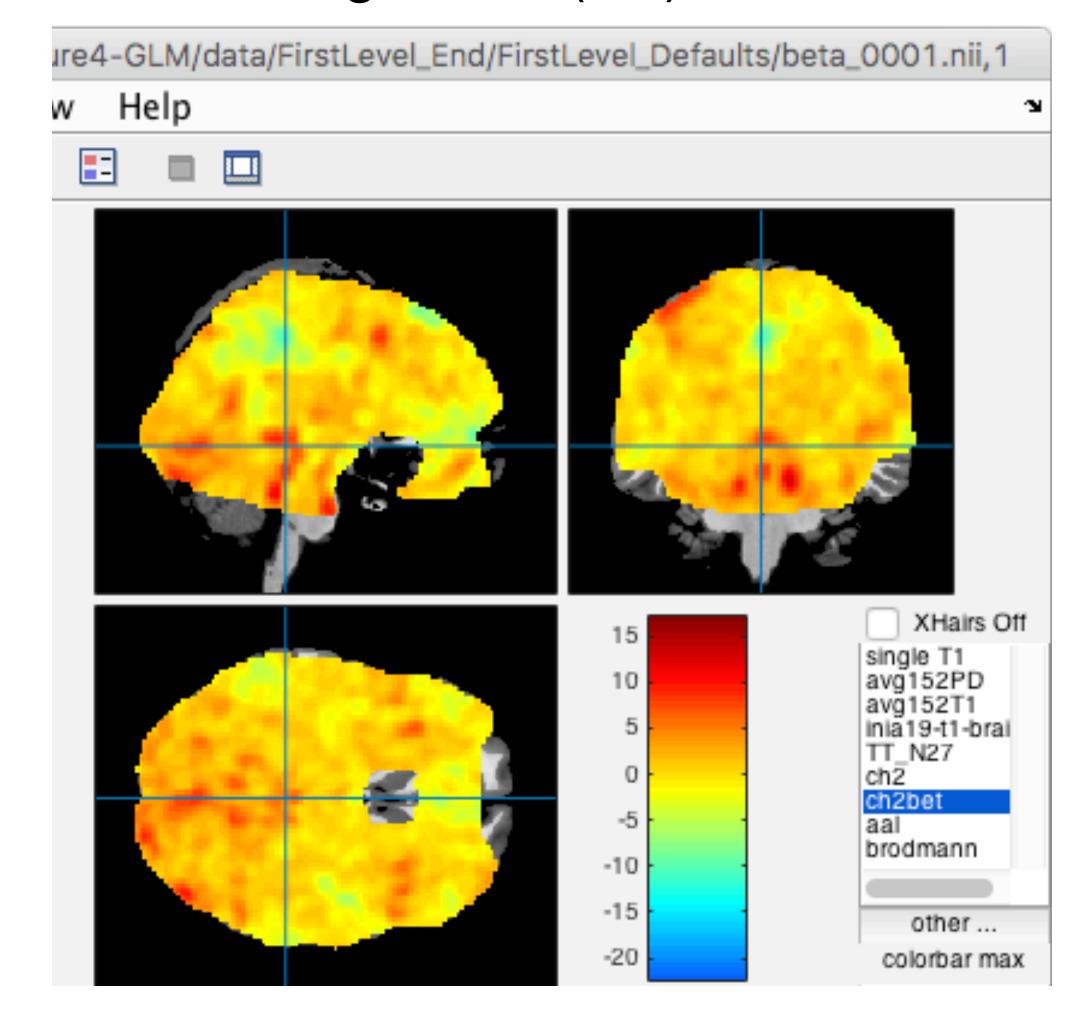


Con vs Beta files

T-contrast: 1000000000;



첫번째 Regressor (U1) 에 대한 beta

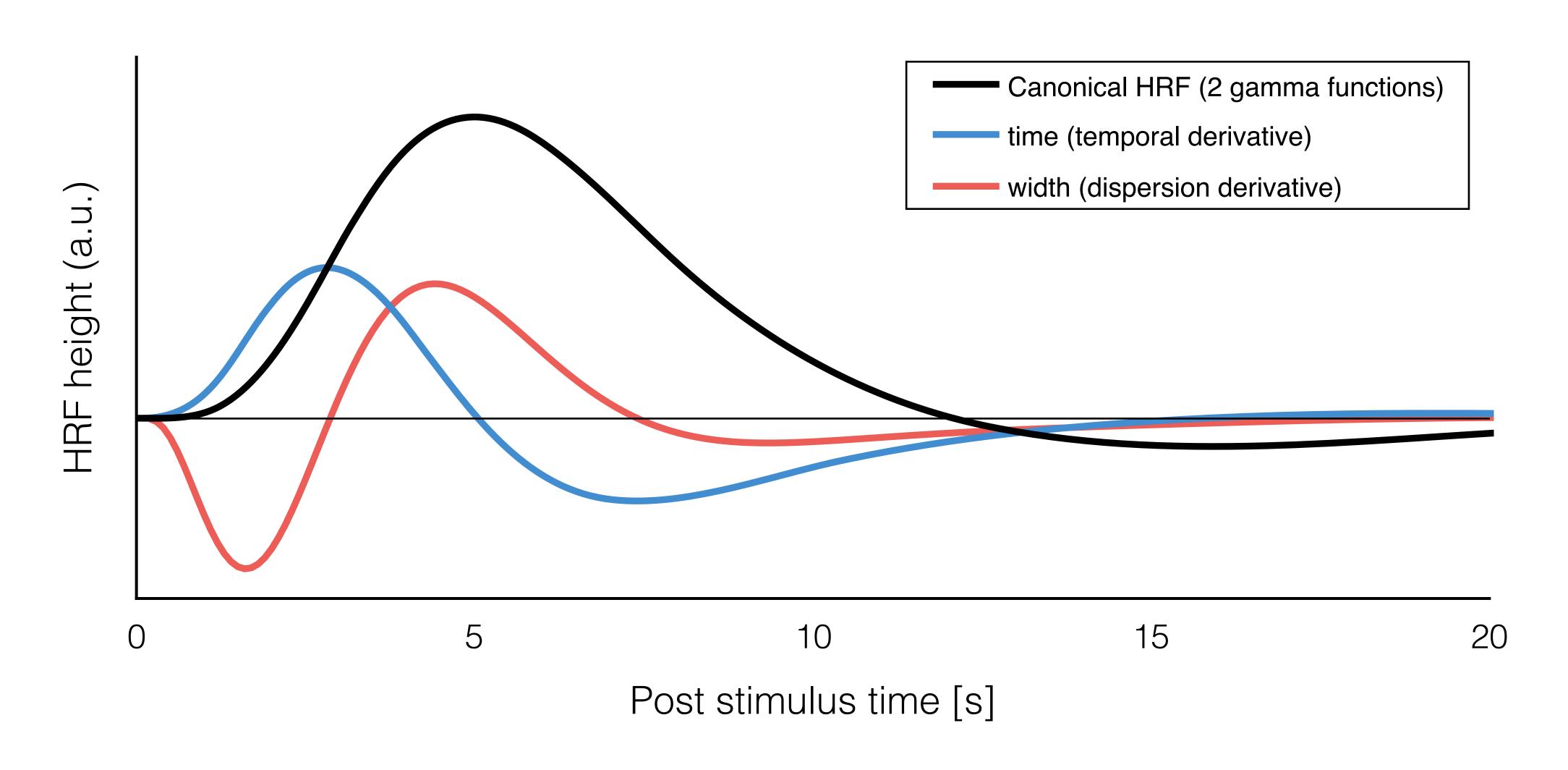


Con vs Beta files

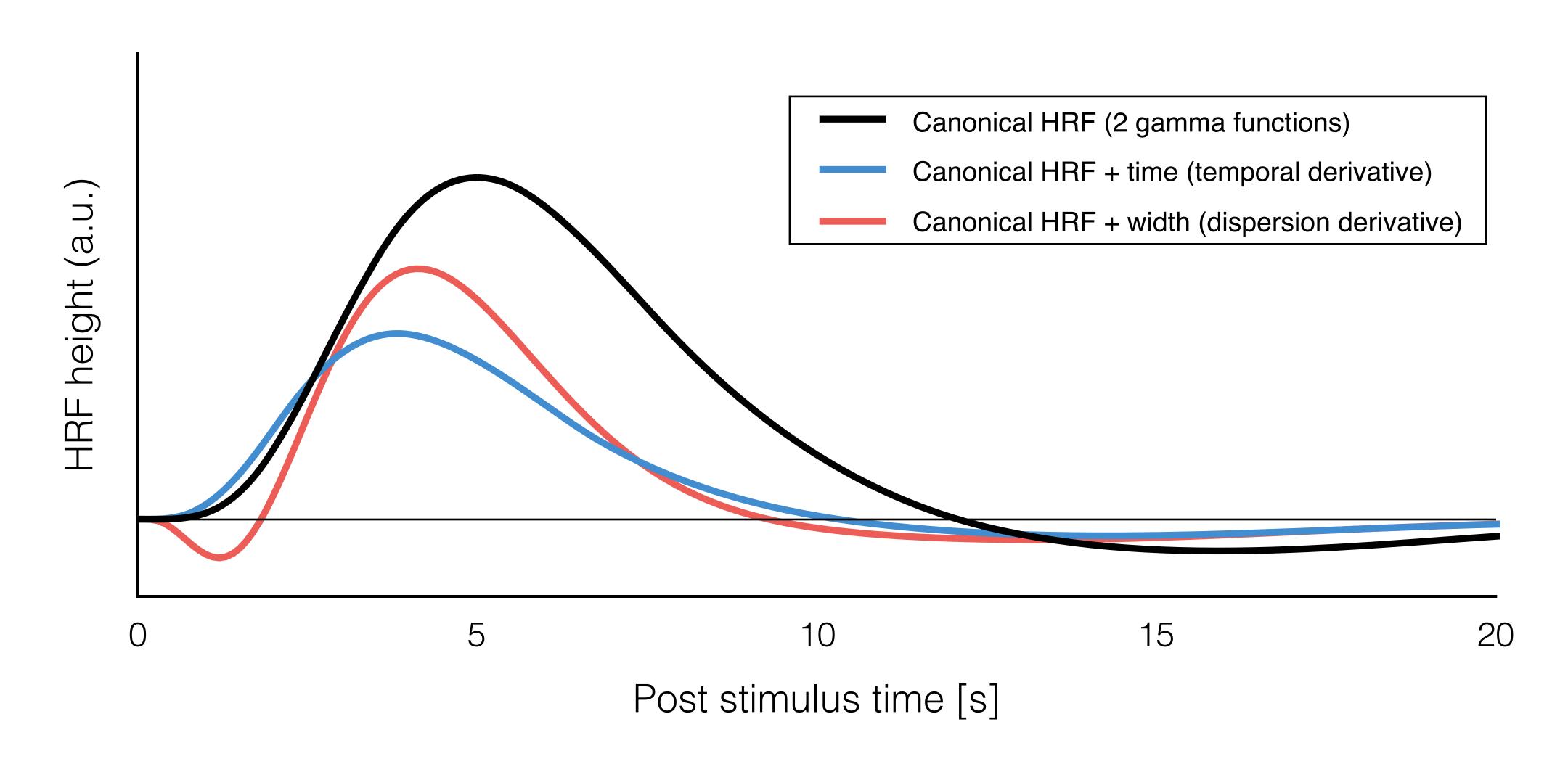
- 왜 같을까?
- 만약 세션이 2개라면, 2 세션에서 각각 estimated된 평균 beta 값이 con 파일로 생성될 것임.
- 만약, 서로 다른 조건의 beta에 대한 contrast를 만든다면 조건간 차이값이 con 파일로 생성될 것임.

Inclusion of Higher Order Canonical HRF

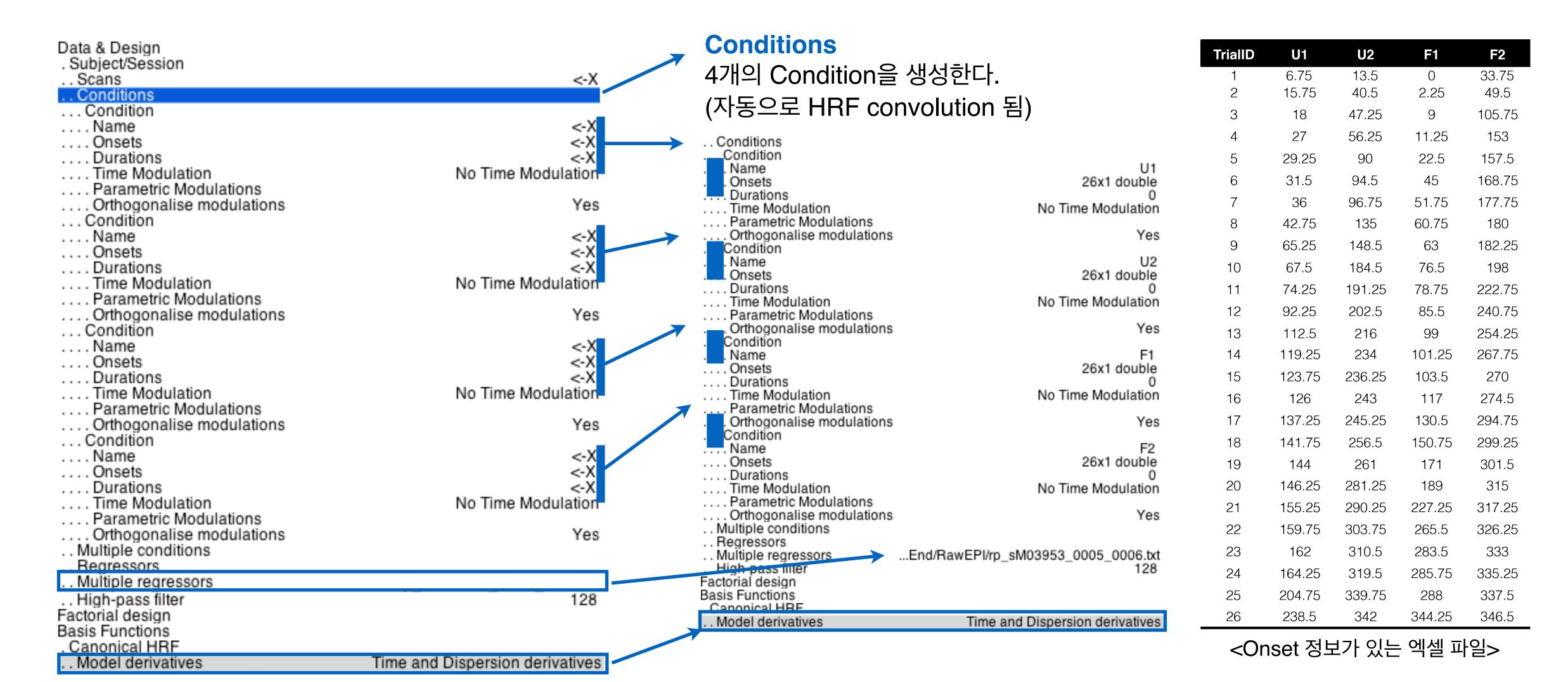
What are HRFs?



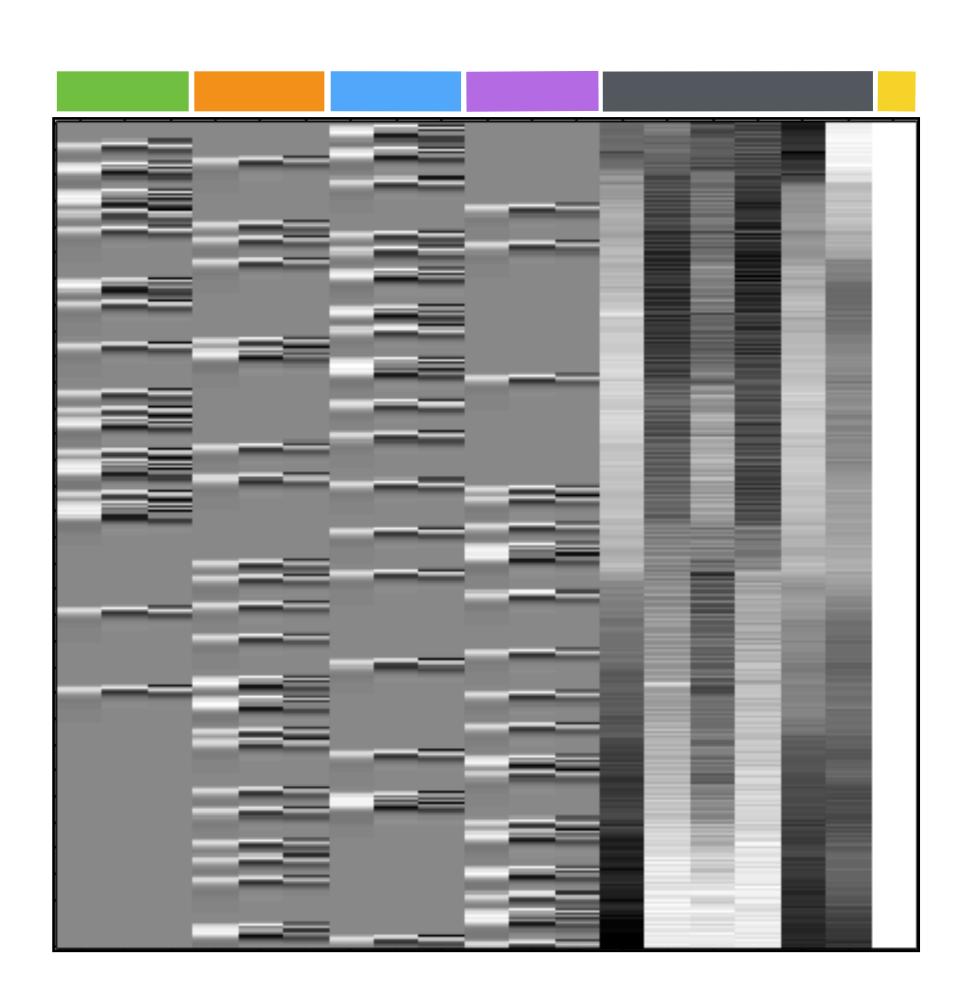
Variants of Canonical HRF



실습 - Specify 1st-level (time modulation)



Voxel-wise 1st-level model



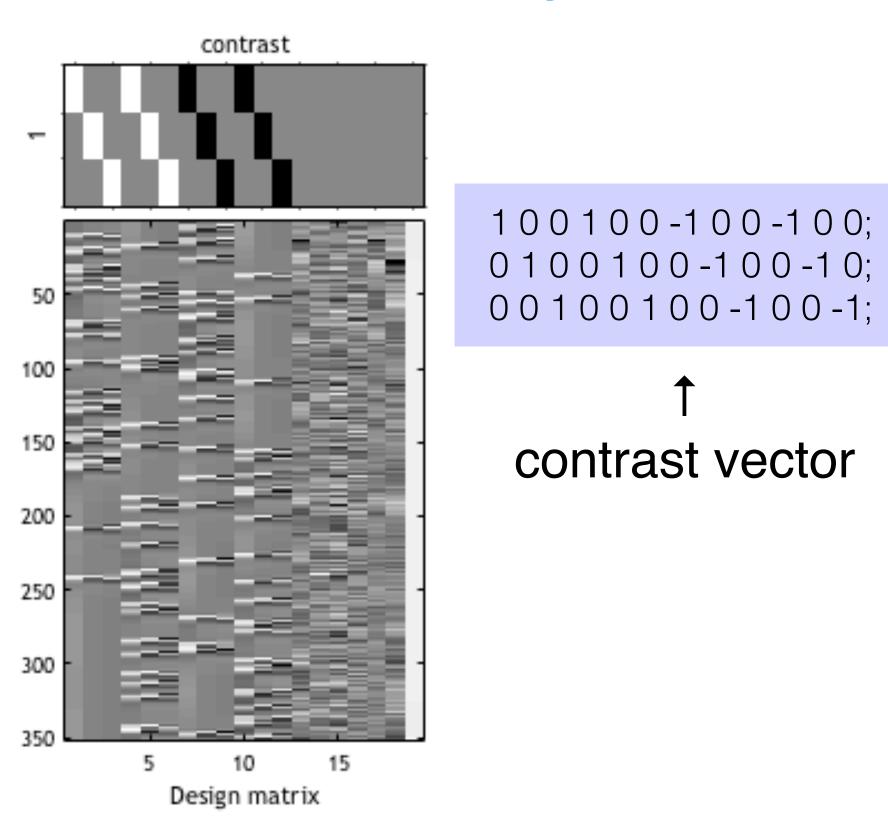
- **U1**: HRF convolved U1 condition and 1st and 2nd order derivatives of HRF
- **U2**: HRF convolved U2 condition and 1st and 2nd order derivatives of HRF
- F1: HRF convolved F1 condition and 1st and 2nd order derivatives of HRF
- **F2**: HRF convolved F2 condition and 1st and 2nd order derivatives of HRF
- Head motion parameters (HRF convolution 되지 않음.)
- Constant term: 상수항!

Time modulations?

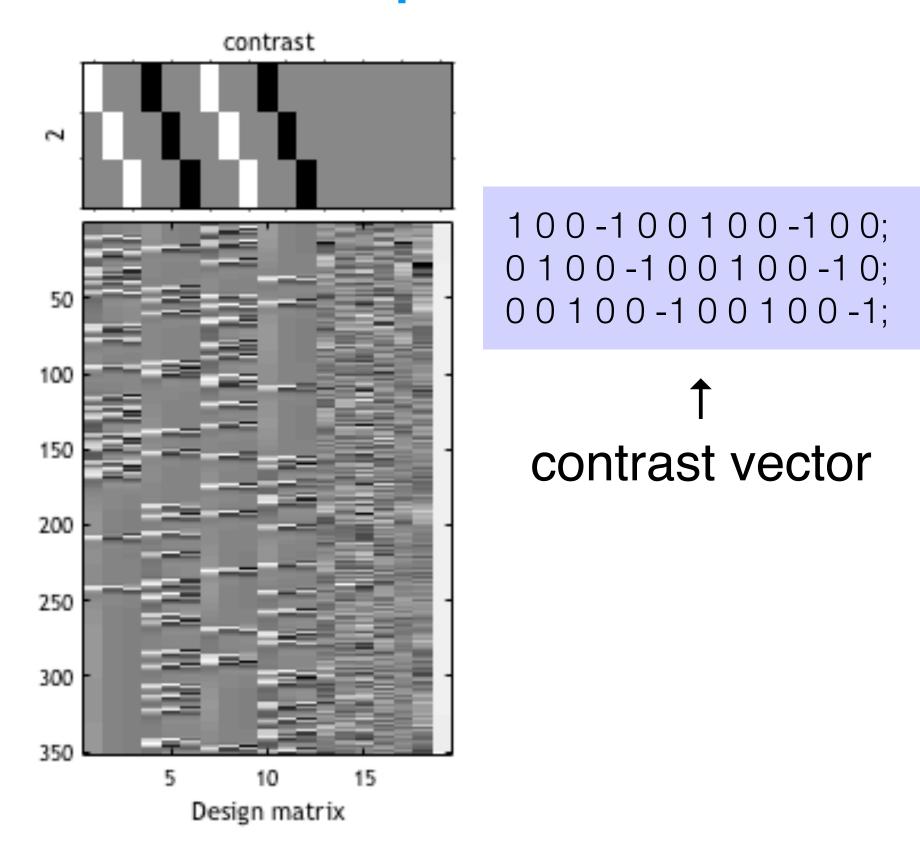
For example, 1st order modulation would model the stick functions and a linear change of the stick function heights over time. Higher order modulation will introduce further volumes that contain the stick functions scaled by time squared, time cubed etc.

실습 - Results (Create F-contrasts)

Effects of Familiarity

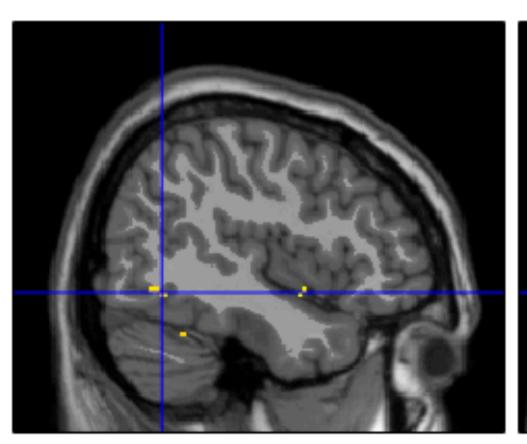


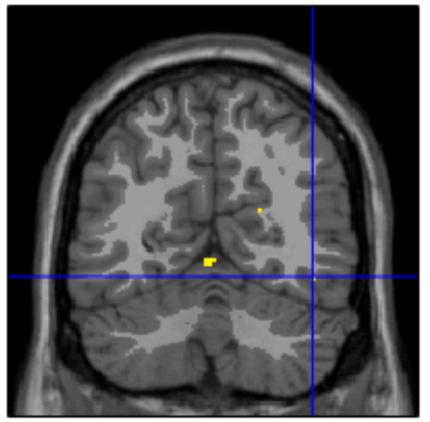
Effects of Repetition

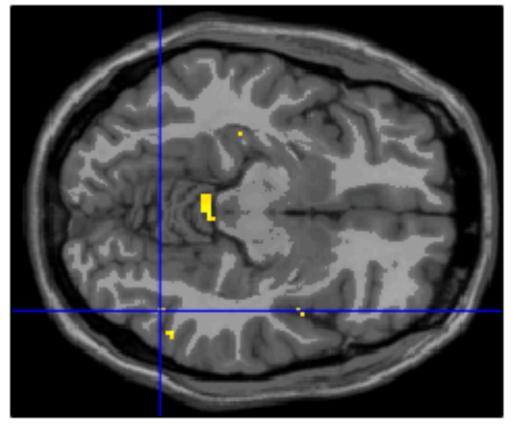


실습 - Plotting Time-courses

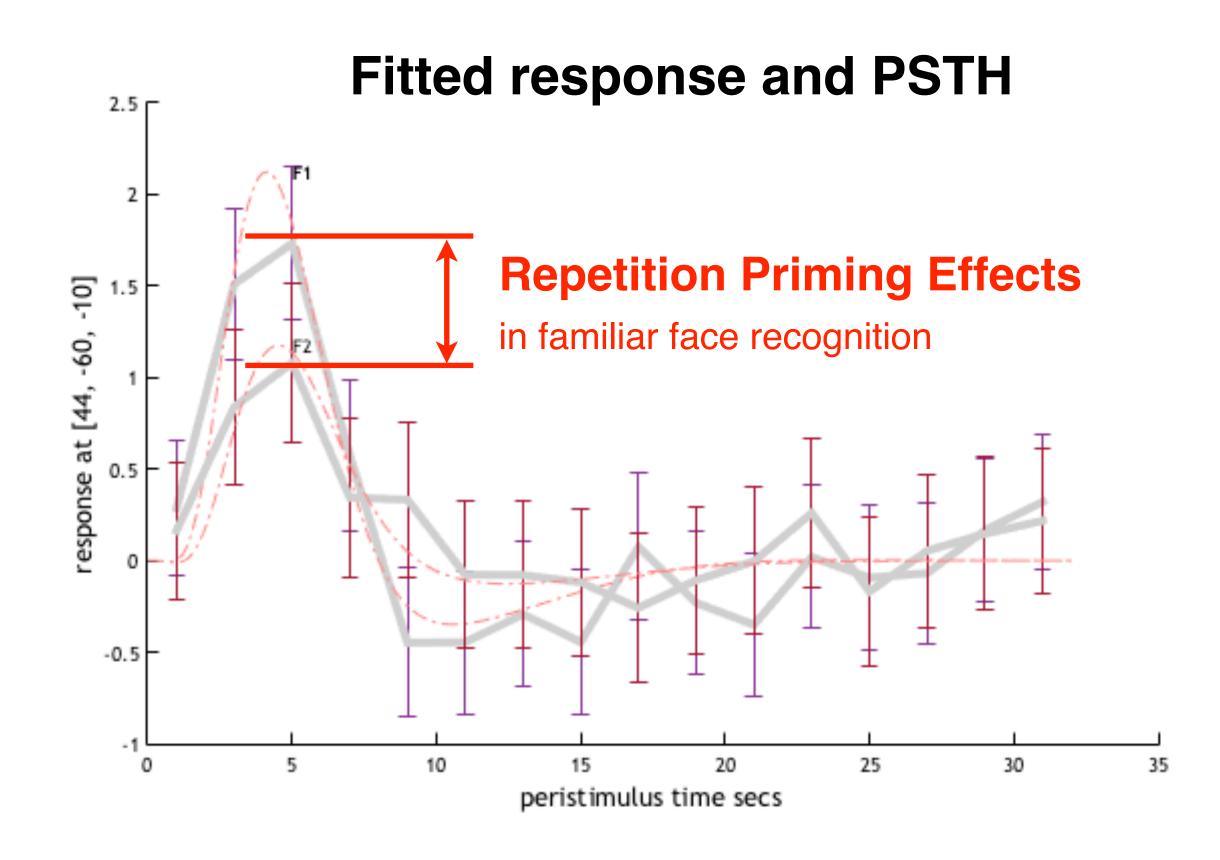
Effects of Repetition (F-contrast)







Fusiform Face Area (FFA) (MNI = 44, -60, -10)

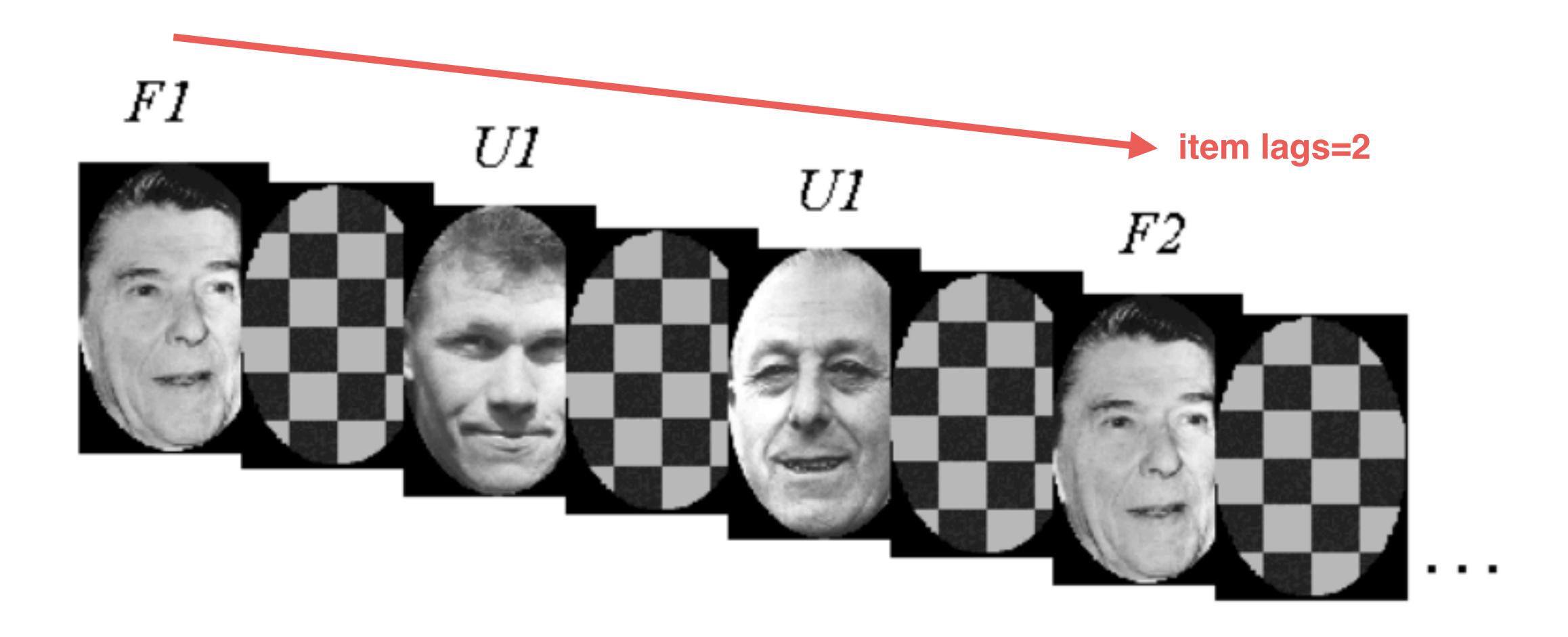


Neural activity in the right FFA decreases for repeated familiar face recognition.

Modeling parametric responses

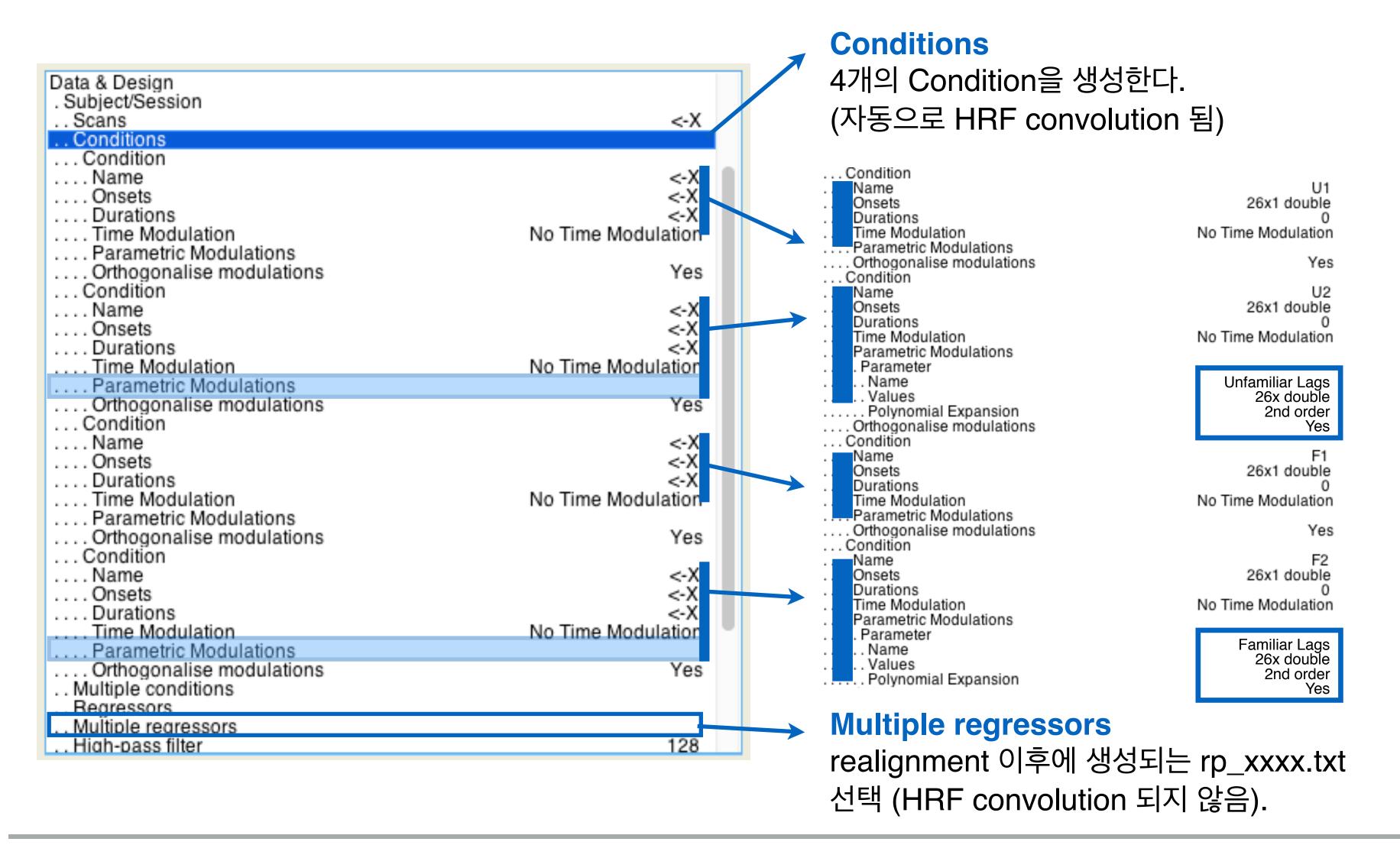
Item Lags

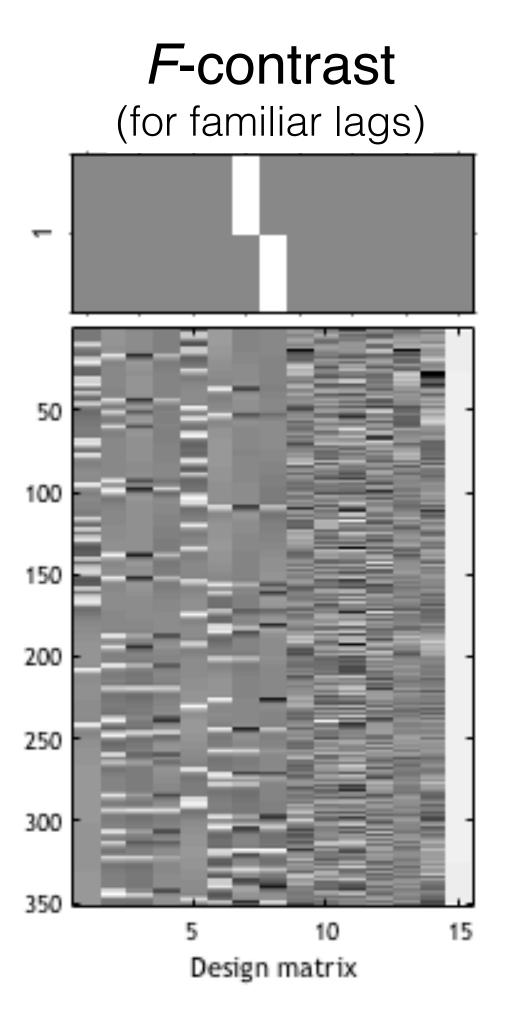
Number of other faces intervening between this (repeated) presentation and its previous (first) presentation



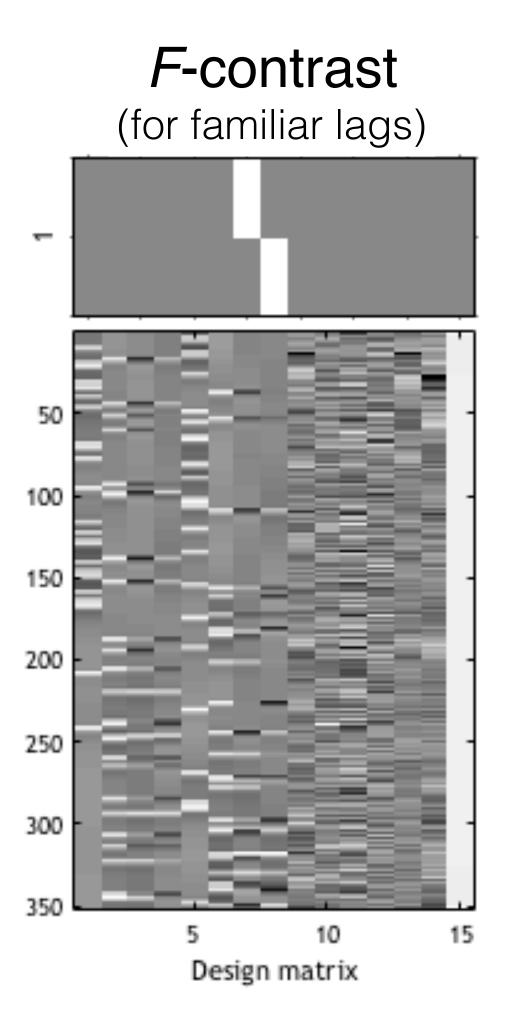
TriallD	U1	U2	U2 (item lags)	F1	F2	F2 (item lags)
1	6.75	13.5	3	0	33.75	11
2	15.75	40.5	3	2.25	49.5	14
3	18	47.25	10	9	105.75	2
4	27	56.25	10	11.25	153	47
5	29.25	90	14	22.5	157.5	36
6	31.5	94.5	1	45	168.75	18
7	36	96.75	23	51.75	177.75	37
8	42.75	135	3	60.75	180	59
9	65.25	148.5	3	63	182.25	11
10	67.5	184.5	37	76.5	198	56
11	74.25	191.25	10	78.75	222.75	33
12	92.25	202.5	42	85.5	240.75	4
13	112.5	216	61	99	254.25	57
14	119.25	234	33	101.25	267.75	18
15	123.75	236.25	27	103.5	270	59
16	126	243	61	117	274.5	55
17	137.25	245.25	28	130.5	294.75	46
18	141.75	256.5	22	150.75	299.25	61
19	144	261	39	171	301.5	4
20	146.25	281.25	37	189	315	67
21	155.25	290.25	62	227.25	317.25	9
22	159.75	303.75	37	265.5	326.25	63
23	162	310.5	20	283.5	333	13
24	164.25	319.5	54	285.75	335.25	19
25	204.75	339.75	34	288	337.5	42
26	238.5	342	50	344.25	346.5	1

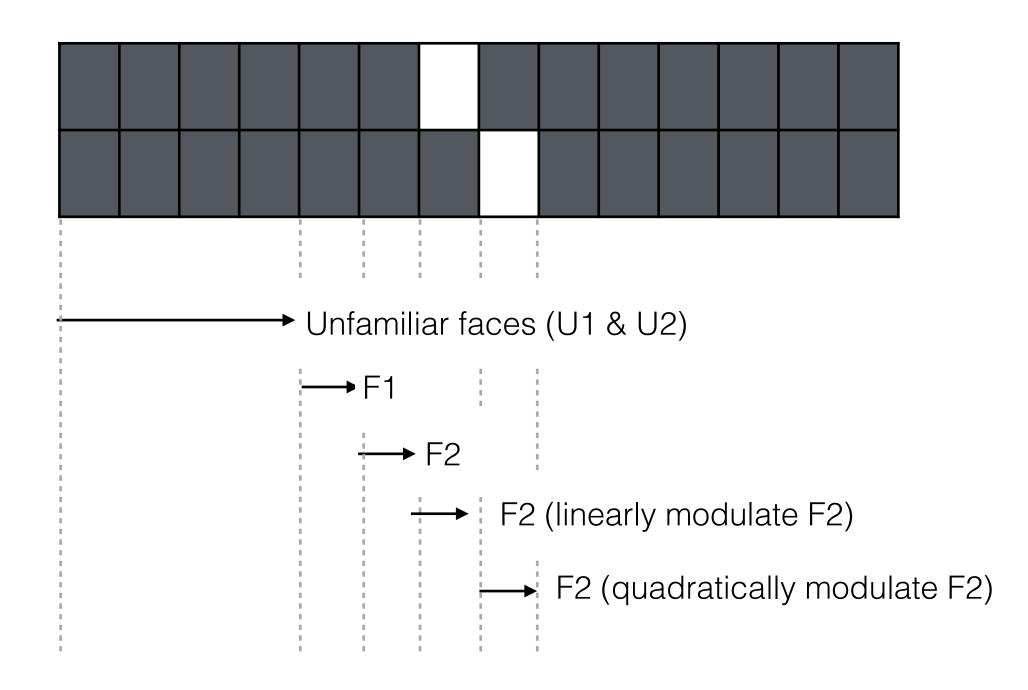
실습 - Specify 1st-level (Item Lags)





F-contrasts for familiar lags



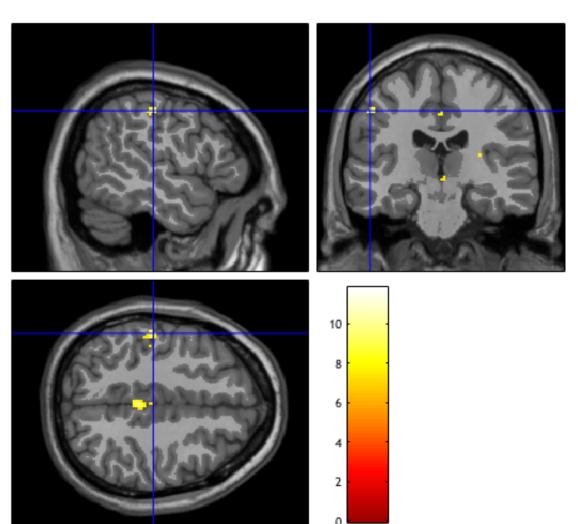


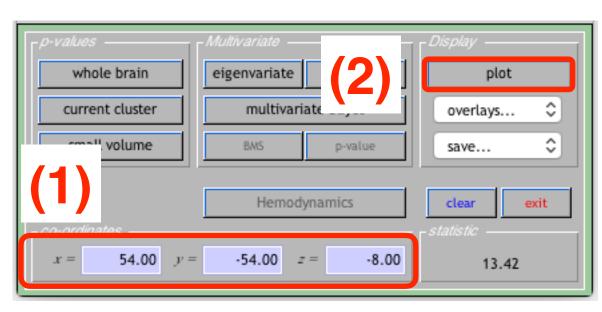
0000010000000; 0000001000000;

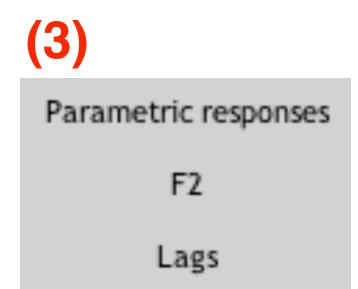
contrast vector

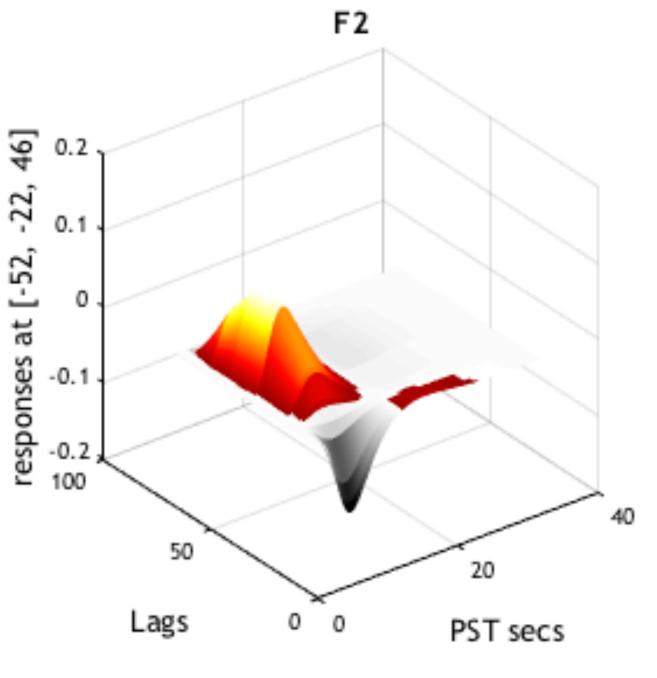
실습 - Plotting Parametric Responses

Left parietal region MNI: [-52, -22, 46]



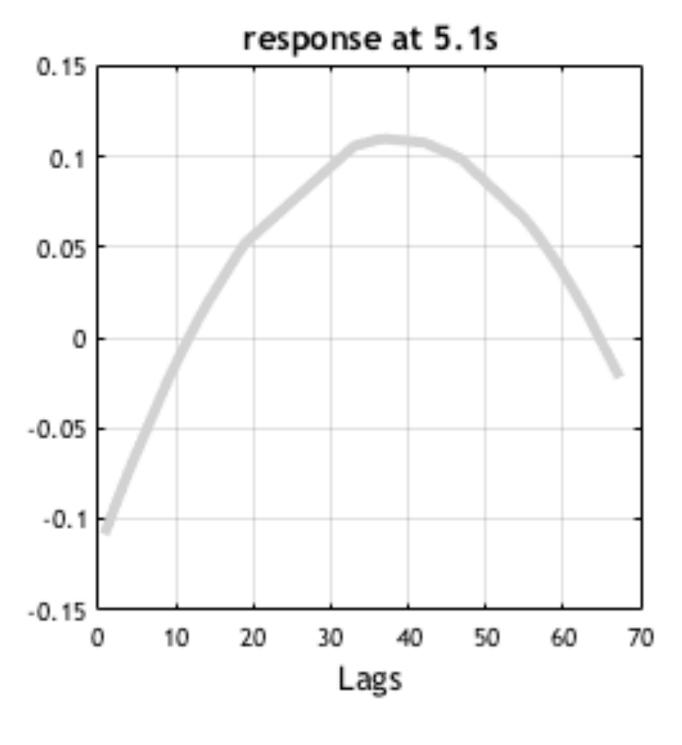






where **PST** represents peristimulus time

Quadratic effects of lag



Removal of linear and quadratic trends



Peripheral inflammation related to lower fMRI activation during a working memory task and resting functional connectivity among older adults: a preliminary study

Sheena I. Dev^{1,2}, Raeanne C. Moore^{1,3}, Benchawanna Soontornniyomkij¹, Cristian L. Achim¹, Dilip V. Jeste^{1,3} and Lisa T. Eyler^{1,3,4}

ranges of quality ay accuracy and ole and accurate

Image acquisition

Imaging data were acquired using a research dedicated 3 Tesla General Electric Excite MRI scanner with an 8channel head coil. High resolution structural T1weighted MRI images were acquired using a magnetization-prepared rapid acquisition gradient echo (MPRAGE) sequence. The resulting images were utilized to localize the functional signal. BOLD signal was acquired during the n-Back functional scan using gradient echo planar imaging (TR=2500 msec, $TE = 32 \, \text{ms}$ slice thickness/no 4-mm gap, FOV = 25.6 cm, bandwidth = 125, 195 repetitions). The BOLD signal for the resting state connectivity scan was measured with T2*-weighted echo planar

NeuroImages (AFNI) software package (Cox, 1996), using a streamlined pathway that included (i) removal of the first time point to account for signal stabilization; (ii) removal of skull and surrounding tissue; (iii) spatial smoothing to 6 full-width-to-halfmaximum; (iv) grand mean scaling; (v) application of high-pass temporal filter and low-pass temporal filter; and (vi) removal of linear and quadratic trends. Each participant's anatomical scan underwent cerebral spinal fluid, white matter (WM) and grey matter (GM) segmentation using the Oxford Centre for Functional Magnetic Resonance Imaging of the Brain (FMRIB) Software Library (FSL) FMRIB Linear Image Registration Tool (FLIRT) program and were functional subsequently registered to Automated motion correction was then applied to all participants to correct for excessive motion during scan time. A visual inspection was conducted and remaining data points with excessive motion were

rejected.

S. I. Dev et al.

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Neural Predictors of Purchases

Brian Knutson,1,* Scott Rick,2 G. Elliott Wimmer,1 Drazen Prelec,3 and George Loewer Psychology and Neuroscience, Stanford University, Building 420, Jordan Hall, Stanford, CA 94305 ²Social and Decision Sciences, Carnegie Mellon University, 208 Porter Hall, Pittsburgh, PA 15213, University, 208 Porter Hall, Pittsburgh, 208 Porter Hall, P ³MIT Sloan School of Management, Massachusetts Institute of Technology, E56-320, Cambridge, I *Correspondence: knutson@psych.stanford.edu DOI 10.1016/j.neuron.2006.11.010

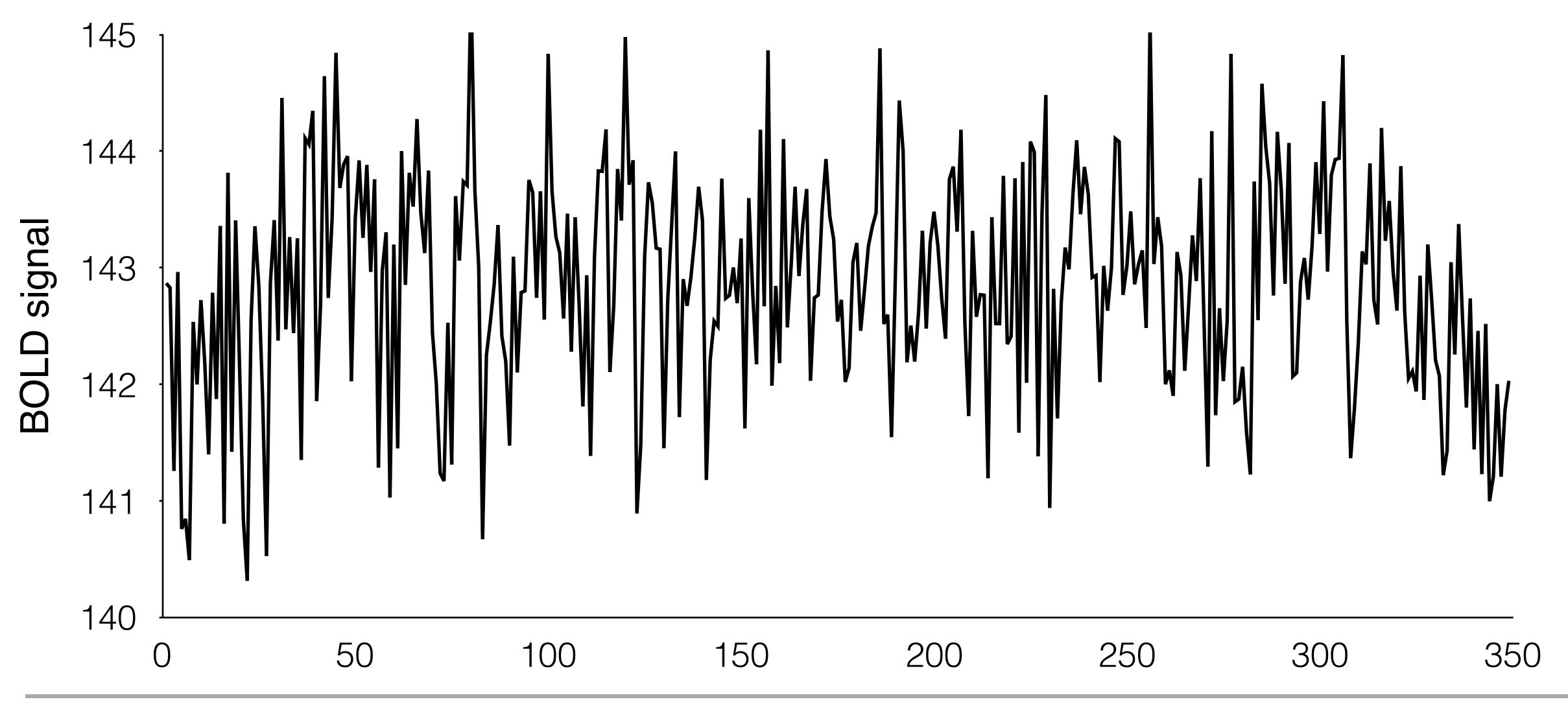
fMRI Acquisition and Analysis

Images were acquired with a 1.5-T General Electric MRI scanner using a standard birdcage quadrature head coil. Twenty-four four-millimeter-thick slices (in-plane resolution 3.75×3.75 mm, no gap) extended axially from the mid-pons to the top of the skull, providing whole-brain coverage and adequate spatial resolution of subcortical regions of interest (e.g., midbrain, NAcc, OFC). Whole-brain functional scans were acquired with a T2*-sensitive spiral in-/out- pulse sequence (TR = 2 s, TE = 40 ms, flip = 90°) designed to minimize signal dropout at the base of the brain (Glover and Law, 2001) (Supplement 3). High-resolution structural scans were also acquired to facilitate localization and coregistration of functional data using a T1-weighted spoiled grass sequence (TR = 100 ms, TE = 7 ms, flip = 90°).

Analyses were conducted using Analysis of Functional Neural Images (AFNI) software (Cox, 1996). For preprocessing, voxel time series were sinc interpolated to correct for nonsimultaneous slice acquisition within each volume, concatenated across runs, corrected for motion, high-pass filtered (admitting frequencies with period <90 s), and normalized to percent signal change with respect to the voxel mean for the entire task. Visual inspection of motion correction estimates confirmed that no subject's head moved more than 2.0 mm in any dimension from one volume acquisition to the next. All regression models included six regressors indexing residual motion and six regressors modeling baseline, linear, and quadratic trends for each of the two runs.

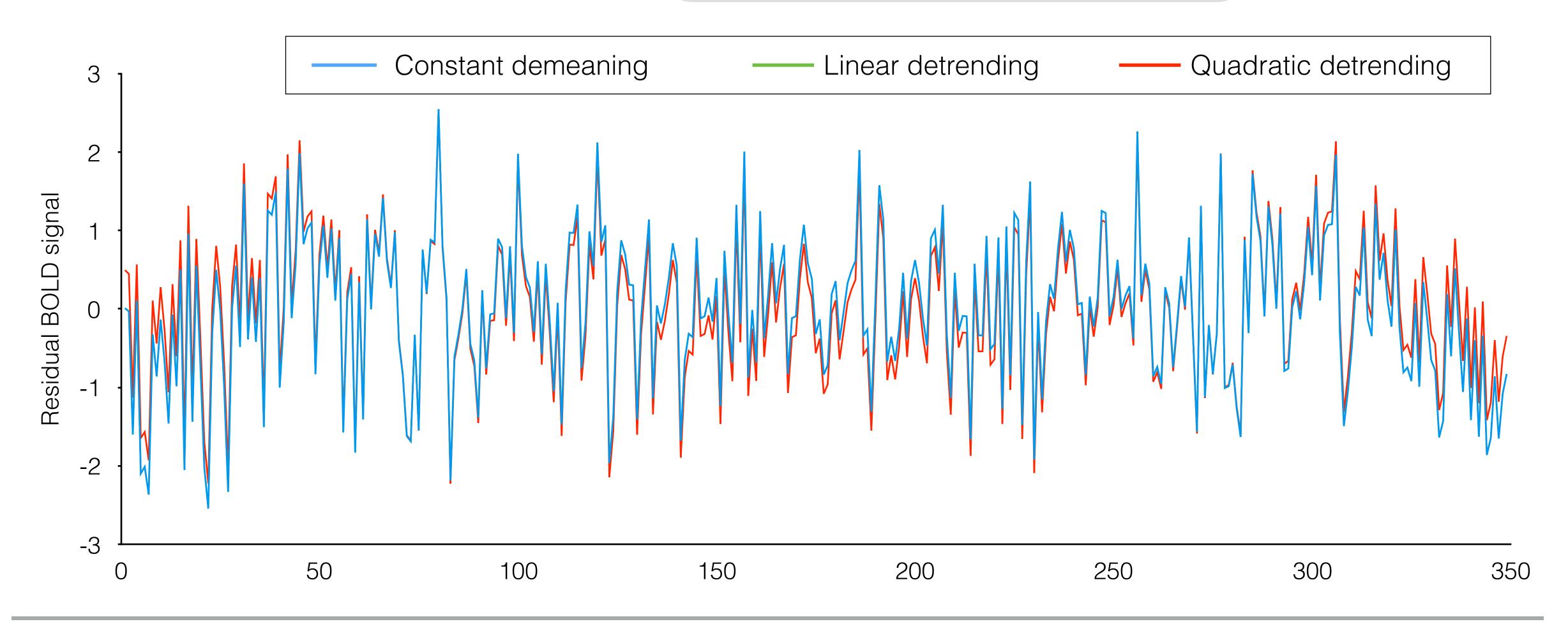
BOLD fMRI time-series

at MNI = [44,-60,-10]

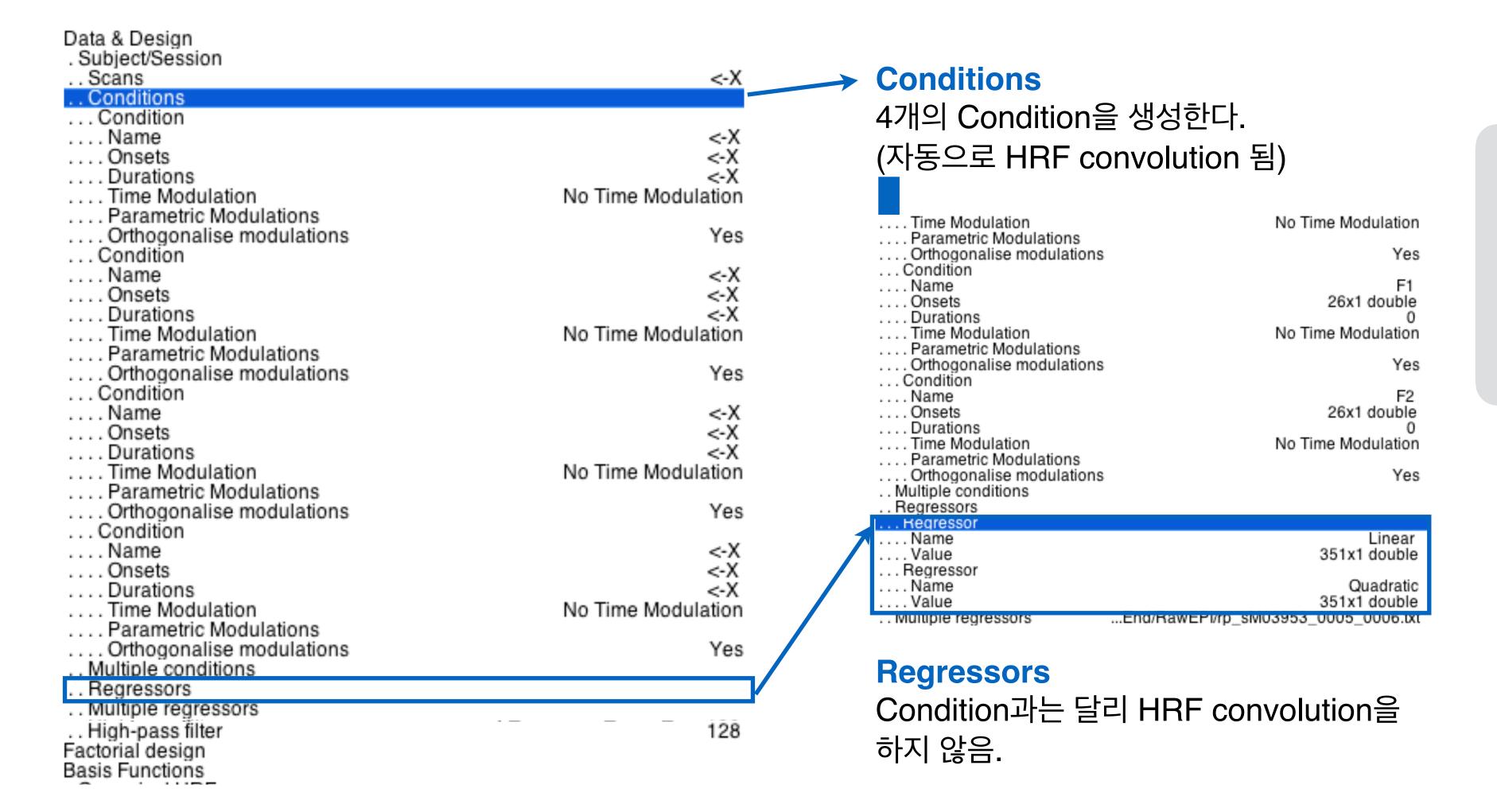


Constant, linear, quadratic detrending

Linear Regression Model:
$$Y_0=\beta_0+\beta_1x+\beta_2x^2+arepsilon$$



실습 - Specify 1st-level (detrending)



In tutorial directory,

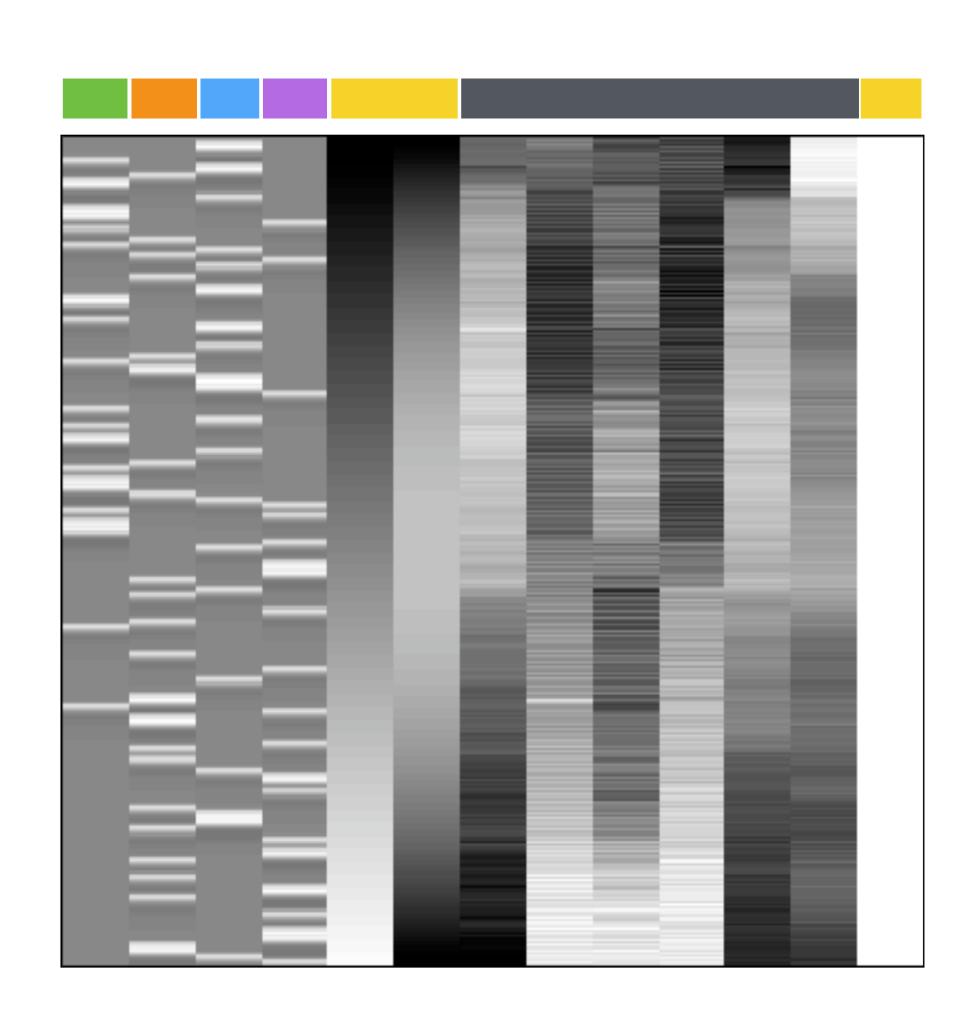
Linear function:

y = regressor_linear (nscan)

Quadratic function:

y = regressor_quadratic (nscan)

Voxel-wise 1st-level model



- **U1**: HRF convolved U1 condition
- **U2**: HRF convolved U2 condition
- **F1**: HRF convolved F1 condition
- **F2**: HRF convolved F2 condition
- Head motion parameters (HRF convolution 되지 않음.)
- Constant, linear, quadratic term: 상수항, 1차항, 2차항!

Summary

- SPM12 를 이용한 개별 fMRI 데이터 통계 분석 방법을 익힘.
- Specify 1st-level에서 Conditions에 Onset으로 입력한 vector값은 자동으로 HRF 함수가 convolution 되어 선형회귀분석에 모델링 됨.
- HRF의 1st-order derivatives and 2nd-order derivatives를 모델에 포함하는 방법을 공부함. 포함하지 않은경우와 비교하여, 결과가 어떻게 달라지는지 확인함.
- Head motion과 관련된 잡음은 어떤 패턴으로 활성화 맵에 표시 되는지 확인함.
- Parametric modulation을 관찰하기 위한 1st-level 분석을 어떻게 하는지 공부함.
- Constant(default), linear, quadratic trending signals을 SPM에서 제거하는 방법 공부함.

Coming soon!

2nd-level (or group-level) statistical inference in SPM12