

# Estimation of NMR Signals in the Time Domain: Methodology, Applications and Software

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For Mum and Dad,  
a constant source of support and inspiration



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# Abstract

Nuclear magnetic resonance spectroscopy (NMR) is an analytical technique employed in many scientific disciplines that is able to provide insights into the structures and dynamics of chemical species. To maximise the utility of NMR experiments, appropriate data treatment and analysis is necessary. The conventional route to extracting quantitative information from the raw experimental data — the free induction decay (FID) — is to convert it to an NMR spectrum, through application of the Fourier transform (FT). Such spectra provide a human-interpretable representation of data, with trained practitioners able to rationalise their appearance by mapping peaks in the spectrum to chemical environments in a given sample. However, the FT suffers from poor resolution, with peaks of similar frequencies often overlapping. Disentangling the quantitative information associated with such peaks is not feasible using typical methods such as spectrum integration. As an alternative, parametric estimation techniques aim to provide detailed information about each individual signal present in the data. These have been shown to perform effectively even in scenarios where significant signal overlap exists.

This thesis focusses on the development of a parametric estimation method for the analysis of FIDs derived from solution-state NMR experiments. The guiding principle behind the method is that it should require as little user input as possible, yet be able to provide accurate predictions of the parameters which describe an FID's contributing signals. Beyond simply providing a breakdown of individual signal components, many useful applications may be realised when estimation techniques are employed. The initial motivation for this work was to develop a procedure for the generation of pure shift NMR spectra with desirable properties from two-dimensional J-resolved (2DJ) datasets. Furthermore, a means of analysing 2D datasets such as those from inversion recovery ( $T_1$ ), Carl-Purcell-Meiboom-Gill (CPMG) ( $T_2$ ), and diffusion experiments, in which each FID exhibits a variation in its amplitude, is presented. The last application described is a means of producing phased, ultra-broadband NMR spectra from an experiment comprising a single frequency-swept (FS) (chirp) excitation pulse. The methods presented in this thesis are incorporated into a software package written in the PYTHON programming language, called NMR estimation in Python (NMR-EsPy).



# Acronyms

**1D** one-dimensional

**2D** two-dimensional

**2DJ** two-dimensional J-resolved

**3D** three-dimensional

**AIC** Akaike information criterion

**ALPESTRE** a linear predictive estimation of signal time reversal

**AMARES** advanced method for accurate, robust, and efficient spectral fitting

**API** application programming interface

**AR** autoregressive

**ARMA** autoregressive moving average

**AWGN** additive white Gaussian noise

**BFGS** Broyden-Fletcher-Goldfarb-Shanno

**BIRD** bilinear rotation decoupling

**CHORUS** chirped, ordered pulses for ultra-broadband spectroscopy

**CORE** component resolution

**COSY** correlation spectroscopy

**CPMG** Carl-Purcell-Meiboom-Gill

**CPU** central processing unit

**CRAFT** complete reduction to amplitude frequency table

**CSR** compressed sparse row

**CUPID** computer-assisted undiminished-sensitivity protocol for ideal decoupling

**DECRA** direct exponential curve resolution algorithm

**DFT** discrete Fourier transform

**DMSO** Dimethyl sulfoxide, (H<sub>3</sub>C)<sub>2</sub>SO

**DMSO-d<sub>6</sub>** Deuterated DMSO

**DOSY** diffusion-ordered spectroscopy

**EYM** Eckart-Young-Mirsky

**FID** free induction decay

**FDM** filter diagonalisation method

**FFT** fast Fourier transform

**FS** frequency-swept

**FT** Fourier transform

**GN** Gauss-Newton

**GNAT** General NMR Analysis Toolbox

**GUI** graphical user interface

**HSVD** Hankel singular value decomposition

**IFT** inverse Fourier transform

**INEPT** insensitive nuclei enhancement by polarization transfer

**ITMPM** information theoretic matrix pencil method

**LED** longitudinal eddy current delay

**LM** Levenberg-Marquardt

**LP** linear prediction

**LPSVD** linear prediction singular value decomposition

**MDL** minimum description length

**MEMPM** matrix enhancement and matrix pencil method

**MLE** maximum likelihood estimate

**MMEMPM** modified matrix enhancement and matrix pencil method

**MPM** matrix pencil method

**MRI** magnetic resonance imaging

- MRS** *in vivo* magnetic resonance spectroscopy
- NLP** non-linear programming
- NMR** nuclear magnetic resonance spectroscopy
- NMR-EsPy** NMR estimation in Python
- NOESY** nuclear Overhauser effect spectroscopy
- PDF** probability density function
- PFG** pulsed field gradient
- PGSE** pulsed gradient spin echo
- PGSTE** pulsed gradient stimulated echo
- PGSTEBP** pulsed gradient stimulated echo with bipolar gradients
- PROJECT** Periodic Refocusing of J Evolution by Coherence Transfer
- PSYCHE** pure shift yielded by chirp excitation
- RAM** random access memory
- RF** radio-frequency
- RSS** residual sum-of-squares
- SCORE** speedy component resolution
- SNR** signal-to-noise ratio
- ST** Steihaug-Toint
- SVD** singular value decomposition
- TSE-PSYCHE** triple spin echo PSYCHE
- TROSY** transverse relaxation optimised spectroscopy
- VARPRO** variable projection
- VE** virtual echo
- WURST** wideband, uniform rate, smooth truncation
- ZS** Zanger-Sterk



# Nomenclature

## General Mathematics

$\mathcal{A} := \mathcal{B}$       $\mathcal{A}$  is defined to be equal to  $\mathcal{B}$

$\lfloor a \rfloor$      The nearest integer to  $a$ , such that  $\lfloor a \rfloor \leq a$

$\lceil a \rceil$      The nearest integer to  $a$ , such that  $\lceil a \rceil \geq a$

$\lceil a \rceil$      The nearest integer to  $a$

$a \bmod b$       $a$  modulo  $b$ , given by

$$a \bmod b = a - \left\lfloor \frac{a}{b} \right\rfloor$$

## Complex Numbers

$i$      The imaginary unit,  $i := \sqrt{-1}$

$\Re(z)$      The real component of  $z$

$\Im(z)$      The imaginary component of  $z$

$|z|$      The absolute value of  $z$ , given by

$$|z| = \sqrt{\Re(z)^2 + \Im(z)^2}$$

## Number sets

$\mathbb{C}$      The set of complex numbers

$\mathbb{N}$      The set of natural numbers with zero excluded

$\mathbb{N}_0$      The set of natural numbers with zero included

$\mathbb{R}$      The set of real numbers

$\mathbb{R}_{>0}$      The set of positive real numbers

$\mathbb{Z}$      The set of integers

## Probability

$x \sim \mathcal{X}$        $x$  behaves according to distribution  $\mathcal{X}$

$A \perp\!\!\!\perp B$        $A$  and  $B$  are conditionally independent

$\mathcal{N}(\mu, \sigma^2)$       Normal (Gaussian) distribution with mean  $\mu$  and variance  $\sigma^2$ :

$$\mathcal{N}(x | \mu, \sigma^2) = \frac{1}{\sqrt{2\pi\sigma^2}} \exp\left(-\frac{(x - \mu)^2}{2\sigma^2}\right)$$

$\mathcal{N}_C(\mu, \sigma^2)$       Complex normal distribution with mean  $\mu$  and variance  $\sigma^2/2$

$\mathcal{U}(l, r)$       Uniform distribution with bounds  $l$  and  $r$ :

$$\mathcal{U}(x | l, r) = \begin{cases} \frac{1}{r-l} & l \leq x \leq r \\ 0 & \text{otherwise} \end{cases}$$

## Vectors, Matrices, and Arrays

$x, X, x_n$       Vectors are denoted with bold italic lower-case letters. Matrices, array with  $> 2$  dimensions, and generic arrays with variable numbers of dimensions are denoted with bold italic capital letters. Individual elements of such objects are denoted by italic letters with subscripts denoting their index. E.g. The element located at the second row and third column of a matrix  $Y$  would be denoted  $y_{2,3}$ . In some circumstances where it is more appropriate, indexing begins at 0 rather than 1.

$X^T$       Transpose

$X^\dagger$       Conjugate transpose

$X^{-1}$       Inverse of a square, non-singular matrix

$X^+$       Moore-Penrose pseudo-inverse of a matrix.

$X^{\circlearrowleft(d)}$       Right circular rotation along axis  $d$  of an array by one element. As an example, for a 2D matrix  $X \in \mathbb{F}^{M \times N}$ ,  $X^{\circlearrowleft(1)}$  is given by

$$\begin{bmatrix} x_{M,1} & x_{M,2} & \cdots & x_{M,N} \\ x_{1,1} & x_{1,2} & \cdots & x_{1,N} \\ \vdots & \vdots & \ddots & \vdots \\ x_{M-1,1} & x_{M-1,2} & \cdots & x_{M-1,N} \end{bmatrix},$$

while  $X^{\circlearrowleft(2)}$  is

$$\begin{bmatrix} x_{1,N} & x_{1,1} & \cdots & x_{1,N-1} \\ x_{2,N} & x_{2,1} & \cdots & x_{2,N-1} \\ \vdots & \vdots & \ddots & \vdots \\ x_{M,N} & x_{M,1} & \cdots & x_{M,N-1} \end{bmatrix}.$$

$X^{\leftrightarrow(d)}$  Reversal of elements along axis  $d$  of an array. As an example, for a 2D matrix  $X \in \mathbb{F}^{M \times N}$ ,  $X^{\leftrightarrow(1)}$  is given by

$$\begin{bmatrix} x_{M,1} & x_{M,2} & \cdots & x_{M,N} \\ x_{M-1,1} & x_{M-1,2} & \cdots & x_{M-1,N} \\ \vdots & \vdots & \ddots & \vdots \\ x_{2,1} & x_{2,2} & \cdots & x_{2,N} \\ x_{1,1} & x_{1,2} & \cdots & x_{1,N} \end{bmatrix},$$

$\text{diag}(x)$  Given a vector  $x \in \mathbb{F}^N$ ,  $\text{diag}(x)$  is a matrix  $\in \mathbb{F}^{N \times N}$  of the form

$$\begin{bmatrix} x_1 & 0 & \cdots & 0 \\ 0 & x_2 & \cdots & 0 \\ \vdots & \vdots & \ddots & \vdots \\ 0 & 0 & \cdots & x_N \end{bmatrix}$$

$\langle X, Y \rangle$  Inner product of two arrays with identical shapes. Given  $X$  and  $Y$ , two  $D$ -dimensional arrays  $\in \mathbb{C}^{N_1 \times \cdots \times N_D}$ :

$$\langle X, Y \rangle = \sum_{n_1=1}^{N_1} \cdots \sum_{n_D=1}^{N_D} x_{n_1, \dots, n_D}^* y_{n_1, \dots, n_D}$$

$\|X\|$  Norm, equivalent to  $\sqrt{\langle X, X \rangle}$ .

$x \otimes y$  Outer product of  $x \in \mathbb{F}^M$  and  $y \in \mathbb{F}^N$ , which generates a matrix  $A \in \mathbb{F}^{M \times N}$ , such that

$$a_{m,n} = x_m y_n$$

$x \times y$  Cross product of two vectors  $x \in \mathbb{R}^3$  and  $y \in \mathbb{R}^3$ , given by

$$x \times y = \|x\| \|y\| \sin(\theta) \mathbf{n},$$

where  $\theta$  is the angle between  $x$  and  $y$ , in the plane containing them, and  $\mathbf{n}$  is the

unit vector perpendicular to said plane. N.B. the times symbol is occasionally used to denote scalar multiplication as well.

## Calculus

$\nabla f(\mathbf{x})$  Gradient vector of a differentiable, scalar value function  $f(\mathbf{x}) : \mathbb{R}^N \rightarrow \mathbb{R}$ :

$$\nabla f(\mathbf{x}) = \begin{bmatrix} \frac{\partial f}{\partial x_1} & \frac{\partial f}{\partial x_2} & \dots & \frac{\partial f}{\partial x_N} \end{bmatrix}^T$$

$\nabla^2 f(\mathbf{x})$  Hessian matrix of a twice-differentiable, scalar value function  $f(\mathbf{x}) : \mathbb{R}^N \rightarrow \mathbb{R}$ :

$$\nabla^2 f(\mathbf{x}) = \begin{bmatrix} \frac{\partial^2 f}{\partial x_1^2} & \frac{\partial^2 f}{\partial x_1 \partial x_2} & \dots & \frac{\partial^2 f}{\partial x_1 \partial x_N} \\ \frac{\partial^2 f}{\partial x_2 \partial x_1} & \frac{\partial^2 f}{\partial x_2^2} & \dots & \frac{\partial^2 f}{\partial x_2 \partial x_N} \\ \vdots & \vdots & \ddots & \vdots \\ \frac{\partial^2 f}{\partial x_N \partial x_1} & \frac{\partial^2 f}{\partial x_N \partial x_2} & \dots & \frac{\partial^2 f}{\partial x_N^2} \end{bmatrix}$$

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# Preliminaries

1

This thesis is principally focussed on extracting quantitative information from nuclear magnetic resonance spectroscopy (NMR) data. In this first chapter, concepts are introduced to help contextualise the work undertaken. After a brief introduction to NMR, including key historical developments and a simple description of its theoretical underpinnings, focus turns to the form that NMR data takes. The means by which said data is conventionally processed and analysed to gain chemical insights is discussed. Techniques which estimate the parameters which describe NMR data based on a model of summed complex sinusoids are an alternate means of analysing NMR data. While able to afford richer information than conventional approaches, these are not widely employed in NMR, despite many effective methods existing. A review of some of the most prominent ones are given. Finally, the motivation for the project undertaken is discussed, and an outline of the rest of the thesis is given.

## 1.1 An Introduction to NMR

### 1.1.1 A Brief History

Since its conception almost 80 years ago, NMR has become a ubiquitous technique in chemistry, biochemistry and numerous other disciplines, thanks to the unique insights into the structure and dynamics of chemical species that it can provide. The origins of the subject can be traced back to 1945, when independent work by Felix Bloch on water[1] and Edward Purcell on parrafin[2] gave rise to the first illustrations of nuclear magnetic resonances in condensed phases. The two hadn't met before their respective papers were published with about a month's separation[3]. Both received the Nobel Prize in Physics in 1952 for their pioneering work in the field. A notable mention should also be given to Yevgeny Zavoisky, the father of electron paramagnetic resonance, who probably observed NMR as far back as 1941[4]. Alas, he dismissed his results as irreproducible. In

1949 and 1950, work investigating NMR spectra from compounds containing Cu,  $^{31}\text{P}$ ,  $^{14}\text{N}$ , and  $^{19}\text{F}$  nuclei illustrated the concept of the chemical shift[5–7], in which nuclei in different chemical environments exhibit non-identical resonant frequencies. Chemists regarded these results with great interest, as these findings suggested that NMR could give insights into molecular structure.

Russel Varian secured the first patent for a commercial NMR machine, with a 30 MHz spectrometer following soon after. The first spectrometers functioned by slowly sweeping the magnetic field, causing spins to come into resonance at different times, in a process referred to as continuous wave spectroscopy. Richard Ernst and Weston Anderson, working at Varian Inc. at the time, proposed an alternative method: pulsed Fourier transform (FT) spectroscopy[8]. This was not seen as a fruitful endeavour by the company, largely because of the very long time it took to digitise the signal, and subsequently compute its FT[9]. Instead, the first commercial pulsed FT spectrometer was produced by Bruker Corp. in 1969, which revolutionised NMR. The emergence of the Cooley and Tukey's fast Fourier transform (FFT) algorithm[10] led to vast improvements in the speed with which experiments could be conducted, which incentivised the development of the new pulsed FT approach.

The idea of 2D NMR spectroscopy was proposed by Jean Jeener in 1971[11, 12], which Ernst and co-workers showcased a few years later in the form of a correlation spectroscopy (COSY) experiment[13]. The use of multiple dimensions to spread out signals enabled vastly more complex structures to be studied. In 1985, a report of the first protein assigned by NMR — using COSY and nuclear Overhauser effect spectroscopy (NOESY) experiments — was presented by Kurt Wüthrich and co-workers[14]. Over time, extensive developments in techniques for biomolecular systems have occurred, including the creation of 3D and 4D “triple resonance” experiments[15, 16], as well transverse relaxation optimised spectroscopy (TROSY) experiments[17] for the study of large proteins.

NMR's significance as an analytical tool is evidenced by Nobel Prizes in Chemistry being awarded for work in the field on two separate occasions. First, Ernst received the prize in 1991 “for his contributions to the development of the methodology of high resolution nuclear magnetic resonance spectroscopy”[18]. In 2002, Wüthrich was recognised “for his development of nuclear magnetic resonance spectroscopy for determining the three-dimensional structure of biological macromolecules in solution”[19].

### 1.1.2 The Bloch model of NMR

**Remark 1.** *In most of this work, vectors are expressed as lower-case bold letters and matrices/multidimensional arrays are expressed as upper-case bold letters. In this section however, notation frequently encountered in the literature is used; certain vector quantities are denoted with upper-case letters.*

NMR relies on an intrinsic property of certain nuclei called *spin* which, along with orbital angular momentum, is one of the two sources of angular momentum in quantum mechanics. The angular momentum associated with a nuclear spin is characterised by the quantum number  $I \in \{0, 1/2, 1, 3/2, \dots\}$ . Spin- $1/2$  nuclei are the most commonly studied in NMR, as those with  $I > 1/2$  often have very short-lived excited states, due to electric quadrupole effects. A rigorous description of NMR requires the application of quantum mechanics, with many excellent texts devoted to the subject[20–22]. However, a basic appreciation can be gained using the *Bloch model*, a semi-classical description of the simplest of possible system to study: a ensemble of isolated, identical spin- $1/2$  nuclei[23: Chapter 1]. The Bloch model becomes inadequate when more complex spin systems are considered, featuring non-identical spins which interact through mechanisms such as scalar ( $J$ ) couplings. However, it provides valuable insights into the basic principles of NMR, including the form that a typical dataset acquired by an experiment takes.

The nuclear spin angular momentum  $\mathbf{I} \in \mathbb{R}^3$  is a vector with squared magnitude

$$\mathbf{I}^2 = \mathbf{I} \cdot \mathbf{I} = \hbar I(I+1), \quad (1.1)$$

where  $\hbar = h/2\pi$  is the reduced Planck constant. While it is not possible to specify multiple components of the angular momentum simultaneously due to the uncertainty principle, it is possible to specify one of these along with  $\mathbf{I}^2$ . Conventionally, this is chosen to be the  $z$ -component, for which

$$I_z = \hbar m, \quad (1.2)$$

with  $m \in \{-I, -I+1, \dots, I-1, I\}$ . Equation 1.2 implies that the magnitude of the  $z$ -component may only adopt certain discrete values (i.e. it is quantised). A nucleus with non-zero spin has an associated *magnetic moment*, given by:

$$\boldsymbol{\mu} = \gamma \mathbf{I} \implies \mu_z = \gamma I_z = \gamma \hbar m. \quad (1.3)$$

$\gamma \in \mathbb{R}$  is a proportionality constant called the *gyromagnetic ratio*, which is dependent on the nucleus of interest. Table 1.1 provides the gyromagnetic ratios for some low-mass nuclei commonly encountered in NMR, along with some which are spin-0 and therefore “invisible” in the context of NMR. Sadly the most abundant isotopes of two of the most prominent atoms in organic chemistry fall into this category.

Without the presence of an external magnetic field, the nuclear spin states of different  $m$  are degenerate. However, when subjected to such a field, the *Zeeman effect* is observed, in which the relative energies of the different states diverge. The energy of a given magnetic moment relative to

Nucleus	$I$	$\gamma (\text{rad T}^{-1} \text{s}^{-1})$	Relative Abundance (%)
$^1\text{H}$	$1/2$	$2.6752 \times 10^8$	99.9885
$^2\text{H}$	1	$4.1066 \times 10^7$	0.0115
$^6\text{Li}$	1	$3.9371 \times 10^7$	7.59
$^7\text{Li}$	$3/2$	$1.0398 \times 10^8$	92.41
$^{12}\text{C}$	0	-	98.93
$^{13}\text{C}$	$1/2$	$6.7283 \times 10^7$	1.07
$^{14}\text{N}$	1	$1.9338 \times 10^7$	99.636
$^{15}\text{N}$	$1/2$	$-2.7126 \times 10^7$	0.364
$^{16}\text{O}$	0	-	99.756
$^{17}\text{O}$	$5/2$	$-3.6281 \times 10^7$	0.038
$^{19}\text{F}$	$1/2$	$2.5162 \times 10^8$	100
$^{31}\text{P}$	$1/2$	$1.0839 \times 10^8$	100

**Table 1.1:** A table of regularly encountered nuclei in NMR, along with common nuclei which are not NMR active.

its zero-field energy is given by

$$E = -\boldsymbol{\mu} \cdot \mathbf{B}_0, \quad (1.4)$$

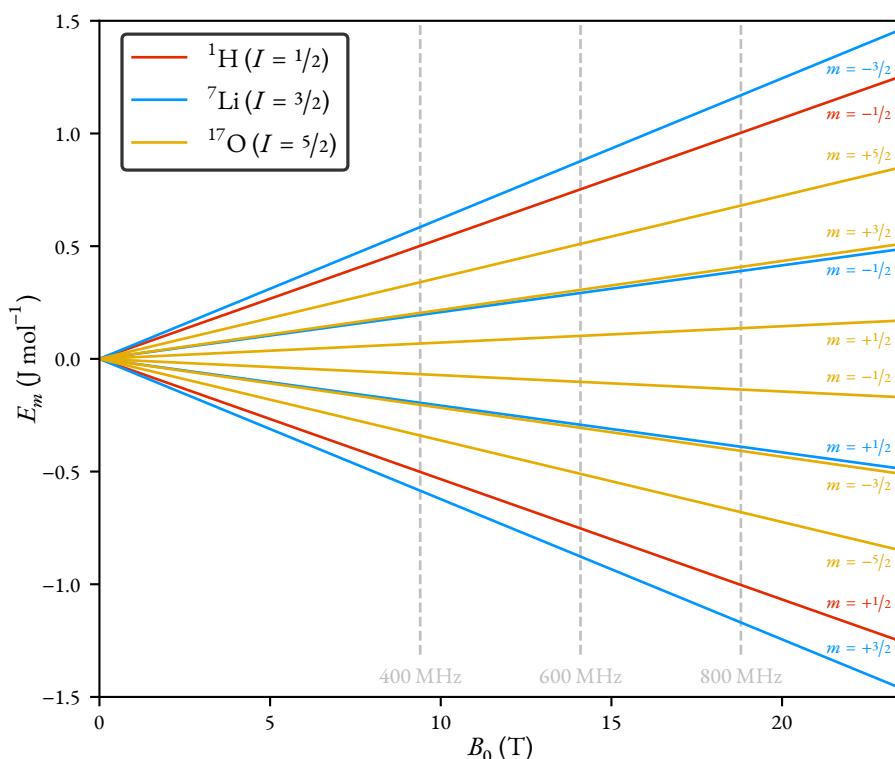
where  $\mathbf{B}_0 \in \mathbb{R}^3$  is the magnetic field vector. In NMR it is conventional to define the external field as directed along the laboratory  $z$ -axis, such that  $B_{0,x} = B_{0,y} = 0$  and  $B_{0,z} = B_0$  where  $B_0$  is the magnetic field strength. The energies of the individual spin states are therefore (Figure 1.1)

$$E_m = -\gamma I_z B_0 = -m\hbar\gamma B_0. \quad (1.5)$$

NMR samples comprise a vast ensemble of equivalent spin systems, and it is the macroscopic properties of the sample that are observed. At thermal equilibrium, the various spin states will be disproportionately populated in accordance with the Boltzmann distribution, with lower energy states being more heavily populated. For example, an ensemble of non-interacting spin- $1/2$  nuclei with  $\gamma > 0$  will have a more populated  $m = +1/2$  ( $\alpha$ ) state, relative to the  $m = -1/2$  ( $\beta$ ) state. Due to the very small relative energy difference however, it should be noted that the discrepancy in state populations is very small. The ensemble acquires a net (bulk) magnetic moment  $\mathbf{M}$ , given by the sum of all the individual spin moments:

$$\mathbf{M} = \sum_{s=1}^S \boldsymbol{\mu}_s, \quad (1.6)$$

where  $S \gg 1$  is the number of spins in the ensemble. At equilibrium, the  $x$ - and  $y$ -components of



**Figure 1.1:** The variation of energy of the spin states of  $^1\text{H}$ ,  $^7\text{Li}$ , and  $^{17}\text{O}$  with external magnetic field strength ( $B_0$ ), up to 23.5 T, which is approximately the strength of a 1 GHz NMR magnet. Three common field strengths for commercial NMR magnets are indicated: 9.40 T (400 MHz), 14.10 T (600 MHz), and 18.79 T (800 MHz).

the bulk magnetisation are zero, i.e.

$$\sum_{s=1}^S \mu_{x,s} = \sum_{s=1}^S \mu_{y,s} = 0. \quad (1.7)$$

Therefore, the bulk magnetisation is collinear with the field direction, with a magnitude  $M_0$ , which is approximately given by[22: Section 1.1].

$$M_0 \approx \frac{S\gamma^2\hbar^2B_0I(I+1)}{3k_B T}, \quad (1.8)$$

where  $k_B$  is the Boltzmann constant, and  $T$  is the sample temperature. To maximise experiment sensitivity, it is desirable to utilise nuclei with high natural abundance (affecting  $S$ ), and high gyro-magnetic ratio. Along with other favourable attributes such as its ubiquity in organic molecules,  $^1\text{H}$  is therefore by far the most popular nucleus to study using NMR, at least in solution-state contexts.

The bulk magnetism experiences a torque induced by the magnetic field, with its of rate of change with respect to time being

$$\frac{d\mathbf{M}(t)}{dt} = \mathbf{M}(t) \times \gamma \mathbf{B}(t). \quad (1.9)$$

The essence of NMR is to manipulate and subsequently detect the evolution of  $\mathbf{M}$ . Manipulation is achieved by applying short bursts of radio-frequency (RF) radiation known as *pulses* which perturb the net magnetic field away from  $\mathbf{B}_0$ . The contribution to the field induced by pulses is commonly denoted  $\mathbf{B}_1$ , such that at any given time

$$\mathbf{B}(t) = \mathbf{B}_0 + \mathbf{B}_1(t). \quad (1.10)$$

Whenever the magnetisation vector is not collinear with the field vector\*, it undergoes *precession* about the field vector. Free precession occurs when the magnetisation is aligned away from the  $z$ -axis, and  $\mathbf{B}_1 = \mathbf{0}$ , such that

$$\frac{d\mathbf{M}(t)}{dt} = -\gamma B_0 [M_y \ -M_x \ 0]^T. \quad (1.11)$$

Under free precession, the magnetisation precesses around the  $z$ -axis at the *Larmor frequency*  $\omega_0 = -\gamma B_0$ .<sup>†</sup>

\*The cross product of two collinear vectors is 0, so  $\mathbf{M}$  remains fixed when it is aligned with  $\mathbf{B}$ , as is the case at equilibrium.

<sup>†</sup>While the SI base unit of magnetic field strength is the Tesla (T), when referring to the field strength that a spectrometer operates at, it is common to use MHz instead. This refers to the Larmor frequency of a reference  $^1\text{H}$  nucleus at the given field strength. For example, a 500 MHz spectrometer operates at a field strength of  $5 \times 10^8 \text{ Hz} / 4.2577 \times 10^7 \text{ T}^{-1} \text{ Hz} \approx 11.74 \text{ T}$ .

Assuming the RF field is linearly polarised along the  $x$ -axis, it can be written to a high degree of accuracy as

$$\mathbf{B}_1(t) = B_1 (\cos(\omega_{\text{RF}}t + \phi_{\text{RF}})\mathbf{i} + \sin(\omega_{\text{RF}}t + \phi_{\text{RF}})\mathbf{j}), \quad (1.12)$$

with  $\mathbf{i}$ ,  $\mathbf{j}$  and  $\mathbf{k}$  (encountered shortly) being unit vectors along the  $x$ -,  $y$ -, and  $z$ -axes, respectively.  $B_1$  is the strength of the RF field,  $\omega_{\text{RF}}$  is its angular frequency, and  $\phi_{\text{RF}}$  is its phase. A great simplification to the model is realised by considering a frame of reference which, rather than being static, rotates at  $\omega_{\text{RF}}$ , as this makes the RF field appear to be time-independent. This is referred to as the *rotating frame*, and leads to Equation 1.9 being recast as

$$\frac{d\tilde{\mathbf{M}}(t)}{dt} = \tilde{\mathbf{M}}(t) \times \gamma \tilde{\mathbf{B}}(t), \quad (1.13a)$$

$$\tilde{\mathbf{B}} = B_1 \cos(\phi_{\text{RF}})\tilde{\mathbf{i}} + B_1 \sin(\phi_{\text{RF}})\tilde{\mathbf{j}} + \Delta B_0 \tilde{\mathbf{k}}, \quad (1.13b)$$

$$\Delta B_0 = -\frac{\Omega}{\gamma}, \quad (1.13c)$$

$$\Omega = -\gamma B_0 - \omega_{\text{RF}}, \quad (1.13d)$$

$$\tilde{\mathbf{i}} = \cos(\omega_{\text{RF}})\mathbf{i}, \quad (1.13e)$$

$$\tilde{\mathbf{j}} = \sin(\omega_{\text{RF}})\mathbf{j}, \quad (1.13f)$$

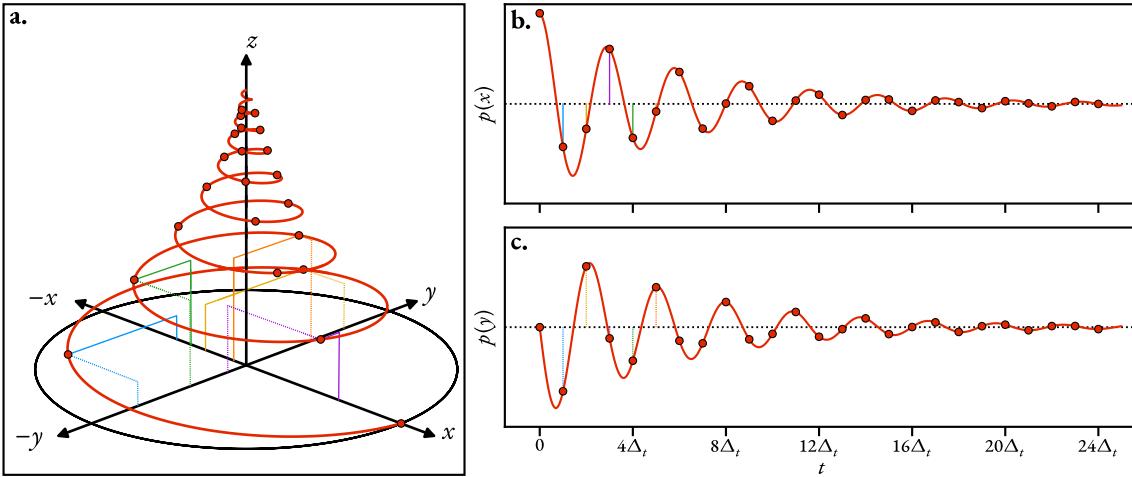
$$\tilde{\mathbf{k}} = \mathbf{k}. \quad (1.13g)$$

$\Omega = \omega_0 - \omega_{\text{RF}}$  is the *offset* of the spin magnetisation. When  $\Omega = 0 \text{ rad s}^{-1}$ , the system is said to be on-resonance, and at times when an RF field is not being applied, the magnetisation vector appears to be static in the rotating frame.

Consider a scenario where a short RF pulse is applied to the system, which is then allowed to undergo free precession. Equation 1.13 implies that  $\tilde{\mathbf{M}}$  will rotate indefinitely about the  $z$ -axis with a frequency of  $\Omega$ . However, in reality the system is driven to re-establish its thermal equilibrium state,  $\mathbf{M}_{\text{eq}} \equiv \tilde{\mathbf{M}}_{\text{eq}} = [0, 0, M_0]^T$ . In the Bloch model, two processes are introduced to account for this<sup>‡</sup>. *Longitudinal* (spin-lattice) relaxation is responsible for the recovery of the spin states to their equilibrium populations, according to the Boltzmann distribution. A reversion of the  $z$ -component of the magnetisation to  $M_0$  accompanies this. *Transverse* (spin-spin) relaxation leads to the  $x$ - and  $y$ -components of the bulk magnetisation decaying to 0. These phenomena commonly exhibit exponential evolution profiles, and are assigned rates  $R_1$  and  $R_2$ , respectively. The corresponding times (inverse rates) are often considered instead:  $T_1 := 1/R_1$ ,  $T_2 := 1/R_2$ .

Everything has now been established to state the Bloch equations, which describe the evolution of

<sup>‡</sup>The introduction of relaxation is phenomenological in the Bloch model; the reversion of the spin system to equilibrium is included purely to ensure the model agrees with observation. More sophisticated theories invoking Liouville-space quantum mechanics can account for relaxation[24, 25].



**Figure 1.2:** **a.** An illustration of the free evolution of the bulk magnetisation of an ensemble of spin- $1/2$  nuclei immediately after the application of a  $90^\circ_y$  pulse according to the Bloch model. The projections of the magnetisation vector onto the  $x$ - and  $y$ -axes are plotted in panels **b.** and **c.**, respectively. Modern NMR spectrometers utilise quadrature detection, such that the  $x$ - and  $y$ -projections of the time-varying magnetisation are sampled at regular time intervals, separated by  $\Delta_t$ . The resulting FID is given by the complex value  $p(x) + ip(y)$ .

the bulk magnetisation of an ensemble of identical spin- $1/2$  nuclei in the rotating frame:

$$\frac{d\tilde{\mathbf{M}}(t)}{dt} = \begin{bmatrix} -R_2 & -\Omega & -\gamma B_1 \sin(\phi_{RF}) \\ \Omega & -R_2 & \gamma B_1 \cos(\phi_{RF}) \\ \gamma B_1 \sin(\phi_{RF}) & -\gamma B_1 \cos(\phi_{RF}) & -R_1 \end{bmatrix} \tilde{\mathbf{M}}(t) + R_1 M_0 \begin{bmatrix} 0 \\ 0 \\ 1 \end{bmatrix}, \quad (1.14)$$

Panel a of Figure 1.2 depicts the evolution of an off-resonance ( $\Omega \neq 0 \text{ rad s}^{-1}$ ) magnetisation vector after the application of an RF pulse with  $\phi_{RF} = \pi/2$ , and an appropriate combination of duration and power to induce a clockwise rotation of  $90^\circ$  about the  $y$ -axis; such a pulse is denoted  $90^\circ_y$ . Assuming that negligible evolution due to the offset occurs during the pulse, the magnetisation vector will land on the  $x$ -axis, and evolve according to

$$\tilde{M}_x(t) = M_0 \cos(\Omega t) \exp(-R_2 t), \quad (1.15a)$$

$$\tilde{M}_y(t) = M_0 \sin(\Omega t) \exp(-R_2 t), \quad (1.15b)$$

$$\tilde{M}_z(t) = M_0 (1 - \exp(-R_1 t)). \quad (1.15c)$$

During acquisition, the transverse components of the bulk magnetisation are detected by the spectrometer probe circuitry, such that the resulting signal, called the *free induction decay* (FID), is given by

$$y(t) = c\tilde{M}_+(t), \quad (1.16a)$$

$$\tilde{M}_+(t) = \tilde{M}_x(t) + i\tilde{M}_y(t) = M_0 \exp(i\Omega t - R_2 t), \quad (1.16b)$$

with  $c \in \mathbb{R}_{>0}$  being a proportionality constant.

### 1.1.3 The NMR Spectrometer

Modern NMR spectrometers are capable of conducting a plethora of experiments which can aide chemists. In essence, a spectrometer comprises a high-field magnet, a probe, components which are used to transmit RF pulses to the probe, and components which are used to process the resulting signal from the probe. A brief summary of these is now given.

#### The Magnet

The static  $B_0$  field is generated by a magnet, composed of a superconducting solenoid immersed in liquid helium. Common materials used for the solenoid include Nb-Ti alloy and Nb<sub>3</sub>Sn. To minimise the extent of helium evaporation, the dewar containing the helium is lined with a thermal radiation shield. The helium dewar is then surrounded by a larger dewar containing liquid nitrogen. A bore passes through the  $z$ -direction of the magnet, which is maintained at a user-controlled temperature. Within the bore sits the probe as well as the sample. Magnets with high field strengths are desirable, as both the resolution ( $\propto B_0$ ) and sensitivity ( $\propto B_0^{3/2}$ ) of the data are affected. At the time of writing, commercial spectrometers which operate at and above a <sup>1</sup>H Larmor frequency of 1 GHz (23.5 T) exist, though these are uncommon and are employed primarily for the study of large biomolecules. For most applications, including the study of small molecules, spectrometers with more modest field strengths are typically adequate.

To maintain high spatial field homogeneity (a necessity for data with acceptable resolution) a series of coils called *shims* surround the sample. Each coil produces a weak magnetic field with a specific spatial profile in accordance with a spherical harmonic function. A collection of shim coils can cancel out any inhomogeneity inherent to the main magnet.

A field-frequency lock is used to ensure the stability of the field. The lock is effectively a small NMR spectrometer, tuned to a specified isotope (typically <sup>2</sup>H<sup>\$</sup>), which monitors the resonance frequency of the isotope over time. If the frequency begins to drift, implying that the field strength is changing, the current in the “ $Z_0$  coil” is adjusted to ensure a consistent field strength is maintained.

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<sup>\$</sup><sup>2</sup>H-enriched solvents are routinely used to make up NMR samples. In <sup>1</sup>H NMR experiments, this ensures that an extremely intense signal due to the solvent does not dwarf the signals from other spins in the sample. This makes <sup>2</sup>H a suitable nucleus to monitor by the lock, as it is ubiquitous, but rarely directly studied.

## The Probe

The probe sits inside the bore of the magnet, and features the coils used to pulse the sample with RF radiation. The same coils also receive the response from the sample. The principle source of noise in NMR experiments is thermal noise within the probe circuitry. For this reason, cryogenic probes[26] have become a prominent development, in which the coils and other probe electronics are maintained at a very low temperature (typically about 20 K).

## The Transmitter

The transmitter is responsible for the generation of RF pulses with specified power, timing and phase. A synthesiser acts as an RF source, producing a continuous carrier wave at or very close to the Larmor frequency of the target nucleus. This frequency ( $\omega_{RF}$ ) can be adjusted in order to determine the center of the spectrum. The difference between the carrier frequency and the reference “basic frequency” of the spectrometer is referred to as the *transmitter offset*  $f_{\text{off}}$ . The output of the synthesiser is gated to ensure pulses are applied at the desired times. Attenuators/amplifiers then adjust the power of the pulse, which travels to the probe.

## The Receiver

During acquisition, the time-varying current induced in the probe coil by the sample magnetisation is sent to a receiver, comprising a series of components designed to convert the analogue current to the digital FID which is stored in computer memory. One of the processes that the receiver is responsible for is *quadrature detection*[27: Section 13.6]. Quadrature detection ensures FIDs are frequency discriminated, i.e. that they possess the requisite information to determine whether a given signal in FID has a frequency that is above or below the transmitter frequency, which sits in the middle of the spectral window. This is achieved by splitting the signal from the probe into two channels. In each channel, the signal, which is of a very high frequency (MHz), is mixed with a reference signal of frequency  $\omega_{RF}$ . The mixing process results in a low-frequency (kHz) signal being generated, along with a very high frequency signal. The reference signal in one channel possesses a phase which is shifted by  $90^\circ$  relative to the other, such that the combined signal constitutes a quadrature pair. Both signals are then sent through a low-pass filter to remove the high frequency component produced through mixing. Finally, an analogue to digital converter translates the signal to the real and imaginary components of a binary dataset which is stored in memory.

### 1.1.4 The structure of the FID

The result of running an NMR experiment is an FID  $\mathbf{y} \in \mathbb{C}^N$  which is sampled at equally spaced points in time, with consecutive samples separated by time  $\Delta_t$ :

$$\begin{aligned}\mathbf{y} &= [y_0 \quad y_1 \quad y_2 \quad \cdots \quad y_{N-1}]^T \\ &\equiv [y(t=0) \quad y(t=\Delta_t) \quad y(t=2\Delta_t) \quad \cdots \quad y(t=(N-1)\Delta_t)]^T,\end{aligned}\tag{1.17}$$

where  $y(t)$  is the (continuous) variation of the generated signal with time, and  $N$  is the number of points sampled. The inverse of the sampling rate,  $1/\Delta_t$ , is the *sweep width*  $f_{\text{sw}}$  which defines how wide the range of samplable frequencies is, in accordance with the Nyquist theorem[28].

FIDs adopt the form of a summation of  $M \in \mathbb{N}$  complex exponentials (signals). Each signal will be subjected to damping due to transverse relaxation, which is typically exponential in nature. An FID therefore takes the form<sup>¶</sup>

$$y_n = x_n(\theta) + w_n \quad \forall n \in \{0, 1, \dots, N-1\},\tag{1.18a}$$

$$x_n(\theta) = \sum_{m=1}^M a_m \exp(i\phi_m) \exp((2\pi i(f_m - f_{\text{off}}) - \eta_m)n\Delta_t).\tag{1.18b}$$

Equation 1.18 indicates that an FID comprises contributions from the (deterministic) evolution of the spin magnetisation  $\mathbf{x}$  and experimental noise  $\mathbf{w}$  (*vide infra*). Each signal which contributes to  $\mathbf{x}$  is defined by four parameters:

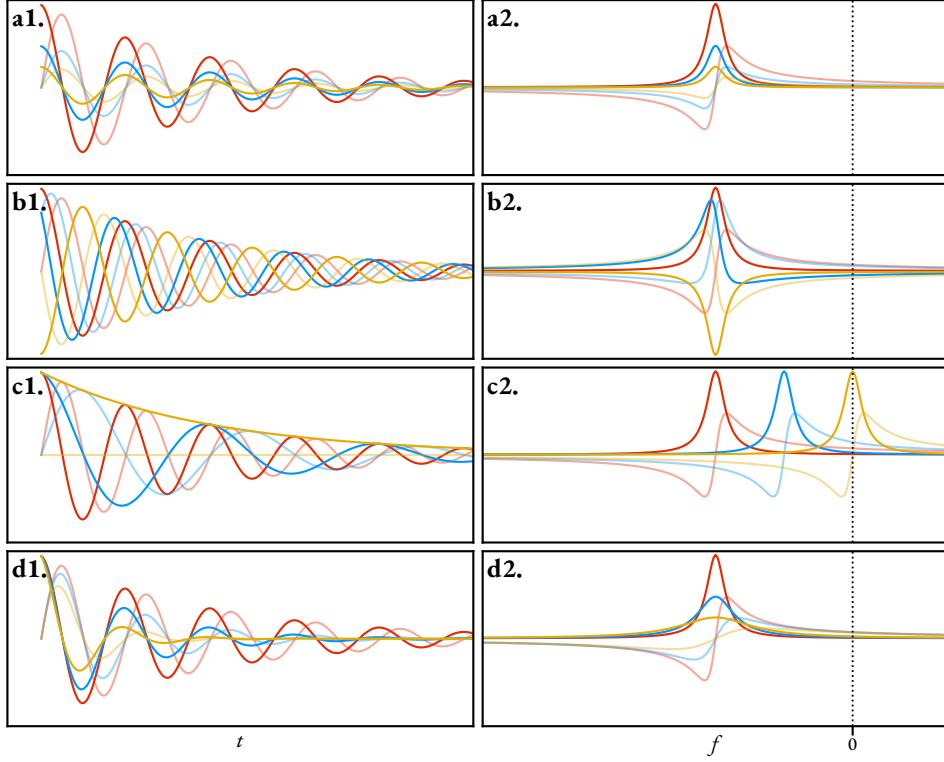
- Amplitude  $a \in \mathbb{R}_{>0}$ ,
- Phase  $\phi \in (-\pi, \pi]$  (rad),
- Frequency  $f \in [f_{\text{off}} - 1/2f_{\text{sw}}, f_{\text{off}} + 1/2f_{\text{sw}}]$  (Hz),
- Damping factor  $\eta \in \mathbb{R}_{>0}$  ( $s^{-1}$ ).

An FID can therefore be parameterised by the vector  $\theta \in \mathbb{R}^{4M}$ :

$$\theta = [\mathbf{a}^T \quad \boldsymbol{\phi}^T \quad \mathbf{f}^T \quad \boldsymbol{\eta}^T]^T,\tag{1.19}$$

where  $\mathbf{a} \in \mathbb{R}^M = [a_1 \ a_2 \ \cdots \ a_M]^T$  is a vector of all amplitudes,  $\boldsymbol{\phi} \in \mathbb{R}^M$  is a vector of all phases, etc. An alternative, more concise, notation for Equation 2.1b involves the *complex amplitudes*

<sup>¶</sup>This provides an idealised model of an FID, based on the underlying theory of the experiment. In reality, there is the possibility of significant deviations from this model being realised. One potential cause of this is the influence of magnetic field inhomogeneities, which will cause spectral peaks to deviate from an idealised Lorentzian lineshape (Section 1.2.1). In cases where distortions to the data have occurred, techniques such as *reference deconvolution*[29] can be used as a corrective measure in a bid to make the data agree more closely with this model.



**Figure 1.3:** An illustration of the influence of the four parameters associated with a signal in both the time-domain (panels **a1.** – **d1.**) and Fourier-domain (panels **a2.** – **d2.**). The red signal is generated with the same parameters across all panels:  $\alpha = \alpha_{\text{red}}$ ,  $\phi = 0$  rad,  $f = f_{\text{red}}$ ,  $\eta = \eta_{\text{red}}$ . The blue and yellow signals were produced by altering one parameter out of the four. **a.**  $\alpha_{\text{yellow}} = 1/2\alpha_{\text{blue}} = 1/4\alpha_{\text{red}}$ . **b.**  $\phi_{\text{blue}} = \pi/4$  rad,  $\phi_{\text{yellow}} = \pi$  rad. **c.**  $f_{\text{blue}} = 1/2f_{\text{red}}$ ,  $f_{\text{yellow}} = 0$ . **d.**  $\eta_{\text{yellow}} = 1/2\eta_{\text{blue}} = 1/4\eta_{\text{red}}$ . The real and imaginary components of each signal are plotted, with the imaginary component being paler than its real counterpart.

and *signal poles* associated with the FID:

$$x_n(\theta) = \sum_{m=1}^M \alpha_m z_m^n, \quad (1.20\text{a})$$

$$\alpha_m = \alpha_m \exp(i\phi_m), \quad (1.20\text{b})$$

$$z_m = \exp((2\pi i (f_m - f_{\text{off}}) - \eta_m) \Delta_t). \quad (1.20\text{c})$$

The respective influences of the four parameters on a time-domain signal are depicted in panels a1 to d1 in Figure 1.3.

Multidimensional experiments involve incrementing one or more delay within the pulse sequence, in order to obtain an array of one-dimensional (1D) FIDs. In a  $D$ -dimensional dataset, each contributing signal is parameterised by an amplitude and phase as before, along with  $D$  distinct fre-

quencies and damping factors, such that a general parameter vector  $\theta \in \mathbb{R}^{2(1+D)M}$  is given by

$$\theta = \begin{bmatrix} \alpha^T & \phi^T & f^{(1)T} & \dots & f^{(D)T} & \eta^{(1)T} & \dots & \eta^{(D)T} \end{bmatrix}^T, \quad (1.21)$$

where  $f^{(D)}$  and  $\eta^{(D)}$  are the frequencies and damping factors in the actively acquired (direct) dimension, and  $\{f^{(1)}, \dots, f^{(D-1)}\}$  and  $\{\eta^{(1)}, \dots, \eta^{(D-1)}\}$  are those for the indirect dimension(s). Indirect dimensions can exhibit different forms of evolution, depending on the precise nature of the pulse sequence. Two common functional forms exist[22: Section 4.3.4]. Signals of the form  $\cos(2\pi ft)$  and  $\sin(2\pi ft)$  modulate the amplitude of the direct dimension signal across increments, while those of the form  $\exp(2\pi ift)$  and  $\exp(-2\pi ift)$  modulate the phase instead. For experiments which produce amplitude-modulated FIDs, it is desirable to generate both the cosine and sine forms, as this enables spectra with desirable properties to be generated. The same is true for the “positive” and “negative” forms when phase-modulated FIDs are acquired (*vide infra*). In general, a  $D$ -dimensional FID  $Y \in \mathbb{C}^{N^{(1)} \times \dots \times N^{(D)}}$  can be expressed as

$$y_{n^{(1)}, \dots, n^{(D)}} = x_{n^{(1)}, \dots, n^{(D)}}(\theta) + w_{n^{(1)}, \dots, n^{(D)}}, \quad (1.22a)$$

$$x_{n^{(1)}, \dots, n^{(D)}} = \sum_{m=1}^M a_m \exp(i\phi_m) \prod_{d=1}^D \zeta^{(d)} \left( 2\pi \left( f_m^{(d)} - f_{\text{off}}^{(d)} \right) n^{(d)} \Delta_t^{(d)} \right) \exp \left( -\eta_m^{(d)} n^{(d)} \Delta_t^{(d)} \right), \quad (1.22b)$$

$$\zeta^{(d)}(\cdot) \begin{cases} = \exp(i\cdot) & d = D \\ \in \{\cos(\cdot), \sin(\cdot), \exp(i\cdot) \exp(-i\cdot)\} & \text{otherwise} \end{cases}, \quad (1.22c)$$

It is typical to assume that the data is corrupted by an array of additive white Gaussian noise (AWGN), i.e. the noise instances are described by a complex normal distribution with mean 0, and pairs of noise instances are statistically independent, regardless of their time separation:

$$w_{n^{(1)}, \dots, n^{(D)}} \sim \mathcal{N}_C(0, 2\sigma^2) \quad (1.23a)$$

$$\begin{aligned} \implies \Re(w_{n^{(1)}, \dots, n^{(D)}}) &\perp\!\!\!\perp \Im(w_{n^{(1)}, \dots, n^{(D)}}), \\ \Re(w_{n^{(1)}, \dots, n^{(D)}}) &\sim \mathcal{N}(0, \sigma^2), \\ \Im(w_{n^{(1)}, \dots, n^{(D)}}) &\sim \mathcal{N}(0, \sigma^2). \end{aligned} \quad (1.23b)$$

The extent by which a signal is corrupted by noise is given by the signal-to-noise ratio (SNR), the

ratio of signal power and noise power:

$$\text{SNR}(\mathbf{Y}) := \frac{1}{2\mathfrak{N}\sigma^2} \sum_{n^{(1)}=0}^{N^{(1)}-1} \cdots \sum_{n^{(D)}=0}^{N^{(D)}-1} \left| \mathbf{x}_{n^{(1)}, \dots, n^{(D)}} \right|^2, \quad (1.24)$$

where  $\mathfrak{N} := N^{(1)} \times \cdots \times N^{(D)}$  is the total number of points the signal comprises. Due to the large dynamic range of the SNR across datasets, it is common to express it using a logarithmic scale instead, in units of decibels (dB):

$$\text{SNR}_{\text{dB}} := 10 \log_{10} (\text{SNR}). \quad (1.25)$$

## 1.2 NMR Data Processing and Analysis

**Remark 2.** In contexts where 1D datasets are considered specifically, the redundant dimension index  $^{(1)}$  will be neglected for conciseness.

### 1.2.1 Conventional NMR Processing

The typical means of processing NMR data is to transform the time (measured) domain FID into the frequency domain, yielding an NMR spectrum. This is achieved through application of the FT. The FT converts a continuous function over time  $t$ , to one over frequency  $F$  as follows<sup>||</sup>:

$$s(F) = \int_0^\infty x(t) \exp(-2\pi i t F) dt \quad (1.26)$$

In practice, the discrete signal acquired by the spectrometer is processed using the discrete Fourier transform (DFT):

$$s_n = \sum_{k=0}^{N-1} x_k \exp\left(-\frac{2\pi i k n}{N}\right) \quad \forall n \in \{0, \dots, N-1\}. \quad (1.27)$$

The FT of a continuous exponentially-damped complex sinusoid takes the form of a *Lorentzian*:

$$s(F) = \int_0^\infty a \exp(i\phi) \exp((2\pi i f - \gamma)t) \exp(-2\pi i t F) dt, \quad (1.28a)$$

$$s(F) = \frac{a \exp(i\phi)}{\gamma + 2\pi i(f - F)}. \quad (1.28b)$$

When processing discrete data, the DFT of an FID features a vertical offset, such that the baseline does not sit at 0[30]. This results from only possessing data for positive values of  $t$ , rather than

<sup>||</sup>In general, the FT is defined over the range  $(-\infty, \infty)$ . Since NMR data isn't defined for  $t < 0$ , the FT has been defined over the range  $[0, \infty)$ .

having a “full echo”, where negative values of  $t$  are accounted for too. Fortunately, this can be corrected easily by halving the initial point of the FID prior to DFT. The FT is a linear function, such that the FT of a summation of signals is equivalent to the summation of all signals’ FTs. A corollary is that an NMR spectrum comprises a series of Lorentzian “peaks”, located at the frequencies of the signals in the FID:

$$s(F) = \sum_{m=1}^M \frac{\alpha_m \exp(i\phi_m)}{\eta_m + 2\pi i(f_m - F)}. \quad (1.29)$$

The FT is a very attractive means of processing NMR data, as it presents the data in a format which is human-interpretable; the basic rules describing how chemical structure is mapped to NMR spectra is a fundamental skill that experimentalists in many fields require[31]. Due to innate properties of the NMR experiment, as well as issues arising from analysing discrete signals, the FT of the raw FID has undesirable characteristics without further manipulation. Additional processing steps that are frequently applied to NMR data are now outlined, in the order that they are usually employed. Note that apodisation and zero filling are applied prior to FT (i.e. to the FID), while phase correction and baseline correction are applied after FT (i.e. to the resulting spectrum).

### **Apodisation**

Apodisation refers to the process of mutating a signal by multiplying it with a specified function, often called a *window function*[32: Section 3.2.7], in order to enhance either the sensitivity or the resolution of the final spectrum, albeit at the cost of worsening the other feature.

*Sensitivity Enhancement* As an FID progresses with time, the contributions from the desirable signal ( $x$ ) and experimental noise ( $w$ ) becomes more weighted towards the noise, as spin relaxation phenomena attenuate the signal. Multiplying the FID with a function which decreases with time can be used to enhance the SNR of the FID. The most common function to achieve this is the negative exponential, in which a given point is multiplied by  $\exp(-kn/N-1)$ .  $k$  is referred to as the line broadening factor, since the increased dampening applied to the signal causes the linewidth of the spectral peaks to increase (see panel d of Figure 1.3).

*Resolution Enhancement* By contrast, resolution enhancement can be achieved by applying a window function that artificially reduces the rate of signal decay. This is achievable through the attention of points that are early in the FID. Popular examples of window functions for resolution enhancement are the Lorentz-Gauss function, which bestow a sharper, Gaussian shape to the peaks, and the sine-bell, which is commonly used in multidimensional experiments. Since the initial points in the FID are reduced in magnitude, these window functions decrease the sensitivity

of the resulting spectra.

By being defined to decay to a sufficiently small value (or 0 itself) at the end of the FID, window functions are also able to suppress *truncation artefacts*, which appear when the FID still possesses appreciable signal amplitude at the end of the acquisition period. Truncated FIDs produce spectra with peaks of a form that is akin to the convolution of the FT of the untruncated FID, with the FT of a box-function, taking the form of a sinc function ( $\frac{\sin(x)}{x}$ ). The resulting artefacts in spectra are often referred to as *sinc wiggles* for this reason.

### Zero-filling

Zero-filling refers to the process of appending zeros to the end of an FID. One reason why this is often done is to ensure that the number of points in the FID is a power of 2, making the FID of an optimal size for processing by divide and conquer methods like the Cooley-Tukey algorithm[10]. Beyond this, it is actually possible to enhance the information content of the real component of the spectrum if an FID comprising  $2^{x-1} < N \leq 2^x$  points is zero-filled to  $2^{x+1}$  points[33]. By doing this, the real and imaginary components of the spectrum become causally linked; the real component can be derived from the imaginary component and vice versa according to the Kramers-Kronig relations via the Hilbert transform. Zero-filling beyond a factor of 2 can bestow a cosmetic improvement to spectra, but it does not incorporate any new information into them: any additional points are simply interpolations.

### Phase correction

The real and imaginary components of Equation 1.29 are as follows:

$$\Re(s(F)) = \sum_m a_m (\cos(\phi_m) \mathcal{A}_m(F) + \sin(\phi_m) \mathcal{D}_m(F)), \quad (1.30a)$$

$$\Im(s(F)) = \sum_m a_m (\sin(\phi_m) \mathcal{A}_m(F) - \cos(\phi_m) \mathcal{D}_m(F)), \quad (1.30b)$$

where  $\mathcal{A}_m$  and  $\mathcal{D}_m$  denote *absorption* and *dispersion* Lorentzians, respectively:

$$\mathcal{A}_m(F) = \frac{\eta_m}{\eta_m^2 + 4\pi^2(f_m - F)^2}, \quad (1.31a)$$

$$\mathcal{D}_m(F) = \frac{2\pi(f_m - F)}{\eta_m^2 + 4\pi^2(f_m - F)^2}. \quad (1.31b)$$

As illustrated most clearly in panel c2 of Figure 1.3, a peak with an absorption lineshape is far more desirable than one with a dispersion lineshape for two key reasons:

1. Its maximum corresponds to the signal frequency, while a dispersion Lorentzian has a mag-

nitude of 0 at this frequency.

2. It decays more rapidly and therefore exhibits better resolution; at large frequency offsets, absorption Lorentzians decay at a rate  $\propto 1/(f_m - F)^2$ , while dispersive Lorentzians decay at a rate  $\propto 1/(f_m - F)$ .

Generating a spectrum whose real component comprises peaks which all possess absorption Lorentzians is therefore desired, which is possible if all signals have a phase of 0°:

$$\Re(s(F)) = \sum_m a_m \mathcal{A}_m(F), \quad (1.32a)$$

$$\Im(s(F)) = - \sum_m a_m \mathcal{D}_m(F). \quad (1.32b)$$

For the majority of NMR experiments\*\*, the contributing signals possess phases which depend linearly on their frequencies, i.e.

$$\phi_m = \Phi_0 + \Phi_1 f_m, \quad (1.33)$$

where  $\Phi_0 \in (-\pi, \pi]$  and  $\Phi_1 \in \mathbb{R}$  are zero- and first-order phase terms. Phase correction refers to the process in which  $\Phi_0$  and  $\Phi_1$  are determined by inspecting the appearance of the spectrum  $s_\phi$  for different values of  $p_0$  and  $p_1$ , according to

$$s_{\phi,n} = s_n \exp \left( -i \left( p_0 + \frac{p_1 n}{N-1} \right) \right). \quad (1.34)$$

When  $p_0 = \Phi_0$  and  $p_1 = \Phi_1$ , the spectrum will be correctly phased.

### Baseline correction

The *baseline* of an NMR spectrum is used to describe regions where no discernible peaks reside (i.e. only experimental noise exists). Baseline distortion describes scenarios in which the baseline, rather than exhibiting a flat profile with an average of zero, has some other form. There are a number of potential causes of baseline distortion, including “clipping” of the initial points due to excessive receiver gain, and pulse breakthrough. Whatever the cause(s), it is typically a corruption of the initial points in the FID that causes baseline distortion. It is common to apply a baseline correction algorithm to negate any distortion, which involves adding a spline or high-order polynomial to the spectrum. One class of approaches which are used widely involve the two principal steps of (a) determining spectral regions which are part of the baseline, and (b) fitting the baseline regions to the chosen function before subtracting the fit from the spectrum [34, 35].

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\*\*An example of an exception to this rule is when frequency-swept pulses are applied, which generate datasets with quadratic phase behaviour. This is discussed in more detail in Section 3.3.

### 1.2.2 Conventional processing for multidimensional datasets

As for 1D datasets, it is desirable that multidimensional NMR spectra feature peaks which are frequency discriminated, and comprise pure absorption lineshapes in each dimension. A description of how this can be achieved with both amplitude- and phase-modulated datasets is now given, through the consideration of two-dimensional (2D) signals.

#### Amplitude-modulated signals

It is clear that a cosine-modulated signal, given by Equation 1.22 with  $D = 2$  and  $\zeta^{(1)} = \cos(\cdot)$  cannot achieve frequency discrimination, on account of the relation

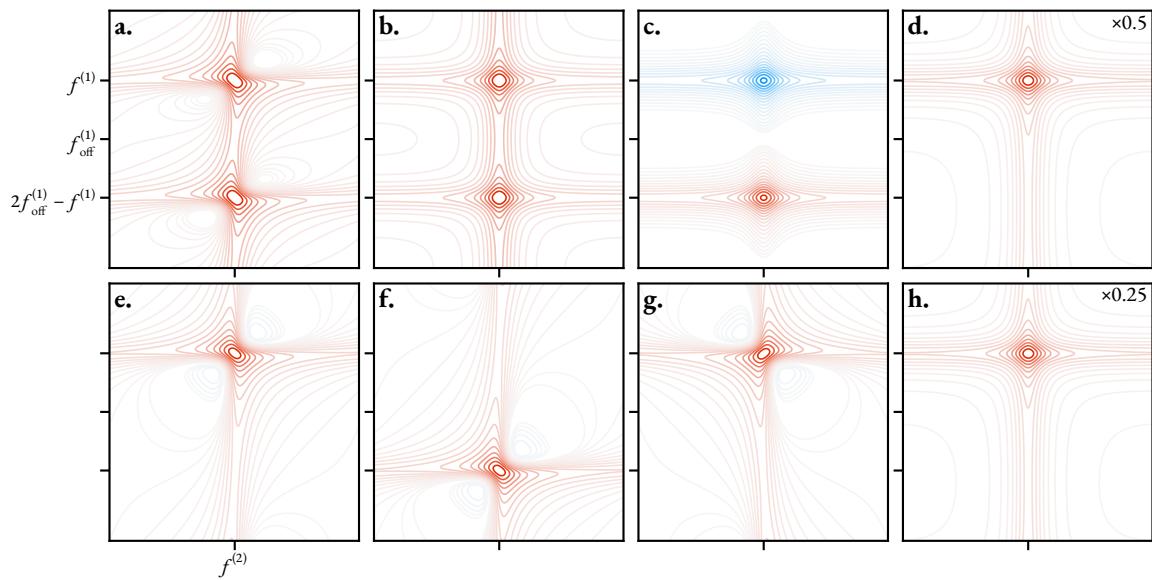
$$\cos(2\pi f^{(1)} t^{(1)}) = \frac{1}{2} (\exp(2\pi i f^{(1)} t^{(1)}) + \exp(-2\pi i f^{(1)} t^{(1)})) \quad (1.35)$$

Performing FT on such a signal in both dimensions leads to a spectrum whose real component comprises two peaks: one at the true resonance frequency  $(f^{(1)}, f^{(2)})$ , and the other at the mirror-image frequency in the indirect dimension,  $(2f_{\text{off}}^{(1)} - f^{(1)}, f^{(2)})$ . On top of this, the peaks possess a mixture of absorption and dispersion character, with the resultant peak shape often referred to as *phase twist*[36]. A spectrum of this form is presented in panel a of Figure 1.4. It is possible to generate pure absorption peaks by applying FT in the direct dimension, setting the imaginary component to zero, and finally applying FT in the indirect dimension. The real component of the result (panel b) is referred to as a double absorption spectrum.

For frequency discrimination, it is necessary to also possess the analogous sine-modulated signal ( $\zeta^{(1)} = \sin(\cdot)$ ) as this achieves quadrature detection in the indirect dimension. For numerous multidimensional experiments, repeating the pulse sequence, with careful adjustments to the phases of particular pulses, in a process referred to as phase cycling, enables this[27: Chapter 11]. Applying the same processing as that which achieved the double absorption spectrum for the cosine-modulated case generates a spectrum whose imaginary component features two peaks, but with opposite signs (panel c) on account of sine being an odd function. It then becomes possible to generate a frequency discriminated spectrum by subtracting the sine spectrum from the cosine spectrum (panel d).

#### Phase-modulated signals

A positive phase-modulated signal with the form  $\zeta^{(1)} = \exp(i\cdot)$  (commonly referred to as *hypercomplex*) is frequency discriminated due to its quadrature nature. However, direct FT of such a signal in both dimensions leads to a peak with a phase twist lineshape, with no means of separating the absorption and dispersion contributions (panel e). Certain pulse sequences, including two-dimensional J-resolved (2DJ) spectroscopy[37, 38] (see Chapter 4) and COSY[11–13] produce



**Figure 1.4:** Spectra acquired from amplitude- and phase- modulated 2D signals. Red contour lines denote positive values, while blue contours denote negative values. **a.** The FT of a cosine-modulated FID, featuring peaks both at the true resonance frequency ( $f^{(1)}$ ) and the mirrored frequency ( $2f_{\text{off}}^{(1)} - f^{(1)}$ ), and with phase-twist lineshapes. **b.** Double-absorption spectrum generated by applying FT in the direct dimension, setting the imaginary component to zero, applying FT in the indirect dimension, and retaining the real component. **c.** Spectrum acquired with the same processing method as in **b.** but with a sine-modulated FID, and with the imaginary component retained. **d.** The subtraction of the spectrum in **c.** from that in **b.** leads to a spectrum with frequency discrimination and a pure absorption lineshape. **e.** The FT of a positive phase-modulated FID, exhibiting frequency discrimination, but with a phase twist shape. **f.** The FT of a negative phase-modulated FID. **g.** The spectrum in **f.** inverted along the indirect axis, about  $f_{\text{off}}^{(1)}$ . **h.** The summation of **e.** and **g.** generates a spectrum with an absorption lineshape.

hypercomplex datasets, and the conventional means of processing is simply to display the spectrum in *magnitude-mode*, where the absolute value of each complex point is plotted. While the phase twist shapes are removed by doing this, the resulting peaks have broad “wings”, due to the influence of the dispersive components, and also from significant non-linearities. In scenarios where it is possible, it is desirable to acquire the equivalent negative signal ( $\zeta^{(1)} = \exp(-i\cdot)$ ), whose FT leads to a peak with the same phase twist form, but centered at  $2f_{\text{off}}^{(1)} - f^{(1)}$  (panel f). Inverting this spectrum about  $f_{\text{off}}^{(1)}$  (panel g), and summing with the positive spectrum nullifies the dispersive contribution, generating a spectrum with an absorption lineshape[39] (panel h).

The concepts described here for 2D signals can be extended for the processing of NMR datasets with any number of dimensions, provided that in each indirect dimension, the requisite pair of amplitude- or phase-modulated signals exist. As such, a set of  $2^{D-1}$  signals need to be acquired to produce  $D$ -dimensional spectra with absorption-mode peaks in all dimensions.

### 1.2.3 Conventional NMR analysis

The amount of detail required from an NMR dataset depends on the user’s requirements. In synthetic organic chemistry, NMR is often used simply as a means of verifying that a particular step in a synthetic pathway was successful. A simple inspection of peak locations and splittings due to scalar couplings in the spectrum may be sufficient to verify that the desired molecule was created. In many situations however, a detailed quantitative description of the data is desired. Some examples include:

- Deducing the relative concentrations of a mixture of different molecules, with application in areas such as reaction monitoring[40] and metabolomics[41]. In these circumstances, it is necessary to deduce the relative amplitudes of the signals in the data.
- Determining properties such as translational diffusion coefficients and relaxation rates, which can be achieved using a suite of 2D experiments in which each successive 1D FIDs exhibit attenuations in their signal amplitudes (these are discussed in Section 3.2). Typical approaches to analysing these datasets requires identification of the frequencies of spectral peaks of interest, from which amplitudes are extracted and fit to a function which describes how the amplitudes decay.

Most NMR users are principally interested in the integrals and positions of peaks in spectra<sup>††</sup>. Integrals are usually computed by applying a discrete integration method such as Simpson’s rule on a collection of consecutive points in the spectrum which lie within user-specified regions. The

<sup>††</sup>There may be some situations where the linewidth of the peaks are of interest too. An absorption Lorentzian produced from an exponentially-damped complex sinusoid with a damping factor  $\gamma$  will have a linewidth at half its maximum intensity of  $\gamma/\pi$ . The linewidth of peaks give an insight into the rate of transverse relaxation ( $T_2$ ) associated with a given spin.

most rudimentary form of “peak picking” — beyond the user simply defining where peaks are by inspecting the spectrum — involves assessing where relative maxima exist in the spectrum, subject to tolerances which ensure that maxima that are likely due to the presence of noise are not defined as peak positions.

### 1.2.4 Estimation Techniques for NMR Analysis

While integration and peak picking works adequately for high SNR spectra featuring very well-separated peaks, in most practical situations accurate quantification of individual signals is impossible using this approach, principally due to the inherently poor resolution associated with the FT. For this reason, considerable interest has been given to the development of techniques which are better-able to quantify NMR datasets, by attempting to estimate the optimal set of parameters  $\theta$  which describe them<sup>‡‡</sup>. Here, a summary of some of the most prominent methods for quantifying NMR data are given. Attention is primarily given to methods which consider time-domain data; for reasons that will be explained shortly, time-domain estimation is the focus of this work.

#### Linear prediction

Linear prediction (LP)[42–45] is a procedure which is widely used in NMR data analysis, for the purposes of (a) propagating an FID further in time in order to reduce the presence of truncation artefacts without the reliance on severe apodisation, and/or (b) correcting the commonly corrupted initial points of the FID, as a means of improving the spectral baseline. LP is notably different to the other methods presented here; while the other approaches aim to determine the parameters defining each contributing signal in the FID, LP is used to provide a holistic picture, describing how a datapoint in the FID is related to datapoints which precede or succeed it. As such, LP does not provide insights into individual signals in the FID.

The concept of LP stems from the idea that an FID can be described as an autoregressive (AR) process, meaning that a given sample from the dataset is a linear combination of an appropriate number  $L$  of previous samples. For a 1D FID, it is assumed that

$$y_n = \sum_{l=1}^L c_l y_{n-l} + e_l \quad \forall n \in \{L, L+1, \dots, N-1\}, \quad (1.36)$$

where  $L \in \mathbb{N}$  defines the order of the linear estimator, and  $c \in \mathbb{R}^L$  is a set of *forward* LP coefficients.  $e \in \mathbb{R}^L$  is a set of parameters, often called the innovations, which account of error in the LP model.

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<sup>‡‡</sup>The process of estimating the parameters describing an NMR dataset is often referred to as *deconvolution*. The term is not used here as it is a misnomer; deconvolution is simply the inverse operation of convolution, and has nothing to do with estimation. Equivalently, *convolution* is not the process of generating an NMR signal by the process of summing a number of complex sinusoids, though it is often described as so in the NMR literature.

A datapoint can also be described by a linear combination of subsequent points, using the set of *backward* LP coefficients  $\mathbf{b} \in \mathbb{R}^L$ :

$$y_n = \sum_{l=1}^L b_l y_{n+l} + e_l \quad \forall n \in \{0, 1, \dots, N-L-1\}. \quad (1.37)$$

Determining the LP coefficients enables the estimation of FID values beyond the data actually acquired ( $n > N-1$ ), as well as to replace datapoints which are anticipated to be corrupted. It should be noted that Equations 1.36 and 1.37 are only technically valid for FIDs without any corruption from experimental noise. Noisy datasets are instead an example of an autoregressive moving average (ARMA) process. Despite this, due to the greater simplicity of the AR model, it is far more common to employ this, with good results attainable as long as the data is not extrapolated by too great an extent. The most common means of performing LP is by solving the Yule-Walker equations[46, 47], which describe the relationship between the signal autocorrelation coefficients and the LP coefficients[43: Section 3.3], with the Levinson-Durbin algorithm providing an efficient means of solving the equations[48, 49].

### SVD-based methods

Some of the most prevalent methods for NMR estimation involve *singular value decomposition* (SVD) as a key component (Appendix B.1.1). For each of these methods, SVD is applied to a Hankel or Toeplitz matrix containing the FID. Above a certain SNR threshold, it is found that the singular values in the data matrix are larger than those related to noise, and as such forming a low-rank approximation of the data matrix nullifies contributions from noise in the parameter estimate. The degree of truncation required is dependent on the suspected *model order* (i.e. the number of contributing signals,  $M$ ) of the dataset, which must be supplied, or determined by some appropriate metric. All the SVD-based techniques determine the non-linear parameters (frequencies and damping factors, incorporated in the signal poles) associated with the dataset. Subsequently, the amplitudes and phases can be computed by solving a linear least-squares problem involving the pseudo-inverse of a Vanermonde matrix of the signal poles:

$$\boldsymbol{\alpha} = \mathbf{Z}^+ \mathbf{y}, \quad (1.38a)$$

$$\mathbf{Z} = \begin{bmatrix} 1 & 1 & \dots & 1 \\ z_1^1 & z_2^1 & \dots & z_M^1 \\ \vdots & \vdots & \ddots & \vdots \\ z_1^{N-1} & z_2^{N-1} & \dots & z_M^{N-1} \end{bmatrix}. \quad (1.38b)$$

Both linear prediction singular value decomposition (LPSVD)[50, 51] and Hankel singular value

decomposition (HSVD)[52] have been used extensively in the field of *in vivo* magnetic resonance spectroscopy (MRS) after introduction by Barkhuijsen and co-workers[53–57]. With LPSVD, the signal poles are determined by finding the roots of a polynomial which features the backward LP coefficients associated with the signal, in a similar fashion to the classical Prony method[58]. HSVD is based on the “state-space” principle, which generated interest in part because it meant that the computationally costly polynomial rooting step in LPSVD was avoided. A further technique in this category, the matrix pencil method (MPM)[59–61] is based on solving a generalised eigenvalue problem. Pines and coworkers introduced the information theoretic matrix pencil method (ITMPM)[62], for use in NMR, which combines the MPM with a method for estimating the model order, such that no *a priori* information is required from the user. Recently, the MPM has been employed for the analysis of NMR relaxometry data[63, 64]. Outlines of the MPM and its 2D equivalent, the modified matrix enhancement and matrix pencil method (MMEMPM)[65, 66] are provided in detail in Section 2.2.1.

### Iterative Methods

For problems involving nonlinear function fitting, the most widespread approaches are iterative techniques. The variable projection (VARPRO) method[67] is such an example, which has been applied extensively in the field of MRS, following its introduction by van der Veen and co-workers[68, 69]. VARPRO relies on determining the following quantity, an example of a residual sum-of-squares (RSS) problem:

$$\theta^{(*)} = \arg \min_{\theta \in \mathbb{R}^{4M}} \|y - x(\theta)\|^2 \equiv \arg \min_{\theta \in \mathbb{R}^{4M}} \|y - Z\alpha\|^2, \quad (1.39)$$

where  $\theta^{(*)}$  is the optimal set of parameters which describe the data, often referred to as the maximum likelihood estimate (MLE). The linear parameters, residing in the vector of complex amplitudes, can be expressed as  $Z^+y$  (see Equation 1.38). By doing this, it becomes possible to recast the optimisation problem to only solve for the nonlinear terms:

$$[f^T \ \eta^T]^{(*)T} = \arg \min_{[f^T \ \eta^T]^T \in \mathbb{R}^{2M}} \|y - ZZ^+y\|^2. \quad (1.40)$$

The Levenberg-Marquardt (LM) algorithm[70, 71] is typically employed to perform the optimisation routine, with amplitudes and phases determined with linear least squares afterwards.

For such a routine to be effective, a large amount of *a priori* information needs to be provided, in the form of a set of estimated frequencies and damping factors in the data; iterative methods like the LM algorithm only tend to perform successfully if they start with a set of parameters sufficiently close to the optimal parameter estimate in the parameter space. Further specifications

can be supplied to VARPRO, reflecting the spectroscopist's knowledge of the signal under inspection. For example, damping factors corresponding to signals that form a particular multiplet can be constrained to be equal. Advanced method for accurate, robust, and efficient spectral fitting (AMARES) is an improvement of VARPRO, which facilitates a wider variety of linear constraints to be imposed on the parameter set[72], and is now established as one of the most prominent means of quantifying MRS signals.

There is not much precedent for using iterative schemes for NMR analysis, despite its widespread adoption in MRS. The main cause of this is probably due to the requirement to supply a large amount of prior knowledge; in MRS, it is likely that the practitioner has an intimate understanding of the expected signals which will be present in an acquired dataset, since all signals will derive from species which make up the human metabolome, whose chemical shifts and multiplet structures will be well-established. As  $^{31}\text{P}$  is the most common nucleus studies in MRS, the number of potential species contributing to datasets is reduced even further. Over many experiments, little adjustment to the information provided to the optimiser will need to be given, making the process facile. In NMR experiments, there is a far greater variation in the appearance of the data, such that the process of defining *a priori* information for each dataset of interest may become time-consuming and cumbersome. There is also a good possibility that the expected identity of the dataset is unknown in NMR, making any method which requires intimate knowledge about the data worthless.

## Bayesian Methods

Complete reduction to amplitude frequency table (CRAFT)[73, 74] is a routine developed by Krishnamurthy, inspired by previous work by Brethorst[75–79], for the parametric estimation based on the principle of Bayesian inference. In brief, CRAFT consists of defining prior distributions for the signal parameters, and gradually increasing the number of signal components in the model until a maximisation of the posterior probably is achieved, such that both model order selection and parameter estimation are achieved simultaneously. In order to reduce the computational burden of the estimation, the complete FID is downsampled into a series of “sub-FIDs”, with each sub-FID being analysed separately. CRAFT has been extended for the consideration of 2D FIDs, through a simple extension of the 1D estimation procedure[80]. After the direct-dimension of the dataset is processed using the conventional FT approach, each FID in the indirect-dimension is estimated separately, yielding a  $4 \times M$  parameter set for each indirect increment. Such an approach is not able to extract all  $6 \times M$  parameters associated with the 2D dataset however.

## Machine Learning Methods

The vast surge in prevalence of machine learning across virtually all scientific disciplines has unsurprisingly lead to work which applies it for the purposes of NMR estimation in recent years. At the time of writing, approaches have focussed on Fourier-domain estimation[81, 82]. The currently available methods employ deep (i.e. many-layered) neural networks, featuring numerous deconvolution layers, which have been shown to be widely successful in image- and signal processing applications.

# 1.3 Overview of this work

## 1.3.1 Conception and motivation

The central focus of this work is the development of a routine which performs parametric estimation on NMR datasets. Motivation initially came from discussions within the NMR Methodology Group in Manchester involving Dr Mohammadali Foroozandeh and co-workers — notably Prof. Gareth Morris and Prof. Mathias Nilsson — while Dr Foroozandeh was a Postdoctoral researcher there. The group were interested in generating pure shift NMR spectra from 2DJ datasets via appropriate post-processing of the data. While little progress was made when Dr Foroozandeh was based in Manchester, he wished to continue with the project after moving to Oxford to take up a research fellowship, which I took the reins of when I joined his nascent research group as a PhD student.

To ensure its applicability to 2DJ datasets, the following properties were sought when devising what the estimation routine would entail:

*Support for 1D and 2D data* The method should be able to analyse both 1D FIDs and also hypercomplex 2D FIDs (the form which 2DJ datasets take). 2D data should be analysed holistically, rather than as successive 1D increments, as is the case in methods like CRAFT[80]. This is since better signal resolution is often available when both dimensions are considered at the same time; certain signals which exhibit clear resolution in a 2D dataset may be heavily overlapping in 1D data and are therefore more challenging if not impossible to quantify accurately.

*Time-domain based* As discussed in Section 1.2.2, due to the hypercomplex nature of 2DJ FIDs, generating spectra with desirable absorption lineshapes is not possible. Typically, resorting to displaying the spectra in magnitude-mode is deemed optimal, as this overcomes the phase-twist peak lineshapes. Such spectra suffer from severe non-linearities and dispersion-mode contributions, both of which make the task of estimating 2DJ data in the Fourier domain challenging. For this reason, estimating the dataset by considering its FID rather than its spectrum is preferred.

*Accessibility* To achieve wide-spread adoption, especially by non-expert NMR users, the method should require minimal user intervention to perform effectively. As such, a method requiring the specification of as little prior knowledge about the data as possible is desired. On top of this, the method should be available as software that users can gain familiarity with easily.

### 1.3.2 Thesis Overview

This thesis is broken into the following chapters:

- **Chapter 2** discusses the theory behind routines which can be applied to determine parameter estimates related to 1D and 2D FIDs.
- **Chapter 3** provides illustrations of the performance of the estimation routine on 1D NMR datasets. Furthermore, means in which parametric estimation routine can be harnessed for two applications are explored:
  - The analysis of amplitude-attenuated datasets, such as those derived from diffusion,  $T_1$ - and  $T_2$ -measuring experiments (Section 3.2).
  - Overcoming quadratic phase behaviour and baseline distortions associated with ultra-broadband excitation by a single frequency-swept pulse (Section 3.3).
- **Chapter 4** outlines a devised method, given the acronym CUPID, for generating pure shift spectra from the estimation of 2DJ datasets.
- **Chapter 5** describes the source code developed as part of this project call NMR estimation in Python (NMR-EsPy).
- Finally, conclusions and considerations for further potential developments are discussed in **Chapter 6**.

Additional supporting information can be found in the appendix:

- **Appendix A** provides a glossary of terms related to NMR which are not introduced in much detail in the main text.
- **Appendix B** provides additional information on the theory related to this work, including descriptions of mathematical concepts, and outlines of relevant algorithms.
- **Appendix C** provides code listings outlining how the methods described in this work can be implemented in the PYTHON programming language. These are effectively minimalist variants of code found in the NMR-EsPy package.
- **Appendix D** outlines how the simulated and experimental datasets considered in this work were generated.

- **Appendix E** provides two insert from relevant documents. The first is a chapter from the documentation of NMR-EsPy, which comprises tutorials to help users get started with the package. The second is the current state of a draft for a paper to be submitted to *Angewandte Chemie* (see below).

The following publications are related to this work:

S. G. Hulse and M. Foroozandeh. “Newton meets Ockham: Parameter estimation and model selection of NMR data with NMR-EsPy”. In: *Journal of Magnetic Resonance* 338 (2022), p. 107173

At the time of writing (22/9/2023) a draft for a communication exists which outlines the 2DJ/pure shift work outlined in Chapter 4, and is written for a wide chemistry audience. It is intended that this will shortly be submitted to *Angewandte Chemie*. See Appendix E.b for the current form of the draft.



# Theory

2

This chapter provides a description of the theory behind an estimation routine which has been developed for the consideration of time domain NMR data. In essence, the routine consists of generating a parameter estimate using the SVD-based MPM, which is fed to a non-linear programming (NLP) routine to produce a final result. The MPM is employed to generate an initial guess of parameters, while the NLP routine behaves as a means of validation, by attempting to make the parameter estimate consistent with known features of the data. The technique can be thought of as a compromise between “black-box” methods[84] which require little to no prior knowledge about the data, and iterative methods like VARPRO and AMARES, which require vast amounts of user input, but are typically able to estimate complex datasets more effectively. Furthermore, after profiling the run time and memory consumption of the technique, a method for producing filtered FIDs, featuring a subset of the signals and (optionally) fewer datapoints relative to the full FID is presented, which can drastically reduce the burden on computational resources.

Outlines of relevant algorithms and corresponding `PYTHON` implementations are provided to supplement this chapter. As well as those present within the main text, further pseudo-code algorithms can be found in Appendix B.4, while `PYTHON` implementations can be found in Appendix C.

## 2.1 Outline of the Problem

Through the application of NMR theory, one can rationalise how a particular spin system, subjected to a given pulse sequence, is mapped to an FID. This is an example of a *forward problem*, in which one wishes to determine how a set of parameters is mapped to the resulting data. The chemical shifts, J-couplings, dipolar couplings, etc. of the spin system may be recast as a list of signal amplitudes, phases, frequencies and damping factors, which define the form of the FID.

Many sophisticated pieces of software such as SPINACH[85] solve this forward problem, yielding NMR experiment simulations. Simulating an NMR experiment is a *well-posed* problem, since it satisfies the following properties:

1. The problem has a solution.
2. The solution is unique.
3. The solution's behaviour changes continuously with the parameters provided. For example, continuously changing the chemical shift of a given spin will lead to the position of its signal(s) in the resulting spectrum to continuously vary. Other phenomena such as strong coupling effects may manifest as a given spin's chemical shift changes; these will also evolve in a continuous fashion as well.

The parametric estimation of FIDs is an example of an *inverse problem*; given an acquired dataset, one seeks to determine the set of parameters which went into constructing it. Parametric estimation, as with many inverse problems, is *ill-posed*[86]. These problems do not satisfy at least one of the three properties above. For example, given an FID, it is possible to conceive of numerous signal parameter specifications which would lead to a faithful representation of the data in a least squares sense. Therefore, determining the “optimal” parameter set is a rather difficult challenge.

For the purposes of this work, it is always assumed that an FID to be estimated  $\mathbf{Y} \in \mathbb{C}^{N^{(1)} \times \dots \times N^{(D)}}$  is hypercomplex in form, meaning that it obeys Equation 1.22 with  $\zeta^{(d)} = \exp(i \cdot)$   $\forall d \in \{1, \dots, D\}$ :

$$\gamma_{n^{(1)}, \dots, n^{(D)}} = x_{n^{(1)}, \dots, n^{(D)}}(\theta) + w_{n^{(1)}, \dots, n^{(D)}}, \quad (2.1a)$$

$$x_{n^{(1)}, \dots, n^{(D)}}(\theta) = \sum_{m=1}^M \alpha_m \exp(i\phi_m) \prod_{d=1}^D \exp\left(\left(2\pi i \left(f_m^{(d)} - f_{\text{off}}^{(d)}\right) - \gamma_m^{(d)}\right) n^{(d)} \Delta_t^{(d)}\right), \quad (2.1b)$$

$$w_{n^{(1)}, \dots, n^{(D)}} \sim \mathcal{N}_C(0, 2\sigma^2), \quad (2.1c)$$

where  $\Delta_t^{(d)} = 1/f_{\text{sw}}^{(d)}$ . It should be noted that, prior to estimating the dataset, it is normalised such that the signal actually under consideration is  $\mathbf{Y}/\|\mathbf{Y}\|$ . To make the final result reflect the unnormalised dataset, the estimated amplitudes can be multiplied by  $\|\mathbf{Y}\|$ . Under this model, it is assumed that an FID consists of a summation of  $M$  damped complex sinusoids in the presence in AWGN. It is the goal of parametric estimation to establish the identity of all the quantities which describe the model component  $\mathbf{X}$ , which are distilled into the vector  $\theta \in \mathbb{R}^{2(D+1)M}$ , given by Equation 1.21. Equation 2.1b can be expressed in terms of complex amplitudes and signals poles as follows:

$$x_{n^{(1)}, \dots, n^{(D)}}(\theta) = \sum_{m=1}^M \alpha_m \prod_{d=1}^D z_m^{(d)} n^{(d)}, \quad (2.2a)$$

$$\alpha_m = \alpha_m \exp(i\phi_m), \quad (2.2b)$$

$$z_m^{(d)} = \exp \left( \left( 2\pi i \left( f_m^{(d)} - f_{\text{off}}^{(d)} \right) - \eta_m^{(d)} \right) \Delta_t^{(d)} \right). \quad (2.2c)$$

Due to the assumed AWGN nature of the noise array, the probability density function (PDF) of an individual noise component is

$$p(w_{n^{(1)}, \dots, n^{(D)}}) = \frac{1}{2\pi\sigma^2} \exp \left( -\frac{|w_{n^{(1)}, \dots, n^{(D)}}|^2}{2\sigma^2} \right). \quad (2.3)$$

As the elements are independent and identically distributed, the joint PDF describing the entire noise array is given by the product of all the elements' PDFs:

$$\begin{aligned} p(\mathbf{W}) &= \prod_{n^{(1)}=0}^{N^{(1)}-1} \cdots \prod_{n^{(D)}=0}^{N^{(D)}-1} \frac{1}{2\pi\sigma^2} \exp \left( -\frac{|w_{n^{(1)}, \dots, n^{(D)}}|^2}{2\sigma^2} \right) \\ &= \frac{1}{(2\pi\sigma^2)^{\mathfrak{N}}} \exp \left( -\frac{\|\mathbf{W}\|^2}{2\sigma^2} \right). \end{aligned} \quad (2.4)$$

As the noise array is the difference between the data and model, the likelihood function of  $\theta$  given the FID  $\mathbf{Y}$  is

$$\mathcal{L}(\theta|\mathbf{Y}) = \frac{1}{(2\pi\sigma^2)^{\mathfrak{N}}} \exp \left( -\frac{\|\mathbf{Y} - \mathbf{X}(\theta)\|^2}{2\sigma^2} \right). \quad (2.5)$$

It is common to consider instead the log-likelihood function,  $\ell(\theta|\mathbf{Y}) := \ln \mathcal{L}(\theta|\mathbf{Y})$ :

$$\ell(\theta|\mathbf{Y}) = -\mathfrak{N} \ln (2\pi\sigma^2) - \frac{\|\mathbf{Y} - \mathbf{X}(\theta)\|^2}{2\sigma^2}. \quad (2.6)$$

As application of the logarithm is a monotonic transformation, the arguments of the maxima of  $\mathcal{L}$  and  $\ell$  are equivalent. Equation 2.6 implies that the optimal set of parameters  $\theta^{(*)}$ , i.e. the MLE, is that which minimises the RSS between the data and the model:

$$\theta^{(*)} = \arg \max_{\theta \in \mathbb{R}^{2(D+1)M}} \ell(\theta|\mathbf{Y}) \equiv \arg \min_{\theta \in \mathbb{R}^{2(D+1)M}} \|\mathbf{Y} - \mathbf{X}(\theta)\|^2. \quad (2.7)$$

The application of NLP is a well-established approach to solve such a problem[87, 88]. The basic principle behind NLP is to iteratively explore, in a methodical way, how a function varies with its arguments. By using information about the function and optionally its derivatives, such a routine attempts to find a minimum in the function, and terminates once this has been achieved. While derivative-free approaches to NLP do exist[89–91], in scenarios where the function under consideration has well-defined, computationally tractable derivatives, the use of these can be valuable

to solving optimisation problems; the problem outlined in Equation 2.7 is such an example.

As discussed already, for NLP to perform effectively, a large amount of *a priori* information is typically required, in the form of an initial guess, possibly alongside other constraints. To achieve this, the method employed in this work makes use of the MPM, the subject of the next section.

## 2.2 The matrix pencil method

In this section, a description of the MPM is provided. This work is limited to the consideration of 1D and 2D NMR data, and so both the original 1D MPM and its 2D analogue, the MMEMPM are discussed.

### 2.2.1 1D Matrix Pencil Method

The MPM, developed by Hua and Sarkar[59–61], provides a route to extracting the signal poles of a 1D dataset, based on the assumption that the number of signals  $M$  that the data comprises is known. To motivate how the MPM works, first consider a dataset which is devoid of noise, given by Equation 2.2 with  $D = 1$ :

$$x_n(\theta) = \sum_{m=1}^M \alpha_m z_m^n \quad \forall n \in \{0, \dots, N-1\}. \quad (2.8)$$

Consider the Hankel matrix  $\mathbf{H}_x \in \mathbb{C}^{(N-L) \times (L+1)}$ :

$$\mathbf{H}_x = \begin{bmatrix} x_0 & x_1 & \cdots & x_L \\ x_1 & x_2 & \cdots & x_{L+1} \\ \vdots & \vdots & \ddots & \vdots \\ x_{N-L-1} & x_{N-L} & \cdots & x_{N-1} \end{bmatrix}. \quad (2.9)$$

This matrix comprises windowed segments of the FID, with each row featuring the segment shifted to the right by one point relative to the row above.  $L \in \mathbb{N}$  is referred to as the *pencil parameter*, which dictates the size of each window. From  $\mathbf{H}_x$ , two matrices are defined:  $\mathbf{H}_{x1}$  and  $\mathbf{H}_{x2}$ . These are formed by the removal of the last and first column of  $\mathbf{H}_x$ , respectively:

$$\mathbf{H}_{x1} = \begin{bmatrix} x_0 & x_1 & \cdots & x_{L-1} \\ x_1 & x_2 & \cdots & x_L \\ \vdots & \vdots & \ddots & \vdots \\ x_{N-L-1} & x_{N-L} & \cdots & x_{N-2} \end{bmatrix}, \quad (2.10a)$$

$$\mathbf{H}_{x2} = \begin{bmatrix} x_1 & x_2 & \cdots & x_L \\ x_2 & x_3 & \cdots & x_{L+1} \\ \vdots & \vdots & \ddots & \vdots \\ x_{N-L} & x_{N-L+1} & \cdots & x_{N-1} \end{bmatrix}. \quad (2.10b)$$

$\mathbf{H}_{x1}$  and  $\mathbf{H}_{x2}$  can be deconstructed into the following forms involving matrices containing the  $M$  signal poles and complex amplitudes that the data comprises:

$$\mathbf{H}_{x1} = \mathbf{Z}_L \mathbf{A} \mathbf{Z}_R, \quad (2.11a)$$

$$\mathbf{H}_{x2} = \mathbf{Z}_L \mathbf{A} \mathbf{Z}_D \mathbf{Z}_R, \quad (2.11b)$$

$$\mathbb{C}^{\binom{N^{(1)} - L^{(1)}}{1} \times M} \ni \mathbf{Z}_L = \begin{bmatrix} 1 & z & z^2 & \cdots & z^{N-L-1} \end{bmatrix}^T, \quad (2.11c)$$

$$\mathbb{C}^{M \times L} \ni \mathbf{Z}_R = \begin{bmatrix} 1 & z & z^2 & \cdots & z^{L-1} \end{bmatrix}, \quad (2.11d)$$

$$\mathbb{C}^{M \times M} \ni \mathbf{Z}_D = \text{diag}(z), \quad (2.11e)$$

$$\mathbb{C}^{M \times M} \ni \mathbf{A} = \text{diag}(\alpha), \quad (2.11f)$$

$$\alpha = \begin{bmatrix} \alpha_1 & \alpha_2 & \cdots & \alpha_M \end{bmatrix}^T, \quad (2.11g)$$

$$z = \begin{bmatrix} z_1 & z_2 & \cdots & z_M \end{bmatrix}^T. \quad (2.11h)$$

The *matrix pencil*  $\mathbf{H}_{x2} - \lambda \mathbf{H}_{x1}$ , with  $\lambda \in \mathbb{C}$ , can therefore be expressed as

$$\mathbf{H}_{x2} - \lambda \mathbf{H}_{x1} = \mathbf{Z}_L \mathbf{A} (\mathbf{Z}_D - \lambda \mathbf{I}_M) \mathbf{Z}_R, \quad (2.12)$$

where  $\mathbf{I}_M \in \mathbb{C}^{M \times M}$  is the identity matrix. Assuming that the condition  $M \leq L \leq N - M$  is met — this ensures that both the number of rows and columns of the matrix pencil are at least  $M$  — the rank of the matrix pencil will be  $M$ . Now consider the case when the scalar  $\lambda$  is equal to one of the signal poles i.e.  $\lambda = z_m \forall m \in \{1, \dots, M\}$ : the element  $[\mathbf{Z}_D - \lambda \mathbf{I}_M]_{m,m}$  becomes 0, which will lead to the determinant of the matrix pencil being 0. The signal poles are therefore the *generalised eigenvalues* of  $\mathbf{H}_{x2} - \lambda \mathbf{H}_{x1}$ , defined by [92: Section 7.7]:

$$z = \{z \in \mathbb{C} : \det(\mathbf{H}_{x2} - z \mathbf{H}_{x1}) = 0\} \quad (2.13)$$

One means of finding the signal poles is by finding the eigenvalues of the matrix  $\mathbf{H}_{x1}^+ \mathbf{H}_{x2}$ . Deriving the corresponding complex amplitudes can then be achieved by solving the set of linear equations given by Equation 1.38, with  $y$  replaced by  $x$ . Extraction of the amplitudes, phases, frequencies, and damping factors from the signal poles and complex amplitudes can then take place:

$$\alpha = |\alpha|, \quad (2.14a)$$

$$\phi = \arctan \left( \frac{\Im(\alpha)}{\Re(\alpha)} \right), \quad (2.14b)$$

$$f = \frac{f_{\text{sw}}}{2\pi} \Im(\ln z) + f_{\text{off}}, \quad (2.14c)$$

$$\eta = -f_{\text{sw}} \Re(\ln z). \quad (2.14d)$$

Noise corruption complicates the process of determining the  $M$  signal poles. The Hankel matrix associated with an FID corrupted by noise  $\mathbf{H}_y$  is likely to be of full-rank, i.e.  $\text{rank}(\mathbf{H}_y) = \min(N - L, L + 1)$ . To minimise the influence of noise on the estimated signal poles, it is necessary to generate a rank-reduced matrix  $\tilde{\mathbf{H}}_y$ . By employing the Eckart-Young-Mirsky (EYM) theorem[92: Section 2.2], an appropriate matrix can be obtained through SVD (see Appendix B.1.1):

$$\tilde{\mathbf{H}}_y = \mathbf{U}_M \Sigma_M \mathbf{V}_M^\dagger \quad (2.15a)$$

$$\mathbb{C}^{(N^{(1)} - L^{(1)}) \times M} \ni \mathbf{U}_M = [\mathbf{u}_1 \ \mathbf{u}_2 \ \dots \ \mathbf{u}_M], \quad (2.15b)$$

$$\mathbb{C}^{(L^{(1)} + 1) \times M} \ni \mathbf{V}_M = [\mathbf{v}_1 \ \mathbf{v}_2 \ \dots \ \mathbf{v}_M], \quad (2.15c)$$

$$\mathbb{C}^{M \times M} \ni \Sigma_M = \text{diag}(\sigma_1, \sigma_2, \dots, \sigma_M). \quad (2.15d)$$

$\sigma_m$  is the  $m^{\text{th}}$  largest singular value of  $\mathbf{H}_y$ , while  $\mathbf{u}_m \in \mathbb{C}^{N-L}$  and  $\mathbf{v}_m \in \mathbb{C}^{L+1}$  are the corresponding left and right singular vectors, respectively. The EYM theorem proves that  $\tilde{\mathbf{H}}_y$  is the closest matrix of rank  $M$  to  $\mathbf{H}_y$  in a Frobenius norm sense, i.e.

$$\tilde{\mathbf{H}}_y = \arg \min_{\mathbf{A}: \text{rank}(\mathbf{A})=M} \|\mathbf{A} - \mathbf{H}_y\|. \quad (2.16)$$

The intention behind applying the SVD in the MPM and other SVD-based methods is to discard components in the Hankel matrix that are associated with noise. Assuming the SNR of an FID is sufficiently high, a clear distinction is often found between the singular values associated with true signal components and those associated with noise (see panel b of Figure 2.2 for an example of this).

The signal poles are finally extracted by computing the eigenvalues of  $\tilde{\mathbf{H}}_{y1}^+ \tilde{\mathbf{H}}_{y2}$ , where  $\tilde{\mathbf{H}}_{y1}$  and  $\tilde{\mathbf{H}}_{y2}$  have the same relation to  $\tilde{\mathbf{H}}_y$  as  $\mathbf{H}_{x1}$  and  $\mathbf{H}_{x2}$  do to  $\mathbf{H}_x$ . As a less expensive alternative, the same result can be achieved by computing the eigenvalues of  $\mathbf{U}_{M1}^+ \mathbf{U}_{M2}$ , with

$$\mathbf{U}_{M1} = [\mathbf{u}_1 \ \mathbf{u}_2 \ \dots \ \mathbf{u}_{M-1}], \quad (2.17a)$$

$$\mathbf{U}_{M2} = [\mathbf{u}_2 \ \mathbf{u}_3 \ \dots \ \mathbf{u}_M]. \quad (2.17b)$$

Algorithm 2.1 provides a pseudo-code description of the MPM, while Code Listing C.3 provides an example PYTHON implementation. For optimal results, the pencil parameter should adhere to  $\lfloor N/3 \rfloor \leq L \leq \lfloor 2N/3 \rfloor$ [59]. In this work,  $\lfloor N/3 \rfloor$  is always used, primarily since the computational burden of the method is at a maximum when  $L = N/2^*$ .

**Algorithm 2.1** The MPM, with the optional prediction of model order using the MDL if  $M$  is set to 0.

---

```

1: procedure MPM( $y \in \mathbb{C}^N, f_{\text{sw}} \in \mathbb{R}_{>0}, f_{\text{off}} \in \mathbb{R}, M \in \mathbb{N}$ )
2:    $L \leftarrow \lfloor N/3 \rfloor;$ 
3:    $H_y \leftarrow \begin{bmatrix} y_0 & y_1 & \cdots & y_L \\ y_1 & y_2 & \cdots & y_{L+1} \\ \vdots & \vdots & \ddots & \vdots \\ y_{N-L-1} & y_{N-L} & \cdots & y_{N-1} \end{bmatrix};$ 
4:    $U, \sigma, V \leftarrow \text{SVD}(H_y);$ 
5:   if  $M = 0$  then
6:      $M \leftarrow \text{MDL}(\sigma, L, N);$ 
7:   end if
8:    $U_{M1}, U_{M2} \leftarrow [u_1 \ u_2 \ \cdots \ u_{M-1}], [u_2 \ u_3 \ \cdots \ u_M];$ 
9:    $z \leftarrow \text{EIGENVALUES}(U_{M1}^T U_{M2});$ 
10:   $Z \leftarrow [1 \ z \ z^2 \ \cdots \ z^N]^T;$ 
11:   $\alpha \leftarrow Z^T y;$ 
12:   $\alpha, \phi \leftarrow |\alpha|, \arctan\left(\frac{\Im(\alpha)}{\Re(\alpha)}\right);$ 
13:   $f, \eta \leftarrow \frac{f_{\text{sw}}}{2\pi} \Im(\ln z) + f_{\text{off}}, -f_{\text{sw}} \Re(\ln z);$ 
14:  if  $\eta$  contains negative values then ▷ Purge any oscillators with negative damping
15:    Remove these from  $\eta$ , and remove the corresponding values from  $\alpha, \phi$ , and  $f$ ;
16:  end if
17:   $\theta^{(0)} \leftarrow [\alpha^T \ \phi^T \ f^T \ \eta^T]^T;$ 
18:  return  $\theta^{(0)};$ 
19: end procedure

20: procedure MDL( $\sigma \in \mathbb{R}^{L+1}, L \in \mathbb{N}, N \in \mathbb{N}$ )
21:   for  $k = 0, \dots, L$  do
22:      $\text{MDL}_k \leftarrow -\ln\left(\frac{\prod_{r=k}^{L-1} \sigma_{r+1}^{1/(L-k)}}{\frac{1}{L-k} \sum_{r=k}^{L-1} \sigma_{r+1}}\right)^{(L-k)N} + \frac{1}{2}k(2L-k)\ln N;$ 
23:     if  $k > 0$  and  $\text{MDL}_k > \text{MDL}_{k-1}$  then
24:        $M \leftarrow k-1;$ 
25:       break;
26:     end if
27:   end for
28:   return  $M;$ 
29: end procedure

```

---

### 2.2.2 2D Matrix Enhancement and Matrix Pencil Method

The MPM was extended for the consideration of 2D data by Hua with the *matrix enhancement and matrix pencil method* (MEMPM)[65]. The method centers around the enhanced matrix  $E_Y \in$

\*With  $L = \lfloor N/2 \rfloor$ , the matrix  $H_y$  is at its most “square” i.e. the number of rows and columns are at their most similar. Matrices which are more square will increase the demands on computing the SVD, with a complexity  $\mathcal{O}(\min(L+1, N-L+1)^2 \times \max(L+1, N-L+1))$ .

$\mathbb{C}^{L^{(1)}L^{(2)} \times (N^{(1)} - L^{(1)} + 1)(N^{(2)} - L^{(2)} + 1)}$ , a block Hankel matrix of the form

$$\mathbf{E}_Y = \begin{bmatrix} \mathbf{H}_{y,0} & \mathbf{H}_{y,1} & \cdots & \mathbf{H}_{y,N^{(1)}-L^{(1)}} \\ \mathbf{H}_{y,1} & \mathbf{H}_{y,2} & \cdots & \mathbf{H}_{y,N^{(1)}-L^{(1)}+1} \\ \vdots & \vdots & \ddots & \vdots \\ \mathbf{H}_{y,L^{(1)}-1} & \mathbf{H}_{y,L^{(1)}} & \cdots & \mathbf{H}_{y,N^{(1)}-1} \end{bmatrix}, \quad (2.18a)$$

$$\mathbf{H}_{y,n^{(1)}} = \begin{bmatrix} \gamma_{n^{(1)},0} & \gamma_{n^{(1)},1} & \cdots & \gamma_{n^{(1)},N^{(2)}-L^{(2)}} \\ \gamma_{n^{(1)},1} & \gamma_{n^{(1)},2} & \cdots & \gamma_{n^{(1)},N^{(2)}-L^{(2)}+1} \\ \vdots & \vdots & \ddots & \vdots \\ \gamma_{n^{(1)},L^{(2)}-1} & \gamma_{n^{(1)},L^{(2)}} & \cdots & \gamma_{n^{(1)},N^{(2)}-1} \end{bmatrix}. \quad (2.18b)$$

In an equivalent fashion to Equation 2.11,  $\mathbf{H}_{x,n^{(1)}}$ , the noiseless equivalent to  $\mathbf{H}_{y,n^{(1)}}$ , can be expressed as

$$\mathbf{H}_{x,n^{(1)}} = \mathbf{Z}_L^{(2)} \mathbf{A} \mathbf{Z}_D^{(1)} n^{(1)} \mathbf{Z}_R^{(2)}. \quad (2.19)$$

This then enables the noiseless enhanced matrix to be decomposed as follows:

$$\mathbf{E}_X = \mathbf{E}_L \mathbf{A} \mathbf{E}_R, \quad (2.20a)$$

$$\mathbb{C}^{L^{(1)}L^{(2)} \times M} \ni \mathbf{E}_L = \begin{bmatrix} \mathbf{Z}_L^{(2)} \\ \mathbf{Z}_L^{(2)} \mathbf{Z}_D^{(1)} \\ \vdots \\ \mathbf{Z}_L^{(2)} \mathbf{Z}_D^{(1)L^{(1)}-1} \end{bmatrix}, \quad (2.20b)$$

$$\mathbb{C}^{M \times (N^{(1)} - L^{(1)} + 1)(N^{(2)} - L^{(2)} + 1)} \ni \mathbf{E}_R = \left[ \mathbf{Z}_R^{(2)} \quad \mathbf{Z}_D^{(1)} \mathbf{Z}_R^{(2)} \quad \dots \quad \mathbf{Z}_D^{(1)^{N^{(1)}-L^{(1)}}} \mathbf{Z}_R^{(2)} \right]. \quad (2.20c)$$

As was the case in the 1D MPM, SVD can be utilised to generate a filtered matrix  $\tilde{\mathbf{E}}_Y$  with its rank reduced to  $M$ , in accordance with the EYM theorem:

$$\tilde{\mathbf{E}}_Y = \mathbf{U}_M \boldsymbol{\Sigma}_M \mathbf{V}_M^\dagger \quad (2.21)$$

Due to the large size of the enhanced matrix, a vast improvement in the speed of the MEMPM can be realised when, rather than compute the SVD in its entirety, a *truncated* SVD is computed, in which only the first  $M$  components of the SVD are determined using iterative approaches like the Arnoldi method[93, 94].

If the conditions  $N^{(d)} - L^{(d)} + 1 \geq M \forall d \in \{1, 2\}$  are met,  $\text{range}(\mathbf{U}_M) = \text{range}(\mathbf{E}_L)$ . This

implies that there is some nonsingular matrix  $\mathbf{T} \in \mathbb{C}^{M \times M}$  such that

$$\mathbf{U}_M = \mathbf{E}_L \mathbf{T}. \quad (2.22)$$

Now consider the following two matrices:

$$\mathbf{U}_{M1} = \mathbf{E}_{L1} \mathbf{T}, \quad (2.23a)$$

$$\mathbf{U}_{M2} = \mathbf{E}_{L1} \mathbf{Z}_D^{(1)} \mathbf{T}, \quad (2.23b)$$

$$\mathbf{C}^{L^{(1)}(L^{(2)}-1) \times M} \ni \mathbf{E}_{L1} = \begin{bmatrix} \mathbf{Z}_L^{(2)} \\ \mathbf{Z}_L^{(2)} \mathbf{Z}_D^{(1)} \\ \vdots \\ \mathbf{Z}_L^{(2)} \mathbf{Z}_D^{(1)L^{(1)}-2} \end{bmatrix}. \quad (2.23c)$$

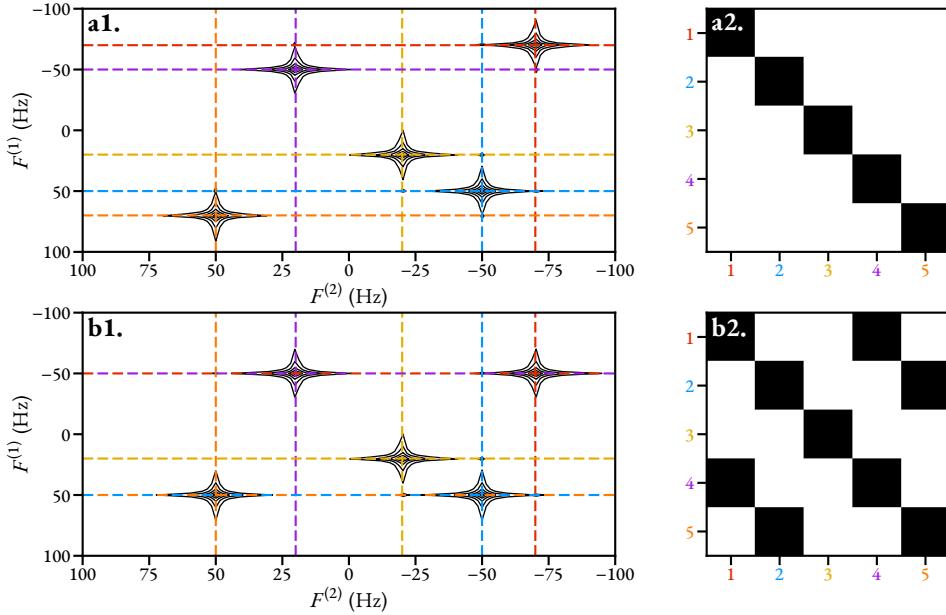
$\mathbf{E}_{L1}$  is derived from  $\mathbf{E}_L$  through the removal of its last  $L^{(2)}$  rows. As such,  $\mathbf{U}_{M1}$  and  $\mathbf{U}_{M2}$  correspond to the  $\mathbf{U}_M$  with the last and first  $L^{(2)}$  rows removed, respectively. The matrix pencil for  $\mathbf{U}_{M1}$  and  $\mathbf{U}_{M2}$  can be expressed as

$$\mathbf{U}_{M1} - \lambda \mathbf{U}_{M2} = \mathbf{E}_{L1} \left( \mathbf{Z}_D^{(1)} - \lambda \mathbf{I}_M \right) \mathbf{T}. \quad (2.24)$$

As seen previously, this matrix structure implies that the signal poles in the first dimension  $\mathbf{z}^{(1)}$  are the solutions of the generalised eigenvalue problem for  $\mathbf{U}_{M1} - \lambda \mathbf{U}_{M2}$ , such that they are the eigenvalues of  $\mathbf{U}_{M1}^+ \mathbf{U}_{M2}$ .

To extract the signal poles in the other dimension,  $\mathbf{z}^{(2)}$ , the permutation matrix  $\mathbf{P} \in \mathbb{R}^{L^{(1)}L^{(2)} \times L^{(1)}L^{(2)}}$  is defined:

$$\mathbf{P} = \begin{bmatrix} e(1) \\ e(1 + L^{(2)}) \\ \vdots \\ e(1 + (L^{(1)} - 1)L^{(2)}) \\ e(2) \\ e(2 + L^{(2)}) \\ \vdots \\ e(2 + (L^{(1)} - 1)L^{(2)}) \\ \vdots \\ e(L^{(2)}) \\ e(2L^{(2)}) \\ \vdots \\ e(L^{(1)}L^{(2)}) \end{bmatrix}. \quad (2.25)$$



**Figure 2.1:** A comparison of the structure of the matrix  $\mathbf{G}$  from the MMEMPM (Equation 2.27), for the cases of an FID with **a.** distinct signal poles in  $F^{(1)}$  and **b.** one with repeated signal poles. **a1.** Magnitude-mode spectrum of a hypercomplex 2D FID, with  $M = 5$ , and all indirect-dimension frequencies having distinct values. **b1.** An equivalent spectrum with two pairs of the 5 indirect-dimension frequencies being identical ( $\{1, 4\}$  and  $\{2, 5\}$ ). **a2.** A representation of the matrix  $|\mathbf{G}|$  for the dataset depicted in a1. All values which are greater than  $10^{-10}$  are coloured black, while those that are less than  $10^{-10}$  are white. N.B. all the black values are  $\gg 10^{-10}$ . **b2.** An analogous representation for the dataset in b1. Note that  $\mathbf{G}$  is no longer diagonal, but possesses non-zero off-diagonal elements in agreement with signals with equivalent poles. With an appropriate re-ordering of the rows and columns (i.e. swapping the rows and columns of 2 and 4), this could be recast as a block-diagonal matrix of the form in Equation 2.28, featuring 3 blocks, one which is  $1 \times 1$ , and two which are  $2 \times 2$ .

$e(i) \in \mathbb{R}^{L^{(1)}L^{(2)}}$  corresponds to a unit row vector comprising zeros except for  $e_i = 1$ . Multiplying  $\mathbf{E}_L$  by the permutation matrix leads to a matrix in which the roles of the two sets of signal poles are effectively swapped:

$$\mathbf{E}_{LP} := \mathbf{P}\mathbf{E}_L = \begin{bmatrix} \mathbf{Z}_L^{(1)} \\ \mathbf{Z}_L^{(1)}\mathbf{Z}_D^{(2)} \\ \vdots \\ \mathbf{Z}_L^{(1)}\mathbf{Z}_D^{(2)^{L^{(2)}-1}} \end{bmatrix}. \quad (2.26)$$

Note the similarity of Equation 2.26 with Equation 2.20b, which implies that with the same reasoning as above,  $\mathbf{z}^{(2)}$  can be derived by extracting the eigenvalues of  $\mathbf{U}_{MP1}^+ \mathbf{U}_{MP2}$ , where  $\mathbf{U}_{MP1}$  and  $\mathbf{U}_{MP2}$  correspond to  $\mathbf{P}\mathbf{U}_M$  with the last and first  $L^{(1)}$  rows removed, respectively.

In the original account on the MEMPM, the final stage employed a pairing algorithm in order to assign the uncorrelated signal poles in  $\mathbf{z}^{(1)}$  with  $\mathbf{z}^{(2)}$  [65]. The *modified* MEMPM (MMEMPM) was developed in order to overcome two issues with the pairing algorithm: (a) it is computation-

ally expensive (b) it is prone to return incorrect pairings[66]. The procedure for extracting the paired poles differs slightly depending on whether all the signal poles in  $\mathbf{z}^{(1)}$  are distinct or not. As well as the eigenvalues of  $\mathbf{U}_{M1}^+ \mathbf{U}_{M2}$ , the MMEMPM requires the corresponding eigenvectors too, contained in the matrix  $\mathbf{W}^{(1)}$ . Assuming that there are no repeated poles in  $\mathbf{z}^{(1)\dagger}$ , the following holds:

$$\mathbf{Z}_D^{(2)} \equiv \mathbf{G} = \mathbf{W}^{(1)\dagger} \mathbf{U}_{MP1}^+ \mathbf{U}_{MP2} \mathbf{W}^{(1)}, \quad (2.27)$$

such that the second dimension signal poles can be extracted from the main diagonal of  $\mathbf{G}$  (see panels a1 & a2 of Figure 2.1). If some values in  $\mathbf{z}^{(1)}$  are repeated, the matrix  $\mathbf{G}$  is no longer diagonal, but instead and can be expressed as block-diagonal; assuming there are  $R < M$  unique signal poles  $\mathbf{G}$  may be expressed in the form, allowing for reorganisation of rows and columns:

$$\mathbf{G} = \begin{bmatrix} G_1 & 0 & \cdots & 0 \\ 0 & G_2 & \cdots & 0 \\ \vdots & \vdots & \ddots & \vdots \\ 0 & 0 & \cdots & G_R \end{bmatrix} \quad (2.28)$$

where  $G_r \in \mathbb{C}^{b_r \times b_r}$  is a sub-matrix corresponding to the  $r^{\text{th}}$  unique signal pole with multiplicity  $b_r$  (see panels b1 & b2 of Figure 2.1). Note that  $\sum_{r=1}^R b_r = M$ . When  $b_r > 1$ , the subset of poles  $\mathbf{z}_r^{(2)}$  are determined by computing the eigenvalues of the matrix  $\mathbf{G}_r$ .

With the signal poles in both dimensions determined, the complex amplitudes are finally computed as follows:

$$\boldsymbol{\alpha} = \text{diag}(\mathbf{E}_L^+ \mathbf{E}_Y \mathbf{E}_R^+). \quad (2.29)$$

See Algorithm B.1 for a pseudo-code outline, and Code Listing C.4 for a `PYTHON` implementation of the MMEMPM.

### 2.2.3 Model Order Selection

The MPM and MMEMPM operate under the assumption that the model order  $M$  is known, or at least has been predicted. It is possible that an individual inspecting the NMR spectrum could predict  $M$  based on the number of peaks visible, however subjective means of predicting model order are typically viewed as disadvantageous as they have bias associated with them. On top of this, scenarios may crop up where a user is unable to recognise that certain heavily overlapping peaks in the spectrum constitute a more than one signal, leading to under-estimates of  $M$ . There

---

<sup>†</sup>For the purposes of FID estimation, it is deemed that a given pair  $i, j \in \{1, \dots, M\}$  of poles is repeated if their frequencies satisfy  $|f_i^{(1)} - f_j^{(1)}| < f_{sw}^{(1)}/N^{(1)}$  (recall Equation 2.14c, which states the relationship between a signal pole and its frequency).

are various non-subjective criteria which have been established for estimating the model order of a given signal, with probably the two most prominent being the Akaike information criterion (AIC)[95] and minimum description length (MDL)[96, 97]. Both of these consider a family of potential models which describe a given set of observations, parametrised by the vector  $\theta$ . For the purpose of 1D FID estimation, the family of potential models comprise Equation 2.1b, with variable  $M$ . Both the AIC and MDL take the same general form:

$$\mathcal{C}(k) = -c \ln (\mathcal{L}(\theta^{(*)} | \mathbf{y})) + \mathcal{P}(k) \text{ with } \theta^{(*)} \in \mathbb{R}^{4k} \quad \forall k \in \{0, 1, \dots\}. \quad (2.30)$$

$\mathcal{L}(\theta^{(*)} | \mathbf{y})$  is the likelihood function of a given model with order  $k$  at the MLE  $\theta^{(*)}$ ,  $c \in \mathbb{R}_{>0}$  is a scaling constant, and  $\mathcal{P}$  is a penalising function, which acts to correct for bias. As the model order increases, the likelihood function at the MLE will increase in size, as a model with more parameters will be able to fit a given dataset more accurately. However, as the model order increases, there will become a point where practically all of the deterministic part of the signal has been incorporated into the model, and increasing the model order further leads to the model which also features influence from the noise. The penalising term  $\mathcal{P}(k)$ , which is always increasing, is required in order to obtain a parsimonious model order estimate. Wax and Kailath derived an expression for the likelihood at the MLE for models comprising a summation of complex sinusoids[98]<sup>‡</sup>:

$$\mathcal{L}(\theta^{(*)} \in \mathbb{R}^{4k} | \mathbf{y}) = \left( \frac{\prod_{r=k}^{L-1} \sigma_{r+1}^{1/(L-k)}}{\frac{1}{L-k} \sum_{r=k}^{L-1} \sigma_{r+1}} \right)^{(L-k)N}, \quad (2.31)$$

$\forall k \in \{0, 1, \dots, L-1\}$ .  $\sigma \in \mathbb{R}^L$  is the set of singular values of  $\mathbf{H}_y$ , in decreasing order. The forms of the AIC and MDL are given by

$$\text{AIC}(k) = -2 \ln (\mathcal{L}(\theta^{(*)} | \mathbf{y})) + 2k(2L - k), \quad (2.32a)$$

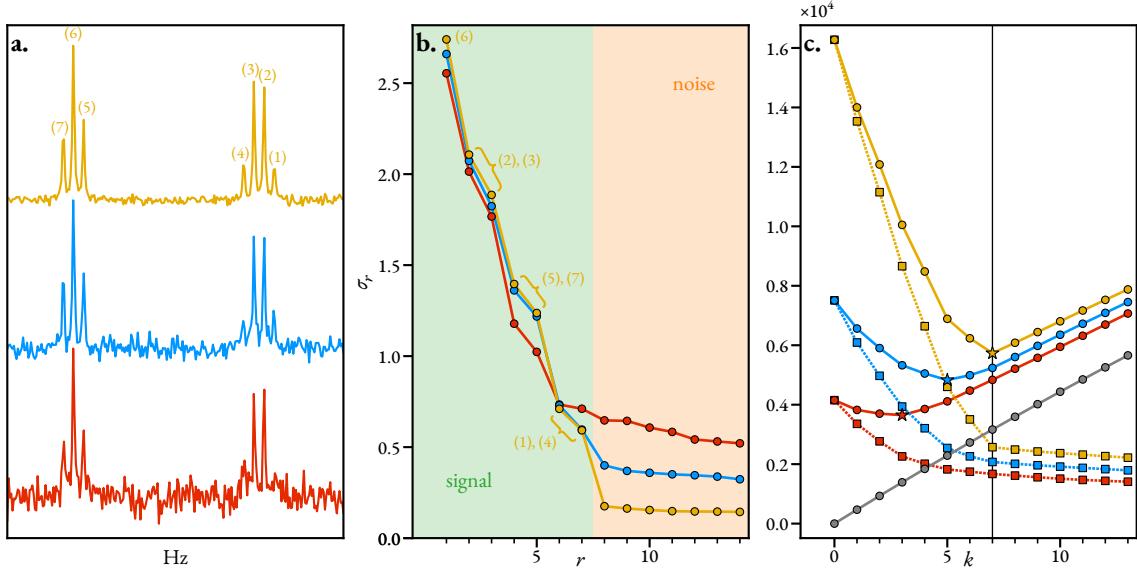
$$\text{MDL}(k) = -\ln (\mathcal{L}(\theta^{(*)} | \mathbf{y})) + \frac{1}{2}k(2L - k) \ln N. \quad (2.32b)$$

The AIC has been shown to be inconsistent in that it tends to overestimate the model order as the number of samples increases[98]. For this reason, the MDL has found greater favour in signal processing applications, and is employed in this work<sup>§</sup>:

$$M = \arg \min_{k \in \mathbb{N}_0: k < L} \text{MDL}(k). \quad (2.33)$$

<sup>‡</sup>The expression in original paper considers the eigenvalues of the covariance matrix for the signal, rather than the singular values of  $\mathbf{H}_y$ . These are equivalent.

<sup>§</sup>In practice, rather than compute the global minimum of the MDL, the first relative minimum is determined (see Algorithm 2.1, Line 20). When  $k$  is very large, it has been noticed that the MDL can spuriously jump in value. This often occurs when FIDs with very high SNRs are analysed; the singular values involved can tend so closely to zero that issues related to the instability of floating-point arithmetic involving these values manifest.



**Figure 2.2:** A visualisation of the behaviour of the MDL for three different FIDs comprising the same deterministic component ( $x$ ) but with different noise instances of differing variances. The model used to construct the FIDs features 7 signals. The three SNRs used were 7 dB (red), 12 dB (blue), and 20 dB (yellow). The FIDs were generated with  $N = 256$ . **a.** Spectra of the three FIDs. **b.** The values of the 14 most significant singular values associated with the Hankel matrix  $H_y$ , with the pencil parameter  $L$  set to  $\lfloor N/3 \rfloor = 85$ . **c.** Square points with dotted lines: The negative log-likelihood at the MLE, i.e. the first term of Equation 2.32b. Grey line: the penalty component of the MDL, given by the second term in Equation 2.32b. Circular points with solid lines: the MDL. Stars denote the minimum of the MDL for a given FID. The 20 dB signal is correctly deemed to have a model order of 7, while the other two are underestimated (predicted models orders are 5 and 3 for the 12 dB and 7 dB FIDs, respectively).

Applying the MDL for model order selection, and subsequently using the MPM for parameter estimation is the basis of the ITMPM[62]. Figure 2.2 illustrates the form of the MDL for three FIDs with equivalent underlying models, comprising 7 signals, and noise instances with different variances. The first 14 singular values of  $H_y$  are plotted in panel b, where it can be seen that beyond the first 7, which account for signal components, the subsequent singular values, decrease at a far slower rate. The noise subspace for FIDs with higher SNRs have singular values which are (a) smaller in magnitude and (b) more consistent, such that distinguishing the noise and signal subspaces is an easier task (cf. the yellow and red lines in panel b). As such, it is perhaps unsurprising that the MDL is more likely to provide a faithful estimate of the FID's model order when the SNR is higher (panel c).

## 2.3 Non-linear programming

### 2.3.1 An overview of NLP

In an optimisation problem, the goal is to determine the minimum<sup>¶</sup> of a function  $\mathcal{F}(\theta) : \mathbb{R}^n \rightarrow \mathbb{R}$ ,  $n \in \mathbb{N}$ , often called the *cost function* or *fidelity*. This is typically with the goal of determining the argument  $\theta^{(*)}$  at which the minimum is found:

$$\theta^{(*)} = \arg \min_{\theta \in \mathbb{R}^n} \mathcal{F}(\theta). \quad (2.34)$$

The above problem is *unconstrained*, as there are no limitations that the parameter vector is subjected to. Unless  $\mathcal{F}(\theta)$  has particular properties, such as convexity<sup>||</sup>, it is generally only possible to determine a *local* minimum, rather than a *global* minimum for high-dimensionality problems such as the one of interest here.  $\theta^{(*)}$  is a local minimiser of  $\mathcal{F}(\theta)$  if there is a neighbourhood  $V \ni \theta^{(*)}$  for which

$$\mathcal{F}(\theta^{(*)}) \leq \mathcal{F}(\theta) \forall \theta \in V. \quad (2.35)$$

$V \subset \mathbb{R}^n$  is a continuous space such that one can move some amount in any direction away from  $\theta^{(*)}$  and still be in  $V$ . Key to NLP are the *necessary conditions*, which define whether a given vector  $\theta$  is a local minimum of the fidelity. The *first necessary condition* states that if  $\mathcal{F}(\theta)$  is continuously differentiable, and  $\theta^{(*)}$  is a local extremum<sup>\*\*</sup> of  $\mathcal{F}(\theta)$ , then the gradient vector  $g(\theta^{(*)}) := \nabla \mathcal{F}(\theta^{(*)})$  is the zero vector:

$$g(\theta^{(*)}) = \mathbf{0} \in \mathbb{R}^n \quad (2.36)$$

The *second necessary condition* subsequently states that if  $\mathcal{F}(\theta)$  and  $g(\theta)$  are continuously differentiable, and  $\theta^{(*)}$  is a local minimiser of  $\mathcal{F}(\theta)$ , then the Hessian matrix  $H(\theta^{(*)}) := \nabla^2 \mathcal{F}(\theta^{(*)})$  is positive semidefinite, i.e.

$$\mathbf{v}^T H(\theta^{(*)}) \mathbf{v} \geq 0 \quad \forall \mathbf{v} \in \mathbb{R}^n. \quad (2.37)$$

Furthermore, it is a *unique* local minimiser if the *second-order sufficient condition* is also satisfied, i.e. that the Hessian is positive definite:

$$\mathbf{v}^T H(\theta^{(*)}) \mathbf{v} > 0 \quad \forall \mathbf{v} \in \mathbb{R}^n. \quad (2.38)$$

---

<sup>¶</sup>In certain applications, the interest could actually be to find the maximum of a function. However, it is trivial to transform a maximisation problem into a minimisation problem by finding the minimum of negative of the function.

<sup>||</sup>A convex function is one such that a line segment through any two points of the function lies above it.

<sup>\*\*</sup>“Extremum” is used here instead of “minimum”, as the first necessary condition applies to maxima of a function as well as minima.

A plethora of approaches have been established to determine local minima of scalar functions. One of the better-known strategies is *Newton's method*, in which a quadratic approximation of the fidelity is considered. For a given iteration  $k \in \mathbb{N}_0$ , the fidelity is approximated using

$$\mathcal{F}_Q(\theta) = \mathcal{F}(\theta^{(k)}) + \mathbf{b}^T \mathbf{g}(\theta^{(k)}) + \frac{1}{2} \mathbf{b}^T \mathbf{H}(\theta^{(k)}) \mathbf{b}, \quad (2.39)$$

where  $\mathbf{b} = \theta - \theta^{(k)}$ . An updated prediction of the parameter vector is derived by finding the minimum of this quadratic approximation:

$$\begin{aligned} \frac{\partial \mathcal{F}(\theta)}{\partial \mathbf{b}} &= \mathbf{g}(\theta^{(k)}) + \mathbf{H}(\theta^{(k)}) \mathbf{b} \\ \implies 0 &= \mathbf{g}(\theta^{(k)}) + \mathbf{H}(\theta^{(k)}) (\theta^{(k+1)} - \theta^{(k)}) \\ \therefore \theta^{(k+1)} &= \theta^{(k)} - \mathbf{H}(\theta^{(k)})^{-1} \mathbf{g}(\theta^{(k)}). \end{aligned} \quad (2.40)$$

This process is repeated, until the convergence criterion has been met:

$$\|\mathbf{g}(\theta^{(k)})\| \leq \epsilon. \quad (2.41)$$

The convergence threshold  $\epsilon > 0$  can be tuned based on the desired accuracy of the result. Equation 2.40 tends not to be used as the update formula in real optimisation problems; one of the major downsides of the Newton update is the possibility that it is not a minimising update if the Hessian is not positive definite. Two primary strategies have emerged which are typically used instead:

- *Line search methods*[88: Chapter 3] determine an appropriate direction  $\mathbf{p}^{(k)}$  along which the updated parameter vector is sourced. After this, an appropriate step length  $\alpha^{(k)}$  is determined — typically in an efficient, though not optimal manner — leading to  $\theta^{(k+1)} = \theta^{(k)} - \alpha^{(k)} \mathbf{p}^{(k)}$ .
- *Trust region methods*[88: Chapter 4] define a radius  $\Delta^{(k)} > 0$ , and determine the minimum of Equation 2.39 subject to the constraint that  $\|\mathbf{b}\| \leq \Delta^{(k)}$ .

A trust region method is applied in this work, and as such further consideration of it will now be made.

The structure of a typical trust region method is presented in Algorithm 2.2 (ignoring Lines 19 to 22, which is a custom addition, see Section 2.3.5). An initial radius for the trust region  $\Delta^{(0)}$  is defined, along with a maximum permitted radius  $\Delta_{\max}$ , to ensure that excessively adventurous

**Algorithm 2.2** NLP routine employed in this work. This makes use of Algorithms 4.1 & 7.2 in [88], with a extra check inserted to deal with any negative-amplitude oscillators which may be generated as the routine evolves (Lines 19 to 22).

---

```

1: procedure NLP( $Y \in \mathbb{C}^{N^{(1)} \times \dots \times N^{(D)}}$ ,  $\theta^{(0)} \in \mathbb{R}^{2(D+1)M}$ )
2:    $\Delta^{(0)} \leftarrow 1/10 \|g(\theta^{(0)} | Y)\|;$ 
3:    $\Delta_{\max} \leftarrow 16\Delta^{(0)};$ 
4:   for  $k = 0, 1, \dots$  do
5:      $p^{(k)} \leftarrow \text{STEIHAUGTOINT}(Y, \theta^{(k)}, \Delta^{(k)})$ ; ▷ See Algorithm B.2
6:      $\rho^{(k)} \leftarrow \frac{\mathcal{F}_\phi(\theta^{(k)}) - \mathcal{F}_\phi(\theta^{(k)} + p^{(k)})}{\mathcal{F}_{\phi Q}(\theta^{(k)}) - \mathcal{F}_{\phi Q}(\theta^{(k)} + p^{(k)})};$ 
7:     if  $\rho_k < 1/4$  then
8:        $\Delta^{(k+1)} \leftarrow 1/4\Delta^{(k)};$ 
9:     else if  $\rho_k > 3/4$  and  $\|p^{(k)}\| = \Delta^{(k)}$  then
10:       $\Delta^{(k+1)} \leftarrow \min(2\Delta^{(k)}, \Delta_{\max});$ 
11:    else
12:       $\Delta^{(k+1)} \leftarrow \Delta^{(k)};$ 
13:    end if
14:    if  $\rho^{(k)} > 3/20$  then
15:       $\theta^{(k+1)} \leftarrow \theta^{(k)} + p^{(k)};$ 
16:    else
17:       $\theta^{(k+1)} \leftarrow \theta^{(k)};$ 
18:    end if
19:    if  $k \bmod 25 = 0$  and  $\theta^{(k+1)}$  contains negative amplitudes then
20:       $\theta^{(0)} \leftarrow \theta^{(k+1)}$  with negative-amplitude oscillators removed;
21:       $\theta^{(*)}, \epsilon^{(*)} \leftarrow \text{NLP}(Y, \theta^{(0)})$ ;
22:    end if
23:    if  $\|g(\theta^{(k+1)})\| < 10^{-8}$  then
24:      break;
25:    end if
26:  end for
27:   $\theta^{(*)} \leftarrow \theta^{(k+1)}$ 
28:   $\epsilon^{(*)} \leftarrow \sqrt{\frac{\mathcal{F}(\theta^{(*)}) \text{diag}([H(\theta^{(*)})]^{-1})}{(N^{(1)} \dots N^{(D)})^{-1}}}$ 
29:  return  $\theta^{(*)}, \epsilon^{(*)}$ ;
30: end procedure

```

---

steps do not take place. For each iteration, a solution to the following sub-problem is sought:

$$\begin{aligned} \mathbf{p}^{(k)} = \arg \min_{\mathbf{p} \in \mathbb{R}^n} \mathcal{F}(\boldsymbol{\theta}^{(k)}) + (\boldsymbol{\theta}^{(k)} + \mathbf{p})^\top \mathbf{g}(\boldsymbol{\theta}^{(k)}) + \frac{1}{2} (\boldsymbol{\theta}^{(k)} + \mathbf{p})^\top \mathbf{H}(\boldsymbol{\theta}^{(k)}) (\boldsymbol{\theta}^{(k)} + \mathbf{p}) \\ \text{subject to } \|\mathbf{p}\| \leq \Delta^{(k)}. \end{aligned} \quad (2.42)$$

This sub-problem is not usually minimised exactly, but instead an efficient means of determining a sufficiently good update is used. Common approaches include computing the Cauchy point, the Dogleg method, and a truncated conjugate-gradient approach commonly called the Steihaug-Toint (ST) method[88: Chapter 7]. The latter is employed in this work (see Algorithm B.2 and Code Listing C.5). In the ST approach, iterates of the conjugate-gradient method[88: Chapter 5] are computed, either until an iterate which is outside the trust region is computed, or negative curvature is discovered.

Once a provisional update  $\boldsymbol{\theta}^{(k+1)} = \boldsymbol{\theta}^{(k)} + \mathbf{p}^{(k)}$  is determined using the ST method, a metric is considered which indicates how well the quadratic estimate agrees with the true value of the fidelity:

$$\rho^{(k)} = \frac{\mathcal{F}(\boldsymbol{\theta}^{(k)}) - \mathcal{F}(\boldsymbol{\theta}^{(k)} + \mathbf{p}^{(k)})}{\mathcal{F}_Q(\boldsymbol{\theta}^{(k)}) - \mathcal{F}_Q(\boldsymbol{\theta}^{(k)} + \mathbf{p}^{(k)})}. \quad (2.43)$$

$\rho^{(k)}$  is the ratio between the actual reduction of the fidelity caused by taking the proposed step, and the predicted reduction based on the quadratic model. If  $\rho^{(k)}$  is sufficiently close to 1, the quadratic model being used to generate new iterates is deemed to be acting well enough to warrant accepting the proposed update (Lines 14 and 15). Furthermore, if  $\rho^{(k)}$  is particularly close to 1, and the proposed update is at the boundary of the trust radius, it is appropriate to enlarge the radius of the trust region for the next iteration in an attempt to increase the rate of convergence (Lines 9 and 10). On the other hand, a small value of  $\rho^{(k)}$  implies that the quadratic model reflects the true fidelity poorly, such that the proposed update should be rejected (Lines 16 and 17). As well as this, the trust region's radius should be decreased such that the model is more likely to behave faithfully (Lines 7 and 8). In general, the thresholds which dictate whether to accept an update, and whether to adjust the trust region radius are customisable. The hard-coded numerical values found in Algorithm 2.2 are the values used for the results presented in this work.

### 2.3.2 NLP applied to FID estimation

Focus now turns to the specific problem of FID estimation using NLP, for which a general  $D$ -dimensional dataset will be considered. As established in Section 2.1, the fidelity  $\mathcal{F}(\boldsymbol{\theta} | \mathbf{Y}) : \mathbb{C}^{N^{(1)} \times \dots \times N^{(D)}} \times \mathbb{R}^{2(1+D)M} \rightarrow \mathbb{R}$  is given by

$$\mathcal{F}(\boldsymbol{\theta} | \mathbf{Y}) = \|\mathbf{Y} - \mathbf{X}(\boldsymbol{\theta})\|^2. \quad (2.44)$$

The elements of the gradient vector  $\mathbf{g}(\boldsymbol{\theta} | \mathbf{Y}) \in \mathbb{R}^{2(1+D)M}$  and the Hessian matrix  $\mathbf{H}(\boldsymbol{\theta} | \mathbf{Y}) \in \mathbb{R}^{2(1+D)M \times 2(1+D)M}$  are derived by taking the first and second partial derivatives of the fidelity with respect to the elements in  $\boldsymbol{\theta}$ :

$$g_i = -2\Re \left( (\mathbf{Y} - \mathbf{X}), \frac{\partial \mathbf{X}}{\partial \theta_i} \right), \quad (2.45a)$$

$$b_{i,j} = 2\Re \left( \underbrace{\left( \frac{\partial \mathbf{X}}{\partial \theta_i}, \frac{\partial \mathbf{X}}{\partial \theta_j} \right)}_{(1)} - \underbrace{\left( (\mathbf{Y} - \mathbf{X}), \frac{\partial^2 \mathbf{X}}{\partial \theta_i \partial \theta_j} \right)}_{(2)} \right), \quad (2.45b)$$

$\forall i, j \in \{1, \dots, 2(1+D)M\}$ . The complete set of first and second derivatives of a particular element of the model  $x := x_{n^{(1)}, \dots, n^{(D)}}$ , given by Equation 2.1b, is as follows  $\forall m \in \{1, \dots, M\}$ ,  $\forall d, d' \in \{1, \dots, D\}$ :

*First derivatives*

$$\frac{\partial x}{\partial \theta_m} \equiv \frac{\partial x}{\partial a_m} = \frac{x}{a_m}, \quad (2.46a)$$

$$\frac{\partial x}{\partial \theta_{m+M}} \equiv \frac{\partial x}{\partial \phi_m} = ix, \quad (2.46b)$$

$$\frac{\partial x}{\partial \theta_{m+(d+1)M}} \equiv \frac{\partial x}{\partial f_m^{(d)}} = 2\pi i \Delta_t^{(d)} n^{(d)} x, \quad (2.46c)$$

$$\frac{\partial x}{\partial \theta_{m+(d+D+1)M}} \equiv \frac{\partial x}{\partial \eta_m^{(d)}} = -\Delta_t^{(d)} n^{(d)} x. \quad (2.46d)$$

*Second derivatives*

$$\frac{\partial^2 x}{\partial \theta_m^2} \equiv \frac{\partial^2 x}{\partial a_m^2} = 0, \quad (2.47a)$$

$$\frac{\partial^2 x}{\partial \theta_m \partial \theta_{m+M}} \equiv \frac{\partial^2 x}{\partial a_m \partial \phi_m} = \frac{ix}{a_m}, \quad (2.47b)$$

$$\frac{\partial^2 x}{\partial \theta_m \partial \theta_{m+(d+1)M}} \equiv \frac{\partial^2 x}{\partial a_m \partial f_m^{(d)}} = \frac{2\pi i \Delta_t^{(d)} n^{(d)} x}{a_m}, \quad (2.47c)$$

$$\frac{\partial^2 x}{\partial \theta_m \partial \theta_{m+(d+D+1)M}} \equiv \frac{\partial^2 x}{\partial a_m \partial \eta_m^{(d)}} = \frac{-\Delta_t^{(d)} n^{(d)} x}{a_m}, \quad (2.47d)$$

$$\frac{\partial^2 x}{\partial \theta_{m+M}^2} \equiv \frac{\partial^2 x}{\partial \phi_m^2} = -x, \quad (2.47e)$$

$$\frac{\partial^2 x}{\partial \theta_{m+M} \partial \theta_{m+(d+1)M}} \equiv \frac{\partial^2 x}{\partial \phi_m \partial f_m^{(d)}} = -2\pi \Delta_t^{(d)} n^{(d)} x, \quad (2.47f)$$

Dimensions	# 1 <sup>st</sup> derivatives	# 2 <sup>nd</sup> derivatives
1	$4MN^{(1)}$	$9MN^{(1)}$
2	$6MN^{(1)}N^{(2)}$	$20MN^{(1)}N^{(2)}$
3	$8MN^{(1)}N^{(2)}N^{(3)}$	$35MN^{(1)}N^{(2)}N^{(3)}$
$D$	$2(1+D)M\mathfrak{N}$	$((1+D)(3+2D)-1)M\mathfrak{N}$

**Table 2.1:** The number of first and second derivatives that are necessary to compute the gradient vector and Hessian matrix of the fidelity for 1- 2- and 3-dimensional datasets, as well as a general  $D$ -dimensional dataset.

$$\frac{\partial^2 x}{\partial \theta_{m+M} \partial \theta_{m+(d+D+1)M}} \equiv \frac{\partial^2 x}{\partial \phi_m \partial \eta_m^{(d)}} = -i \Delta_t^{(d)} n^{(d)} x, \quad (2.47g)$$

$$\frac{\partial^2 x}{\partial \theta_{m+(d+1)M} \partial \theta_{m+(d'+1)M}} \equiv \frac{\partial^2 x}{\partial f_m^{(d)} \partial f_m^{(d')}} = -4\pi^2 \left( \Delta_t^{(d)} n^{(d)} \right) \left( \Delta_t^{(d')} n^{(d')} \right) x, \quad (2.47h)$$

$$\frac{\partial^2 x}{\partial \theta_{m+(d+1)M} \partial \theta_{m+(d'+D+1)M}} \equiv \frac{\partial^2 x}{\partial f_m^{(d)} \partial \eta_m^{(d')}} = -2\pi i \left( \Delta_t^{(d)} n^{(d)} \right) \left( \Delta_t^{(d')} n^{(d')} \right) x, \quad (2.47i)$$

$$\frac{\partial^2 x}{\partial \theta_{m+(d+D+1)M} \partial \theta_{m+(d'+D+1)M}} \equiv \frac{\partial^2 x}{\partial \eta_m^{(d)} \partial \eta_m^{(d')}} = \left( \Delta_t^{(d)} n^{(d)} \right) \left( \Delta_t^{(d')} n^{(d')} \right) x, \quad (2.47j)$$

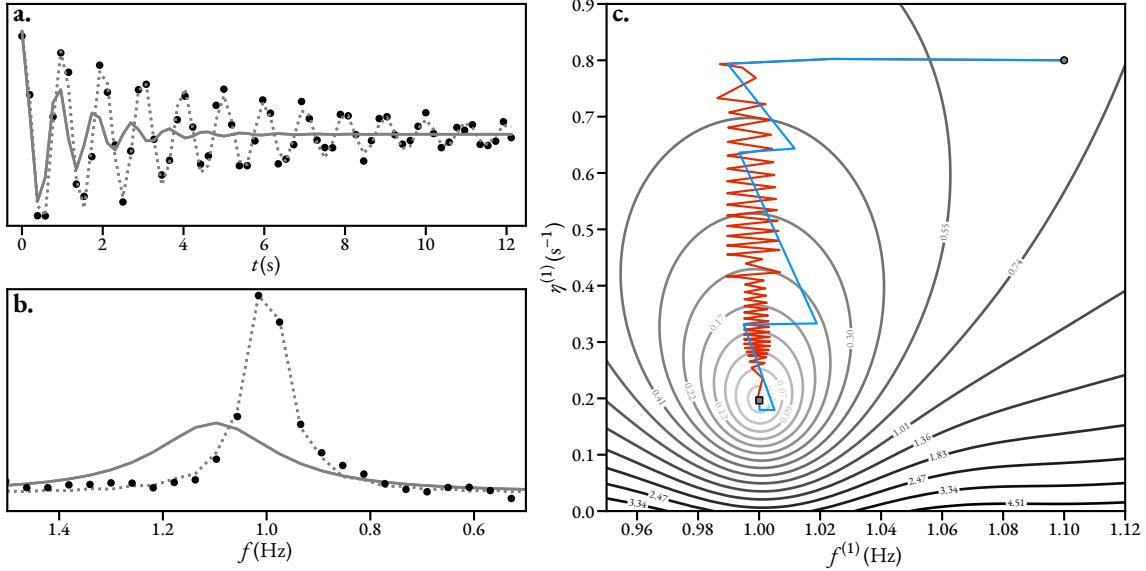
$$\frac{\partial^2 x}{\partial \theta_i \partial \theta_j} = \frac{\partial^2 x}{\partial \theta_j \partial \theta_i}, \quad (2.47k)$$

$$\frac{\partial^2 x}{\partial \theta_i \partial \theta_j} = 0 \text{ if not specified above.} \quad (2.47l)$$

Equation 2.47l indicates that any second derivative with respect to two parameters which do not belong to the same oscillator in then model will always be 0. This, along with the symmetrical nature of the second derivatives (Equation 2.47k) drastically reduces the required number to explicitly compute, from  $4(1+D)^2 M^2$  per data-point to  $(1+D)(3+2D)M$ . Finally, Equation 2.47a indicates that another  $M$  second derivatives do not need to be computed, as they are always 0. See Table 2.1 for the total number of derivatives that need to be computed for datasets with different numbers of dimensions.

### 2.3.3 Approximating the Hessian

Despite many of the model second derivatives being 0, computation of those that are not zero, and subsequently using these the form the Hessian matrix, can be an expensive part of the optimisation routine. Numerous optimisation problems exist where this is the case, and as such there is considerable precedent for improving the efficiency of optimisation algorithms by generating approximations of the Hessian which are demanding to compute. Examples include the Gauss-Newton (GN) method and LM algorithm, which are specifically for RSS problems[88: Chapter



**Figure 2.3:** A visualisation of the trajectory of a 2-parameter optimisation involving a simulated FID comprising a single signal. **a.** & **b.** Representations of the signal in the time domain and Fourier domain, respectively. Black dots: the signal to be estimated  $y$ . Solid grey line: the model generated using the initial guess  $x(\theta^{(0)})$ . Dotted grey line: the model generated using the optimised result,  $x(\theta^{(*)})$ . **c.** A contour plot of the fidelity. Blue line: the trajectory of the parameter vector with the true Hessian matrix used in computing each update. Red line: the analogous trajectory using the Hessian approximation in place of the true Hessian.

[10], as well as quasi-Newton methods such as the Broyden-Fletcher-Goldfarb-Shanno (BFGS) method[88: Chapter 6].

The GN and LM approaches replace the true Hessian matrix at each iteration with the following expression:

$$b_{i,j} = 2\Re \left\{ \frac{\partial X}{\partial \theta_i}, \frac{\partial X}{\partial \theta_j} \right\}, \quad (2.48)$$

i.e. term ② in Equation 2.45b, which involves the model second derivatives, is neglected. All that needs to be generated is the Jacobian  $J = \partial X / \partial \theta$ . This can bring a very large reduction in the computational cost, as no extra derivatives need to be computed for the Hessian at all, since the Jacobian is already required for generating the gradient vector. In situations where the residuals between the data and model are small, term ① will tend to dominate term ②, and as such these methods often enjoy a convergence rate which is comparable to that of Newton's method when close to local minima. Despite this, by invoking this approximation, the rate of convergence, i.e. the number of iterations required to reach  $\theta^{(*)}$ , tends to be adversely affected. See Section 2.3.4 for an example of this phenomenon.

### 2.3.4 Visualisation of a simple example

Figure 2.3 provides a visual example of the application of NLP to estimate a simulated 1D FID comprising a single signal. The FID was constructed using Equation 1.22 with  $M = 1$ ,  $N = 64$ ,  $f_{\text{sw}} = 5.2 \text{ Hz}$  ( $\Delta_t \approx 0.192 \text{ s}$ ), and  $f_{\text{off}} = 0 \text{ Hz}$ . The signal was parameterised by  $\theta \in \mathbb{R}^4$  comprising  $a = 1$ ,  $\phi = 0 \text{ rad}$ ,  $f = 1 \text{ Hz}$ ,  $\eta = 0.2 \text{ s}^{-1}$ . AWGN was added to the FID to give it an SNR of approximately 10 dB. As the visualisation of 5D space is beyond the scope of this work, only two parameters, the frequency and damping factor, were optimised from an initial guess  $\theta^{(0)}$ ; the amplitude and phase were fixed to their true values throughout. The initial guess comprised a frequency of 1.1 Hz, and a damping factor of  $0.8 \text{ s}^{-1}$ , with the solid grey lines in panels a & b denoting the model generated in the time- and Fourier-domains, respectively.  $\theta^{(0)}$  was subjected to NLP twice. In the first instance, the exact Hessian matrix, given by Equation 2.45b was used in order to compute each update step, while in the second the Hessian approximation given by Equation 2.48 was used. The initial radius of the trust region was set to  $1/10$  of the gradient norm ( $\approx 0.3$ ), which has a precedent in the literature[99]. The trajectories of the parameter vector are denoted by coloured lines in panel c. In both cases, the NLP routine successfully converged at a result  $\theta^{(*)}$  in agreement with the true frequency and damping factor used to construct the FID. However, it is clear that using the true Hessian matrix (blue) led to a far better rate of convergence compared with the approximated analogue (red), which exhibited “zig-zagging”<sup>††</sup>. 14 iterations were required to reach the convergence criterion  $\epsilon \leq 10^{-8}$  when the true Hessian was used, while 81 were required for the approximated case. Despite being an anecdotal example, this highlights that use of the true Hessian matrix tends to allow a better rate of convergence. However, for FIDs comprising many signals and far more points, the approximated form often requires a shorter time to converge overall, especially for 2D FIDs, as will be illustrated in Section 2.4.

### 2.3.5 Phase Variance Minimisation

An NLP procedure tasked with minimising the discrepancy between the model  $X$  and the observed data  $Y$  is well-suited to produce an accurate holistic representation of the data, assuming a sufficiently large model order is used. However, as has already been discussed, this is not necessarily sufficient due to the ill-posed nature of the estimation problem. It is desirable to produce an estimate which not only achieves a good fit to the data in an RSS sense, but which is also in agreement with the process underpinning the observation. It is for this reason that iterative procedures typically require significant quantities of prior knowledge, beyond basic assumptions of the underlying model, in order to produce meaningful estimation results. This is also why they are often able to produce results which agree better with a spectroscopist’s conception of what

<sup>††</sup>This phenomenon is often seen in gradient descent methods, in which each update occurs along the opposite direction to the gradient.

the “correct” parameter estimate should look like, relative to other methods where such detailed information is not exploited.

While the MPM is often able to generate seemingly reasonable parameter estimates, one particular feature has been noticed in many of its results: often, oscillators in the result exhibit spurious phase behaviour. As has been discussed (Section 1.2.1), NMR datasets for most experiments comprise signals whose phases depend on their resonance frequencies to first order. This is routinely corrected in conventional NMR spectral processing, such that all signals are adjusted to acquire a phase of 0 rad. This feature of the dataset can be exploited in order to overcome the aforementioned shortcoming of the MPM, through appropriate regularisation of the NLP routine. Assuming that the data has been phase corrected<sup>#</sup>, incorporating the variance of oscillator phases into the fidelity can lead to improved estimation results; examples of this will be provided later (Section 3.1). The updated fidelity becomes

$$\mathcal{F}_\phi(\boldsymbol{\theta} | \mathbf{Y}) = \|\mathbf{Y} - \mathbf{X}(\boldsymbol{\theta})\|^2 + \text{Var}_o(\boldsymbol{\phi}), \quad (2.49)$$

where  $\text{Var}_o(\boldsymbol{\phi})$  is the *circular variance* of the oscillator phases. Oscillator phases are an example of a circular variable, as all phases are wrapped within an interval of size  $2\pi$  rad. Given an unwrapped phase  $\tilde{\phi} \in \mathbb{R}$ , the corresponding wrapped phase  $\phi \in (-\pi, \pi]$  is given by

$$\phi = (\tilde{\phi} + \pi) \bmod 2\pi - \pi. \quad (2.50)$$

This makes the conventional (linear) definition of variance, given by

$$\text{Var}_l(\boldsymbol{\phi}) = \frac{1}{M} \sum_{m=1}^M (\phi_m - \mu(\boldsymbol{\phi}))^2, \quad (2.51a)$$

$$\mu(\boldsymbol{\phi}) = \frac{1}{M} \sum_m \phi_m, \quad (2.51b)$$

unsuitable as a metric to define the variation in phases. Consider as a simple example a scenario where there are two oscillators with phases  $\tilde{\boldsymbol{\phi}} = [\pi + \delta \ \pi - \delta]^T$  for some small  $\delta$ . The phase variance is expected to be small as the phases are similar. However, with the inclusion of wrapping through application of Equation 2.50, these phases would actually be set to  $\boldsymbol{\phi} = [-\pi + \delta \ \pi - \delta]^T$ , and the linear phase variance would be large. It is therefore apparent that a definition of variance

---

<sup>#</sup>Rather than rely on the data being phase-corrected, one could envisage replacing the phase variance with a term which guides the oscillators to adopt a first-order phase relationship. The reason why the phase variance has been chosen is two-fold: (i) Applying phase-correction to NMR data is straightforward and can be automated, meaning the user would experience minimal burden. (ii) As will be discussed in Section 2.5, it is beneficial to have a spectrum comprising pure absorption-mode Lorentzians in order to produce frequency-filtered “sub-FIDs” from the original data, so the data being estimated will be phase-corrected anyway.

which accounts for the periodicity of the phases is needed. The circular variance is defined as[100: Chapter 3]

$$[0, 1] \ni \text{Var}_o(\phi) = 1 - \frac{R}{M}, \quad (2.52a)$$

$$R = \sqrt{c_{\Sigma}^2 + s_{\Sigma}^2}, \quad (2.52b)$$

$$c_{\Sigma} = \sum_{m=1}^M \cos \phi_m, \quad (2.52c)$$

$$s_{\Sigma} = \sum_{m=1}^M \sin \phi_m. \quad (2.52d)$$

$R$  is the length of the resultant vector produced by summing  $M$  unit vectors with angles given by  $\phi$ . In the case that all the vectors have the same angle,  $R = M$ , leading to the variance being 0 as expected. At the other extreme, with  $M$  vectors uniformly separated about the unit circle — such that there is an angle of  $2\pi/M-1$  rad between all pairs of adjacent vectors — the vectors will perfectly cancel, leading to  $R = 0$ . In this case, the maximum variance of 1 is obtained. The inclusion of the phase variance into the fidelity is one of the motivating reasons for normalising the data prior to estimation (see ??). Since  $\text{Var}_o(\phi)$  is constrained to the interval  $[0, 1]$ , if the data were not normalised it is likely that  $\|Y - X\|^2$  would dominate  $\text{Var}_o(\phi)$  in Equation 2.49, such that the influence of the phase variance would be negligible.

The first and second derivatives of the circular variance are required for the computation of the gradient vector and Hessian matrix, whose updated forms are

$$g_i = -2\Re \left\langle (Y - X), \frac{\partial X}{\partial \theta_i} \right\rangle + \frac{\partial \text{Var}_o(\phi)}{\partial \theta_i}, \quad (2.53a)$$

$$b_{i,j} = 2\Re \left( \left\langle \frac{\partial X}{\partial \theta_i}, \frac{\partial X}{\partial \theta_j} \right\rangle - \underbrace{\left\langle (Y - X), \frac{\partial^2 X}{\partial \theta_i \partial \theta_j} \right\rangle}_{\text{Neglected if approximation used}} \right) + \frac{\partial^2 \text{Var}_o(\phi)}{\partial \theta_i \partial \theta_j}. \quad (2.53b)$$

The derivatives of the phase variance are given by:

$$\frac{\partial \text{Var}_o(\phi)}{\partial \theta_i} = \begin{cases} \frac{1}{RM} (c_{\Sigma} \sin \phi_{i-M} - s_{\Sigma} \cos \phi_{i-M}) & M \leq i < 2M \\ 0 & \text{otherwise} \end{cases} \quad (2.54a)$$

$$\frac{\partial^2 \text{Var}_o(\phi)}{\partial \theta_i \partial \theta_j} = \begin{cases} \frac{1}{RM} \left[ \frac{1}{R^2} (c_\Sigma \sin \phi_{i-M} - s_\Sigma \cos \phi_{i-M})^2 + c_\Sigma \cos \phi_{i-M} + s_\Sigma \sin \phi_{i-M} - 1 \right] & M \leq i, j < 2M, i = j \\ \frac{1}{RM} \left[ \frac{1}{R^2} (c_\Sigma \sin \phi_{i-M} - s_\Sigma \cos \phi_{i-M}) \times (c_\Sigma \sin \phi_{j-M} - s_\Sigma \cos \phi_{j-M}) - \cos(\phi_{i-M} - \phi_{j-M}) \right] & M \leq i, j < 2M, i \neq j \\ 0 & \text{otherwise} \end{cases} \quad (2.54b)$$

The phase variance-regularised fidelity (Equation 2.49) is minimised according the unconstrained NLP routine described above. It is therefore possible for oscillators to acquire parameters which are unrealistic as the optimiser evolves (see Page 11 for an outline of the expected ranges that the parameters reside in). With the inclusion of the variance of oscillator phases, there are situations where oscillators acquire negative amplitudes. Typically, this occurs when there are oscillators in the MPM result which start out with phases that are far from 0 rad. By acquiring a negative amplitude and a phase close to 0 rad — the expected phase of most oscillators in the parameter set — little change to the RSS term is made, while  $\text{Var}_o(\phi)$  will be reduced. The presence of such oscillators is undesirable, as they are spurious in the context of phased data. As a result, the NLP routine periodically checks for negative-amplitude oscillators (Lines 19 to 22 in Algorithm 2.2). After a given number of iterations (25 is the value given in Algorithm 2.2) if any oscillators have acquired negative amplitudes, these are removed from the model, and the routine continues with a reduced number of oscillators. While not infallible, this can help to get rid of excessive oscillators in the model which do not correspond to true signals in the data. For example, in scenarios where an overestimate of model order has occurred, noise components will be incorporated into the MPM result. These typically have greater variability in their phases; often, such oscillators gain negative amplitudes as the NLP routine evolves, leading to unwanted signals being removed and a more parsimonious result being obtained.

## 2.4 Profiling the MPM and NLP

The routine described for FID estimation involves operations which can be computationally demanding, with the burden on computational resources increasing with the number of points in the FID, as well as the number of oscillators in the model. This is the case both in terms of the amount of work done by the central processing unit (CPU), and the amount of random access memory (RAM) needed to store all the required data as the routine runs. For the MPM, the most demanding aspect is SVD calculations while for numerical optimisation, it is generation of the Hessian matrix in each iteration. Detailed accounts of the computational complexity of the MPM and MMEMPM have been presented[65, 66]. However, it is useful to consider what the

actual run times of these routines are on a modern computer; a lot of accounts on the MPM are from decades before this work, and so the run time will have decreased considerably thanks to improvements in processing power. As an example, the account by Pines a co-workers from 1997 outlining the ITMPM states that a signal comprising 1024 points would take about 4.5 min to be processed by the MDL and MPM, using a 100 MHz CPU[62]. On the system used for all results generated for this work (see Remark 3) an equivalent computation takes about 100 ms. PYTHON implementations of the aforementioned parts of the estimation routine were run, with profiling software used to assess both the line-by-line execution times[101], and the time-dependent RAM usage[102].

**Remark 3.** *All results generated in this work were acquired using a workstation featuring a Intel® Core™ i9-10900X CPU @ 3.7 GHz, and 32 GiB of RAM.*

### 2.4.1 The MPM and MMEMPM

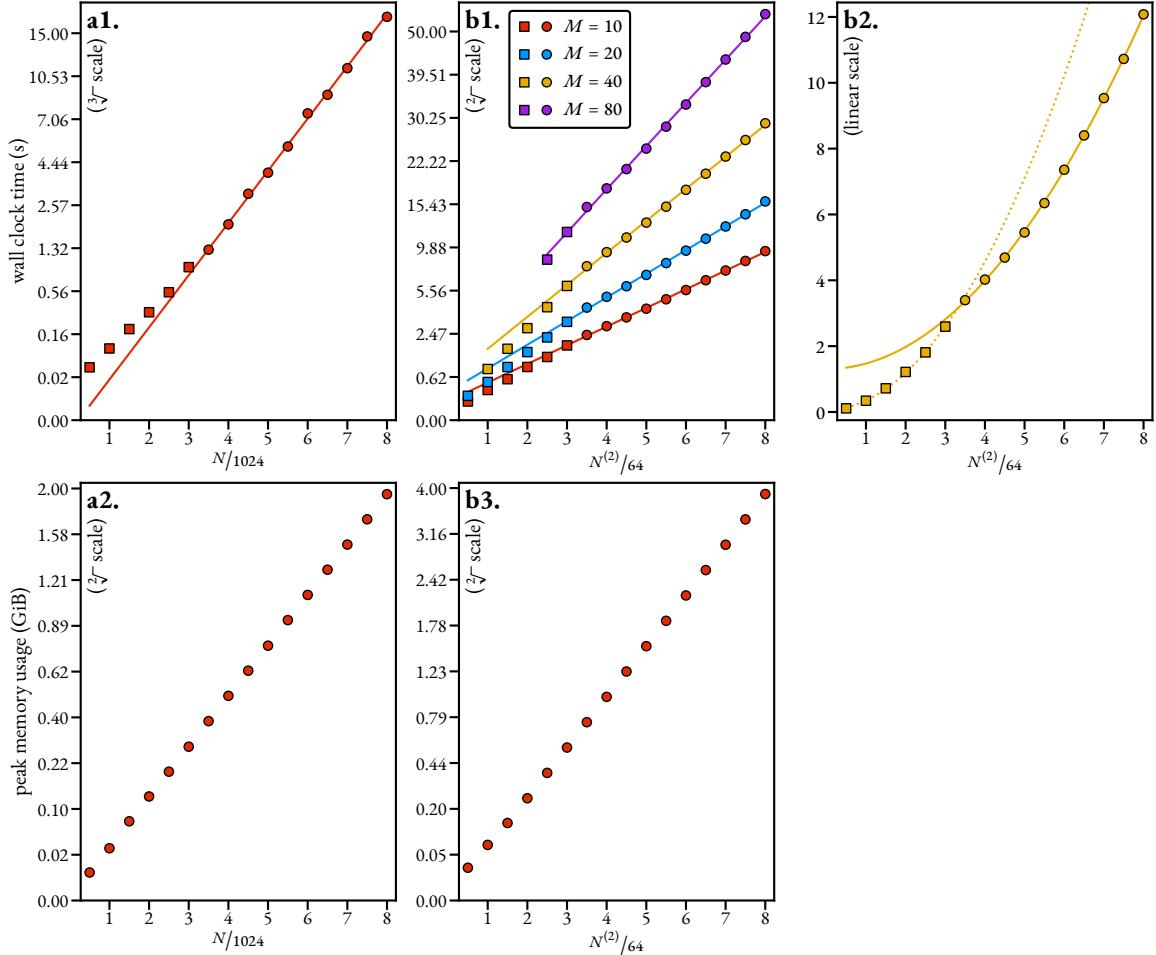
A series of synthetic 1D FIDs were constructed, comprising 10 evenly-spaced signals, with a variable number of time-points  $N \in \{512k : k \in \{1, 2, \dots, 16\}\}$ . For each FID, the MPM routine outlined in Code Listing C.3 was performed 5 times. The mean time to perform the MPM across the 5 runs is plotted as a function of  $N$  in panel a1 of Figure 2.4, where it can be seen that for the larger values of  $N$  considered, the MPM is computed in approximately  $\mathcal{O}(N^3)$  time; a fit of a cubic function of the form  $aN^3 + b$  to the data satisfying  $7 \leq k \leq 16$  is plotted to highlight this. The cubic dependence is realised since the rate-limiting step of the MPM is SVD of  $\mathbf{H}_y$ , whose size is to a very good approximation  $\frac{2N}{3} \times \frac{N}{3}$ <sup>§§</sup>. For smaller values of  $N$ , a deviation away from a cubic relationship is observed; This arises because the computation of the complex amplitudes using Equation 1.38 has a comparatively significant run time relative to SVD in the low- $N$  regime; for a 512 point signal, SVD of  $\mathbf{H}_y$  took up roughly 80% of the complete run time, while the computation of the complex amplitudes took up roughly 20%. For a 8192 point signal, these percentages had changed to >99% and <1%, respectively.

The MPM was run once more on each generated FID in order to assess the effect of  $N$  on the space complexity. The peak RAM consumption is plotted in panel a2 of Figure 2.4. A clear quadratic dependence on consumption is realised as function of  $N$ , again in agreement with the expected space complexity of the SVD<sup>§§</sup>.

A similar study was conducted in consideration of the MMEMPM. A series of hypercomplex 2D FIDs were simulated, all of which all comprised  $N^{(1)} = 64$ . The FIDs possessed values of  $N^{(2)} \in \{32k : k \in \{1, \dots, 16\}\}$ . With the MPM, since a complete SVD of the matrix  $\mathbf{H}_y$  is

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<sup>§§</sup> The time complexity for the SVD of generic a  $m \times n$  matrix is  $\mathcal{O}(\min(m, n)^2 \cdot \max(m, n))$ , while the space complexity is  $\mathcal{O}(mn)$ .



**Figure 2.4:** Outlines of the run times and peak memory consumption of the 1D MPM and 2D MMEMPM. The FIDs that were used to acquire these results are described in the main text. **a1.** The amount of time required to compute the MPM, as a function of number of points. Also plotted is a cubic fit of the circular points. **a2.** Peak memory consumption in performing the MPM as a function of the number of points. **b1.** The run times for computing the MMEMPM of FIDs with  $N^{(1)} = 64$ , and variable  $N^{(2)}$  and  $M$ . **b2.** The time required to compute the SVD of  $E_Y$  for the  $M = 40$  FIDs. The solid line is a quadratic fit of the circular points, while the dashed line is a quadratic fit of the square points. **b3.** Peak memory consumption in performing the MMEMPM for the  $M = 40$  FIDs.

computed, the model order is irrelevant in dictating the run time (at least when  $M \ll N$ ). This is not the case for the MMEMPM; because the PYTHON implementation used (Code Listing C.4) employs a truncated SVD in order to compute only the first  $M$  components of  $\mathbf{E}_Y$ , the elected model order will have an impact on run time. Therefore, FIDs with different model orders were generated:  $M \in \{10, 20, 40, 80\}$ .

The MMEMPM was repeated 5 times for each FID, and the mean run times for each  $N^{(2)}$  and  $M$  considered is plotted in panel b1 of Figure 2.4. Only the results for cases where the MMEMPM was able to yield a satisfactory estimation result, in close agreement with the model used to generate the FID, are presented; for certain FIDs with low  $N^{(2)}$  and high  $M$ , appropriate estimation results could not be yielded as the constituent signals were too poorly resolved. While in the high- $N$  regime the MPM has a cubic time dependence on the number of points, the MMEMPM can be seen to have an approximately quadratic complexity regarding  $N^{(2)}$ . For all combinations of  $N^{(2)}$  and  $M$ , the truncated SVD was the most time consuming aspect of the routine, however other steps have notable run times too. Most of the run time is due to the following five steps (with the relevant lines in Code Listing C.4 given):

- Step 1: Construction of  $\mathbf{E}_Y$ . This involves building the Hankel matrices  $\{\mathbf{H}_{y,n^{(1)}} : n^{(1)} \in \{0, \dots, 63\}\}$ , assigning them to the correct locations in  $\mathbf{E}_Y$ , and finally converting  $\mathbf{E}_Y$  to a sparse matrix<sup>99</sup> (Lines 45 to 65).
- Step 2: Truncated SVD of  $\mathbf{E}_Y$  to generate  $\mathbf{U}_M$  (Line 67).
- Step 3: Determining  $\mathbf{z}^{(1)}$  and  $\mathbf{W}^{(1)}$  by computing the eigenvalue decomposition of  $\mathbf{U}_{M1}^+ \mathbf{U}_{M2}$  (Lines 68 to 70).
- Step 4: Generating the second set of signal poles  $\mathbf{z}^{(2)}$ , by multiplying  $\mathbf{U}_M$  by the permutation matrix, and extracting the diagonal from matrix  $\mathbf{G}$ , computed using Equation 2.27 (Lines 72 to 85). N.B. The FIDs were constructed such that the signal poles were unique on all occasions, so the additional treatment of repeated signal poles was not necessary.
- Step 5: Computation of the complex amplitudes using Equation 2.29 (Lines 117 to 132).

A comparison of the relative times to perform these steps for some select pairings of  $M$  and  $N^{(2)}$  is provided by Table 2.2. It can be seen that as  $M$  increases, the relative amount of time spent performing SVD increases, while the amount of time to generate  $\mathbf{E}_Y$  decreases. This reflects the greater number of iterations required by the truncated SVD routine[94] to produce the desired number of components, while the run time to generate  $\mathbf{E}_Y$  remains fixed.

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<sup>99</sup>Truncated SVD is only available for sparse matrices in NUMPY[94]. Some experimenting was done to determine the most efficient means of generating  $\mathbf{E}_Y$  in sparse form, and subsequently compute its SVD. It was determined that constructing  $\mathbf{E}_Y$  using a standard NUMPY array before converting it to compressed sparse row (CSR) format[103] was optimal.

$N^{(2)}$	$M$	Step 1	Step 2	Step 3	Step 4	Step 5
64	10	12.2%	60.6%	2.9%	9.7%	13.8%
64	40	4%	74.6%	1.9%	8.9%	9.6%
512	10	22.1%	67.2%	0.2%	3.1%	7.2%
512	40	7.4%	81.9%	0.1%	1.3%	9.4%
512	80	3.8%	85.8%	0.1%	0.8%	9.4%

**Table 2.2:** A comparison of the relative times to perform the key steps in the MMEMPM, for selected pairings on  $M$  and  $N^{(2)}$ . See the main text for a description of what each step entails.

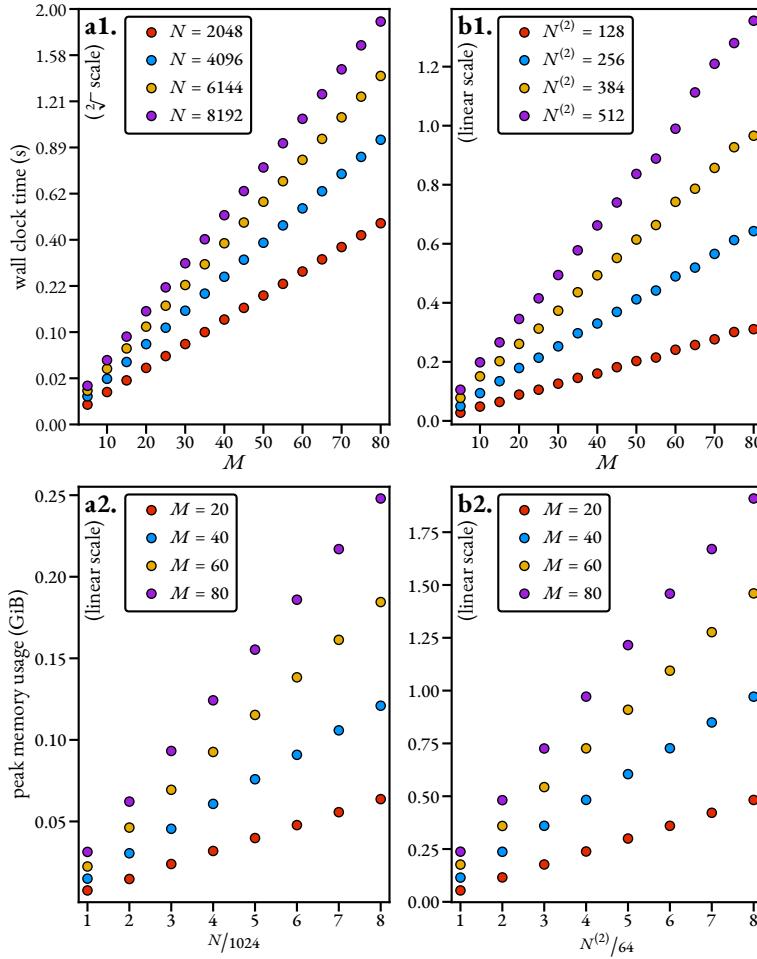
Interestingly, the plots for a given value of  $M$  in panel b1 do not exhibit consistent quadratic behaviour throughout. After a certain value of  $N^{(2)}$ , a slight reduction in the gradient of the plots in panel b1 is observed (cf the square and circular points). This was found to be caused by the SVD computation, whose run times for the  $M = 40$  FIDs are plotted in panel b2. The square and circular points both display quadratic behaviour, though the exact form of the function which describes them are different; both sets of points have been fit to curves of the form  $aN^{(2)2} + b$ . After  $N^{(2)}$  becomes larger than roughly 200, the SVD run time appears to enter a new regime in which subsequent increases in  $N^{(2)}$  cause the rate of SVD to increase at a slower rate than was the case previously. The exact reason for this probably lies in the exact implementation of the SVD but was not explicitly ascertained.

The peak RAM usage for the  $M = 40$  FIDs as a function of  $N^{(2)}$  is plotted in panel b3, where a quadratic complexity is observed. The variation in memory consumption barely changes as a function of the model order, since the peak usage is largely dependent on the size of  $E_Y$ .

It should be noted that the run time and peak RAM consumption will also be (roughly) quadratically dependent on  $N^{(1)}$ , just as with  $N^{(2)}$ , i.e. increasing  $N^{(1)}$  from 64 to 128 would cause all the run times in panel b1 and peak memory usages in panel b3 to quadruple in value.

#### 2.4.2 Computing the Hessian for NLP

A consideration of the burden on the CPU and RAM in computing the Hessian matrix for 1D and 2D FIDs (Equation 2.45b) is presented in Figure 2.5. It should be noted that for a typical NLP routine, the Hessian will need to be computed many times (on the order of magnitude of  $10^2$  is common) so while the times presented in the figure may seem small, a rather long total time to run NLP is possible if it takes seconds to compute the Hessian once. For the 1D case, simulated FIDs were generated with both a variable number of contributing signals:  $M \in \{5k : k \in \{1, 2, \dots, 16\}\}$  and datapoints:  $N \in \{1024k : k \in \{1, 2, \dots, 8\}\}$ . For each signal, the Hessian matrix was computed using the `obj_grad_hess_1d` function, given by Lines 46 to 131 in Code



**Figure 2.5:** Outlines of the run time and peak memory consumption in computing the Hessian matrix for NLP. The FIDs that were used to acquire these results are described in the main text. **a1.** & **b1.** The amount of time required to compute the Hessian for 1D and 2D FIDs, respectively. **a2.** & **b2.** Equivalent plots showing the peak memory consumption in computing the Hessian.

$N/N^{(2)}$	$M$	Step 1	Step 2	Step 3	Step 4
<b>1D Hessian</b>					
2048	20	3.7%	9.6%	6%	76.4%
8192	20	3.5%	10.7%	6.3%	75%
2048	80	1%	3%	2%	92.6%
8192	80	1.2%	3.3%	1.9%	92.4%
<b>2D Hessian</b>					
64	20	8.2%	32.5%	18.5%	38.5%
256	20	12.3%	50.2%	21.3%	14.3%
64	80	10.8%	41%	24.3%	21.5%
256	80	14.9%	45.4%	24.1%	13.8%

**Table 2.3:** A comparison of the relative times to perform the key steps in computing the Hessian matrix for NLP, for selected pairings of  $M$  and  $N$  (1D)/ $N^{(2)}$  (2D).

Listing C.6\*\*\*. There are 4 main steps in computing the Hessian matrix:

- Step 1: Generation of all the first partial derivatives (Equation 2.46), which are stored in a  $4M \times N$  array.
- Step 2: Generation of all the non-trivially zero second partial derivatives (Equation 2.47), which are stored in a  $10M \times N$  array.
- Step 3: Computing the non-zero elements of term ② in Equation 2.45b.
- Step 4: Computing term ① in Equation 2.45b.

These steps produce an exact Hessian. Neglecting steps 2 & 3 leads to the formation of the approximated Hessian as described in Section 2.3.3. Panel a1 in Figure 2.5 shows that the time to compute the Hessian matrix scales quadratically with  $M$ , and linearly with  $N$ . The cause of this is the fact that the most time-consuming aspect of the routine is step 4, which involves multiplying the  $4M \times N$  matrix of first derivatives with its  $N \times 4M$  conjugate transpose, with a complexity  $\mathcal{O}(M^2N)$ . The relative amount of the total run time which is spent performing step 4 increases steadily as the model order increase, as seen in Table 2.3. As such, for 1D FIDs, it is common, especially when the data comprises a large number of signals, for the discrepancy in the amount of time to compute the true Hessian relative to its approximation to be small. In these cases, it may be valuable to compute the exact Hessian if it leads to a reduced number of required iterations for convergence.

To assess the effect of the number of signals and datapoints on Hessian computation for 2D FIDs,

\*\*\* A slight variant of this function was used, which neglected the computation of the objective and gradient, and returned only the Hessian.

a series of signals were generated with a fixed number of datapoints in the first dimension:  $N^{(1)} = 64$ . FIDs were then constructed with the same values of  $M$  as the 1D case, and  $N^{(2)} \in \{64k : k \in \{1, 2, \dots, 8\}\}$ . In contrast to the 1D case, it is seen that the run time in computing the Hessian now scales approximately linearly, rather than quadratically. Much more of the run time is taken up by the first three steps in comparison; computing the  $6MN^{(1)}N^{(2)}$  first derivatives,  $21MN^{(1)}N^{(2)}$  second derivatives, and forming term ② all scale linearly with  $M$ ,  $N^{(1)}$ , and  $N^{(2)}$ . The relative times spent performing steps 2 & 3 compared with 1 & 4 imply that for the 2D case especially, a large saving in computational time is likely to be achieved when the Hessian approximation is utilised over the exact form.

Both the time- and space-complexity of computing the Hessian is found to be roughly linear with both  $M$  and the number of datapoints in each dimension for 1D and 2D FIDs (see panels a2 and b2 of Figure 2.5). Most of the RAM usage comes from storing arrays of the first and second partial derivatives. In general, the typical space requirements for both 1D and 2D FIDs should be tolerable on modern computers, which tend to possess at least 8 GiB of RAM.

## 2.5 Frequency Filtration

The previous section provides motivation for finding ways to reduce both the number of datapoints and the number of signals present in an FID, without compromising the ability of the estimation routine to parameterise it. A means of generating frequency-filtered “sub-FIDs” is presented, which is able to achieve both of these. In essence, this sub-FID approach transforms the problem of FID estimation from a single large-scale estimation problem to a plurality of smaller-scale problems. As well as realising vast improvements in computational speed, filtering also enables a user to focus solely on spectral regions that are of interest. It is common for certain spectral regions to be so densely populated that it is futile to attempt to extract meaningful quantitative information at the per-signal level, especially with 1D NMR data. Through data filtration, all focus can be devoted to those frequency regions which can realistically be studied.

### 2.5.1 The virtual echo

The key steps of the filtering procedure are (i) transforming the time-domain data to the frequency domain, (ii) applying a band-pass filter to the spectral region of interest, and (iii) returning the spectrum back to the time-domain for estimation. For a filtered sub-FID to still be faithfully modelled by a summation of exponentially damped complex sinusoids, it is necessary that the

spectral peaks of interest lie (effectively) entirely within the filter region<sup>†††</sup>. Due to their narrower linewidths relative to dispersion Lorentzians, a phased spectrum solely comprising absorption Lorentzians is therefore desired. The virtual echo (VE) has been employed here, which has found application in the field of compressed sensing NMR[104–106]. The VE is a signal with double the size as the original FID, with the key characteristic that its FT has an imaginary component of zeros. The VE concept can be applied to data of any number of dimensions. However, discussion here will be limited to 1D VEs. An account of the 2D VE is provided in Appendix B.3.

Assuming that a 1D FID  $y \in \mathbb{C}^N$  is phased, such that  $\phi = \mathbf{0} \in \mathbb{R}^M$ , it can be described by

$$y_n = \xi_n(c_n + i s_n) + w_n, \quad (2.55a)$$

$$\xi_n = \sum_m a_m \exp(-\eta_m n \Delta_t), \quad (2.55b)$$

$$c_n / s_n = \sum_m \cos / \sin(2\pi f_m n \Delta_t). \quad (2.55c)$$

The frequency-dependence has been decomposed into its real and imaginary components. With this in mind, a conjugate pair of signals  $\psi_{\pm} \in \mathbb{C}^N$  are defined:

$$\psi_{\pm,n} = \xi_n(c_n \pm i s_n) + w_n \equiv \Re(y_n) \pm i \Im(y_n) \quad (2.56)$$

Two vectors  $t_1, t_2 \in \mathbb{C}^{2N}$  are constructed using the conjugate pair.  $t_1$  is given by  $\psi_+$  padded with zeros from below:

$$t_1 = \begin{bmatrix} \psi_+ \\ \mathbf{0} \in \mathbb{C}^N \end{bmatrix}. \quad (2.57)$$

$t_2$  is given by  $\psi_-$  with its elements in reversed order ( $\cdot^{\leftrightarrow}$ ), padded with zeros from above, and finally subjected to a right circular shift by one element ( $\cdot^{\circlearrowright}$ ):

$$t_2 = \begin{bmatrix} \mathbf{0} \in \mathbb{C}^N \\ \psi_-^{\leftrightarrow} \end{bmatrix}^{\circlearrowright}. \quad (2.58)$$

The VE  $y_{ve}$  is then given by  $t_1 + t_2$ , with the first element divided by 2. This is equivalent to

$$y_{ve} = \begin{bmatrix} \Re(y_0) & y_1 & \cdots & y_{N-1} & 0 & y_{N-1}^* & \cdots & y_1^* \end{bmatrix}^T. \quad (2.59)$$

As eluded to already, the FT of  $y_{ve}$  produces a spectrum  $s_{ve}$  such that  $\Im(s_{ve}) = \mathbf{0}$ , with  $\Re(s_{ve})$  featuring absorption Lorentzian peaks.

---

<sup>†††</sup>Lorentzian lineshapes tend to but never explicitly reach zero as the distance from their maximum tends to  $\infty$  (Equation 1.28). However, as long as a sufficiently wide filter region is defined, the extent to which the “tails” of the Lorentzian fall outside the filter window can be assumed to be negligible, especially when in the presence of noise.

### 2.5.2 The filtering process

To filter the spectrum  $s_{ve}$ , it is subjected multiplication with a function which acts as a band-pass filter. An example of a suitable filter is a *super-Gaussian*  $g \in \mathbb{C}^{2N}$  defined by a central index  $c \in \{0, \dots, 2N - 1\}$  and a bandwidth  $b \in \{0, \dots, 2N - 1\}$ :

$$g_n = \exp \left( -2^{p+1} \left( \frac{n - c}{b} \right)^p \right). \quad (2.60)$$

The scalar  $p \in \mathbb{R}_{>0}$  dictates the steepness of the filter at the boundaries, with the function becoming more rectangular as it increases. The central index and bandwidth of the super-Gaussian filter function are given by the following expressions:

$$c = \frac{1}{2} (l_{\text{idx}} + r_{\text{idx}}), \quad (2.61a)$$

$$b = r_{\text{idx}} - l_{\text{idx}}, \quad (2.61b)$$

where  $l_{\text{idx}}, r_{\text{idx}} \in \{0, \dots, 2N - 1\}$ ,  $r_{\text{idx}} > l_{\text{idx}}$  denote the left and right boundaries of the region of interest, defined by the user, expressed as vector indices. The vector indices can be obtained from the corresponding spectral frequencies  $f_{\text{Hz}}$  via

$$f_{\text{idx}} = \left\lfloor \frac{(2N - 1) (f_{\text{sw}} + 2 (f_{\text{off}} - f_{\text{Hz}}))}{2f_{\text{sw}}} \right\rfloor \quad (2.62)$$

$$\forall f_{\text{Hz}} \in \left[ f_{\text{off}} - \frac{1}{2} f_{\text{sw}}, f_{\text{off}} + \frac{1}{2} f_{\text{sw}} \right].$$

Alternatively, conversion from ppm to array indices can be achieved by replacing  $f_{\text{Hz}}$  in Equation 2.62 with  $f_{\text{ppm}} f_{\text{sfo}}$ , where  $f_{\text{sfo}}$  is the transmitter frequency (MHz) and  $f_{\text{ppm}}$  is the frequency expressed as a chemical shift.

Application of the super-Gaussian filter to  $s_{ve}$  would lead to large sections of the filtered spectrum being 0. This has an undesired impact on the MDL, as noise that resides within the filter region will now seem to resemble true signal, as its amplitude is infinitely greater than the zeroed regions. A massive over-estimation of model order results from this. In order to obtain better predictions from model order selection, an array of synthetic AWGN is added to the filtered spectrum. To achieve this, a region in  $s_{ve}$  is specified by the user which contains no discernible signal peaks (referred to as the *noise region*). The variance of this region  $\sigma^2$  is determined, and used to construct a vector of values sampled from a normal distribution with mean 0 and variance  $\sigma^2$ ,  $w_{\sigma^2} \in \mathbb{R}^{2N}$ . The filtered spectrum is then given by

$$\tilde{s}_{ve} = s_{ve} \odot g + w_{\sigma^2} \odot (1 - g). \quad (2.63)$$

Note that the noise array's magnitude at each point is attenuated based on the value of the super-Gaussian filter, as a means of ensuring the noise variance remains consistent across the frequency space.

After filtering,  $\tilde{s}_{ve}$  is returned to the time-domain by inverse Fourier transform (IFT). The IFT of a real-valued spectrum generates a conjugate-symmetric signal, which is also a VE. This is sliced so as to retain the first half, which is the final filtered sub-FID  $\tilde{y} \in \mathbb{C}^N$ . A depiction of the key elements involved in the filtering process is provided by Figure 2.6, while a step-by-step outline is provided by Algorithm 2.3.

Thus far, the method described is able to reduce the number of signals, though the filtered sub-FID still comprises the same number of points. However, it is clear that there are a large number of points outside the region of interest in  $\tilde{s}_{ve}$  that do not possess any meaningful information. Discarding such points will then lead to a sub-FID with the same information, but in a more compressed FID. To achieve this, a slicing ratio is defined,  $\chi > 1$ , which dictates the left and right boundaries of a region outside of which points will be discarded:

$$l_{\text{slice}} = \max \left( c - \left\lfloor \frac{b\chi}{2} \right\rfloor, 0 \right), \quad (2.64a)$$

$$r_{\text{slice}} = \min \left( c + \left\lceil \frac{b\chi}{2} \right\rceil, 2N - 1 \right). \quad (2.64b)$$

The filtered spectrum is then sliced accordingly:

$$\mathbb{R}^{r_{\text{slice}} - l_{\text{slice}}} \ni \tilde{s}_{ve,\text{slice}} = \tilde{s}_{ve}[l_{\text{slice}} : r_{\text{slice}} + 1] \equiv [\tilde{s}_{ve,l_{\text{slice}}} \quad \tilde{s}_{ve,l_{\text{slice}}+1} \quad \dots \quad \tilde{s}_{ve,r_{\text{slice}}} \quad \tilde{s}_{ve,r_{\text{slice}}+1}]^T. \quad (2.65)$$

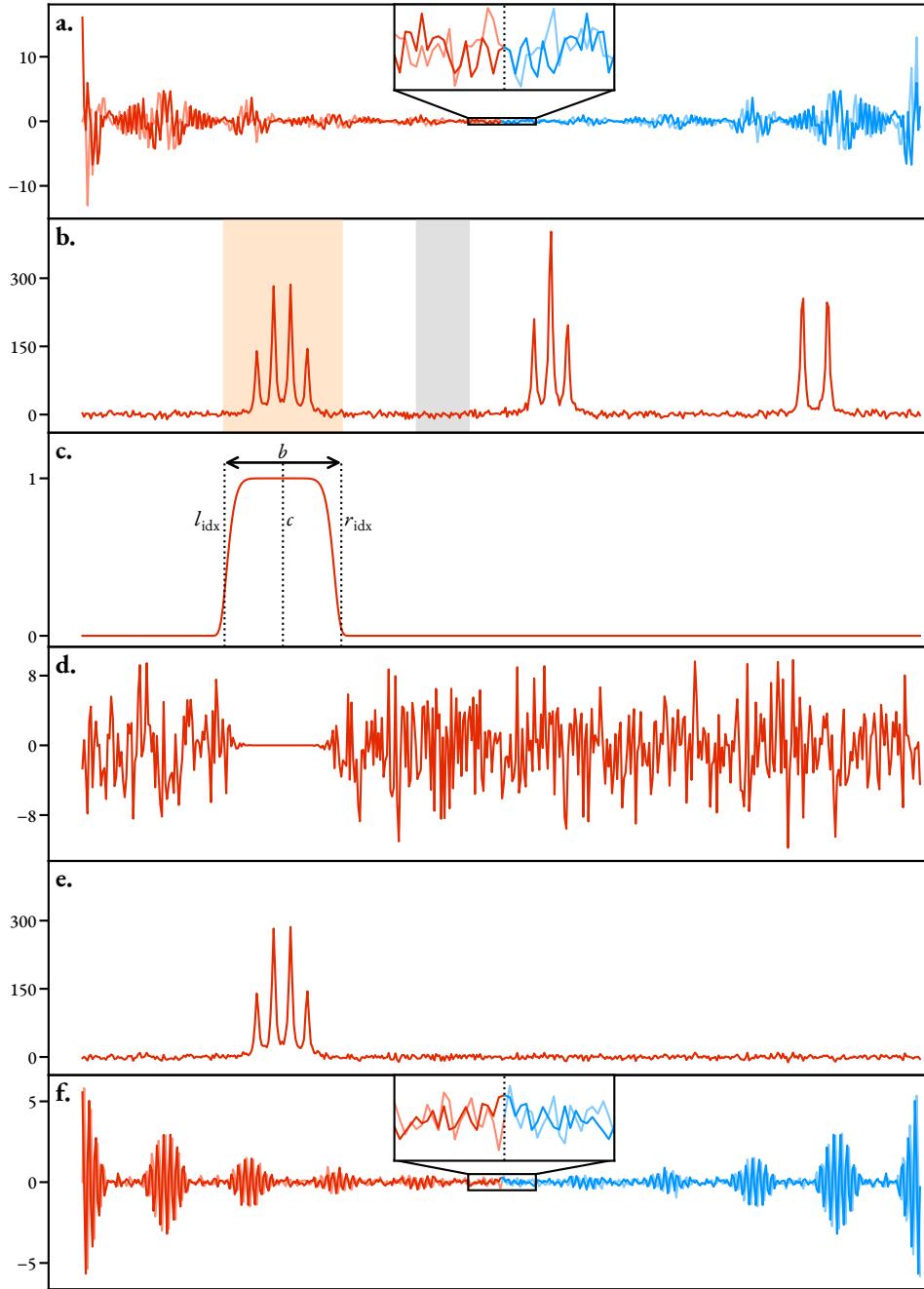
Generation of the final sub-FID is then achieved in a similar fashion to before, by performing IFT, and retaining the first half of the signal. It is also necessary to scale the signal by the ratio of the number of points in the sliced spectrum and its unsliced counterpart, in order to ensure that the amplitudes of each signal are unaffected:

$$\tilde{y} = \frac{r_{\text{slice}} - l_{\text{slice}}}{2N} \text{IFT}(\tilde{s}_{ve,\text{slice}})[0 : N_{\text{slice}}], \quad (2.66a)$$

$$N_{\text{slice}} = \left\lfloor \frac{r_{\text{slice}} - l_{\text{slice}}}{2} \right\rfloor \quad (2.66b)$$

The associated sweep width and transmitter offset of the FID will have been altered by this process, and in order to derive accurate frequencies and damping factors for the sliced signal, it is necessary to determine these. The corrected values can be computed using

$$f_{sw,\text{slice}} = \frac{r_{\text{slice}} - l_{\text{slice}}}{2N - 1} f_{sw} \quad (2.67a)$$



**Figure 2.6:** An illustration of the filtering procedure applied to a 1D FID. **a.** A VE  $y_{ve}$ , with the first and last  $N$  points coloured red and blue, respectively. The middle of the VE is magnified to highlight its conjugate symmetry. **b.** The FT of the VE,  $s_{ve}$ . The region of interest (orange) and noise region (grey) are denoted. **c.** A super-Gaussian function used as a band-pass filter,  $g$ . **d.** Synthetic noise vector to be added to the filtered spectrum,  $w_{\sigma^2}(1 - g)$ . **e.** The filtered spectrum  $\tilde{s}_{ve}$ , formed by applying the super-Gaussian filter, and adding the noise vector. **f.** The IFT of the filtered spectrum,  $\tilde{y}_{ve}$ , from which the final filtered signal  $\tilde{y}$  is obtained by extracting the first  $N$  (red) points.

$$f_{\text{off,slice}} = f_{\text{off}} + \frac{f_{\text{sw}}}{2} \left( 1 - \frac{l_{\text{slice}} + r_{\text{slice}}}{2N - 1} \right) \quad (2.67\text{b})$$

---

**Algorithm 2.3** Filtering procedure for 1D data.  $l_{\text{idx}}$  and  $r_{\text{idx}}$  are indices of the left and right bounds of the region of interest.  $l_{\text{idx,noise}}$  and  $r_{\text{idx,noise}}$  are the analogous bounds for the noise region. All of these values should be  $\in \{0, \dots, 2N - 1\}$ . These would typically be provided in units of Hz or ppm by a user; conversion to indices can be carried out using Equation 2.62.

---

```

procedure FILTER1D( $y \in \mathbb{C}^N, l_{\text{idx}}, r_{\text{idx}}, l_{\text{idx,noise}}, r_{\text{idx,noise}}, \chi \in \mathbb{R} : \chi > 1$ )
     $s_{\text{ve}} \leftarrow \text{VIRTUALECHO1D}(y);$ 
     $s_{\text{ve}} \leftarrow \text{FT}(s_{\text{ve}});$ 
     $c_{\text{idx}} \leftarrow (l_{\text{idx}} + r_{\text{idx}})/2;$ 
     $b_{\text{idx}} \leftarrow r_{\text{idx}} - l_{\text{idx}};$ 
     $g \leftarrow \text{SUPERGAUSSIAN1D}(2N, c_{\text{idx}}, b_{\text{idx}});$ 
     $s_{\text{noise}} \leftarrow s_{\text{ve}}[l_{\text{idx,noise}} : r_{\text{idx,noise}} + 1];$ 
     $\sigma^2 \leftarrow \text{Var}(s_{\text{noise}});$ 
     $w_{\sigma^2} \leftarrow \mathbf{0} \in \mathbb{R}^{2N};$ 
    for  $n = 0, \dots, 2N - 1$  do
         $w_{\sigma^2,n} \leftarrow \text{RANDOMSAMPLE}(\mathcal{N}(0, \sigma^2));$ 
    end for
     $\tilde{s}_{\text{ve}} \leftarrow s_{\text{ve}} \odot g + w_{\sigma^2} \odot (1 - g);$ 
     $l_{\text{slice}} \leftarrow \max\left(c - \left\lfloor \frac{b\chi}{2} \right\rfloor, 0\right);$ 
     $r_{\text{slice}} \leftarrow \min\left(c + \left\lceil \frac{b\chi}{2} \right\rceil, 2N - 1\right);$ 
     $\tilde{s}_{\text{ve,slice}} \leftarrow \tilde{s}_{\text{ve}}[l_{\text{slice}} : r_{\text{slice}} + 1];$ 
     $\tilde{y}_{\text{ve}} \leftarrow \frac{r_{\text{slice}} - l_{\text{slice}}}{2N} \text{IFT}(\tilde{s}_{\text{ve,slice}});$ 
     $\tilde{y} \leftarrow \tilde{y}_{\text{ve}}\left[:, \left\lfloor \frac{r_{\text{slice}} - l_{\text{slice}}}{2} \right\rfloor\right];$ 
    return  $\tilde{y};$ 
end procedure

procedure VIRTUALECHO1D( $y \in \mathbb{C}^N$ )
    return  $[\Re(y_0) \quad y_1 \quad \cdots \quad y_{N-1} \quad 0 \quad y_{N-1}^* \quad \cdots \quad y_1^*]^T$ 
end procedure

procedure SUPERGAUSSIAN1D( $N \in \mathbb{N}, c_{\text{idx}}, b_{\text{idx}}$ )
     $g \leftarrow \mathbf{0} \in \mathbb{R}^N;$ 
    for  $n = 0, \dots, N - 1$  do
         $g_n \leftarrow \exp\left(-2^{41} \left(\frac{n - c_{\text{idx}}}{b_{\text{idx}}}\right)^{40}\right);$ 
    end for
    return  $g$ 
end procedure

```

---

## 2.6 Summary

The MPM is well established as an effective method for the parametric estimation of signals in a number of disciplines. One notable downside of the technique that has been realised while assessing its effectiveness in parametrising NMR FIDs is its propensity to return oscillators with unexpected phase behaviour, especially in scenarios involving signals with similar frequencies, ex-

$\triangleright p$  in Equation 2.60 has been set to 40.

hibiting considerable overlap in the Fourier domain. For this reason, using the result of the MPM as an initial guess to feed into a phase-variance regularised NLP routine is proposed as a means of returning improved parameter estimates. The theory underpinning the procedure has been explored in this chapter.

The computational burden of running the procedure is large and often intractable for complete NMR datasets, which commonly comprise thousands of points, and at least hundreds of contributing signals. As has been shown by profiling both the CPU time and the peak memory consumption for the 1D and 2D methods, there are greater demands when the FID of interest comprises more datapoints and is composed of more signals. For this reason, a method to break the estimation problem into a series of smaller, computationally tractable problems, through the construction of frequency-filtered sub-FIDs, has been introduced.

Having established an estimation routine, the next chapter focusses on its performance in analysing 1D NMR datasets, along with two specific applications that arise.



# Results and Applications Involving 1D Estimation

3

This chapter showcases results generated using the 1D estimation technique outlined in the previous chapter. Furthermore, two means by which the standard 1D estimation procedure can be utilised for specific applications are presented. Section 3.1 provides some examples of how the estimation routine performs on 1D NMR datasets acquired using a pulse-acquire experiment. Section 3.2 illustrates how the basic 1D estimation routine can be extended to enable the consideration of datasets comprising a series of FIDs which feature attenuations in signal amplitudes across increments, including inversion recovery and diffusion experiments. Finally, Section 3.3 describes a protocol to generate ultra-broadband spectra through application of a single  $90^\circ$  frequency-swept pulse, which are devoid of quadratic phase dependencies as well as baseline distortions.

All the results presented were produced on the same computer (see Remark 3), using the NMR-EsPy package which is described in Chapter 5. Details about the datasets generated are provided in Appendix D.

## 3.1 Conventional 1D datasets

As mentioned in Section 2.3.5, one of the disadvantages of SVD-based methods like the MPM is their propensity to generate parameter estimates featuring oscillators with spurious phase behaviour. Such behaviour is most prevalent in FIDs featuring signals with very similar frequencies, causing considerable peak overlap in the Fourier domain, and low SNR. To assess the ability of the inclusion of the phase variance-regularised NLP routine to produce parameter estimates in better agreement with known features about the data, comparisons are now made between results generated with the MPM in isolation, and with the inclusion of phase variance-regularised NLP. For the experimental datasets considered (Sections 3.1.2 and 3.1.3), the data was pre-processed using

BRUKER’s TOPSPIN software, using the series of commands `ft`; `pk`; `abs`, which perform FT, automatic phase correction, and baseline correction, respectively. The data was then converted back to the time-domain using IFT.

### 3.1.1 “Twenty signals”

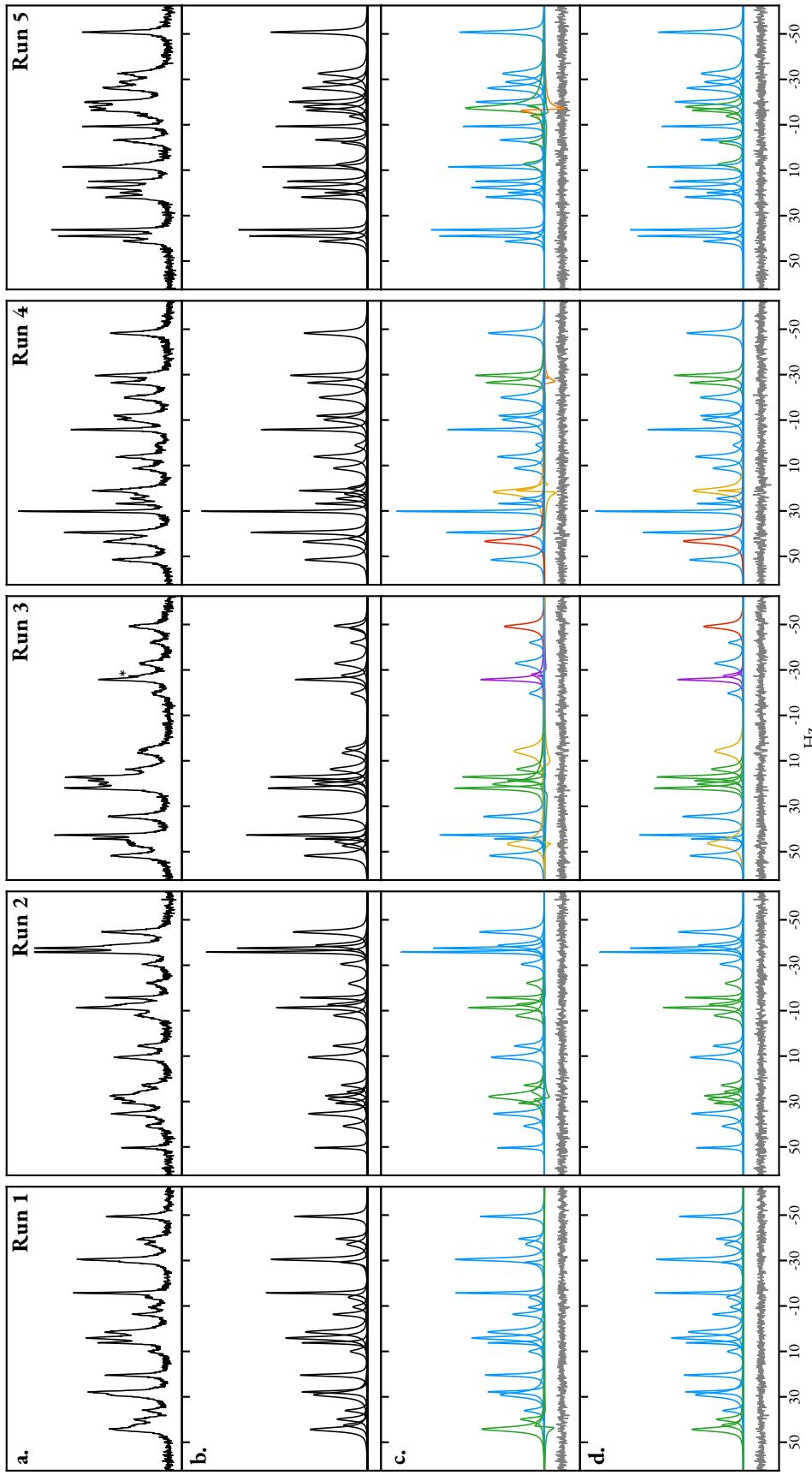
A series of five simulated FIDs were constructed using Equation 2.1 with  $D = 1$ . For each FID, a model order of  $M = 20$  was used, the number of points sampled was  $N = 1024$ , the sweep width was  $f_{\text{sw}} = 125$  Hz, and the transmitter offset was  $f_{\text{off}} = 0$  Hz. Each oscillator was assigned a phase of  $0^\circ$ , while the amplitudes, frequencies and damping factors were drawn at random from the following distributions:  $a_m \sim \mathcal{U}(1, 5)$ ,  $f_m \sim \mathcal{U}(-55 \text{ Hz}, 55 \text{ Hz})$ ,  $\eta_m \sim \mathcal{U}(2 \text{ s}^{-1}, 8 \text{ s}^{-1}) \forall m \in \{1, \dots, 20\}$ . An extra constraint was applied to the frequencies, such that no two oscillators were permitted to have frequencies that differed by less than  $4f_{\text{sw}}^{(1)}/N^{(1)} \approx 0.49$  Hz. Each noiseless FID  $x$  was then corrupted with AWGN, with a target SNR of 25 dB, with the corresponding noise variance for each FID determined using the equation

$$\sigma^2 = \frac{1}{20^{2.5} \times 1024} \sum_{n=0}^{1023} |x_n|^2. \quad (3.1)$$

The spectra of the simulated FIDs are presented in panel a of Figure 3.1, with the set of oscillator peaks which contribute to the spectrum in panel b. With the criteria used, it can be seen that such datasets feature signals which often suffer from severe overlap, with the high noise variance compounding the opportunity to clearly identify all contributing signals.

For each FID, the MPM was performed, assuming that the model order is 30, constituting a considerable over-fit. The MDL tended to produce considerable under-estimates of  $M$  when applied to these FIDs, so the hard-coded value was used instead. When an excessive model order is provided to the MPM, it is typical that oscillators corresponding to the noise subspace of the data matrix  $H_y$  are characterised by small amplitudes and/or very small damping factors. For this reason, prior to subjecting the MPM result to NLP, oscillators which satisfied  $a_m < 0.1$  and/or  $\eta_m < 0.7 \text{ s}^{-1}$  were removed from the parameter set. The individual oscillators which make up the MPM result after purging spurious components are displayed in panel c of Figure 3.1, along with the residual between the data and the summation of all the oscillator peaks.

The MPM consistently generated a model with good agreement with the data in a least squares sense, as evidenced by the residual. However, it can be seen that in several spectral regions across the datasets, especially ones that are highly crowded, oscillators possess parameters which deviate significantly from the true signal parameters used to construct the FIDs. Most notably, individual oscillator phases regularly stray far from  $0^\circ$ , and their associated amplitudes are often con-



**Figure 3.1:** The result of estimating a series of 5 simulated signals comprising 20 signals (see the main text for details on how the datasets were constructed). **a.** Spectra of the datasets generated. **b.** Spectral lines corresponding to the set of signals used to generate each dataset. **c.** Plots of peaks for each oscillator generated using the MPM. **d.** An equivalent plot for the result after applying phase variance-regularisedNLP, using the MPM result as an initial guess. Also included in **c.** and **d.** is the residual between the data and the sum of the oscillators in panels **c** and **d** is described in the main text.

siderably different too. In panel c of Figure 3.1, blue oscillators are those which agree very closely with a particular true signal in the data. Oscillators with other colours are not in agreement with a true signal, with the different colourings described shortly. The desired outcome of the NLP routine is for it to adjust the non-blue oscillator parameters in panel c such that they agree with true signals, while having little to no effect on the blue oscillators. The results after application of NLP are provided in panel d.

In discussing the outcome of the routine, it will be helpful to employ the concept of a *frequency neighbourhood*, a loose term which describes a small, continuous subset of frequencies within the spectral window. As the NLP routine involves taking small steps in parameter space over a number of iterations, it is unlikely that an oscillator which starts off with a frequency far away from a particular frequency neighbourhood will eventually enter it. As such, in order for the NLP routine to successfully estimate the signals within a given frequency neighbourhood of the data, sufficient oscillators need to present within the neighbourhood in the initial guess.

Cases where the MPM generated enough oscillators for a given frequency neighbourhood, albeit with parameters which are noticeably deviate from the true signals are coloured either green or yellow. Green oscillators are those which the NLP routine was able to adjust so as to achieve agreement with true signals; they indicate improvements to the estimation result in comparison with the MPM result. Conversely, yellow oscillators denote cases where, though sufficient oscillators existed in the frequency neighbourhood in the initial guess, the NLP routine evolved such that at least one of the oscillators was driven by the phase variance constraint to acquire a negative amplitude, such that it was removed from the parameter set. This typically occurred with oscillators that had an initial phase which was either  $> \pi/2$  rad, or  $< -\pi/2$  rad. Yellow oscillators therefore indicate cases where the final result underfit the dataset.

There are a few instances, denoted by red oscillators, where the MPM assigned too few oscillators to a particular frequency neighbourhood, and as such the NLP would not have been able to yield any improvement. This occurred in what can safely be described as fiendishly difficult cases, where severe signal overlap and low SNR make it very difficult to associate certain spectral regions with more than one signal by eye.

The final two oscillator groupings, coloured purple and orange respectively, indicate scenarios where the MPM generated more oscillators than true signals in a given frequency neighbourhood (i.e. the data was over-fit in this region). Orange oscillators were purged by the NLP routine as they acquired negative amplitudes. This enabled parsimonious fits of the relevant frequency neighbourhoods by the oscillators which remained. Finally, the purple oscillators denote the one occasion (Run 3) where an over-fit occurred, and the model order was not successfully reduced by the NLP routine. One of the purple oscillators in the MPM appears to agree closely with a significant

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### 3.1 Conventional 1D datasets

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“blip” in the noise, denoted by an asterisk in panel a of Figure 3.1. The over-fit has therefore occurred because this noise component was incorporated into the final result; it was neither purged based on the amplitude and damping factor criteria outlined above, nor by acquiring a negative amplitude during NLP.

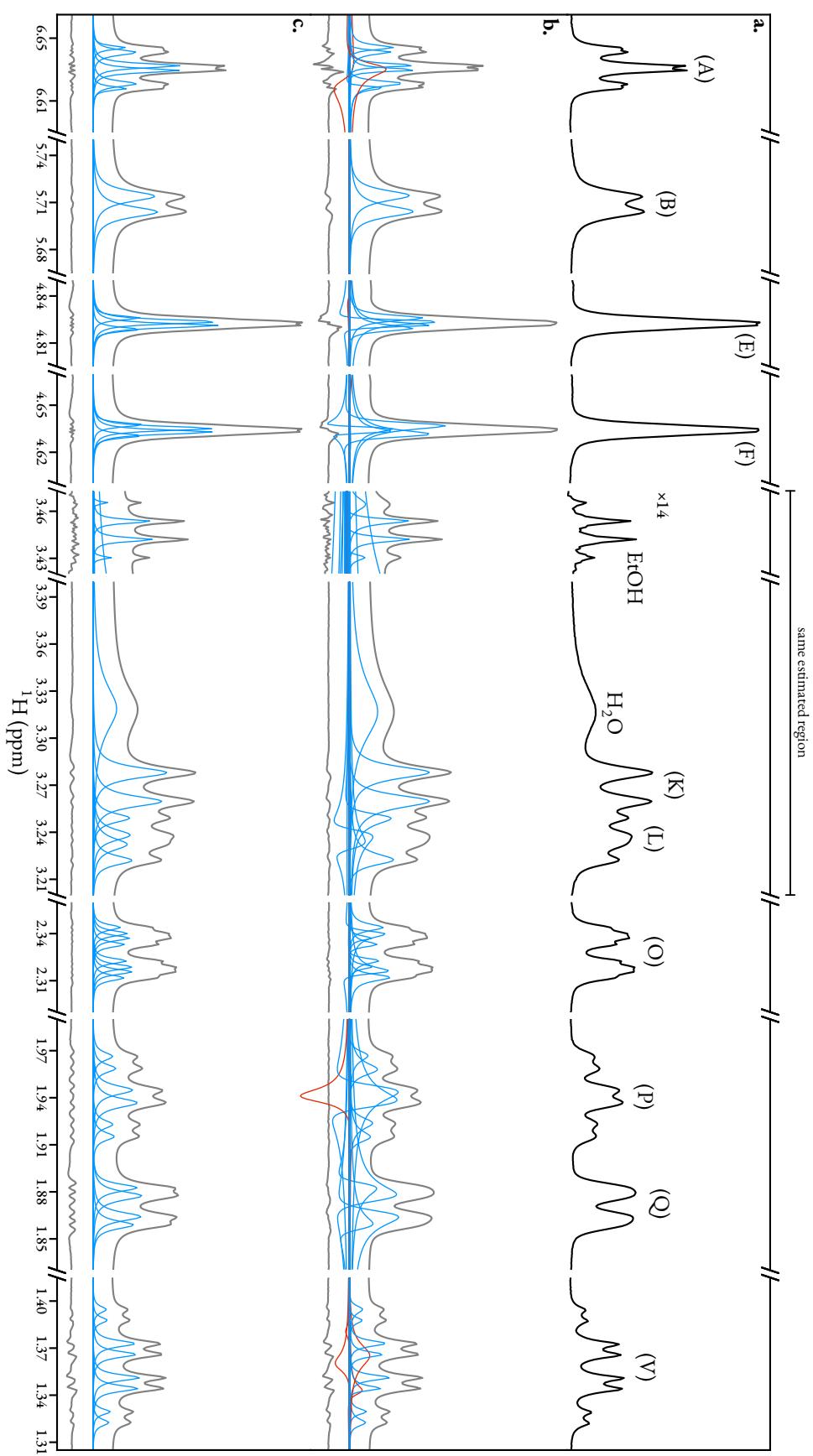
#### 3.1.2 Andrographolide

Figure 3.2 illustrates the outcome of applying the estimation routine to a  $^1\text{H}$  dataset of andrographolide (Figure D.1.e) in  $\text{DMSO-d}_6$ , acquired with a 600 MHz spectrometer. Various spectral regions were chosen for study, and for each one, a frequency-filtered sub-FID was produced using the approach in Section 2.5. The MPM was used to generate an initial guess of parameters, using the MDL to predict the model order in each case. The result of applying the MPM are presented in panel b of Figure 3.2. The initial guess was then subjected to NLP, giving rise to the result in panel c.

The NLP routine was effective at resolving the spurious phase behaviour often generated by the MPM. The estimation method’s ability to parametrise signals with high dynamic range and high variation of damping factors is also evidenced; a broad intense singlet from water, and a low-intensity quartet from residual ethanol in the sample, present in the same sub-FID, were both estimated admirably. For some of the sub-FIDs considered, the MPM output featured oscillators, commonly with very high damping factor and/or phases far from  $0^\circ$ , which were removed during the NLP routine (see the red peaks in panel b). The removal of these, along with the enforcement of consistent oscillator phases, leads to parameter estimates which describe the apparent multiplet structures associated with each spin reasonably well. Table 3.1 provides an overview of the most significant couplings associated with the spins giving rise to the multiplet structures considered.

One of the most challenging aspects of estimating NMR signals is common presence of signals within the dataset that have incredibly similar frequencies due to the influence of scalar couplings. Molecules with fused ring systems such as andrographolide are prime examples of spin systems which generate such datasets, as they tend to have very dense coupling networks leading to complex multiplet structures. Furthermore, fused systems often exhibit appreciable long-range couplings (between spins separated by four or more bonds) alongside the ubiquitous two-bond (geminal) and three-bond (vicinal) couplings. Long range couplings can be particularly challenging to resolve, as they are often of a comparable magnitude to the spectral resolution ( $f_{\text{sw}}/N$ ), making individual signals barely perceptible.

Take the multiplet structure from spin (Q) as an example of a particularly challenging estimation problem. (Q) has separate vicinal couplings to the diastereotopic protons (M) and (N), which are likely the greatest magnitude couplings associated with (Q). If these were the only couplings, a



**Figure 3.2:** Result of applying the estimation routine to selected regions of a pulse-acquire dataset of andrographolide in DMSO-d<sub>6</sub>. **a.** Spectral regions considered. **b.** The result of applying the MPM to the regions, with the model order predicted with the MDL. Blue/red lines: Individual oscillator peaks, grey line above: the model (sum of all oscillators), grey line below: the residual between the data and the model. **c.** The result after convergence of the NLP routine, again with the model above and residual below. Red peaks in panel b correspond to oscillators which acquire negative amplitudes and are removed during the NLP routine. One of the estimated regions has been split in two in the figure to save space, with one half, featuring a signal from ethanol, being magnified.

Spin	Coupling partners	Multiplet structure
<b>Andrographolide</b>		
(A)	(D) <sup>long</sup> , (M) <sup>vic</sup> , (N) <sup>vic</sup>	ddd ( <i>dt</i> )
(B)	(D) <sup>ex</sup>	d
(E)	(F) <sup>viny1</sup> ...	d...
(F)	(E) <sup>viny1</sup> ...	d...
(K)	(J) <sup>gem</sup> , (H) <sup>ex</sup>	d
(L)	(C) <sup>ex</sup> , (T) <sup>180</sup> , (U) <sup>60</sup>	dd
(O)	(P) <sup>gem</sup> , (R) <sup>60</sup> , (V) <sup>60</sup>	ddd
(P)	(O) <sup>gem</sup> , (R) <sup>60</sup> , (V) <sup>180</sup>	ddd ( <i>dt</i> )
(Q)	(M) <sup>vic</sup> , (N) <sup>vic</sup> ...	dd...
(V)	(O) <sup>60</sup> , (P) <sup>180</sup> , (R) <sup>g</sup> , (W) <sup>180</sup>	dddd ( <i>dq</i> )
<b>Cyclosporin A</b>		
(A)	diastereotopic pair on $\beta$ C	dd
(B)	—”—	dd
(C)	—”— & amide proton	ddd ( <i>dt</i> )
(D)	proton on $\beta$ C & amide proton	dd
(E)	methyl protons on $\beta$ C & amide proton	dq
(F)	—”—	dq ( <i>quintet</i> )

**Table 3.1:** Major coupling partners associated with spins in andrographolide and cyclosporin, considered in Figures 3.2 and 3.3 respectively, along with the multiplet structures that arise. For andrographolide, coupling partners are labelled as follows: <sup>viny1</sup> geminal coupling between two vinylic protons, <sup>ex</sup> geminal coupling between two protons, in which one is bonded to an oxygen, leading to exchange decoupling[32: Section 2.6.1.5], <sup>gem</sup> geminal coupling between two spins whose dihedral angle not fixed, <sup>long</sup> long-range coupling, <sup>vic</sup> vicinal coupling, <sup>60</sup> geminal coupling, with a fixed dihedral angle of 60° between the spins, <sup>180</sup> geminal coupling, with a fixed dihedral angle of 180° between the spins. All cyclosporin couplings of significance are geminal couplings. In cases where the observed multiplet structure is different to the true structure, the observed structure is in brackets. Ellipses denote cases where more (long-range) coupling partners are likely, based on the estimation result generated/the appearance of the spectrum, though these have not been explicitly assigned.

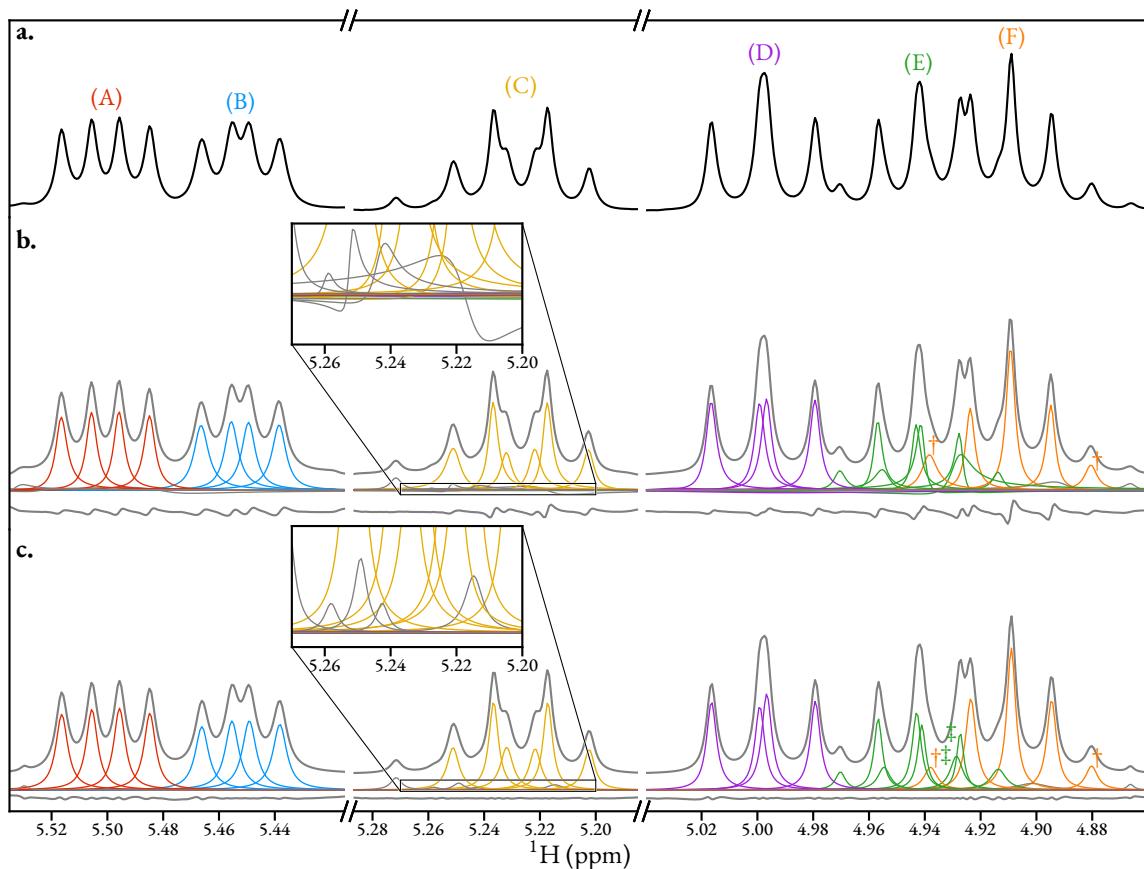
doublet of doublets (dd) structure would be expected, which is what has been generated by the estimation routine (see panel c in the region 1.85 ppm to 1.9 ppm). However, a comparison of the data and the model indicates that there is a clear discrepancy between the two, evidenced by systematic “wiggles” in the residual. This feature hints at an underfit of the multiplet structure. The MPM generated oscillators with phases deviating far from  $0^\circ$ , which enabled good agreement with the data in a residual sense, though of course such a set of oscillators is unrealistic in the context of a phased FID. Long-range couplings with magnitudes that are large enough to influence the appearance of (Q)’s multiplet structure are likely to be present, which leads to a signal in which all contributing resonances are too poorly resolved to realistically gleam any further meaningful information, at least at the field strength used.

As a second illustration, the multiplet structure corresponding to spin (V) is also under-fit, this time because the presence of a number of couplings of similar magnitude leads to resonances coalescing at roughly the same frequency; a multiplet structure featuring 16 resonances forming in a “dddd” structure is expected, however 3 of the couplings are of similar magnitudes, such that individual resonances coalesce to form what is apparently a quartet of doublets (dq). The estimation routine was able to resolve this dq structure, however the large wiggles in the residual again imply that under-fitting has occurred, and each oscillator in the parameter set is in fact being used to fit two or more signals present in the FID. Again, at the field strength used to acquire the FID, it is unlikely that an accurate resolution of all 16 signals by estimation is feasible.

At this point, with two examples provided of cases where poor RSS fits have resulted, one may question whether the underlying model is actually suited to describe the data. There is for example precedent for fitting oscillators with non-exponential decay profiles — profiles which lead to Voigt and Gaussian spectral lineshapes are common — to improve the model fit[107]. However, for some multiplet structures in Figure 3.2, exceptionally good agreement between the model and data are made, using a parsimonious set of parameters. With three couplings of different magnitude, spin (O) exhibits a “ddd” multiplet structure in which all 8 signals are discernible. The NLP routine performed well in taking the initial guess from the MPM — featuring the correct number of oscillators albeit with spurious phases — and generating a well-phased set of oscillators defining the ddd structure, with a very small associated residual. This highlights that in cases where all signals present in a given frequency region are resolvable, exceptionally good fits can be achieved using the exponentially-damped sinusoids model.

### 3.1.3 Cyclosporin A

The estimation routine was also applied to selected regions of a  $^1\text{H}$  pulse-acquire dataset of cyclosporin A [Structure in appendix](#) — a cyclic peptide comprising 11 amino acids — in benzene-



**Figure 3.3:** Result of applying the estimation routine to selected regions of a pulse-acquire dataset of cyclosporin A in benzene-d<sub>6</sub>. The figure is of a similar layout to Figure 3.2. Coloured peaks correspond to oscillators which have been assigned to multiplet structures of known spins. Grey oscillators correspond to those with an unknown association to a particular spin.

$d_6$ . The regions considered all comprise signals arising from protons bound to  $C^\alpha$  atoms in the peptide backbone[108]. The estimation procedure used was equivalent to that used for the andrographolide example. For the most downfield region considered, featuring signals from spins (A) and (B), the MPM performed admirably, with the two well-resolved dd multiplet structures present accurately parametrised by 8 oscillators in the model; the NLP routine hardly perturbed the initial guess as a result.

The most downfield region contains three separate multiplet structures featuring significant signal overlap in the Fourier domain, particularly with signals corresponding to spins (E) and (F). The MPM produced sufficient oscillators to model these structures (see Table 3.1 for an outline of the structures present). However, particularly in the most crowded section around 4.96 ppm to 4.92 ppm it can be seen that certain oscillators have phases which noticeably deviate from  $0^\circ$ . In applying the NLP routine, not only did the phases become more consistent, but the set of oscillators became more in agreement with the multiplet structures present. For example, the highest- and lowest-frequency oscillators in the model associated with the 1:3:6:3:1 quintet of spin (F) (denoted by  $\dagger$  in panels b & c of the figure) acquire amplitudes which are much closer in value as expected. The most notable flaw in the final result is associated with the two oscillators marked by  $\ddagger$  in panel c, both of which are associated with the 1:3:1:3:3:1:3:1 dq structure from spin (E). A 1:3 amplitude ratio is expected between these oscillators. However, the final NLP result assigned these with an unexpected ratio of  $\approx 1 : 1$ . It is not surprising that greater deviations from expected behaviour occur in more heavily crowded spectral regions, since there is a larger set of values in the parameter space which will lead to acceptable fits of the data in an RSS sense. Nonetheless, armed simply with knowledge that the data is phased, the routine performs admirably in highlighting how the spectrum breaks down into its various multiplet structures. An improved estimation result could be attained by supplying the NLP routine with more knowledge. For example, one could include extra constraints to ensure that the green oscillators in panel c of Figure 3.3 agree with the aforementioned relative ratios. While this has not been implemented in this work, it is discussed in Section 6.2 as a possible pursuit for the future.

## 3.2 Amplitude-attenuated Datasets

There are a number of NMR experiments in which the variation of a particular pulse sequence parameter over a number of iterations leads to the generation of a series of FIDs with the same form except for discrepancies in their amplitudes. In this section, an extension of the established 1D estimation technique is described, facilitating the analysis of datasets acquired using these experiments. After the most prominent examples of the relevant experiments are introduced, the theory behind the extended estimation method is described. Finally, its performance when ap-

plied to both simulated and experimental datasets is showcased.

### 3.2.1 Relaxation experiments

Any spin system which has been perturbed from its equilibrium position will eventually return to equilibrium due to relaxation. As introduced in Chapter 1, the simplest model of relaxation centers around two processes: longitudinal relaxation and transverse relaxation, whose rates are quantified by the times  $T_1$  and  $T_2$  respectively. The  $T_1$  and  $T_2$  values of the spins in a sample provide valuable insight into the chemical system being studied, and can also help to guide spectroscopists in the determination of optimal pulse sequence parameters\*. Numerous factors affect  $T_1$  and  $T_2$ , including the rate at which the spin tumbles in space, and its electronic environment.

#### Measuring $T_1$ : Inversion recovery

The inversion recovery experiment involves the simple pulse sequence  $180^\circ \rightarrow \tau \rightarrow 90^\circ \rightarrow t^{(1)}$ , where  $t^{(1)}$  is the period during which FID acquisition takes place. The initial  $180^\circ$  pulse inverts the magnetisation, so that it is along  $-z$  from the Bloch model perspective. During  $\tau$ , the spin system undergoes longitudinal relaxation, with the spin state populations gradually being driven back to their equilibrium configuration. The  $90^\circ$  pulse rotates the magnetisation into the transverse plane, enabling detection. The resultant phase and magnitude of the signal is directly related to the amount of time that longitudinal relaxation is allowed to occur. With  $\tau = 0\text{ s}$ , a signal with maximal amplitude, but a phase of  $180^\circ$ , equivalent to a negative amplitude, will result. At the other extreme of  $\tau \gg T_1$ , the spin system will have reverted back to equilibrium, such that the signal will also have maximal amplitude, but a phase of  $0^\circ$ . By sequentially adjusting  $\tau$  in a 2D experiment, a series of FIDs will be obtained in which the intensity of a given signal, arising from a spin with longitudinal time  $T_1$ , will vary according to

$$\alpha(\tau) = \alpha_\infty \left( 1 - 2 \exp\left(-\frac{\tau}{T_1}\right) \right), \quad (3.2)$$

where  $\alpha_\infty$  is the intensity of the signal when the spin system has returned to equilibrium. Note that  $\alpha(0) = -\alpha_\infty$ , as the magnetisation has been completely inverted, and no time has been allowed for longitudinal relaxation to take place. An example of a series of spectra acquired using a (simulated) inversion recovery experiment is given by panel d in Figure 3.5.

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\*For example, after a pulse sequence has been run, it is necessary to include a delay (often called the *relaxation delay*) prior to re-running it, to enable the spin system's longitudinal magnetisation to sufficiently recover. Having an understanding of the  $T_1$  values associated with a sample can help to determine a relaxation delay which is long enough to facilitate the recovery, but that is not overly long, to avoid an experiment time which is longer than necessary.

### Measuring $T_2$ : CPMG

Inspired by the inversion recovery experiment, one might assume that the pulse sequence  $90^\circ \rightarrow \tau \rightarrow t^{(1)}$  would be effective for  $T_2$  determination. However the effects of J-modulation would generate undesirable spectra with phase-modulated peaks. As well as this the presence of field inhomogeneities will cause relaxation at a faster rate than anticipated; the effect of field inhomogeneities is incorporated into the “observed” transverse relaxation time,  $T_2^* < T_2^\dagger$ [109]. The effects of J-modulation and field inhomogeneity can be nullified if rapid refocussing is applied, by subjecting the spin system to a train of spin echoes. The classic route to  $T_2$  measurement is the Carl-Purcell-Meiboom-Gill (CPMG) experiment[110, 111], comprising  $90^\circ_x \rightarrow [\tau \rightarrow 180^\circ_y \rightarrow \tau]_n \rightarrow t^{(1)}$ , where the spin echo duration  $\tau$  is short and fixed, and the number of cycles  $n$  can be varied to alter the total evolution time. The number of CPMG cycles applied affects the intensity of the resulting signal according to

$$\alpha(n) = \alpha_0 \exp\left(-\frac{2\tau n}{T_2}\right), \quad (3.3)$$

where  $\alpha_0$  is the intensity where no spin echo cycles were employed, such that the pulse sequence is reduced to the standard pulse-acquire experiment. Recent enhancements to the CPMG approach, including the Periodic Refocusing of J Evolution by Coherence Transfer (PROJECT) pulse sequence[112] are also well-suited to  $T_2$  determination.

### 3.2.2 Diffusion experiments

NMR is well established as a means of determining the rates of translational diffusion of chemical species[113, 114]. The rate of translation of a species is given by the translational diffusion coefficient,  $D$  ( $\text{m}^2 \text{s}^{-1}$ )[115: Chapter 19]. The first showcase for determining the diffusion coefficient using NMR came from Stejskal and Tanner, in which they described the pulsed gradient spin echo (PGSE) pulse sequence[116] (Figure 3.4.a). The PGSE sequence consists of a conventional spin-echo ( $90^\circ_x \xrightarrow{\tau} 180^\circ_y \xrightarrow{\tau} \text{acquire}$ ), with pulsed field gradients (PFGs) applied after each of the RF pulses. As a simple overview of how the pulse sequence works, consider a single spin on resonance with the transmitter (i.e. its rotating frame frequency is zero) in a sample tube at position  $z \in [-l_z/2, l_z/2]$  along the main field axis, where  $l_z$  is the length of the sample lying within the receiver coil ( $\approx 1.5$  cm). After the  $90^\circ$  pulse, the magnetisation will be  $-M_y$ . During the first PFG, the spin’s resonance frequency will become  $\omega_{\text{PFG}} = -\gamma g z$ , where  $g$  is the strength of the PFG ( $\text{T m}^{-1}$ )<sup>‡</sup>. Assuming the gradient is applied for a time  $\delta$ , the spin will precess by an angle of

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<sup>†</sup> $T_2^*$  is defined by the expression  $1/T_2^* := 1/T_2 + \gamma \Delta B_0$ , where  $\Delta B_0$  is the variation in magnetic field strength across the sample volume.

<sup>‡</sup>Gradient strengths are often expressed in units of  $\text{G cm}^{-1}$ , which is equivalent to  $10^{-2} \text{ T m}^{-1}$ .

$\alpha = -\gamma g z \delta$ . After the  $180^\circ$  pulse, the spin's magnetisation is as follows:

$$-M_y \xrightarrow{\text{PFG}} -M_y \cos(\alpha) + M_x \sin(\alpha) \xrightarrow{180^\circ} -M_y \cos(\alpha) - M_x \sin(\alpha).$$

Suppose the spin has moved to a new position  $z + \Delta_z$  between the end of the first gradient and the beginning of the second. Application of the second gradient will cause precession by the angle  $\beta = -\gamma g(z + \Delta_z)\delta$ :

$$\begin{aligned} & \xrightarrow{\text{PFG}} -M_y \cos(\alpha) \cos(\beta) + M_x \cos(\alpha) \sin(\beta) - M_x \sin(\alpha) \cos(\beta) - M_y \sin(\alpha) \sin(\beta) \\ &= -M_y \cos(\gamma g \delta \Delta_z) - M_x \sin(\gamma g \delta \Delta_z), \end{aligned}$$

The PFGs have been employed to encode the change in  $z$ -coordinate of the spin after a known amount of time, by influencing the phase of the magnetisation relative to its phase immediately after the  $90^\circ$  pulse. Extending this idea to a system of many identical spins, which will translate by different extents between the PFGs, individual spin contributions to the bulk magnetisation will become dephased, leading to an attenuation of the amplitude of the resulting FID. For species which diffuse at a faster rate, this effect is more severe, such that a more rapid attenuation results.

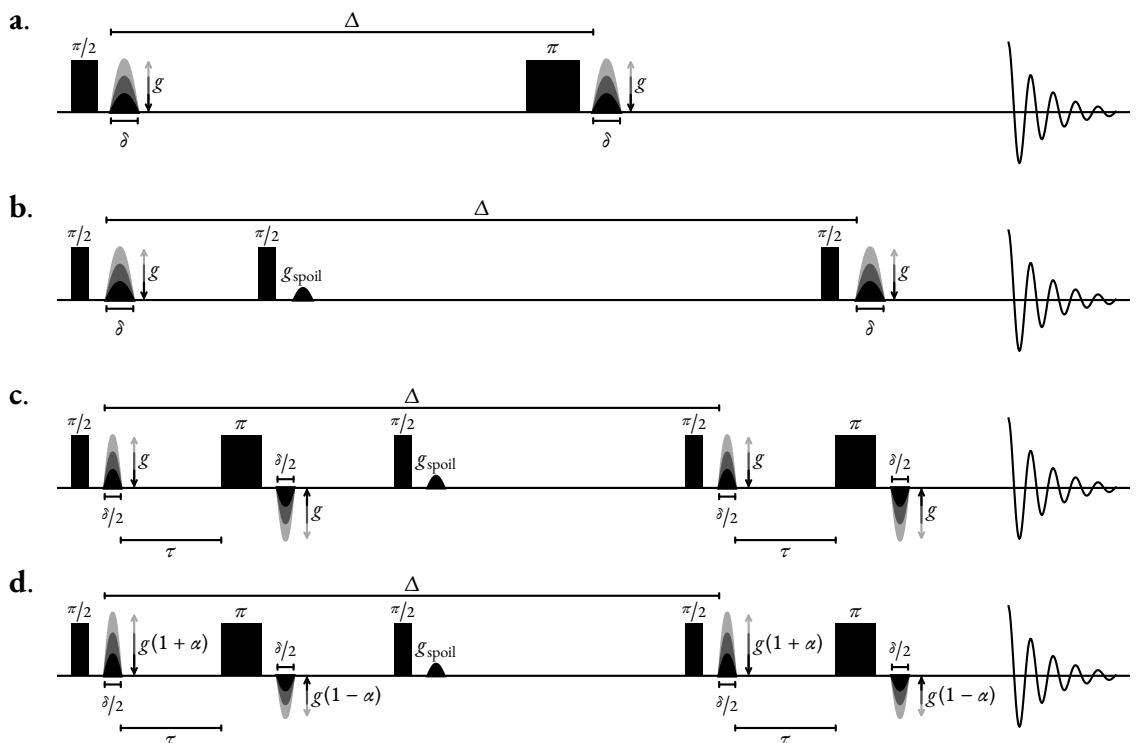
Through consideration of the Bloch-Torrey equations[117], which extend the classic Bloch equations to account for the effects of diffusion on magnetisation, the following equation, known as the *Stejskal-Tanner equation*, may be derived:

$$\alpha(g) = \alpha_0 \exp\left(-\gamma^2 \delta^2 g^2 D \left(\Delta - \frac{\delta}{3}\right)\right), \quad (3.4)$$

where  $\alpha_0 = \lim_{g \rightarrow 0} \alpha$ ,  $\delta$  is the duration of each PFG (s), and  $\Delta$  is the delay between the PFGs, often known as the *diffusion time* (s). While Equation 3.4 is widely stated in the diffusion NMR literature, it is only strictly applicable when the PGSE sequence is used, and PFGs with rectangular amplitude profiles are applied<sup>§</sup>. As will be discussed soon, the exact form of the pulse sequence impacts the functional form by which  $\alpha(g)$  varies.

Tanner introduced a variant of the original PGSE experiment called pulsed gradient stimulated echo (PGSTE)[118] (Figure 3.4.b). Instead of the diffusion period being bisected by a  $180^\circ$  pulse, PGSTE features two  $90^\circ$  pulses at the beginning and end of the diffusion period. Hence, signal loss due to decoherence is a result of longitudinal relaxation in PGSTE, as opposed to transverse relaxation in PGSE. PGSTE is therefore favoured in scenarios where  $T_1 \ll T_2$ , as improved data sensitivity is achievable.

<sup>§</sup>Rectangular PFGs (i.e. those in which there is an infinitesimal time to rise to full strength, and to fall back to zero) are technically impossible to achieve as they would require gradient coils with zero inductance, though in practice it is possible to generate gradients with behaviour close to this.



**Figure 3.4:** Pulse sequences used for the determination of translational diffusion constants. **a.** PGSE, **b.** PGSTE, **c.** PGSTEBP, **d.** One-shot DOSY. RF pulses are denoted by solid rectangles. Diffusion-encoding gradients are denoted by sine-bell shapes with varying shades, indicating that the intensity ( $g$ ) is incremented to create a 2D dataset. Spoiler gradients are denoted by solid black sine-bell shapes.

Both PGSE and PGSTE employ *monopolar* PFGs for diffusion encoding. Experiments also exist which employ *bipolar* gradient elements, which consist of a PFG, followed by a 180° pulse, and then a second PFG with the opposite polarity to the first[119, 120]. The pulsed gradient stimulated echo with bipolar gradients (PGSTEBP) experiment (Figure 3.4.c) can be thought of as the bipolar analogue of PGSTE. Bipolar gradients are useful in circumstances where it is important to purge the effects of static gradients in the sample, caused by field inhomogeneities. Morris and coworkers have developed the *one-shot* experiment[121] (Figure 3.4.d), which requires a single transient per gradient strength (i.e. there is no requirement for a phase-cycling scheme). This is achieved through the use of bipolar gradients which comprise asymmetrical PFGs with relative powers  $1 + \alpha : 1 - \alpha$  for some  $0 > \alpha > 1$  (commonly,  $\alpha = 0.2$ ).

The most common means of conducting a diffusion experiment is to run one of pulse sequences mentioned above (or variants thereof) with  $g$  varied across increments. It is virtually always the case that the FID's signal amplitudes will abide by the following general form of the Stejskal-Tanner equation, regardless of the exact pulse sequence used:

$$\alpha(g) = \alpha_0 \exp(-cg^2D), \quad (3.5)$$

for some constant  $c$  ( $T s^{-2}$ ). The functional form of  $c$  depends on the type of experiment used, as well as the amplitude profile (*shape*) of the PFGs. A consideration of the Bloch-Torrey equations for a given experiment is necessary, with an extensive overview provided by Sinnaeve for most diffusion NMR experiments[122]. In general,  $c$  is as follows:

$$c = \gamma^2 \delta^2 \sigma^2 \Delta'. \quad (3.6)$$

$\sigma$  is the *shape factor* of the PFGs (*vide infra*), and  $\Delta'$  is the effective time that diffusion is allowed to occur. Examples of the form that  $\Delta'$  takes include:

$$\Delta' = \begin{cases} \Delta + 2(\kappa - \lambda)\delta & \text{PGSE, PGSTE} \\ \Delta + \frac{(2\kappa - 2\lambda - 1)\delta}{4} - \frac{\tau}{2} & \text{PGSTEBP} \\ \Delta + \frac{(\kappa - \lambda)(\alpha^2 + 1)\delta}{2} + \frac{(\delta + 2\tau)(\alpha^2 - 1)}{4} & \text{One-shot} \end{cases}. \quad (3.7)$$

$\tau$  is the delay between the initial PFG and the 180° pulse in experiments with bipolar gradients. The factors  $\sigma$ ,  $\lambda$ , and  $\kappa$  are related to the shape function  $s(\epsilon) : \epsilon \in [0, 1]$  of the PFG, which describes the variation of the gradient amplitude as a function of its progression. For a rectangular gradient,  $s(\epsilon) = 1 \forall \epsilon$ , whereas for a sine-bell gradient,  $s(\epsilon) = \sin(\pi\epsilon)$ . The cumulative distribution

of the shape function is given by:

$$S(\epsilon) = \int_0^\epsilon s(\epsilon') d\epsilon' \quad \forall \epsilon \in [0, 1]. \quad (3.8)$$

The corresponding definition of  $S$  for the case of a gradient made of  $N$  discrete steps with shape  $s \in \mathbb{R}^N$  is

$$S_n = \frac{1}{n} \sum_{i=1}^n s_i \quad \forall n \in \{1, \dots, N\}, \quad (3.9)$$

$\sigma$ ,  $\lambda$ , and  $\kappa$  are related to the shape function cumulative distribution as follows:

$$\sigma = S(1), \quad (3.10a)$$

$$\lambda = \frac{1}{\sigma} \int_0^1 S(\epsilon) d\epsilon, \quad (3.10b)$$

$$\kappa = \frac{1}{\sigma^2} \int_0^1 S^2(\epsilon) d\epsilon, \quad (3.10c)$$

with their discrete counterparts being:

$$\sigma = S_N \quad (3.11a)$$

$$\lambda = \frac{1}{\sigma N} \sum_{n=1}^N S_n = \frac{1}{\sigma N} \sum_{n=1}^N \left( \frac{1}{n} \sum_{i=1}^n s_i \right) \quad (3.11b)$$

$$\kappa = \frac{1}{\sigma^2 N} \sum_{n=1}^N S_n^2 = \frac{1}{\sigma^2 N} \sum_{n=1}^N \left( \frac{1}{n} \sum_{i=1}^n s_i \right)^2. \quad (3.11c)$$

For PFGs with a symmetrical shape,  $\lambda = 1/2$ .  $\kappa$  is typically equal to or close to  $1/3$ . It can now be seen that the original Stejskal-Tanner equation (Equation 3.4) for the PGSE experiment comes from inserting Equation 3.7 into Equation 3.6, assuming a rectangular shape factor for the PFG:  $\sigma = 1$ ,  $\lambda = 1/2$ , and  $\kappa = \frac{1}{3}$ . In many situations,  $\Delta$  dominates in the expression of  $\Delta'$ , and so ensuring the correct form of  $c$  could be seen as excessive. However, especially when  $\Delta$  is not orders of magnitude greater than  $\delta$ , the exact form of  $\Delta'$  used in Equation 3.6 will be important for accurate measurements of the diffusion coefficient.

Determining the quantity of interest from the above experiments is most typically done using the following procedure:

1. The series of FIDs are processed in an equivalent fashion, leading to a set of 1D spectra.
2. Peak-picking is performed to locate the chemical shift values which correspond to signals of interest within the spectra.
3. For each chemical shift of interest, the values of the spectra are extracted, and the relevant function (see Table 3.2) is fit to these values.

This method is *univariate* in the sense that it considers a single sample (chemical shift) in isolation from the rest of the data. It is popular to visualise the result of univariate fitting by plotting 2D pseudo-spectra, featuring axes denoting (a) chemical shift, and (b) the parameter of interest. Distributions taking into account the predicted value of interest and the associated uncertainty are plotted at each chemical shift. In the context of diffusion NMR, this form of data analysis is referred to as diffusion-ordered spectroscopy (DOSY)[114]. The DOSY approach works well in cases where peaks of interest are intense and well-resolved. However, when there is considerable peak overlap, accurately determining the parameter of interest associated with a given signal becomes more challenging, since nearby signals will influence the rate of amplitude decay at the chemical shift of interest. An aggregated value of the contributing decay rates will be predicted using the above approach. In such cases, it is possible to instead fit a superposition of functions to the spectral amplitudes, as a means of separating out contributions from the overlapping signals[123]. However, this process is usually only effective when the data has very high SNR, and the quantities of interest associated with the overlapping signals differ considerably.

An alternative approach is to use a *multivariate* analysis method, which considers the entire spectrum holistically, and attempts to decompose the spectrum into components with different decay rates. Prominent examples of multivariate methods developed for diffusion data analysis are direct exponential curve resolution algorithm (DECRA)[124] and *speedy* component resolution (SCORE)[125], an improvement over the original CORE[126, 127]. Multivariate techniques tend to only be only effective in situations where a few (2 or 3) different signal decay rates are present. In diffusion NMR, each molecule in the sample will give rise to the same decay rate across its signals (effects such as chemical exchange can lead to exceptions to this: see Figure 3.6). These methods are generally unsuitable for inversion recovery and CPMG datasets: each spin in a sample will possess different  $T_1$  and  $T_2$  values, such that a far greater number of decay rates will be present.

### 3.2.3 Methodology

A straightforward extension of 1D parametric estimation provides a route to estimating amplitude-attenuated datasets in a fashion with similarities to the traditional univariate (DOSY) approach. In this section, the theory of this method is discussed.

The datasets of interest can be considered in a general fashion. Suppose the experiment is run with  $K \in \mathbb{N}$  increments, such that there is a vector  $\mathbf{p} \in \mathbb{R}^K$  comprising the values of the pulse sequence variable used to acquire each 1D FID in the data. The complete dataset is expected to take the form  $\mathbf{Y} \in \mathbb{C}^{K \times N}$  in which the value of the pulse sequence variable affects the amplitudes of the

contributing signals:

$$\gamma_{k,n} = \sum_{m=1}^M a_{k,m} \exp(i\phi_m) \exp((2\pi i(f_m - f_{\text{off}}) - \eta_m)n\Delta_t). \quad (3.12)$$

$\forall k \in \{1, \dots, K\}$ ,  $\forall n \in \{0, \dots, N-1\}$ .  $\mathbf{A} \in \mathbb{R}^{K \times M}$  is a matrix of the signal amplitudes across the FIDs:

$$\mathbf{A} = \begin{bmatrix} a_{1,1} & a_{1,2} & \cdots & a_{1,M} \\ a_{2,1} & a_{2,2} & \cdots & a_{2,M} \\ \vdots & \vdots & \ddots & \vdots \\ a_{K,1} & a_{K,2} & \cdots & a_{K,M} \end{bmatrix} \quad (3.13)$$

A complete parameter vector for the dataset is given by  $\theta \in \mathbb{R}^{(K+3)M}$ :

$$\theta = [a_1 \ \cdots \ a_K \ \phi^T \ f^T \ \eta^T]^T, \quad (3.14)$$

where  $a_k$  denotes the relevant row in  $\mathbf{A}$ . The amplitudes are a function of the pulse sequence variable with the following form:

$$a_{k,m} = a_{0,m} \mathcal{A}(\psi_m | p_k). \quad (3.15)$$

$a_0 \in \mathbb{R}^M$  is a vector of the “maximal amplitudes” of the signals, and  $\psi \in \mathbb{R}^M$  is a vector of the parameter of interest ( $T_1, T_2, D$ ) associated with each signal.  $a_{0,m}$  can be thought of as the largest possible amplitude that could be obtained for signal  $m$  with the given pulse sequence:

- In an inversion recovery experiment, the largest amplitude is achieved as  $\tau \rightarrow \infty$ , as the spin system will have returned back to equilibrium prior to the  $90^\circ$  pulse.
- With CPMG experiments, the largest amplitude will occur when  $n = 0$ , as no time is designated for transverse relaxation to take place.
- For diffusion experiments, the largest amplitude is achieved when  $g = 0$ , since no diffusion-induced dephasing of spins will have occurred.

The function  $\mathcal{A}$  describes how the amplitudes of resonances are attenuated by the experimental variable, and has a form which is intimately linked to the type of experiment. For the experiments described in Sections 3.2.1 and 3.2.2, the forms of  $\mathcal{A}$  are listed in Table 3.2.

### Estimating amplitude-attenuated datasets

The close relationship between the FIDs within the dataset means that completely estimating all of them separately, without exploiting information from previously estimated FIDs, is unnecessary. Instead, after the first increment is estimated without prior knowledge, yielding  $\theta_{k=1} \in \mathbb{R}^{4M}$ , the

Experiment	$p$	$\psi$	$\mathcal{A}(\psi p)$	$\frac{\partial \mathcal{A}(\psi p)}{\partial \psi}$	$\frac{\partial^2 \mathcal{A}(\psi p)}{\partial \psi^2}$
Inv. Recov.	$\tau$	$T_1$	$(1 - 2 \exp(-\frac{\tau}{T_1}))$	$-\frac{2\tau}{T_1^2} \exp(-\frac{\tau}{T_1})$	$\frac{2\tau}{T_1^3} \exp(-\frac{\tau}{T_1}) (2 - \frac{\tau}{T_1})$
CPMG	$n$	$T_2$	$\exp(-\frac{2\tau n}{T_2})$	$\frac{2\tau n}{T_2^2} \exp(-\frac{2\tau n}{T_2})$	$\frac{2\tau n}{T_2^3} \exp(-\frac{2\tau n}{T_2}) (\frac{2\tau n}{T_2} - 2)$
Diffusion	$g$	$D$	$\exp(-cg^2 D)$	$-cg^2 \exp(-cg^2 D)$	$c^2 g^4 \exp(-cg^2 D)$

**Table 3.2:** The various functional forms of  $\mathcal{A}$  according to the different amplitude-attenuating NMR experiments considered, along with its first and second derivatives, which are required to extract estimates of  $\psi$  using NLP.

phases, frequencies and damping factors, all of which should remain the same across the FIDs, are fixed. Subsequent parameter estimates are determined by taking the estimate of the previous FID, and subjecting it to an NLP routine in which only the amplitudes are optimised. Thus, estimating each iteration  $k \in \{2, \dots, K\}$  is reduced to the problem<sup>¶</sup>

$$\boldsymbol{a}_k = \arg \min_{\boldsymbol{a} \in \mathbb{R}^M} \mathcal{F}(\boldsymbol{a} | \boldsymbol{\phi}_{k=1}, \boldsymbol{f}_{k=1}, \boldsymbol{\eta}_{k=1}, \boldsymbol{y}_k). \quad (3.16)$$

An NLP routine can solve this very efficiently, typically in a few iterations, on account of the linear dependence of the model with respect to the oscillator amplitudes. The linear dependence means that second derivatives of the model are all zero (see Equation 2.47a), such that only first derivatives need to be computed to derive an exact Hessian matrix of the fidelity. Due to the linear dependence on amplitudes, an alternative means of deriving amplitudes for each increment is to determine the following:

$$\boldsymbol{a}_k = \boldsymbol{Z}^+ \boldsymbol{y}_k, \quad (3.17a)$$

$$\boldsymbol{Z} = \begin{bmatrix} 1 & \dots & 1 \\ z_1 & \dots & z_M \\ \vdots & \ddots & \vdots \\ z_1^{N-1} & \dots & z_M^{N-1} \end{bmatrix} \begin{bmatrix} \exp(i\phi_1) \\ \vdots \\ \exp(i\phi_M) \end{bmatrix}, \quad (3.17b)$$

$$z_m = \exp((2\pi i(f_m - f_{\text{off}}) - \eta_m)\Delta_t). \quad (3.17c)$$

An outline of the estimation procedure is provided by Algorithm 3.1.

<sup>¶</sup> $\mathcal{F}$  in Equation 3.16 reads as “the fidelity with respect to the amplitudes  $\boldsymbol{a}$ , given phases  $\boldsymbol{\phi}_{k=1}$ , frequencies  $\boldsymbol{f}_{k=1}$ , damping factors  $\boldsymbol{\eta}_{k=1}$ , and FID  $\boldsymbol{y}_k$ ”. The fidelity has exactly the same mathematical form as Equation 2.44, though it has been emphasised that the phases, frequencies and damping factors are no longer variables to be optimised, but fixed parameters.

---

**Algorithm 3.1** Routine for estimating a sequence of 1D FIDs which exhibit variation in amplitudes across increments. NLPAMP denotes a routine which is akin to NLP (Algorithm 2.2), except only amplitudes are optimised; phases, frequencies and damping factors are fixed.

---

```

1: procedure ESTIMATEAMPATTENUATED(  $Y \in \mathbb{C}^{K \times N}$ ,  $\mathbf{r}_{\text{interest}} \in \mathbb{R}^2$ ,  $\mathbf{r}_{\text{noise}} \in \mathbb{R}^2$ ,  $M \in \mathbb{N}_0$  )
2:    $\theta_1, \epsilon_1 \leftarrow \text{ESTIMATE1D}(y_1, \mathbf{r}_{\text{interest}}, \mathbf{r}_{\text{noise}}, M)$ ;                                 $\triangleright$  Estimate first increment
3:    $M \leftarrow \text{len}(\theta_1)/4$ ;
4:    $\theta, \epsilon \leftarrow \mathbf{0} \in \mathbb{R}^{(K+3)M}, \mathbf{0} \in \mathbb{R}^{(K+3)M}$ ;                                 $\triangleright$  Initialise complete parameter vector.
5:    $\theta[:M], \epsilon[:M] \leftarrow \theta_1[:M], \epsilon_1[:M]$ ;                                 $\triangleright$  Amplitudes for first increment.
6:    $\theta[KM:], \epsilon[KM:] \leftarrow \theta_1[M:], \epsilon_1[M:]$ ;       $\triangleright$  Phases, frequencies and damping factors, which are held
   constant across increments.
7:   for  $k = 2, \dots, K$  do
8:      $\tilde{\mathbf{y}} \leftarrow \text{FILTER1D}(y_k, \mathbf{r}_{\text{interest}}, \mathbf{r}_{\text{noise}})$ ;                                 $\triangleright$  Algorithm 2.3.
9:      $\theta_k, \epsilon_k \leftarrow \text{NLPAMP}(\tilde{\mathbf{y}}, \theta_k)$ ;
10:     $\theta[kM:(k+1)M], \epsilon[kM:(k+1)M] \leftarrow \theta_k[:M], \epsilon_k[:M]$ ;       $\triangleright$  Extract amplitudes.
11:   end for
12:   return  $\theta, \epsilon$ ;
13: end procedure

```

---

### Determining the parameter of interest

Having generated a parameter estimate for each FID in the dataset, focus now moves to determining the parameter of interest for each signal  $\psi$ . For each oscillator, the maximal amplitude and parameter of interest are determined by solving the following problem  $\forall m \in \{1, \dots, M\}$ :

$$\begin{bmatrix} a_{0,m}^{(*)} \\ \psi_m^{(*)} \end{bmatrix} = \arg \min_{[a_0 \ \psi]^T \in \mathbb{R}^2} \| \mathbf{a}_m - a_0 \mathcal{A}(\psi | \mathbf{p}) \|^2, \quad (3.18)$$

where  $\mathbf{a}_m$  corresponds to the  $m^{\text{th}}$  column of  $\mathcal{A}$ . This is another example of an RSS problem, which can be solved using an NLP routine as already described. The gradient vector and Hessian matrix of the fidelity take very similar functional forms to those for FID estimation for this reason (see Equation 2.45a and Equation 2.45b), and are as follows  $\forall i, j \in \{0, 1\}$ :

$$g_i = -2 \left( \mathbf{a}_m - a_0 \mathcal{A}(\psi | \mathbf{p}), \frac{\partial a_0 \mathcal{A}(\psi | \mathbf{p})}{\partial \theta_i} \right), \quad (3.19a)$$

$$b_{i,j} = 2 \left( \left( \frac{\partial a_0 \mathcal{A}(\psi | \mathbf{p})}{\partial \theta_i}, \frac{\partial a_0 \mathcal{A}(\psi | \mathbf{p})}{\partial \theta_j} \right) - \left( \mathbf{a}_m - a_0 \mathcal{A}(\psi | \mathbf{p}), \frac{\partial^2 a_0 \mathcal{A}(\psi | \mathbf{p})}{\partial \theta_i \partial \theta_j} \right) \right), \quad (3.19b)$$

$$\theta = [a_0 \ \psi]^T, \quad (3.19c)$$

with explicit expressions for the requisite first and second derivatives being

$$\frac{\partial a_0 \mathcal{A}(\psi | \mathbf{p})}{\partial a_0} = \mathcal{A}(\psi | \mathbf{p}), \quad (3.20a)$$

$$\frac{\partial a_0 \mathcal{A}(\psi | \mathbf{p})}{\partial \psi} = a_0 \frac{\partial \mathcal{A}(\psi | \mathbf{p})}{\partial \psi}, \quad (3.20b)$$

$$\frac{\partial^2 \alpha_0 \mathcal{A}(\psi | \mathbf{p})}{\partial \alpha_0^2} = 0, \quad (3.20c)$$

$$\frac{\partial^2 \alpha_0 \mathcal{A}(\psi | \mathbf{p})}{\partial \psi^2} = \alpha_0 \frac{\partial^2 \mathcal{A}(\psi | \mathbf{p})}{\partial \psi^2}, \quad (3.20d)$$

$$\frac{\partial^2 \alpha_0 \mathcal{A}(\psi | \mathbf{p})}{\partial \alpha_0 \partial \psi} = \frac{\partial^2 \alpha_0 \mathcal{A}(\psi | \mathbf{p})}{\partial \psi \partial \alpha_0} = \frac{\partial \mathcal{A}(\psi | \mathbf{p})}{\partial \psi}. \quad (3.20e)$$

The functional forms of the first and second derivatives for the different experiments of interest of  $\mathcal{A}$  are given in Table 3.2.

### Displaying results

It is possible to visualise the estimation results acquired by this method in a similar fashion to DOSY analysis. For each oscillator in the estimated model, a 2D array is generated, corresponding to the outer product of the FT of the model oscillator ( $s_m$ ) and a distribution describing the predicted value of  $\psi$  ( $d_m$ ).

$$\mathbb{R}^{R \times N} \ni S = \sum_{m=1}^M d_m \otimes s_m, \quad (3.21a)$$

$$s_m = \Re(\text{FT}(x_m)), \quad (3.21b)$$

$$x_{m,n} = \alpha_{0,m} \exp(i\phi_m) \exp((2\pi i(f_m - f_{\text{off}}) - \eta_m)n\Delta_t), \quad (3.21c)$$

where  $R \in \mathbb{N}$  is the number of samples to generate the distribution from. The exact form that the distribution  $d_m$  should take is arbitrary, though it should indicate two key pieces of information: (a) its maximum should coincide with the predicted value of  $\psi_m$ , and (b) its broadness should indicate the level of uncertainty associated with the prediction. In this work, the distribution used is a Gaussian distribution with mean  $\psi_m$  and standard deviation  $c\epsilon_m$ , where  $\epsilon_m$  is the estimation error associated with oscillator  $m$ 's parameter of interest, and  $c \in \mathbb{R}_{>0}$  is an arbitrary broadening factor which can be chosen to ensure clear visibility of the peaks.<sup>||</sup>

$$d_{m,r} = -\frac{1}{\sqrt{2\pi(c\epsilon_m)^2}} \exp\left(-\frac{(p_r - \psi_m)^2}{2(c\epsilon_m)^2}\right) \quad \forall r \in \{1, \dots, R\}, \quad (3.22a)$$

$$p_r = p_{\min} + \frac{(r-1)(p_{\max} - p_{\min})}{R-1}. \quad (3.22b)$$

$p_{\min}$  and  $p_{\max}$  specify the range of values over which to generate the distribution. The errors  $\epsilon$  can be extracted from the Hessian matrix at convergence; more detail on this is provided in Ap-

<sup>||</sup>In cases where the error in estimating  $\psi_m$  is very small, it may be that the distribution derived from Equation 3.22 satisfies  $\max(d_m) = 0$  if the peak of the distribution does not closely coincide with any of the sampled values. The affected oscillator will not appear in the DOSY-like spectrum under these circumstances. Broadening the distribution (i.e. setting  $c > 1$ ) resolves this.

pendix B.2.

### 3.2.4 Results

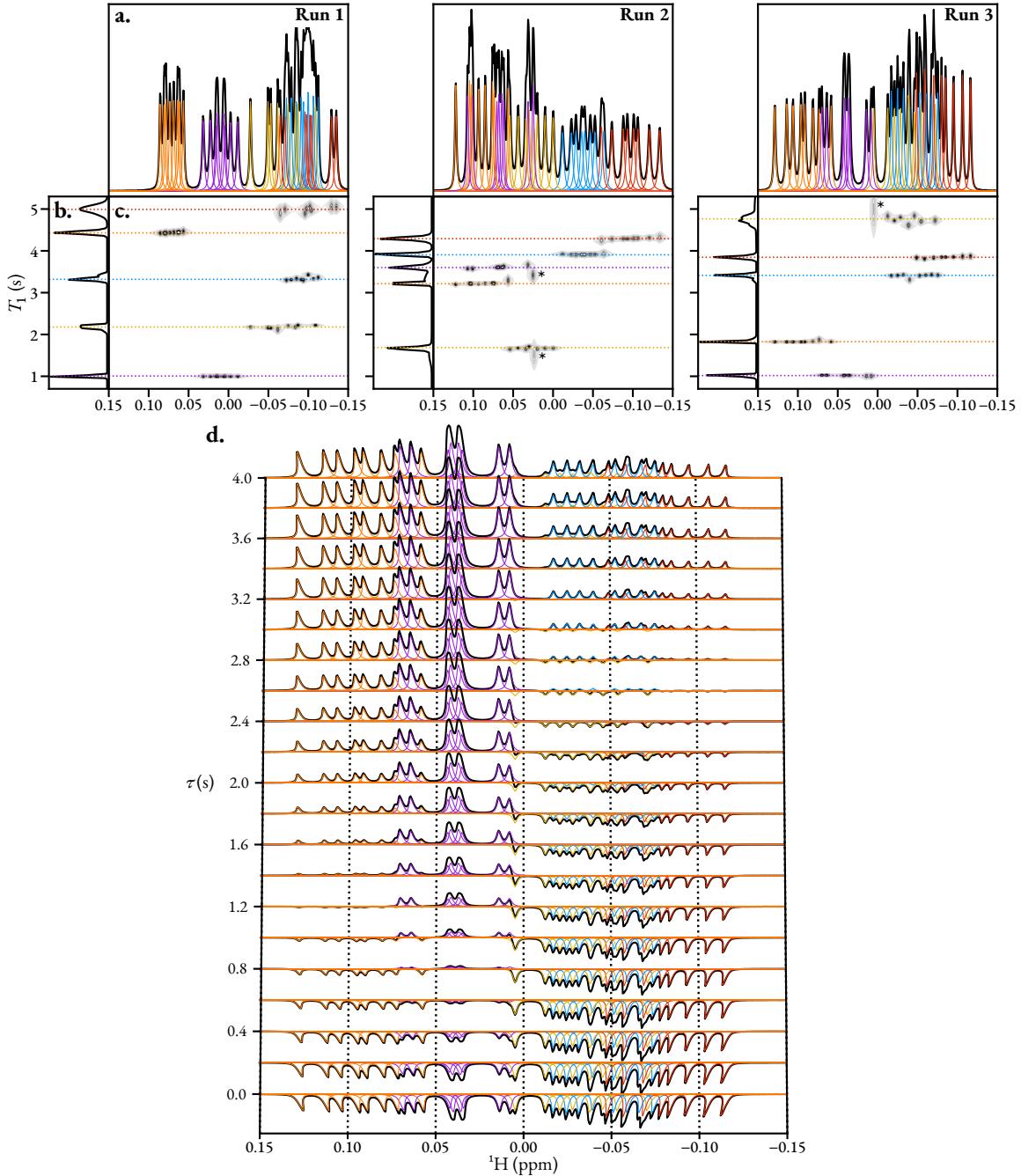
#### “Five multiplets”

Figure 3.5 shows the result achieved by applying the described method in determining the  $T_1$  associated with signals in a set of three of simulated inversion recovery datasets featuring 5 overlapping ddd multiplet structures. Each dataset was generated using spin systems such that within a known region of the spectrum (0.15 ppm to  $-0.15$  ppm) five ddd multiplet structures with significant overlap, abiding by the weak coupling approximation, were present. Constraints were placed on the shifts and couplings of the spin system to ensure that no two signals would have frequencies with a difference less than  $f_{\text{sw}}^{(1)}/N^{(1)}$ . For each spin, a  $T_1$  value was sampled from  $\mathcal{U}(1 \text{ s}, 5 \text{ s})$ , and a  $T_2$  value was sampled from  $\mathcal{U}(0.2 \text{ s}, 0.6 \text{ s})$ . The inversion recovery experiment was simulated using SPINACH, with the relaxation phenomena described by the “extended  $T_1/T_2$  approximation” (see Appendix D.1.3 for more information). Each dataset was corrupted by AWGN with a target SNR of 40 dB for the dataset as a whole. The estimation routine outlined by Algorithm 3.1 was applied to the generate a parameter estimate of the region of interest.

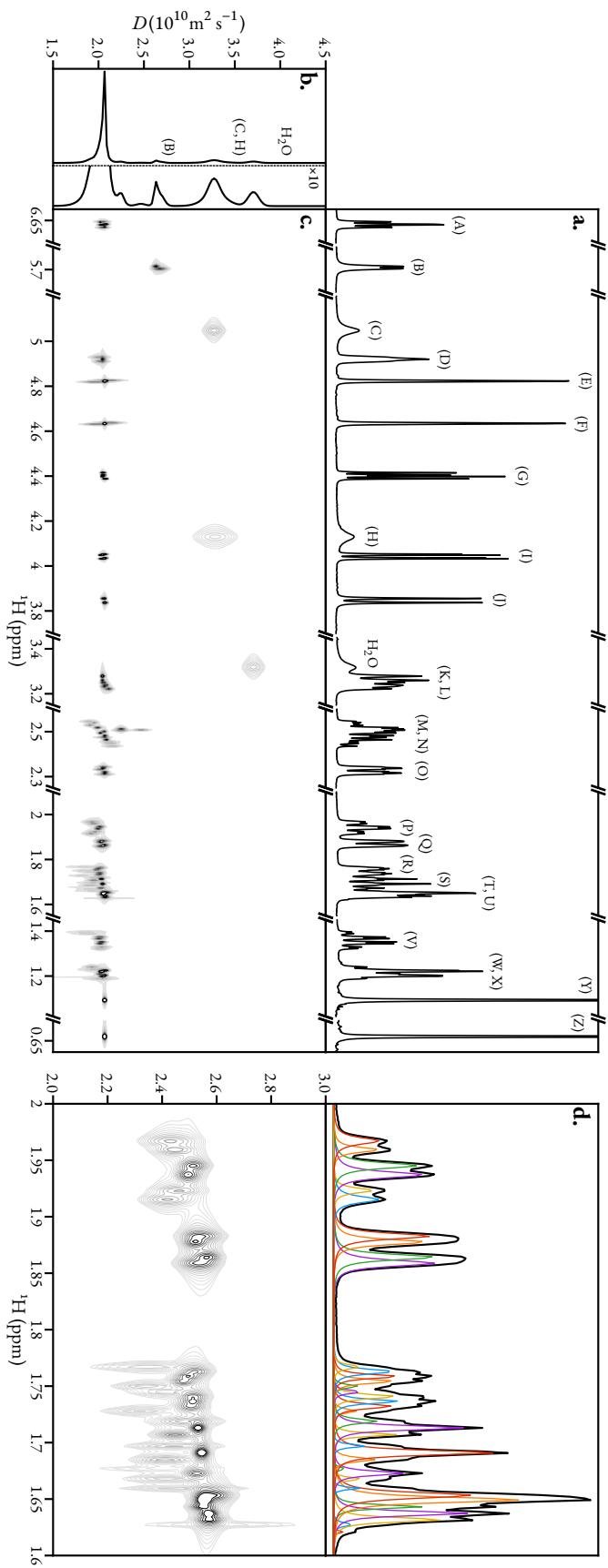
Despite heavy overlap between peaks, the routine was successful at assigning each signal in the dataset with a  $T_1$  value that closely agreed with the  $T_1$  of the spin giving rise to it (see panel b.). As is to be expected, in scenarios where little overlap existed between signals with different decay rates,  $T_1$  predictions tended to be more accurate, with smaller associated errors (see for example the purple and orange multiplets in Run 1). Nevertheless, adequate estimates could still be obtained in cases of severe overlap (see the red, blue and yellow multiplets in Run 1). Particular oscillators for which the estimate of  $T_1$  is notably far from the true value tended to be associated with large errors, with examples denoted with an asterisk in panel c.

#### Andrographolide Diffusion

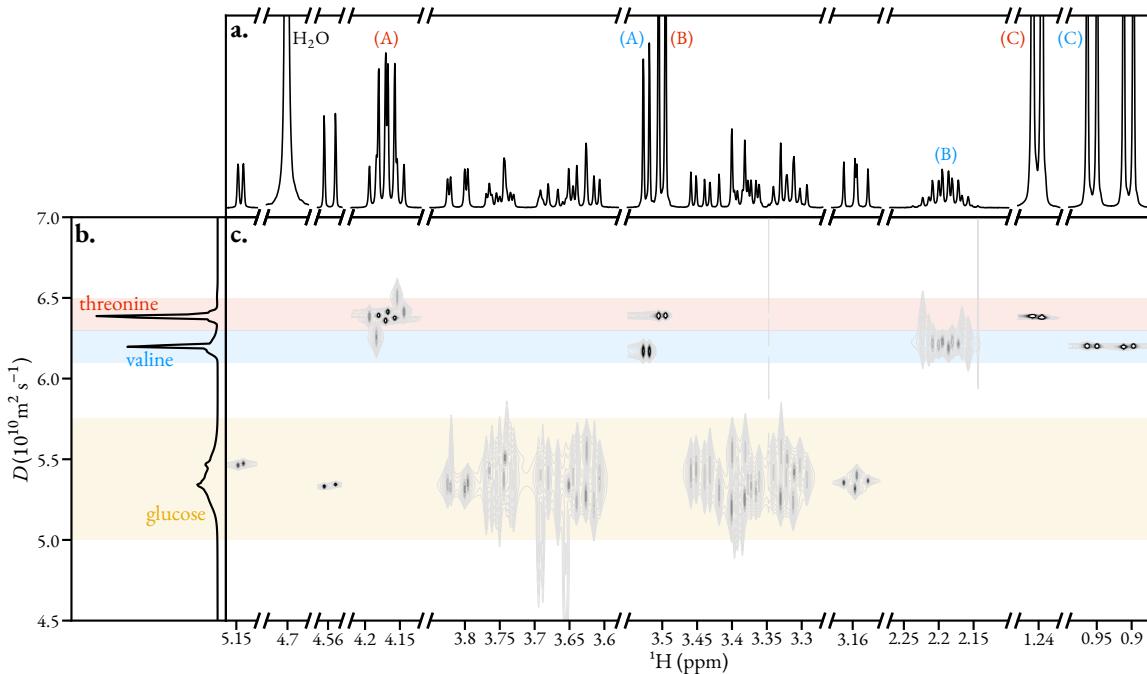
Figure 3.6 shows the result of applying the estimation technique on a oneshot DOSY dataset of andrographolide in unfresh DMSO-d<sub>6</sub> at 298 K. Exposure of the sample to water is evidenced by the broad peak around 3.3 ppm, estimated to have a diffusion constant of  $3.7 \times 10^{-10} \text{ m}^2 \text{ s}^{-1}$ . On top of this, the acidic hydroxyl protons (B, C, H) of andrographolide show significant line-broadening, and their estimated diffusion coefficients are considerably different compared with those of the non-hydroxyl protons, due chemical exchange with water in the sample[128]. The diffusion profile generated suggests a diffusion constant of andrographolide of  $2.07 \times 10^{-10} \text{ m}^2 \text{ s}^{-1}$ . The predicted diffusion constant for each estimated oscillator, especially those with greater intensity, shows decent consistency. Lower intensity oscillators, especially those which significantly



**Figure 3.5:** Three examples of results generated when considering simulated inversion recovery datasets comprising five ddd multiplet structures. **a.** Plot of the result generated for the first increment ( $\tau = 0$  s), with all the plots multiplied by  $-1$ . Black: spectrum of the data. Coloured lines: spectra of individual oscillators present in the estimated model. Oscillators with the same colour are components of the same multiplet. **b.** Distribution of  $T_1$  values, generated using Equation 3.22, with  $p_{\min} = 0.7$  s,  $p_{\max} = 5.3$  s,  $c = 40$ ,  $R = 128$ . **c.** DOSY-style representation of the result, generated using Equation 3.21. Dashed horizontal lines denote the true  $T_1$  values for each spin. **d.** Estimation result for each increment for Run 3, illustrating the evolution of the amplitudes of each oscillator with  $\tau$ .



**Figure 3.6:** Result of estimating a Oneshot DOSY dataset of andrographolide in unfresh Deuterated DMSO (DMSO-d<sub>6</sub>). **a.** 1D spectrum. **b.** Diffusion profile obtained by summing the contour plot in **c.** along the *x*-axis. **c.** Contour plot mapping estimated oscillators to diffusion constants, with  $p_{\min} = 2 \times 10^{-10} \text{ m}^2 \text{s}^{-1}$ ,  $p_{\max} = 5 \times 10^{-10} \text{ m}^2 \text{s}^{-1}$ ,  $c = 2.5$ ,  $R = 128$ . **d.** Magnified view of the 2 ppm to 1.6 ppm spectral range, with estimated oscillator peaks plotted.



**Figure 3.7:** Result of estimating a diffusion dataset for a mixture of L-threonine, L-valine and D-(+)-glucose in  $\text{D}_2\text{O}$ . **a.** 1D spectrum, taken from the first FID of the diffusion dataset. **b.** Diffusion coefficient distribution. **c.** DOSY-style plot of chemical shifts vs diffusion constant, generated using Equation 3.22, with  $p_{\min} = 4.5 \times 10^{-10} \text{ m}^2 \text{ s}^{-1}$ ,  $p_{\max} = 7 \times 10^{-10} \text{ m}^2 \text{ s}^{-1}$ ,  $R = 256$ , and  $c = 1.5$ .

overlap with others, tended to be associated with less consistent diffusion constants and larger errors with examples of this phenomenon apparent in panel d of the figure. A few oscillators also show a significant deviation at around 2.5 ppm. This is due to the presence of a 1:2:3:2:1 quintet from partially protonated DMSO. As the data is insufficiently resolved to enable the separation of andrographolide and DMSO signals, oscillators exist which will have an amplitude profile influenced by both species, leading to an aggregated diffusion constant. As  $D_{\text{DMSO}} > D_{\text{andrographolide}}$ , the affected oscillators possess larger predicted diffusion constants.

### Glucose/valine/threonine diffusion

Another diffusion example is provided by Figure 3.7, where the estimation routine was applied to a dataset derived from a sample comprising the molecules L-valine ( $M_r = 117.148 \text{ g mol}^{-1}$ ), L-threonine ( $M_r = 119.120 \text{ g mol}^{-1}$ ), and D-(+)-glucose ( $M_r = 180.156 \text{ g mol}^{-1}$ ) dissolved in  $\text{D}_2\text{O}$  at 298 K. Not included in the figure is the result for the water signal, for which a diffusion constant of  $1.88 \times 10^{-9} \text{ m}^2 \text{ s}^{-1}$  was determined. The routine achieved decent separation of the three species in the sample. Predicted diffusion coefficients for valine and threonine were  $6.20 \times 10^{-10} \text{ m}^2 \text{ s}^{-1}$  and  $6.39 \times 10^{-10} \text{ m}^2 \text{ s}^{-1}$ , respectively. For glucose, the situation is complicated by the presence

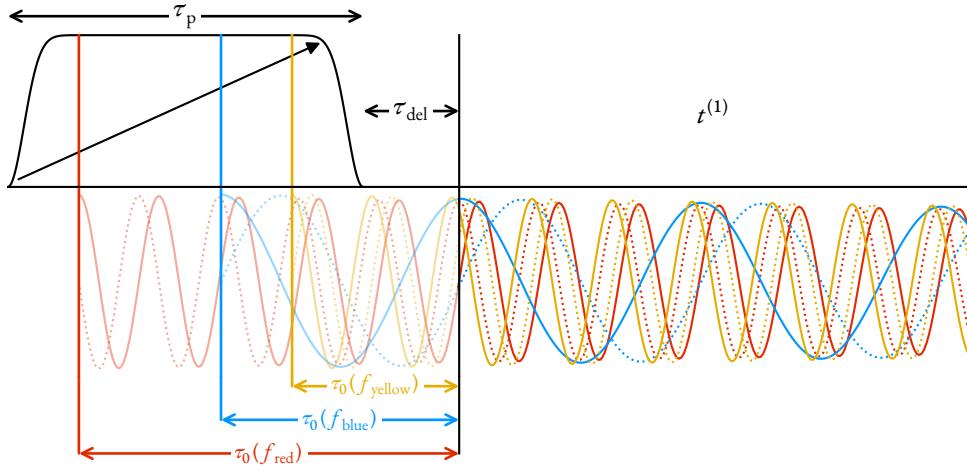
of two major anomeric forms:  $\alpha$ -D-glucopyranose and  $\beta$ -D-glucopyranose\*\*[129: Chapter 3]. There is some evidence of separation of these anomers, principally due to the downfield doublets at 5.15 ppm ( $\alpha$ ) and 4.56 ppm ( $\beta$ ), which have estimated diffusion coefficients of  $5.47 \times 10^{-10} \text{ m}^2 \text{ s}^{-1}$  and  $5.34 \times 10^{-10} \text{ m}^2 \text{ s}^{-1}$ , respectively. Beyond these however, the other estimated oscillators corresponding to glucose have associated errors which are too large for clear resolution of the two species.

As is to be expected, signals which are of greater intensity, and which are more clearly resolved enable the determination of diffusion coefficients with lower errors. A clear example of this behaviour can be recognised when considering the valine result (see the area shaded blue in panel c). The oscillators which lead to diffusion constants with the lowest errors correspond to the high intensity doublet of doublets around 0.95 ppm, resulting from six equivalent protons from two methyl groups. Far greater uncertainty is observed for the predictions associated with proton (B), which has a doublet of septets structure, featuring many low-intensity signals. Application of multivariate methods on the dataset was unsuccessful at extracting diffusion information for the separate components. Both DECRA and SCORE could extract the water signal from the rest of the dataset, with the two components having associated diffusion coefficients of  $6.31 \times 10^{-10} \text{ m}^2 \text{ s}^{-1}$  and  $1.88 \times 10^{-9} \text{ m}^2 \text{ s}^{-1}$ , respectively.

### 3.3 Ideal spectra from single-chirp excitation

The are numerous nuclei of value in NMR with very wide chemical shift ranges, including  $^{13}\text{C}$ ,  $^{19}\text{F}$  (of particular interest in the pharmaceutical industry)  $^{31}\text{P}$ , and  $^{195}\text{Pt}$ . Attaining spectra covering the entire chemical shift range of such spins for use in quantitative applications is challenging due to off-resonance effects, which severely alter the amplitudes and phases of resonances with frequencies far from the transmitter frequency[22: Section 3.4.1]. One popular means of achieving broadband excitation, in which a consistent amplitude- and phase-profile across a spectral window of tens or even hundreds of kHz is achieved, is to use frequency-swept (FS) pulses, during which the frequency of RF irradiation varies with time[130]. One of the most common classes of FS pulses are those where the variation of frequency with time is linear, with such pulses commonly referred to as *chirp* pulses. The application of a single  $90^\circ$  chirp pulse to achieve broadband excitation, while simple, yields spectra with undesirable phase behaviour, on account of resonances with different frequencies being excited at different moments in time. There are well-established methods for overcoming this using pulse sequences featuring an initial excitation, followed by one or more refocussing FS pulses[131–135].

\*\*The equilibrium mixture in water comprises 38% of the  $\alpha$  isomer and 62% of the  $\beta$  isomer. This is evidenced by the spectrum in Figure 3.7.a, where the relative integrals of the doublets at 5.15 ppm and 4.56 ppm agree with this ratio. A tiny amount of the open-chain form will also be present, though in a negligible quantity.



**Figure 3.8:** An illustration of an experiment comprising a single chirp pulse sweeping low to high frequencies of duration  $\tau_p$ , followed by a pre-scan delay period or  $\tau_{\text{del}}$ , prior to acquisition. The fate of three resonances with different frequencies is denoted, with  $f_{\text{red}} < f_{\text{blue}} < f_{\text{yellow}}$ . Each resonance is excited at different points in time, with lower frequency resonances being excited earlier, such that each resonance is allowed to evolve for different amounts of time prior to acquisition ( $\tau_0$ ). The resulting FID possesses quadratic phase behaviour. Coloured oscillations denote the evolution of each resonance, with solid and dashed lines representing real and imaginary components, respectively. It is assumed that the  $90^\circ$  chirp rotates each resonance to be initially in phase with the receiver.

With knowledge of the form of the chirp pulse, the expected phase of a particular resonance is determinable, and in this section, it will be shown that well-phased spectra can be obtained from excitation with a single FS pulse when appropriate post-processing of the FID is employed. The main advantage of being able to derive spectra with desirable features from a single chirp excitation experiment is the fact that ultra-broadband spectra can be generated using with a far shorter pulse sequence than state of the art methods such as chirped, ordered pulses for ultra-broadband spectroscopy (CHORUS)[134, 135], where both a  $90^\circ$  chirp pulse, and two  $180^\circ$  chirp pulses are applied. Spectra with improved sensitivity could therefore be realised. Here, a description of the technique is presented, followed by an illustration of its performance on a simulated and an experimental dataset. This work is fairly nascent, and while the initial results presented here show promise, there is yet to be consideration on samples of greater interest.

### 3.3.1 Chirp excitation

Focus is limited to chirp pulses which sweep from low to high frequencies. Such a pulse is parameterised by its duration  $\tau_p$  (s), excitation bandwidth  $\Delta F$  (Hz), and RF “amplitude”  $\omega_{\text{RF}}$  (Hz). The frequencies that the pulse sweeps through are in the range  $[f_{\text{off}} - 1/2\Delta F, f_{\text{off}} + 1/2\Delta F]$ , and the rate at which the frequency of the chirp is increased (the sweep rate) is given by  $\Delta F/\tau_p$ . Figure 3.8 provides an illustration of a single chirp excitation experiment. After application of the chirp pulse, there is typically a short pre-scan delay  $\tau_{\text{del}}$ , usually on the order of a few  $\mu\text{s}$ , prior to the start of

acquisition. While the pre-scan delay can be determined if an intimate knowledge of the spectrometer hardware is known, this varies from instrument to instrument, and is not trivial to ascertain. It is this delay which induces a first-order phase shift in NMR experiments, and which is routinely corrected for by phase correction. The various pulse parameters are inter-related as follows[135, 136]:

$$\omega_{\text{RF}} = \sqrt{\frac{\Delta F Q}{2\pi\tau_p}}, \quad (3.23)$$

where  $Q \in \mathbb{R}_{>0}$  is the *adiabaticity factor*. For a pulse with flip angle  $\beta < 180^\circ$ ,  $Q$  is related to  $\beta$  via

$$Q = \frac{2}{\pi} \ln \left( \frac{2}{\cos(\beta) + 1} \right), \quad (3.24)$$

such that an appropriate pulse to achieve a flip angle of  $90^\circ$  requires selecting a combination of  $\omega_{\text{RF}}$ ,  $\Delta F$ , and  $\tau_p$  which satisfies  $Q \approx 0.441$ . The combination used in examples in this work are  $\Delta F = 400 \text{ kHz}$ ,  $\tau_p = 100 \mu\text{s}$ , and  $\omega_{\text{RF}} \approx 16.8 \text{ kHz}$ . For a pulse with sufficiently low  $\omega_{\text{RF}}$  — this requires a sufficiently large pulse duration for a given excitation bandwidth — it is reasonable to assume that the chirp pulse induces an instantaneous  $90^\circ$  rotation at the point of resonance, as illustrated in Figure 3.8. As such, resonances with different Larmor frequencies evolve for different amounts of time prior to the start of acquisition, according to

$$\tau_0(f) = \tau_{\text{del}} + \frac{\tau_p}{2} - \frac{(f - f_{\text{off}})\tau_p}{2\Delta F}. \quad (3.25)$$

$\tau_{\text{del}} + \tau_p/2$  is the amount of time between excitation and detection for the on-resonance case, in which excitation occurs exactly halfway through the pulse. Resonances with a frequency smaller than that of the transmitter are excited earlier and hence have a larger  $\tau_0$ , while the converse is true for resonances with greater frequencies. The resulting overall phase as a function of frequency can be approximated as[135]

$$\phi(f) = \phi_0 + 2\pi \left( \tau_{\text{del}} + \frac{\tau_p}{2} \right) (f - f_{\text{off}}) - 2\pi \left( \frac{\tau_p}{2\Delta F} \right) (f - f_{\text{off}})^2. \quad (3.26)$$

One might assume that it is possible to generate phased spectra by simply applying phase correction to the spectrum, via

$$s_\phi(f) = s(f) \exp(-i\phi(f)). \quad (3.27)$$

While the quadratic phase behaviour of peaks is corrected by doing this, another issue with the dataset is not addressed. For any resonance, the signal that is detected can be thought of as the difference between two signals: (a) the “complete” signal, which starts at the time of excitation, and (b) a “truncated” signal which is identical to the complete signal before acquisition, and which

comprises zeros once acquisition has begun. The linear nature of the FT dictates that the resulting delayed-acquisition spectrum comprises the difference between the FTs of the complete signal and the truncated signal. The FT of a severely truncated FID is well approximated as a broad sinc function with its maximum at the resonance frequency. The appearance of the sinc “wiggle” depends on the gap between excitation and acquisition. Resonances of lower frequencies will exhibit deeper, narrower artefacts since the signal is more significantly truncated. The result of applying quadratic phase correction is therefore a spectrum of well-phased peaks, but with major baseline distortions, particularly to the low-frequency end. Panel b in Figures 3.9 and 3.10 both provide examples of this phenomenon.

### 3.3.2 Methodology

Both the quadratic phase behaviour and delay-induced baseline distortions can be resolved if an estimate of the FID’s parameters is obtained. This enables the construction synthetic FID featuring oscillators which are back-propagated, such that they begin not at the point of acquisition, but at the point of excitation. The appropriate start time for an oscillator with frequency  $f$  is given by  $-\tau_0$ , with  $\tau_0$  defined in Equation 3.25. The resulting corrected FID  $y \in \mathbb{C}^N$  is defined as

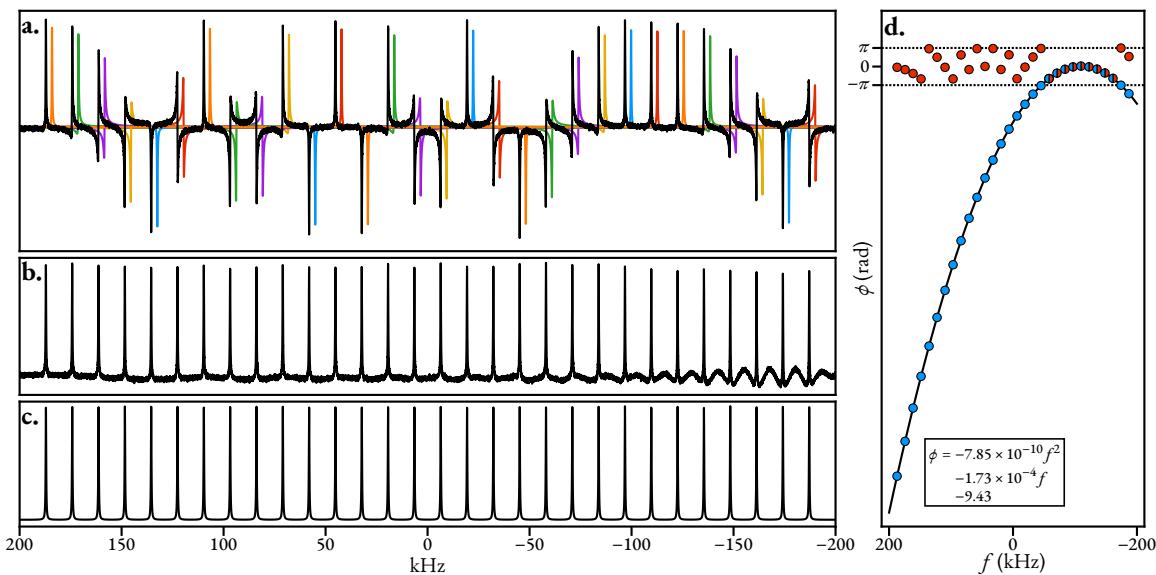
$$y_n = \sum_{m=1}^M a_m \exp(i\phi_m) \exp((2\pi i(f_m - f_{\text{off}}) - \eta_m)(n\Delta_t - \tau_0(f_m))), \quad (3.28)$$

$\forall n \in \{0, \dots, N-1\}$ . This concept has similarities to the use of LP in order to back-propagate an FID to correct for corrupted initial points. However, a holistic approach such as LP is not of use in this application, as each signal component must be treated differently according to its frequency.

Thus far in this work, it has been assumed that all signals which make up a dataset are of the same phase. Of course this isn’t the case for FIDs generated from single-chirp excitation. As such, it is inappropriate to incorporate the variance of oscillator phases in fidelity for NLP. For the examples presented in this section, NLP was not applied at all; the direct output of the MPM was used as the estimate of the FIDs parameters.

### 3.3.3 Results

Figures 3.9 and 3.10 present comparisons between the application of quadratic phase correction and the proposed back-propagation procedure. In the former, a simulated dataset is considered, comprising 30 evenly-spaced signals, and generated using Equation 3.28 with  $-\tau_0(f_m)$  replaced with  $+\tau_0(f_m)$ . Other relevant parameters used are stated in the caption. A very large damping factor ( $1000 \text{ s}^{-1}$ ) was assigned to each oscillator, as this augments the baseline distortions in the spectrum. AWGN was added to the FID, with a target SNR of 25 dB.



**Figure 3.9:** Comparison of quadratic phase correction vs frequency-dependent back-propagation in treating simulated single-chirp excitation data. **a.** Simulated spectrum for a spin system comprising 30 spins with uniformly-separated resonance frequencies. The data was generated with  $N = 2^{14}$ ,  $f_{\text{sw}} = 400$  kHz,  $f_{\text{off}} = 0$  Hz,  $\tau_p = 100$   $\mu$ s,  $\tau_{\text{del}} = 0$  s,  $\Delta F = 400$  kHz. Coloured lines depict individual signals generated using the MPM; these have been slightly offset for clarity. **b.** Spectrum generated using quadratic phase correction, with Equation 3.27. **c.** Spectrum generated from estimation using the MPM, and back-propagation. **d.** Estimated phases of each oscillator as a function of frequency. Red points: phases wrapped within the range  $(-\pi, \pi]$ . Blue points: the same phases, adjusted by addition of a suitable multiple of  $2\pi$  to each red point in order to display the quadratic dependence of the phases. Black curve: quadratic fit of the blue points.

The spectrum after quadratic phase correction, in panel b, exhibits the undesired baseline distortions as discussed, with more intense, narrower baseline distortions associated with lower-frequency signals. The MPM was used to estimate the FID's parameters, with only the first 2048 points considered<sup>††</sup>. The spectrum generated via back-propagation is presented in panel c of Figure 3.9, where a well-phased spectrum without baseline distortion was generated. The variation of the estimated oscillator phases against their frequencies is plotted in panel d, with the quadratic dependence clearly illustrated. Fitting the blue points in panel d to a quadratic function yielded a second-order coefficient of  $-7.85 \times 10^{-10} \text{ rad s}^2$ , in agreement with the expected value of  $-2\pi (\tau_p/2\Delta F)$ .

Figure 3.10 features an experimental dataset, acquired from a sample of 1% Gd-doped H<sub>2</sub>O in D<sub>2</sub>O<sup>‡‡</sup>. The dataset was acquired using a 2D experiment, in which the transmitter offset was adjusted for each increment. The result was a series of FIDs, each comprising a single H<sub>2</sub>O signal with differing frequencies. When summed, these lead to an FID with multiple signals at defined frequencies. The resulting spectrum is presented in panel a of Figure 3.10.

To produce the phased spectrum in panel b, only the second-order phase correction was automatically corrected. This was followed by manual first-order phase correction. This was done because, as stated above, the length of the spectrometer delay  $\tau_{\text{del}}$  is not trivial to determine. As with the simulated case, severe baseline wobbles exist in the spectrum making the spectrum unsuitable for quantitative applications.

Analogously, to generate the spectrum via back-propagation, only the contribution to  $\tau_0$  which is dependent on the signal frequency was included, i.e.  $\tau_0$  in Equation 3.28 was replaced with

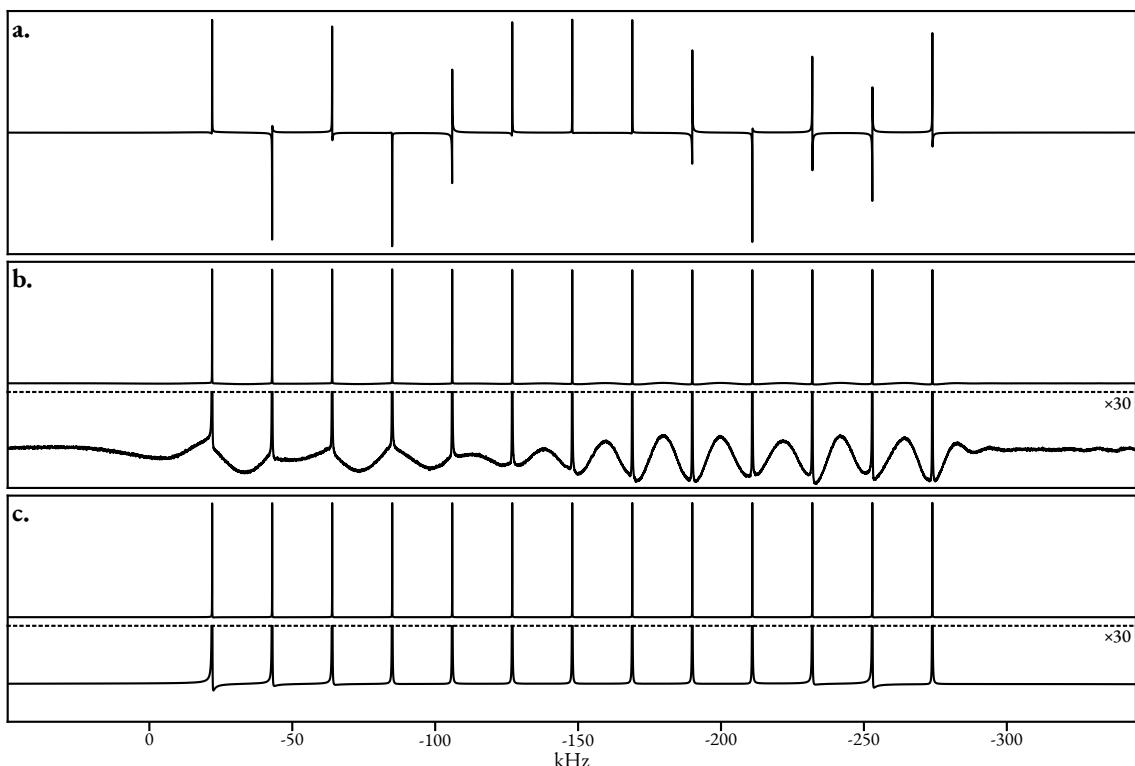
$$\tau'_0 = -\frac{(f - f_{\text{off}})\tau_p}{2\Delta F}. \quad (3.29)$$

First-order phase correction was applied to the spectrum produced from the back-propagated FID to yield the result presented in panel c. In comparison with the quadratic phase-correction approach, it is evident that a far cleaner spectral baseline is achieved. There is not a perfectly consistent phase across all signals; most notably, the highest and second-lowest signals have phases which stray noticeably from 0°. It is likely that this resulted from error associated with the MPM.

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<sup>††</sup>Performing the MPM on a signal with  $2^{14}$  points would take (a) a long time, and (b) require a very large amount of RAM (see panels a1 & a2 in Figure 2.4). Estimating a truncated FID comprising the first 2048 points of the data is justifiable here, since all signal frequencies are spaced reasonably far apart, meaning each signal in the FID becomes resolvable from the others early on into evolution.

<sup>‡‡</sup>The paramagnetic species Gd<sup>III</sup> is a popular example of a contrast agent used in magnetic resonance imaging (MRI), owing to its ability to decrease the  $T_1$  of nearby spins. This typically has an influence on  $T_2$  too, with it being shortened at high enough concentrations. The signal from H<sub>2</sub>O therefore decays at a more rapid rate, such that the baseline distortions observed in the phased spectrum (panel b of Figure 3.10) are more pronounced.



**Figure 3.10:** Comparison of quadratic phase correction vs frequency-dependent back-propagation in treating experimental single-chirp excitation data generated from a sample of 1% Gd-doped H<sub>2</sub>O in D<sub>2</sub>O. **a.** Spectrum generated directly from the acquired FID. **b.** Spectrum generated using quadratic phase correction. **c.** Spectrum generated from estimation using the MPM, followed by frequency-dependent back-propagation.

## 3.4 Summary

In this chapter, numerous results have been presented, all of which feature 1D FID estimation either as the sole focus (Section 3.1) or as a key step in a specific application (Section 3.2 & Section 3.3).

In Section 3.1, it was illustrated that by extending the MPM through the incorporation of the added step of NLP with a phase variance constraint can aid in the generation of parameter estimates which agree with the underlying assumptions of the data structure. Oscillators in the MPM often possess spurious phases; this feature can frequently be rectified though the NLP method.

While there are scenarios where 1D estimation performs admirably, and can enhance the information accessible to a spectroscopist, ironically 1D data is probably the most challenging type of NMR data to estimate from a complexity perspective; with all information about a sample being distilled into a single dimension, it is very common (particularly with  $^1\text{H}$  datasets) for the data to be so densely populated with signals that extracting meaningful information from it at the per-signal level is futile. It should therefore be appreciated that there is a limited scope where estimation methods which rely minimally on user-provided information can find use. Through the separation of signals into more than one detection dimension, multidimensional experiments can yield datasets which have sufficiently well-resolved signals for estimation to be applicable. The 2DJ experiment is such an example, and estimation of datasets acquired from it is the focus of the next chapter.



# 2DJ Estimation for Pure Shift NMR

4

Two key features of the NMR experiment for which improvements are constantly being sought are sensitivity and resolving power. There are numerous means of enhancing sensitivity, such as the use of magnets with higher field strengths[137] (sensitivity  $\propto B_0^{3/2}$ ) and cryogenic probes[26], as well as simply increasing the number of scans (sensitivity  $\propto NS^{1/2}$ ). However, few means of achieving better resolution exist beyond increased field strengths (resolution  $\propto B_0$ ). Significant interest has therefore been given to the development of techniques which generate broadband homodecoupled (*pure shift*) spectra, in which the effects of homonuclear scalar couplings are absent from the data. While often valuable for structural assignment purposes, the influence of scalar couplings can lead to spectra which are too crowded for meaningful insights to be gleamed. While it is commonplace to decouple heteronuclear couplings at the point of FID acquisition[138–140], homonuclear decoupling is far more challenging. At the time of writing, there are a number of well-established pure shift experiments, which involve running a 2D pulse sequence, and concatenating the initial sections of each FID, in a process referred to as “chunking”[141–143]. The key drawback of all of these techniques is that the resultant pure shift signal is considerably less sensitive relative to a standard pulse-acquire experiment, since only a fraction of the available spin magnetisation contributes to that which is detectable by the probe.

In this chapter, a method for deriving pure shift spectra indirectly via the estimation of 2DJ datasets is presented, named *computer-assisted undiminished-sensitivity protocol for ideal decoupling* (CUPID). It is illustrated that by extracting the parameters which describe a 2DJ dataset, a pure shift spectrum with desirable absorption-mode lineshapes can be produced without the signal loss associated with all experimental pure shift methods.

## 4.1 Pure Shift NMR

In this section, a survey of some of the most prominent procedures for producing pure shift spectra are presented.

### 4.1.1 The 2DJ Experiment

The 2DJ experiment[37, 38] provided the first means to achieve broadband homodecoupling. It has the following simple pulse sequence:

$$90^\circ \rightarrow t^{(1)}/2 \rightarrow 180^\circ \rightarrow t^{(1)}/2 \rightarrow t^{(2)}.$$

After excitation of magnetisation onto the transverse plane, the indirect-dimension evolution consists of a spin echo, with acquisition following immediately afterwards. The result in an FID in which only scalar couplings evolve in  $t^{(1)}$ , as the chemical shifts are refocussed by the spin echo, while both chemical shifts and scalar couplings evolve during  $t^{(2)}$ . An FID generated by the 2DJ experiment is hypercomplex, taking the form of Equation 1.22 with  $D = 2$  and  $\zeta^{(1)} = \exp(i\cdot)$ , i.e.

$$\begin{aligned} \gamma_{n^{(1)}, n^{(2)}} = & \sum_{m=1}^M a_m \exp(i\phi_m) \exp\left(\left(2\pi i f_m^{(1)} - \eta_m^{(1)}\right) n^{(1)} \Delta_t^{(1)}\right) \times \\ & \exp\left(\left(2\pi i \left(f_m^{(2)} - f_{\text{off}}\right) - \eta_m^{(2)}\right) n^{(2)} \Delta_t^{(2)}\right) + w_{n^{(1)}, n^{(2)}}. \end{aligned} \quad (4.1)$$

The transmitter offset term has been neglected in the indirect dimension, since chemical shift evolution does not occur. For each signal in the FID, the indirect- and direct-dimension frequencies are intimately linked. Consider a 2DJ dataset generated from a spin system with  $S$  distinct spins. The signals giving rise to a particular spin  $s \in \{1, \dots, S\}$  form a grouping  $G_s \subset \{1, \dots, M\}$ , where  $M$  is the total number of signals that make up the FID. All of the signals in  $G_s$  will have (angular) frequencies given by

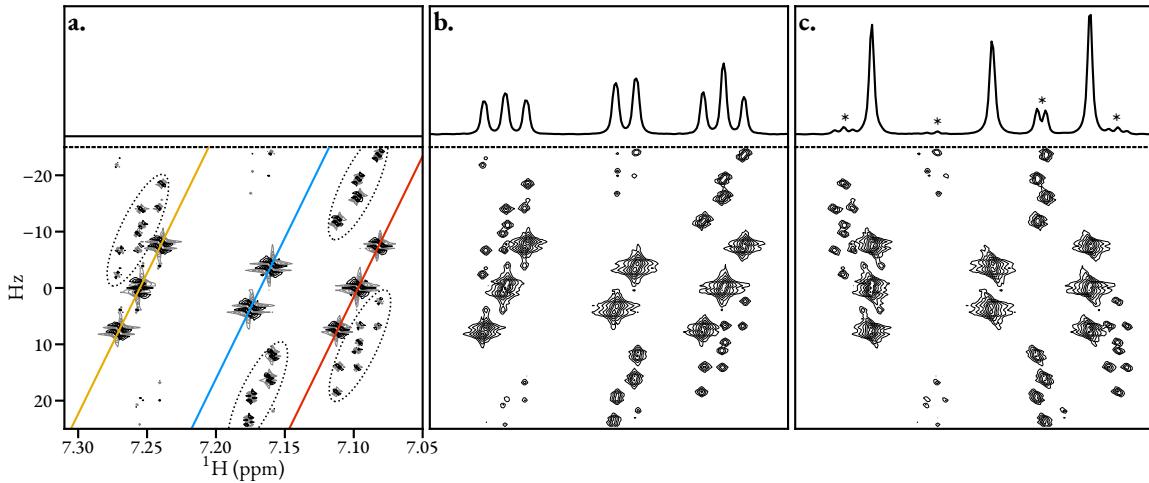
$$2\pi f_m^{(1)} = \Delta\omega_m, \quad (4.2a)$$

$$2\pi f_m^{(2)} = \omega_{0,s} + \Delta\omega_m, \quad (4.2b)$$

$\forall m \in G_s$ , where  $\omega_{0,s}$  is the Larmor frequency of the spin, and  $\Delta\omega_m$  is the displacement of the signal from  $\omega_{0,s}$ , as a result of J-couplings\*. Due to this relationship, all peaks in the Fourier domain which are part of the same multiplet will lie along a line which bisects the  $F^{(1)}$  and  $F^{(2)}$  axes, as depicted in panel a of Figure 4.1.

One limitation of the 2DJ experiment is the fact that peaks comprising pure absorption Lorentzian

\* $\Delta\omega_m$  will be a linear combination of all the J-couplings associated with the spin, with all the coefficients being  $\pm 1/2$ .



**Figure 4.1:** Region of a simulated 2DJ spectrum of strychnine. Each panel depicts the spectrum following different processing procedures. Below: contour plots of the spectrum. Black contours have positive values; grey contours have negative values. Above: the projection of the spectrum onto the indirect ( $F^{(1)}$ ) axis. **a.** Spectrum produced by applying sine-bell apodisation followed by FT in both dimensions. Coloured lines denote  $45^\circ$  cross-sections along which first-order multiplet structures lie. Prominent strong coupling artefacts have been annotated with dotted ellipses. **b.** Magnitude-mode spectrum. **c.** Spectrum generated after application of a  $45^\circ$  shear on the magnitude-mode spectrum. Peaks marked with an asterisk originate from strong coupling artefacts in the 2DJ spectrum.

character cannot be produced. This is since, due to the absence of a mixing period, it is not possible to acquire a complementary pair of phase-modulated FIDs; such a pair could be processed in so as to nullify the dispersive contributions (see Section 1.2.2). The FT of a 2DJ FID produces a spectrum with phase-twist peaks; an example is provided in panel a of Figure 4.1. As with other experiments which produce hypercomplex signals, such as COSY, the data is conventionally displayed in *magnitude-mode* (panel b) in which the absolute value of each complex point in the spectrum is plotted.

### The shear and projection approach

A pure shift spectrum can be acquired from a 2DJ spectrum by performing a  $45^\circ$  shear on the spectrum array; each direct-dimension vector in the spectrum is subjected to a right circular rotation according to

$$\varsigma_{n^{(1)}, n^{(2)}}^{\text{shear}} = \varsigma_{n^{(1)}, n^{(2)'}} \quad (4.3a)$$

$$n^{(2)'} = \left( n^{(2)} + \left\lfloor \frac{f_{\text{sw}}^{(1)} N^{(2)}}{f_{\text{sw}}^{(2)} N^{(1)}} \left( \frac{N^{(1)}}{2} - n^{(1)} \right) \right\rfloor \right) \bmod N^{(2)}. \quad (4.3b)$$

In the limit of continuous sampling, this achieves the relationship

$$s^{\text{shear}}(F^{(1)}, F^{(2)}) \equiv s(F^{(1)}, F^{(2)} - F^{(1)}).$$

By performing a  $45^\circ$  shear, chemical shifts and scalar couplings are separated onto orthogonal axes, such that the peaks of the sheared spectrum which arise from a given spin all reside at the same value of  $F^{(2)}$  (panel c). The effectiveness of the shear is maximised when both  $f_{\text{sw}}^{(2)}/f_{\text{sw}}^{(1)}$  and  $N^{(2)}/N^{(1)}$  are integers. After shearing, projecting the spectrum onto  $F^{(1)}$  (i.e. summing along the indirect-dimension) leads to the 1D pure shift spectrum. If the spectrum wasn't converted to magnitude-mode prior to shearing and projecting, the absorptive and dispersive components of the spectrum would cancel each other out, such that a vector devoid of any signal would be obtained (panel a). With a magnitude-mode spectrum, the process leads to undesirable pure shift spectra with broad “wings” on account of the presence of dispersive character, and non-linearities. These effects can be suppressed by appropriate processing to make the FID envelope symmetric in both dimensions; sine-bell apodisation and pseudo-echo reshaping[144] are common methods. However, these both cause a significant reduction in sensitivity being incurred, along with distortions in relative peak amplitudes such that the data is rendered unsuitable for quantitative applications. Examples of experimental pure shift spectra produced via sine-bell apodisation can be found in panel a in both Figure 4.7 and Figure 4.8, where severe discrepancies in peak integrals are present.

When present, another feature which limits the effectiveness of the 2DJ experiment are *strong coupling artefacts*<sup>†</sup>, which arise due to mixing effects induced by the  $180^\circ$  pulse[145, 146]. These artefacts always have direct-dimension frequencies which match those of the conventional, *first order*<sup>‡</sup> signals, though they do not lie along the same  $45^\circ$  cross sections as these. As a result, the final spectrum produced by shearing and projecting onto  $F^{(1)}$  will feature additional low-intensity “nuisance” signals that compound the task of interpreting the spectrum (see peaks marked with asterisks in Figures 4.1.c, 4.7.a, and 4.8.a).

### Pure shift spectra from 2DJ estimation

Beyond the shearing and projection method, procedures based on the estimation of 2DJ datasets have also been developed to achieve broadband homodecoupling. Nuzillard introduced a linear predictive estimation of signal time reversal (ALPESTRE)[147, 148], in which the parameters of each indirect-dimension FID are estimated using LPSVD, such that a set of parameters  $\Theta \in$

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<sup>†</sup>As stressed in [145], these are not strictly artefacts, but rather genuine signals, which are expected to be present in the 2DJ dataset. Despite this, the term is widespread in the literature, most likely as the term emphasises that the signals hinder analysis of the data.

<sup>‡</sup>First order signals are those which arise under the assumption of the weak coupling regime[22: Section 2.5.2].

$\mathbb{R}^{N^{(2)} \times 4M}$  is generated:

$$\boldsymbol{\theta}_{n^{(2)}} = \begin{bmatrix} \boldsymbol{\alpha}_{n^{(2)}}^T & \boldsymbol{\phi}_{n^{(2)}}^T & \boldsymbol{f}_{n^{(2)}}^T & \boldsymbol{\eta}_{n^{(2)}}^T \end{bmatrix}^T. \quad (4.4)$$

The parameters generated are used to propagate each FID backward into  $-t^{(1)}$ , producing a “full-echo”:

$$\gamma_{n^{(1)}, n^{(2)}}^{\text{full}} = \sum_{m=1}^M \alpha_{n^{(2)}, m} \exp(i\phi_{n^{(2)}, m}) \exp\left(\left(2\pi i f_{n^{(2)}, m} n^{(1)} - \eta_{n^{(2)}, m} |n^{(1)}|\right) \Delta_t^{(1)}\right), \quad (4.5)$$

$$\forall n^{(1)} \in \{-N^{(1)} + 1, \dots, 0, \dots, N^{(1)} - 1\}, \forall n^{(2)} \{0, \dots, N^{(2)} - 1\}.$$

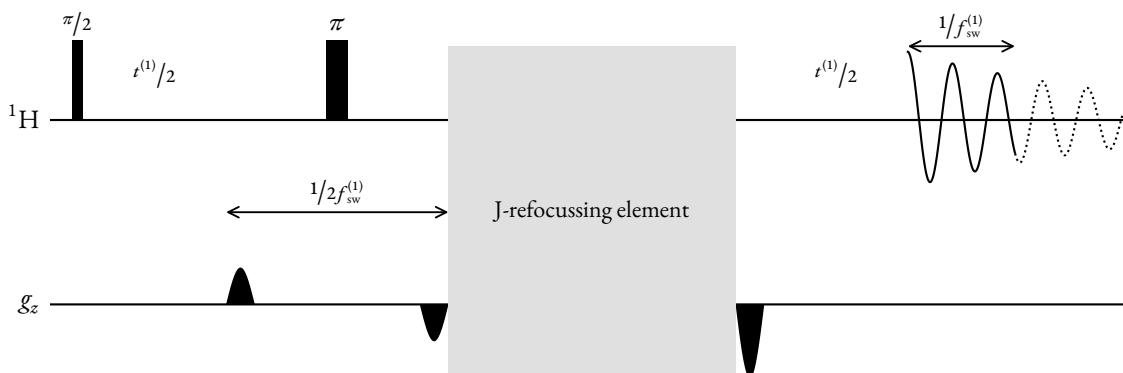
FT of Equation 4.5 generates a spectrum whose real component comprises absorption-mode Lorentzian character in both dimensions. This opens up the means of producing pure-shift spectra from the 2DJ experiment with sharp lineshapes and without signal loss. A similar approach proposed by Mutzenhardt et al. instead constructs full echoes via LP of each direct-dimension FID, and generates a full echo by propagating into  $-t^{(2)}$  [149]. Further to these LP based methods, Mandelshtam and co-workers has also illustrated how the filter diagonalisation method (FDM) can be applied for parametric estimation, followed by pure shift spectrum construction [150, 151].

### 4.1.2 Chunking methods

A popular set of experimental techniques for pure shift NMR comprise 2D pulse sequences in which a short initial section (chunk) of the FID at each increment is retained [142]. The acquired chunks are subsequently concatenated to yield a 1D pure shift signal. All of the sequences are designed such that they refocus the effects J-couplings at a specific time point, with this time being incremented to acquire different chunks of the pure shift FID. It is impossible to refocus the couplings associated with all spins in a sample simultaneously. Instead, the chunking methods operate by ensuring that J-refocussing is achieved for a subset of the spins (the *active spins*) while the rest (the *passive spins*) are manipulated to ensure J-refocussing occurs, but do not contribute to the final FID.

A generalised pulse sequence for the chunking approach is depicted in Figure 4.2. In the middle of the sequence is a  $180^\circ$  hard pulse, which inverts all spins. Following this is an element which is designed to invert the active spins again, while leaving the passive spin coherences unaffected. As such, the active spins experience no net effect (they undergo a  $360^\circ$  rotation) while the passive spins experience a net inversion. This results in the J-couplings associated with the active spins being refocussed at the point that acquisition starts<sup>§</sup>. Rather than acquiring a plurality of points,

<sup>§</sup>In practice, the pulse sequence is usually set up to ensure that the exact point of J-refocussing occurs in the middle of each acquired chunk, rather than at the start of the chunk. This enables double the amount of points to be acquired per increment without noticeable influence from J-couplings.



**Figure 4.2:** The general form of a pulse sequence used for pure shift NMR via the chunking approach. Appropriate examples of J-refocussing elements include BIRD, the Zanger-Sterk element, and the PSYCHE element. The initial chunk of the FID (solid line) is retained and concatenated with other acquired chunks, while the rest (dotted line) is discarded.

one might envisage that only a single point should be acquired at each increment to ensure that the effects of J-couplings are completely negated from the concatenated signal. However, since the rate of J-coupling evolution is slow (on the order of Hz), it is far more efficient to acquire a chunk of points at each iteration for little loss of data quality.

The primary drawback of the chunking approach is that regardless of the J-refocussing element used, a significant reduction in sensitivity is incurred, since only a subset of the magnetisation present in the sample contributes to the detected signal. However, since they are able to produce clean spectra with absorption lineshapes, these methods have largely superseded the original 2DJ processing approach. A summary of some of the most prominent J-refocussing elements is now provided.

### Zanger-Sterk (ZS)

The ZS element employs the concept of “slice-selective excitation” to distinguish between active and passive spins[152, 153]. It consists of the simultaneous application of a low RF power 180° pulse — conventionally, a r-SNOB pulse is used[154] — and a PFG along the laboratory  $z$ -axis. The PFG induces a change in a given spin’s Larmor frequency as a function of its position in the sample. For a low-power RF pulse to excite the spin, its frequency must be at or very close to the Larmor frequency. For spins with different resonance frequencies, the sample region where excitation occurs differs since their Larmor frequencies must be perturbed by different extents for resonance. The net effect of the ZS element is to excite a particular spin in only a narrow range of heights in the sample; the spins which are excited belong to the pool of active spins, while the remainder are the passive spins. In order to achieve effective decoupling of a pair of spins, it is required that the bandwidth of the selective 180°-pulse is smaller than the difference in their

Larmor frequencies. However, with more selective pulses, a smaller proportion of the spins will be in the active subset, and hence the FID's sensitivity will be diminished<sup>1</sup>. Therefore a trade-off exists between effective decoupling of all spins, and achieving the greatest sensitivity possible. When strong coupling is present, the ZS method tends to perform poorly relative to other options for this reason. It is possible to incorporate ZS element into the 2DJ pulse sequence, enabling the generation of 2DJ datasets comprising phase-modulated pairs[155]. With this approach, pure shift spectra with far more desirable lineshapes can be generated via the 45° shear approach relative to using the magnitude-mode spectrum.

### Bilinear rotation decoupling (BIRD)

The BIRD element acts to invert spins bound to a low-abundance heteronucleus, while the remaining spins bound to a high-abundance inert nucleus are unaffected[156, 157]. The two most common heteronuclei exploited when using BIRD are <sup>13</sup>C (1.1% abundance) and <sup>15</sup>N (0.37% abundance). The loss of sensitivity is therefore known and constant across samples. In scenarios where strong coupling exists, BIRD can achieve improved sensitivity over ZS, due to the requirement for a highly selective 180° in the ZS element as discussed above. The BIRD method is particularly attractive in scenarios where the sensitivity penalty due to the involvement of a low-abundance nucleus has already been paid, for example in sequences where an insensitive nuclei enhancement by polarization transfer (INEPT) element is present[158]. One of BIRD's primary drawbacks is the fact that geminal protons cannot be decoupled from each other, since such protons are always in the same active/passive subset. Doublets rather than singlets will arise in such cases.

### Pure shift yielded by chirp excitation (PSYCHE)

The most recent major development in pure shift spectroscopy is the PSYCHE experiment[159, 160]. **Description... Element, How it works (very simple), Effectiveness**

With PSYCHE, the proportion of active and passive spins is dependent on the flip angle of the chirp pulses; for a PSYCHE element featuring chirp pulses with flip angles  $\beta$ , the proportions of are  $\cos^2 \beta$  and  $\sin^2 \beta$ , respectively.

The PSYCHE element has also been employed in conjunction with the 2DJ experiment in order to produce spectra which already feature orthogonal separation of the chemical shifts and couplings along the two frequency axes[161, 162]. Being a 3D experiment, the PSYCHE-2DJ requires long experiment times (typically tens of hours) in order to produce a spectrum with well-resolved multiplet structures in the indirect dimension.

<sup>1</sup>The sensitivity reduction suffered using the ZS element is  $\propto \Delta F / \gamma g l_z$ , where  $\Delta F$  is the selective pulse bandwidth,  $g$  is the strength of the PFG, and  $l_z$  is the length of the sample lying within the receiver coil ( $\approx 1.5$  cm).

## 4.2 Methodology

The method developed as part of this work, CUPID, fits into the category of techniques which aim to generate pure shift spectra by utilising the result of parametric estimation applied to 2DJ data. In this section, a description of the method is given.

### 4.2.1 The estimation routine

Recall that it is assumed that a 2DJ FID take the function form given by Equation 4.1. The primary steps involved in estimating a 2DJ dataset, for each spectral region of interest, are:

1. Generation of frequency-filtered sub-FID corresponding to the region of interest (Section 4.2.3).
2. Prediction of the sub-FID's model order, either by applying the MDL on the first increment in the direct dimension<sup>||</sup>(Section 2.2.3) or by manually specifying a value.
3. Generation of an initial parameter estimate using the MMEMPM (Section 2.2.2).
4. Subjection of the initial parameter estimate to phase variance constrained NLP (Section 2.3).

Instead of estimating successive 1D FIDs, as proposed by Nuzillard and Mutzenhardt et al., 2DJ sub-FIDs are estimated holistically. By doing this, a number of benefits are realised. First, multiplet structures which heavily overlap in a conventional 1D dataset become separated in the 2DJ dataset, assuming that the Larmor frequencies of the relevant spins are sufficiently different. Accurate resolution of the FID's constituent signals in more crowded spectral regions is far more likely to be successful with a full 2D estimation as a result. On top of this, there is an additional resolution advantage relative to the estimation of *direct* dimension FIDs. Due to the presence of a spin echo during  $t^{(1)}$ , signal damping effects caused by field inhomogeneities are nullified, such that damping is dictated solely by transverse relaxation ( $T_2$ ). During  $t^{(2)}$  however, the influence of field inhomogeneities are not corrected, such that damping occurs at a faster rate, characterised by  $T_2^*$ . As such, multiplet structures in the indirect dimension exhibit better resolution (assuming  $f_{\text{sw}}^{(1)}/N^{(1)}$  and  $f_{\text{sw}}^{(2)}/N^{(2)}$  are comparable).

A further benefit comes with having access to the frequencies of each signal in *both* dimensions, since this opens up the opportunity to group together those which belong to the same multiplet, as will be discussed in Section 4.2.4. Similar information can be obtained by extracting slices of a tilted magnitude-mode 2DJ spectrum at appropriate values of  $F^{(2)}$ , though the lineshapes of peaks suffer from the undesirable characteristics described above. The ZS-2DJ[155] and PSYCHE-2DJ[161, 162] experiments are also able to generate individual multiplet structures, though with

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<sup>||</sup>The first increment of a 2DJ experiment, for which  $t^{(1)} = 0$  s, effectively takes the same form as an FID derived from a pulse-acquire experiment.

long three-dimensional (3D) pulse sequences, and with reduced sensitivity relative to a conventional 2DJ experiment.

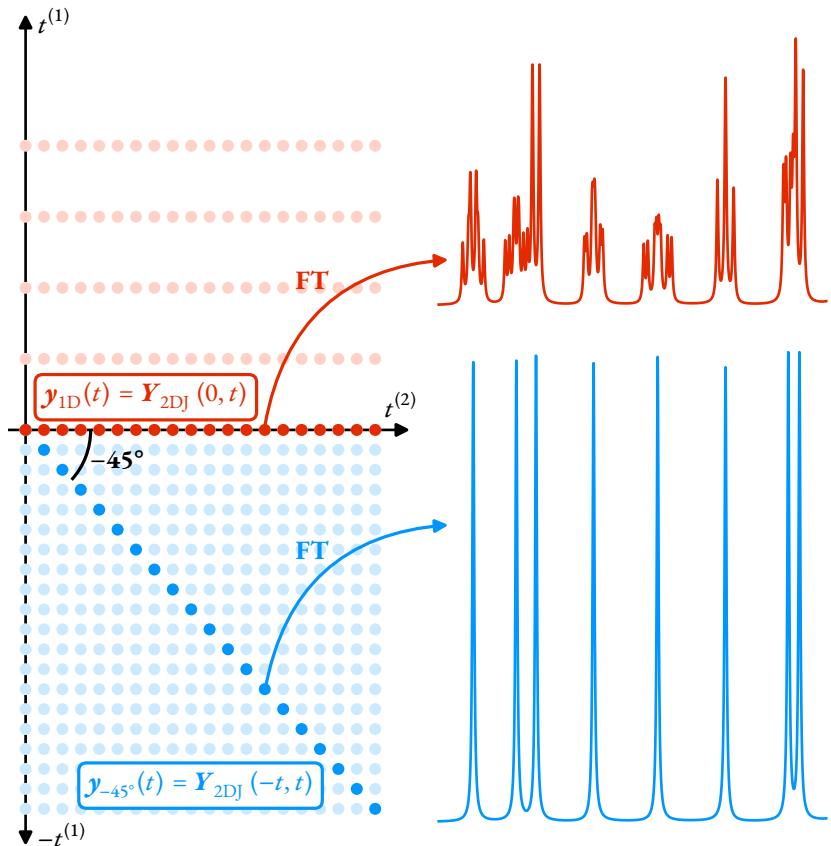
As was mentioned in Section 2.2.3, application of the MDL to a 2D FID is not desirable, since a full SVD would need to be computed on the typically very large block-Hankel matrix  $E_Y$ . Assuming that the spectral region being considered is not too crowded, applying the MDL on the first direct-dimension FID can return reasonable estimates of  $M$  at a far smaller computational cost. For particularly crowded regions, resorting to a manual specification of model order by inspecting the 2DJ spectrum is the best solution currently available. An interesting benefit is sometimes realised when the 1D MDL is applied. As described above, the presence of strong coupling artefacts results in additional nuisance peaks featuring in spectra produced by shearing and projection. Exactly the same phenomenon would occur when parametric estimation is employed, assuming that the strong coupling artefacts signals are quantified. However, since the artefacts have direct-dimension frequencies which are identical to those of first-order signals in the dataset, it is virtually impossible to resolve these using the 1D MDL approach. Therefore, the MDL is often found to generate a model order which agrees with the number of first-order signals, rather than the *true* number of signals in the FID. As the MMEMPM generates a parameter estimate based on the first  $M$  significant components of the dataset, the more intense first-order signals are quantified, whereas the weaker strong coupling artefacts are not included. It should be noted concept is not infallible; it has simply been observed on a number of occasions. There are instances where strong coupling artefacts are incorporated into the estimation result, either because the prediction of  $M$  was excessive, or certain artefacts possess particularly large amplitudes.

#### 4.2.2 The $-45^\circ$ signal

The 2DJ estimation routine yields the parameter vector  $\theta \in \mathbb{R}^{6M}$ . With knowledge of the frequencies and damping factors in both dimensions, it is possible to generate an FID which will produce a pure shift spectrum directly, rather proceeding via the full-echo approach of Nuzillard and Mutzenhardt et al. The desired synthetic FID produced is named the  $-45^\circ$  signal  $y_{-45^\circ} \in \mathbb{C}^{N^{(2)}}$ :

$$y_{-45^\circ, n^{(2)}} = \sum_{m=1}^M a_m \exp(i\phi_m) \exp\left(\left(2\pi i \left(f_m^{(2)} - f_m^{(1)} - f_{\text{off}}\right) - \eta_m^{(2)}\right) n^{(2)} \Delta_t^{(2)}\right), \quad (4.6)$$

with the reasoning behind the name provided by Figure 4.3. The  $-45^\circ$  signal takes the form of a conventional 1D FID, except that the frequency of each oscillator, which would be  $f_m^{(2)}$  in a pulse-acquire experiment, is replaced with  $f_m^{(2)} - f_m^{(1)}$ . Oscillators belonging to the same multiplet  $s$  will all provide a contribution to the FID with the frequency  $\omega_{0,s}$ . Assuming that the parameters associated with the 2DJ FID are accurately determined, a pure shift spectrum with sharp absorption-mode lineshapes and no loss of signal can be generated by constructing the  $-45^\circ$



**Figure 4.3:** An illustration of the reasoning behind the name “ $-45^\circ$  signal”, which is used to generate pure shift spectra as part of the CUPID method. The pale red dots denote a typical 2DJ FID, where the amount and rate of sampling in the direct dimension is greater than in the indirect dimension (i.e.  $N^{(1)} \ll N^{(2)}$  and  $f_{\text{sw}}^{(1)} \ll f_{\text{sw}}^{(2)}$ ). The bright red dots correspond to the first direct-dimension signal  $y(0, t^{(2)})$ , which has the same form as an FID from a pulse-acquire experiment. A hypothetical signal generated by propagating the FID into  $-t^{(1)}$ , with the same rate of sampling in both dimensions, is denoted with pale blue dots. Taking the diagonal of this signal, such that it forms a  $-45^\circ$  angle with the  $t^{(2)}$  axis, yields an FID  $y_{-45^\circ}$  which is homodecoupled. Note that there is a slight discrepancy between Equation 4.6 and this description, in that the indirect-dimension damping factors  $\gamma^{(1)}$  are neglected in the former case.

signal.

### 4.2.3 Filtration of 2DJ data

Unlike the direct-dimension, which can often comprise sparsely distributed peaks in the Fourier domain, the indirect dimension of 2DJ datasets tends to be densely populated since all multiplet structures are centered at 0 Hz, and rarely span beyond  $\pm 50$  Hz. As such, the generation of frequency-filtered sub-FIDs is limited to consideration of the direct dimension. The filtering procedure applied to 2DJ data is an extension of that for 1D data described in Section 2.5, and is depicted in Figure 4.4:

1. The array  $\mathbf{Y}_{\text{ve}} \in \mathbb{C}^{N^{(1)} \times 2N^{(2)}}$ , is constructed, which comprises the virtual echo of each direct-dimension FID. Each row of the array  $\mathbf{y}_{\text{ve},n^{(1)}} \forall n^{(1)} \in \{0, \dots, N^{(1)} - 1\}$  is given by

$$\mathbf{y}_{\text{ve},n^{(1)}} = \begin{bmatrix} \Re(\gamma_{n^{(1)},0}) & \gamma_{n^{(1)},1} & \cdots & \gamma_{n^{(1)},N^{(2)}-1} & 0 & \gamma_{n^{(1)},N^{(2)}-1}^* & \cdots & \gamma_{n^{(1)},1}^* \end{bmatrix}. \quad (4.7)$$

2.  $\mathbf{Y}_{\text{ve}}$  is subjected to FT along the direct dimension to produce the spectrum  $\mathbf{S}_{\text{ve}}$  (Figure 4.4.a). This has an imaginary component of zero.
3. A super-Gaussian  $\mathbf{G} \in \mathbb{R}^{N^{(1)} \times 2N^{(2)}}$  is constructed (Figure 4.4.b):

$$\mathbf{G} = \mathbf{1} \otimes \mathbf{g}^{(2)}, \quad (4.8)$$

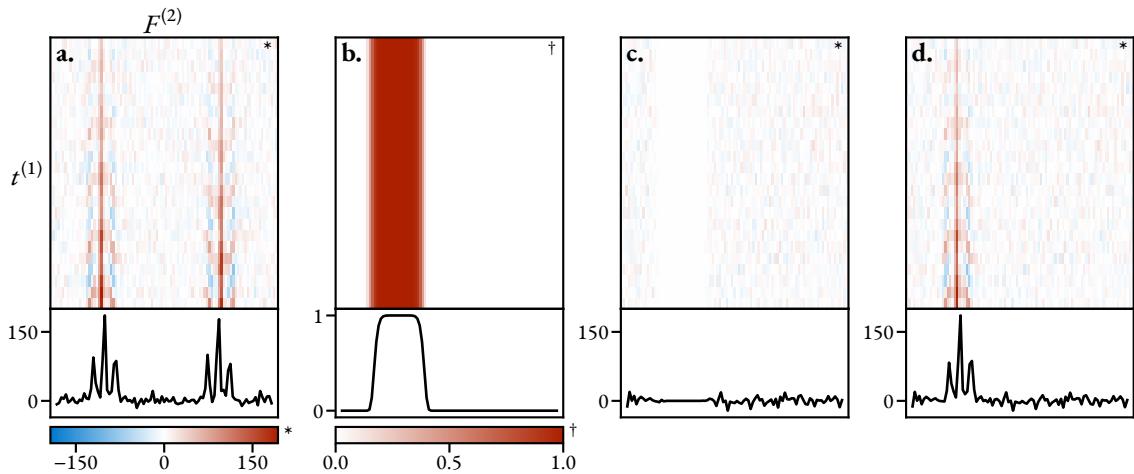
where  $\mathbf{1} \in \mathbb{R}^{N^{(1)}}$  is a vector of ones, and  $\mathbf{g}^{(2)} \in \mathbb{R}^{2N^{(2)}}$  is a super-Gaussian vector given by Equation 2.60.

4. A matrix of additive noise is generated by extracting the variance  $\sigma^2$  of a direct-dimension strip of  $\mathbf{S}_{\text{ve}}$  which is devoid of peaks, and generating an array  $\mathbf{W}_{\sigma^2} \in \mathbb{R}^{N^{(1)} \times 2N^{(2)}}$  with values independently sampled from  $\mathcal{N}(0, \sigma^2)$  (Figure 4.4.c).
5. The spectrum is filtered (Figure 4.4.d):

$$\tilde{\mathbf{S}}_{\text{ve}} = \mathbf{S}_{\text{ve}} \odot \mathbf{G} + \mathbf{W}_{\sigma^2} \odot (\mathbf{1} - \mathbf{G}). \quad (4.9)$$

6.  $\tilde{\mathbf{S}}_{\text{ve}}$  is subjected to IFT and is sliced in half in the direct dimension, yeilding the final filtered signal  $\tilde{\mathbf{Y}}$ .

As with the 1D case before, this method can also be extended to incorporate spectral slicing, acting to reduce the number of points present in the filtered sub-FID.



**Figure 4.4:** An illustration of the filtering procedure for 2DJ data. For each panel is a heat-map of the full 2D signal, as well as a plot underneath of the first slice of the signal in the direct dimension. **a.** The spectrum  $S_{ve}$ , **b.** Super-Gaussian filter  $G$ , **c.** Additive noise, attenuated by the super-Gaussian,  $W_{\sigma^2} \odot (1 - G)$ , **d.** Filtered spectrum  $\tilde{S}_{ve}$ . Panels **a.–d.** are analogous to panels **b.–e.** in Figure 2.6 for the 1D case.

#### 4.2.4 Multiplet Prediction

CUPID's ability to group oscillators present in a parameter set into multiplet structures relies on simultaneously knowing both the indirect- and direct-dimension frequencies of each model oscillator. As has already been established, for oscillators which are associated with the same multiplet grouping  $G_s$ , the quantities  $f_{m_1}^{(2)} - f_{m_1}^{(1)}$  and  $f_{m_2}^{(2)} - f_{m_2}^{(1)}$  should be equal ( $\omega_{0,s}$ ) for any pairing  $m_1, m_2 \in G_s$ . An assessment of whether two oscillators belong to the same multiplet can therefore be made using the following criterion:

$$\left| \left( f_{m_1}^{(2)} - f_{m_1}^{(1)} \right) - \left( f_{m_2}^{(2)} - f_{m_2}^{(1)} \right) \right| < \epsilon. \quad (4.10)$$

$\epsilon \in \mathbb{R}_{>0}$  is a threshold to account for uncertainty in the estimation result. A lower bound on  $\epsilon$  is the separation between adjacent points in the better-resolved dimension of the spectrum, i.e.  $\min(f_{sw}^{(1)}/N^{(1)}, f_{sw}^{(2)}/N^{(2)})$ . However, limitations in resolution due to relaxation-induces signal damping and field inhomogeneities can require  $\epsilon$  to be increased beyond this for effective assignments to be achieved. Listing Code Listing C.8 provides a **PYTHON** routine that can be used for multiplet prediction.

There are certain circumstances where it is safe to assume that a particular oscillator in the estimation result is not associated with a first-order signal in the dataset. No oscillator describing a first-order signal will abide by both of the following:

1. The oscillator is not grouped with any other oscillator as part of the multiplet assignment.
2. The magnitude of the indirect dimension frequency of the oscillator is appreciably greater

than 0 Hz.

If the signal is the only member of a multiplet grouping, it must be a singlet, and as such it will have an indirect-dimension frequency of 0 Hz. Oscillators which do agree with the two points above can be assumed to be related to either strong coupling artefacts or noise, and can be automatically discarded.

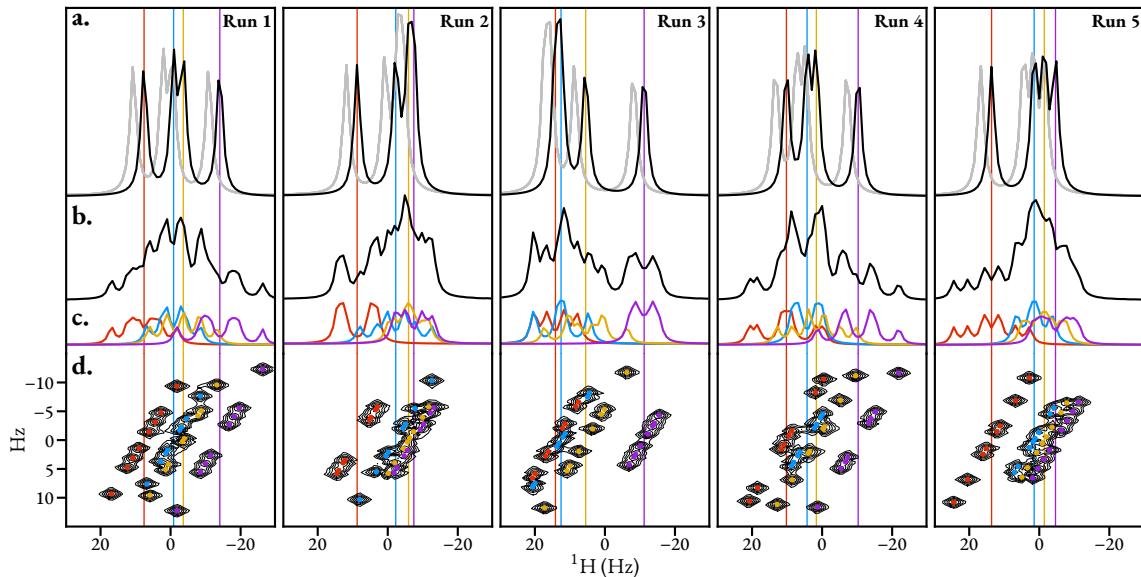
## 4.3 Results

A number of examples of the application of CUPID are now presented. For details relating to generation of the 2DJ datasets, see Appendices D.1 and D.2.4. Useful metrics, such as run times and the number of oscillators present at different stages of the routine are provided in Table D.7.

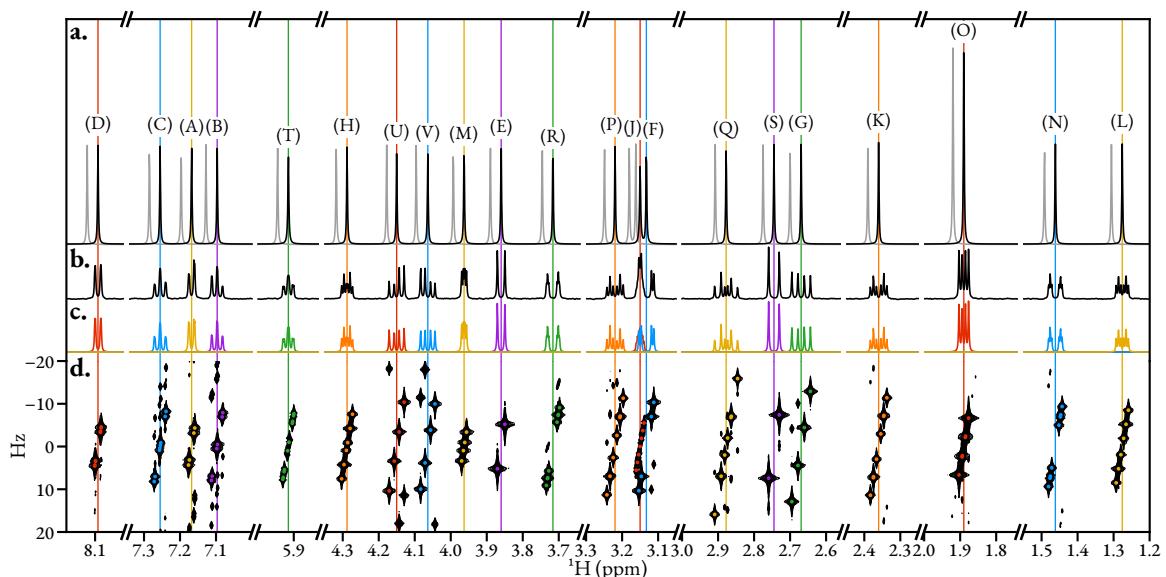
### 4.3.1 Four Multiplets

A series of five simulated 2DJ datasets were generated using SPINACH such that within a known region of the spectrum four ddd multiplet structures with significant overlap were present. AWGN was added to each FID, with a target SNR of 30 dB. Filtering was applied to the datasets to generate sub-FIDs containing the signals in the region of interest (−30 Hz to 30 Hz). Figure 4.5 provides an illustration of CUPID’s performance when applied to the datasets. Each of the sub-FIDs comprised 32 ( $4 \times 2^3$ ) signals. As can be seen in Figure 4.5.b, the first direct-dimension slices of these FIDs are too crowded for reasonable estimates of model order to be made using the MDL, so a value was manually provided; for each run, a random integer from the range [33, 40] was selected as the initial number of oscillators. Hence, the initial guess from the MMEMPM comprised a slightly excessive number of oscillators in each case. For each FID generated, CUPID was able to produce a result with 32 oscillators, as desired, despite the excessive number that were present in the initial guess. Most of the excessive oscillators were purged during the NLP procedure by acquiring negative amplitudes. For 2 of the 5 datasets, the result after NLP comprised 33 oscillators, with a single oscillator being associated with noise remaining in the parameter set. These could be automatically detected and removed using the first-order signal detection criteria described in Section 4.2.4.

With simulated examples such as this, it is possible to confirm that the pure shift spectrum generated using CUPID agrees with the expected result; the “true” pure shift spectrum can be obtained by simulating a pulse-acquire experiment, using a spin system with same chemical shifts, but with all J-couplings set to 0 Hz. As seen in Figure 4.5.a. the spectra produced using CUPID agree well with these. Beyond pure shift spectrum generation, the multiplet assignment was also successful, assigning all the ddd multiplet structures present; these are plotted in Figure 4.5.c.



**Figure 4.5:** The result of applying CUPID to 5 instances of simulated 2DJ datasets with 4 heavily overlapping multiplet structures. **a.** Black: pure shift spectrum generated by CUPID (via the  $-45^\circ$  signal). Grey: 1D spectrum simulated with Spinach, using the same spin system as was used to produce the 2DJ dataset, but with all scalar couplings set to 0 Hz. This has been offset slightly for clarity. **b.** 1D spectrum of the dataset, produced using the first direct-dimension FID in the 2DJ dataset. **c.** Multiplet structures predicted, using a threshold  $\epsilon = f_{\text{sw}}^{(2)}/N^{(2)} \approx 0.98$  Hz. **d.** Contour plot of the magnitude-mode 2DJ spectrum. Coloured points denote the frequencies of oscillators in the estimation result. Coloured vertical lines denote the predicted central frequencies of each multiplet structure, determined using multiplet assignment routine.



**Figure 4.6:** Application of CUPID on a simulated strychnine 2DJ dataset. See Figure 4.5 for a description of the panels. The multiplet structures were assigned using the threshold  $\epsilon = f_{\text{sw}}^{(2)}/N^{(2)} \approx 0.39$  Hz.

### 4.3.2 Strychnine simulated

As a second example of applying CUPID on simulated data, the chemical shifts and isotropic scalar couplings associated with strychnine were used to construct a 2DJ dataset. AWGN was included with a target SNR of 20 dB. The CUPID procedure was applied to filtered sub-FIDs such that the signals arising from all spins were considered, with the result presented in Figure 4.6. There are numerous regions in the dataset where strong coupling artefacts reside, and as such this dataset provides a good gauge on the effectiveness of CUPID when these are present.

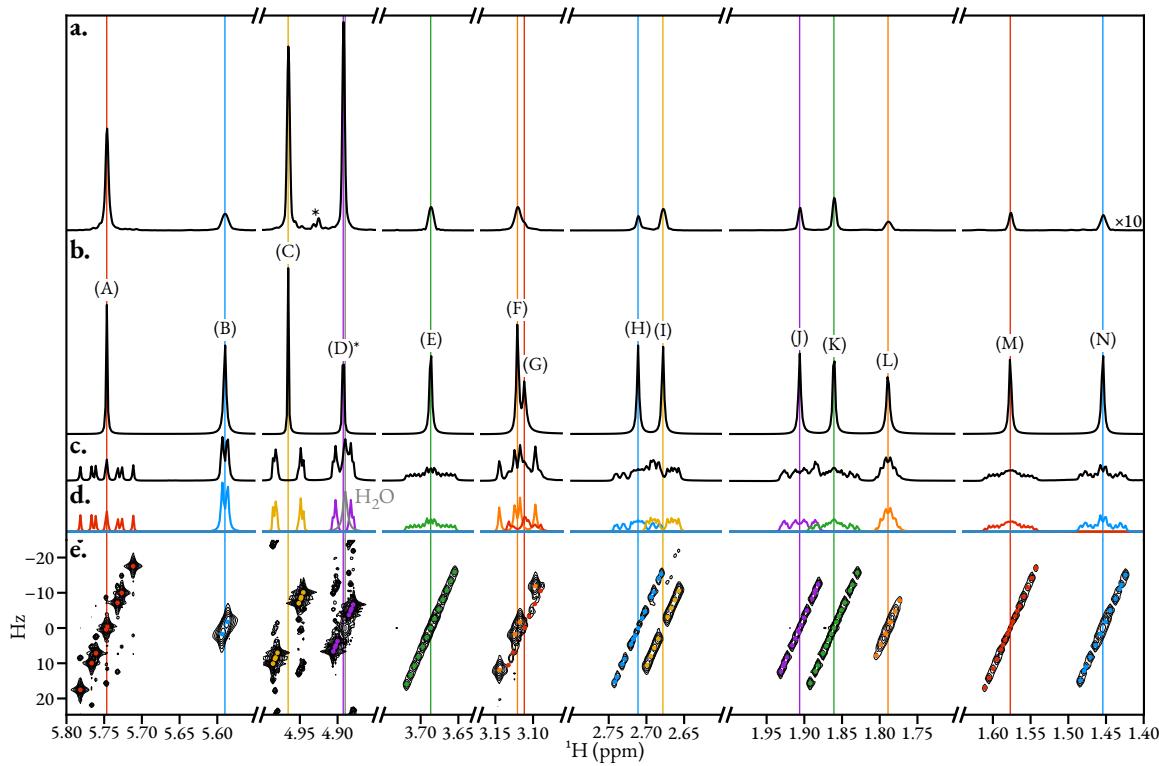
The MDL was applied to the first direct-dimension FID in order to predict model order. In most circumstances, the model order used resulted in estimation results in which the first-order signals were well quantified, while those corresponding to strong coupling artefacts were neglected. In some circumstances, certain strong couplings signals were quantified, though the relevant oscillators were purged on every occasion based on the first-order criteria. As such, no such artefacts appear in the final pure shift spectrum. The absence of strong coupling artefacts in the estimation result also leads to generated multiplet structures which do not exhibit the typical “roofing” effect associated with strongly coupled spins (*cf.* Figures 4.6.b and 4.6.c). The clearest examples of this are associated with the pair (U) and (V), as well as the trio (A), (B) and (C). As with the four multiplets example, good agreement is achieved between the pure shift spectrum generated via the  $-45^\circ$  signal, and a spectrum generated by running a 1D simulation with the same spin system, expect that scalar couplings are set to 0 Hz.

### 4.3.3 Quinine

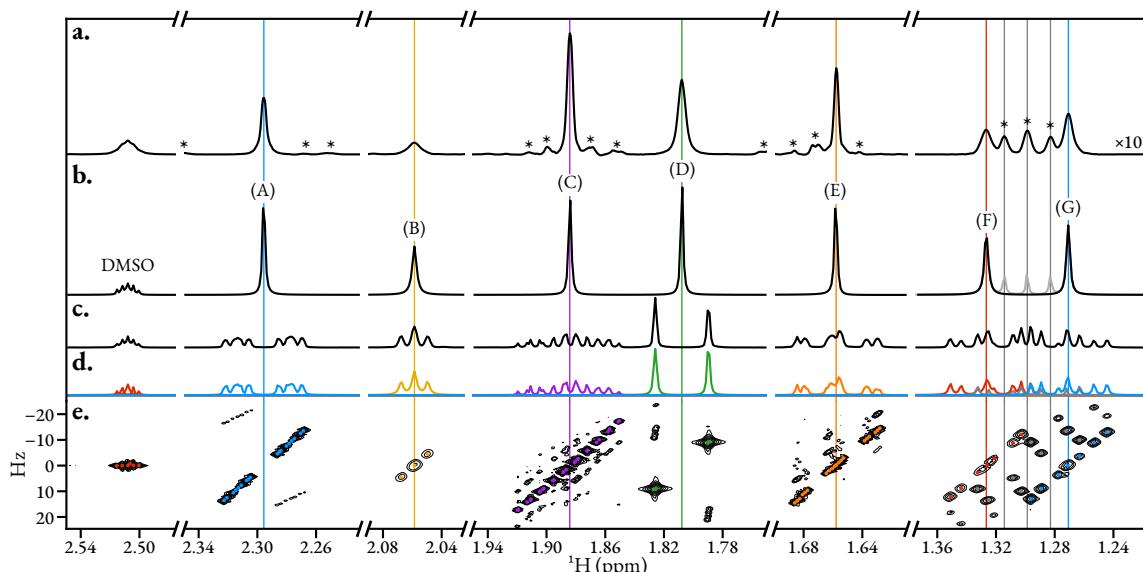
Figure 4.7 illustrates the result of applying CUPID on a dataset generated from a sample comprising quinine (Figure D.1.a) in  $\text{CD}_3\text{OD}$ , with all signals arising from non-aromatic protons considered. For comparison with CUPID, Figure 4.7.a presents a spectrum produced using the shear and projection approach. Because sine-bell apodisation was applied to the FID to suppress dispersive contributions, the relative amplitudes of the pure-shift peaks are drastically different. In particular, the signals from the alkenyl spins (A), (C) and (D) are attenuated less by apodisation relative to the aliphatic signals due to their longer  $T_2$  times\*\*. As well as this, signals arising from strong coupling between (C) and (D) are visible (these are denoted with an asterisk).

CUPID successfully generated a pure shift spectrum with distinct peaks for each  $^1\text{H}$  environment, which possess sharper lines and more consistent integrals relative to the shear and project spectrum (Figure 4.7.b). Furthermore, the strong coupling artefacts between (C) and (D) were not incor-

\*\*Spins with longer  $T_2$ s produce signals which decay less rapidly. Sine-bell apodisation heavily diminishes the intensities of the initial points in the FID. Therefore, if the signal decays less rapidly, the relative extent by which the power of the signal is diminished is less compared with a signal derived from a spin with a small  $T_2$ .



**Figure 4.7:** Application of CUPID on the non-aromatic regions of a quinine 2DJ dataset. **a.** Spectrum produced using the  $45^\circ$  shear and projection approach. The peaks denoted by an asterisk originate from strong coupling artefacts. **b.** The spectrum generated from FT of the  $-45^\circ$  signal, with the signal arising from  $H_2O$  (grey, close to 4.9 ppm neglected). **c.** Spectrum of the first direct-dimension signal in the 2DJ FID. **d.** Multiplet structures assigned ( $\epsilon = f_{sw}^{(2)}/N^{(2)} \approx 0.92$  Hz). **e.** Contour plot of the absolute value mode 2DJ spectrum, with the locations of assigned oscillators given as coloured points.



**Figure 4.8:** Application of CUPID on a camphor 2DJ dataset. See Figure 4.7 for a description of the panels. The multiplet structures were assigned using the threshold  $\epsilon = 2f_{sw}^{(2)}/N^{(2)} \approx 1.23$  Hz.

porated into the estimation result, and as such a clean baseline between between (C) and (D) was achieved. The multiplet grouping procedure was also able to resolve the signals corresponding to spin (D) (purple) from the singlet corresponding to residual water in the sample (grey). To obtain a clean signal for spin (D), without heavy overlap with the water signal, the oscillator corresponding to the water was simply neglected from the parameter set used to generate the  $-45^\circ$  signal. This concept of neglecting nuisance signals through post-processing has similarities with SVD-based approaches for solvent suppression[163]. These methods operate by assuming that the most significant component(s) in the data are derived from the solvent; these are subtracted from the dataset to remove their influence. The process of removing the water signal the quinine data has slight differences, since in that it was suppressed manually through inspection of the CUPID result. A knowledgeable user would be able to locate the water signal and neglect it. However, in scenarios where little is known about the sample, or the user does not have a high level of expertise, manually neglecting signals in this manner may not be possible.

This example provides a few examples where a noticeable under-fitting of certain multiplet structures has occurred. The most notable case comes from the spin (G) multiplet, where close proximity with spin (F)'s multiplet has likely compounded the task of accurately estimating the associated signals. With fewer oscillators than the true number of signals at its disposal, the NLP routine has compensated by giving said oscillators large amplitudes and damping factors, so that they can reasonably fit multiple similar-frequency signals. In these situations, pure shift peaks generated via the  $-45^\circ$  signal will possess augmented linewidths. This behaviour is also exhibited to a lesser extent by the multiplet for spin (B), which comprises two pairs of very close signals in a dd structure. A single oscillator is fit to each of the doublets, culminating in a slightly broadened pure shift peak.

#### 4.3.4 Camphor

The application of CUPID to the non-methyl signals of a 2DJ dataset of camphor (Figure D.1.c) in DMSO-d<sub>6</sub> is presented in Figure 4.8. As with the quinine example, a spectrum generated through shearing and projection is presented for comparison. In most regions of the dataset, the estimation technique successfully parametrised the first-order signals, while neglecting strong coupling artefacts. However, it was not possible to solely estimate the first-order signals associated with the pair of spins (F) and (G). The extent of strong coupling between the nuclei is such that some of the strong coupling artefacts have comparable amplitudes to the first-order signals. Reliance on the MMEMPM —which determines the most significant components in the data —therefore makes it challenging to solely estimate the first-order signals in this case. The strong coupling signals which were estimated by the routine are denoted in grey in the 1.36 ppm to 1.24 ppm region of the spectrum. Their contributions to the spectrum of the  $-45^\circ$  signal are also plotted in grey. As with the shear and summation spectrum, three extra peaks reside between the pure shift peaks

associated with (F) and (G), which ideally would not exist. In much the same way that the parameters associated with water in the quinine example were neglected in constructing the  $-45^\circ$  signal, those associated with strong coupling artefacts can be too. In neglecting said parameters, the black spectrum in panel b results. Again, achieving this requires manual intervention, such that the user requires knowledge about the sample to distinguish between first-order signals and strong coupling artefacts.

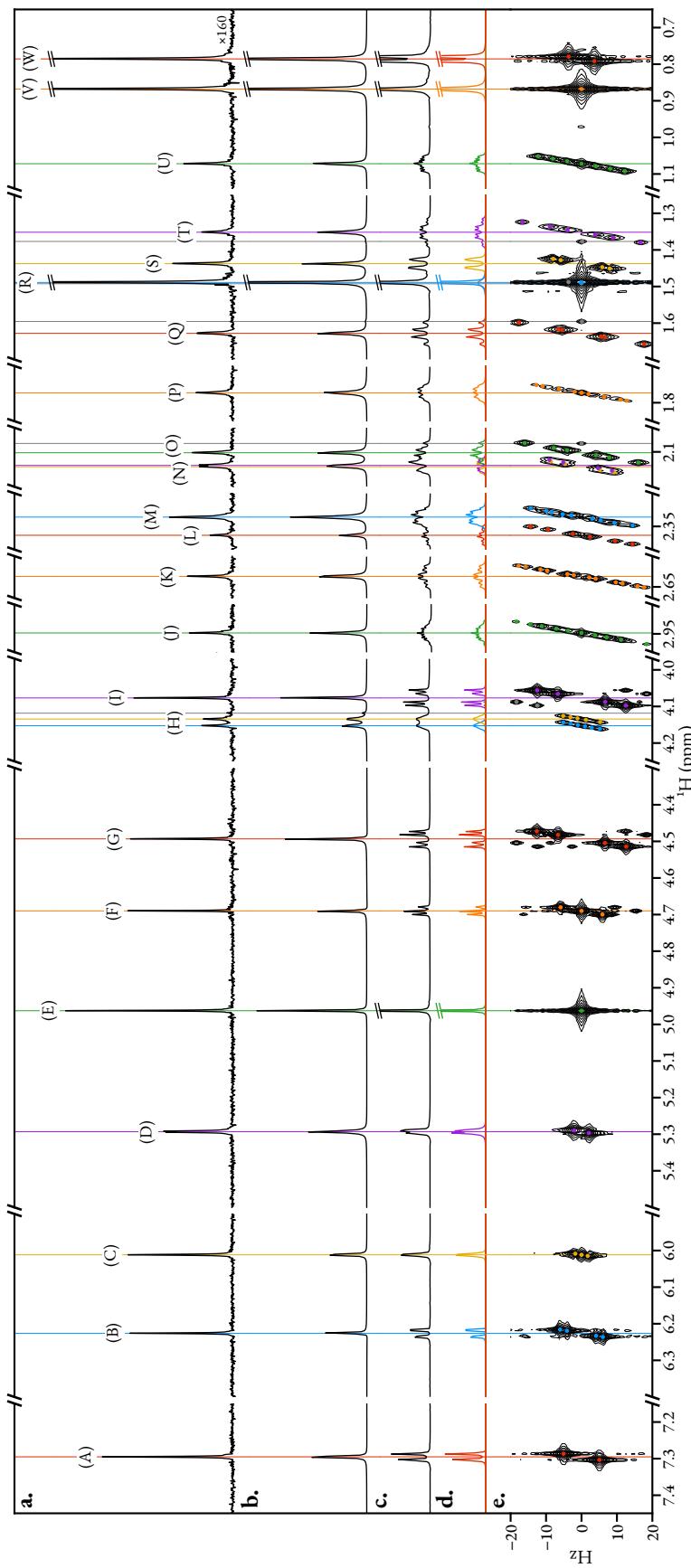
#### 4.3.5 Dexamethasone

Figure 4.9 shows the result of applying CUPID on a dataset acquired from a sample dexamethasone in DMSO-d<sub>6</sub>. A pure shift spectrum was also acquired using the triple spin echo PSYCHE (TSE-PSYCHE) experiment[160, 161] for comparison (see Figure D.5 for a description of the pulse sequence). Overall, excellent agreement is achieved between the PSYCHE spectrum, and that generated using the  $-45^\circ$  signal. The estimation routine performed amicably even in cases where heteronuclear coupling to <sup>19</sup>F exists. For spins (H) and (N), two distinct multiplet structures were assigned, which are coloured blue and yellow (H), and yellow and purple (N) in the figure. The very small though perceptible heteronuclear coupling between <sup>19</sup>F and (D) could not be resolved by the estimation routine however.

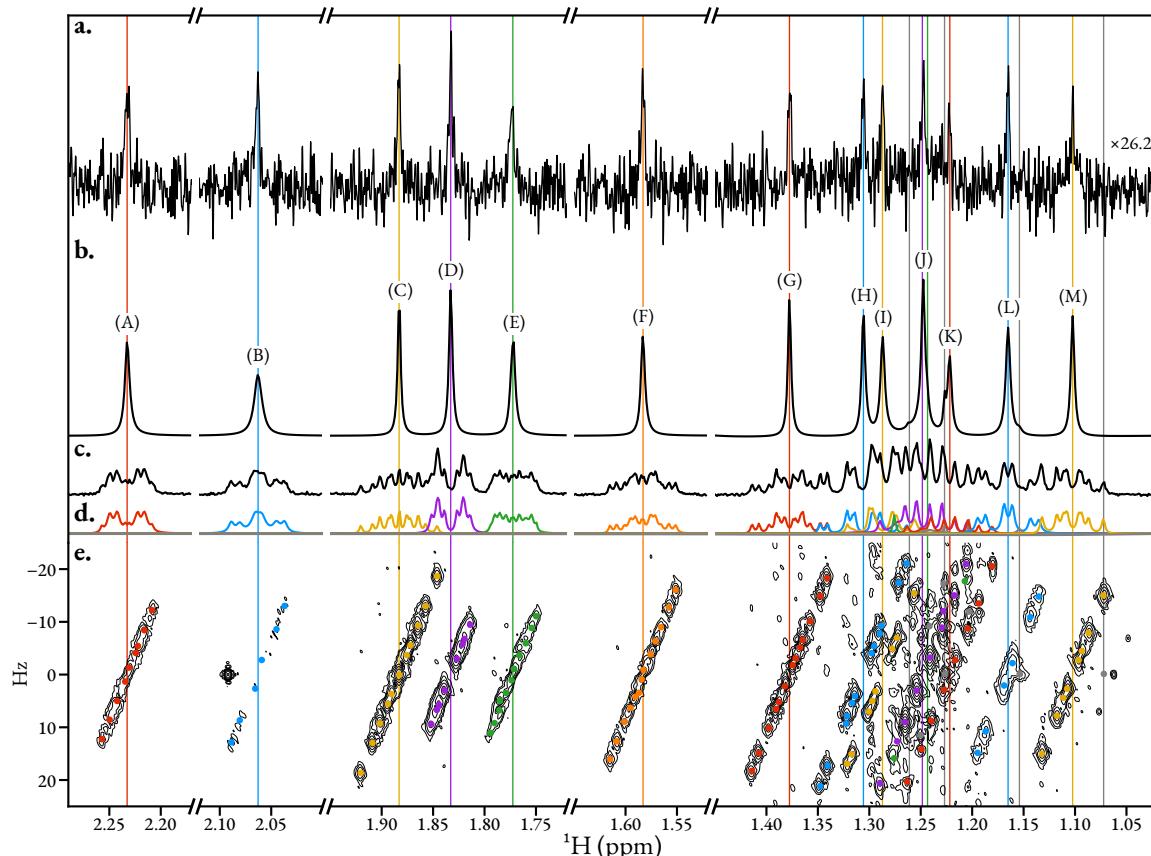
In this example, there are a few cases where oscillators which result from parametrising strong coupling artefacts exist. These persist because either they have an indirect frequency  $\approx 0$  Hz (these exist close to 1.4 ppm, 1.6 ppm, and 2.1 ppm), or because at least two parameterised artefacts are grouped together as part of the multiplet assignment (this occurs close to 4.1 ppm). As with the camphor example, a knowledgeable user could identify and neglect the culprit oscillators if desired, though they are not purged in producing the  $-45^\circ$  signal in this case to illustrate their effect on the final pure shift spectrum.

#### 4.3.6 Estradiol

A final illustration of CUPID's performance is provided by Figure 4.10, where a low concentration (2 mM) sample of 17 $\beta$ -estradiol (Figure D.1.d) in DMSO-d<sub>6</sub> is considered. This is most challenging example presented due to (a) the low SNR of the data and (b) the presence of incredibly complex regions for a small molecule spectrum, featuring many complex overlapping multiplet structures. In fact, because of the considerable complexity estradiol's spectra, it was used as a showcase for the PSYCHE experiment in the original work describing it[159]. With the sample and concentration used, the PSYCHE experiment produced a spectrum with very poor SNR, such that it is barely sensitive enough for pure shift peaks to be distinguished from the noise. However due to the innately higher sensitivity associated with the 2DJ experiment it was still possible to generate



**Figure 4.9:** Application of CUPID on a 2DJ dataset of dexamethasone in DMSO-d<sub>6</sub>. **a.** TSE-PSYCHE. **b.** The spectrum generated from FT of the  $-45^\circ$  signal. **c.** Conventional 1D spectrum. **d.** Multiplet structures assigned ( $\epsilon = f_{\text{sw}}^{(2)}/N^{(2)} \approx 0.92 \text{ Hz}$ ). **e.** Magnitude-mode 2DJ spectrum, with the locations of assigned oscillators given as coloured points.



**Figure 4.10:** Application of CUPID on a 2DJ dataset of  $17\beta$ -estradiol in  $\text{DMSO-d}_6$ . **a.** PSYCHE spectrum. The spectrum has been scaled such that its maximum is of the same magnitude as the CUPID spectrum. **b.** Pure shift spectrum generated via the  $-45^\circ$  signal. **c.** Conventional 1D spectrum. **d.** Multiplet structures assigned ( $\epsilon = 2 \text{ Hz}$ ). **e.** Magnitude-mode 2DJ spectrum, with coloured points denoting the frequencies of oscillators assigned using estimation. N.B. This 2DJ spectrum was produced using a more concentrated sample of estradiol, since the original 2DJ dataset was too insensitive to produce a sufficiently sensitive spectrum after sine-bell apodisation.

a reasonable parameter estimate of the 2DJ dataset, an agreeable pure shift spectrum. Due to the severe signal overlap in the first direct-dimension FID, initial values for the model order had to be manually specified. It is clear from inspection of the most downfield region that certain strong coupling artefacts have been incorporated into the estimation result, manifesting in the appearance of artefacts in the pure shift spectrum (see the positions marked by the grey vertical lines in Figure 4.10.b).

The time elapsed to run the estimation routine was rather long, at 10.25 min for all regions considered (see Table D.7 for a more detailed description of timings). This is largely attributable to the high model orders, particularly in the most downfield region (this region alone took over 5.5 min to estimate).

## 4.4 Summary

In this chapter, CUPID, a procedure for the construction of pure shift spectra via the holistic estimation of 2DJ datasets, is presented. Such spectra can possess myriad beneficial features relative to alternative methods, albeit with the requirement of a complex post-processing procedure.

Through a number of examples, it has been shown that by employing parametric estimation, a simple 2DJ experiment can be harnessed to generate pure shift spectra with sharp absorption Lorentzian peaks which retain the same signal intensity as the 2DJ experiment. It is able to perform admirably even when state of the art techniques like PSYCHE produce spectra with such low SNRs as to render them unusable. Frequently, CUPID is able to automatically discard oscillators present in the model which either correspond to strong coupling artefacts or noise, leading to simplified spectra in which appear to adhere to the weak coupling regime. There are cases where strong coupling artefacts do end up in the estimation result. It has been shown that these can be manually neglected from the parameter set so they don't have an unwanted influence on final pure shift spectrum, though this requires manual intervention from a knowledgeable user.

Simultaneously, CUPID can assign multiplet structures, by grouping oscillators which lie along a specific  $45^\circ$  cross section in frequency space. Achieving this experimentally — effectively involving a 2DJ experiment in conjunction with a pure shift element — requires running an extremely long (hours or even days) 3D pulse sequence. The usefulness of the multiplet structures generated by CUPID is dependent on the level of the estimation routine's accuracy. In numerous occasions in the examples presented here, the estimation routine was unable to resolve certain, similar frequency signals. A complete understanding of the coupling network associated with a given spin is not possible when this is so. However, such multiplet structures can still provide valuable insights into a given sample.

CUPID is limited by the complexity of the dataset of interest. The reasons for this are two-fold. First, with datasets comprising progressively more peaks in a given spectral region, the difficulty in estimating the dataset becomes harder. Second, with an increased model order required to estimate the dataset, the time required for computation increases drastically. This feature is most clearly observed when comparing the times required in estimating the different regions considered in the estradiol example. As a rule of thumb, it is anticipated that CUPID will perform admirably on datasets derived from small molecules, though datasets derived from large molecules such as proteins are likely to be too complex and demanding for good results.

# Software

5

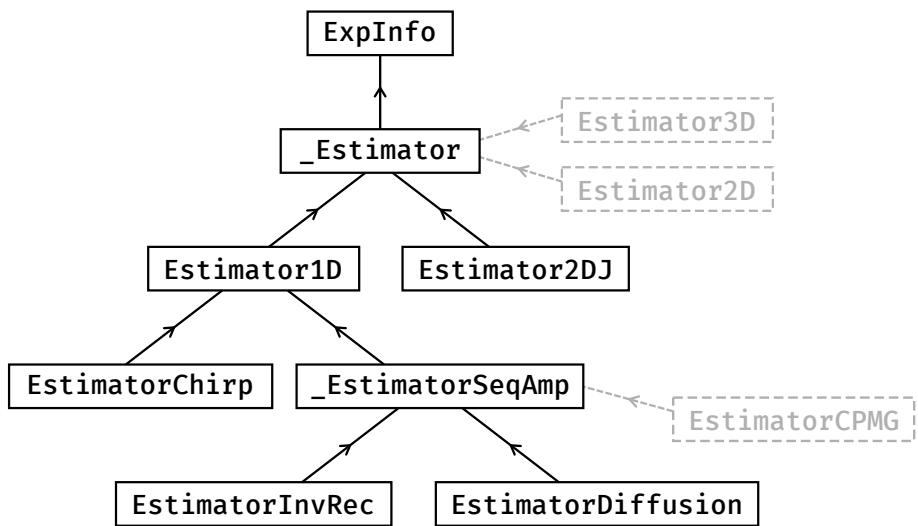
The estimation routine and applications presented in the previous three chapters are accessible via the *NMR estimation in Python* (NMR-EsPy) package. NMR-EsPy aims to provide a feature-rich yet simple interface in order to estimate datasets of interest. In this chapter, a short overview of the package, as well as its accompanying graphical user interface (GUI), is given.

## 5.1 A description of NMR-EsPy

### 5.1.1 Why PYTHON?

There a number of reasons why PYTHON was the chosen programming language for NMR-EsPy:

- It has a large user-base, particularly within the scientific community.
- The SCIPY ecosystem[164], including the packages NUMPY[165] and MATPLOTLIB[166] enables high-performance scientific computation and visualisation in PYTHON, despite the language's reputation for slow speed.
- Being a scripting language with user-friendly syntax makes PYTHON ideal for exploring datasets in a step-by-step fashion. This is useful in the context of NMR-EsPy, as a user will want to (a) inspect and pre-process the data of interest, (b) determine the regions they wish to estimate and set up the estimation routine, (c) output and inspect the result. This can be achieved easily by “hacking” and re-running PYTHON scripts or by using notebook environments, such as JUPYTER.
- It is free and open-source, as opposed to well-known scientific computing platforms such as MATLAB and MATHEMATICA.
- PYTHON supports sophisticated object-oriented programming features, including multiple levels of inheritance. This is exploited in NMR-EsPy in order to create numerous objects



**Figure 5.1:** Inheritance tree for estimation classes in the NMR-EsPy package. Arrows are directed from child classes to the parent class they directly inherit from. Classes in grey are objects that could be added to the application programming interface (API) in the future.

designed with specific NMR data types in mind (see 5.1.2).

Probably the largest disadvantage in using `PYTHON` is its slow performance; some of the features which makes `PYTHON` user-friendly lead to significant runtime overheads\*. While `NUMPY` provides interfaces to run fast computations with pre-compiled C-code, a significant performance benefit would likely be realised if a low-level compiled language like C, C++, or `RUST` were used instead (this is discussed more in Section 6.2). While this may be so, the development time in writing programs with these lower-level languages is typically a lot greater than with a language with a higher level of abstraction like `PYTHON`.

### 5.1.2 Estimator objects

The fundamental user-facing objects (or classes) that NMR-EsPy provides are *estimators*. Instances of these estimator objects contain relevant piece of data called *attributes* (e.g. the FID and experiment parameters including the sweep width and transmitter offset), as well as *methods* which perform useful routines like estimation and result figure generation. Thanks to `PYTHON`'s support for multiple levels of inheritance, it is possible to build numerous objects with certain shared attributes and methods, but which also possess bespoke features that are solely of relevance to the type of NMR data being considered. As an example, only the `Estimator2DJ` object possesses a method called `cupid_spectrum`, which returns the FT of the  $-45^\circ$  signal. Figure 5.1 provides an inheritance diagram for the different estimator classes in NMR-EsPy. Basic overviews of each

\*`PYTHON` is interpreted rather than compiled, dynamically typed rather than statically typed, and it relies on garbage collection for memory management, rather than requiring the programmer to do this manually. All of these features are slower than the alternatives which are mentioned.

class are as follows:

- **ExpInfo** stores the parameters used for a particular NMR experiment. `ExpInfo` also has methods for the generation of the timepoints/chemical shifts sampled based on these parameters, and for producing synthetic FIDs.
- **\_Estimator** inherits experimental parameters from `ExpInfo`, but also possess the NMR dataset itself. This class is designed to contain the functionality which can be generalised across all NMR data types supported by NMR-EsPy. It does not possess all the features necessary to be useful as a standalone object, and as such the user is not permitted to use it directly (such an object is often referred to as an abstract class). For child classes of `_Estimator`, the main feature that requires methods to be defined is the means by which the data is imported into the class.
- **Estimator1D** handles conventional 1D datasets, such as those in Section 3.1.
- **\_EstimatorSeqAmp** is an abstract class which enables the estimation of sequential 1D datasets such as those described in Section 3.2. Analysis of a given dataset varies depending on the type of experiment considered, since the function used for fitting amplitudes (Table 3.2), and the means by which that data should be imported/generated varies. As such, this is not designed for direct use; one of the classes which inherit it should be used instead. Under the hood, `_EstimatorSeqAmp` stores a number of `Estimator1D` objects, with each object containing one of the FIDs in the sequential dataset. Estimation simply comprises looping through these estimators, giving the parameter estimate of the previous estimator to next as its initial guess.
- **EstimatorInvRec** is for the estimation of inversion recovery datasets.
- **EstimatorDiffusion** is for the estimation of diffusion datasets.
- **EstimatorChirp** is for the estimation of FIDs acquired using single-chirp excitation, as described in Section 3.3.
- **Estimator2DJ** is for the estimation of 2DJ data. This class also provides features to generate pure shift spectra and assign multiplet structures using CUPID, as described in Chapter 4.

Other estimator objects which are yet to be implemented, but are potential future additions to the package are also depicted in the inheritance diagram. `EstimatorCPMG` would enable the analysis of CPMG datasets, while `Estimator2D` and `Estimator3D` would be for the estimation of datasets comprising sets of 2D or 3D amplitude- or phase-modulated FIDs, respectively. A discussion of the feasibility of implementing 2D and 3D estimators is given in Section 6.2.

### 5.1.3 Example usage

**Code Listing 5.1:** An example script which makes use of NMR-EsPy in order to make use of the CUPID.

```

1 from pathlib import Path
2 import nmresp as ne
3
4 datapath = Path("~/data/camphor/").expanduser()
5 estimator = ne.Estimator2DJ.new_bruker(datapath / "1")
6 estimator.phase_data(p0=5.238, p1=-6.262)
7 estimator.baseline_correction()
8
9 regions = [
10     (2.55, 2.475), (2.35, 2.23), (2.09, 2.025),
11     (1.95, 1.75), (1.7, 1.61), (1.375, 1.215),
12 ]
13 for region in regions:
14     estimator.estimate(
15         region=region, noise_region=(5.25, 5.21), region_unit="ppm",
16         nlp_trim=2048,
17     )
18
19 estimator.to_pickle(datapath / "camphor_2dj_espy")
20 estimator.write_cupid_to_bruker(datapath, expno=2)
21 thold = 2. * estimator.sw()[1] / estimator.default_pts[1] #  $\epsilon = 2f_{sw}^{(2)}/N^{(2)}$ 
22 fig, _ = estimator.plot_result(multiplet_thold=thold)
23 fig.savefig("camphor_2dj.pdf")

```

Code Listing 5.1 provides an example of NMR-EsPy being used for the consideration of 2DJ data; it is the script which was to generate the camphor result presented in Figure 4.8. The script carries out the following

1. An `Estimator2DJ` object is initialised to import and store the dataset, stored in `BRUKER` format at the path `$HOME/data/camphor/1†` (Line 5).
2. The 2DJ FID is pre-processed to ensure it is phased and features a flat spectral baseline (Lines 6 and 7).
3. The regions of interest are defined, in units of ppm (Lines 9 to 12). Each region is given by a two-element tuple containing its left- and right-boundaries.
4. For each region, parameter estimates are determined using the `Estimator2D.estimate` method, which constructs a filtered sub-FID, and subsequently estimates it (Lines 13 to 17). Most ar-

<sup>†</sup>\$HOME denotes the current user's home directory on a UNIX-based system.

guments given are self-explanatory; `nlp_trim` can be set to truncate the sub-FID in the direct dimension, to reduce the computational burden on the NLP routine.

5. After estimation is complete, the estimator object is saved to a byte stream using PYTHON’s “pickling” protocol[167] (Line 19). This enables the estimator to be recovered at a later time.
6. A pure shift spectrum is produced via the  $-45^\circ$  signal, and stored to the path `$HOME/data/camphor/2` in a format that enables it to be read by software that supports BRUKER datasets (Line 20).
7. Finally, a PDF figure depicting the estimation result is produced and saved (Lines 22 and 23). The form the figure takes is reminiscent of Figure 4.8, though many customisations have been applied to the latter.

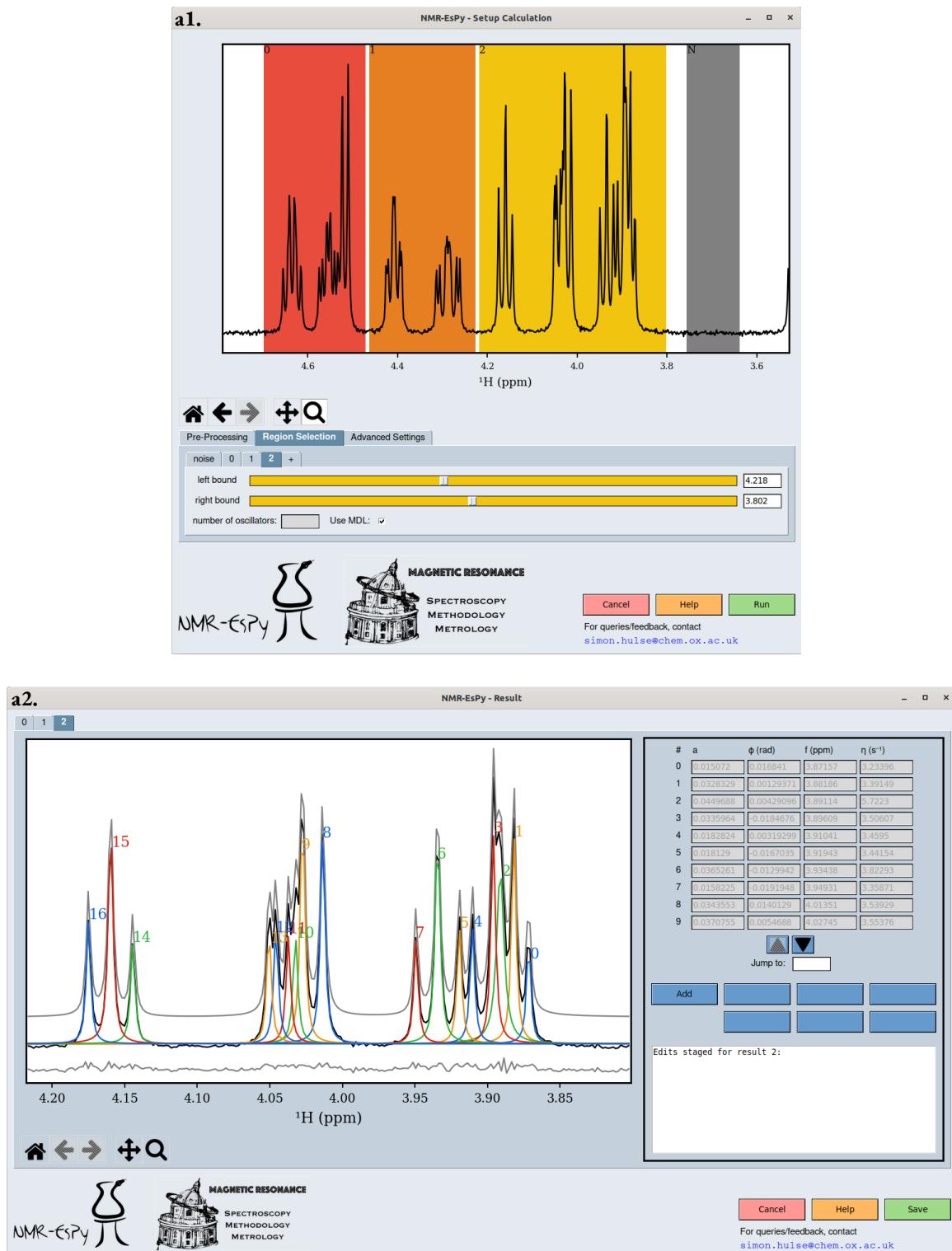
## 5.2 The NMR-EsPy GUI

Along with the NMR-EsPy API, an accompanying GUI which makes use of the TKINTER toolkit[168] ships with the package. This can be accessed either via the command line, or within BRUKER’s TOPSPIN software to provide a more seamless workflow in analysing NMR data acquired on BRUKER spectrometers. At the time of writing, the GUI only supports conventional 1D and 2DJ datasets. Screenshots of the GUIs for both data types are provided in Figure 5.2. The GUI comprises two primary windows; the first enables the estimation routine to be set up (Figures 5.2.a1 and 5.2.b1), while the second is for inspecting the result and exporting result information to desired formats (Figures 5.2.a2 and 5.2.b2). The set-up window allows the following actions are carried out:

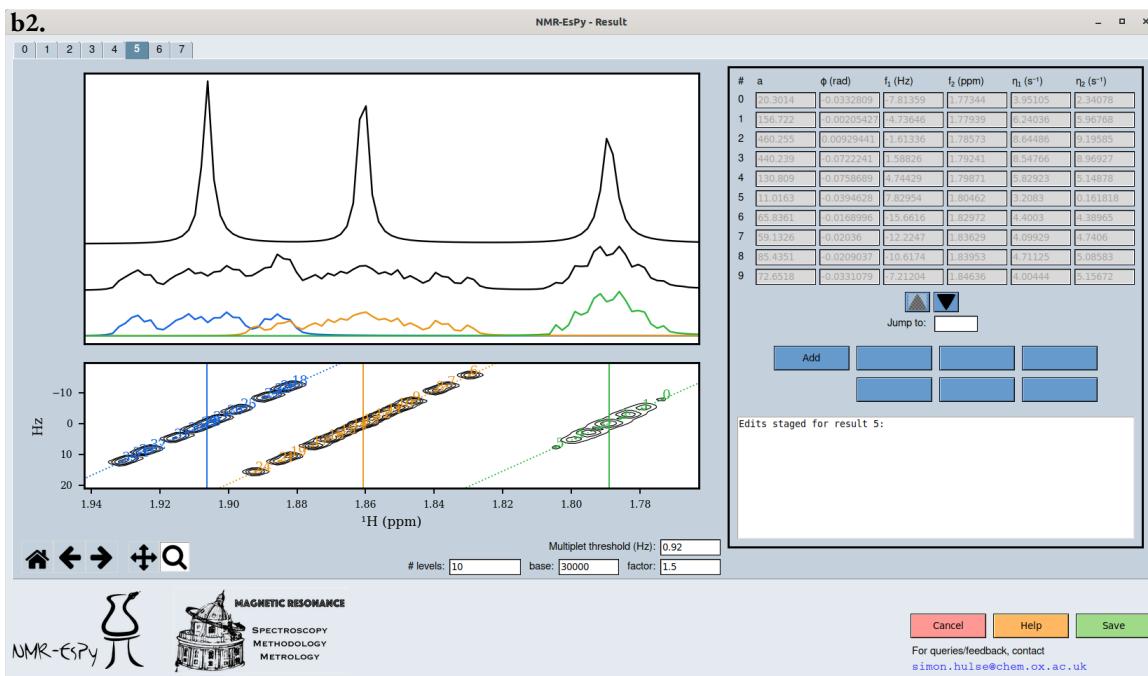
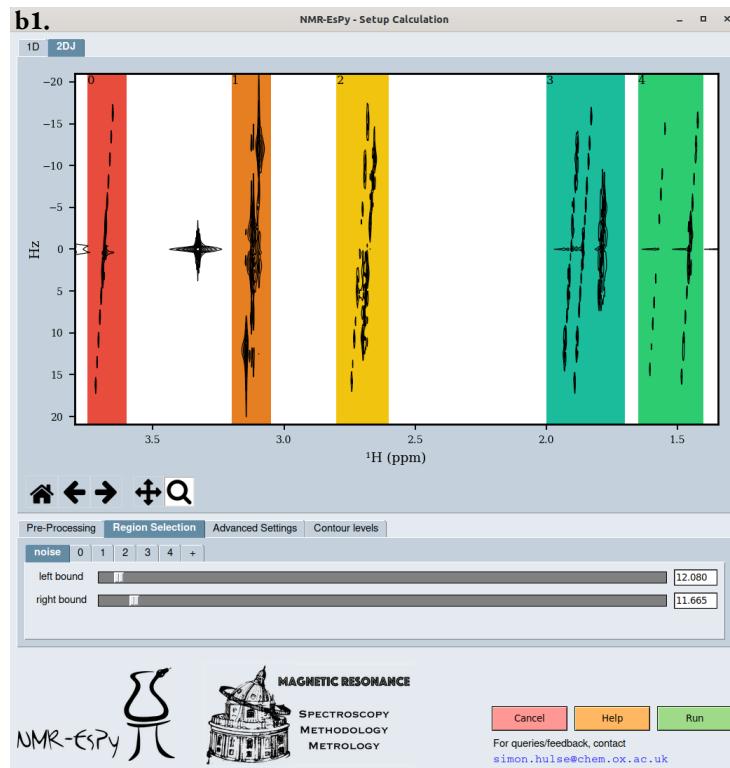
- The *Pre-Processing* tab facilitates phase correction, application of exponential line-broadening<sup>‡</sup>, and baseline correction. If the imported data has already been processed by some other software such as TOPSPIN<sup>§</sup>, this step can be skipped.
- The regions of interest and the noise region are defined with the *Region Selection* tab. Examples of the appearance of the GUI after a number of regions have been defined by the user are given in the figure; regions interest are denoted by various colours, while the noise region is grey.

<sup>‡</sup>Exponential line-broadening is the only type of apodisation which is supported in NMR-EsPy; use of any other window function would render the model used to fit the data incompatible. Line-broadening should only be applied in situations where the FID is truncated, such that sinc wiggles are visible in the spectrum, as these will have an unwanted influence on filtered sub-FIDs generated.

<sup>§</sup>For 1D datasets, it is possible to import raw FID data (`f1d`) or processed spectral data (`1r`). If pre-processed data is imported, NMR-EsPy performs IFT and truncates the conjugate-symmetric signal generated in half to recover the FID. For 2DJ data, it is necessary to import 2DJ data as a raw FID (`ser`).



**Figure 5.2:** Screenshots of windows that form part of the NMR-EsPy GUI for 1D estimation (a.) and 2DJ estimation (b.). For both data types, the windows used to setup the estimation routine (1.) and inspect the result (2.) are shown. (Continues on the next page)



Continuation of FIGURE 5.2.

- *Additional Settings* allows features related to the estimation routine to be customised, including whether to approximate the Hessian matrix or compute its exact form, whether to predict the model order using the MDL or to manually specify a value, and setting a threshold for the maximum number of iterations allowed before the NLP routine terminates.

The result window features a figure depicting the outcome of the estimation routine with a table of all the estimated parameters. The final stage in using the GUI involves specifying the formats to output the result to. Figures and parameter tables summarising the result can be exported to various formats, as well as simulated signals constructed using the parameter estimate (e.g. the pure shift spectrum produced by CUPID).

### 5.3 Summary

In this chapter, an overview of the software associated with this project, a `PYTHON` package call `NMR-EsPy`, has been provided. There are more resources available for additional information on `NMR-EsPy`. A rigorous description of the usage of `NMR-EsPy`, including details on installation, and a reference for the API are given in the documentation for `NMR-EsPy`, found at <https://foroozandehgroup.github.io/NMR-EsPy/>. One chapter of the documentation, which provides tutorials to help users gain familiarity with the API, is included in this work (see Appendix E.1). `NMR-EsPy` is open source, under the MIT license, with the source code hosted on the Foroozan-deh group's GitHub page at <https://github.com/foroozandehgroup/NMR-EsPy>.

# Conclusions and Future Work

6

## 6.1 Conclusions

This work has focussed on the use of parametric estimation as a means of extracting quantitative information from NMR FIDs. The initial motivation can come from interest in developing a technique for quantifying 2DJ datasets, facilitating the generation of broadband homodecoupled NMR spectra with desirable characteristics. To achieve this, the MMEMPM, a 2D extension of the original MPM, was proposed as a suitable technique for parametrising 2DJ datasets in a holistic fashion. However, initial evaluations of estimation results generated by the MPM on 1D FIDs indicated that a particular flaw was common: the phases of individual oscillators were often inconsistent with their expected behaviour. For this reason, a routine was developed which incorporated the result of the MPM as an initial guess of an NLP algorithm. The NLP algorithm included the variance of oscillator phases in the fidelity to be minimised as a means of constraining the phases to adopt similar values. Through a number of examples, it has been shown that improved parameter estimates can be obtained by including this NLP routine.

To alleviate the high computational burden of the proposed method — the most noteworthy aspects being computing the SVD of large matrices and computing large numbers of derivatives to generate Hessian matrices — a frequency-filtration technique has been incorporated, which produces sub-FIDs with reduced numbers of both constituent signals and datapoints. Drastic reductions in both CPU work and RAM usage are possible by doing this. Furthermore, it enables the user to neglect spectral regions that are not of interest/too complex to realistically yield meaningful information from.

Impressive parametrisations of hypercomplex 2DJ FIDs were realised with the estimation routine, leading to CUPID, which is able to generate pure shift spectra without the loss of signal, and featuring peaks with sharp Lorentzian lineshapes. Furthermore, CUPID is able to provide fur-

ther insights, such as harnessing the information from 2DJ estimation to decompose 1D spectra into their constituent multiplet structures. Acquiring the information that CUPID can generate with a simple 2DJ dataset usually requires bespoke 3D pulse sequences with a very large associated run-times.

Further to the original goal of 2DJ estimation, two other applications have been developed and presented here. The first is an alternative means for determining valuable information about molecular species ( $T_1$  and  $T_2$  times of spins, and diffusion coefficients) via datasets which comprise a series of FIDs whose signal amplitudes vary. Whereas typical univariate approaches to analysing these datasets involve fitting single datapoints in frequency space, the method showcased instead aims to gleam the information for each signal explicitly, to overcome the aggregating effect frequently encountered due to signal overlap. While the method works admirably, it couldn't be shown to perform noticeably better than other techniques; in cases where there is severe signal crowding, the difficulty/impossibility of resolving each component leads to similar issues of aggregating signals.

A second application featuring 1D estimation involves generating broadband NMR spectra from an experiment involving excitation by a single chirp pulse. [More here](#)

The software package NMR-EsPy has been developed to facilitate use of the methods described in this thesis. The package's API follows a straightforward object-oriented paradigm, which should make it easily accessible to all members of the NMR community that have experience with scientific computing with PYTHON. Furthermore, the availability of an accompanying GUI widens to accessibility of the package further, meaning NMR-EsPy can be used without writing a single line of code. The package has been heavily documented too; this is a crucial aspect of any piece of user-facing software which seems to often be lacking, especially when it comes to the field of academia.

### **1D estimation hard: lots of overlap, 2D/3D probably more interesting: notable issues (future work)**

It has hopefully been shown that attempting to solve the inverse problem of NMR data estimation is a valuable pursuit; it provides richer information than that which is typically available with the conventional FT method, and it opens up many fruitful applications which can enhance the value that NMR can offer to practitioners in many scientific disciplines.

## **6.2 Future Work**

Any future work related to this project would be centered around extending and improving the NMR-EsPy package. Some possible pursuits include the following:

*Improving performance* Improvements in the speed of the estimation could be realised if the most computationally demanding parts of it were written in a low-level compiled language like C++ or RUST. This may not be the case for the MPM and MMEMPM; the majority of time running these routines involves SVD, with NUMPY’s implementation calling well-optimised routines from the LAPACK and ARPACK software packages. However, in its current state, the NLP routine could well be sped up considerably if the current PYTHON implementation were ported to one of the aforementioned languages.

*A more general platform* Thinking further afield from the specific estimation routine considered in this work, the NMR-EsPy package provides a large number of useful features which would be applicable to the estimation using any conceived method. This includes functionality to import data, pre-process data, and inspect the result of an estimation routine through parameter tables and figures. Incorporating other estimation routines into the software would therefore be rather straightforward, such that NMR-EsPy could become a general-purpose platform for comparing different methods.

*2D and 3D datasets* Another potential future venture would be to extend the routine for the consideration of other 2D datasets, such as those that comprise amplitude- or phase-modulated pairings, as well as 3D datasets, including those acquired from “triple-resonance” experiments which are popular in the biological NMR community[22: Section 7.4]. As shown in Chapter 4, the method is capable of performing well on hypercomplex 2D datasets. In order to achieve 3D estimation, it would be necessary to make use of a 3D equivalent of the MMEMPM. Such a technique exists, and is used principally for sensing applications, in which the direction (i.e. azimuth and elevation angles) as well as the frequency of waves arriving at an antenna are sought[169]. However, there is a key issue with multidimensional NMR signals which would likely hamper the method outlined in this thesis from being effective. 2DJ datasets are rather anomalous in that they have very densely populated indirect dimensions. For this reason, it is not necessary to be concerned about filtering the data in the indirect dimension. However, for most 2D datasets, it would be desirable to filter the data in both dimensions, as both will generally be sparsely populated. While the filtering procedure presented works well on direct-dimension FIDs, which have usually decayed to noise at the end of acquisition, indirect-dimension FIDs are often truncated. The FT of such signals without any treatment would produce spectra with considerable truncation artefacts; filtering such spectra would incorporate undesirable artefacts into a filtered sub-FID, rendering it worthless. Compensating for the truncation could be achieved, by applying exponential apodisation prior to FT. However, this would then lead to spectra with broader lineshapes, such that wider spectral regions would need to be selected, and the resolution of the data would be decreased. Dealing with truncated signals could possibly be handled in one of two ways, beyond running the experiment to acquire the data with a huge number of increments. One option would be to propa-

gate the FID further in time using LP. Another would be to apply conventional apodisation, such as a sine-bell function to the FID, producing a FID without truncation artefacts and acceptable resolution. However, applying a non-exponential weighting to the dataset however render the data incompatible with the estimation routine in its current form, such that a modified routine with a suitable model would need to be implemented. On to of issues with data applicability, for 3D estimation the computational burden required would also likely be too high for the routine to be practicable beyond the simplest datasets with few points and minimal numbers of signals.

*Incorporating constraints into the NLP routine* The estimation routine in its current form is designed to require as little user input as possible while producing faithful parameter estimates. However, in particularly challenging circumstances, most notably when there is extreme signal overlap, the inclusion of oscillator phase variance alone can be insufficient to produce estimates which closely agree with the experiment. When this is the case, it would be useful to enable users to specify additional knowledge, incorporated into the routine as additional regularising terms, *after* the initial estimation has been performed. This concept, while similar to VARPRO and AMARES, differs in that these require very large quantities or prior knowledge *before* estimation. A lot of the heavy lifting towards an accurate parameter estimate could be achieved using phase variance-regularised NLP, with the user indicating erroneous features subsequently.

Take the cyclosporin A result (Figure 3.3) as an example. As discussed already, due to severe signal overlap, the assigned oscillators related to spin (E), while at the correct frequencies, do not have appropriate amplitudes for a dq multiplet structure. As such, re-running NLP, with a new fidelity of

$$\mathcal{F}_\phi(\theta | Y) + \text{Var}(\alpha_{E1}, \frac{1}{3}\alpha_{E2}, \alpha_{E3}, \frac{1}{3}\alpha_{E4}, \frac{1}{3}\alpha_{E5}, \alpha_{E6}, \frac{1}{3}\alpha_{E7}, \alpha_{E8})$$

would likely lead to an improved result.  $\{E1, \dots, E8\} \subset \{1, \dots, M\}$  are the indices of the oscillators corresponding to spin (E), i.e. the green oscillators in the figure.

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# NMR Glossary

A

This glossary comprises many terms related to NMR which are mentioned, but not necessarily described in much detail in the main text.

## TODO

*Chemical Shift* The term chemical shift typically refers to the resonance frequency of a nucleus relative to some standard frequency:

$$\delta = \frac{\omega - \omega_{\text{ref}}}{\omega_{\text{ref}}}.$$
 (A.1)

The numerator and denominator are usually given in units of Hz and MHz, respectively. As such, the unit of the chemical shift is  $10^{-6}$ , i.e. “parts per million” (ppm).



# Additional Theory

B

## B.1 Mathematical definitions

Descriptions of linear algebra and statics concepts that are referred to in this thesis are provided here. More detail can be found in numerous relevant texts[170, 171].

### B.1.1 Linear algebra

**TODO:** null space, rank, range

#### Singular value decomposition

SVD is a generalisation of eigendecomposition for a matrix of any shape. Given a matrix  $\mathbf{A} \in \mathbb{C}^{m \times n}$ , the SVD is a factorisation given by

$$\mathbf{A} = \mathbf{U}\Sigma\mathbf{V}^\dagger. \quad (\text{B.1})$$

The matrices that make up the decomposition are as follows

$\Sigma \in \mathbb{C}^{m \times n}$  is a rectangular diagonal matrix with diagonal elements comprising the *singular values* in descending order of magnitude. The singular values are the square roots of the non-zero eigenvalues of both  $\mathbf{A}^\dagger \mathbf{A}$  and  $\mathbf{A} \mathbf{A}^\dagger$ .

$\mathbf{U} \in \mathbb{C}^{m \times m}$  is a unitary matrix whose columns comprise the *left singular vectors*. The left singular vectors are the eigenvectors of the matrix  $\mathbf{A} \mathbf{A}^\dagger$ .

$\mathbf{V} \in \mathbb{C}^{n \times n}$  is a unitary matrix whose columns comprise the *right singular vectors*. The right singular vectors are the eigenvectors of the matrix  $\mathbf{A}^\dagger \mathbf{A}$ .

One fundamental property of the SVD is that the number of non-zero singular values is equivalent to the rank of the matrix. As the EYM theorem highlights, the SVD is valuable in constructing

low-rank approximations of matrices, with applications in various fields such as signal processing, (see Section 2.2.1) and data compression.

### Special matrices

A *Hankel matrix* is a matrix in which each ascending diagonal from left to right possesses identical elements. While Hankel matrices are often defined to be square, in this work such a restriction is not applied. Given a matrix  $X \in \mathbb{F}^{M \times N}$ , the matrix is Hankel if

$$x_{m,n} = x_{m+1,n-1} \quad (\text{B.2})$$

$\forall m \in \{1, \dots, M - 1\} \forall n \in \{2, \dots, N\}$ . Similarly, a *Toeplitz matrix* is a matrix in which every descending diagonal from left to right possesses identical elements, i.e.

$$x_{m,n} = x_{m+1,n+1} \quad (\text{B.3})$$

$$\forall m \in \{1, \dots, M - 1\} \forall n \in \{1, \dots, N - 1\}.$$

### B.1.2 Statistics and probability

**TODO: Likelihood function, MLE**

**pdf!**

The **pdf!** (**pdf!**)  $p(x) : \mathbb{R} \rightarrow \mathbb{R}$  is a function over a continuous sample space which provides relative likelihoods between potential values of  $x$ . The probability that a random sample obeying a known distribution lies within the range  $[x_a, x_b]$  is given by the integral

$$P(x_a \leq x \leq x_b) = \int_{x_a}^{x_b} p(x) dx. \quad (\text{B.4})$$

The integral of  $p(x)$  over the entire sample space is defined to be unity. Also, the **pdf!** of a specific value is always 0, since the width of the region of integration is 0.

**Likelihood function**

## B.2 Estimation Errors

A measure of the degree of uncertainty in the parameter estimates can be obtained by computing the *standard errors* associated with the NLP routine. Standard errors are related to the *observed*

*Fisher information matrix* at convergence[171: Section 2.7]:

$$\epsilon(\theta^{(*)}) = \sqrt{\text{diag}(\mathbf{I}(\theta^{(*)})^{-1})}, \quad (\text{B.5})$$

where the observed Fisher Information matrix contains the negative partial second derivatives of the log-likelihood with respect to  $\theta$ :

$$\mathbf{I}(\theta)_{i,j} = -\frac{\partial^2 \ell(\theta | Y)}{\partial \theta_i \partial \theta_j}. \quad (\text{B.6})$$

Recalling the form of the log-likelihood given by Equation 2.6, the elements of  $\mathbf{I}(\theta)$  are

$$\mathbf{I}(\theta)_{i,j} = -\frac{1}{\sigma^2} \Re \left( \left\langle \frac{\partial \mathbf{X}}{\partial \theta_i}, \frac{\partial \mathbf{X}}{\partial \theta_j} \right\rangle - \left\langle (\mathbf{Y} - \mathbf{X}), \frac{\partial^2 \mathbf{X}}{\partial \theta_i \partial \theta_j} \right\rangle \right), \quad (\text{B.7})$$

which very closely resembles the Hessian of  $\theta$ :

$$\mathbf{I}(\theta)_{i,j} = \frac{1}{2\sigma^2} \mathbf{H}(\theta)_{i,j}. \quad (\text{B.8})$$

The standard errors therefore take the form

$$\epsilon(\theta^{(*)}) = \sqrt{2\sigma^2 \text{diag}(\mathbf{H}(\theta^{(*)})^{-1})}. \quad (\text{B.9})$$

The mean and variance of the noise are 0 and  $2\sigma^2$ , respectively, leading to:

$$2\sigma^2 = \frac{1}{N-1} \|\mathbf{W}\|^2 = \frac{1}{N-1} \|\mathbf{Y} - \mathbf{X}(\theta^{(*)})\|^2. \quad (\text{B.10})$$

Finally a useable expression for the standard errors is arrived at:

$$\epsilon(\theta^{(*)}) = \sqrt{\frac{\mathcal{F}(\theta^{(*)}) \text{diag}(\mathbf{H}(\theta^{(*)})^{-1})}{N-1}} \quad (\text{B.11})$$

## B.3 Multidimensional virtual echos

The VE concept (Section 2.5.1) can be generalised to any number of dimensions, assuming that a pair of amplitude-modulated signals exist for each indirect-dimension. Thus a set of  $2^{D-1}$  signals is required for a  $D$ -dimensional FID. For the 2D case, this corresponds to the pair of signals  $\{\mathbf{Y}^{\cos}, \mathbf{Y}^{\sin}\}$ , given by Equation 1.22 with  $D = 2$  and  $\zeta = \{\cos(\cdot), \sin(\cdot)\}$ , taking the forms (with

noise neglected)

$$y_{n^{(1)}, n^{(2)}}^{\cos} = \xi_{n^{(1)}, n^{(2)}} c_{n^{(1)}, n^{(2)}}^{(1)} \left( c_{n^{(1)}, n^{(2)}}^{(2)} + i s_{n^{(1)}, n^{(2)}}^{(2)} \right), \quad (\text{B.12a})$$

$$y_{n^{(1)}, n^{(2)}}^{\sin} = \xi_{n^{(1)}, n^{(2)}} s_{n^{(1)}, n^{(2)}}^{(1)} \left( c_{n^{(1)}, n^{(2)}}^{(2)} + i s_{n^{(1)}, n^{(2)}}^{(2)} \right), \quad (\text{B.12b})$$

$$\xi_{n^{(1)}, n^{(2)}} = \sum_m a_m \exp \left( -\eta_m^{(1)} n^{(1)} \Delta_t^{(1)} - \eta_m^{(2)} n^{(2)} \Delta_t^{(2)} \right), \quad (\text{B.12c})$$

$$(c/s)_{n^{(1)}, n^{(2)}}^{(1/2)} = \sum_m \cos / \sin \left( 2\pi f^{(1/2)} n^{(1/2)} \Delta^{(1/2)} \right). \quad (\text{B.12d})$$

Four matrices  $\psi_{\pm\pm}$  are then constructed of the form

$$\begin{aligned} \psi_{\pm\pm, n^{(1)}, n^{(2)}} &= \xi_{n^{(1)}, n^{(2)}} \left( c_{n^{(1)}, n^{(2)}}^{(1)} \pm^{(1)} i s_{n^{(1)}, n^{(2)}}^{(1)} \right) \left( c_{n^{(1)}, n^{(2)}}^{(2)} \pm^{(2)} i s_{n^{(1)}, n^{(2)}}^{(2)} \right) \\ &\equiv \Re \left( y_{n^{(1)}, n^{(2)}}^{\cos} \right) \pm^{(1)} \pm^{(2)} - \Im \left( y_{n^{(1)}, n^{(2)}}^{\sin} \right) + i \left( \pm^{(1)} \Re \left( y_{n^{(1)}, n^{(2)}}^{\sin} \right) \pm^{(2)} \Im \left( y_{n^{(1)}, n^{(2)}}^{\cos} \right) \right), \end{aligned} \quad (\text{B.13})$$

from which the matrices  $T_{1 \rightarrow 4} \in \mathbb{C}^{2N^{(1)} \times 2N^{(2)}}$  are generated:

$$T_1 = \begin{bmatrix} \mathbf{Y}_{++} & \mathbf{0} \\ \mathbf{0} & \mathbf{0} \end{bmatrix}, \quad (\text{B.14a})$$

$$T_2 = \begin{bmatrix} \mathbf{0} & \mathbf{0} \\ \mathbf{Y}_{-+}^{\leftrightarrow(1)} & \mathbf{0} \end{bmatrix}^{\circlearrowleft(1)}, \quad (\text{B.14b})$$

$$T_3 = \begin{bmatrix} \mathbf{0} & \mathbf{Y}_{+-}^{\leftrightarrow(2)} \\ \mathbf{0} & \mathbf{0} \end{bmatrix}^{\circlearrowleft(2)}, \quad (\text{B.14c})$$

$$T_4 = \begin{bmatrix} \mathbf{0} & \mathbf{0} \\ \mathbf{0} & \mathbf{Y}_{--}^{\leftrightarrow(1,2)} \end{bmatrix}^{\circlearrowleft(1,2)}. \quad (\text{B.14d})$$

The virtual echo is then given by  $Y_{\text{ve}} = \sum_{i=1}^4 T_i$ , with the first row and column divided by two. For a full outline of the 2D filtering procedure, see Algorithm B.3.

It is possible to construct a virtual echo using an appropriate set of phase-modulated signals too, which for the 2D case would be  $\{Y^{\text{pos}}, Y^{\text{neg}}\}$ , given by Equation 1.22 with  $D = 2$  and  $\zeta = \{\exp(i \cdot), \exp(-i \cdot)\}$ . These can be used to generate an amplitude modulated pair via

$$Y^{\cos} = \frac{Y^{\text{pos}} + Y^{\text{neg}}}{2}, \quad (\text{B.15a})$$

$$Y^{\sin} = \frac{Y^{\text{pos}} - Y^{\text{neg}}}{2i}. \quad (\text{B.15b})$$

## B.4 Additional algorithms

Last minute edit: manually rearrange algorithms so a masses of white space aren't present

---

**Algorithm B.1** The MMEMPM. TRUNCATEDSVD is a routine which computes the first  $M$  SVD components of a matrix.

---

```

1: procedure MMEMPM( $Y \in \mathbb{C}^{N^{(1)} \times N^{(2)}}, M \in \mathbb{N}$ )
2:    $L^{(1)}, L^{(2)} \leftarrow \lfloor N^{(1)}/2 \rfloor, \lfloor N^{(2)}/2 \rfloor;$ 
3:   for  $n^{(1)} \leftarrow \{0, \dots, N^{(1)} - 1\}$  do
4:      $H_{y,n^{(1)}} \leftarrow \begin{bmatrix} y_{n^{(1)},0} & y_{n^{(1)},1} & \cdots & y_{n^{(1)},N^{(2)}-L^{(2)}} \\ y_{n^{(1)},1} & y_{n^{(1)},2} & \cdots & y_{n^{(1)},N^{(2)}-L^{(2)}+1} \\ \vdots & \vdots & \ddots & \vdots \\ y_{n^{(1)},L^{(2)}-1} & y_{n^{(1)},L^{(2)}} & \cdots & y_{n^{(1)},N^{(2)}-1} \end{bmatrix};$ 
5:   end for
6:    $E_Y \leftarrow \begin{bmatrix} H_{y,0} & H_{y,1} & \cdots & H_{y,N^{(1)}-L^{(1)}} \\ H_{y,1} & H_{y,2} & \cdots & H_{y,N^{(1)}-L^{(1)}+1} \\ \vdots & \vdots & \ddots & \vdots \\ H_{y,L^{(1)}-1} & H_{y,L^{(1)}} & \cdots & H_{y,N^{(1)}-1} \end{bmatrix};$ 
7:    $U_M, \Sigma_M, V_M^\dagger \leftarrow \text{TRUNCATEDSVD}(E_Y, M);$ 
8:    $P \leftarrow \mathbf{0} \in \mathbb{C}^{L^{(1)}L^{(2)} \times L^{(1)}L^{(2)}};$ 
9:    $r \leftarrow 0$ 
10:  for  $i = 0, \dots, L^{(2)} - 1$  do
11:    for  $j = 0, \dots, L^{(1)} - 1$  do
12:       $c \leftarrow i + jL^{(2)};$ 
13:       $p_{r,c} \leftarrow 1;$ 
14:       $r \leftarrow r + 1;$ 
15:    end for
16:  end for
17:   $U_{M1}, U_{M2} \leftarrow U_M \left[ :L^{(1)}(L^{(2)} - 1) \right], U_M \left[ L^{(2)} : \right];$   $\triangleright$  Last/First  $L^{(2)}$  rows deleted
18:   $z^{(1)}, W^{(1)} \leftarrow \text{EIGENDECOMPOSITION}(U_{M1}^+ U_{M2});$ 
19:   $f^{(1)}, \eta^{(1)} \leftarrow (f_{sw}^{(1)}/2\pi) \Im(\ln z^{(1)}) + f_{off}^{(1)}, -f_{sw}^{(1)} \Re(\ln z^{(1)});$ 
20:   $U_{MP} \leftarrow P U_M;$ 
21:   $U_{MP1}, U_{MP2} \leftarrow U_{MP} \left[ :(L^{(1)} - 1)L^{(2)} \right], U_{MP} \left[ L^{(1)} : \right];$   $\triangleright$  Last/First  $L^{(1)}$  rows deleted
22:   $G \leftarrow [W^{(1)}]^{-1} U_{MP1}^+ U_{MP2} W^{(1)};$ 
23:  if all values in  $f^{(1)}$  are distinct then  $\triangleright$  See Footnote †, Page 39
24:     $z^{(2)} \leftarrow \text{diag}(G);$ 
25:  else
26:     $R \leftarrow \text{number of distinct frequencies in } f^{(1)};$ 
27:    for  $r = 1, \dots, R$  do
28:       $C_r^{b_r} \ni z_r^{(2)} \leftarrow \text{EIGENVALUES}(G_r)^*;$   $\triangleright$  See Equation 2.28.
29:    end for
30:  end if
31:   $f^{(2)}, \eta^{(2)} \leftarrow (f_{sw}^{(2)}/2\pi) \Im(\ln z^{(2)}) + f_{off}^{(2)}, -f_{sw}^{(2)} \Re(\ln z^{(2)});$ 

```

---

\*N.B. Here it is assumed that  $G$  is block-diagonal, in accordance with Equation 2.28. In practice  $G$  may not be block-diagonal, as whether it is or not is dependent on the ordering of the rows and columns in the matrix. A more explicit depiction of how  $G_r$  can be extracted from  $G$  is provided by Code Listing C.4 (Lines 88 to 114).

32:  $\mathbf{Z}_L^{(2)} = \begin{bmatrix} \mathbf{1} & z^{(2)} & z^{(2)2} & \dots & z^{(2)L^{(2)}-1} \end{bmatrix}^T;$   
 33:  $\mathbf{Z}_R^{(2)} \leftarrow \begin{bmatrix} \mathbf{1} & z^{(2)} & z^{(2)2} & \dots & z^{(2)N^{(2)}-L^{(2)}} \end{bmatrix};$   
 34:  $\mathbf{Z}_D^{(1)} \leftarrow \text{diag}(z^{(1)});$   
 35:  $\mathbf{E}_L \leftarrow \begin{bmatrix} \mathbf{Z}_L^{(2)} \\ \mathbf{Z}_L^{(2)} \mathbf{Z}_D^{(1)} \\ \vdots \\ \mathbf{Z}_L^{(2)} [\mathbf{Z}_D^{(1)}]^{L^{(1)}-1} \end{bmatrix};$   
 36:  $\mathbf{E}_R \leftarrow \begin{bmatrix} \mathbf{Z}_R^{(2)} & \mathbf{Z}_D^{(1)} \mathbf{Z}_R^{(2)} & \dots & [\mathbf{Z}_D^{(1)}]^{N^{(1)}-L^{(1)}} \mathbf{Z}_R^{(2)} \end{bmatrix};$   
 37:  $\alpha \leftarrow \text{diag}(\mathbf{E}_L^* \mathbf{E}_Y \mathbf{E}_R^*);$   
 38:  $\alpha, \phi \leftarrow |\alpha|, \arctan\left(\frac{\Im(\alpha)}{\Re(\alpha)}\right);$   
 39:  $\theta^{(0)} \leftarrow \begin{bmatrix} \alpha^T & \phi^T & [f^{(1)}]^T & [f^{(2)}]^T & [\eta^{(1)}]^T & [\eta^{(2)}]^T \end{bmatrix}^T;$   
 40: **return**  $\theta^{(0)}$   
 41: **end procedure**

---

---

**Algorithm B.2** ST method for determining an update in NLP. This is equivalent to Algorithm 7.2 in [88].

---

```

1: procedure STEIHAUGTOINT( $Y \in \mathbb{C}^{N^{(1)} \times \dots \times N^{(D)}}$ ,  $\theta^{(k)} \in \mathbb{R}^{2(1+D)M}$ ,  $\Delta^{(k)} \in \mathbb{R}_{>0}$ )
2:    $g \leftarrow \nabla \mathcal{F}_\phi(\theta^{(k)} | Y)$ ; ▷ Grad vector: Equation 2.45a
3:    $H \leftarrow \nabla^2 \mathcal{F}_\phi(\theta^{(k)} | Y)$ ; ▷ Hessian matrix, either exact: Equation 2.45b or approximate: Equation 2.48
4:    $\epsilon^{(k)} \leftarrow \min(1/2, \sqrt{\|g\|}) \|g\|$ ;
5:    $z^{(0)} \leftarrow \mathbf{0} \in \mathbb{R}^{6M}$ ;
6:    $r^{(0)} \leftarrow g$ ;
7:    $d^{(0)} \leftarrow -r^{(0)}$ ;
8:   if  $\|r^{(0)}\| < \epsilon^{(k)}$  then
9:     return  $z^{(0)}$ ;
10:  end if
11:  for  $j = \{0, 1, \dots\}$  do
12:    if  $d^{(j)\top} H d^{(j)} \leq 0$  then
13:      Find  $\tau$  such that  $p^{(k)} = z^{(j)} + \tau d^{(j)}$  minimises  $\mathcal{F}_{\phi Q}(\theta^{(k)} + p^{(k)})$ , subject to  $\|p^{(k)}\| = \Delta^{(k)}$ ;
14:      return  $p^{(k)}$ ;
15:    end if
16:     $\alpha^{(j)} \leftarrow \frac{r^{(j)\top} r^{(j)}}{d^{(j)\top} H d^{(j)}}$ ;
17:     $z^{(j+1)} \leftarrow z^{(j)} + \alpha^{(j)} d^{(j)}$ ;
18:    if  $\|z^{(j+1)}\| < \epsilon^{(k)}$  then
19:      Find  $\tau \in \mathbb{R}_{>0}$  such that  $p^{(k)} = z^{(j)} + \tau d^{(j)}$  satisfies  $\|p^{(k)}\| = \Delta^{(k)}$ ;
20:      return  $p^{(k)}$ ;
21:    end if
22:     $r^{(j+1)} \leftarrow r^{(j)} + \alpha^{(j)} H d^{(j)}$ ;
23:    if  $\|r^{(j+1)}\| < \epsilon^{(k)}$  then
24:      return  $z^{(j+1)}$ ;
25:    end if
26:     $\beta^{(j+1)} \leftarrow \frac{r^{(j+1)\top} r^{(j+1)}}{r^{(j)\top} r^{(j)}}$ ;
27:     $d^{(j+1)} \leftarrow -r^{(j+1)} + \beta^{(j+1)} d^{(j)}$ ;
28:  end for
29: end procedure

```

---

**Algorithm B.3** Filtering procedure for 2D data.

---

```

1: procedure FILTER2D( $Y_{\cos} \in \mathbb{C}^{N^{(1)} \times N^{(2)}}, Y_{\sin} \in \mathbb{C}^{N^{(1)} \times N^{(2)}}, R_{\text{interest}} \in \mathbb{N}_0^{2 \times 2}, R_{\text{noise}} \in \mathbb{N}_0^{2 \times 2}$ )
2:    $Y_{\text{ve}} \leftarrow \text{VIRTUALECHO2D}(Y_{\cos}, Y_{\sin});$ 
3:    $S_{\text{ve}} \leftarrow \text{FT}(Y_{\text{ve}});$ 
4:    $l_{\text{idx}}, r_{\text{idx}}, l_{\text{idx}}, r_{\text{idx}} \leftarrow R_{\text{interest}}[0, 0], R_{\text{interest}}[0, 1], R_{\text{interest}}[1, 0], R_{\text{interest}}[1, 1];$ 
5:   for  $d = 1, 2$  do
6:      $c_{\text{idx}}^{(d)} \leftarrow (l_{\text{idx}}^{(d)} + r_{\text{idx}}^{(d)})/2;$ 
7:      $b_{\text{idx}}^{(d)} \leftarrow r_{\text{idx}}^{(d)} - l_{\text{idx}}^{(d)};$ 
8:      $g^{(d)} \leftarrow \text{SUPERGAUSSIAN1D}\left(2N^{(d)}, c_{\text{idx}}^{(d)}, b_{\text{idx}}^{(d)}\right);$ 
9:      $G \leftarrow g^{(1)} \otimes g^{(2)};$ 
10:    end for
11:     $l_{\text{idx}, \text{noise}}, r_{\text{idx}, \text{noise}}, l_{\text{idx}, \text{noise}}, r_{\text{idx}, \text{noise}} \leftarrow R_{\text{noise}}[0, 0], R_{\text{noise}}[0, 1], R_{\text{noise}}[1, 0], R_{\text{noise}}[1, 1];$ 
12:     $S_{\text{noise}} \leftarrow S_{\text{ve}} \left[ l_{\text{idx}, \text{noise}}^{(1)} : r_{\text{idx}, \text{noise}}^{(1)} + 1, l_{\text{idx}, \text{noise}}^{(2)} : r_{\text{idx}, \text{noise}}^{(2)} + 1 \right]$ 
13:     $\sigma^2 \leftarrow \text{Var}(S_{\text{noise}});$ 
14:     $W_{\sigma^2} \leftarrow \mathbf{0} \in \mathbb{R}^{2N^{(1)} \times 2N^{(2)}};$ 
15:    for  $n^{(1)} = 0, \dots, 2N^{(1)} - 1$  do
16:      for  $n^{(2)} = 0, \dots, 2N^{(2)} - 1$  do
17:         $W_{\sigma^2} \left[ n^{(1)}, n^{(2)} \right] \leftarrow \text{RANDOMSAMPLE}(\mathcal{N}(0, \sigma^2));$ 
18:      end for
19:    end for
20:     $\tilde{S}_{\text{ve}} \leftarrow S_{\text{ve}} \odot G + W_{\sigma^2} \odot (\mathbf{1} - G);$ 
21:     $\tilde{Y}_{\text{ve}} \leftarrow \text{IFT}(\tilde{S}_{\text{ve}});$ 
22:     $\tilde{Y} \leftarrow \tilde{Y}_{\text{ve}} \left[ :, N^{(1)}, :, N^{(2)} \right];$ 
23:    return  $\tilde{Y};$ 
24: end procedure

25: procedure VIRTUALECHO2D( $Y_{\cos} \in \mathbb{C}^{N^{(1)} \times N^{(2)}}, Y_{\sin} \in \mathbb{C}^{N^{(1)} \times N^{(2)}}$ )
26:    $\Psi_{++} \leftarrow \Re(Y_{\cos}) - \Im(Y_{\sin}) + i(\Im(Y_{\cos}) + \Re(Y_{\sin}));$ 
27:    $\Psi_{+-} \leftarrow \Re(Y_{\cos}) + \Im(Y_{\sin}) + i(\Re(Y_{\sin}) - \Im(Y_{\cos}));$ 
28:    $\Psi_{-+} \leftarrow \Re(Y_{\cos}) + \Im(Y_{\sin}) + i(\Im(Y_{\cos}) - \Re(Y_{\sin}));$ 
29:    $\Psi_{--} \leftarrow \Re(Y_{\cos}) - \Im(Y_{\sin}) - i(\Im(Y_{\cos}) + \Re(Y_{\sin}));$ 
30:    $Z \leftarrow \mathbf{0} \in \mathbb{C}^{N^{(1)} \times N^{(2)}}$ 
31:    $T_1 \leftarrow \begin{bmatrix} \Psi_{++} & Z \\ Z & Z \end{bmatrix};$ 
32:    $T_2 \leftarrow \begin{bmatrix} Z & \Psi_{+-}^{*(2)} \\ Z & Z \end{bmatrix}^{\circlearrowleft (2)};$ 
33:    $T_3 \leftarrow \begin{bmatrix} Z & Z \\ \Psi_{-+}^{*(1)} & Z \end{bmatrix}^{\circlearrowleft (1)};$ 
34:    $T_4 \leftarrow \begin{bmatrix} Z & Z \\ Z & \Psi_{--}^{*(1,2)} \end{bmatrix}^{\circlearrowleft (1,2)};$ 
35:    $Y_{\text{ve}} \leftarrow T_1 + T_2 + T_3 + T_4;$ 
36:   for  $n^{(1)} = 0, \dots, 2N^{(1)} - 1$  do
37:      $Y_{\text{ve}} \left[ n^{(1)}, 0 \right] \leftarrow Y_{\text{ve}} \left[ n^{(1)}, 0 \right]/2;$ 
38:   end for
39:   for  $n^{(2)} = 0, \dots, 2N^{(2)} - 1$  do
40:      $Y_{\text{ve}} \left[ 0, n^{(2)} \right] \leftarrow Y_{\text{ve}} \left[ 0, n^{(2)} \right]/2;$ 
41:   end for
42:   return  $Y_{\text{ve}};$ 
43: end procedure

```

---

---

**Algorithm B.4** Filtering procedure for 2DJ data.

---

```

1: procedure FILTER2DJ(  $Y \in \mathbb{C}^{N^{(1)} \times N^{(2)}}$ ,  $\mathbf{r}_{\text{interest}} \in \mathbb{N}_0^2$ ,  $\mathbf{r}_{\text{noise}} \in \mathbb{N}_0^2$  )
2:    $Y_{\text{ve}} \leftarrow \mathbf{0} \in \mathbb{C}^{N^{(1)} \times 2N^{(2)}}$ ;
3:   for  $n^{(1)} = 0, \dots, N^{(1)} - 1$  do
4:      $Y_{\text{ve}} \left[ n^{(1)}, : \right] \leftarrow \text{VIRTUALECHO1D} \left( Y \left[ n^{(1)}, : \right] \right)$ ;
5:   end for
6:    $S_{\text{ve}} \leftarrow \text{FT}^{(2)} \left( Y_{\text{ve}} \right)$ ;
7:    $l_{\text{idx}}, r_{\text{idx}}^{(2)} \leftarrow \mathbf{r}_{\text{interest}}[0], \mathbf{r}_{\text{interest}}[1]$ ;
8:    $l_{\text{idx},\text{noise}}, r_{\text{idx},\text{noise}}^{(2)} \leftarrow \mathbf{r}_{\text{noise}}[0], \mathbf{r}_{\text{noise}}[1]$ ;
9:    $c_{\text{idx}}^{(2)} \leftarrow \left( l_{\text{idx}}^{(2)} + r_{\text{idx}}^{(2)} \right) / 2$ ;
10:   $b_{\text{idx}}^{(2)} \leftarrow r_{\text{idx}}^{(2)} - l_{\text{idx}}^{(2)}$ ;
11:   $\mathbf{g}^{(1)} \leftarrow \mathbf{1} \in \mathbb{R}^{N^{(1)}}$ ;
12:   $\mathbf{g}^{(2)} \leftarrow \text{SUPERGAUSSIAN1D} \left( N^{(2)}, c_{\text{idx}}^{(2)}, b_{\text{idx}}^{(2)} \right)$ ;
13:   $G \leftarrow \mathbf{g}^{(1)} \otimes \mathbf{g}^{(2)}$ ;
14:   $S_{\text{noise}} \leftarrow S_{\text{ve}} \left[ :, l_{\text{idx},\text{noise}}^{(2)} : r_{\text{idx},\text{noise}}^{(2)} + 1 \right]$ ;
15:   $\sigma^2 \leftarrow \text{Var} \left( S_{\text{noise}} \right)$ ;
16:   $\mathbf{W}_{\sigma^2} \leftarrow \mathbf{0} \in \mathbb{R}^{N^{(1)} \times 2N^{(2)}}$ ;
17:  for  $n^{(1)} = 0, \dots, N^{(1)} - 1$  do
18:    for  $n^{(2)} = 0, \dots, 2N^{(2)} - 1$  do
19:       $\mathbf{W}_{\sigma^2} \left[ n^{(1)}, n^{(2)} \right] \leftarrow \text{RANDOMSAMPLE} \left( \mathcal{N} \left( 0, \sigma^2 \right) \right)$ ;
20:    end for
21:  end for
22:   $\tilde{S}_{\text{ve}} \leftarrow S_{\text{ve}} \odot G + \mathbf{W}_{\sigma^2} \odot (1 - G)$ ;
23:   $\tilde{Y}_{\text{ve}} \leftarrow \text{IFT}^{(2)} \left( \tilde{S}_{\text{ve}} \right)$ ;
24:   $\tilde{Y} \leftarrow \tilde{Y}_{\text{ve}} \left[ :, : N^{(2)} \right]$ ;
25:  return  $\tilde{Y}$ ;
26: end procedure

```

---



# Python Listings

C

Presented here are a number of PYTHON implementations for the routines described in this text. These can be thought of bare-bones versions of functions present in NMR-EsPy package. These listings require PYTHON version 3.8 or higher, and also require the numpy and scipy packages to be installed from the PYTHON Package Index.

---

**Code Listing C.1:** Required imports for the subsequent listings in this chapter. The product function is employed in the MMEMPM routine (Code Listing C.4). The imports from the typing module are used to annotate what the expected types are for each argument, and what the return type is. The numpy and scipy modules are ubiquitous in the listings, providing access to efficient routines for numerical computations.

```
1 from itertools import product
2 from typing import Any, Iterable, Optional, Tuple, Union
3 import numpy as np
4 import scipy as sp
```

---

## C.1 Matrix pencil methods

### C.1.1 MDL

---

**Code Listing C.2:** The MDL for estimation of the model order of a 1D FID. The first relative minimum in `mdl_vec` is determined to be the estimate of  $M$ , rather than the global minimum (Line ??), since the presence of very small singular values when  $k$  is large can lead to errors involving floating-point arithmetic.

```
1 def mdl(sigma: np.ndarray, N: int, L: int) -> int:
2     """Compute the Minimum Description Length
3
4     Parameters
```

```

5      -----
6      sigma
7          Vector of singular values associated with the data matrix.
8
9      N
10         Number of points the signal comprises.
11
12     L
13         Pencil parameter.
14 """
15     mdl_vec = np.zeros(L)
16     for k in range(L):
17         mdl_vec[k] = (
18             -N * np.sum(np.log(sigma[k:])) +
19             N * (L - k) * np.log(np.sum(sigma[k:])) / (L - k)) +
20             k * np.log(N) * (2 * L - k) / 2
21     )
22     M = sp.signal.argrelextrema(mdl_vec, np.less)[0][0]
23     ↵ !\label{ln:argmin}!
24     return M

```

### C.1.2 MPM

**Code Listing C.3:** The MPM for estimation of a 1D FID, with the option of estimating the model order using the MDL.

```

1 def mpm(Y: np.ndarray, sw: float, offset: float, M: int = 0) -> np.array:
2     """Matrix Pencil Method for estimating a 1D FID.
3
4     Parameters
5     -----
6     Y
7         FID.
8
9     sw
10        Sweep width (Hz).
11
12    offset
13        Transmitter offset (Hz).
14
15    M
16        Number of oscillators. If 0, this is estimated using the MDL.
17 """
18    N = Y # N(1)
19    L = N // 3 # L(1): pencil parameter

```

```

20     norm = np.linalg.norm(Y) #  $\|Y\|$ 
21     Y /= norm #  $Y/\|Y\|$ 
22     col = Y[: N - L] # First column of  $H_Y$ 
23     row = Y[N - L - 1 :] # Last row of  $H_Y$ 
24     HY = sp.linalg.hankel(col, row) #  $H_Y$ 
25     _, S, Vh = np.linalg.svd(HY) #  $\sigma$  and  $V^\dagger$ 
26     V = Vh.T #  $V$ 
27
28     if M == 0:
29         M = mdl(sigma, N, L)
30
31     VM = V[:, :M] #  $V_M$ 
32     VM1 = Vm[:-1, :] #  $V_{M1}$ 
33     VM2 = Vm[1:, :] #  $V_{M2}$ 
34     VM1inv = np.linalg.pinv(VM1) #  $V_{M1}^+$ 
35     VM1invVM2 = VM1inv @ VM2 #  $V_{M1}^+ V_{M2}$ 
36     z, _ = np.linalg.eig(VM1invVM2) #  $z^{(1)}$ : signal poles
37     Z = np.power.outer(z, np.arange(N)).T #  $Z^{(1)}$ 
38     alpha = np.linalg.pinv(Z) @ Y #  $\alpha$ : complex amplitudes
39
40     # Extract amplitude, phase, frequency and damping factor
41     amp = np.abs(alpha) * norm #  $\alpha$ 
42     phase = np.arctan2(np.imag(alpha), np.real(alpha)) #  $\phi$ 
43     freq = (sw / (2 * np.pi)) * np.imag(np.log(z)) + offset #  $f^{(1)}$ 
44     damp = -sw * np.real(np.log(z)) #  $\gamma^{(1)}$ 
45     theta = np.vstack((amp, phase, freq, damp)).T #  $\theta$ , as a  $M \times 4$  array
46
47     # Remove negative damping factors
48     neg_damp_idx = np.nonzero(damp < 0.)[0]
49     theta = np.delete(theta, neg_damp_idx, axis=0)
50
51     theta = theta[np.argsort(theta[:, 2])] # order by  $f^{(1)}$ 
52     return theta

```

### C.1.3 MMEMPM

**Code Listing C.4:** The MMEMPM for estimation of a 2D hypercomplex FID. Due to the very large size of the Hankel matrix  $E_Y$ , a truncated SVD routine is employed, which determines only the first  $M$  components of the decomposition. This is only available to arrays stored in sparse form in SciPy (Lines 65–67).

```

1 def mmempm(
2     Y: np.ndarray, sw1: float, sw2: float,
3     offset1: float, offset2: float, M: int = 0,
4 ) -> np.ndarray:

```

```

5      """Modified Matrix Enhancement Matrix Pencil Method for estimating a
6      2D FID.
7
8      Parameters
9      -----
10     Y
11         FID.
12
13     sw1
14         Sweep width in first (indirect) dimension (Hz).
15
16     sw2
17         Sweep width in second (direct) dimension (Hz).
18
19     offset1
20         Transmitter offset in first dimension (Hz).
21
22     offset2
23         Transmitter offset in second dimension (Hz).
24
25     M
26         Number of oscillators. If 0, this is estimated by applying the MDL
27         to the first direct dimension FID (i.e. Y[0])
28 """
29 N1, N2 = Y.shape # N(1),N(2)
30 L1, L2 = N1 // 2, N2 // 2 # L(1),L(2): pencil parameters
31 norm = np.linalg.norm(Y) # ||Y||
32 Y /= norm # Y/||Y||
33
34 if M == 0:
35     # Extract first direct dimension signal, and estimate model order
36     # with the MDL
37     L_mdl = N2 // 3
38     Y_mdl = Y[0]
39     col_mdl = Y_mdl[: N2 - L_mdl]
40     row_mdl = Y_mdl[N2 - L_mdl - 1 :]
41     HY_mdl = sp.linalg.hankel(col_mdl, row_mdl)
42     _, sigma_mdl, _ = np.linalg.svd(HY_mdl)
43     M = mdl(sigma_mdl, N2, L_mdl)
44
45     # === Construct block Hankel EY ===
46     row_size = L2
47     col_size = N2 - L2 + 1
48     EY = np.zeros(
49         (L1 * L2, (N1 - L1 + 1) * (N2 - L2 + 1)),

```

```

50         dtype="complex",
51     )
52     for n1 in range(N1):
53         # Construct  $H_{Y,n^{(1)}}$ , and assign to appropriate positions in  $E_Y$ 
54         col = Y[n1, :L2]
55         row = Y[n1, L2 - 1:]
56         HYn1 = sp.linalg.hankel(col, row)
57         for n in range(n1 + 1):
58             r, c = n, n1 - n
59             if r < L1 and c < N1 - L1 + 1:
60                 EY[
61                     r * row_size : (r + 1) * row_size,
62                     c * col_size : (c + 1) * col_size
63                 ] = HYn1  #
64
65 EY = sp.sparse.csr_matrix(EY) # Make  $E_Y$  sparse
66
67 UM, *_ = sp.sparse.linalg.svds(EY, k=M) #  $U_M$ 
68 UM1 = UM[:, L1 * (L2 - 1):] # Last  $L^{(2)}$  rows deleted:  $U_{M1}$ 
69 UM2 = UM[L2:] # First  $L^{(2)}$  rows deleted:  $U_{M2}$ 
70 z1, W1 = np.linalg.eig(np.linalg.pinv(UM1) @ UM2) #  $z^{(1)}$ ,  $W^{(1)}$ 
71
72 # === Construct permutation matrix  $P$  ===
73 P = np.zeros((L1 * L2, L1 * L2))
74 r = 0
75 for l2 in range(L2):
76     for l1 in range(L1):
77         c = l1 * L2 + l2
78         P[r, c] = 1
79         r += 1
80
81 UMP = P @ UM #  $U_{MP}$ 
82 UMP1 = UMP[:, (L1 - 1) * L2:] # Last  $L^{(1)}$  rows deleted:  $U_{MP1}$ 
83 UMP2 = UMP[L1:] # First  $L^{(1)}$  rows deleted:  $U_{MP2}$ 
84 G = np.linalg.inv(W1) @ np.linalg.pinv(UMP1) @ UMP2 @ W1 #  $G$ 
85 z2 = np.diag(G).copy() #  $z^{(2)}$ : copy needed as slice is readonly
86
87 # === Check for and deal with similar frequencies in  $f^{(1)}$  ===
88 freq1 = (0.5 * sw1 / np.pi) * np.imag(np.log(z1)) + offset1 #  $f^{(1)}$ 
89 threshold = sw1 / N1 #  $f_{sw}^{(1)}/N^{(1)}$ 
90 groupings = []
91 # Iterate through values in  $f^{(1)}$  and group any with
92 # similar frequencies together
93 for idx, f1 in enumerate(freq1):
94     assigned = False

```

```

95      for group_f1, indices in groupings.items():
96          if np.abs(f1 - group_f1) < threshold:
97              indices.append(idx)
98              n = len(indices)
99              indices = sorted(indices)
100             # Get new mean freq of the group
101             new_group_f1 = (n * group_f1 + f1) / (n + 1)
102             groupings[new_group_f1] = groupings.pop(group_f1)
103             assigned = True
104             break
105         if not assigned:
106             groupings[f1] = [idx]
107
108     for indices in groupings.values():
109         n = len(indices)
110         if n != 1:
111             Gr_slice = tuple(zip(*product(indices, repeat=2)))
112             Gr = G[Gr_slice].reshape(n, n)
113             new_group_z2, _ = np.linalg.eig(Gr)
114             z2[indices] = new_group_z2  #
115
116     # === Construct  $E_L$  and  $E_R$  ===
117     ZL2 = np.power.outer(z2, np.arange(L2)).T  #  $Z_L^{(2)}$ 
118     ZR2 = np.power.outer(z2, np.arange(N2 - L2 + 1))  #  $Z_R^{(2)}$ 
119     Z1D = np.diag(z1)  #  $Z_D^{(1)}$ 
120
121     EL = np.zeros((L1 * L2, M), dtype="complex")
122     Z2LZ1D = ZL2
123     for i in range(L1):
124         EL[i * row_size : (i + 1) * row_size] = Z2LZ1D
125         Z2LZ1D = Z2LZ1D @ Z1D
126     ER = np.zeros((M, (N1 - L1 + 1) * (N2 - L2 + 1)), dtype="complex")
127     Z1DZ2R = ZR2
128     for i in range(N1 - L1 + 1):
129         ER[:, i * col_size : (i + 1) * col_size] = Z1DZ2R
130         Z1DZ2R = Z1D @ Z1DZ2R
131     #  $\alpha = \text{diag}(E_L^+ E_Y E_R^+)$ 
132     alpha = np.diag(np.linalg.pinv(EL) @ EY @ np.linalg.pinv(ER))  #
133
134     amp = np.abs(alpha) * norm  #  $\alpha$ 
135     phase = np.arctan2(np.imag(alpha), np.real(alpha))  #  $\phi$ 
136     freq2 = (0.5 * sw2 / np.pi) * np.imag(np.log(z2)) + offset2  #  $f^{(2)}$ 
137     damp1 = -sw1 * np.real(np.log(z1))  #  $\eta^{(1)}$ 
138     damp2 = -sw2 * np.real(np.log(z2))  #  $\eta^{(2)}$ 
139     #  $\theta$ , as a  $M \times 6$  array

```

---

```

140     theta = np.vstack((amp, phase, freq1, freq2, damp1, damp2)).T
141
142     # Remove negative damping factors
143     neg_damp_idx1 = list(np.nonzero(damp1 < 0. )[0])
144     neg_damp_idx2 = list(np.nonzero(damp2 < 0. )[0])
145     neg_damp_idx = list(set(neg_damp_idx1 + neg_damp_idx2))
146     theta = np.delete(theta, neg_damp_idx, axis=0)
147
148     theta = theta[np.argsort(theta[:, 3])] # order by  $f^{(2)}$ 
149     return theta

```

---

## C.2 NLP

### C.2.1 Trust Region Algorithm

---

**Code Listing C.5:** Steihaug-Toint trust region algorithm. Included is a check for oscillators with negative amplitudes, which causes the routine to terminate, in order for said oscillators to be purged (Lines ??–??).

---

```

1 def trust_steihaug_toint(
2     theta0: np.ndarray,
3     function_factory: FunctionFactory,
4     args: Iterable[Any] = (),
5 ) -> Tuple[np.ndarray, np.ndarray, bool]:
6     """Trust Region algorithm with Steihaug-Toint subroutine.
7
8     Parameters
9     -----
10    theta0
11        Initial guess, with shape (M, 4).
12
13    function_factory
14        Object for computing the objective, gradient and Hessian.
15
16    args
17        Extra arguments required for computing the objective and its
18        derivatives.
19
20    Returns
21    -----
22    theta
23        Parameter vector at termination.
24
25    errors

```

```
26     Errors associated with parameter vector.
27
28     negative_amps
29         Flag indicating whether or not termination occurred because
30         negative amplitudes were detected.
31     """
32     theta = theta0
33     M = theta.shape[0] // 4
34     factory = function_factory(theta, *args)
35
36     # === Define relevant parameters ===
37     # These have been hard-coded, though in NMR-EsPy they are all
38     # configurable.
39     eta = 0.15,
40     initial_trust_radius = 0.1 * factory.gradient_norm
41     max_trust_radius = 16 * initial_trust_radius
42     epsilon: float = 1.e-8,
43     max_iterations: int = 200,
44     check_neg_amps_every: int = 25,
45
46     k = 0
47     while True:
48         # === Steihaug-Toint ===
49         epsi = min(0.5, np.sqrt(factory.gradient_norm)) *
50             ~ factory.gradient_norm
50         z = np.zeros_like(theta)
51         r = factory.gradient
52         d = -r
53         while True:
54             Bd = factory.hessian @ d
55             dBd = d.T @ Bd
56             if dBd <= 0:
57                 ta, tb = get_boundaries(z, d, trust_radius)
58                 pa = z + ta * d
59                 pb = z + tb * d
60                 p = min(factory.model(pa), factory.model(pb))
61                 hits_boundary = True
62                 break
63             r_sq = r.T @ r
64             alpha = r_sq / dBd
65             z_next = z + alpha * d
66             if sp.linalg.norm(z_next) >= trust_radius:
67                 _, tb = get_boundaries(z, d, trust_radius)
68                 p = z + tb * d
69                 hits_boundary = True
```

```

70           break
71       r_next = r + alpha * Bd
72       r_next_sq = r_next.T @ r_next
73       if np.sqrt(r_next_sq) < epsi:
74           hits_boundary = False
75       p = z_next
76       break
77   beta_next = r_next_sq / r_sq
78   d_next = -r_next + beta_next * d
79   z = z_next
80   r = r_next
81   d = d_next
82
83 # === Assess effectiveness of update ===
84 predicted_value = factory.model(p)
85 theta_proposed = theta + p
86 factory_proposed = function_factory(theta_proposed, *args)
87 actual_reduction = factory.objective - factory_proposed.objective
88 predicted_reduction = factory.objective - predicted_value
89 if predicted_reduction <= 0:
90     # No improvement could be found: terminate
91     negative_amps = False
92     break
93 rho = actual_reduction / predicted_reduction
94 if rho < 0.25:
95     # Quadratic model performing poorly: reduce TR
96     trust_radius *= 0.25
97 elif rho > 0.75 and hits_boundary:
98     # Quadratic model performing well: increase TR
99     trust_radius = min(2 * trust_radius, max_trust_radius)
100 if rho > eta:
101     # Accept update: new iteration
102     theta = theta_proposed
103     factory = factory_proposed
104     k += 1
105
106 # === Check for termination criteria ===
107 if (k % check_neg_amps_every == 0): !\label{ln:negamp1}!
108     neg_amps = np.where(theta[amp_slice] <= 0)[0]
109     print(neg_amps)
110 if neg_amps.size > 0:
111     # Negative amps found: this run in order to purge
112     negative_amps = True
113     break !\label{ln:negamp2}!
114

```

```
115     if factory.gradient_norm < epsilon:
116         # Convergence
117         negative_amps = False
118         break
119
120     if k == max_iterations:
121         # Maximum allowed iterations reached
122         negative_amps = False
123         break
124
125     # Routine terminated: compute errors and return parameter array
126     errors = np.sqrt(
127         factory.objective *
128         np.abs(np.diag(np.linalg.inv(factory.hessian)))
129     )
130     return theta, errors, negative_amps
131
132
133 def get_boundaries(
134     z: np.ndarray, d: np.ndarray, trust_radius: float
135 ) -> Tuple[float, float]:
136     """Determine the intersections of the search direction and the trust
137     region."""
138     a = d.T @ d
139     b = 2 * z.T @ d
140     c = (z.T @ z) - (trust_radius ** 2)
141     aux = b + np.copysign(
142         np.sqrt(b * b - 4 * a * c),
143         b,
144     )
145     return sorted([-aux / (2 * a), -(2 * c) / aux])
```

### C.2.2 Computing $\mathcal{F}_\phi$ , $\nabla \mathcal{F}_\phi$ , and $\nabla^2 \mathcal{F}_\phi$

---

**Code Listing C.6:** Code for the generation of the fidelity for NLP applied to 1D estimation, as well as the gradient and Hessian. The `FunctionFactory` object accepts a parameter set (`theta`) and function (`fun`), which computes the objective, gradient and Hessian. The first time a quantity is requested from the factory, the function is run, and the objective and its derivatives are cached (`memoised`), such that the next time a quantity is requested, the cached result is used, rather than the expensive function being re-computed. `FunctionFactory1D` (Lines ??–??) inherits from the base class, for specific use in 1D estimation, with an approximated Hessian. For the equivalent code for both 2D estimation, and for computing the exact Hessian, the reader is directed to `nmrsp/nlp/_funcs.py` in the NMR-EsPy package.

```

1 class FunctionFactory:
2     """Object which computes and memoises the objective, gradient and
3     hessian for a given set of parameters."""
4     def __init__(self, theta: np.ndarray, fun: callable, *args) -> None:
5         self.theta = theta
6         self._new_theta = True
7         self.fun = fun
8         self.obj = None
9         self.grad = None
10        self.hess = None
11        self.args = args
12
13    def _compute_if_needed(self):
14        """Compute the obj, grad and Hess if they haven't been yet"""
15        if self.obj is None:
16            self.obj, self.grad, self.hess = self.fun(self.theta,
17                *self.args)
18
19    def model(self, p) -> float:
20        return self.objective + self.gradient @ p + 0.5 * (p.T @
21            self.hessian @ p)
22
23    @property
24    def objective(self) -> float:
25        self._compute_if_needed()
26        return self.obj
27
28    @property
29    def gradient(self) -> np.ndarray:
30        self._compute_if_needed()
31        return self.grad
32
33    @property
34    def gradient_norm(self) -> float:

```

```

33         return sp.linalg.norm(self.gradient)
34
35     @property
36     def hessian(self) -> np.ndarray:
37         self._compute_if_needed()
38         return self.hess
39
40
41 class FunctionFactory1D(FunctionFactory): !label{ln:ff1}!
42     def __init__(self, theta: np.ndarray, *args) -> None:
43         super().__init__(theta, obj_grad_hess_1d, *args) !label{ln:ff2}!
44
45
46     def obj_grad_hess_1d( #
47         theta: np.ndarray, *args: Tuple[int, int, np.ndarray],
48     ) -> Tuple[float, np.ndarray, np.ndarray]:
49         Y, tp = args # Unpack args: FID, timepoints
50         N = Y.shape[0]
51         M = theta.shape[0] // 4
52         X_per_osc = np.exp(
53             np.outer(tp, (2j * np.pi * theta[2 * M : 3 * M] - theta[3 * M :]))
54         ) * (theta[:M] * np.exp(1j * theta[M : 2 * M]))
55
56         # === First partial derivatives ===
57         d1 = np.zeros((N, 4 * M), dtype="complex")
58         d1[:, :M] = X_per_osc / theta[:M] #  $\partial x / \partial \alpha_m$ 
59         d1[:, M : 2 * M] = 1j * X_per_osc #  $\partial x / \partial \phi_m$ 
60         d1[:, 2 * M : 3 * M] = \ #  $\partial x / \partial f_m$ 
61             np.einsum("ij,i->ij", X_per_osc, 2j * np.pi * tp)
62         d1[:, 3 * M :] = np.einsum("ij,i->ij", X_per_osc, -tp) #  $\partial x / \partial \eta_m$ 
63
64         # === Second partial derivatives ===
65         d2 = np.zeros((N, 10 * M), dtype="complex")
66         # Note  $\partial^2 x / \partial \alpha_m^2 = 0$  always.
67         d2[:, M : 2 * M] = 1j * d1[:, M : 2 * M] #  $\partial^2 x / \partial \phi_m^2$ 
68         d2[:, 2 * M : 3 * M] = \ #  $\partial^2 x / \partial f_m^2$ 
69             np.einsum("ij,i->ij", d1[:, 2 * M : 3 * M], 2j * np.pi * tp)
70         d2[:, 3 * M : 4 * M] = np.einsum("ij,i->ij", d2[:, 3 * M :], -tp) #
71              $\partial^2 x / \partial \eta_m^2$ 
72         d2[:, 4 * M : 5 * M] = 1j * d1[:, :M] #  $\partial^2 x / \partial \alpha_m \partial \phi_m$ 
73         d2[:, 5 * M : 6 * M] = 1j * d1[:, 2 * M : 3 * M] #  $\partial^2 x / \partial \phi_m \partial f_m$ 
74         d2[:, 6 * M : 7 * M] = \ #  $\partial^2 x / \partial f_m \partial \eta_m$ 
75             np.einsum("ij,i->ij", d2[:, 2 * M : 3 * M], -tp)
76         d2[:, 7 * M : 8 * M] = d1[:, 2 * M : 3 * M] / theta[:M] #  $\partial^2 x / \partial \alpha_m \partial f_m$ 
77         d2[:, 8 * M : 9 * M] = 1j * d1[:, 3 * M : 4 * M] #  $\partial^2 x / \partial \phi_m \partial \eta_m$ 

```

```

77     d2[:, 9 * M :] = d1[:, 3 * M : 4 * M] / theta[:M] #  $\partial^2 x / \partial \alpha_m \partial \gamma_m$ 
78
79     X = np.einsum("ij->i", X_per_osc)
80     Y_minus_X = Y - X
81
82     # === Objective ===
83     obj = np.real(Y_minus_X.conj().T @ Y_minus_X)
84
85     # === Gradient ===
86     grad = -2 * np.real(Y_minus_X.conj().T @ d1)
87
88     # === Hessian ===
89     hess = np.zeros((4 * M, 4 * M))
90     # Compute non-zero elements of term ② of the Hessian,
91     # and assign to upper right triangle.
92     hess_term_2 = -2 * np.real(np.einsum("ji,j->i", d2.conj(), Y_minus_X))
93     term_2_row_idxs = []
94     term_2_col_idxs = []
95     for i in range(4):
96         rows, cols = _diag_idx(4 * M, i * M)
97         term_2_row_idxs.extend(rows)
98         term_2_col_idxs.extend(cols)
99     term_2_idxs = (term_2_row_idxs, term_2_col_idxs)
100    hess[term_2_idxs] = hess_term_2
101    # Add the transpose to fill left bottom triangle
102    # Halve the main diagonal before transposing to avoid doubling
103    main_diag = _diag_idx(4 * M, 0)
104    hess[main_diag] *= 0.5
105    hess += hess.T
106    # Compute term ① of the Hessian
107    hess_term_1 = 2 * np.real(np.einsum("ki,kj->ij", d1.conj(), d1))
108    hess += hess_term_1
109
110    # === Phase variance and derivatives ===
111    phi = theta[M : 2 * M]
112    cos_phi = np.cos(phi)
113    cos_sum = np.sum(cos_phi)
114    sin_phi = np.sin(phi)
115    sin_sum = np.sum(sin_phi)
116    R = np.sqrt(cos_sum ** 2 + sin_sum ** 2)
117    pv_obj = 1 - (R / M)
118    pv_grad = (sin_phi * cos_sum - cos_phi * sin_sum) / (M * R)
119    x = (sin_phi * cos_sum) - (cos_phi * sin_sum)
120    term_1 = np.outer(x, x) / (R ** 2)
121    phi_array = np.zeros((M, M))

```

```
122     phi_array[:] = phi
123     term_2 = -np.cos(phi_array.T - phi_array)
124     pv_hess = term_1 + term_2
125     pv_hess[np.diag_indices(M)] += cos_phi * cos_sum + sin_phi * sin_sum
126     pv_hess /= M * R
127     obj += pv_obj #  $\mathcal{F}_\phi(\theta)$ 
128     grad[M : 2 * M] += pv_grad #  $\nabla \mathcal{F}_\phi(\theta)$ 
129     hess[M : 2 * M, M : 2 * M] += pv_hess #  $\nabla^2 \mathcal{F}_\phi(\theta)$ 
130
131     return obj, grad, hess #
132
133
134 def _diag_idx(size: int, disp: int) -> Tuple[np.ndarray, np.ndarray]:
135     """Return the indices of an array's kth diagonal.
136
137     Parameters
138     -----
139     size
140         The size of the square matrix.
141
142     disp
143         Displacement from the main diagonal.
144
145     Returns
146     -----
147     rows
148         0-axis coordinates of indices.
149
150     cols
151         1-axis coordinates of indices.
152     """
153     rows, cols = np.diag_indices(size)
154     if disp < 0:
155         return rows[-disp:], cols[:disp]
156     elif disp > 0:
157         return rows[:-disp], cols[disp:]
158     else:
159         return rows, cols
```

---

### C.2.3 The main routine

---

**Code Listing C.7:** Code for running the NLP routine for FID estimation. The routine consists of running the ST algorithm (Code Listing C.5) until it returns a parameter array without negative amplitudes. If negative amplitudes are present, the corresponding oscillators are removed, and the ST algorithm is re-run.

```

1 def nlp(
2     Y: np.ndarray,
3     sw: float,
4     offset: float,
5     theta0: np.ndarray,
6 ) -> Tuple[np.ndarray, np.ndarray]:
7     """Nonlinear programming routine for 1D FID estimation.
8
9     Parameters
10    -----
11    Y
12        FID.
13
14    sw
15        Sweep width (Hz).
16
17    offset
18        Transmitter offset (Hz).
19
20    theta0
21        Initial guess, of shape (M, 4)
22
23    Returns
24    -----
25    theta
26        Parameter estimate.
27
28    errors
29        Errors associated with theta.
30    """
31    norm = np.linalg.norm(Y)
32    Y /= norm
33    N = Y.shape[0]
34    M = theta0.shape[0]
35    # Flatten parameter array: Fortran (column-wise) ordering
36    theta0_vec = theta0.flatten(order="F")
37    theta0_vec[:M] /= norm # Normalise amplitudes
38    # Remove transmitter offset from frequencies

```

```
39     theta0_vec[2 * M : 3 * M] -= offset
40
41     # Extra arguments needed to compute the objective, grad, and Hessian:
42     # FID and timepoints sampled
43     opt_args = [Y, np.linspace(0, float(N - 1) / sw, N)]
44
45     while True:
46         theta_vec, errors_vec, negative_amps = trust_ncg(
47             theta0=theta0_vec,
48             function_factory=FunctionFactoryGaussNewton1D,
49             args=opt_args,
50         )
51
52     if negative_amps:
53         # Negative amps exist: remove these
54         negative_idx = list(np.where(theta_vec[:M] <= 0.0)[0])
55         slice_ = []
56         for idx in range(negative_idx):
57             slice_.extend([i * M + idx for i in range(4)])
58         theta_vec = np.delete(theta_vec, slice_)
59         M -= len(negative_idx) # New model order
60
61     else:
62         # No negative amps: routine complete
63         break
64
65     # Reshape parameter array back to (M, 4)
66     theta = theta_vec.reshape((M, 4), order="F")
67     errors = errors_vec.reshape((M, 4), order="F")
68     errors_vec /= N - 1
69     theta[:, 2] += offset # Re-add transmitter offset to frequencies
70     theta[:, 0] *= norm # Re-scale amplitudes
71     errors[:, 0] *= norm
72     theta[:, 1] = (theta[:, 1] + np.pi) % (2 * np.pi) - np.pi # Wrap
73         # phases
74
75     return theta, errors
```

---

## C.3 CUPID

**Code Listing C.8:** Code for performing multiplet assignment as part of CUPID.

```

1 def predict_multiplets(
2     params: np.ndarray,
3     thold: float,
4 ) -> Dict[float, Iterable[int]]:
5     """
6         Parameters
7         -----
8         params
9             Estimated parameter array with shape (M, 6) such that each row
10            provides the parameters of a particular oscillator, in the order
11            [a, ϕ, f1, f2, η1, η2].
12
13         thold
14             Frequency threshold  $\varepsilon > 0$ .
15
16         Returns
17         -----
18         A dictionary with the multiplet central frequencies as keys and
19         oscillator indices as values
20         """
21         multiplets = {}
22         for m, osc in enumerate(params):
23             assigned = False
24             f1, f2 = osc[2], osc[3] # Extract  $f^{(1)}$  and  $f^{(2)}$ 
25             fc = osc[3] - osc[2] # Central frequency for oscillator:  $f_m^{(2)} - f_m^{(1)}$ 
26             # Check whether central frequency agrees with any
27             # already-established multiplet grouping
28             for fmp in multiplets:
29                 if fmp - thold < fc < fmp + thold:
30                     # Update grouping:
31                     # Add m to list of oscillators
32                     # Update central frequency: mean of all oscillators
33                     ms = multiplets.pop(fmp)
34                     ms.append(m)
35                     mp_size = len(ms)
36                     new_fmp = ((mp_size - 1) * fmp + fc) / mp_size
37                     multiplets[new_fmp] = ms
38                     assigned = True

```

```
39             break
40         # No match: create new multiplet group
41         if not assigned:
42             multiplets[fc] = [m]
43
44     return multiplets
```

---

# Information on Datasets and Results

D

## D.1 Simulated datasets

### D.1.1 SPINACH Simulations

Many of the simulated datasets presented in this work were generated using the SPINACH MATLAB package[85]. In each case, the dataset was generated via a call to the `new_spinach` method associated with the relevant `Estimator` object in NMR-EsPy. `new_spinach` works by instantiating a MATLAB engine from PYTHON[172], which then runs a SPINACH simulation of the relevant experiment with the specifications provided. The FID generated is then stored within in a new `Estimator` object along with other necessary information about the simulation.

#### Spin Systems

Table D.1 provides a specification of the chemical shifts and scalar couplings that made up the spin systems used to construct simulated data with SPINACH. Below is a description of how the spin systems were generated.

*“Five Multiplets”* The spin systems used to generate the “five multiplets” inversion recovery datasets featured 8 spins, comprising a group of 5 “estimated spins” and a group of 3 “coupling spins”:

- The estimated spins were each assigned chemical shifts randomly sampled from  $\mathcal{U}(-0.1 \text{ ppm}, 0.1 \text{ ppm})$ .
- The coupling spins were assigned chemical shifts  $\gg 0.15 \text{ ppm}$ . Each coupling spin was assigned a non-zero J-coupling to each of the estimated spins, with the couplings randomly sampled from  $\mathcal{U}(-20 \text{ Hz}, 20 \text{ Hz})$ .

As a result, a region of the dataset, centred at 0 ppm, would feature 5 ddd multiplets, which abide

by the weak coupling approximation. A further constraint was applied, to ensure that the  $40 (5 \times 2^3)$  signals generated by the 5 estimated spins would have sufficiently separated frequencies, such that they could feasibly be resolved by estimation. Each of the spins were assigned longitudinal and transverse relaxation times, using the distributions  $T_1 \sim \mathcal{U}(1\text{ s}, 5\text{ s})$ , and  $T_2 \sim \mathcal{U}(0.2\text{ s}, 0.6\text{ s})$ .

*“Four Multiplets”* The “four multiplets” 2DJ datasets were generated using spin systems with a similar form to the “five multiplets” spin systems. Each spin system comprised 7 spins, with 4 estimated and 3 coupling spins. The estimated spins were assigned chemical shifts randomly sampled from  $\mathcal{U}(-0.03\text{ ppm}, 0.03\text{ ppm})$ , while the coupling spins were given shifts which were  $\gg 0.03\text{ ppm}$ . J-couplings between the estimated and coupling spins were sampled from  $\mathcal{U}(-10\text{ Hz}, 10\text{ Hz})$ .

*Strychnine* The strychnine spin system was derived from the SPINACH function <SPINACHROOT>/etc/strychnine.m, which returns a spin system specification using chemical shifts and scalar couplings from [173: Appendix 5].

**Table D.1:** The isotropic chemical shifts ( $\delta$ ), corresponding rotating frame frequencies ( $\omega_0$ ), and scalar couplings ( $J$ ) associated with spin systems used in SPINACH simulations. For the “Five multiplets” spin systems, the associated  $T_1$  times are provided too.

Spin	$\delta$ (ppm)	$\omega_0$ (Hz)	$J$ (Hz)	$T_1$ (s)
<b>Five Multiplets, Run 1</b>				
(A)	$-6.80 \times 10^{-2}$	-34.01	(F): 10.965, (G): 12.657, (H): 17.070	2.178
(B)	$7.09 \times 10^{-2}$	35.44	(F): 3.610, (G): 2.543, (H): 8.448	4.430
(C)	$-9.23 \times 10^{-2}$	-46.13	(F): 10.630, (G): 6.282, (H): 3.012	3.319
(D)	$1.00 \times 10^{-2}$	5.01	(F): 8.101, (G): 4.589, (H): 9.068	1.007
(E)	$-9.95 \times 10^{-2}$	-49.77	(F): 3.014, (G): 16.537, (H): 15.587	4.992
<b>Five Multiplets, Run 2</b>				
(A)	$6.61 \times 10^{-2}$	33.07	(F): 19.488, (G): 18.279, (H): 3.147	3.600
(B)	$-3.75 \times 10^{-2}$	-18.75	(F): 11.924, (G): 8.400, (H): 5.515	3.905
(C)	$-9.68 \times 10^{-2}$	-48.39	(F): 13.672, (G): 6.543, (H): 16.275	4.291
(D)	$2.70 \times 10^{-2}$	13.48	(F): 12.007, (G): 5.141, (H): 9.981	1.687
(E)	$8.91 \times 10^{-2}$	44.53	(F): 8.715, (G): 14.309, (H): 9.805	3.214
<b>Five Multiplets, Run 3</b>				
(A)	$-8.23 \times 10^{-2}$	-41.13	(F): 4.984, (G): 18.119, (H): 10.642	3.846
(B)	$3.90 \times 10^{-2}$	19.50	(F): 13.518, (G): 14.381, (H): 3.074	1.018
(C)	$-3.33 \times 10^{-2}$	-16.66	(F): 8.758, (G): 16.689, (H): 12.956	4.766
(D)	$-4.60 \times 10^{-2}$	-23.02	(F): 17.648, (G): 7.514, (H): 3.918	3.414
(E)	$9.35 \times 10^{-2}$	46.76	(F): 16.396, (G): 7.455, (H): 11.352	1.827

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Spin	$\delta$ (ppm)	$\omega_0$ (Hz)	$J$ (Hz)	$T_1$ (s)
<b>Four Multiplets, Run 1</b>				
(A)	$-2.78 \times 10^{-2}$	-13.93	(E): -9.627, (F): -8.202, (G): 6.742	-
(B)	$-7.11 \times 10^{-3}$	-3.56	(E): -4.491, (F): 5.333, (G): 9.303	-
(C)	$-1.63 \times 10^{-3}$	-0.81	(E): 3.953, (F): 5.422, (G): 5.914	-
(D)	$1.53 \times 10^{-2}$	7.66	(E): -7.902, (F): -4.556, (G): 6.217	-
<b>Four Multiplets, Run 2</b>				
(A)	$-1.48 \times 10^{-2}$	-7.38	(E): -7.492, (F): 0.917, (G): 2.933	-
(B)	$-1.18 \times 10^{-2}$	-5.88	(E): -4.304, (F): -1.815, (G): 5.420	-
(C)	$-4.32 \times 10^{-3}$	-2.16	(E): 4.832, (F): 7.573, (G): 8.268	-
(D)	$1.76 \times 10^{-2}$	8.80	(E): -9.244, (F): -1.816, (G): -0.478	-
<b>Four Multiplets, Run 3</b>				
(A)	$-2.23 \times 10^{-2}$	-11.17	(E): -5.347, (F): -1.851, (G): 1.407	-
(B)	$1.13 \times 10^{-2}$	5.66	(E): 6.425, (F): 7.291, (G): 9.806	-
(C)	$2.53 \times 10^{-2}$	12.64	(E): -8.640, (F): 0.613, (G): 6.998	-
(D)	$2.84 \times 10^{-2}$	14.21	(E): -8.613, (F): 0.782, (G): 3.830	-
<b>Four Multiplets, Run 4</b>				
(A)	$-2.03 \times 10^{-2}$	-10.16	(E): -8.646, (F): 6.719, (G): 7.921	-
(B)	$3.53 \times 10^{-3}$	1.77	(E): -8.857, (F): 4.314, (G): 9.197	-
(C)	$8.61 \times 10^{-3}$	4.30	(E): -0.620, (F): 1.767, (G): 6.567	-
(D)	$2.06 \times 10^{-2}$	10.30	(E): -9.060, (F): 2.355, (G): 9.810	-
<b>Four Multiplets, Run 5</b>				
(A)	$-9.16 \times 10^{-3}$	-4.58	(E): -8.281, (F): 1.621, (G): 3.229	-
(B)	$-2.79 \times 10^{-3}$	-1.40	(E): 1.655, (F): 4.219, (G): 6.998	-
(C)	$3.00 \times 10^{-3}$	1.50	(E): -4.280, (F): 1.045, (G): 5.896	-
(D)	$2.74 \times 10^{-2}$	13.72	(E): -9.316, (F): -8.322, (G): -3.938	-
<b>Strychnine</b>				
(A)	7.167	3583.5	(B): 7.490, (C): 1.080, (D): 0.230	-
(B)	7.098	3549.0	(A): 7.490, (C): 7.440, (D): 0.980	-
(C)	7.255	3627.5	(A): 1.080, (B): 7.440, (D): 7.900	-
(D)	8.092	4046.0	(A): 0.230, (B): 0.980, (C): 7.900	-
(E)	3.860	1930.0	(I): 10.410	-
(F)	3.132	1566.0	(G): -17.340, (H): 3.340	-
(G)	2.670	1335.0	(F): -17.340, (H): 8.470	-
(H)	4.288	2144.0	(F): 3.340, (G): 8.470, (I): 3.300	-

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Spin	$\delta$ (ppm)	$\omega_0$ (Hz)	$J$ (Hz)	$T_1$ (s)
(I)	1.276	638.0	(E): 10.410, (H): 3.300, (J): 3.290	–
(J)	3.150	1575.0	(I): 3.290, (K): 4.110, (L): 1.960, (R): 1.610, (T): 0.470	–
(K)	2.360	1180.0	(J): 4.110, (L): -14.350, (M): 4.330	–
(L)	1.462	731.0	(J): 1.960, (K): -14.350, (M): 2.420	–
(M)	3.963	1981.5	(K): 4.330, (L): 2.420	–
(N)	1.890	945.0	(O): -13.900, (P): 5.500, (Q): 7.200	–
(O)	1.890	945.0	(N): -13.900, (P): 3.200, (Q): 10.700	–
(P)	3.219	1609.5	(N): 5.500, (O): 3.200, (Q): -13.900	–
(Q)	2.878	1439.0	(N): 7.200, (O): 10.700, (P): -13.900	–
(R)	3.716	1858.0	(J): 1.610, (S): -14.800, (T): 1.790	–
(S)	2.745	1372.5	(R): -14.800	–
(T)	5.915	2957.5	(J): 0.470, (R): 1.790, (U): 7.000, (V): 6.100	–
(U)	4.148	2074.0	(T): 7.000, (V): -13.800	–
(V)	4.066	2033.0	(T): 6.100, (U): -13.800	–

### D.1.2 2DJ

The simulated datasets for the “Four multiplets” and Strychnine results in Sections 4.3.1 and 4.3.2 were generated using NMR-EsPy’s `Estimator2DJ.new_spinach` method, with parameters used in the simulation provided by Table D.2.

Parameter	Four Multiplets	Strychnine
$f_{bf}^{(1)}$ (MHz)	500	499.9
$f_{off}^{(2)}$ (Hz)	0	2500
$f_{off}^{(2)}$ (ppm)	0	5.001
$f_{sw}^{(1)}$ (Hz)	40	50
$f_{sw}^{(2)}$ (Hz)	1000	5000
$f_{sw}^{(2)}$ (ppm)	2	10
$N^{(1)}$	128	128
$N^{(2)}$	1024	8192

**Table D.2:** Experiment parameters for 2DJ simulations run using SPINACH.

A 2DJ pulse sequence simulation does not ship with SPINACH. Therefore, an in-house one was written, which is given by Code Listing D.1.

**Code Listing D.1:** Function for simulating 2DJ experiments using SPINACH.

---

```

1 function fid = jres_seq(spin_system, parameters, H, R, K)
2     % Compose Liouvillian
3     L = H + 1i * R + 1i * K; clear('H', 'R', 'K');
4     % Coherent evolution timestep
5     d1 = 1 / parameters.sweep(1);
6     d2 = 1 / parameters.sweep(2);
7     % Number of points
8     pts1 = parameters.npoints(1);
9     pts2 = parameters.npoints(2);
10    % Targeted nucleus
11    nuc = parameters.spins{1}
12    % Initial state
13    rho = state(spin_system, 'Lz', nuc);
14    % Detection state
15    coil = state(spin_system, 'L+', nuc);
16    % Get the pulse operators
17    Lp = operator(spin_system, 'L+', nuc);
18    Lx = (Lp + Lp') / 2;
19    % First pulse: 90 about x
20    rho = step(spin_system, Lx, rho, pi / 2);
21    % First half of t1 evolution
22    rho = evolution(spin_system, L, [], rho, d1 / 2, pts1 - 1,
23    ↵ 'trajectory');
23    % Select "-1" coherence
24    rho = coherence(spin_system, rho, {{nuc, -1}});
25    % Second pulse: 180 about x
26    rho = step(spin_system, Lx, rho, pi);
27    % Select "+1" coherence
28    rho = coherence(spin_system, rho, {{nuc, +1}});
29    % Second half of t1 evolution
30    rho = evolution(spin_system, L, [], rho, d1 / 2, pts1 - 1, 'refocus');
31    % Run the F2 evolution
32    fid = evolution(spin_system, L, coil, rho, d2, pts2 - 1, 'observable');
33 end

```

---

### D.1.3 Inversion recovery

The simulated datasets for the “Five multiplets” results in Section 3.2.4 was generated using NMR-EsPy’s `EsimatorInvRec.new_spinach` method, with parameters used in the simulation provided by Table D.3. To model relaxation, SPINACH’s  $T_1/T_2$  approximation was used[174]. Under this model, all longitudinal states associated with a given spin relax at a rate  $R_1 := 1/T_1$ , while transverse states relax at a rate  $R_2 := 1/T_2$ . For multi-spin order states, the relaxation rate is given by the sum of the appropriate rates. The dataset was produced using SPINACH’s built-in inversion recovery pulse

sequence simulation, found at <SPINACHROOT>/experiments/inv\_rec.m. 21 evenly-spaced increments of  $\tau$  were used; the first increment was 0 s, the last was 4 s, and consecutive increments differed by 0.4 s.

Parameter	Five Multiplets
$f_{\text{bf}}^{(1)}$ (MHz)	500
$f_{\text{off}}^{(1)}$ (Hz)	2500
$f_{\text{off}}^{(1)}$ (ppm)	5
$f_{\text{sw}}^{(1)}$ (Hz)	5000
$f_{\text{sw}}^{(1)}$ (ppm)	10
$N^{(1)}$	16384

Table D.3: Parameters for the “five multiplets” inversion recovery simulation run using SPINACH.

## D.2 Experimental datasets

### D.2.1 Structures

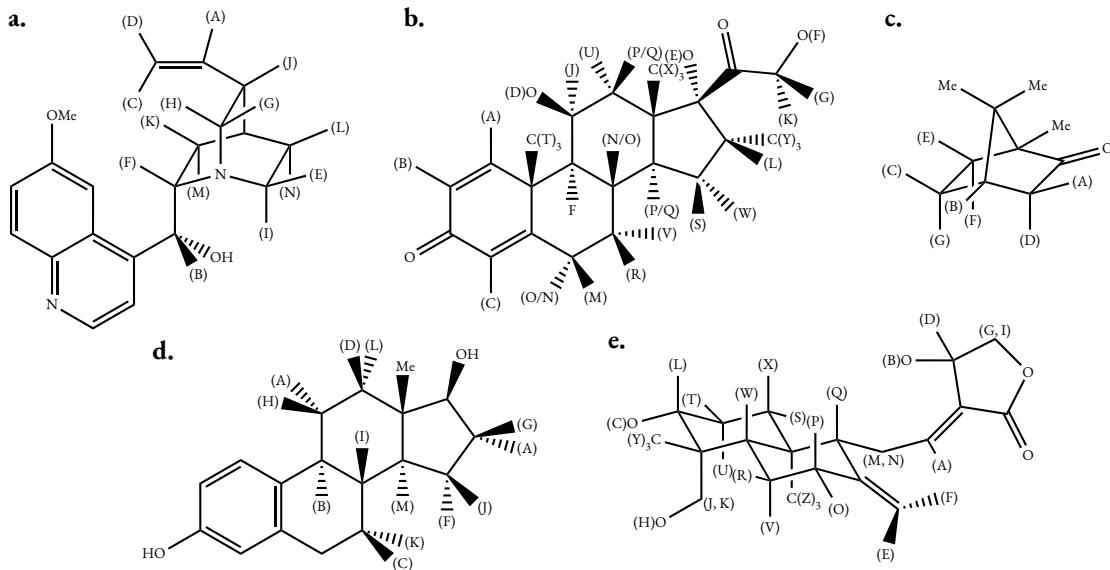


Figure D.1: The molecular structures of species giving rise to the experimental NMR datasets considered in this work. a. Quinine, b. Dexamethasone, c. Camphor, d. 17 $\beta$ -estradiol, e. Andrographolide. Proton environments giving rise to signals which are considered in this work are denoted with bracketed alphabetical characters. Non-bracketed alphabetical characters denote chemical symbols. Me denotes the methyl group, equivalent to CH<sub>3</sub>. **TODO: check assignments (esp. estradiol). If more structures need adding, edit the ChemDraw file on Chive called simon\_stuff/thesis\_structures.cdxml. Use EB-Garamond for atom labels. One a structure is made, scale to 75% of original size, and set font to 7pt. Then in inkscape, rescale this by multiplying by 0.8. Dexamethasone: replace (J) with (H), (K) with (I), etc...**

### D.2.2 1D datasets

Both the andrographolide and cyclosporin A pulse-acquire experiments were acquired BRUKER's zg30 pulse sequence, which involves applying a pulse with a target flip angle of 30°, followed by acquisition. The cyclosporin A pulse-acquire dataset was taken from BRUKER's TOPSPIN software (v 4.0.8), located at <TOPSPINROOT>/topspin4.0.8/examdata/exam1d\_1H/1.

	Andrographolide	Cyclosporin A
$f_{bf}$ (MHz)	600.18	500.13
$f_{off}$ (Hz)	2400.7	2249.2
$f_{off}$ (ppm)	4	4.4972
$f_{sw}$ (Hz)	4795.4	5494.5
$f_{sw}$ (ppm)	7.9899	10.986
$N$	16384	65384
NS	1	16
DS	0	2
PLW1 (W)	24	?
P1 ( $\mu$ s)	12	10.8
D1 (s)	1	1

**Table D.4:** Noteworthy experiment parameters for the pulse-acquire datasets used. NS: Number of scans, DS: Number of dummy scans, PLW1: Hard pulse power (W), P1: Duration of  $\pi/2$  pulse, D1: Duration of relaxation delay. N.B. The duration of the pulse used was 1/3 that of P1. PLW1 for the cyclosporin dataset could not be found.

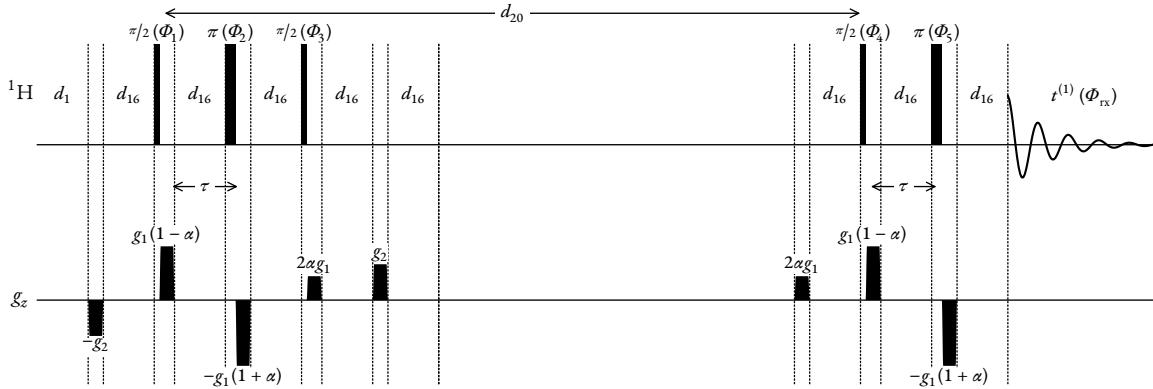
	Andrographolide	Glucose/valine/threonine
$f_{\text{bf}}$ (MHz)	600.18	499.98
$f_{\text{off}}$ (Hz)	3000.9	2499.9
$f_{\text{off}}$ (ppm)	5	5
$f_{\text{sw}}$ (Hz)	7211.5	10000
$f_{\text{sw}}$ (ppm)	12.016	20.001
$N$	16384	65536
NS	4	32
DS	2	4
PLW1 (W)	24	18.204
P1 ( $\mu\text{s}$ )	12	10
D1 (s)	1.5	6

**Table D.5:** Noteworthy experiment parameters for the diffusion datasets used. NS: Number of scans, DS: Number of dummy scans, PLW1: Hard pulse power (W), P1: Duration of  $\pi/2$  pulse, D1: Duration of relaxation delay.

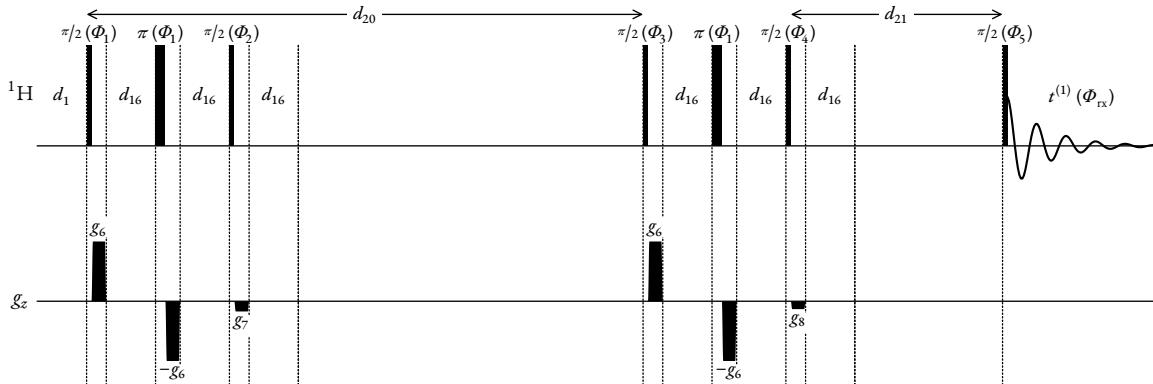
### D.2.3 Diffusion datasets

The andrographolide diffusion dataset (Figure 3.6) was acquired using the one-shot DOSY pulse sequence[121] (version 1.0c, published on 27/3/2012), accessible via the webpage <https://www.nmr.chemistry.manchester.ac.uk/?q=node/264>. The pulse sequence is displayed in Figure D.2.

The glucose/valine/threonine diffusion dataset (Figure 3.7) was acquired using Bruker’s ledpgp2s pulse sequence (version 1.9, published on 19/2/2011). This is a stimulated echo pulse sequence, featuring bipolar gradients and a longitudinal eddy current delay (LED) component[120]. The pulse sequence is displayed in Figure D.3. Analysis of the dataset using the multivariate methods DECRA and SCORE was facilitated through use of The University of Manchester’s General NMR Analysis Toolbox (GNAT) software[175].



**Figure D.2:** Oneshot DOSY pulse sequence used for the acquisition of andrographolide data (Figure 3.6). All delays are included, though they are not to scale. Delays:  $d_1$  (relaxation delay): 1.5 s,  $d_{16}$  (gradient recovery delay): 200  $\mu\text{s}$ ,  $d_{20}$  (diffusion time, equivalent to  $\mathcal{A}$ ): 0.1 s. Hard pulses had a power of 24 W, with the duration of the  $\pi/2$  pulse being 12  $\mu\text{s}$ . Diffusion encoding gradients had a smoothed square profile (SMSQ10.100), a duration of 1 ms, and had strengths related to the values  $g_1$  and  $\alpha = 0.2$ .  $g_1$  was varied across increments, with the values used being ( $\text{G cm}^{-1}$ ): 6.270, 12.470, 16.483, 19.695, 22.451, 24.905, 27.137, 29.200, 31.126, 32.939, 34.658, 36.296, 37.862, 39.367, 40.816, 42.215, 43.570, 44.883, 46.159, 47.401. Spoiler gradients had the same SMSQ10.100 profile, had a duration of 600  $\mu\text{s}$ , and a strength which was 75% of  $g_1$ . The phase cycling scheme used was:  $\Phi_1 : 2 \times (0^\circ, 180^\circ)$ ;  $\Phi_2 : 4 \times 0^\circ$ ;  $\Phi_3 : 4 \times 0^\circ$ ;  $\Phi_4 : 2 \times 0^\circ, 2 \times 180^\circ$ ;  $\Phi_5 : 4 \times 0^\circ$ ;  $\Phi_{rx} : 0^\circ, 180^\circ, 180^\circ, 0^\circ$ .



**Figure D.3:** Pulse sequence used for the acquisition of glucose/threonine/valine diffusion data (Figure 3.7). All delays are included, though they are not to scale. Delays:  $d_1$  (relaxation delay): 6 s,  $d_{16}$  (gradient recovery delay): 200  $\mu\text{s}$ ,  $d_{20}$  (diffusion time, equivalent to  $\mathcal{A}$ ): 0.1 s,  $d_{21}$  (eddy-current delay): 5 ms. Hard pulses had a power of 18.204 W, with the duration of the  $\pi/2$  pulse being 10  $\mu\text{s}$ . All gradients had a smoothed square profile (SMSQ10.100). Gradients for diffusion encoding had a duration of 1 ms, with strength  $g_6$  varied across increments, with the values used being ( $\text{G cm}^{-1}$ ): 4.500, 12.728, 17.428, 21.107, 24.233, 27.000, 29.508, 31.820, 33.974, 36.000. Spoiler gradients had a duration of 600  $\mu\text{s}$ . The gradients had the relative strengths  $g_7 = -0.1713g_6$  and  $g_8 = -0.1317g_6$ . The phase cycling scheme used was:  $\Phi_1 : 32 \times 0^\circ$ ;  $\Phi_2 : 8 \times (2 \times 0^\circ, 2 \times 180^\circ)$ ;  $\Phi_3 : 2 \times (4 \times 0^\circ, 4 \times 180^\circ, 4 \times 90^\circ, 4 \times 270^\circ)$ ;  $\Phi_4 : 2 \times (2 \times (0^\circ, 180^\circ), 2 \times (180^\circ, 0^\circ), 2 \times (90^\circ, 270^\circ), 2 \times (270^\circ, 90^\circ))$ ;  $\Phi_5 : 2 \times (4 \times 0^\circ, 4 \times 180^\circ, 4 \times 90^\circ, 4 \times 270^\circ)$ ;  $\Phi_{rx} : 2 \times (0^\circ, 180^\circ, 180^\circ, 0^\circ, 180^\circ, 0^\circ, 180^\circ, 270^\circ, 90^\circ, 90^\circ, 270^\circ, 90^\circ, 270^\circ, 90^\circ)$ .

### D.2.4 2DJ datasets

The 2D J-Resolved datasets presented were acquired using Bruker's `jresqf` pulse sequence (version 1.7, released 31/1/2012). This pulse sequence comprises  $\pi/2(\Phi_1) \rightarrow t^{(1)}/2 \rightarrow \pi(\Phi_2) \rightarrow t^{(1)}/2 \rightarrow t^{(2)}(\Phi_{\text{rx}})$ , with the EXORCYCLE phase-cycling scheme[27: Section 11.6]:

$$\begin{array}{llll} \Phi_1 : & 0^\circ & 0^\circ & 0^\circ \\ \Phi_2 : & 0^\circ & 90^\circ & 180^\circ & 270^\circ \\ \Phi_{\text{rx}} : & 0^\circ & 180^\circ & 0^\circ & 180^\circ \end{array}$$

Key experiment parameters are provided in Table D.6.

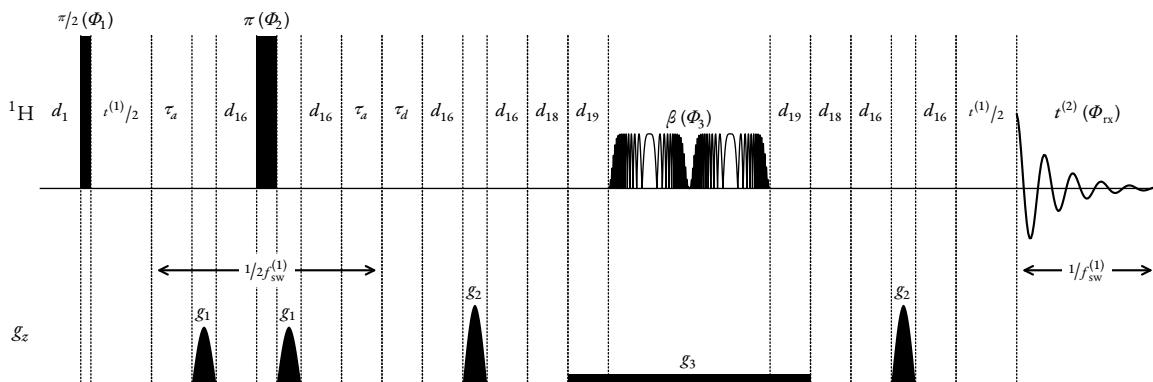
	Quinine	Dexamethasone	Camphor	Estradiol
$f_{\text{bf}}$ (MHz)	500.13	600.18	500.13	500.3
$f_{\text{off}}^{(2)}$ (Hz)	2500	2815.4	1000	2501.5
$f_{\text{sw}}^{(1)}$ (Hz)	50	50	50	100
$f_{\text{sw}}^{(2)}$ (Hz)	7500	7211.5	5000	5000
$f_{\text{sw}}^{(2)}$ (ppm)	14.996	12.016	9.9974	9.994
$N^{(1)}$	128	64	128	128
$N^{(2)}$	16384	8192	16384	16384
NS	4	2	4	4
DS	4	8	4	2
PLW1 (W)	20.893	24	20.893	31.537
P1 ( $\mu\text{s}$ )	10	12	10	15
D1 (s)	2	1.5	2	1

**Table D.6:** Noteworthy experiment parameters for the 2D J-Resolved and PSYCHE experiments used. NS: Number of scans, DS: Number of dummy scans, PLW1: Hard pulse power (W), P1: Duration of  $\pi/2$  pulse, D1: Duration of relaxation delay.

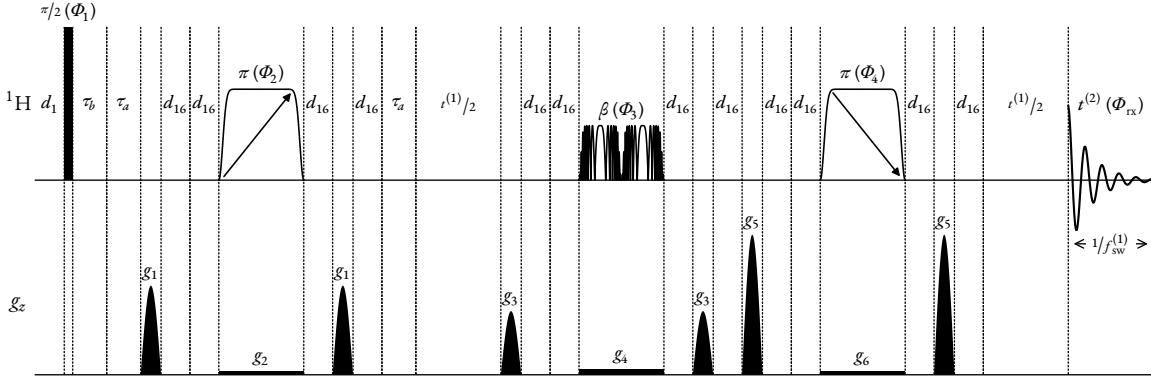
### D.2.5 PSYCHE datasets

The pulse sequence used for the acquisition of the estradiol PSYCHE spectrum (Figure 4.10) is presented in Figure D.4, where pulses, gradients, and delays are described in detail. Equivalent parameters were used for the basic setup as the estradiol 2DJ experiment, given in Table D.6.

The pure shift spectrum of dexamethasone (Figure 4.9.a) was acquired using a TSE-PSYCHE experiment (Figure D.5). The pulse sequence file UoM\_1d\_if\_tsepsyche\_ts4x can be obtained via the link <https://research.manchester.ac.uk/en/datasets/manchester-pure-shift-nmr-workshop-bruker-software>.



**Figure D.4:** PSYCHE pulse sequence used for the acquisition of estradiol data. All delays are included, though they are not to scale. Delays:  $d_1$  (relaxation delay): 1 s,  $d_{16}$ : (gradient recovery delay): 200  $\mu$ s,  $d_{18}$ : 200  $\mu$ s,  $d_{19}$ : 1 ms,  $\tau_a$ : 1.3 ms,  $\tau_d$ : 18.9 ms. The PSYCHE element featured two saltire chirp pulses with a wideband, uniform rate, smooth truncation (WURST)[176] amplitude envelope, with a target flip angle  $\beta = 20^\circ$ . Each saltire pulse had a bandwidth of 10 kHz, a duration of 25 ms, and a power of 280  $\mu$ W. Hard pulses had a power of 31.537 W, with the duration of the  $\pi/2$  pulse being 15  $\mu$ s.  $G_1$  and  $G_2$  were gradients for coherence order selection. Each comprised a 100-point sine shape profile, and lasted 1 ms.  $G_3$  was a rectangular weak gradient applied during the PSYCHE element, with a duration of 52 ms. The gradeint strengths as a percentage of the maximum permissible z-gradient were, respectively 31%, 47%, 1.6%. The phase cycling scheme used was:  $\Phi_1 : 2 \times (0^\circ, 180^\circ)$ ;  $\Phi_2 : 4 \times 0^\circ$ ;  $\Phi_3 : 2 \times 0^\circ, 2 \times 90^\circ$ ;  $\Phi_{rx} : 0^\circ, 180^\circ, 180^\circ, 0^\circ$ .



**Figure D.5:** TSE-PSYCHE pulse sequence used for the acquisition of dexamethasone data (Figure 4.9.a). Delays:  $d_1$  (relaxation delay): 2 s,  $d_{16}$ : 200  $\mu\text{s}$ ,  $\tau_a$ : 5 ms ( $= 1/4f_{sw}^{(1)}$ ). The hard  $\pi/2$  pulse had a duration of 12  $\mu\text{s}$ , and a power of 24 mW. The two  $\pi$  pulses were unidirectional frequency-swept (chirped) pulses, with the first pulse sweeping from low to high frequencies, and the second pulse sweeping from high to low. These each had a WURST amplitude envelope, lasted a duration of 40 ms, and had a power of 11.05 mW. The PSYCHE element had a target flip angle  $\beta = 15^\circ$ , and featured two saltire chirp pulses. Both saltire pulses had a WURST amplitude envelope, a duration of 15 ms, and a power of 1.28 mW.  $g_1$ ,  $g_3$  and  $g_5$  were gradients for coherence order selection. Each comprised a 100-point sine profile, and lasted 1 ms.  $g_2$ ,  $g_4$  and  $g_6$  were weak rectangular gradients which were applied at the same time as the chirped pulses. The magnitudes of gradients  $g_1$  to  $g_6$  as a percentage of the maximum permitted gradient were, respectively: 49%, 2%, 35%, 3%, 77%, 2%. The phase cycling scheme used was:  $\Phi_1 : 8 \times 0^\circ$ ;  $\Phi_2 : 2 \times (2 \times 0^\circ, 2 \times 180^\circ)$ ;  $\Phi_3 : 2 \times (0^\circ, 90^\circ), 2 \times (180^\circ, 270^\circ)$ ;  $\Phi_4 : 8 \times 0^\circ$ ;  $\Phi_{rx} : 4 \times (0^\circ, 180^\circ)$ .

### D.3 CUPID result metrics

Needs updating: replace sucrose with strychnine, re-order according to the order in the thesis.

### D.3 CUPID result metrics

**Table D.7:** Metrics for all the results generated using CUPID (Section 4.3). The *Initial M* specifies the number of oscillators given to the MMEMP. Values with a \* indicate that they were determined by applying the MDL on the first direct-dimension slice of the data. Values with a † indicate that they were manually provided. The *M after MMEMP* column indicates how many oscillators were present in the initial guess  $\theta^{(0)}$ . This can differ from *Initial M*, as any oscillators possessing negative damping factors in the MMEMP result were purged. The *M after NLP* column indicates how many oscillators were present in  $\theta^{(*)}$ , the result of nonlinear programming. When this value is smaller than *M after MMEMP*, negative-amplitude oscillators were found and purged during the optimisation. *Purged oscillators* indicates how many oscillators were removed from the final estimation result, based on the first-order signal criteria outlined in Section 4.2.4.

Region (ppm)	Initial M	MMEMP time (s)	M after MMEMP	NLP time (s)	NLP iterations	M after NLP	Purged oscillators
<b>Quinine</b>							
5.8 – 5.55	18*	11.2	18	61.4	124	10	None
5 – 4.85	17†	3.5	17	32.1	47	17	None
3.75 – 3.63	15*	2.4	15	34.7	69	13	None
3.17 – 3.06	15*	1.9	15	67.9	150	10	None
2.8 – 2.6	25†	7.5	25	112.9	125	22	None
2 – 1.7	40†	19.8	40	233.3	150	37	1
1.64 – 1.52	20*	2.8	20	38.4	55	18	None
1.52 – 1.4	14*	2.6	13	26.6	58	12	None
<b>Estradiol</b>							
2.29 – 2.17	20†	11.5	17	31.7	150	11	2
2.12 – 2	15†	11.4	15	27.9	150	9	3
1.95 – 1.72	40†	42.7	40	93.2	125	34	4
1.65 – 1.52	20†	12.2	19	47.9	150	15	2
1.45 – 1.02	90†	65.6	86	271.3	150	80	8
<b>Sucrose</b>							

Continues on next page...

Region (ppm)	Initial $M$	MMEMP time (s)	$M$ after MMEMP	NLP time (s)	NLP iterations	$M$ after NLP	Purged oscillators
6.08 – 5.91	2*	0.7	2	0.3	10	2	None
4.72 – 4.46	16†	2.2	16	3.5	21	16	None
4.46 – 4.22	16†	2.1	16	4.5	32	16	None
4.22 – 4.1	4†	0.5	4	3.2	95	4	None
4.09 – 3.98	6*	0.3	6	0.9	12	6	None
3.98 – 3.83	10†	0.6	10	2.9	31	10	None
3.58 – 3.28	12*	2.5	12	3.0	26	12	None
2.08 – 1.16	3*	3.9	3	0.4	9	3	None
1.05 – 0.0	8*	4.0	8	1.1	10	8	None
Four Multiplets (Run 1)							
0.06 – -0.06	34†	3.2	34	45.7	65	33	1
Four Multiplets (Run 2)							
0.06 – -0.06	38†	4.2	38	76.9	105	32	None
Four Multiplets (Run 3)							
0.06 – -0.06	39†	4.3	38	27.6	35	32	None
Four Multiplets (Run 4)							
0.06 – -0.06	40†	4.2	40	45.6	61	32	None
Four Multiplets (Run 5)							
0.06 – -0.06	37†	3.5	37	74.8	100	33	1
Camphor							
2.55 – 2.475	9*	2.0	8	40.6	150	6	1
2.35 – 2.23	18*	5.7	18	68.3	100	18	None

Region (ppm)	Initial $M$	MMEMP time (s)	$M$ after MMEMP	NLP time (s)	NLP iterations	$M$ after NLP	Purged oscillators
2.09 – 2.025	8*	1.3	18	18.3	96	3	None
1.95 – 1.75	35*	19.9	32	260.2	225	30	None
1.7 – 1.61	21*	3.9	21	72.3	84	21	1
1.375 – 1.215	29*	10.6	29	117.2	123	22	None
<b>Dexamethasone</b>							
7.45 – 7.15	2†	0.8	2	0.5	13	2	None
6.4 – 5.9	15*	4.4	7	14.2	66	7	None
5.5 – 4.8	3†	4.0	3	1.1	17	3	None
4.8 – 4.3	11*	3.2	11	12.7	58	9	2
4.25 – 3.97	20†	1.1	19	35.2	133	17	0
3 – 2.87	13*	0.3	11	48.8	219	10	None
2.68 – 2.43	23*	1.2	18	68.2	250	14	None
2.413 – 2.26	18*	0.395	17	61.7	197	15	None
2.195 – 2.034	17*	0.4	17	61.7	200	17	None
1.85 – 1.7	12*	0.4	10	15.0	79	9	None
1.7 – 1.25	30*	3.2	30	127.2	250	27	8
1.14 – 1	12*	0.4	10	36.9	183	10	3
1 – 0.65	3†	2.0	3	0.9	17	3	None



# Document Inserts

E

The remainder of this thesis comprises inserts from two documents:

- E.1 provides Chapter 2 from the documentation of version 2.0 of NMR-EsPy. The section of the documentation included provides tutorials describing how to use the package's API for the consideration of 1D and 2DJ NMR datasets. These tutorials provide a short description of the key features associated with the package, and is an ideal point of reference for new users to gain familiarity with NMR-EsPy.
- E.2 provides the current state of a draft for a communication to be submitted to *Angewandte Chemie*. This communication outlines the methodology and results acquired using CUPID.

---

**CHAPTER  
TWO**

---

**WALKTHROUGHS**

In this chapter, walkthroughs are provided to help you get up-and-running with the main features of the NMR-EsPy API. For a rigorous description of the API, you should consult the [Reference](#) afterwards.

## 2.1 Using Estimator1D

The `nmrespy.Estimator1D` class is provided for the consideration of 1D NMR data.

### 2.1.1 Generating an instance

There are a few ways to create a new instance of the estimator depending on the source of the data

#### Bruker data

It is possible to load both raw FID data and processed spectral data from Bruker using `new_bruker()`. All that is needed is the path to the dataset:

1. If you wish to import FID data, set the path as "`<path_to_data>/<expno>/`". There should be an `fid` file and an `acqus` file directly under this directory. The data in the `fid` file will be imported, and the artefact from digital filtering is removed by a first-order phase shift.

---

**Note:** If you import FID data, there is a high chance that you will need to phase the data, and apply baseline correction before proceeding to run estimation. Look at `phase_data()` and `baseline_correction()`, respectively.

---

```
>>> import nmrespy as ne
>>> estimator = ne.Estimator1D.new_bruker("/home/simon/nmr_data/andrographolide/1")
>>> estimator.phase_data(p0=2.653, p1=-5.686, pivot=13596)
>>> estimator.baseline_correction()
```

2. To import processed data, set the path as "`<path_to_data>/<expno>/pdata/<procno>`". There should be a `1r` file and a `procs` file directly under this directory. The data in `1r` will be Inverse Fourier Transformed, and the resulting time-domain signal is sliced so that only the first half is retained.

---

**Note:** It can be more convenient to provide processed data, even though the data will be converted to the time-domain for estimation, as you can then rely on TopSpin's automated processing scripts

---

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to phase and baseline correct. However, **you should not apply any window function to the data other than exponential line broadening.**

```
>>> import nmresp as ne
>>> estimator = ne.Estimator1D.new_bruker("home/simon/nmr_data/andrographolide/1/pdata/1")
>>> # Note there is no need for extra data-processing steps
```

**Simulated data from a set of oscillator parameters**

You can create an estimator with synthetic data constructed from known parameters using `new_from_parameters()`. The parameters must be provided as a 2D NumPy array with `params.shape[1] == 4`. Each row should contain an oscillator's amplitude, phase (rad), frequency (Hz), and damping factor ( $\text{s}^{-1}$ ).

```
>>> import nmresp as ne
>>> import numpy as np
>>> # Using frequencies of 2,3-Dibromopropanoic acid @ 500MHz
>>> params = np.array([
>>>     [1., 0., 1864.4, 7.],
>>>     [1., 0., 1855.8, 7.],
>>>     [1., 0., 1844.2, 7.],
>>>     [1., 0., 1835.6, 7.],
>>>     [1., 0., 1981.4, 7.],
>>>     [1., 0., 1961.2, 7.],
>>>     [1., 0., 1958.8, 7.],
>>>     [1., 0., 1938.6, 7.],
>>>     [1., 0., 2265.6, 7.],
>>>     [1., 0., 2257.0, 7.],
>>>     [1., 0., 2243.0, 7.],
>>>     [1., 0., 2234.4, 7.],
>>> ])
>>> sfo = 500.
>>> estimator = ne.Estimator1D.new_from_parameters(
>>>     params=params,
>>>     pts=2048,
>>>     sw=1.2 * sfo, # 1ppm
>>>     offset=4.1 * sfo, # 4.1ppm
>>>     sfo=sfo,
>>>     snr=40.,
>>> )
```

**Note:** For the rest of this tutorial, we will be using the estimator created in the above code snippet.

### Simulated data from Spinach

Assuming you have installed the *relevant requirements*, you can create an instance with data simulated using Spinach with `new_spinach()`. The spin system is defined by a specification of isotropic chemical shifts, and scalar couplings:

- For the chemical shift, a list of floats is required.
- For J-couplings, a list with 3-element tuples of the form (`spin1, spin2, coupling`) is required.  
**N.B. the spin indices start at “1” rather than “0”.**

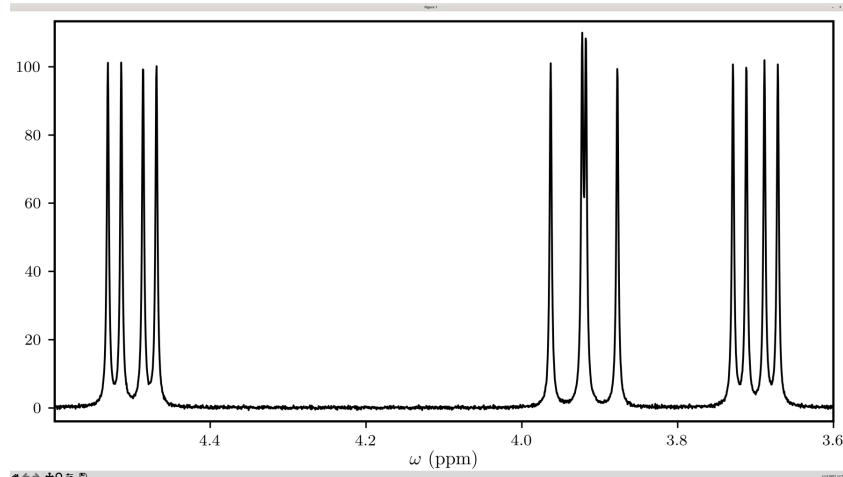
It can take some time to run this function if it involves (a) starting up MATLAB and (b) running a simulation of the experiment.

```
>>> import nmrespy as ne
>>> # 2,3-Dibromopropionic acid
>>> shifts = [3.7, 3.92, 4.5]
>>> couplings = [(1, 2, -10.1), (1, 3, 4.3), (2, 3, 11.3)]
>>> sfo = 500.
>>> offset = 4.1 * sfo # Hz
>>> sw = 1.2 * sfo
>>> estimator = ne.Estimator1D.new_spinach(
>>>     shifts=shifts,
>>>     couplings=couplings,
>>>     pts=2048,
>>>     sw=sw,
>>>     offset=offset,
>>>     sfo=sfo,
>>> )
```

### 2.1.2 Viewing and accessing the dataset

You can inspect the data associated with the estimator with `view_data()`, which loads an interactive matplotlib figure:

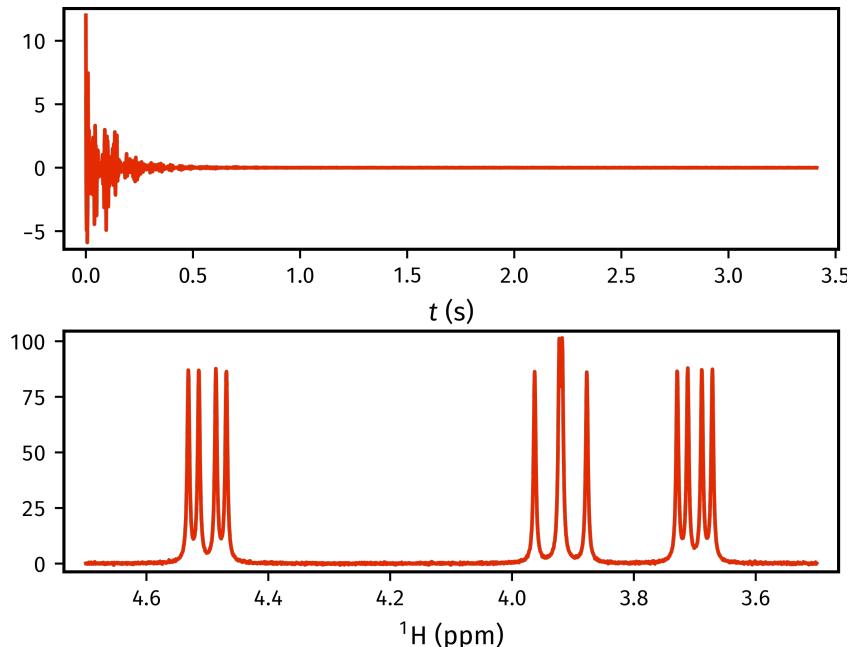
```
>>> estimator.view_data(freq_unit="ppm")
```



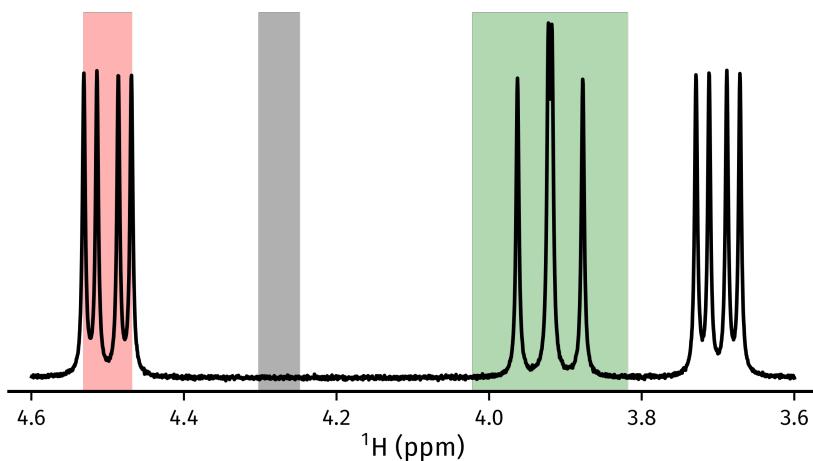
You can access the time-domain data with the `data()` property, and the associated time-points can be retrieved using `get_timepoints()`. The spectral data is accessed with `spectrum()`, and the corresponding chemical shifts with `get_shifts()`.

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```
>>> fid = estimator.data
>>> tp = estimator.get_timepoints()[0]
>>> spectrum = estimator.spectrum
>>> shifts = estimator.get_shifts(unit="ppm")[0]
>>> fig, axs = plt.subplots(nrows=2)
>>> axs[0].plot(tp, fid.real)
>>> axs[0].set_xlabel("$t$ (s)")
>>> axs[1].plot(shifts, spectrum.real)
>>> # Flip x-axis limits (ensure plotting from high to low shifts)
>>> axs[1].set_xlim(reversed(axs[1].get_xlim())))
>>> axs[1].set_xlabel("$^1\text{H}$ (ppm)")
>>> plt.show()
```

**2.1.3 Estimating the dataset**

The generation of parameter estimates for the dataset is facilitated using the `estimate()` method. In most scenarios, your dataset will possess too many oscillators for it to be feasible computationally to estimate the entire signal at once. For this reason, NMR-EsPy generates frequency-filtered “sub-FIDs” to break the problem down into more manageable chunks. To create suitable sub-FIDs, it is important to select regions where the bounds are placed at points that comprise the baseline. As well as this, a region that comprises just the baseline must be indicated. In the figure below, the red region would be inappropriate as it slices through signal. The green region is acceptable, as the bounds are located on the baseline. Finally, the grey region is a suitable noise region as it contains only baseline.



For our dataset, we will estimate three regions, comprising each multiplet structure in the spectrum. A region should be given as a tuple of 2 floats, specifying the left and right boundaries of the region of interest (the order of these doesn't matter). By default, these are assumed to be given in Hz, unless `region_unit` is set to "ppm".

```
>>> regions = [(4.6, 4.4), (4.02, 3.82), (3.8, 3.6)]
>>> noise_region = (4.3, 4.25)
>>> for region in regions:
>>>     estimator.estimate(
>>>         region=region, noise_region=noise_region, region_unit="ppm",
>>>     )
```

## 2.1.4 Inspecting estimation results

### Note: Result Indices

Each time the `estimate()` method is called, the result is appended to a list of all generated results. For many methods that use estimation results, an argument called `indices` exists. This lets you specify the results you are interested in. By default (`indices = None`) all results will be used. A subset of the results can be considered by including a list of integers. For example `indices = [0, 2]` would mean only the 1st and 3rd results acquired with the estimator are considered.

A NumPy array of the generated results can be acquired using `get_params()`. The corresponding errors associated with each parameters are obtained with `get_errors()`.

```
>>> # All params, frequencies in Hz:
>>> estimator.get_params()
[[ 1.0018e+00  1.5921e-03  1.8356e+03  7.0187e+00]
 [ 1.0003e+00  2.4881e-03  1.8442e+03  6.9968e+00]
 [ 1.0024e+00  1.5817e-03  1.8558e+03  7.0281e+00]
 [ 1.0008e+00  9.1591e-04  1.8644e+03  7.0007e+00]
 [ 1.0022e+00  7.1936e-04  1.9386e+03  7.0109e+00]
 [ 9.9470e-01 -7.4609e-04  1.9588e+03  6.9866e+00]
 [ 1.0080e+00 -1.0112e-03  1.9612e+03  7.0448e+00]
 [ 1.0009e+00 -7.1398e-04  1.9814e+03  7.0131e+00]
 [ 1.0003e+00  1.1306e-03  2.2344e+03  7.0095e+00]
 [ 1.0011e+00  6.0150e-04  2.2430e+03  7.0011e+00]]
```

(continues on next page)

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```
[ 9.9902e-01  2.8231e-04  2.2570e+03  6.9856e+00]
[ 1.0004e+00 -1.8229e-03  2.2656e+03  7.0057e+00]]
>>> # All errors, frequencies in Hz
>>> estimator.get_errors()
[[0.0013 0.0013 0.0019 0.0121]
 [0.0014 0.0014 0.002  0.0124]
 [0.0014 0.0014 0.002  0.0125]
 [0.0013 0.0013 0.0019 0.012 ]
 [0.0012 0.0012 0.0018 0.0114]
 [0.0036 0.0036 0.0034 0.0212]
 [0.0036 0.0036 0.0034 0.0213]
 [0.0012 0.0012 0.0018 0.0114]
 [0.0013 0.0013 0.0019 0.0116]
 [0.0013 0.0013 0.0019 0.0118]
 [0.0013 0.0013 0.0019 0.0118]
 [0.0013 0.0013 0.0018 0.0116]]
>>> # Params for first region, frequencies in ppm
>>> estimator.get_params(indices=[0], funit="ppm")
[[ 1.0003e+00  1.1306e-03  4.4688e+00  7.0095e+00]
 [ 1.0011e+00  6.0150e-04  4.4860e+00  7.0011e+00]
 [ 9.9902e-01  2.8231e-04  4.5140e+00  6.9856e+00]
 [ 1.0004e+00 -1.8229e-03  4.5312e+00  7.0057e+00]]
>>> # Params for second and third regions, split up
>>> estimator.get_params(indices=[1, 2], merge=False, funit="ppm")
[array([[ 1.0022e+00,  7.1936e-04,  3.8772e+00,  7.0109e+00],
       [ 9.9470e-01, -7.4609e-04,  3.9176e+00,  6.9866e+00],
       [ 1.0080e+00, -1.0112e-03,  3.9224e+00,  7.0448e+00],
       [ 1.0009e+00, -7.1398e-04,  3.9628e+00,  7.0131e+00]], array([[1.0018e+00,  1.5921e-03,
       3.6712e+00,  7.0187e+00],
       [1.0003e+00,  2.4881e-03,  3.6884e+00,  6.9968e+00],
       [1.0024e+00,  1.5817e-03,  3.7116e+00,  7.0281e+00],
       [1.0008e+00,  9.1591e-04,  3.7288e+00,  7.0007e+00]])]
```

**Writing result tables**

Tables of parameters can be saved to .txt and .pdf formats, using `write_result()`. For PDF generation, you will need a working LaTeX installation. See the [installation instructions](#).

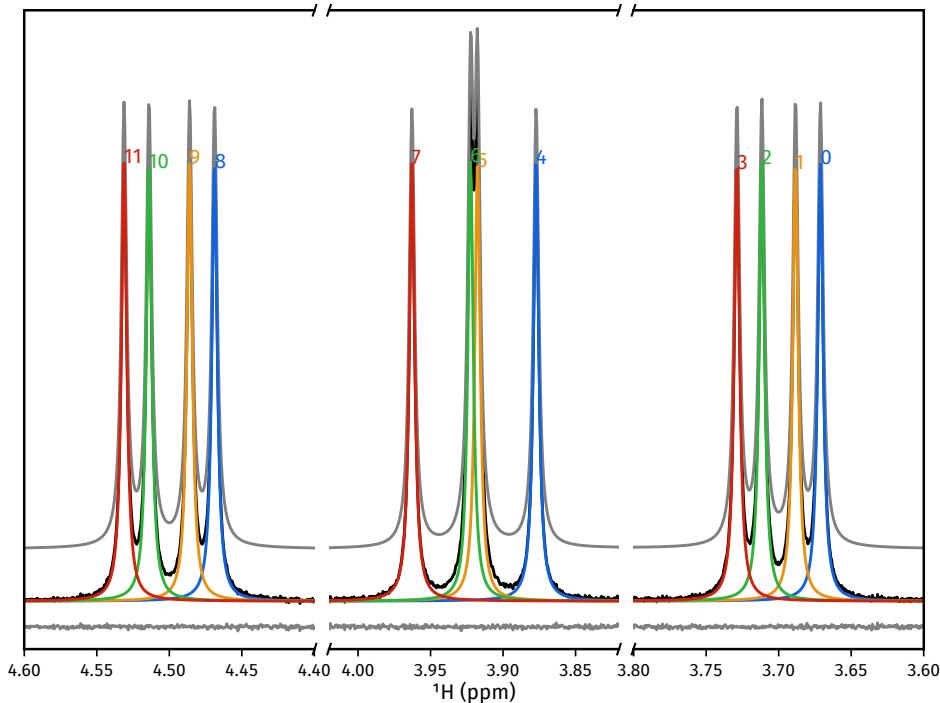
```
>>> for fmt in ("txt", "pdf"):
>>>     estimator.write_result(
>>>         path="tutorial_1d",
>>>         fmt=fmt,
>>>         description="Simulated 2,3-Dibromopropanoic acid signal.",
>>>     )
Saved file tutorial_1d.txt.
Saved file tutorial_1d.tex.
Saved file tutorial_1d.pdf.
You can view and customise the corresponding TeX file at tutorial_1d.tex.
```

## Creating result plots

Figures giving an overview of the estimation result can be generated using `plot_result()`.

```
>>> for (txt, indices) in zip(("complete", "index_1"), (None, [1])):
>>>     fig, ax = estimator.plot_result(
>>>         indices=indices,
>>>         figure_size=(4.5, 3.),
>>>         region_unit="ppm",
>>>         axes_left=0.03,
>>>         axes_right=0.97,
>>>         axes_top=0.98,
>>>         axes_bottom=0.09,
>>>     )
>>>     fig.savefig(f"tutorial_1d_{txt}_fig.pdf")
```

Below is the figure `tutorial_1d_complete_fig.pdf`:



## Saving the estimator

The `estimator` object itself can be saved and reloaded for future use with the `to_pickle()` and `from_pickle()` methods, respectively:

```
>>> estimator.to_pickle("tutorial_1d")
Saved file tutorial_1d.pkl.
>>> # Load the estimator and save to the `estimator_cp` variable
>>> estimator_cp = ne.Estimator1D.from_pickle("tutorial_1d")
```

**NMR-EsPy, Release 2.0****Saving a logfile**

A logfile listing all the methods called on the estimator can be saved using `save_log()`:

```
>>> estimator.save_log("tutorial_1d")
Saved file tutorial_1d.log.
```

## 2.2 Using Estimator2DJ

The `nmrespy.Estimator2DJ` class enables the estimation of J-Resolved (2DJ) spectroscopy datasets. This facilitates use of **CUPID** (Computer-assisted Ultrahigh-resolution Protocol for Ideal Decoupling) which can be used to generate homodecoupled spectra and to predicting multiplet structures.

Many methods in this class have analogues in `Estimator1D`. You are advised to read through the *1D walkthrough* before continuing, as I will be providing minimal descriptions of things covered in that.

### 2.2.1 Generating an instance

#### Bruker data

Use `new_bruker()`. Unlike `Estimator1D`, you must import time-domain 2DJ data. The path should be set as "`<path_to_data>/<exnpo>`". There should be a `ser` file, an `acqus` file, and an `acqu2s` file directly under this directory. Again, phasing in the direct-dimension will be needed. If deemed necessary, baseline correction is possible too.

```
>>> import nmrespy as ne
>>> estimator = ne.Estimator2DJ.new_bruker("/home/simon/nmr_data/quinine/dexamethasone/2")
>>> estimator.phase_data(p0=0.041, p1=-6.383, pivot=1923)
>>> estimator.baseline_correction()
<Estimator2DJ object at 0x7f4b7e1f5cd0>
```

#### Experiment Information

Parameter	F1	F2
Nucleus	<sup>1</sup> H	<sup>1</sup> H
Transmitter Frequency (MHz)	N/A	600.18
Sweep Width (Hz)	50	7211.5
Sweep Width (ppm)	N/A	12.016
Transmitter Offset (Hz)	0	2815.4
Transmitter Offset (ppm)	N/A	4.691

No estimation performed yet.

## Simulated data from Spinach

Use `new_spinach()`

```
>>> # Sucrose shifts and couplings
>>> shifts = [
>>>     6.005,
>>>     3.510,
>>>     3.934,
>>>     3.423,
>>>     4.554,
>>>     3.891,
>>>     4.287,
>>>     3.332,
>>>     1.908,
>>>     1.555,
>>>     0.644,
>>>     4.042,
>>>     4.517,
>>>     3.889,
>>>     4.635,
>>>     4.160,
>>>     4.021,
>>>     4.408,
>>>     0.311,
>>>     1.334,
>>>     0.893,
>>>     0.150,
>>> ]
>>> couplings = [
>>>     (1, 2, 2.285),
>>>     (2, 3, 4.657),
>>>     (2, 8, 4.828),
>>>     (3, 4, 4.326),
>>>     (4, 5, 4.851),
>>>     (5, 6, 5.440),
>>>     (5, 7, 2.288),
>>>     (6, 7, -6.210),
>>>     (7, 11, 7.256),
>>>     (12, 13, -4.005),
>>>     (12, 19, 1.460),
>>>     (14, 15, 4.253),
>>>     (15, 16, 4.448),
>>>     (15, 21, 3.221),
>>>     (16, 18, 4.733),
>>>     (17, 18, -4.182),
>>>     (18, 22, 1.350),
>>> ]
>>> estimator = ne.Estimator2DJ.new_spinach(
>>>     shifts=shifts,
>>>     couplings=couplings,
>>>     pts=(64, 4096),
>>>     sw=(30., 2200.),
>>>     offset=1000.,
>>>     field=300.,
>>>     field_unit="MHz",
>>>     snr=20.,
>>> )
```

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**Note:** We will be using the estimator generated above for the rest of this tutorial. If you do not have access to MATLAB/Spinach, you can construct the estimator by using an FID I made earlier:

```
>>> import nmrspy as ne
>>> from pathlib import Path
>>> import pickle
>>> fid_path = Path(ne.__file__).expanduser().parents[1] \
...     / "samples/jres_sucrose_sythetic/sucrose_jres_fid.pkl"
>>> with open(fid_path, "rb") as fh:
...     fid = pickle.load(fh)
...
>>> expinfo = ne.ExpInfo(
...     dim=2,
...     sw=(30., 2200.),
...     offset=(0., 1000.),
...     sfo=(None, 300.),
...     nucleus=(None, "1H"),
...     default_pts=(64, 4096),
... )
>>> estimator = ne.Estimator2DJ(fid, expinfo)
```

## 2.2.2 Estimating the dataset

The procedure for estimating 2DJ data is very similar to that of 1D data. You need to specify regions in the direct dimension that are of interest for generating filtered sub-FIDs. No filtering is done in the indirect dimension. In our example, it turns out that for a couple of the regions selected, the number of oscillators automatically generated is slightly smaller than the “true” number, and so we force the optimiser to use the true number (see the lines involving `initial_guesses`).

```
>>> regions = (
...     (6.08, 5.91),
...     (4.72, 4.46),
...     (4.46, 4.22),
...     (4.22, 4.1),
...     (4.09, 3.98),
...     (3.98, 3.83),
...     (3.58, 3.28),
...     (2.08, 1.16),
...     (1.05, 0.0),
... )
>>> n_regions = len(regions)
>>> initial_guesses = n_regions * [None]
>>> initial_guesses[1:3] = [16, 16]
>>> # kwargs common to estimation of each region
>>> common_kwargs = {
...     "noise_region": (5.5, 5.33),
...     "region_unit": "ppm",
...     "max_iterations": 200,
...     "phase_variance": True,
... }
>>> for init_guess, region in zip(initial_guesses, regions):
...     kwargs = {{"region": region, "initial_guess": init_guess}, **common_kwargs}
...     estimator.estimate(**kwargs)
```

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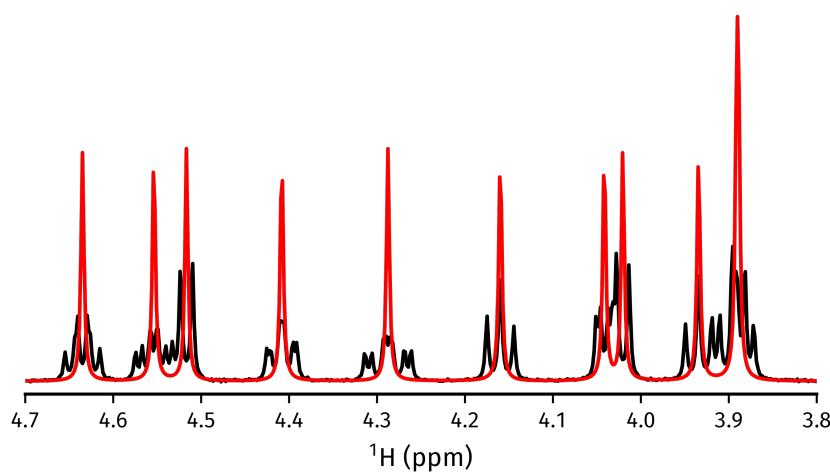
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```
>>> # It is a good idea to pickle the estimator after estimation
>>> estimator.to_pickle("sucrose")
```

### 2.2.3 Acquiring a homodecoupled spectrum

The `cupid_spectrum()` method produces a homodecoupled spectrum using the estimation parameters. In the code snippet below, a figure is made comparing the homodecoupled spectrum with the spectrum of the first direct-dimension slice in the 2DJ data, which is a normal 1D spectrum.

```
>>> # Normal 1D spectrum
>>> init_spectrum = estimator.spectrum_zero_t1.real
>>> # Homodecoupled spectrum produced using CUPID
>>> cupid_spectrum = estimator.cupid_spectrum().real
>>> # Get direct-dimension shifts
>>> shifts = estimator.get_shifts(unit="ppm", meshgrid=False)[-1]
>>> import matplotlib.pyplot as plt
>>> fig, ax = plt.subplots(figsize=(4.5, 2.5))
>>> ax.plot(shifts, init_spectrum, color="k")
>>> ax.plot(shifts, cupid_spectrum, color="r")
>>> # The most interesting region of the spectrum
>>> ax.set_xlim(4.7, 3.8)
>>> # =====
>>> # These lines are just for plot aesthetics
>>> for x in ("top", "left", "right"):
>>>     ax.spines[x].set_visible(False)
>>> ax.set_xticks([4.7 - 0.1 * i for i in range(10)])
>>> ax.set_yticks([])
>>> ax.set_position([0.03, 0.175, 0.94, 0.83])
>>> ax.set_xlabel(f"{estimator.latex_nuclei[1]} (ppm)")
>>> # =====
>>> fig.savefig("cupid_spectrum.png")
```



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## 2.2.4 Multiplet prediction

Oscillators belonging to the same multiplet can be predicted based on the fact that in a 2DJ signal any pair should satisfy the following:

$$\left| \left( f_i^{(2)} - f_i^{(1)} \right) - \left( f_j^{(2)} - f_j^{(1)} \right) \right| < \epsilon$$

where  $\epsilon$  is an error threshold.  $f^{(1)}$  and  $f^{(2)}$  are the indirect- and direct-dimension frequencies, respectively. The `predict_multiplets()` generates groups of oscillator indices satisfying the above criterion. A key parameter for this is `thold`, which sets the error threshold  $\epsilon$ . By default, this is set to be  $\max(f_{\text{sw}}^{(1)}/N^{(1)}, f_{\text{sw}}^{(2)}/N^{(2)})$ , i.e whichever is larger out of the indirect- and direct-dimension spectral resolutions. However, especially when considering real data, this threshold can be a little optimistic. For good multiplet groupings, you may need to manually provide a slightly larger threshold.

In the example below, multiplet groups are determined for regions with indices 1-5 (covering the region plotted above).

```
>>> indices = [1, 2, 3, 4, 5]
>>> multiplets = estimator.predict_multiplets(indices=indices)
>>> for (freq, idx) in multiplets.items():
...     print(f"freq / estimator.sfo[1]:.4f}ppm: {idx}")
...
3.8890ppm: [1, 4]
3.8910ppm: [0, 2, 3, 5]
3.9344ppm: [6, 7, 8]
4.0205ppm: [9, 10]
4.0416ppm: [11, 12, 13, 14]
4.1598ppm: [15, 16, 17]
4.2876ppm: [18, 19, 20, 21, 22, 23, 24, 25]
4.4083ppm: [26, 27, 28, 29, 30, 31, 32, 33]
4.5167ppm: [34, 35]
4.5537ppm: [36, 37, 38, 39, 40, 41, 42, 43]
4.6349ppm: [44, 45, 46, 47, 48, 49]
```

To generate FIDs corresponding to each multiplet structure, use the `construct_multiplet_fids()` method. In the following code snippet, each generated FID undergoes FT, with all the spectra being plotted.

```
>>> # Direct-dimension shifts
>>> shifts_f2 = estimator.get_shifts(unit="ppm", meshgrid=False)[-1]
>>> fids = estimator.construct_multiplet_fids(indices=indices)
>>> # Create an iterator which cycles through values infinitely
>>> from itertools import cycle
>>> colors = cycle(["#84c757", "#ef476f", "#ffd166", "#36c9c6"])
>>> fig, ax = plt.subplots(figsize=(4.5, 2.5))
>>> for fid in fids:
...     # Halve first point prior to FT to prevent vertical baseline shift
...     fid[0] *= 0.5
...     # FT and retrieve real component
...     spectrum = ne.sig.ft(fid).real
...     ax.plot(shifts_f2, spectrum, color=next(colors))
...
>>> ax.set_xlim(4.7, 3.8)
>>> # =====
>>> # These lines are just for plot aesthetics
>>> for x in ("top", "left", "right"):
```

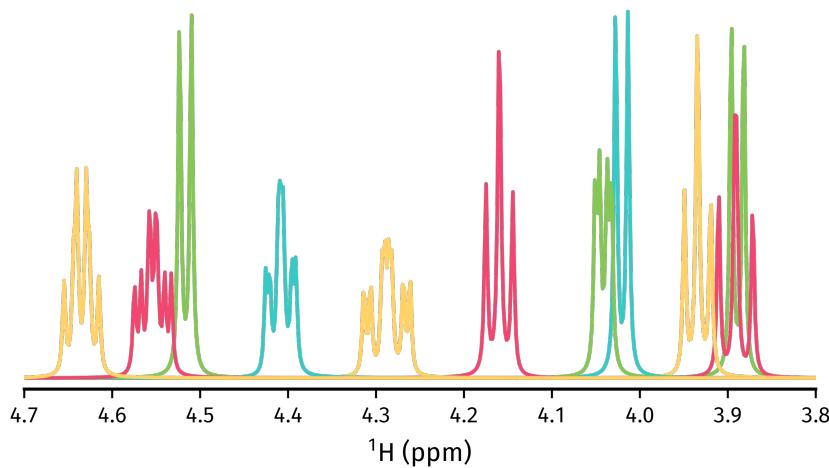
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```

...     ax.spines[x].set_visible(False)
...
>>> ax.set_xticks([4.7 - 0.1 * i for i in range(10)])
>>> ax.set_yticks([])
>>> ax.set_position([0.03, 0.175, 0.94, 0.83])
>>> ax.set_xlabel(f"{estimator.latex_nuclei[1]} (ppm)")
>>> # =====
>>> fig.savefig("multiplets.png")

```



## 2.2.5 Generating tilted spectra

The well-known 45° “tilt” that is applied to 2DJ spectra for orthogonal separation of chemical shifts and scalar couplings effectively maps the frequencies in the direct dimension  $f^{(2)}$  to  $f^{(2)} - f^{(1)}$ . Armed with an estimation result, a signal with these adjusted frequencies can easily be constructed. As well as this, generating a pair of phase- or amplitude-modulated FIDs enables the construction of absorption-mode spectra. Use `nmrespypy.Estimator2DJ.sheared_signal()`, with `indirect_modulation` set to either "amp" or "phase" to generate the desired spectra. Then, you can use either `nmrespypy.sig.proc_phase_modulated()` or `nmrespypy.sig.proc_amp_modulated()` as appropriate to construct the spectrum:

```

>>> # Generate P- and N- type FIDs with "sheared" frequencies
>>> sheared_fid = estimator.sheared_signal(indirect_modulation="phase")
>>> # sheared_fid[0] -> P-type, sheared_fid[1] -> N-type
>>> sheared_fid.shape
(2, 64, 4096)
>>> # Generates 2rr, 2ri, 2ir, 2ii spectra
>>> sheared_spectrum = ne.sig.proc_phase_modulated(sheared_fid)
>>> sheared_spectrum.shape
(4, 64, 4096)
>>> spectrum_2rr = sheared_spectrum[0]
>>> # Note the `meshgrid` kwarg is True here to make 2D shift arrays
>>> shifts_f1, shifts_f2 = estimator.get_shifts(unit="ppm")
>>> fig, ax = plt.subplots(figsize=(4.5, 2.5))
>>> # Contour levels
>>> base, factor, nlevels = 25, 1.3, 10
>>> levels = [base * factor ** i for i in range(nlevels)]
>>> ax.contour(

```

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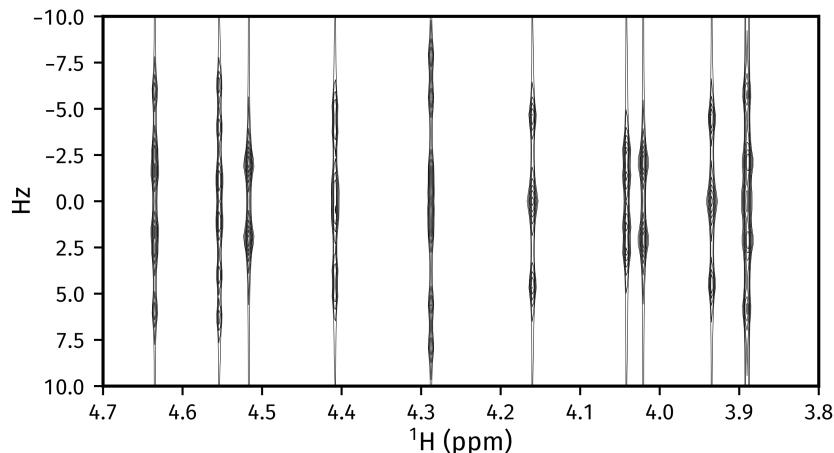
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```

...
    shifts_f2,
...
    shifts_f1,
...
    spectrum_2rr,
    colors="k",
...
    levels=levels,
    linewidths=0.3,
...
)
>>> ax.set_xlim(4.7, 3.8)
>>> ax.set_ylim(10., -10.)
>>> # =====
>>> # These lines are just for plot aesthetics
>>> ax.set_xticks([4.7 - 0.1 * i for i in range(10)])
>>> ax.set_position([0.12, 0.175, 0.85, 0.79])
>>> ax.set_xlabel(f"{estimator.latex_nuclei[1]} (ppm)", labelpad=1)
>>> ax.set_ylabel("Hz", labelpad=1)
>>> # =====
>>> fig.savefig("sheared_spectrum.png")

```

**2.2.6 Plotting result figures**

The `plot_result()` method enables the generation of a figure giving an overview of the estimation result. The figure comprises the following, from top to bottom:

- The homodecoupled spectrum generated using `cupid_spectrum()`.
- The 1D spectrum corresponding to the 2DJ dataset.
- The multiplet structures predicted. Note that to get decent multiplet assignments, you may need to increase the value of the `multiplet_thold` argument manually.
- A contour plot of the 2DJ spectrum, with points indicating the positions of estimated peaks.

```

>>> fig, axs = estimator.plot_result(
...     indices=[1, 2, 3, 4, 5],
...     region_unit="ppm",
...     marker_size=5.,
...     figsize=(4.5, 2.5),
...     # Number of points to construct homodecoupled signal

```

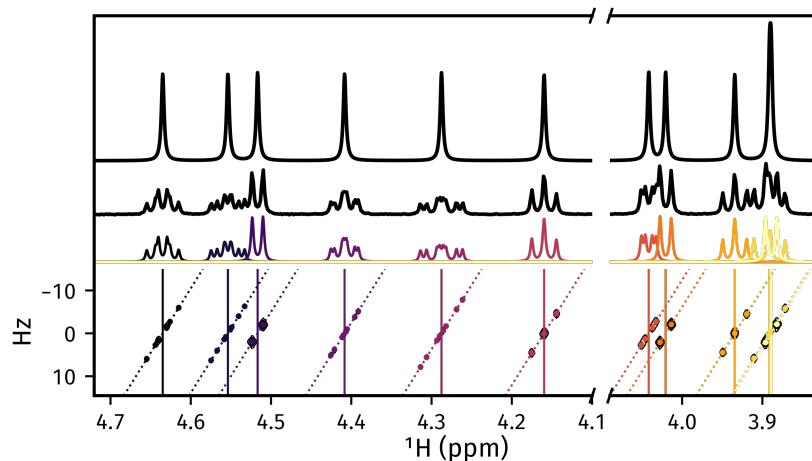
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```

...
# and multiplet structures from
...
high_resolution_pts=16384,
...
# There is a lot of scope for editing the colours of
# multiplets. See the reference!
...
# Here I specify a recognised name of a colourmap in
# matplotlib.
...
multiplet_colors="inferno",
...
# Arguments of the position of the plot in the figure
...
axes_left=0.1,
...
axes_bottom=0.15,
...
)
>>> fig.savefig("plot_result_2dj.png")

```



## 2.2.7 Writing data to Bruker format

**Note:** I am aware that it is currently not possible to analyse the pdata that is generated by NMR-EsPy (you'll get an error along the lines of "*This application requires frequency domain data*" if you try to peak pick, integrate etc). As a workaround for now, you can run a processing script on the FID to generate processed data that is readable by TopSpin. All I do to get the spectrum from the FID is halve the initial point and FT (there is no apodisation).

### Multiplets

To write individual multiplet structures to separate Bruker experiments, you can use `write_multiplets_to_bruker()`. It is a good idea to set a prefix for the experiment numbers, especially if the directory you are saving to already has data directories, so you can easily remember which of the directories correspond to multiplet structures. In the example below, as 22 multiplets were resolved, and `expno_prefix` was set to 99, the directories 9901/, 9902/, ..., 9922/ are created.

```

>>> estimator.write_multiplets_to_bruker(
...
    path=".",
...
    expno_prefix=99,
...
    pts=16384,

```

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```
...     force_overwrite=True,
...
Saved multiplets to folders ./[9901-9922]/
```

**CUPID data**

To save the homodecoupled signal generated by our CUPID method, use `write_cupid_to_bruker()`:

```
>>> estimator.write_cupid_to_bruker(
...     path=".",
...     expno=1111,
...     pts=16384,
...
Saved CUPID signal to ./1111/
```

**2.2.8 Miscellaneous**

For writing result tables to text and PDF files, saving estimators to binary files for later use, and saving log files, look at the relevant sections in the [Using Estimator1D](#) walkthrough. The process is identical.



# Ultrahigh-Resolution NMR at Full Sensitivity

Simon G. Hulse,<sup>[a]</sup> Mohammadali Foroozandeh<sup>\*[a]</sup>

We present CUPID (Computer-assisted Undiminished-sensitivity Protocol for Ideal Decoupling), a technique which uses parametric estimation to produce pure shift spectra from easy-to-acquire J-Resolved datasets without loss of sensitivity, and with absorption-mode lineshapes. We illustrate that it is effective even in scenarios where state-of-the-art pure shift experimental techniques are too insensitive, and where undesired solvent/impurity peaks overlap with signals of interest. The method also enables the assignment of multiplet structures based on a simple criterion involving the relationship between a particular resonance's direct- and indirect-dimension frequencies. The functionality required to use CUPID is provided by NMR Estimation in Python (NMR-EsPy), an open source package with a simple-to-use API and supporting graphical interface.

2D J-resolved (2DJ) spectroscopy<sup>[1,2]</sup> is a valuable technique for separating chemical shift and scalar coupling information. The experiment is commonly used to acquire broadband homodecoupled (pure shift) spectra, achieved by applying a 45° shear to the spectral data such that  $S(f^{(1)}, f^{(2)}) \rightarrow S(f^{(1)}, f^{(2)} - f^{(1)})$ . This transformation leaves chemical shifts and scalar couplings lying perfectly orthogonally to each other, along the  $F^{(2)}$  and  $F^{(1)}$  axes, respectively. A subsequent summation along  $F^{(1)}$  yields the pure shift spectrum. Despite the simplicity of this approach, J-Resolved datasets are hypercomplex (i.e. phase-modulated with respect to both time dimensions), from which it is impossible to generate a spectrum with desirable absorption-mode Lorentzian lineshapes. In fact, summation of the spectrum, which comprises “phase-twist” lineshapes leads to positive and negative contributions cancelling each other out. It is therefore conventional to display 2DJ spectra using magnitude mode, leading to pure shift spectra with broad wings as they possess both absorption- and dispersion-mode character. Post-processing techniques such as pseudo-echo reshaping<sup>[3]</sup> and sine-bell apodisation<sup>[4]</sup> can help suppress the dispersive component, though these induce a significant hit to sensitivity, principally as they drastically reduce the magnitude of the initial points in the FID. There has been considerable development of “1D” pure shift methods, which typically involve concatenating the initial “chunks” of FIDs in a 2D experiment. Prominent examples involve the use of the Zanger-Sterk (ZS) pulse element<sup>[5,6]</sup>, Bilinear rotational Decoupling (BIRD)<sup>[7,8]</sup>, and Pure Shift Yielded by Chirp Excitation (PSYCHE)<sup>[9,10]</sup>. These techniques all suffer from a significant reduction in sensitivity as only a subset of the available spin magnetisation contributes to the final signal, albeit for differing reasons (see<sup>[11]</sup> for an overview).

We introduce a new method to generate pure shift spectra, which utilises NMR Estimation in Python (NMR-EsPy), an open source package we recently presented<sup>[12]</sup>. The technique involves estimation of the parameters which describe the 2DJ FID. With knowledge of these parameters, it is possible to generate pure shift spectra with absorption-mode lineshapes, with the same sensitivity as a simple pulse-acquire experiment. We name the technique CUPID (Computer-assisted Undiminished-sensitivity Protocol for Ideal Decoupling). Using parametric estimation as a route to pure shift spectra also provides extra benefits, such as the ability to assign multiplet structures, and remove unwanted signals such as solvent peaks, and peaks which arise from strong coupling effects<sup>[13,14]</sup>.

2DJ FIDs can be modelled as a summation of exponentially damped hypercomplex oscillators, with six parameters that define each oscillator: amplitude ( $a$ ), phase ( $\phi$ ), two frequencies ( $f^{(1)}, f^{(2)}$ ), and two damping factors ( $\eta^{(1)}, \eta^{(2)}$ ), such that a signal comprising  $M$  oscillators can be fully described by  $6M$  parameters. A technique has been previously presented which estimates the  $4M$  parameters associated with 1D NMR signals using NMR-EsPy, which employs numerical optimisation to minimise a cost function associated with how well a given set of parameters describes the underlying data<sup>[12]</sup>. NMR-EsPy has been extended to support the estimation of hypercomplex 2D datasets, with more detail of the underlying theory provided in Section A of the supplementary material. One noteworthy feature of the technique is it typically requires the generation of frequency-filtered “sub-FIDs” in the direct dimension, as the computational requirements scale considerably with (a) the number of data points, and especially (b) the model order  $M$ .

The key principle behind CUPID is generation of a 1D FID from the estimated parameters, named the “−45° signal”<sup>1</sup>  $\mathbf{y}_{-45^\circ} \in \mathbb{C}^N$ :

$$\mathbf{y}_{-45^\circ}[n] = \sum_{m=1}^M a_m e^{i\phi_m} e^{(2\pi i (f_m^{(2)} - f_m^{(1)}) - \eta_m^{(2)}) n \Delta t}, \quad (1)$$

$\forall n \in \{0, \dots, N-1\}$ . This signal takes the same mathematical form as a conventional FID acquired by a pulse-acquire experiment, except the usual frequencies  $\{f_m^{(2)}\} \forall m = 1, \dots, M$  are replaced with  $\{f_m^{(2)} - f_m^{(1)}\}$ . Oscillators which belong to a particular multiplet have frequencies  $f_m^{(1)} = f_d$  and  $f^{(2)} = f_c + f_d$  in 2DJ datasets, where  $f_c$  is the multiplet's central frequency, and  $f_d$  is the displacement of a given oscillator from the central frequency<sup>2</sup>. **Rethink notation here perhaps.** Hence, all oscillators belonging to the same multiplet will contribute a component with the multiplet's central frequency ( $f_c$ ) in the −45° signal. It is worth restating here that under the assumption of successful extraction of the 2DJ FID's parameters, Equation 1 leads to spectra with

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<sup>1</sup>See Section A.6 of the supplementary material for the reasoning behind the name.

<sup>2</sup> $f_d$  will be some linear combination of the scalar couplings associated with a given spin, with all coefficients in the combination being ±1

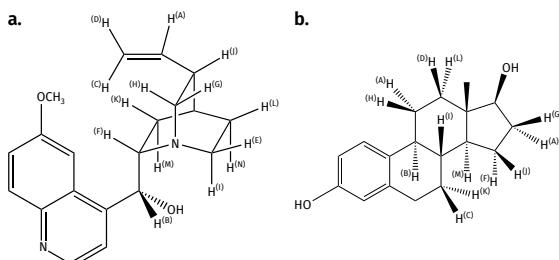
absorption Lorentzian lineshapes without any loss of sensitivity.

The assignment of multiplet structures can be achieved by grouping together oscillators in an estimation result, such that any pair of oscillators  $\{i, j\}$  that are part of the same multiplet satisfy

$$\left| \left( f_i^{(2)} - f_i^{(1)} \right) - \left( f_j^{(2)} - f_j^{(1)} \right) \right| < \epsilon, \quad (2)$$

where  $\epsilon$  is a threshold to account for uncertainty in the estimation. A sensible threshold to set for  $\epsilon$  is the sampling rate in the more poorly resolved dimension. In practice, this can be a little too optimistic, and  $\epsilon$  sometimes needs to be slightly increased to resolve multiplets effectively.

The process we describe has similarities with work from Nuzillard<sup>[15,16]</sup>, and Mutzenhardt et al.<sup>[17]</sup>, in which 1D estimation is used to determine signal parameters for each slice either in  $t^{(1)}$  (Nuzillard) or  $t^{(2)}$  (Mutzendardt et al.). A “Full echo” is generated via propagation into negative time in estimated dimension, with Fourier Transformation producing to an absorption-mode spectrum which can be sheared and summed as described already. Use of a holistic 2D estimation routine as employed here opens up the possibility of (a) estimating more complex datasets, as individual resonances are more separated, and (b) assigning 1D multiplet structures, which requires knowledge of oscillator frequencies in both dimensions.

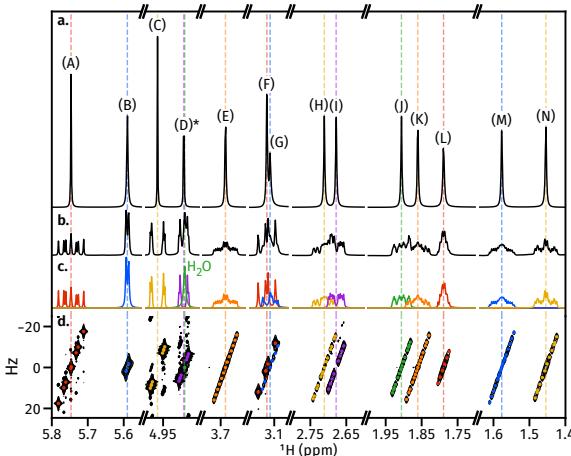


**Figure 1.** The structures of molecules considered. **a.** quinine, **b.** 17 $\beta$ -estradiol.

We present here two examples of the application of CUPID, on the following samples (Figure 1):

- Quinine in CD<sub>3</sub>OD (Figure 2).
- Low concentration (2 mM) 17 $\beta$ -estradiol in DMSO-d<sub>6</sub> (Figure 3). A PSYCHE spectrum was also acquired for comparison.

Extra examples are presented in Section B of the supplementary material, including results involving simulated data, which illustrates that in the limit of a “perfect” estimation result, a spectrum which agrees exactly with the expected pure-shift spectrum is achievable. After the generation of each result, certain oscillators were removed from the set of parameters. The oscillators in question were typically spurious and of low-intensity. These tend to arise in situations where a slight over-fitting of the data has occurred. Most of these could be removed automatically, based on a couple of simple criteria outlined in the supplementary material (Section A.7). The updated results re-underwent optimisation after editing. While these edits did improve the results by removing spurious oscillators, the original results still successfully generated homodecoupled spectra with only a small differences to the final spectra presented here.



**Figure 2.** Application of CUPID on the non-aromatic regions of a quinine dataset. **a.** Spectrum generated using CUPID, with a signal arising from residual water, overlapping with proton (D), neglected. **b.** 1D spectrum, produced from Fourier Transformation of the first direct-dimension FID in the 2DJ dataset. **c.** Multiplets assigned, using a threshold  $\epsilon = 0.92$  Hz, the digital resolution in the direct dimension. **d.** The 2DJ spectrum, displayed in magnitude mode, with positions of assigned peaks marked. Vertical lines mark the central frequencies of predicted multiplets.

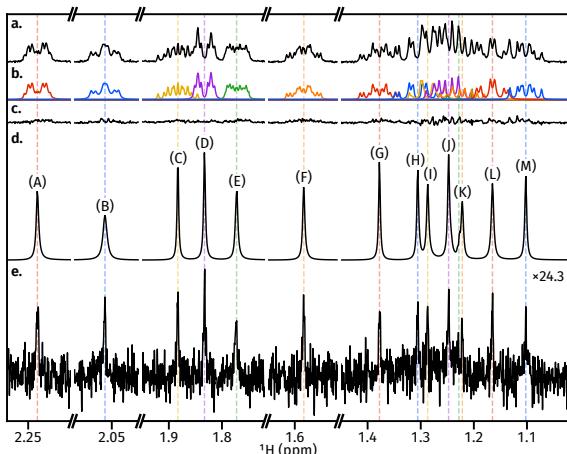
The quinine example provides an example of suppressing an undesired signal from the final pure shift spectrum. An intense broad singlet arising from residual water was detected with a very similar frequency to the central frequency of the multiplet arising from proton D. The parameters describing the water resonance was simply neglected prior to construction of the pure shift spectrum, leading to a peak which is solely derived from proton D. A similar approach can also be applied to remove components arising from strong coupling artefacts from the final spectrum. An example of this is illustrated in the Supplementary Material, where a 2DJ dataset of camphor is considered. The application of CUPID to the estradiol example illustrates that it is able to cope with datasets with highly complex overlapping multiplet structures, in signal-to-noise regimes where PSYCHE is approaching the point of being too insensitive to generate usable spectra.

CUPID works even in scenarios where the estimation routine has under-fit a particular multiplet structure. However, the resulting pure shift peak tends to be broadened beyond the “true” linewidth in these situations. This effect can be seen for peak (B) in the estradiol result. These under-fitting phenomena do not tend to significantly perturb the integrals of the peaks however.

All the results presented in this paper were generated using the NMR-EsPy Python package. The typical CUPID workflow is as follows:

1. Acquire a magnitude-mode J-Resolved dataset for the sample of interest. As a rule of thumb, it is recommended to have an indirect-dimension of at least 64 points. If you can spare the time, or if you have particularly complex regions, such as with the estradiol example, more points are advised.
2. Import the data<sup>3</sup>, phase the direct dimension, and (optionally) baseline correct<sup>[18]</sup>.

<sup>3</sup>Currently, only data in Bruker format is supported



**Figure 3.** The result of applying CUPID on a 2DJ dataset of 2 mM estradiol in  $\text{DMSO-d}_6$ . **a.** Conventional 1D spectrum, generated from the FT of the first direct-dimension signal of the 2DJ FID. **b.** Multiplets assigned ( $\epsilon = 2 \text{ Hz}$ ). **c.** Residual for the first direct-dimension signal in the dataset, given by subtracting the sum of lines in panel b from the line in panel a. **d.** Pure-shift spectrum generated from the FT of the  $-45^\circ$  signal. **e.** PSYCHE spectrum for the same sample. The PSYCHE spectrum is scaled so that the most intense point has same magnitude as the equivalent point in the CUPID spectrum.

3. Select direct-dimension regions of interest, generate filtered sub-FIDs for each region, and estimate the parameters of each sub-FID.
4. (Optional) make edits to correct spurious features in the estimation result if required (i.e. removal of unnecessary oscillators), and re-run the optimisation.
5. Construct the pure shift spectrum and, if desired, spectra for assigned multiplets, and export to the desired format<sup>3</sup>.

From version 2.0, NMR-EsPy provides the functionality to easily achieve the last 4 points, either by writing Python scripts making use of the `Estimator2DJ` object, or with a graphical user interface, which can be loaded from both the command line or within TopSpin. The reader is directed to the documentation for details on usage, found at <https://foroozandehgroup.github.io/NMR-EsPy/>. The project's source code is hosted on GitHub at <https://github.com/foroozandehgroup/NMR-EsPy/>. We welcome queries on usage, bug reports, and suggestions of features to add/improvements.

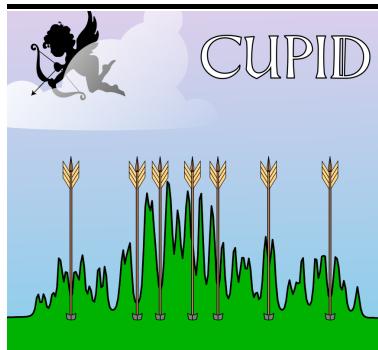
We have presented CUPID, a procedure which generates pure shift spectra from 2DJ datasets via parametric estimation. CUPID can produce spectra with absorption-mode lineshapes, with full sensitivity, and as a complement can predict multiplet structures of crowded spectral regions. CUPID has been shown to be effective even in scenarios where state-of-art pure shift methods are too insensitive to provide useful results.

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**Entry for the Table of Contents**

A procedure for generating pure shift NMR spectra by extracting the parameters which describe 2D J-Resolved data is presented. The spectra generated comprise sharp (absorption-mode) peaks, and do not suffer from a reduction in sensitivity which affects state-of-the-art experimental pure shift techniques.

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