## **Applications of Medical Robotics**

There are 4 types of Robots

- Robots for **Navigation**Surgical drill for Precise positioning, motion compensation..
- Robots for **Imaging** *Minimally-invasive surgery* by Motion downscaling, reduce tremor...
- Robots for **Motion Replication**Robotic ultrasound for Automation, speed...
- Rehabilitation and Prosthetics

  Exoskeletons that Replace damaged structures, autonomous rehabilitation...

Application: Epiphyseolysis

### **Navigation**

Problem: We have an image.

- Where is the **Robot** in the image coordinate system?
- Where is the **Target** in the image?

### Ingridients for Radiologic Navigation:

• C-Arm Robot:

A mobile x-ray system, robot containing 2 prismatic and 3 revolute Joints

• Infrared Tracking:

Place Marker on Endeffector, on Target and on C-Arm. A Camera the ncalculates the positions:

- Skin incision
- Place marker on bone
- Take 2 C-Arm images
- Tavigate
- ⇒ Navigation, Registration, Calibration!

### **Spatial position and orientation**

Every Transformation is a multiplication, simply write down the vectors. Rotatory Matrices:

$$R(x,\theta) = \begin{pmatrix} 1 & 0 & 0 & 0 \\ 0 & C_{\theta} & -S_{\theta} & 0 \\ 0 & S_{\theta} & C_{\theta} & 0 \\ 0 & 0 & 0 & 1 \end{pmatrix}, \ R(y,\theta) = \begin{pmatrix} C_{\theta} & 0 & S_{\theta} & 0 \\ 0 & 1 & 0 & 0 \\ -S_{\theta} & 0 & C_{\theta} & 0 \\ 0 & 0 & 0 & 1 \end{pmatrix}, \ R(z,\theta) = \begin{pmatrix} C_{\theta} & -S_{\theta} & 0 & 0 \\ S_{\theta} & C_{\theta} & 0 & 0 \\ 0 & 0 & 1 & 0 \\ 0 & 0 & 0 & 1 \end{pmatrix}$$

Translatory Matrices:

$$T(x,a) = \begin{pmatrix} 1 & 0 & 0 & a \\ 0 & 1 & 0 & 0 \\ 0 & 0 & 1 & 0 \\ 0 & 0 & 0 & 1 \end{pmatrix}, \ T(y,a) = \begin{pmatrix} 1 & 0 & 0 & 0 \\ 0 & 1 & 0 & a \\ 0 & 0 & 1 & 0 \\ 0 & 0 & 0 & 1 \end{pmatrix}, \ T(z,a) = \begin{pmatrix} 1 & 0 & 0 & 0 \\ 0 & 1 & 0 & 0 \\ 0 & 0 & 1 & a \\ 0 & 0 & 0 & 1 \end{pmatrix}$$

#### **Denavit Hartenberg Parameter**

#### TODO

In Forward Kinematics, we derive the Endeffector Position by multiplication of given Joint Matrices, e.g.

$${}^{B}M_{G} = {}^{B}M_{1} \cdot {}^{1}M_{2} \cdot {}^{2}M_{3} \cdot {}^{3}M_{G}$$

In Reverse Kinematics, we calculate the Joint angles from a given Endeffector Position, e.g. One Joint Robot:

$$P = (P_X, P_Y)$$
, Get Angle  $\theta$  by:  $\frac{P_Y}{P_X} = \frac{\sin \theta}{\cos \theta} = \tan \theta \implies \theta = atan2(P_Y, P_X)$   
Use atan2-Function, as it gives back the angles of full circle depending on signs

# **Navigation & Registration**

### Problem: We have >1 images.

- Rotate images in such way, that images align
- Output is  $\theta, \triangle x, \triangle y$

There are various types of Registration:

- point-based
- landmark-based
- contour-based
- intensity-based
- elastic

### Landmark based registration

Situation: We have an MR image of a head. We place 4 Landmarks (Nose and Mouth). The Target Point is given with respect to the four landmark points. From this, two point clouds A, B are generated.

We assume: #A = #B, 2D,  $a_1 \rightarrow b_1$  etc.

If we move B, this leads to:

$$b_1 \rightsquigarrow R \cdot b_1 + t, \ R = \begin{pmatrix} \cos \theta & -\sin \theta \\ \sin \theta & \cos \theta \end{pmatrix}, \ t = \begin{pmatrix} t_x \\ t_y \end{pmatrix}$$
$$b_2 \rightsquigarrow R \cdot b_2 + t$$
$$\vdots$$
$$b_n \rightsquigarrow R \cdot b_n + t$$

We create a function f, which is the distance between the two point clouds A and B. We want to minimize this function:

$$f = ||R \cdot b_1 + t - a_1||^2 + \dots + ||R \cdot b_n + t - a_n||^2$$

### **Gaussian Least Square**

If we assume that the angle  $\theta$  is small, we can linearize the rotational matrix R such that:

$$\cos \theta \sim 1, \ \sin \theta \sim \theta \implies R = \begin{pmatrix} 1 & -\theta \\ \theta & 1 \end{pmatrix}$$

This matrix R is linear in  $\theta$ .

We can also linearize the 3D rotation matrix as follows:

$$R(x,\alpha) \cdot R(y,\beta) \cdot R(z,\gamma) = \begin{pmatrix} 1 & \gamma & -\beta \\ -\gamma & 1 & \alpha \\ \beta & \alpha & 1 \end{pmatrix}$$

As the multiplication of two small values leads to an even smaller value. This method works fine until angles of 10 degrees.

## Iterative Closest Points (ICP)

Assume we have a point cloud A and a point cloud B. We want know the transformation needed to overlap B over A. We do **not** deform B, as all motion is rigid (rotation and translation).

2 | 1 | 1

	1	1	3	3		2
	1	1	3	3		2
	2	2	3	3		3
Cloud A:	2	2	3	3	Cloud B	3
Cloud A:					Cioua D	

But sometimes, coloring differs in images depending on the imaging process. For Example, in CT the bone has a bright white color, while in MR the bone is more grav:

	1	1	3	3		3	3	
	1	1	3	3		3	3	
	2	2	3	3		2	2	
١.	2	2	3	3	Claud D	2	2	

### Mutual Information (MI)

For Mutual Information Registration, the color mapping does not have to be exactly 1x1. It can be different, as shown in the example above.

### **Basic Definition:**

We generate Images A, B in a random process. For each pixel of the image, we throw a dice (random generation), so we map 6 colors  $\{1, \ldots, 6\}$  to each pixel. A, B are random variables with distributions  $P_A, P_B$ , namely:

- $P_A(a)$  = Probability of grey level value a in image A
- $P_B(b)$  = Probability of grey level value b in image B
- $\implies P_{A,B}(a,b) = \text{Probability of grey level value } a \text{ in image } A \text{ occurring at the}$ same position in image B

#### Examples:

- $A \neq B$ : A tells nothing about B, 2 different images
- A = B : A tells everything about B
- A tells something about B

Keep in mind the law of Independence of two random variables:

$$P_{A,B}(a,b) = P_A(a) \cdot P_B(b)$$

We want to know the maximum Mutual Information, calculated as follows:

$$I(A,B) = \sum_{a,b} P_{A,B}(a,b) \cdot \log_2 \left( \frac{P_{A,B}(a,b)}{P_A(a) \cdot P_B(b)} \right)$$

The Sum ranges over all greyscale pairs of diefferent colors. I(A, B) measures the information dependencies. We maximize the Mutual Information to find exact position.

#### Example 1:

$$A = \begin{bmatrix} 0 & 1 \\ 1 & 0 \\ \end{bmatrix}, \quad B = \begin{bmatrix} 0 & 1 \\ 1 & 0 \\ \end{bmatrix}$$

# **Medical Robotics**

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## Zusammenfassung

 $P_A(0) = 0.5, P_B(0) = 0.5$ 

 $P_A(1) = 0.5, P_B(1) = 0.5$ 

$$\begin{split} P_{A,B}(0,0) &= 0.5, \ P_{A,B}(0,1) = 0 \\ P_{A,B}(1,1) &= 0.5, \ P_{A,B}(1,0) = 0 \\ \sum &= 1 \\ I(A,B) &= \sum_{a,b} P_{A,B}(a,b) \cdot \log_2 \left( \frac{P_{A,B}(a,b)}{P_A(a) \cdot P_B(b)} \right) \\ &= 0.5 \cdot \log_2 \left( \frac{P_{A,B}(0,0)}{P_A(0) \cdot P_B(0)} \right) + 0.5 \cdot \log_2 \left( \frac{P_{A,B}(1,1)}{P_A(1) \cdot P_B(1)} \right) + 0 \cdot \log_2 \left( \frac{P_{A,B}(0,1)}{P_A(0) \cdot P_B(1)} \right) + 0 \cdot \log_2 \left( \frac{P_{A,B}(1,0)}{P_A(1) \cdot P_B(0)} \right) \\ &= 0.5 \cdot \log_2(2) + 0.5 \cdot \log_2(2) \\ &= 1 \end{split}$$

Example 2:

$$A = \begin{bmatrix} 0 & 1 \\ 1 & 0 \\ \end{bmatrix}, \quad B = \begin{bmatrix} 1 & 0 \\ 0 & 1 \\ \end{bmatrix}$$

MI(A, B) = 1, as we care for the structure of the image. The color values do not really matter. Example 3:

$$A = \begin{bmatrix} 0 & 1 \\ 1 & 0 \end{bmatrix}, \quad B = \begin{bmatrix} 1 & 1 \\ 1 & 1 \end{bmatrix}$$

MI(A, B) = 0, as the structures are very different. Example 4:

$$A = \begin{bmatrix} 0 & 1 \\ 1 & 0 \\ \end{bmatrix}, \quad B = \begin{bmatrix} 0 & 1 \\ 1 & 1 \\ \end{bmatrix}$$

$$MI(A,B) = 0.32$$

Keep in mind that  $MI \geq 0$ , but can go up to 100 for large images!

### Calculating $P_A$ , $P_B$ , $P_{A,B}$

Just create a table, then divide the right hand side by the amount of pixels/voxels:

0	number of Pixels in image $A$ with greylevel $0$
:	<b>:</b>
255	number of Pixels in image $A$ with greylevel 255

Calculating  $P_{A,B}$  is a little difficult:

	0	i	255
0			
:		<b>:</b>	
i		# pixel pins with colors $i, j$	
÷			
255			

There are 3 algorithms/methods for calculation:

- 1. Nearest Neighbour (NN)
- 2. Trilinear Interpolation (TI)
- 3. Trilinear Partial Volume (TPV)

## **Imaging**

#### **Image Deformation**

There are multiple applications:

- Elastic Registration
- Distortion Correction

#### **Bilinear Onterpolation**

Assume we have 2 adjacent grid points u, v. To get from G' to G we have to deform u in x-direction by du. We obtain information for w by linear interpolation. Same for the y-direction.

#### Advantage:

- Simplicity
- We will move all points to its goal  $\implies$  Accuracy!

#### Disadvantage:

• Not smooth

### **Cubic Spline Interpolation**

We define a correction polynomial, two variables x, y

$$a_0 + a_1x + a_2y + a_3xy + a_4x^2 + a_5y^2 + a_6xy^2 + a_7x^2y + a_8x^3 + a_9y^3$$

$$b_0 + b_1x + b_2y + b_3xy + b_4x^2 + b_5y^2 + b_6xy^2 + b_7x^2y + b_8x^3 + b_9y^3$$

We have our model:  $(x_m, y_m)$  and our distorted points  $(x_d, y_d)$ .

We further assume, that a's and b's are variables, while x, y are constant.

We set up f as:

$$f = [(x_m, y_m) - (x_d, y_d)]^2$$

For N grid points, we adjust f to:

$$f = [(x_m^{(1)}, y_m^{(1)}) - (x_d^{(1)}, y_d^{(1)})]^2 + \dots + [(x_m^{(N)}, y_m^{(N)}) - (x_d^{(N)}, y_d^{(N)})]^2$$

With  $x_d$  being the a-Polynomial and  $x_m$  being the b-Polynomial, function f is quadratic in the a's and b's.

## **Motion Replication**