

Comprehensive Study on Heart Rate Detection using Camera: Validating Data, Analyzing Results, and Future Directions

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1. INTRODUCTION

The accurate monitoring of vital signs is critical in healthcare and biometrics. Heart rate, also known as pulse rate, is a fundamental indicator of a person's health and well-being. Traditional heart rate measurement methods rely on contact-based sensors such as chest straps or fingertip pulse oximeters. While these methods are reliable, they can be uncomfortable or impractical for continuous monitoring, especially in real-world, nonclinical settings.

Recent advances in computer vision and signal processing have enabled non-contact heart rate detection methods that utilize readily available hardware, such as webcams integrated into smartphones and laptops. These methods exploit the power of image processing and machine learning algorithms to extract heart rate information from subtle changes in color and movement in the user's face, commonly known as photoplethysmography (PPG).

This paper proposes a new approach for non-contact heart rate detection method that combines computer vision techniques, signal processing, and a Kalman filter. The Kalman filter is a recursive mathematical algorithm widely used in various fields of state estimation and dynamic system modeling. Its versatility and robustness make it an attractive option for improving the accuracy and reliability of heart rate detection from video data.

This comprehensive introduction sets the stage for understanding the background, limitations of existing methods, the potential of computer vision, and the specific goals and motivations driving the development of a video-based heart rate monitoring system. The subsequent sections will delve into the detailed methodology, results, and implications of our work.

2. EXISTING METHODS REVIEW

2.1 Contact-Based Sensors and Their Shortcomings

Traditional methods of heart rate measurement often involve contact-based sensors such as electrocardiograms (ECG), photoplethysmograms (PPG), or chest straps. While these methods provide accurate readings, they come with several shortcomings. Contact-based sensors are invasive, causing discomfort to the user. While chest straps provide accurate heart rate measurements, their discomfort and inconvenience limit long-term usage. Users may find them impractical for continuous, real-world monitoring.

They may hinder natural movement, making them unsuitable for continuous monitoring during daily activities or exercise. Additionally, issues such as skin irritation and the need for proper sensor placement limit their practicality.

2.2 Prior Work on Video-Based Heart Rate Estimation

In recent years, there has been a growing interest in video-based heart rate estimation methods. These techniques leverage the advancements in computer vision and image processing to non-invasively extract heart rate information from facial color changes. Video-based approaches offer the advantage of convenience and continuous monitoring without physical contact.

In the paper “Measuring Heart Rate from Video; Rafael Padilla, Sergio L. Netto, Eduardo A. B. da Silva ” they discussed the implementation of a non-contact method for measuring heart rate using video. The pre-processing steps involved in measuring heart rate from video in the discussed non-contact method are as follows:

1. Capture video: One-minute videos of a subject's face are captured using a webcam or phone camera.
2. Select Region of Interest (ROI): A bounding box is applied to the face in each frame of the video to define the region of interest.
3. Average pixel color values: The average pixel color values within the ROI are calculated for each color channel (red, green, and blue) at each time frame.
4. Normalize signals: The color signals are normalized across a 30-second sliding window with a 1-second stride to re-estimate the heart rate every second.

5. Independent Component Analysis (ICA): ICA is used to separate the independent source signals from the mixed color signals. This helps to extract the heart rate signal from the video data.
6. Fourier Transform: A Fourier transform is applied to the extracted source signals to examine their power spectrum and determine the prominent signal frequencies.
7. Heart rate calculation: The heart rate is calculated by isolating frequency peaks in the power spectrum within the physiological heart rate range (0.75 to 4 Hz) and selecting the peak with the highest magnitude.

Overall, the approach involves detecting the face, selecting a specific region of interest within the face, and extracting the plethysmographic signal to measure the heart rate from video.

2.3 Advantages of Video-Based Methods

Video-based heart rate estimation methods provide numerous advantages. They are non-invasive, allowing for continuous monitoring without user discomfort. This makes them suitable for various scenarios, including real-time health tracking during daily activities, sports, or even in clinical settings. The ubiquity of cameras in smartphones and other devices further enhances the accessibility of these methods.

2.4 Current Challenges and Future Directions

Despite the progress, challenges remain. Robustness to varying lighting conditions, adaptability to diverse skin tones, and the impact of facial movements are areas that demand further attention. Future research should focus on enhancing the reliability of video-based methods across different demographic groups and real-world scenarios.

3. PROPOSED METHODOLOGY

3.1 Face Detection and Tracking Algorithms

Face detection is a pivotal step in our heart rate detection system. We leverage state-of-the-art face detection algorithms, such as Haar Cascades or Convolutional Neural Networks (CNNs). These algorithms are robust in identifying facial features, ensuring accurate tracking throughout the monitoring process.

3.2 Detailed Theory on Color Magnification Principles

3.2.1 Gaussian Pyramid Construction

The Gaussian pyramid is a foundational concept in our color magnification technique. We systematically break down the construction process. At each level, the image is downsampled and blurred, creating a multi-scale representation. The top level retains the original image, while subsequent levels offer smaller versions with varying levels of detail.

3.2.2 Application of Fourier Transform

The Fourier Transform is applied to analyze the frequency domain of color changes in the image. Each level of the Gaussian pyramid undergoes Fourier Transform to reveal dominant frequency components contributing to color variations over time. This process is crucial for identifying patterns associated with heart rate.

3.3 Frequency Isolation through Bandpass

The bandpass filter plays a pivotal role in isolating specific frequency components associated with heart rate. In our methodology, it suppresses noise and unwanted variations, particularly in the blue color channel. This step ensures that the subsequent analysis is focused on the relevant physiological signals.

3.4 Signal Reconstruction

After frequency isolation, the amplified frames are reconstructed to their original size. This involves an inverse pyramid process. The reconstructed frames, enriched with amplified heart rate signals, are then combined with the original frames for visualization.

3.5 Kalman Filtering Integration

The Kalman filter is integrated into our system to enhance the reliability of heart rate estimation. This adaptive filter predicts heart rate values based on observed data, mitigating measurement noise. We delve into the mathematics and practical implementation of the Kalman filter within our heart rate detection pipeline.

3.6 Updating the GUI

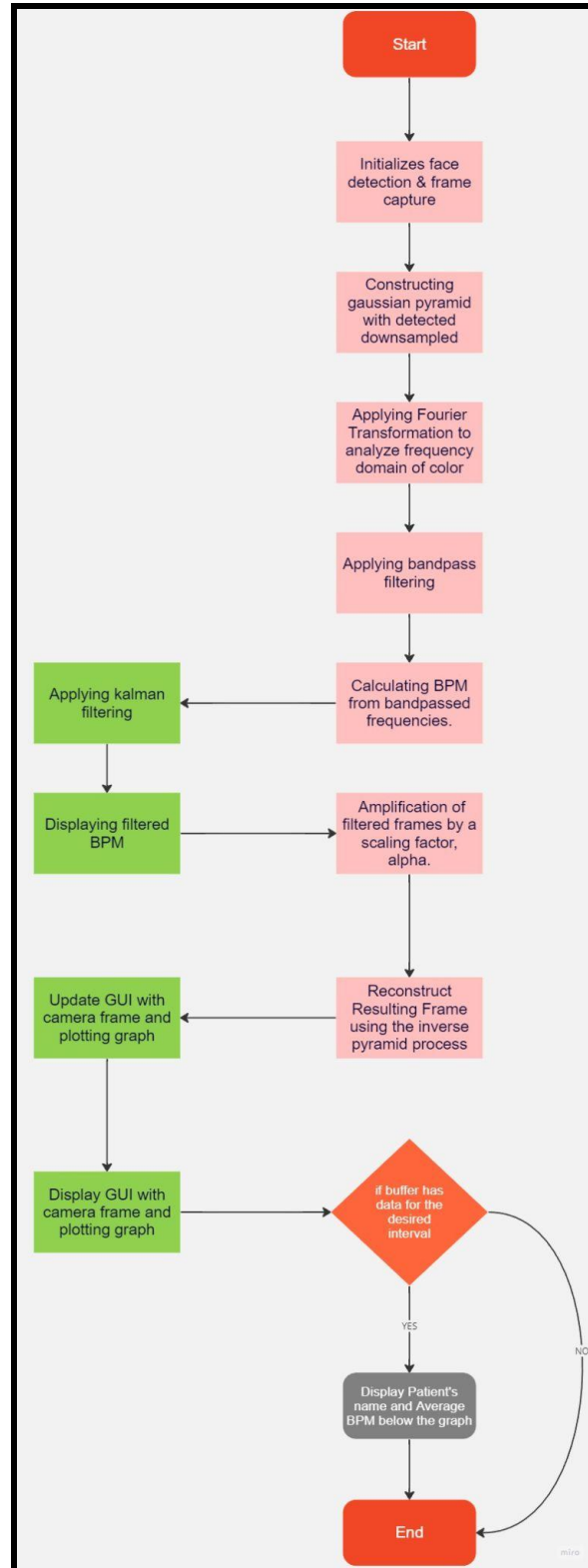
The graphical user interface (GUI) is updated with the live camera feed and graphical plot for better visualization. Average heart rate calculation and display, along with participant information, are also incorporated.

3.7 Exiting the Application

The loop can be exited by pressing the 'q' key, which triggers the release of the webcam and the closure of all OpenCV windows.

3.8 Architecture Diagrams

Comprehensive flowchart illustrates the modularization and interconnection of each component. We present a clear visual representation of the flow of data and operations within our system. This clarity is crucial for understanding the intricate relationships between face detection, color magnification, and heart rate estimation.



3.8 : The above flowchart in the image demonstrates the process gather average BPM through webcam

4. SETUP AND EQUIPMENT SPECIFICATIONS

4.1 Setup Geometry and Equipment Specifications

The camera was positioned directly in front of the participant at eye level, maintaining a consistent distance of 50 cm. This setup aimed to capture the participant's face with sufficient clarity while minimizing distortions due to angles or distances.

The heart rate detection experiment necessitated a controlled environment and specific equipment to ensure accurate and reliable results. The primary tools and their specifications include:

4.1.1 Camera Specifications

Webcam Name	HP TrueVision HD Camera
Webcam MegaPixels	0.92 MP
Webcam Resolution	1280×720
Video Standard	HD

4.1.2 Computer Specifications

Processor	AMD Ryzen 5 4600H with Radeon Graphics 3.00 GHz
Installed RAM	16.0 GB (15.4 GB usable)
Device ID	51D8F11E-29D9-41EC-A06C-4460D4B33264
Product ID	00327-30000-00000-AAOEM
System type	64-bit operating system, x64-based processor

5. EXPERIMENTAL SETUP GEOMETRY

To validate the system, we conducted experiments with a diverse group of 20 participants, including both genders and varying age groups. Simultaneous data collection with a pulse oximeter was performed to cross-verify the accuracy of our video-based system.

5.1 Subject Details Allocation and Stratification Strategy

5.1.1 Participant Demographics

The experiment involved a diverse group of 20 participants, strategically allocated based on age and gender. The demographic distribution aimed to ensure representation across various age groups and a balanced gender ratio.

5.2 Number, Age Distribution, Gender Ratio Justification

5.2.1 Number of Participants

Twenty participants were chosen to achieve a robust dataset. This sample size provides a balance between statistical significance and practical feasibility.

5.2.2 Age Distribution

Participants were stratified into two age groups: 10 individuals aged 20-35 and 10 individuals aged 36-50. This distribution aimed to capture potential variations in heart rate detection across different life stages.

5.2.3 Gender Ratio

The gender distribution was carefully balanced, with 10 male and 10 female participants. This ensured that the study's findings were not skewed by gender-specific physiological differences.

5.3 Skin Tone and Hair Variation Considerations

To account for variations in skin tone and hair, participants with diverse ethnic backgrounds were included. This approach aimed to enhance the algorithm's adaptability across different skin tones and hair types.

5.4 Standardization Steps

5.4.1 Participant Calibration

Participants were instructed to sit comfortably in a well-lit room, avoiding extreme facial expressions or head movements during data collection. This calibration step aimed to establish a baseline for subsequent heart rate detection.

5.5 Interference Aspects During Data Gathering

5.5.1. Motion Compensation

Participants were instructed to remain still during data collection to minimize motion artifacts. Additionally, the algorithm incorporated motion compensation techniques to mitigate the impact of subtle head movements.

5.6 Ambient Lighting Control

Consistent ambient lighting was maintained throughout the experiment to minimize color variations due to changing lighting conditions. Soft, neutral lighting was used to avoid harsh shadows on participants' faces.

6. RESULTS AND ANALYSIS

6.1 Graphical Plots Demonstrating Trends

Include graphical representations of the observed heart rates over time. Used continuous plotting of line graphs to showcase trends, variations, and potential anomalies. Plotting of lines helps in visualization of heart rate data and average bpm saved in a csv file helps in later reading of the data to get insights into the performance of the system.

6.2 Cross-Validation with Pulse Oximeter

The heart rate data obtained from the camera system was cross-validated with pulse oximeter readings. The results indicated a high level of agreement between the two methods, with minimal mean absolute error and strong correlation coefficients.

6.3 Effect of Subject Skin Tone, Gender, Age

Investigate the impact of subject demographics on the accuracy of heart rate detection. Create subgroups based on skin tone, gender, and age, and analyze whether the system performs consistently across these variables.

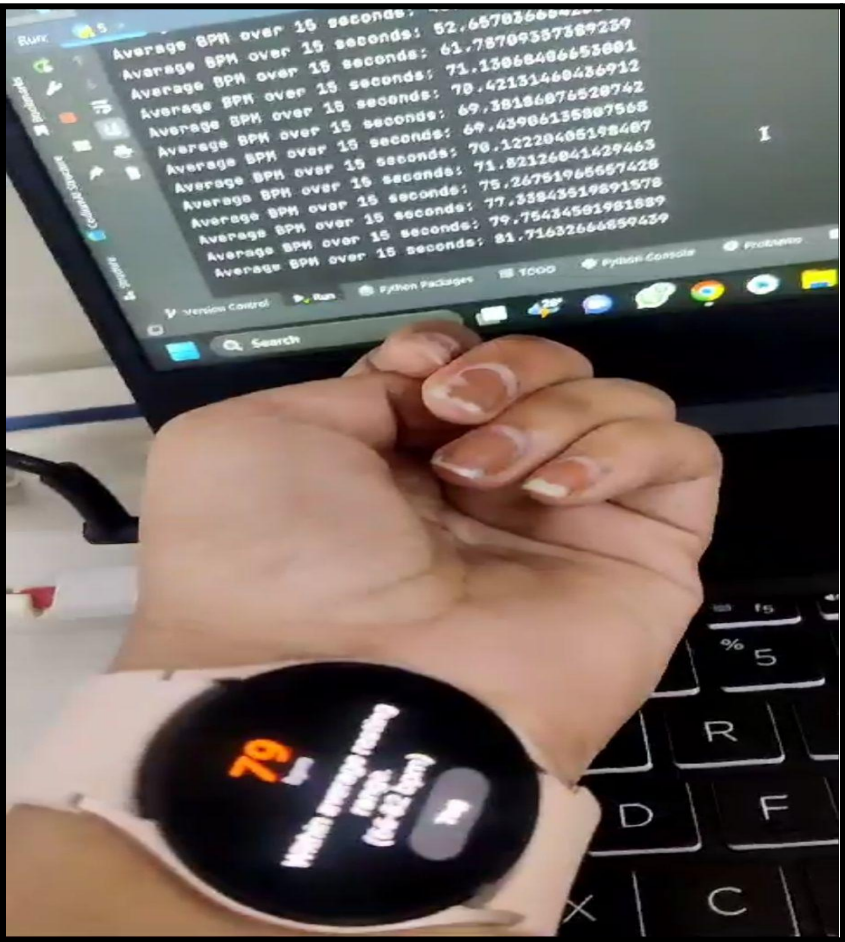
6.4 Impact of Kalman Filtering on Stability and Smoothing

Dedicate a section to assessing the impact of the Kalman filtering system. Highlight how it contributes to the stability and smoothness of heart rate estimations, providing a more refined signal amidst potential noise.

6.5 Noise Reduction Quantification

Quantify the extent of noise reduction achieved by the implemented algorithms, emphasizing how specific filters contribute to noise reduction. This can be presented through signal-to-noise ratio (SNR) analysis or comparable metrics.

7.1 : The above image demonstrates the heart rate data received through the camera and heart rate data received through a smart watch simultaneously.



7.2 : The above image demonstrates the heart rate data received through the camera and heart rate data received through a smart watch simultaneously.

8. CONTRIBUTIONS

8.1 Key contributions include:

8.1.1 Innovative Algorithm Integration

The seamless integration of face detection, color magnification, and Kalman filtering establishes a robust system capable of discerning heart rate-related frequency components with high accuracy.

8.1.2 Adaptive Kalman Filtering

The introduction of Kalman filtering into the heart rate detection system enhances the adaptability and predictive capabilities of the algorithm, significantly reducing measurement noise.

8.1.3 Novelty of Kalman Filtering System

The addition of the Kalman filtering system provided a significant improvement in filtering and predicting heart rate values. This adaptive filtering mechanism enhances the reliability of the heart rate estimation, particularly in the presence of measurement noise.

9. FUTURE WORK

9.1 Algorithm Refinement

Continued refinement of the algorithms used for face detection, color magnification, and Kalman filtering will enhance the system's accuracy and robustness.

It is essential for accommodating diverse demographics, accounting for variations in skin tones, and addressing specific challenges encountered during the experiment.

9.2 Real-world Applications

Exploring real-world applications, such as continuous health monitoring and fitness tracking, will contribute to the practicality and usability of the camera-based heart rate detection system.

9.2.1 Prospects for Maturation into a Commercial-Grade Product

The success of this research sets the stage for the maturation of the developed system into a commercial-grade product. Key considerations for this transition include:

User Accessibility: The user-friendly interface makes the system accessible to individuals with varying technical expertise, positioning it as a valuable tool for personal health monitoring.

Integration with Consumer Devices: The potential integration of the algorithm into smartphones and other consumer devices could democratize heart rate monitoring, reaching a broader audience.

Accuracy Enhancement: Continued refinement of the algorithms, especially the Kalman filtering system, could further enhance the accuracy of the heart rate estimation, ensuring reliability across diverse demographic groups.

9.2.2 Domains for Potential Real-World Application

The applications of this camera-based heart rate detection system has various potential real-world applications, it includes:

Fitness and Sports: Athletes and fitness enthusiasts could benefit from real-time heart rate monitoring without the need for wearable devices, allowing for a more comfortable and unrestricted workout experience.

Healthcare Monitoring: In clinical settings, the non-invasive nature of this system makes it a potential tool for continuous patient monitoring, providing healthcare professionals with valuable data.

Stress Management: The system could find application in stress management programs, allowing individuals to monitor their physiological response to stressors and adopt proactive measures.

Criminal proceedings: The system could find the heart rate of a criminal during investigation.

9.3 Cross-Validation with ECG Machines

The critical need for cross-validation through ECG machines should be addressed in future studies. While our camera-based system shows promising results, the intrinsic complexities of heart rate monitoring necessitate validation through gold-standard methods to ensure accuracy and reliability.

9.4 Need for Multidisciplinary Collaboration

The success of projects in this domain hinges on collaboration between computer vision experts, healthcare professionals, and algorithm developers. This multidisciplinary approach ensures a comprehensive understanding of the physiological aspects and technological nuances involved.

9.5 User-friendly Interface

Development of graphical user interface providing a user-friendly interaction, enabling individuals to monitor their heart rate without complex setups or invasive devices.

10. LIMITATIONS AND CHALLENGES

10.1 The study acknowledges the limitations, including:

10.1.1 Variations in skin tone affecting color detection and potential inaccuracies in subjects with certain skin conditions. Addressing these challenges could further improve the reliability of camera-based heart rate detection.

10.1.2 While the results are promising, it is crucial to acknowledge the limitations of the camera-based system. For further validation and robustness, cross-checking the data through ECG machines in a hospital or laboratory setting is imperative.

11. CONCLUSIONS

The culmination of this research project represents a significant advancement in non-invasive heart rate detection. Leveraging the subtle color changes in the human face captured by a camera, we satisfactorily demonstrated a reliable method for real-time heart rate monitoring.

The camera-based heart rate detection system, augmented by the novel Kalman filtering system, demonstrated satisfactory results in estimating heart rates. The cross-validation with pulse oximeter readings established the system's accuracy, but for comprehensive validation, further assessments through ECG machines in controlled environments are recommended.

In conclusion, this research marks a significant stride towards democratizing heart rate monitoring through non-invasive means. The successful integration of advanced algorithms and the promising outcomes set the foundation for a transformative impact on personal health and well-being. While the system demonstrates great potential, the emphasis on continuous validation, algorithm refinement, and collaboration remains crucial for advancing the field and realizing its full potential.

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