



SiPM Single Photon Timing Resolution

Stefan Gundacker^{1, 2}

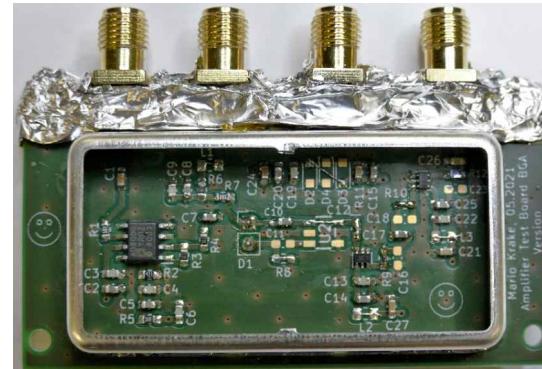
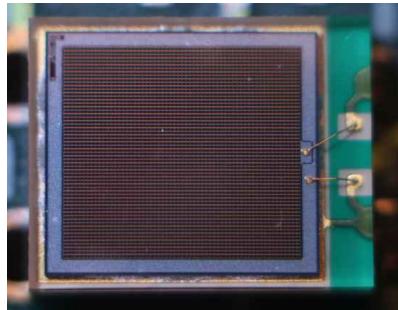
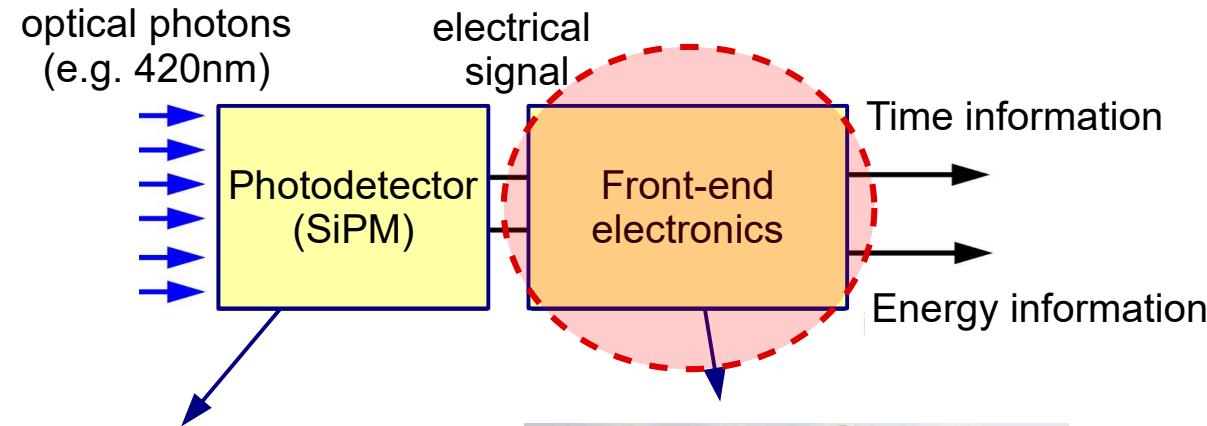
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² Department of Physics of Molecular Imaging Systems (PMI), RWTH Aachen University, Aachen, Germany

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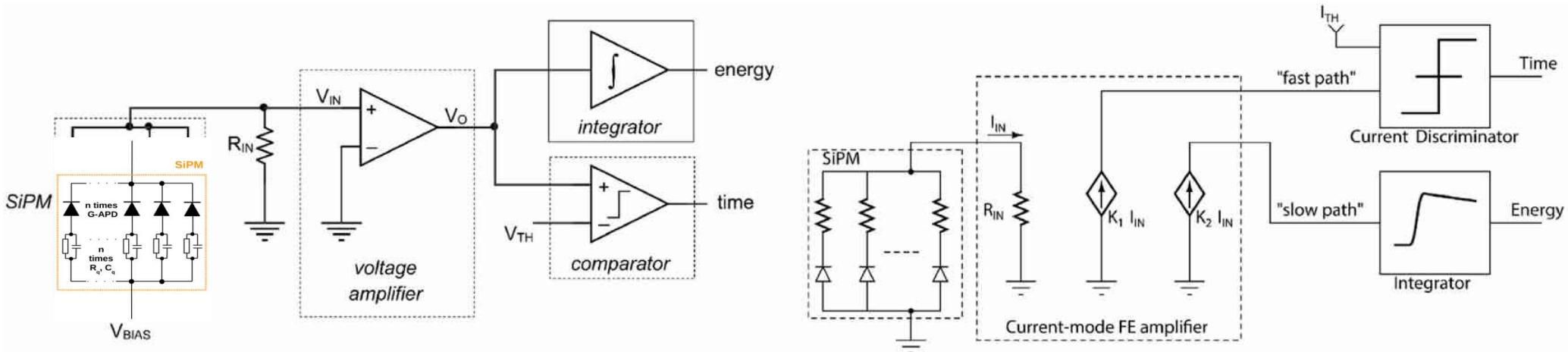
Electronic readout concepts of SiPMs

Reading the SiPM signals



F. Acerbi and S. Gundacker, "Understanding and simulating SiPMs", Nuclear Inst. and Methods in Physics Research, A 926 (2019) 16–35

Front-end basics



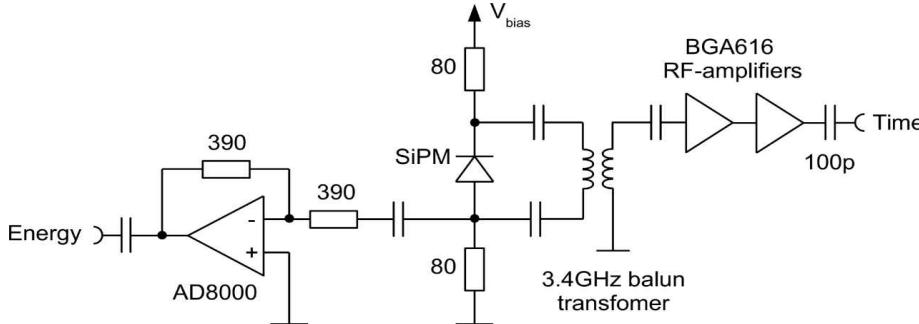
Voltage readout:

- senses the voltage drop on R_{IN}
- potentially very high bandwidth
- small signal amplitudes for large active SiPM areas
- e.g. Radioroc, **HF-readout**

Current readout:

- measures the current or charge directly
- bandwidth limited by large passive C of SiPM
- signal height theoretically not altered by SiPM active area (for low frequencies)
- e.g. TOF-PET2 ASIC, **NINO**

High-frequency readout as test vehicle



This design pushed forward the state-of-the-art, especially in understanding the SPTR.

J. Cates et.al,
Phys. Med. Biol. 63 185022, 2018, <https://doi.org/10.1088/1361-6560/aabdc0>

S. Gundacker et.al.
Phys. Med. Biol. 64 055012, 2019, <https://doi.org/10.1088/1361-6560/aafdf2>

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Phys. Med. Biol. 63 (2018) 185022 (11pp)

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PAPER

Improved single photon time resolution for analog SiPMs with front end readout that reduces influence of electronic noise

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Keywords: silicon photomultiplier, single photon time resolution, timing resolution

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Phys. Med. Biol. 64 (2019) 055012 (9pp)

<https://doi.org/10.1088/1361-6560/aafdf2>



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PAPER

High-frequency SiPM readout advances measured coincidence time resolution limits in TOF-PET

Stefan Gundacker^{1,*}, Rosana Martinez Tortos², Etienne Auffray¹, Marco Paganoni¹ and Paul Lecoq²

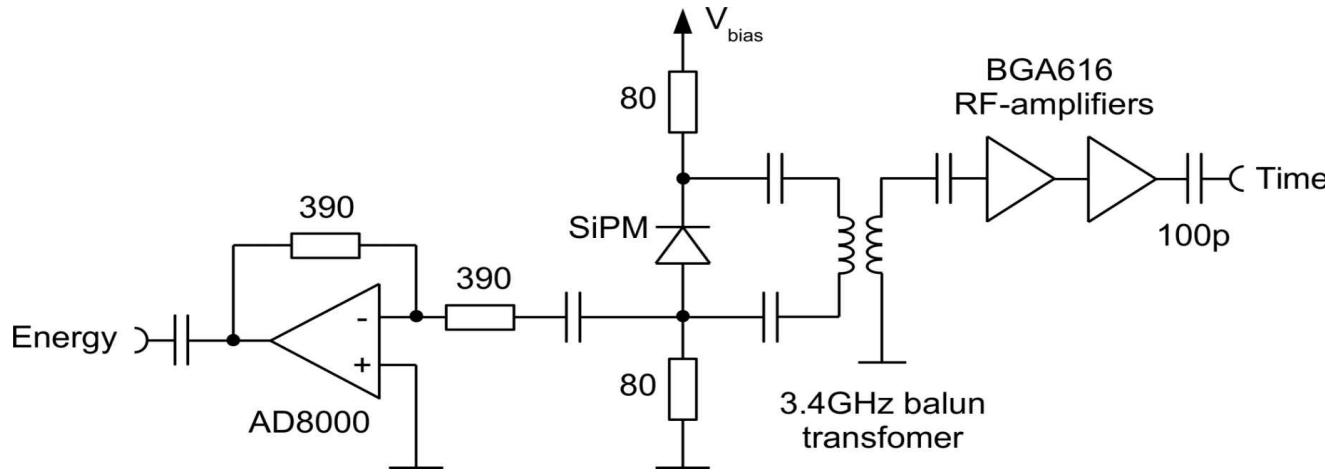
¹ UniMiB, Piazza dell'Ateneo Nuovo, 1—20126, Milano, Italy

² CERN, 1211 Geneva 23, Switzerland

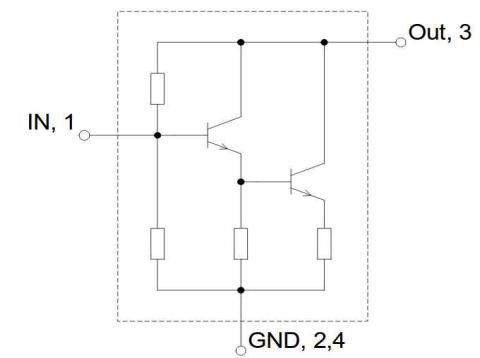
E-mail: stefan.gundacker@cern.ch

Keywords: high-frequency electronics, TOF-PET, ISO:Ce codoped with Ca, fast timing, coincidence time resolution, single photon time resolution, Cherenkov emission in scintillators

High-frequency readout as test vehicle



BGA616 data sheet

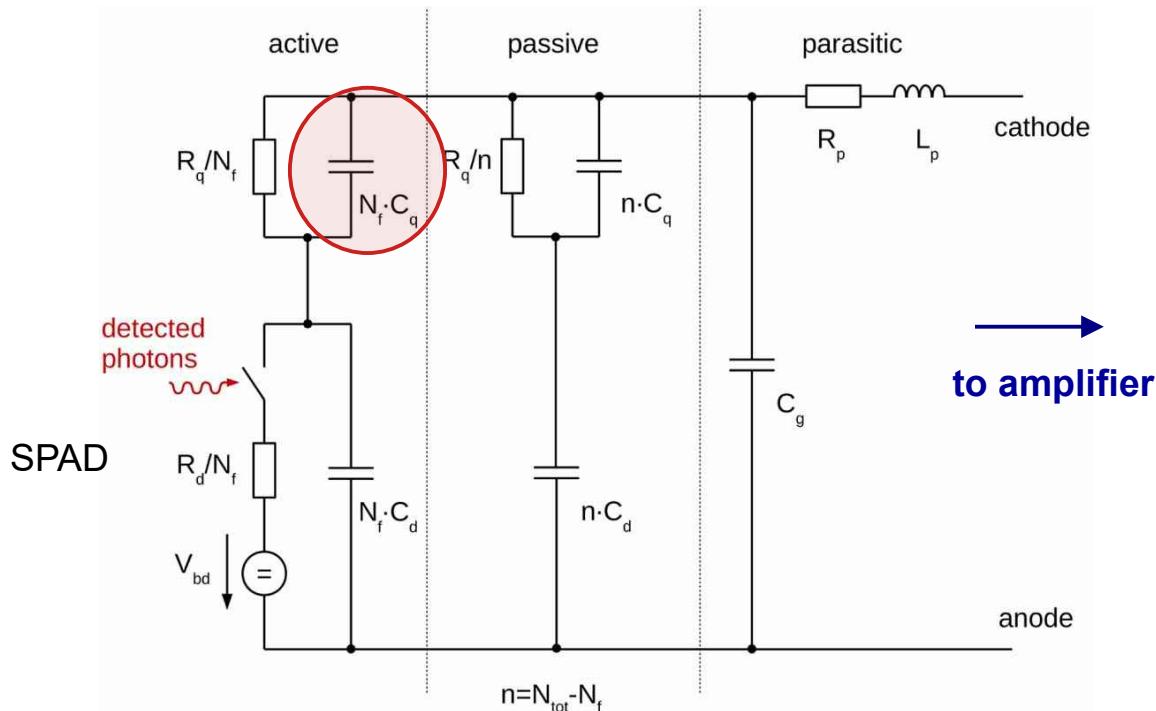


- BGA616 RF-amplifier reads SiPM differentially via RF balun
- High-frequency path via SPAD quenching capacitance C_q
- High frequency for time ~ 1.5 GHz bandwidth
- **Minimizes the impact of electronics to the timing performance of the SiPM**

J.W. Cates, S. Gundacker, E. Auffray, P. Lecoq and C.S. Levin, "Improved single photon time resolution for analog SiPMs with front end readout that reduces influence of electronic noise", Phys. Med. Biol. 63 (2018) 185022 (11pp)

High-frequency path via quenching C_q

SiPM equivalent circuit:



Working principle:

- capacitive divider of signal to SiPM anode-cathode
- signal amplitude proportional to SiPM area (terminal C)
- voltage readout with high-bandwidth MMIC, RF amplifiers
- no bandwidth limitation! (larger 1.5 GHz tested)

Too high power consumption of first prototypes

Amplifier	Supply voltage [V]	Supply current [mA]	Power [mW] (single channel)	Gain [dB]	Noise figure	Price [€/amplifier] (year 2021)
BGA616	6	48	288	19	2.5	1.36

Power consumption of first implementation of HF-amplifiers was above 290mW per channel.

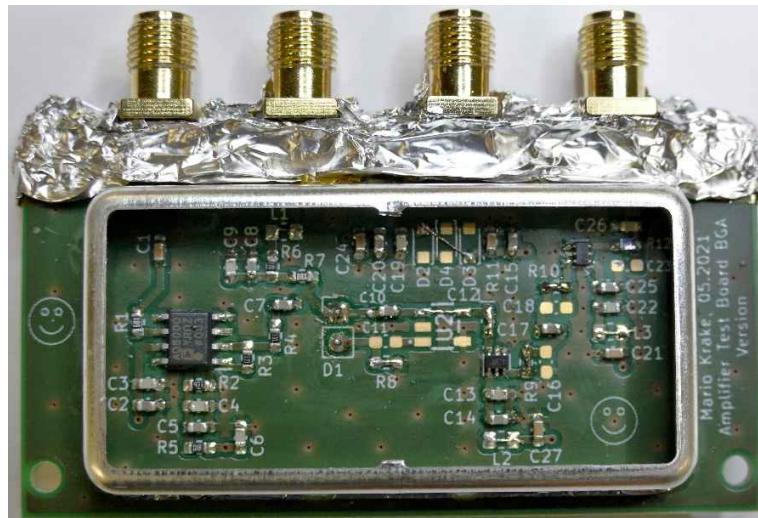
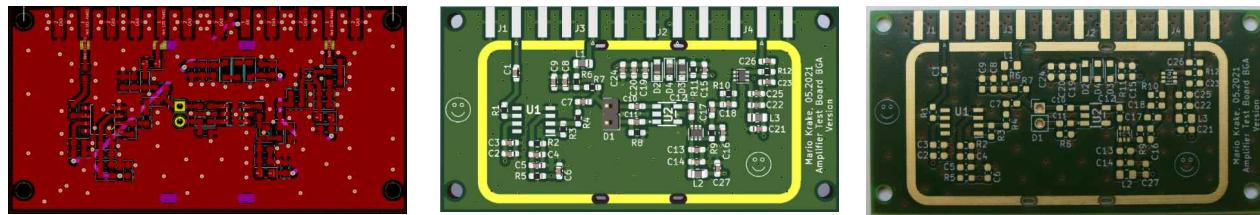
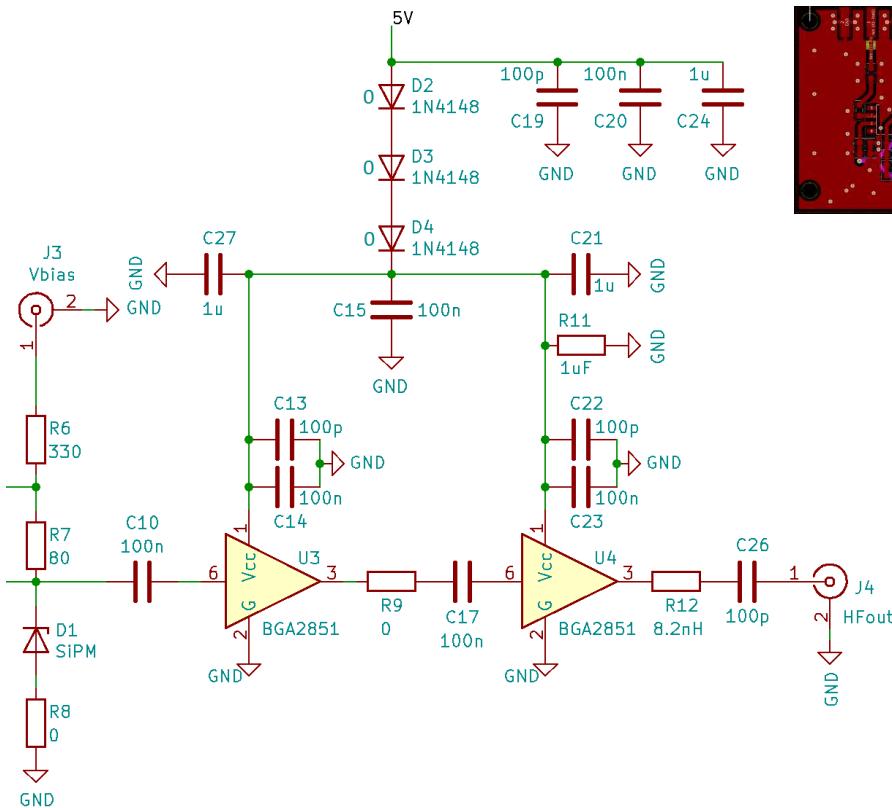
M. Krake, V. Nadig, V. Schulz, and S. Gundacker, "Power-efficient high-frequency readout concepts of sipms for TOF-PET and HEP," NIM A, vol. VCI2022 conference proceeding, submitted 2022.

Low power amplifier types tested

Amplifier	Supply voltage [V]	Supply current [mA]	Power [mW] (single channel)	Gain [dB]	Noise figure	Price [€/amplifier] (year 2021)
BGA616	6	48	288	19	2.5	1.36
BGA2803	3	5.8	17	23.6	3.6	0.291
BGA2851	5	7	35	24.8	3.2	0.32
BGA2869	5	24	120	31.7	3.1	0.362

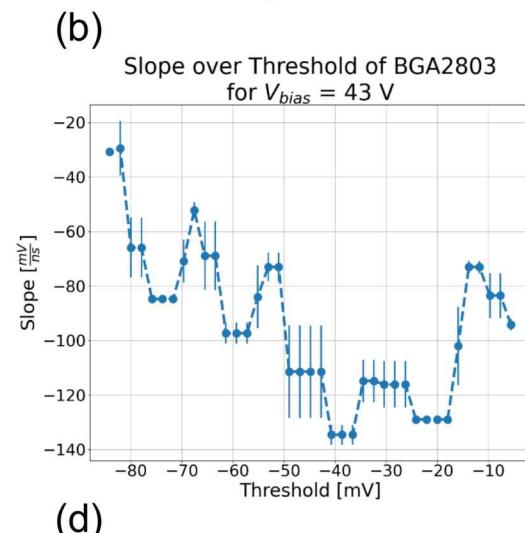
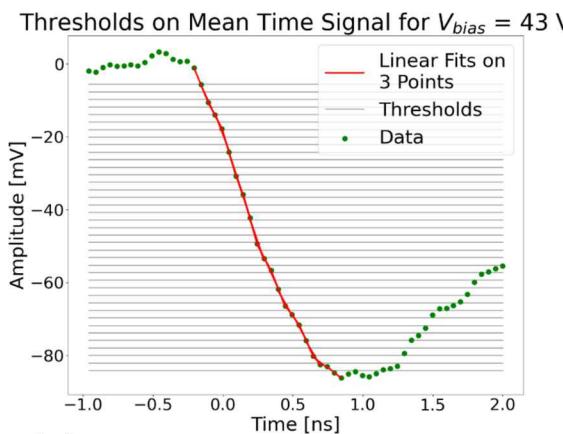
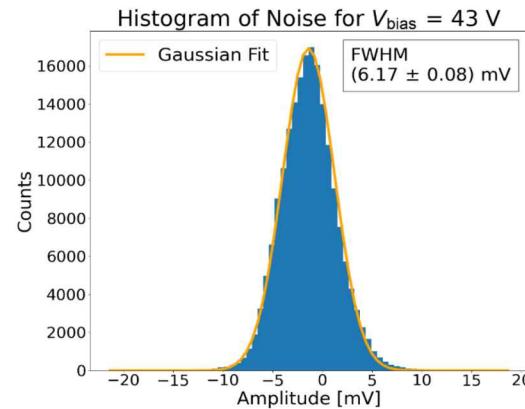
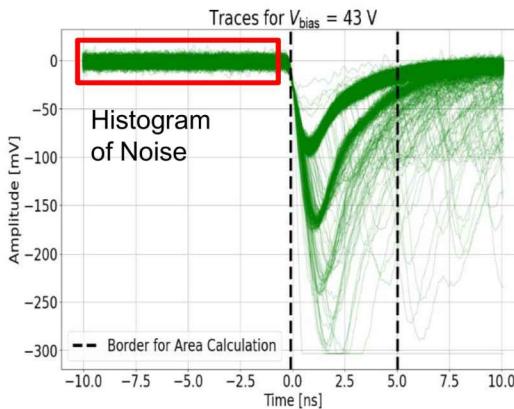
- Bandwidth above 2 GHz for all amplifiers
- Many more types available; a good device for a particular application can always be found

Power-efficient HF implementation



M. Krake, V. Nadig, V. Schulz, and S. Gundacker, "Power-efficient high-frequency readout concepts of SiPMs for TOF-PET and HEP," NIM A, vol. 1039 (2022) 167032

Electronic time resolution with single photons

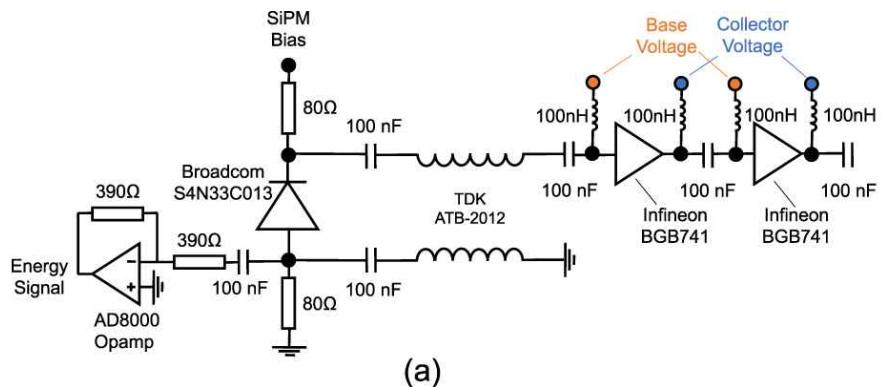


- Noise amplitudes before single photon signal (a) inserted into histogram (b)
- Single photon traces are averaged (c) and dV/dt at different thresholds calculated (d)
- The electronic time resolution is calculated:

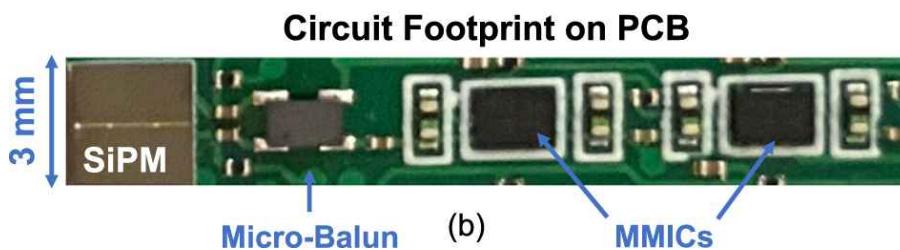
$$TR_{SPAD} = \frac{FWHM_{Noise}}{dV/dt_{@threshold}}$$

All amplifiers tested similar performance in TR_{SPAD} .

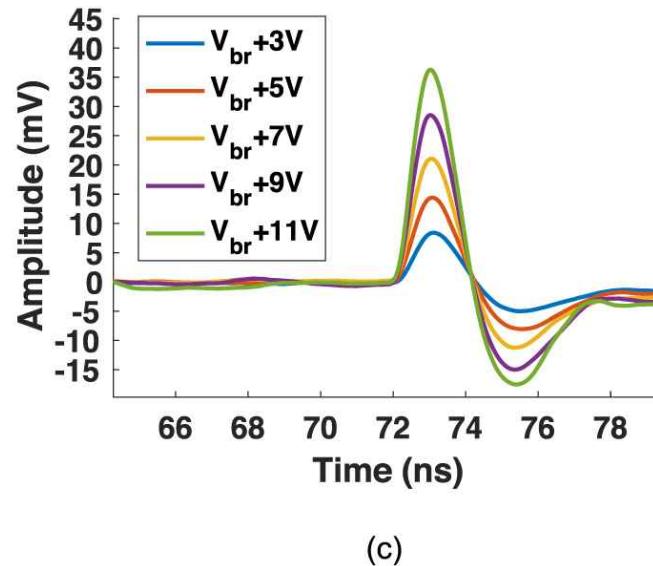
Another example of low power implementation



(a)



(b)

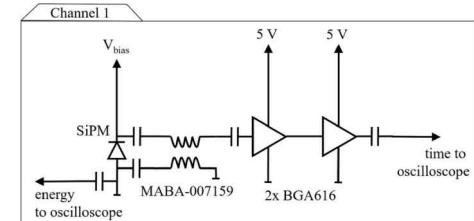


(c)

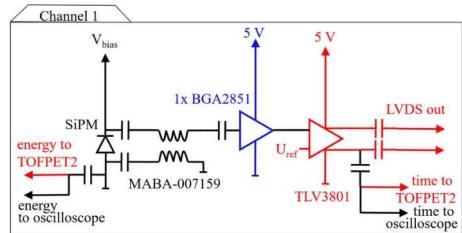
Excellent performance down to 15 mW power consumption per channel.

J. W. Cates and W-S. Choong, "Low power implementation of high frequency SiPM readout for Cherenkov and scintillation detectors in TOF-PET", Phys. Med. Biol. 67 (2022) 195009

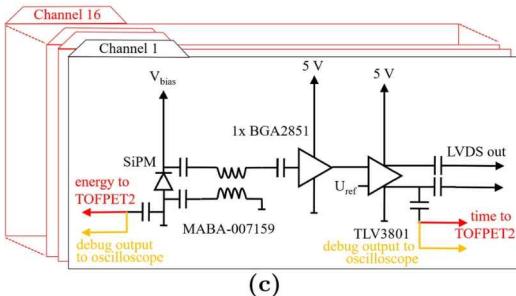
Next step: multichannel HF-readout



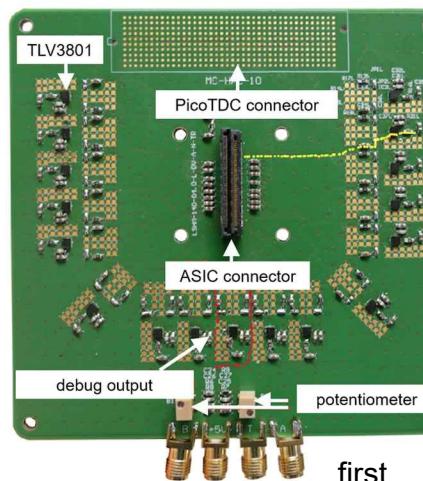
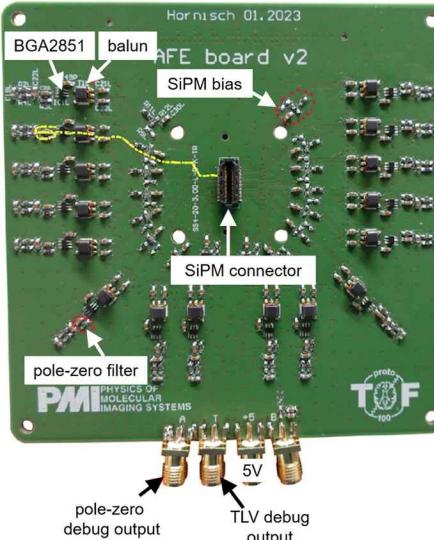
(a)



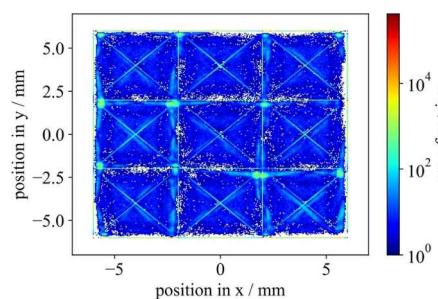
(b)



(c)



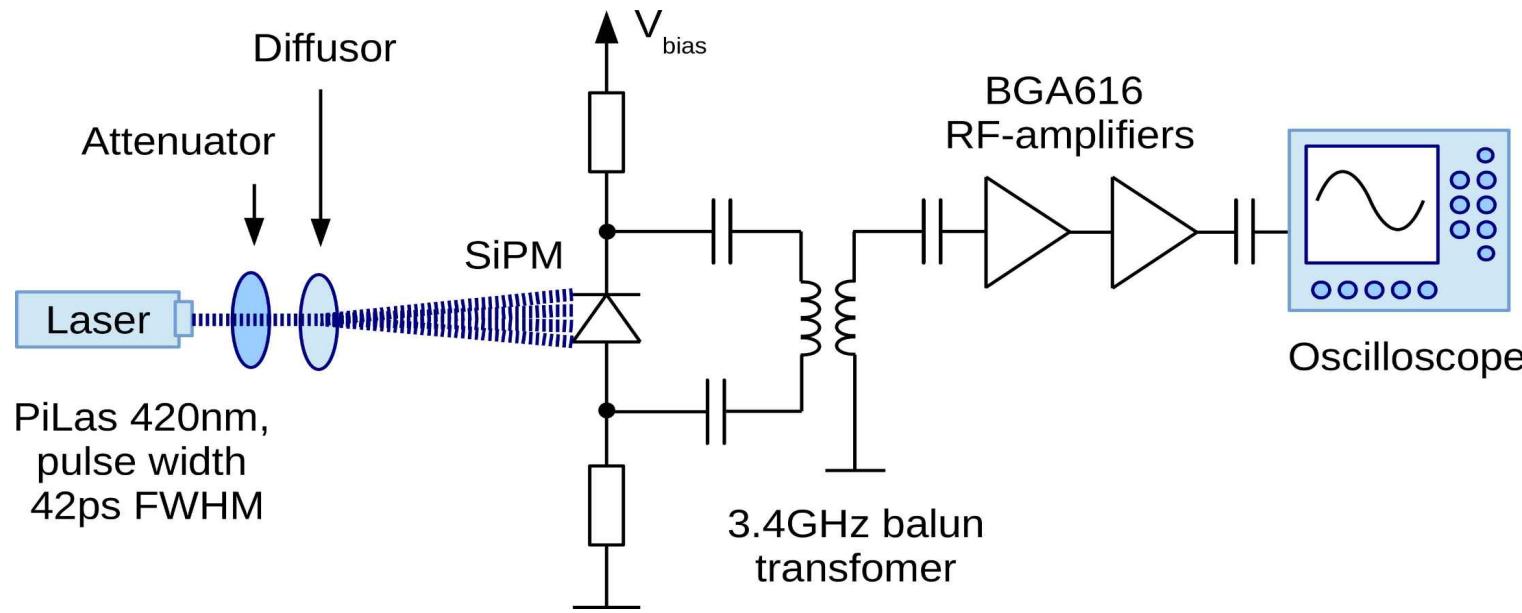
first
prototype



V. Nadig et.al, "16-channel SiPM high-frequency readout with time-over-threshold discrimination for ultrafast time-of-flight applications", EJNMMI Physics (2023) 10/76

SPTR measurement with laser

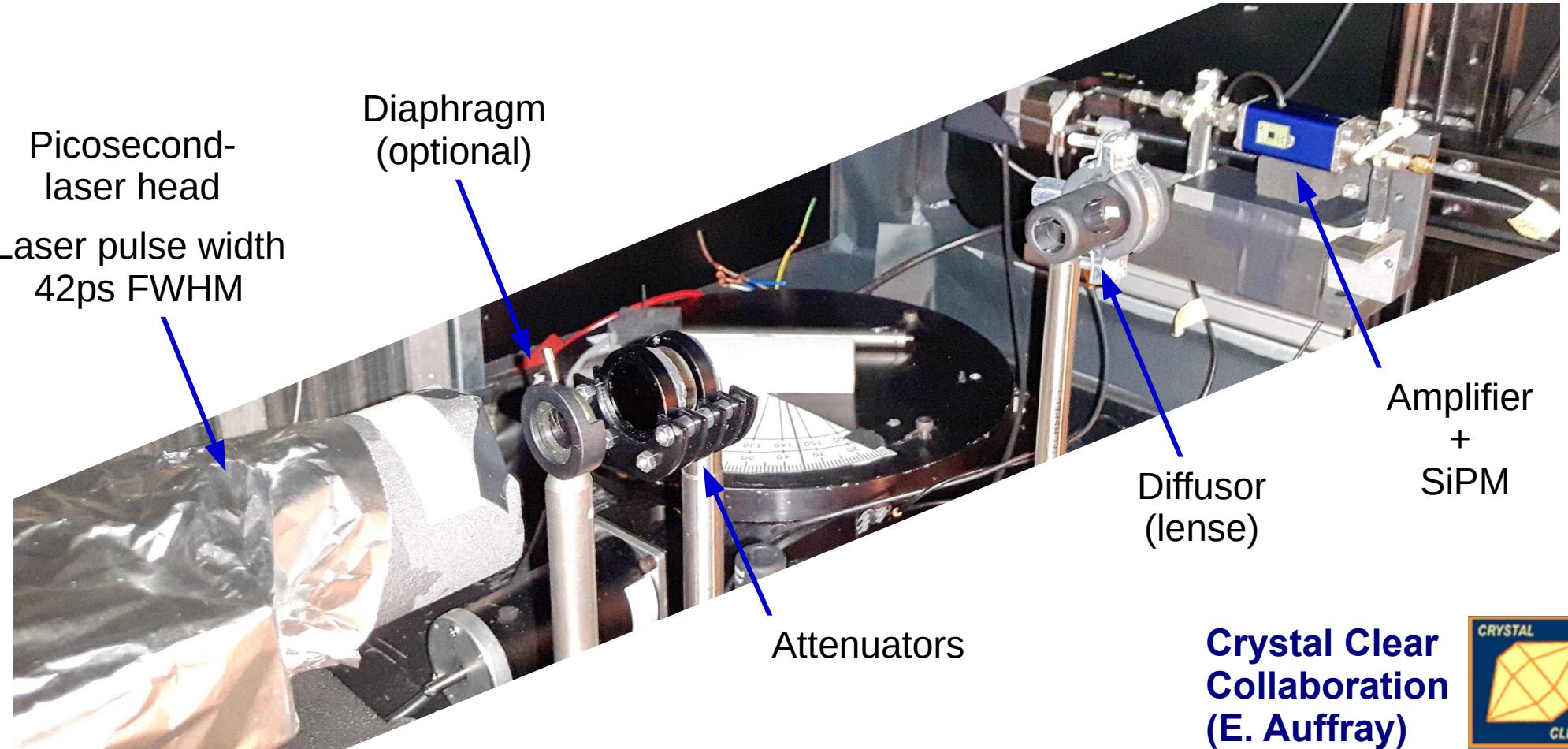
Single photon time resolution (S PTR) setup



J.W. Cates, S. Gundacker, E. Auffray, P. Lecoq and C.S. Levin, "Improved single photon time resolution for analog SiPMs with front end readout that reduces influence of electronic noise", Phys. Med. Biol. 63 (2018) 185022 (11pp)

S. Gundacker et.al, "Experimental time resolution limits of modern SiPMs and TOF-PET detectors exploring different scintillators and Cherenkov emission," Physics in Medicine & Biology, vol. 65, p. 025001, Jan 2020.

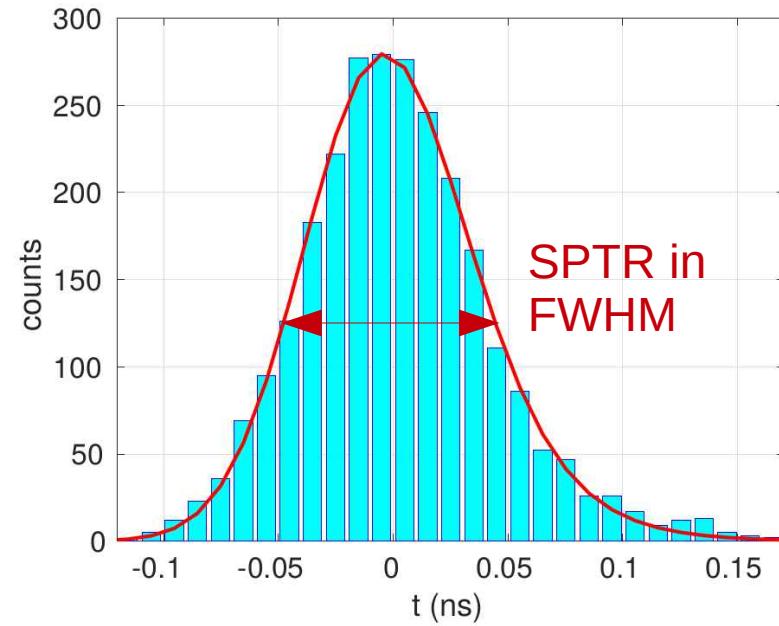
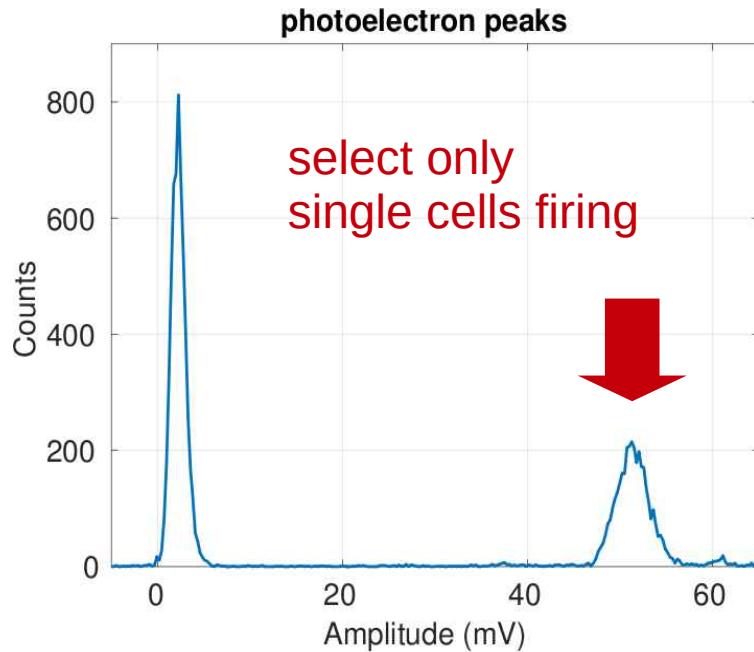
Single photon time resolution setup at CERN



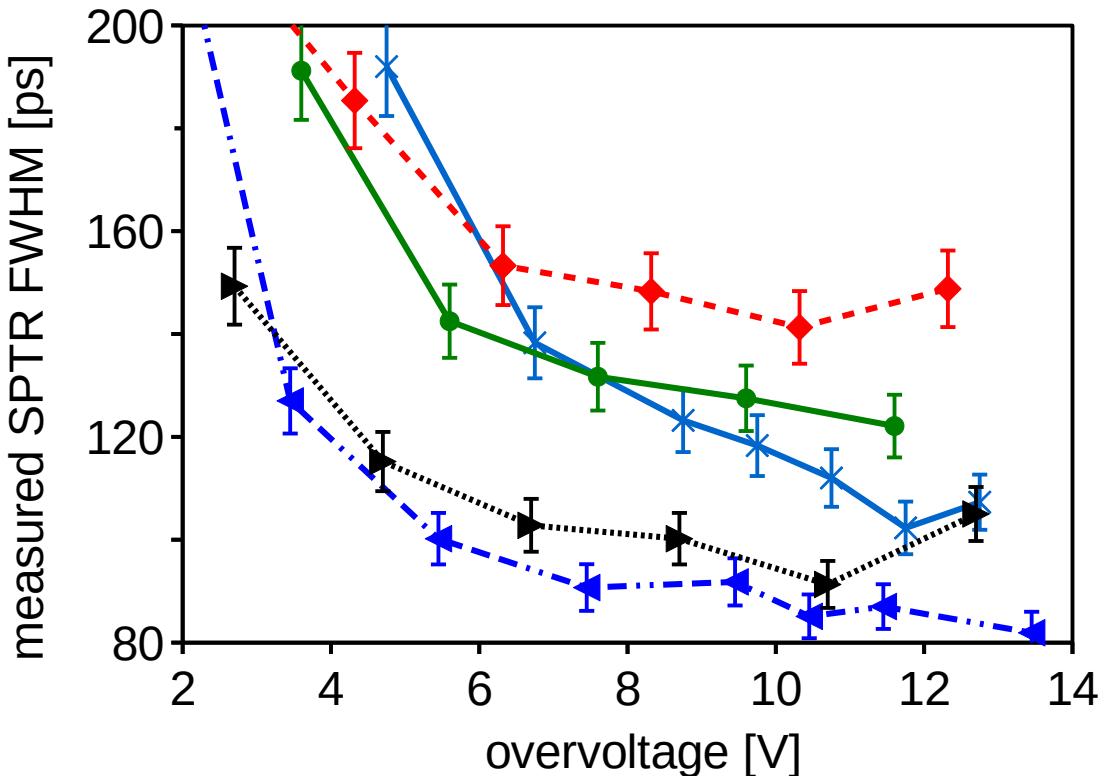
Crystal Clear
Collaboration
(E. Auffray)



SPTR data analysis



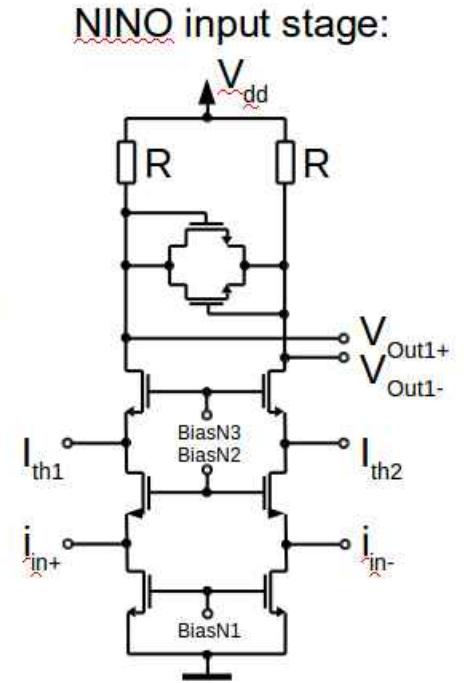
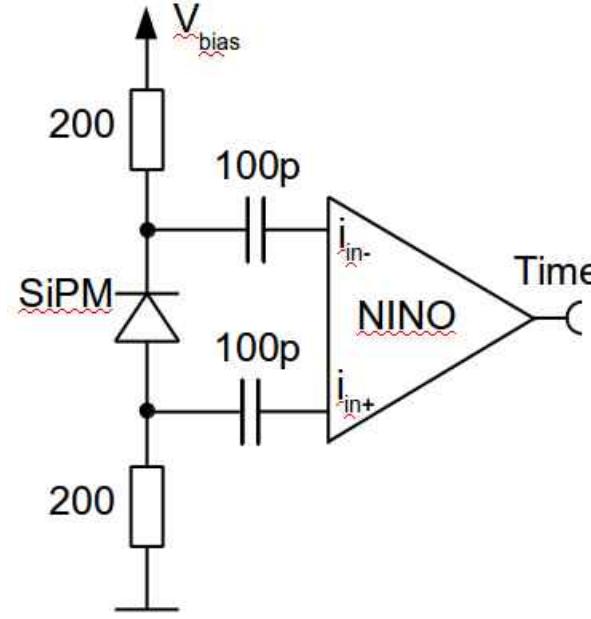
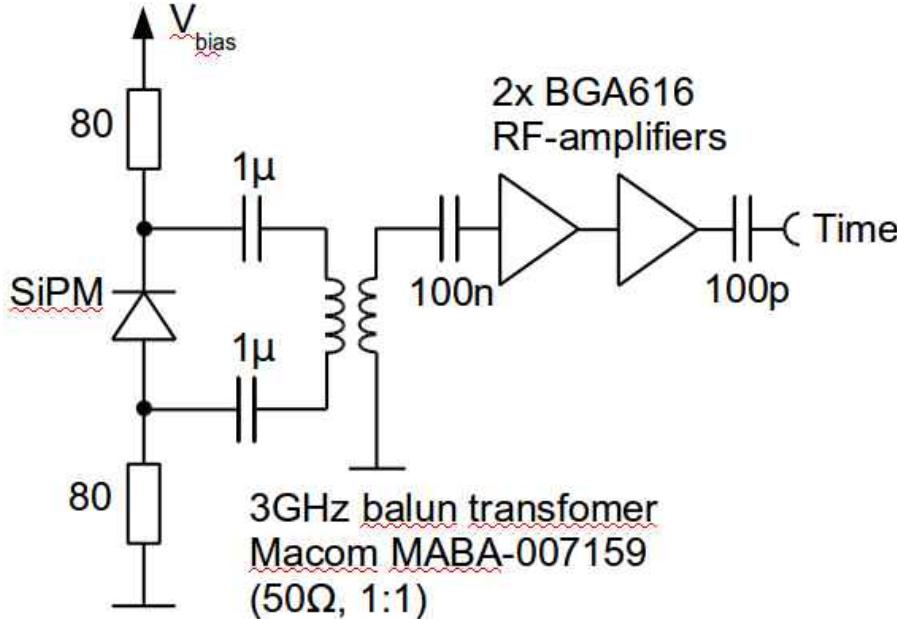
SPTR for different producers with HF-electronics



HPK S13360, 3x3 mm², 50 µm
SensL FJ, 3x3 mm², 35 µm
Broadcom, 4x4 mm², 30 µm
Ketek WBA0, 3x3 mm², 50 µm
FBK NUV-HD, 4x4 mm², 40 µm

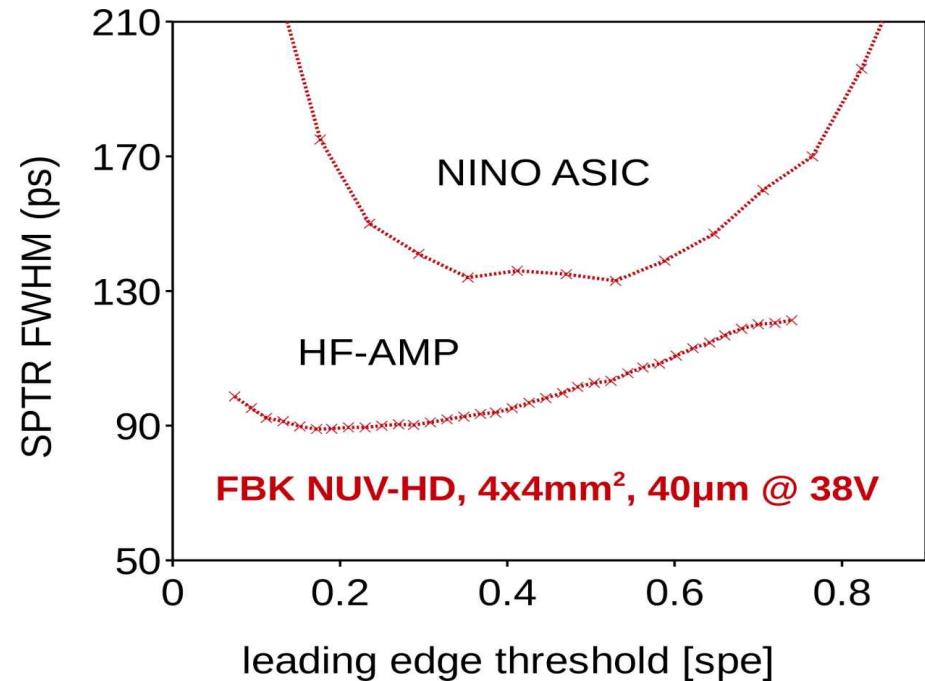
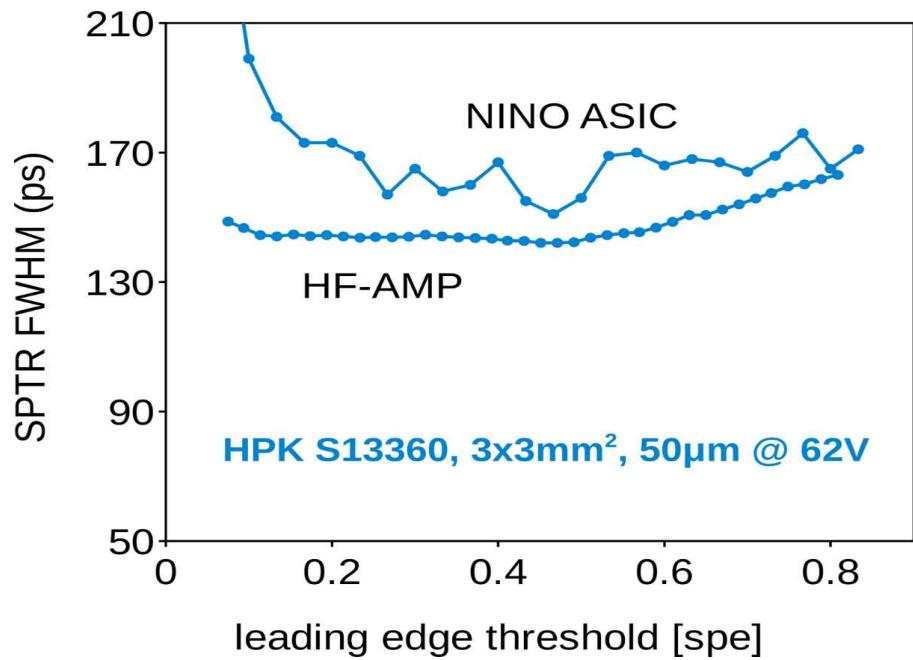
S. Gundacker et.al, "Experimental time resolution limits of modern SiPMs and TOF-PET detectors exploring different scintillators and Cherenkov emission," Physics in Medicine & Biology, vol. 65, p. 025001, Jan 2020.

Comparing HF-electronics with NINO ASIC



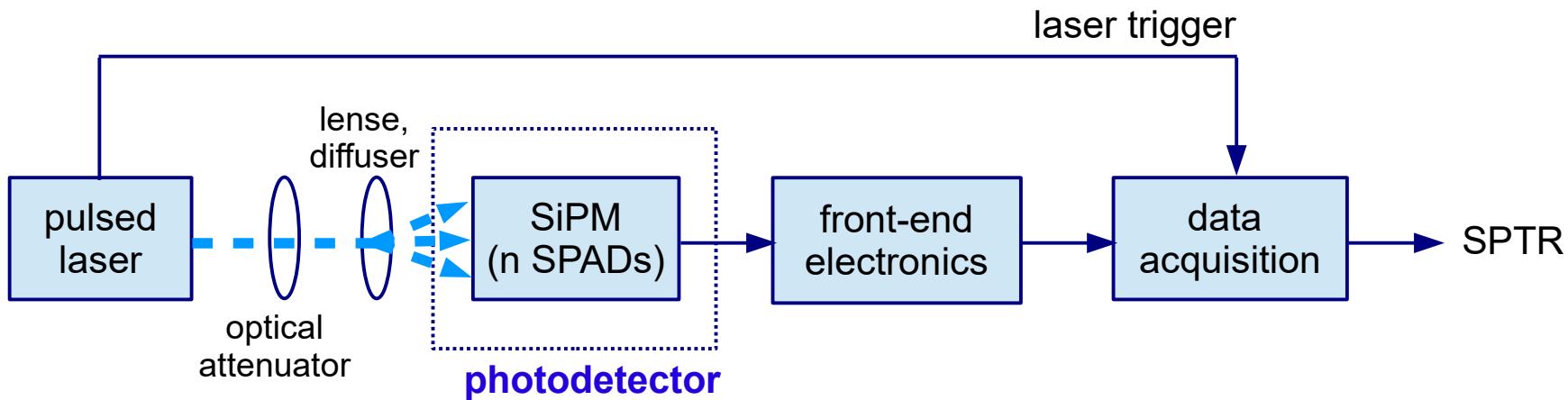
Anghinolfi F, Jarron P, Krummenacher F, Usenko E and Williams M 2004
NINO: aN ultrafast low-power front-end amplifier discriminator for the time-of-flight detector in the ALICE experiment IEEE Trans. Nucl. Sci. 51 1974–8

SPTR with NINO & HF-electronics



S. Gundacker et.al, "High-frequency SiPM readout advances measured coincidence time resolution limits in TOF-PET", Phys. Med. Biol. 64 (2019)

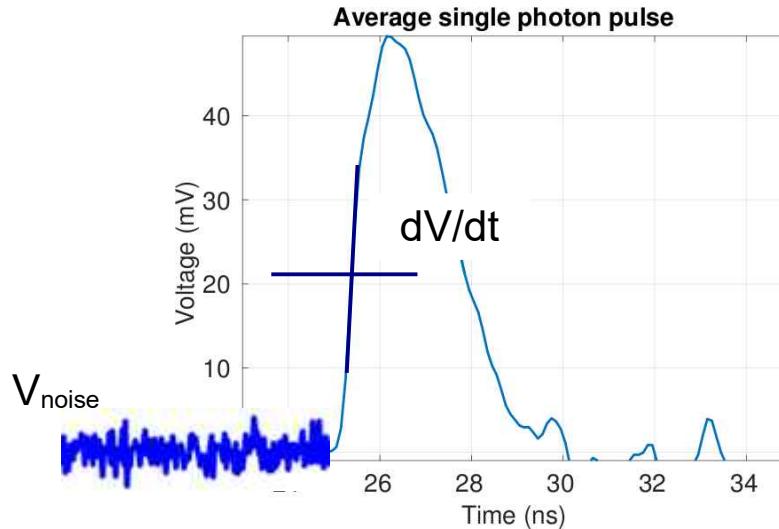
Intrinsic single photon time resolution (S PTR)



$$\text{S PTR}_{\text{measured}} = \text{S PTR}_{\text{intrinsic}} \otimes \text{electronic noise jitter} \left(\frac{V_{\text{noise}}}{dV/dt} \right) \\ \otimes \text{acquisition jitter} \otimes \text{laser pulse shape} \otimes \text{laser trigger jitter}$$

Laser pulse width is 42 ps FWHM
(measured with streak-camera).

Electronic noise jitter

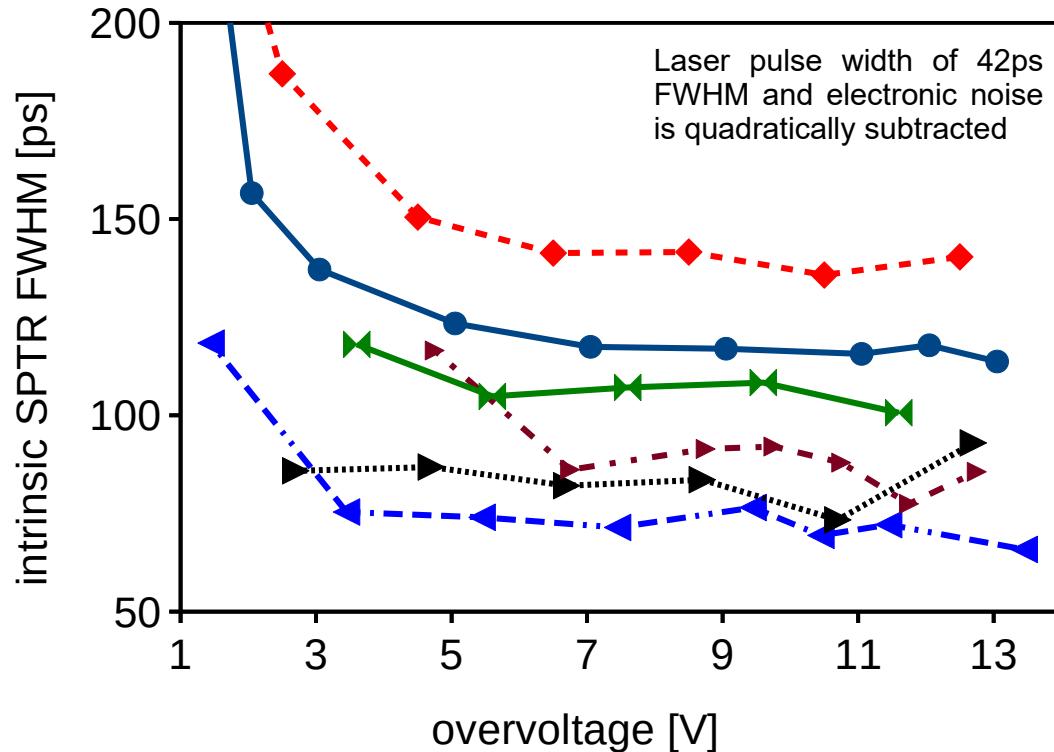


$$\text{electronic noise jitter} = \left(\frac{V_{\text{noise}}}{dV/dt} \right)$$

FBK-NUVHD 4x4 mm² and 40 μm SPAD:

- 10% to 90% rise time of single cell signal is ~700 ps
- maximum dV/dt = 90 V/μs
- noise floor: V_{noise} = 1.07 mV rms
- S PTR_{measured} = 85 ps FWHM @ 39 V bias (S PTR_{intrinsic} = 70 ps FWHM)

Intrinsic S PTR (SiPM uniformly illuminated)



HPK S13360, 3x3mm², 50µm
HPK S14160, 3x3mm², 50µm
SensL FJ, 3x3mm², 35µm
Broadcom, 4x4mm², 30µm
Ketek WBA0, 3x3mm², 50µm
FBK NUV-HD, 4x4mm², 40µm

S. Gundacker et.al, "Experimental time resolution limits of modern SiPMs and TOF-PET detectors exploring different scintillators and Cherenkov emission," Physics in Medicine & Biology, vol. 65, p. 025001, Jan 2020.

Overview of SiPM performances

<i>SiPM producers</i>	<i>PDE [%]</i>	<i>SPTR intrinsic [ps]</i>
HPK S13360 3x3mm ² (50µm)	59 ± 3	135 ± 8
HPK S14160 3x3mm ² (50µm)	57 ± 3	117 ± 6
Ketek PM 3325 (WBA0) 3x3mm ² (25µm)	53 ± 3	161 ± 9
Ketek PM 3350 (WBA0) 3x3mm ² (50µm)	51 ± 3	74 ± 6
SensL FJ 30035 3x3mm ² (35µm)	50 ± 3	108 ± 7
Broadcom AFBR-S4N44C013 (30µm)	55 ± 3	88 ± 6
FBK NUV-HD 4x4mm ² (40µm)	59 ± 3	68 ± 6
FBK NUV-HD 4x4mm ² (40µm) no resin	59 ± 3	69 ± 6

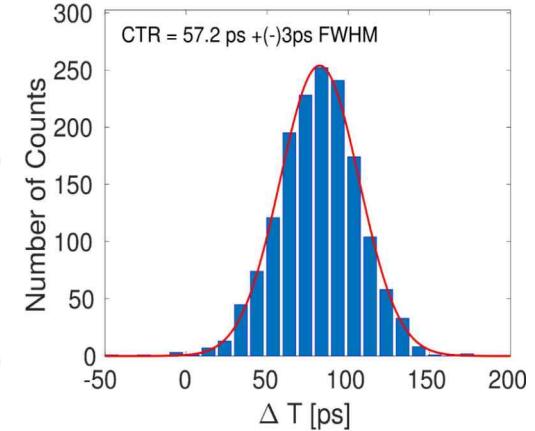
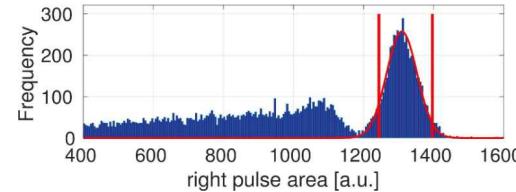
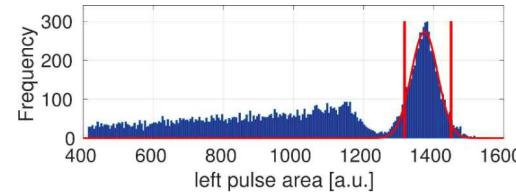
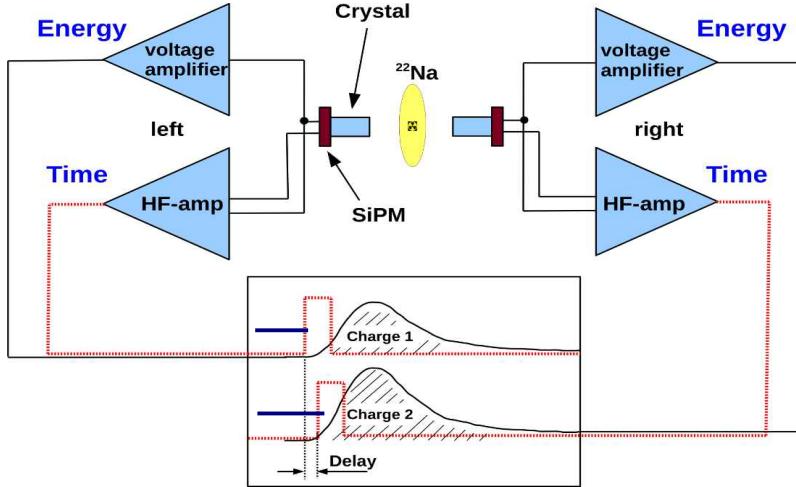
S. Gundacker et.al, "Experimental time resolution limits of modern SiPMs and TOF-PET detectors exploring different scintillators and Cherenkov emission," Physics in Medicine & Biology, vol. 65, p. 025001, Jan 2020.

Another way to measure the S PTR?

Problems of picosecond lasers:

- laser head noise pick-up
- sometimes difficult to exactly know the laser pulse shape

Coincidence time resolution (CTR) setup

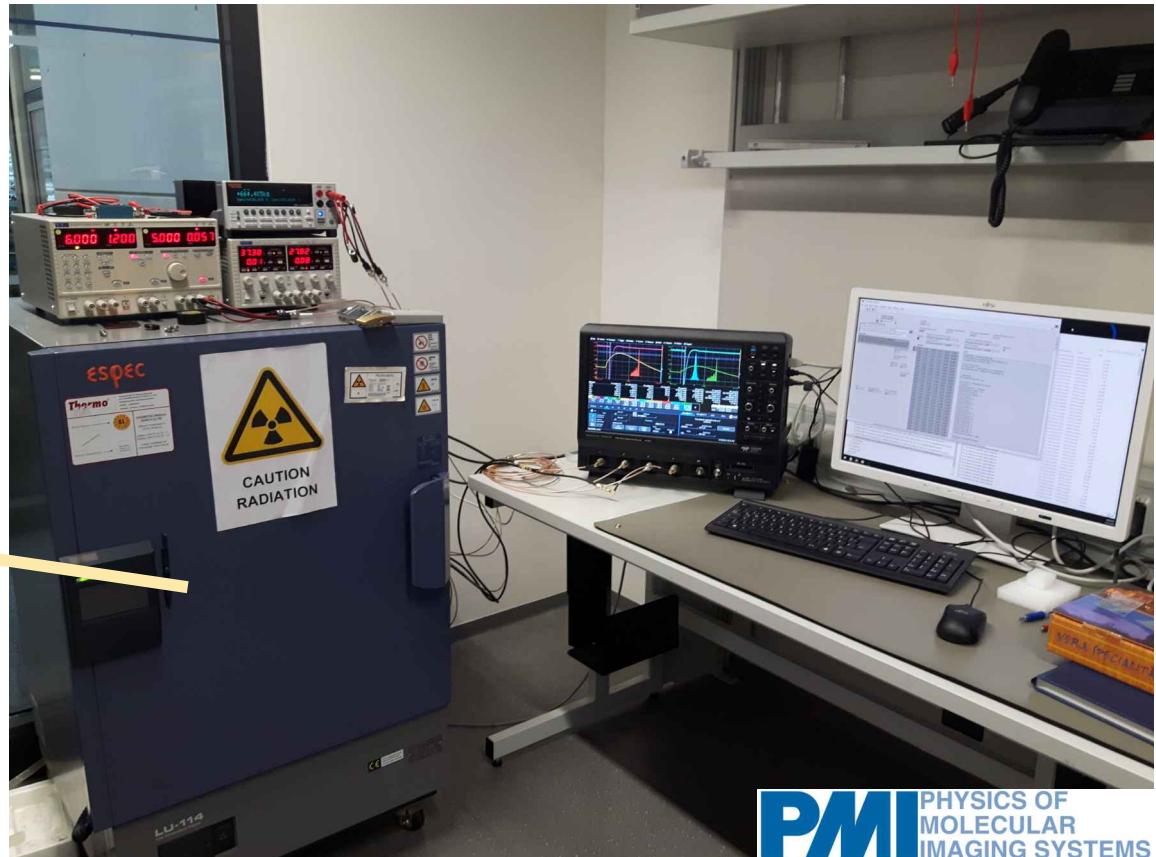
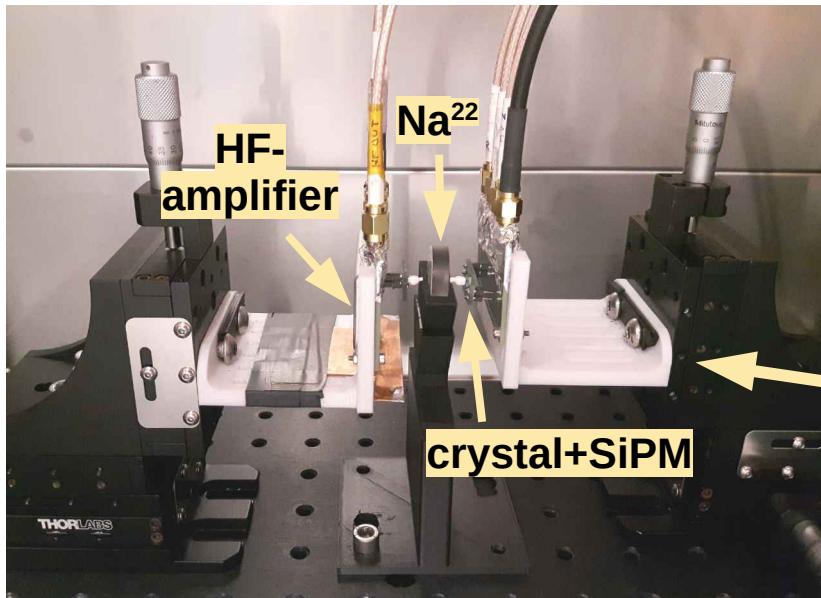


Teledyne LeCroy oscilloscope with 4 GHz bandwidth and 20 Gs/s sampling rate.

Temperature stabilized at 16°C.

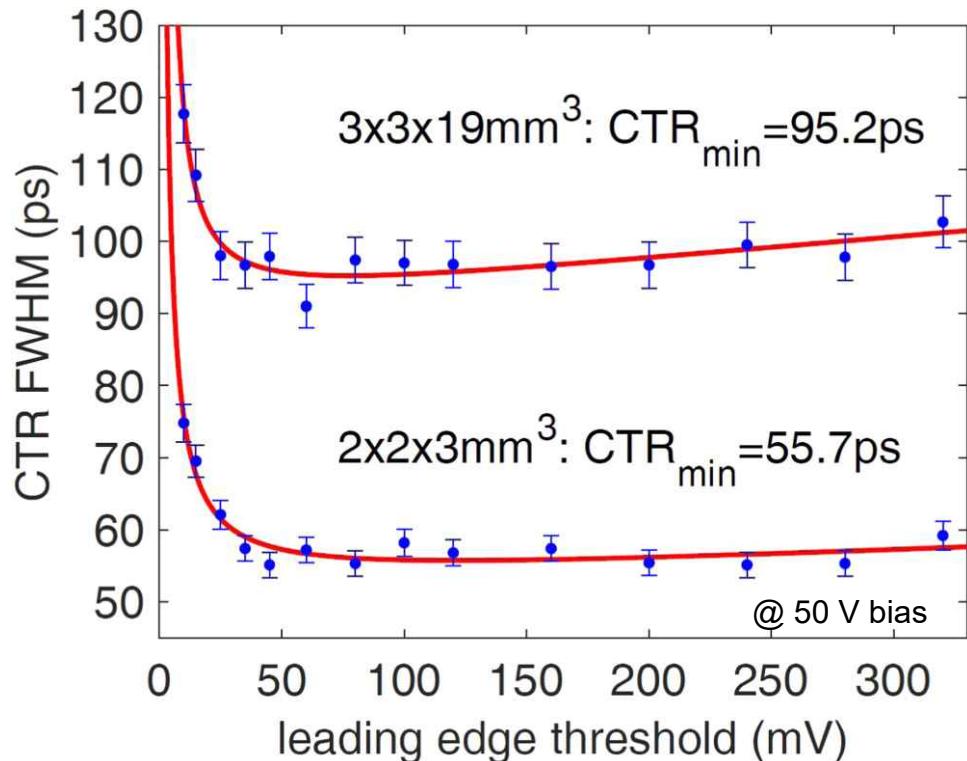
S. Gundacker et.al, "High-frequency SiPM readout advances measured coincidence time resolution limits in TOF-PET", Phys. Med. Biol. 64 (2019)

Some impressions from the lab



PMI PHYSICS OF
MOLECULAR
IMAGING SYSTEMS

CTR with Broadcam NUV-MT



SiPM active area $3 \times 3 \text{ mm}^2$,
LYSO:Ce,Ca from TAC of
 $2 \times 2 \times 3 \text{ mm}^3$ and $3 \times 3 \times 19 \text{ mm}^3$

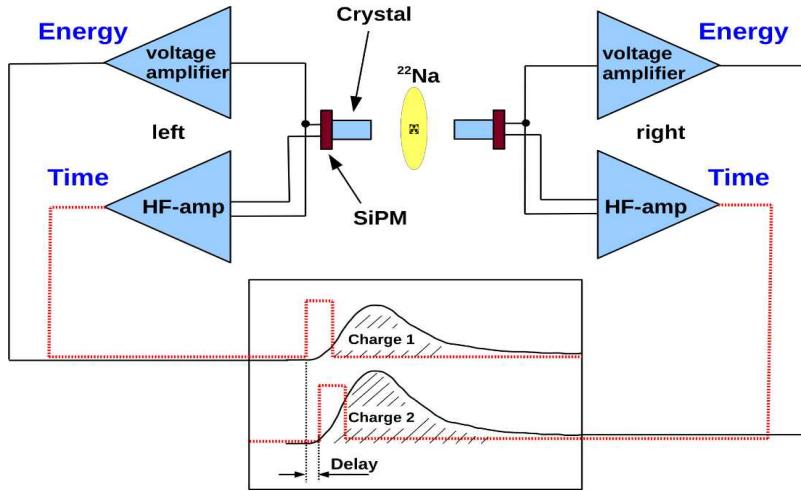
$3 \times 3 \times 20 \text{ mm}^3$ LYSO:Ce,Ca
CTR=95 ps FWHM

$2 \times 2 \times 3 \text{ mm}^3$ LYSO:Ce,Ca
CTR=56 ps FWHM

→ Detector time resolution:
 $\text{CTR}/\sqrt{2}=39 \text{ ps}$

V. Nadig et.al, "Timing advances of commercial divalent-ion co-doped LYSO:Ce and SiPMs in sub-100 ps time-of-flight positron emission tomography", Phys. Med. Biol. 68 (2023) 075002

Cherenkov radiation in PbF_2



- standard CTR setup with reference detector on left side: CTR=56-66 ps FWHM
- on device under test glued (Meltmount) and black painted PbF_2 crystal of $2 \times 2 \times 3 \text{ mm}^3$ size (negligible photon transfer spread)
- select to single photon, subtract DTR of reference and the electronic noise jitter

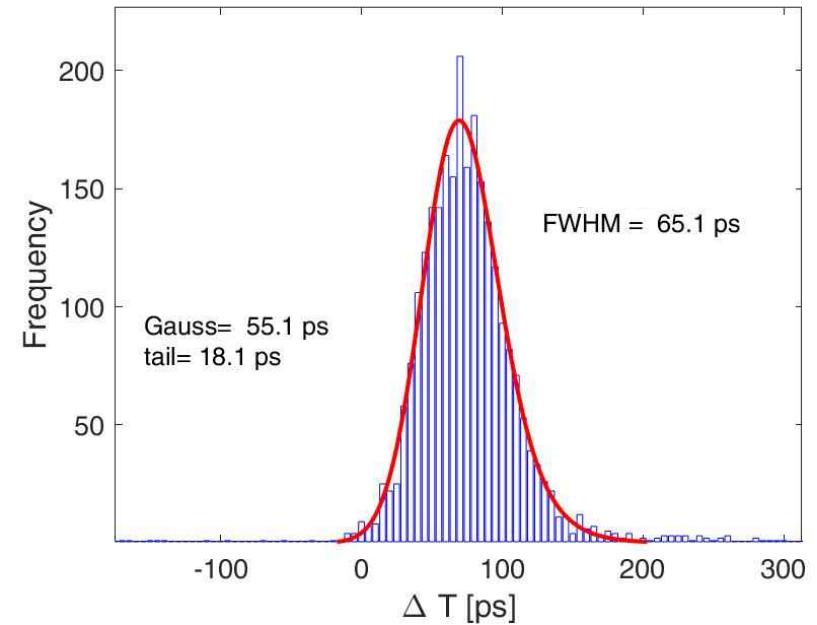
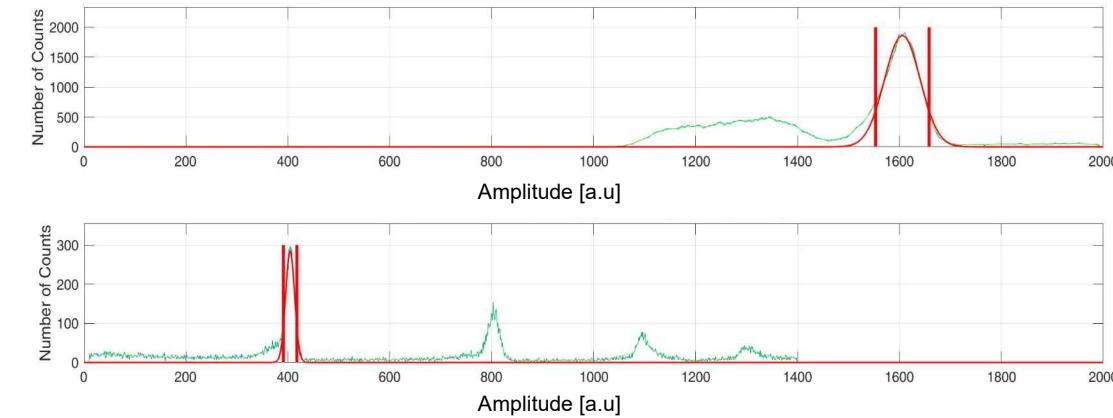
$$S PTR_{measured} = S PTR_{intrinsic} \otimes CTR/\sqrt{2} \otimes \text{electronic noise jitter} \left(\frac{V_{noise}}{dV/dt} \right)$$

N. Kratochwil, S. Gundacker and E. Auffray, "A roadmap for sole Cherenkov radiators with SiPMs in TOF-PET", Phys. Med. Biol. 66 (2021) 195001

S. Gundacker et.al, "On timing-optimized SiPMs for Cherenkov detection to boost low cost time-of-flight PET", Phys. Med. Biol. 68 (2023)



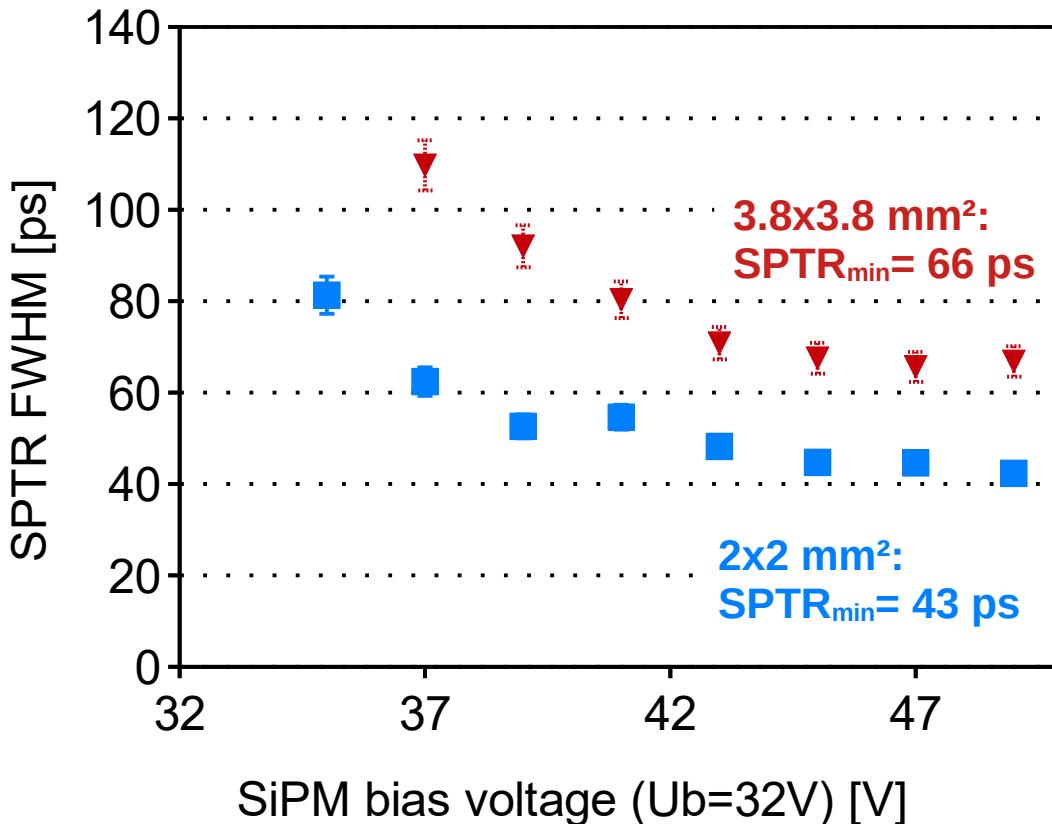
SPTR example plot & analysis



$$\text{S PTR}_{\text{intrinsic}} = \sqrt{\text{FWHM}_{\text{measured}}^2 - \text{DTR}^2 - (\text{electr. noise})^2}$$

S. Gundacker et.al, "On timing-optimized SiPMs for Cherenkov detection to boost low cost time-of-flight PET", Phys. Med. Biol. 68 (2023)

SPTR with Broadcom NUV-MT and black PbF₂



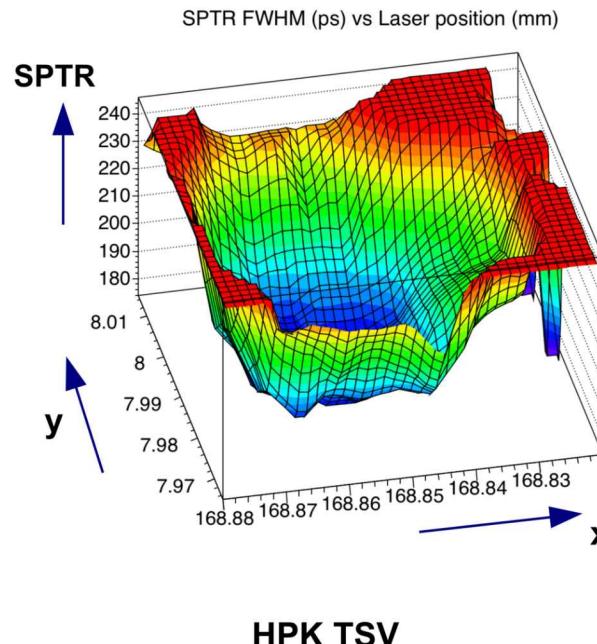
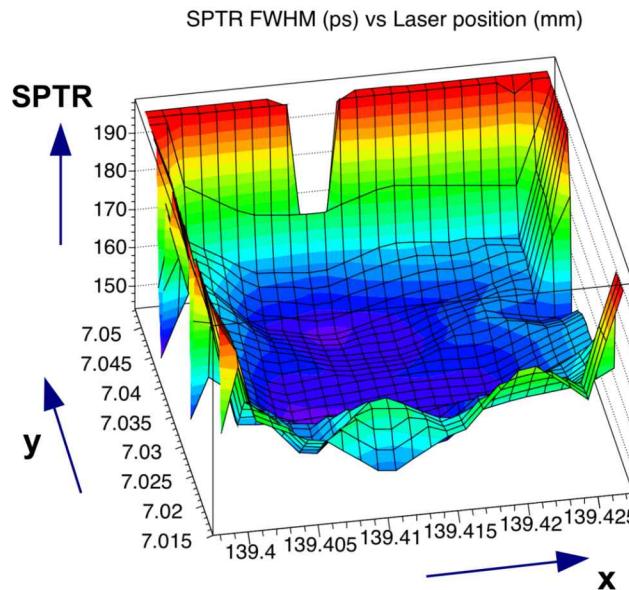
NUV-MT SiPM (AFBR-S4N44P014M), 40µm SPAD pitch from Broadcom, active area 2x2 mm² and 3.8x3.8 mm³.

Readout with power-efficient HF-electronics (Krake et.al., NIM A vol. 1039 (2022)).

Electronic noise not subtracted, but almost negligible due to high SiPM overvoltage.

Prospects of the S PTR

Edge effects in SPADs and masking



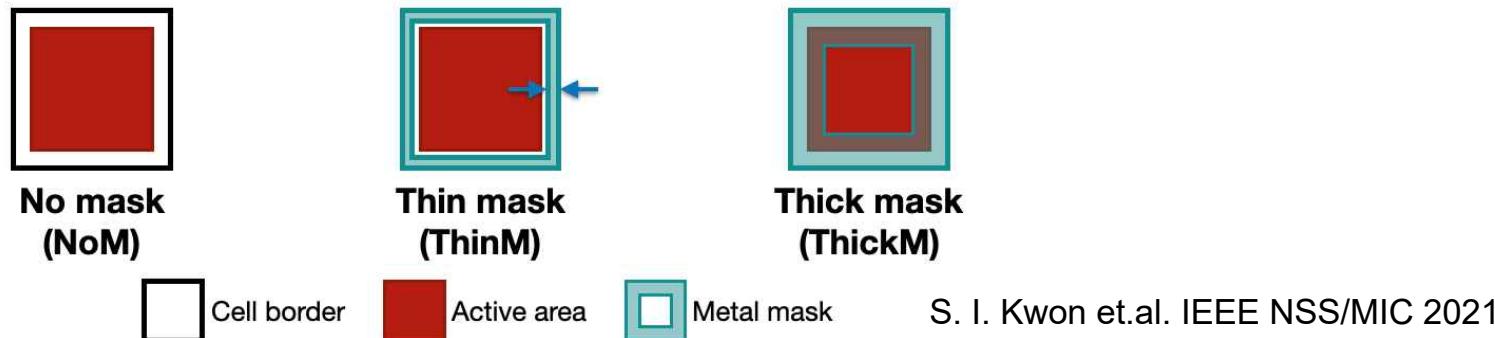
- **Masking of edges (FBK SiPMs of different types)**
- Improved SPTR and improved signal quality due to higher C_q

M.V. Nemallapudi, S. Gundacker, P. Lecoq and E. Auffray, "Single photon time resolution of state of the art SiPMs", October 2016.
JINST 11 P10016, DOI:10.1088/1748-0221/11/10/P10016

S. Gundacker et.al, "On timing-optimized SiPMs for Cherenkov detection to boost low cost time-of-flight PET", Phys. Med. Biol. 68 (2023)

Differently masked SiPMs tested

- Different **devices from FBK**: With and without SPAD masking (devices $4 \times 4 \text{ mm}^2$ and $3 \times 3 \text{ mm}^2$ active area, $40 \mu\text{m}$ SPAD pitch)



- measure the single photon time resolution (**SPTR**) with black painted PbF_2

S. Gundacker et.al, "On timing-optimized SiPMs for Cherenkov detection to boost low cost time-of-flight PET", Phys. Med. Biol. 68 (2023)

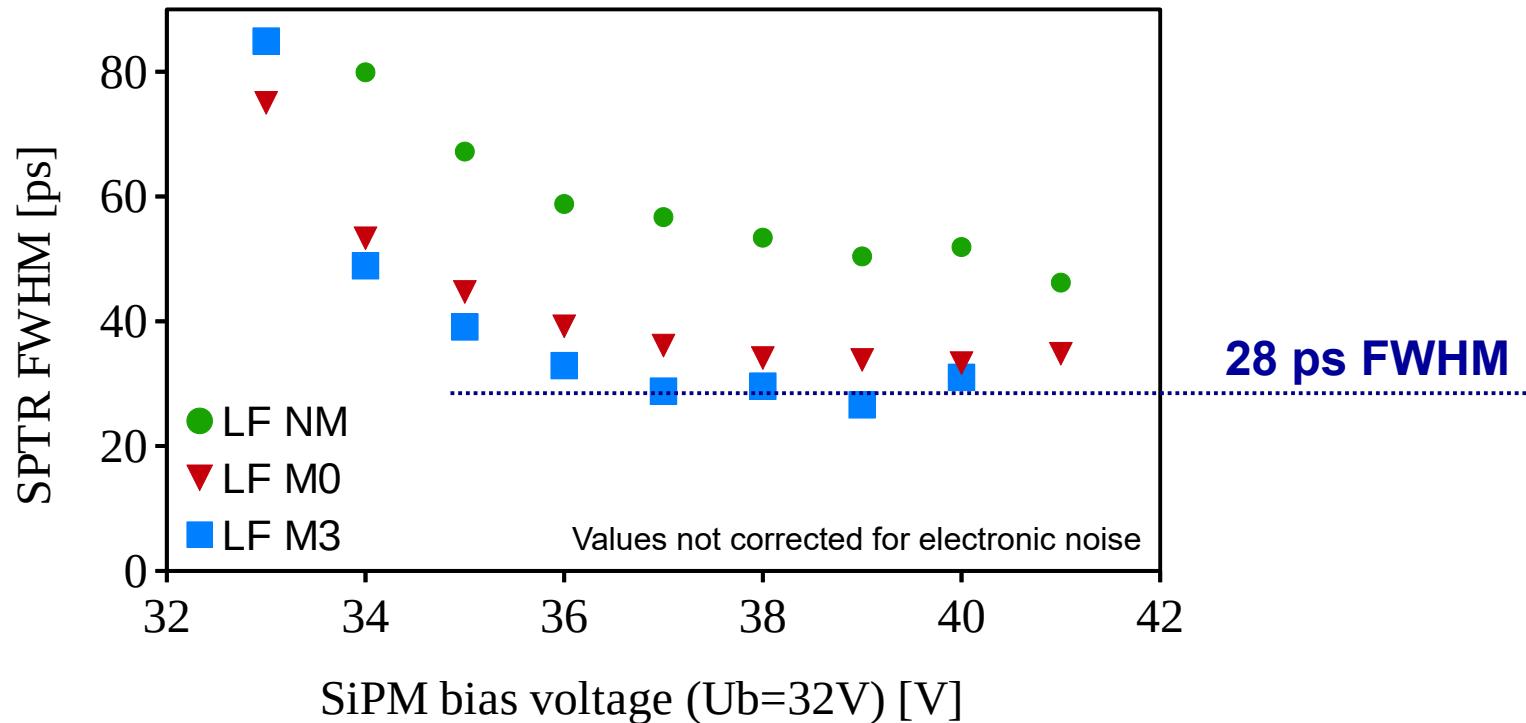
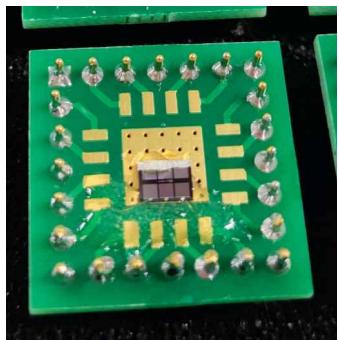
Tests with timing optimized 3x3 mm² SiPMs

<i>SiPM types (active area 3x3mm²)</i>	<i>S PTR FWHM intrinsic [ps]</i>	Speed of light: 3.3 ps/mm in vacuum. 40 ps → 1.2 cm resolution (single photon)
FBK SF (standard)	68 ± 4	
FBK LF2	65 ± 4	
FBK LF2 M0	50 ± 3	
FBK LF2 M1	47 ± 3	
FBK LF2 M3	42 ± 3	
Broadcom AFBR-S4N44C013 (commercial)	65 ± 4	
HPK S14160-3050HS (commercial)	125 ± 5	

FBK ... Fondazione Bruno Kessler, Trento, Italy

S. Gundacker et.al, "On timing-optimized SiPMs for Cherenkov detection to boost low cost time-of-flight PET", Phys. Med. Biol. 68 (2023)

SPTR with 1x1 mm² SiPMs

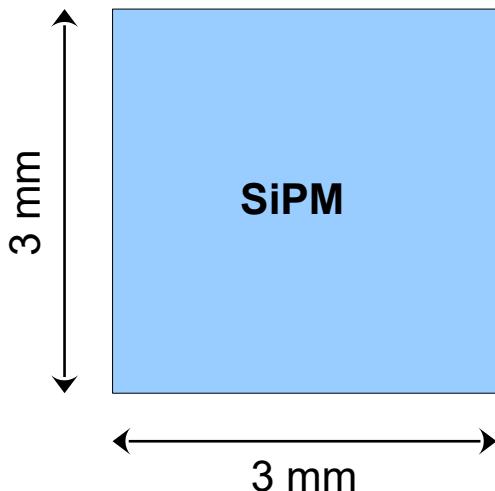


S. Gundacker et.al, "On timing-optimized SiPMs for Cherenkov detection to boost low cost time-of-flight PET", Phys. Med. Biol. 68 (2023)

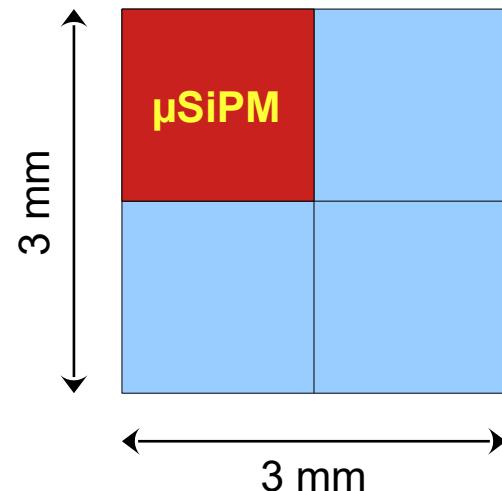
SPTR insights within the project

Segmenting the SiPM into μ SiPMs for BGO PET

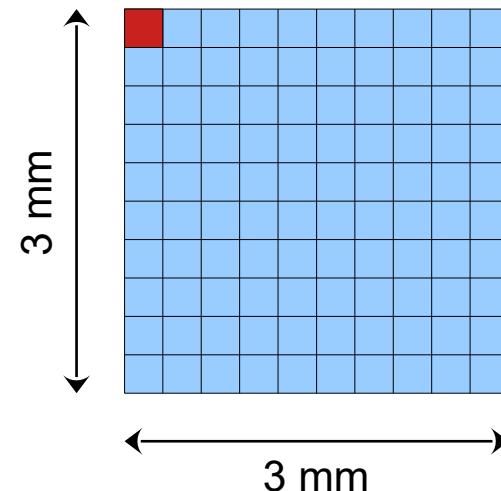
SiPM: 3x3 mm²
SPAD: 50 x 50 μ m²
1x1 μ SiPM array
(3600 SPADs per SiPM)



SiPM: 3x3 mm²
SPAD: 50 x 50 μ m²
2x2 μ SiPM array
(900 SPADs per μ SiPM)

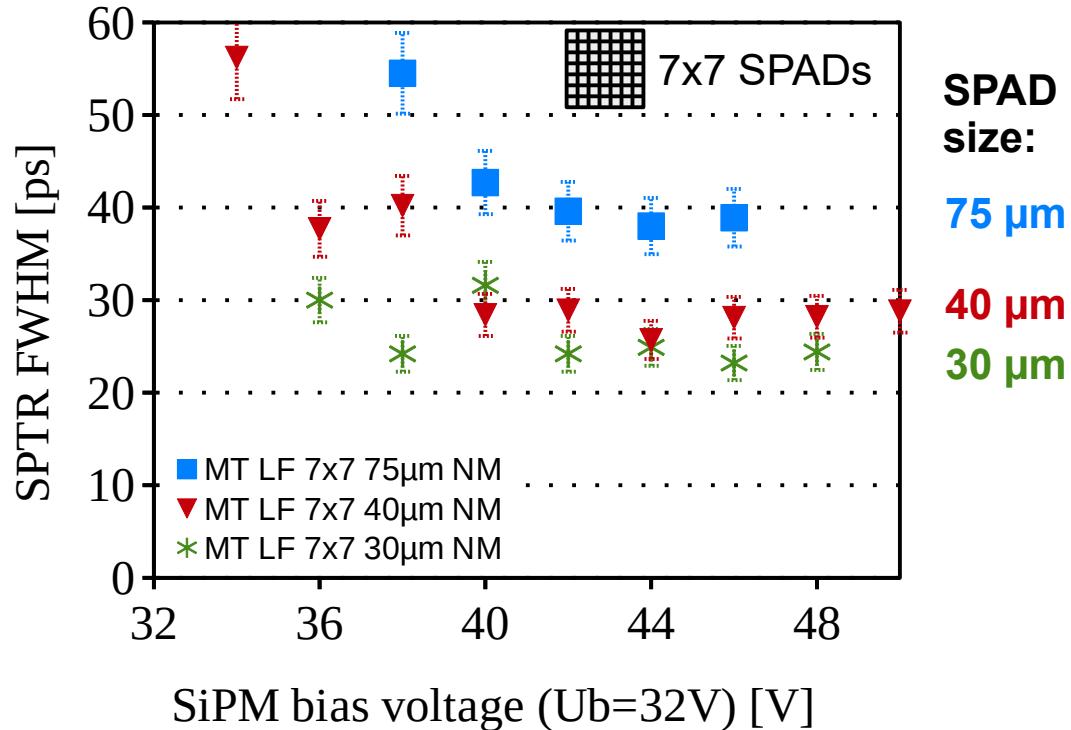


SiPM: 3x3 mm²
SPAD: 50 x 50 μ m²
10x10 μ SiPM array
(36 SPADs per μ SiPM)



- Lower capacitance C → higher electrical signal
- smaller SiPM size → better SPTR

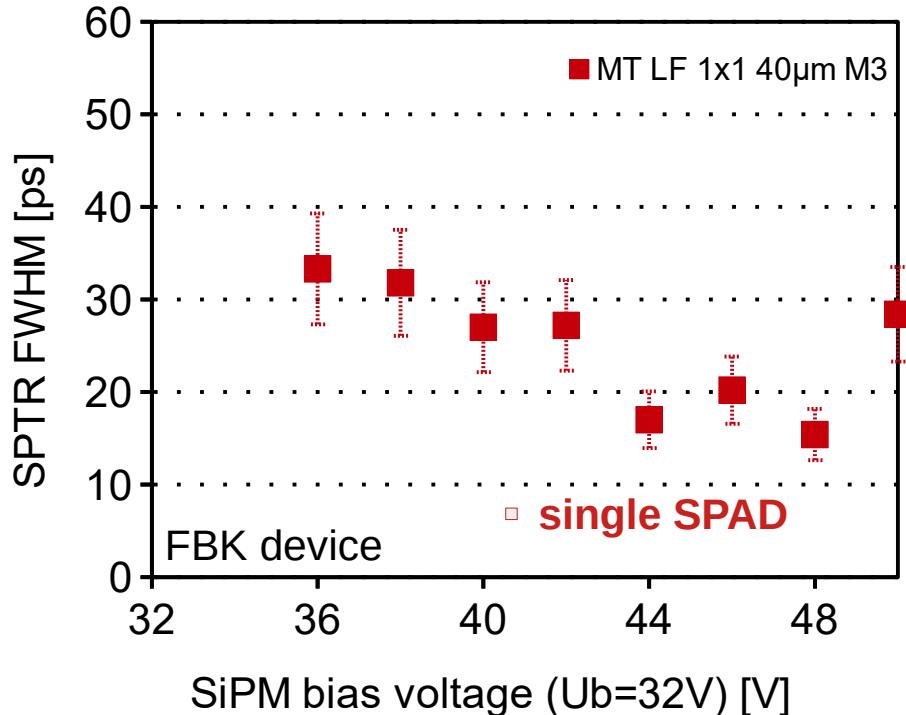
SPTR with different SPAD sizes



SPAD
size:
75 μm
40 μm
30 μm

- μSiPM consisting of 7x7 SPADs
- SPADs are not masked
- SPTR performance deteriorates with SPAD size
- Best value ~ 25 ps FWHM

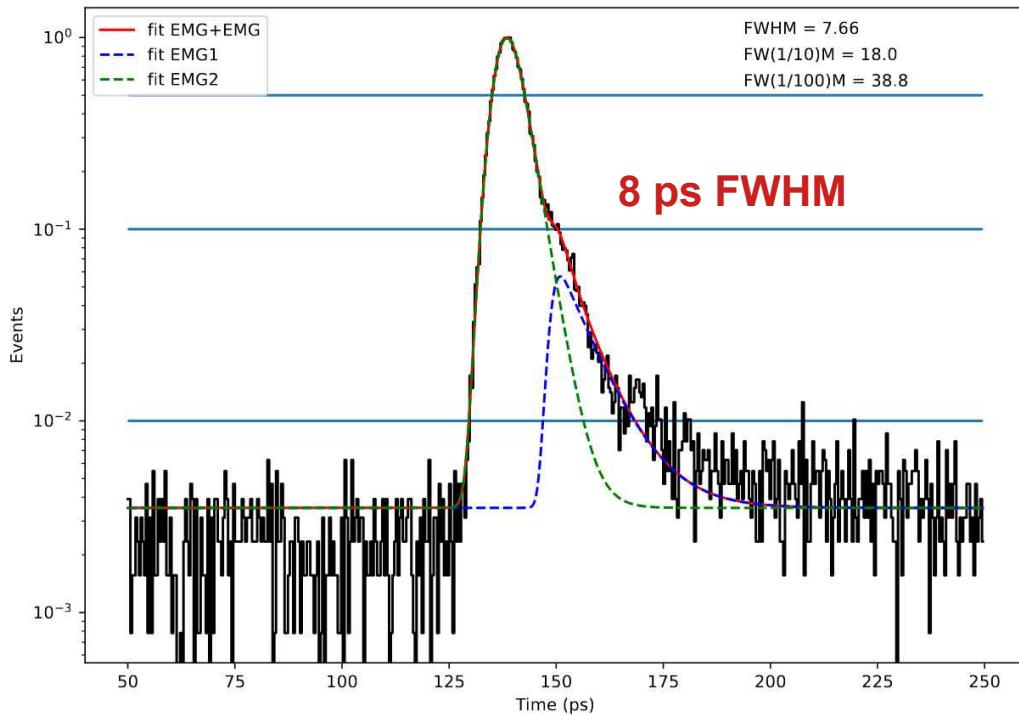
SPTR limits of single analog SPADs



- Single $40\mu\text{m}^2$ SPAD can reach an **S PTR of well below 20 ps FWHM if masked**.
- Exact value starts to be limited by resolution of our measurement method.

See also: M.V. Nemallapudi, S. Gundacker, P. Lecoq and E. Auffray, "Single photon time resolution of state of the art SiPMs", October 2016. JINST 11 P10016, DOI:10.1088/1748-0221/11/10/P10016

"Digital" SPADs achieve even sub-10 ps



- Sherbrooke, Canada and EPFL (AQUA), Switzerland achieve sub-10 ps with digital-readout.
- See work of J. F. Pratte and E. Charbon

F. Nolet et.al, "Quenching Circuit Discriminator Architecture Impact on a Sub-10 ps FWHM Single-Photon Timing Resolution SPAD", MDPI Instruments, 2023, 7, 16

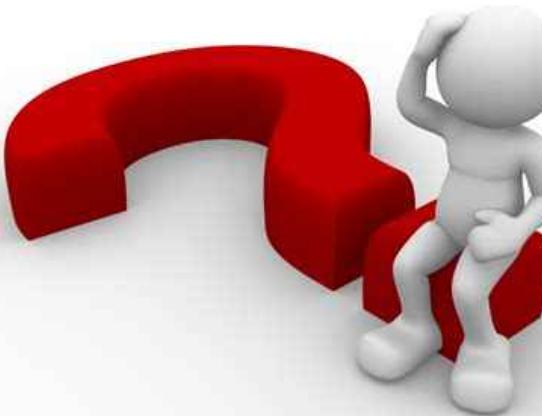
F. Gramuglia et.al, "A Low-Noise CMOS SPAD Pixel With 12.1 Ps S PTR and 3 ns Dead Time", IEEE Journal of Selected Topics in Quantum Electronics , vol. 28, no. 2, March/April 2022

Conclusions

- HF-readout allows to study intrinsic SPTR, also for larger devices ($3 \times 3 \text{mm}^2$).
- Power-efficient (<20mW) high-bandwidth amplifiers work well, which can be used for studying system related effects in multi-channel experiments.
- Best SPTR of commercial devices:
 - ✓ **SPTR of 66ps FWHM for Broadcom NUV-MT** ($3.8 \times 3.8 \text{mm}^2$ SiPM) and **SPTR of 117ps FWHM for HPK** ($3 \times 3 \text{mm}^2$ SiPM). Difference due to different SPAD structure.
 - ✓ **SPTR of 43ps FWHM for Broadcom NUV-MT (2x2mm² SiPM).**
- Masked SiPMs with 3μm mask overhang from FBK:
 - ✓ **SPTR of 42ps FWHM (3x3mm² SiPM).**
 - ✓ **SPTR of 28ps FWHM (1x1mm² SiPM).**
- SPAD size influences SPTR with worse performance for larger SPADs.
- SPAD limits **below 20ps FWHM (analog)** and **below 10ps FWHM (digital)**.



I am happy to
answer your
questions

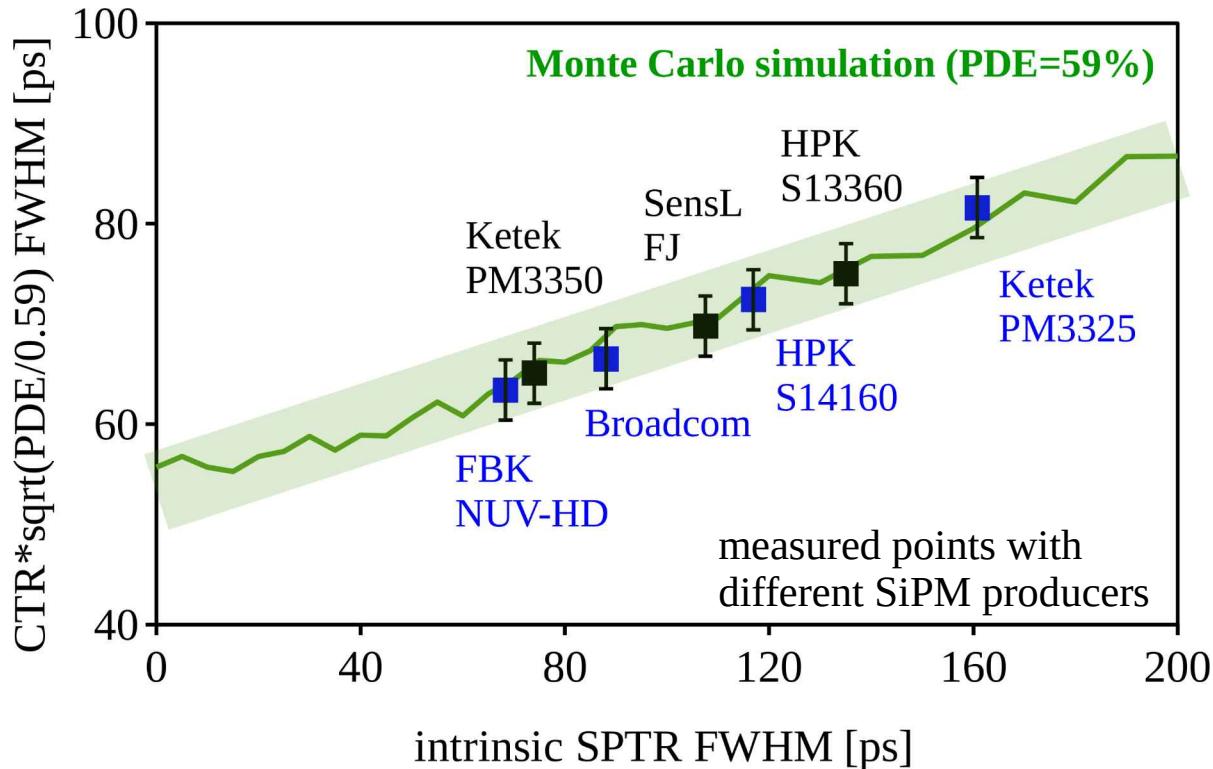


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The impact of the S PTR to the CTR



S. Gundacker et.al, "Experimental time resolution limits of modern SiPMs and TOF-PET detectors exploring different scintillators and Cherenkov emission," Physics in Medicine & Biology, vol. 65, p. 025001, Jan 2020.