PHOTOPLETHYSMOGRAPH SIGNAL
RECONSTRUCTION BASED ON A NOVEL HYBRID
MOTION ARTIFACT DETECTION – REDUCTION
APPROACH.
PART I: MOTION AND NOISE ARTIFACT DETECTION

PPG and MNA

- Photoplethysmograph (PPG): device to monitor blood volume changes on peripheral tissues. It is used to obtain HR, RR and SPO_2 .
- Motion and Noise Artifacts (MNA): serious obstacles for PPG recording, difficult to filter.

Sources:

- Environmental artifacts
- Physiological artifacts
- Experimental artifacts

Causes:

- Movement of venous blood and other non-pulsative components along with pulsatile arterial blood
- Variations in the optical coupling between the sensor and the skin

MNA detection difficulties and how the paper approaches the problem

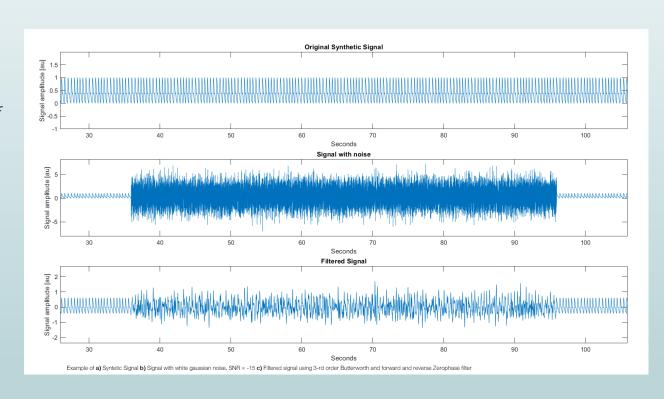
- They don't have a predetermined frequency band
- Overlapped spectrum with the desire PPG signal
- Use of 4-time domain parameters to quantify MNA as input of a SVM because there are noticeably differences between the values of clean and corrupted parts.
- First step in order to later reconstruct the detected corrupted segments without compromising the clean part of the signal.

Dataset

- Synthetic Dataset for Respiratory Rate Estimation which simulates PPG signals.
- Three respiratory modulations:
 - Baseline Wander (low frequency artifact in the ECG)
 - Amplitude Modulation (proportional to the amplitude of the signal)
 - Frequency Modulation (proportional to the frequency of the signal)
- Sampling Frequency (Fs) = 500 Hz
- Number of samples = $105\ 000 \rightarrow 210\ s$
- Data split by respiratory modulation and then divided into training and test phase.

Common procedure for each signal

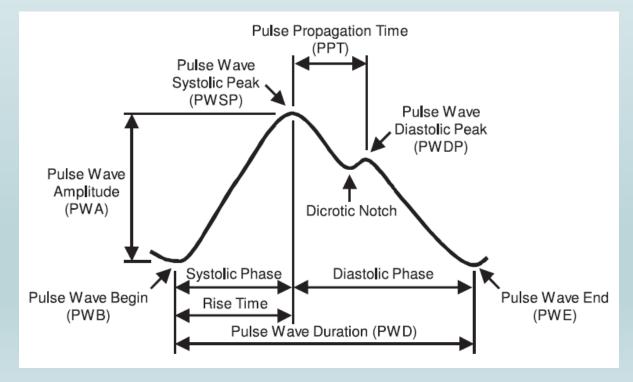
- Adding gaussian white noise
 - Noisy Signal = Orginal Signal + $\sigma(Signal) \cdot random \ value$
 - To the whole signal with SNR = 25 dB
 - To 30 000 samples (60 s), around the 29% of the total, with SNR $\in [-25 10 \ dB]$
- Applying a 3rd order Butterworth bandpass filter with cutoff frequencies of 0.5 and 12 Hz
- Applying a zero phase and reverse filtering
- Splitting the signal into 7-seconds long segments, 30 in total.
- For each segment:
 - Computing 4 parameters
 - Computing labels: 0 = clean, 1 = corrupted (if less than 85% of the segment is free from noise)



Standard Deviation of Peak-to-Peak Interval

$$- STD_{HR} = \sqrt{\frac{1}{N}\sum_{i=1}^{N}(D_{n,i} - \overline{D_n})^2}$$

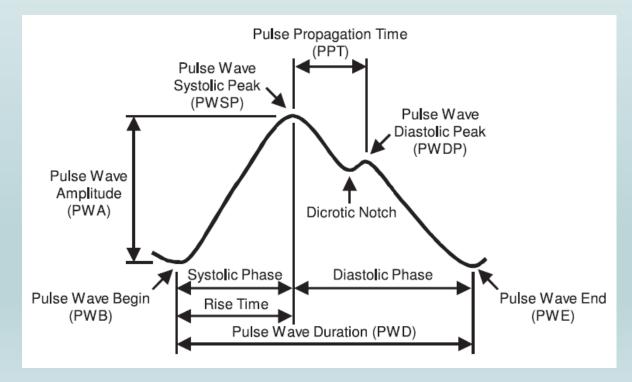
- $D_{n,i} = T_{peak.n,i} T_{peak.n,i-1}$
- $\overline{D_n}$ mean peak-to-peak interval of the nth segment



Standard Deviation of Peak-to-Peak Amplitude

$$- STD_{AMP} = \sqrt{\frac{1}{N} \sum_{i=1}^{N} (A_{n,i} - \overline{A_n})^2}$$

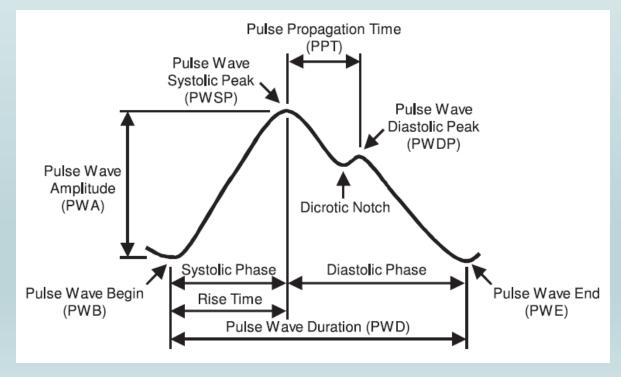
- $A_{n,i} = A_{peak.n,i} A_{trough.n,i+1}$
- $\overline{A_n}$ mean peak-to-peak interval amplitude of the nth segment



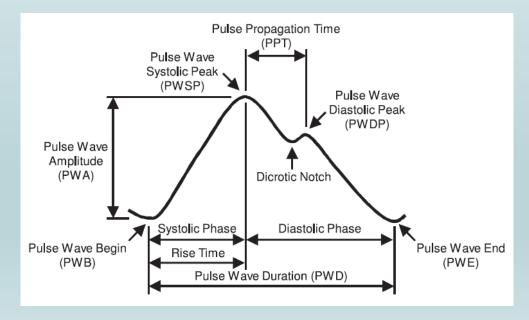
Standard Deviation of Systolic and Diastolic Ratio

$$- STD_{SD} = \sqrt{\frac{1}{N} \sum_{i=1}^{N} (R_{SD,n,i} - \overline{R}_{SD,n})^2}$$

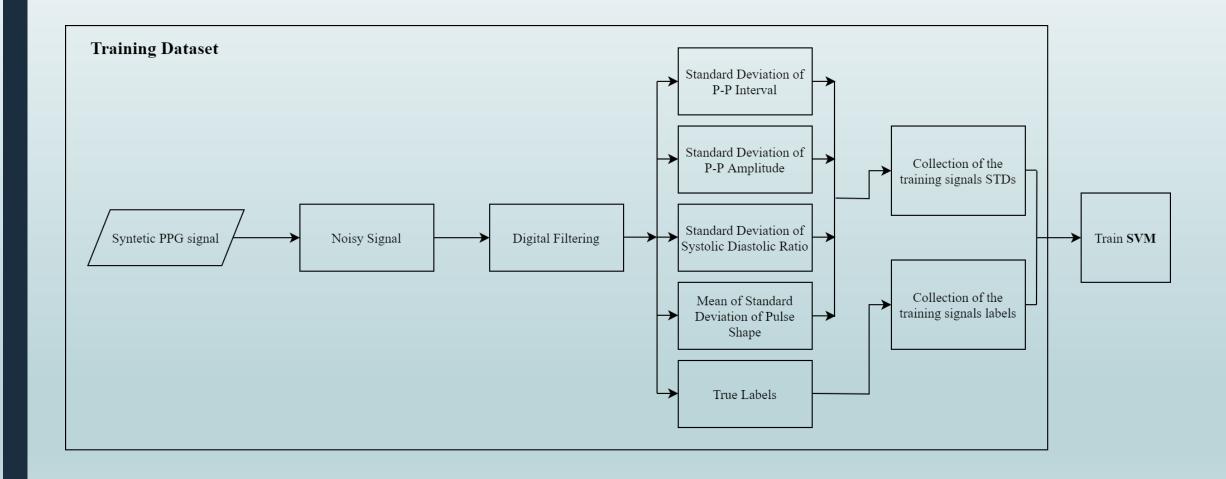
- $R_{SD,n,i} = (T_{trough,n,i} T_{peak,n,i}) / (T_{peak,n,i} T_{trough,n,i-1})$
- $\overline{R_{SD,n}}$ mean systolic and diastolic time interval ratio of the nth segment

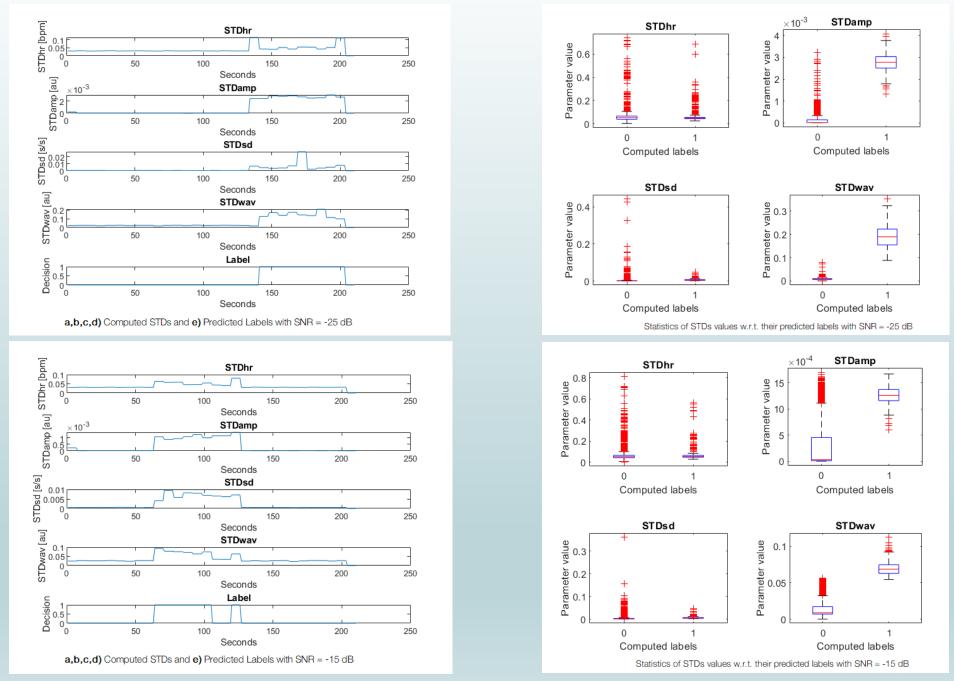


- Standard Deviation of Peak-to-Peak Amplitude
 - $STD_{WAV,n} = E[STD_{WAV,n,m}]$
 - $STD_{WAV,n,m} = \sqrt{\frac{1}{N} \sum_{i=1}^{N} (q_{n,i}(m) \overline{q_{n(m)}})^2}$
 - $q_{n,i}(m)$ mth sample [of N_{samp} taken from a pulse] at the ith pulse of the nth segment
 - $\overline{q_{n(m)}}$ mean at the mth sample of the nth segment



Training Procedure





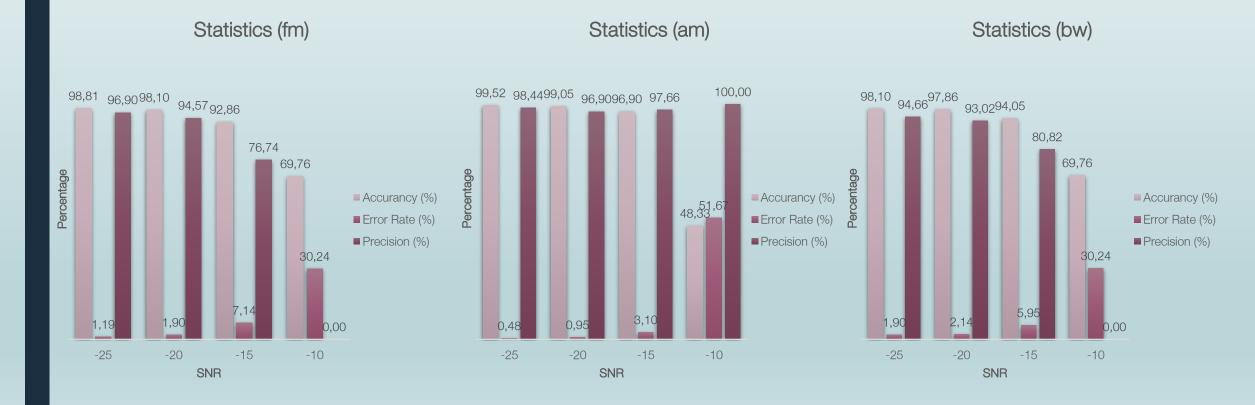
Alice Sansoni Biomedical Signal Processing a.a. 2020-2021

Parameters obtained from the confusion matrix

Accuracy = (TP + TN)/Tot Error Rate = (FP + FN)/Tot = 1 - Accuracy Precision = TP / (TP+FP)

TP = True Positive TN = True Negative

FP = False Positive FN = False Negative



THE END

THANK YOU FOR LISTENING.