

# Riemannian classification of EEG signals with missing values

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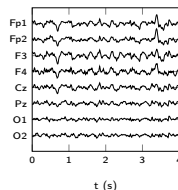
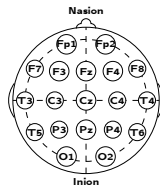
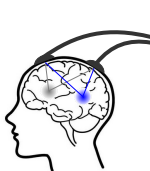
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Annecy, France

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# What is electroencephalography?

- Electroencephalography (EEG): recording the **brain activity**
- **Non-invasive** neuroimagery modality
- Used in **Brain Computer Interface** (BCI) – *e.g.*, exoskeleton control, help mechanical ventilation, games, *etc.*



- BCI boils down to a **classification task** of brain signals at hand – *e.g.*, recognize a mental task, exposition to a stimulus, *etc.*  
 ⇒ Here we focus on the minimum distance to Riemannian mean  
 [Barachant et al., 2011]

# Motivation of the study

## Advantages

low-cost

high temporal resolution

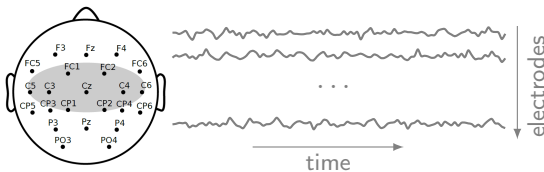
## Drawbacks

low spatial resolution

low SNR

- EEG data also contains **faulty measurements** due to impedance change, electrode popping or artifacts...

⇒ Leads to missing data ⇐



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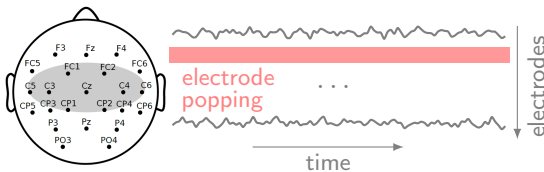
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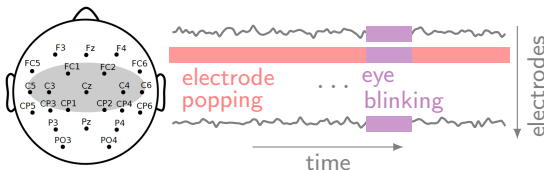
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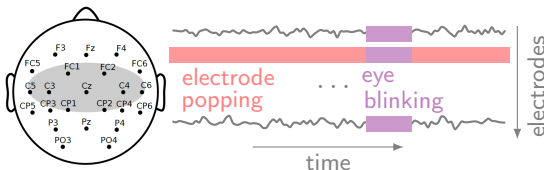
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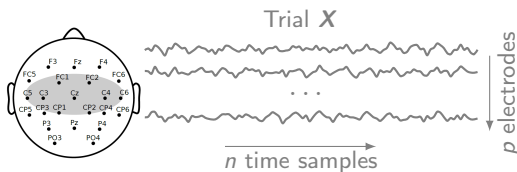
⇒ Leads to missing data ⇐



⇒ Need to propose **new classification methods** that **handle missing data** for BCI applications.

# Data representation and feature extraction

⇒ EEG recordings are usually represented by **trials**.



- Data:  $\mathbf{X} = [\mathbf{x}_1, \dots, \mathbf{x}_n] \in \mathbb{R}^{p \times n}$
- Common hypothesis:  $\mathbf{X} \sim \mathcal{N}(\mathbf{0}, \mathbf{\Sigma})$
- Spatial **covariance matrices** are used as **features**

$$\mathbf{\Sigma} = \frac{1}{n} \mathbf{X} \mathbf{X}^\top$$

1 trial = 1 covariance matrix to classify !

## Minimum distance to Riemannian mean [Barachant et al., 2011]

- **Affine invariant distance** based on the geometry of the space of SPD matrices:

$$\delta_{\mathcal{AF}}(\mathbf{\Sigma}_1, \mathbf{\Sigma}_2) = \left\| \log \left( \mathbf{\Sigma}_1^{-1/2} \mathbf{\Sigma}_2 \mathbf{\Sigma}_1^{-1/2} \right) \right\|_F.$$



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Given a  $Z$ -classes classification problem, with training data  $(\mathbf{\Sigma}_\ell, y_\ell)_{1 \leq \ell \leq L}$ :

## Training

Compute the mean of each class

$\{\bar{\mathbf{\Sigma}}^{(z)} : z \in \{1, \dots, Z\}\}$ :

$$\bar{\mathbf{\Sigma}}^{(z)} = \arg \min_{\mathbf{\Sigma} \in S_p^{++}} \sum_{\ell=1}^L \delta_{\mathcal{AF}}^2(\mathbf{\Sigma}, \mathbf{\Sigma}_\ell)$$

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## Testing

Prediction of a label  $y^*$  on a new sample  $\mathbf{\Sigma}$ :

$$y^* = \arg \min_{z \in \{1, \dots, Z\}} \delta_{\mathcal{AF}}(\mathbf{\Sigma}, \bar{\mathbf{\Sigma}}^{(z)})$$

⇒ **assignment to the closest mean**

# EEG classification with missing values

## Strategies to classify incomplete data using the covariance matrix

- **Impute** the data, then classify – e.g.,  $k$ -nearest neighbors (KNN)  
[Troyanskaya et al., 2001]
- MDRM with incomplete data: **masked** minimum to Riemannian mean  
[Yger et al., 2020]
- **Expectation-Maximization** (EM) algorithm  $\Rightarrow$  handy iterative procedure to find  $\hat{\Sigma}_{ML}$ .  
[Hippert-Ferrer et al., 2022]

In what follows, **let us consider**:

- **Complete data**  $\{\mathbf{y}_i\}_{i=1}^n \in \mathbb{R}^p$  and  $\mathbf{y}_i = \{\mathbf{y}_i^o, \mathbf{y}_i^m\}$
- **Unknown parameter** of interest  $\boldsymbol{\theta} \in \Omega$ : in our case  $\boldsymbol{\Sigma} \in S_p^{++}$
- A **probabilistic model** of the data  $p(\mathbf{y}|\boldsymbol{\theta})$
- **Maximum likelihood** (ML):  $\hat{\boldsymbol{\theta}}_{ML} = \arg \max_{\boldsymbol{\theta} \in \Omega} p(\{\mathbf{y}_i^o\}|\boldsymbol{\theta})$

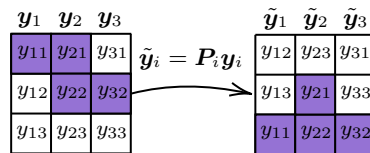
# Data incompleteness model

- Data transformation:

$$\tilde{\mathbf{y}}_i = \mathbf{P}_i \mathbf{y}_i = \begin{pmatrix} \mathbf{y}_i^o \\ \mathbf{y}_i^m \end{pmatrix}, \quad i \in [1, n]$$

$\{\mathbf{P}_i\}_{i=1}^n \in \mathbb{R}^{p \times p}$ : set of  $n$  permutation matrix.

- Example:  $n = p = 3$



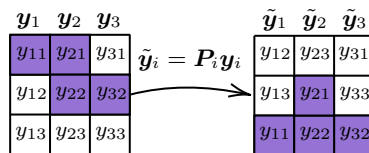
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- Covariance matrix:

$$\tilde{\Sigma}_i = \begin{pmatrix} \tilde{\Sigma}_{i,oo} & \tilde{\Sigma}_{i,mo} \\ \tilde{\Sigma}_{i,om} & \tilde{\Sigma}_{i,mm} \end{pmatrix} = \mathbf{P}_i \Sigma \mathbf{P}_i^\top$$

$\tilde{\Sigma}_{i,mm}$ ,  $\tilde{\Sigma}_{i,mo}$ ,  $\tilde{\Sigma}_{i,oo}$  are the **block CM** of  $\mathbf{y}_i^m$ ,  $\mathbf{y}_i^m$  and  $\mathbf{y}_i^o$ , and  $\mathbf{y}_i^o$ .

# Ingredients for our EM

1. Transformed data:  $\tilde{\mathbf{y}}_i = \mathbf{P}_i \mathbf{y}_i = \begin{pmatrix} \mathbf{y}_i^o \\ \mathbf{y}_i^m \end{pmatrix}$
2. Transformed CM:  $\tilde{\Sigma}_i = \mathbf{P}_i \Sigma \mathbf{P}_i^\top$
3. The complete loglikelihood  $\mathcal{L}_c$ :

$$\mathcal{L}_c(\theta | \mathbf{Y}) \propto -n \log |\Sigma| - p \sum_{i=1}^n \log \tau_i - \sum_{i=1}^n \tilde{\mathbf{y}}_i^\top \tilde{\Sigma}_i^{-1} \tilde{\mathbf{y}}_i$$

# The EM algorithm

Parameter:  $\theta = \{\Sigma\}$ .

E-step: compute the expectation of  $\mathcal{L}_c$

$$Q_i(\theta|\theta^{(t)}) = \mathbb{E}_{\mathbf{y}_i^m|\mathbf{y}_i^o, \theta^{(t)}} [\mathcal{L}_c(\theta|\mathbf{y}_i^o, \mathbf{y}_i^m)] = \text{tr}\{\mathbf{B}_i^{(t)} \tilde{\Sigma}_i^{-1}\}$$

need few manipulations

with  $\mathbf{B}_i^{(t)} = \begin{pmatrix} \mathbf{y}_i^o \mathbf{y}_i^{o\top} & \mathbf{y}_i^o \mathbb{E}[\mathbf{y}_i^{m\top}] \\ \mathbb{E}[\mathbf{y}_i^m] \mathbf{y}_i^{o\top} & \mathbb{E}[\mathbf{y}_i^m \mathbf{y}_i^{m\top}] \end{pmatrix}.$

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M-step: obtain  $\Sigma^{(t+1)}$  as the solution of the following max. problem

$$\theta^{(t+1)} = \arg \max_{\theta \in \mathcal{S}_{++}^p} \sum_{i=1}^n Q_i(\theta|\theta^{(t)})$$



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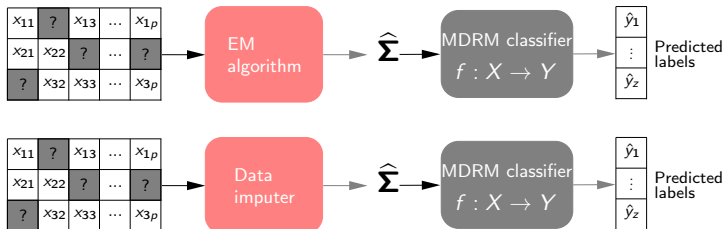
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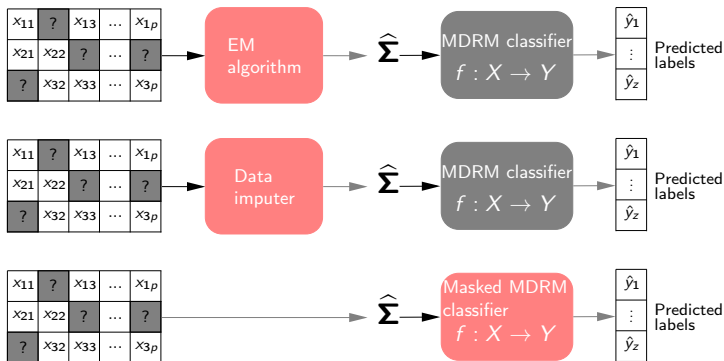
Closed-form expression:  $\Sigma^{(t+1)} = \frac{1}{n} \sum_{i=1}^n \mathbf{P}_i \mathbf{B}_i^{(t)\top} \mathbf{P}_i^\top$



# Classification pipelines



# Classification pipelines



# Moabb datasets

Considered EEG recordings are from the **moabb database**:

## Dataset 1 – P300 Event related potentials

Potentials are triggered from target stimuli consisting of flashes.

- 10 subjects, 16 electrodes
- **Binary** classification problem (flash stimulus or no flash)
- $L = 1728$  **covariance matrices** to classify with  $p = 16$  and  $n = 103$

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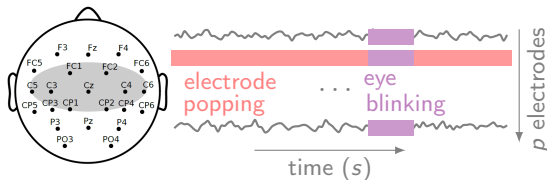
## Dataset 2 – Motor Imagery

Imagination of movement of left hand (class 1), right hand (class 2), both feet (class 3) and tongue (class 4):

- 9 subjects, 22 electrodes
- **4-classes** classification problem
- $L = 576$  **covariance matrices** to classify with  $p = 22$  and  $n = 1001$

## Missing data scenario

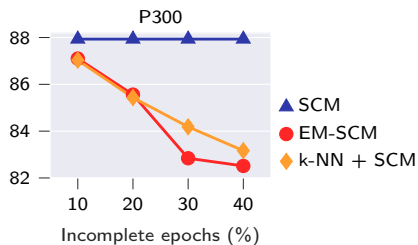
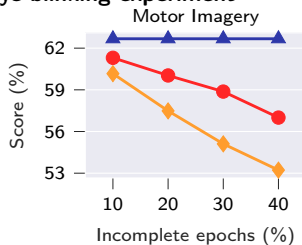
- **Electrode popping:** multiple electrodes are entirely removed during the experiment.
- **Eye blinking:** multiple electrodes are removed for a short period of time ( $\sim 200$  ms).



	KNN [Troyanskaya et al., 2001]	Masked mean [Yger et al., 2020]	EM [Hippert-Ferrer et al., 2022]
Electrode popping	✗	✓	✓
Eye blinking	✓	✗	✓

# Results on moabb datasets

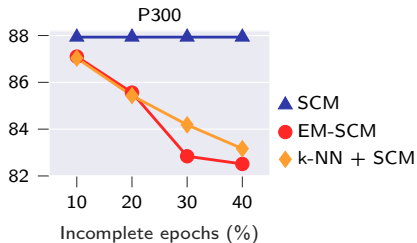
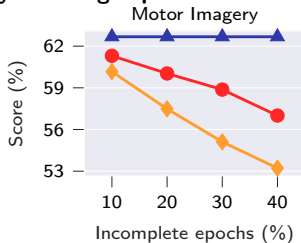
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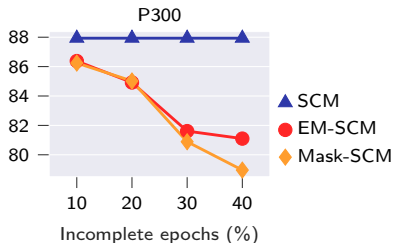
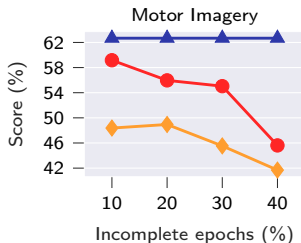


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### Eye blinking experiment



### Electrode popping experiment



## Conclusion and perspectives

- A new strategy to handle missing data in the context of EEG classification
- Relies on a simple yet powerful tool: the EM algorithm
- Works on a **wider range of missing data scenario** compared to KNN imputation and masked Riemannian means
- Competitive in terms of **accuracy**

### Some interesting perspectives include...

- Consider **robust estimation** ( $M$ -estimators,  $t$ -distribution) instead of Gaussian estimation
- Adapt other classifiers to missing data: tangent space, common spatial filters, *etc.*



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