

# Mini-Project 2: EMG Signal Analysis

NX-421- Neural Signals  
and Signal Processing  
Profs. Van de Ville, Micera

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# MOTIVATION

To build a movement intention decoder using sEMG  
and glove EMG data for prosthetics and assistive  
devices

# PART 1

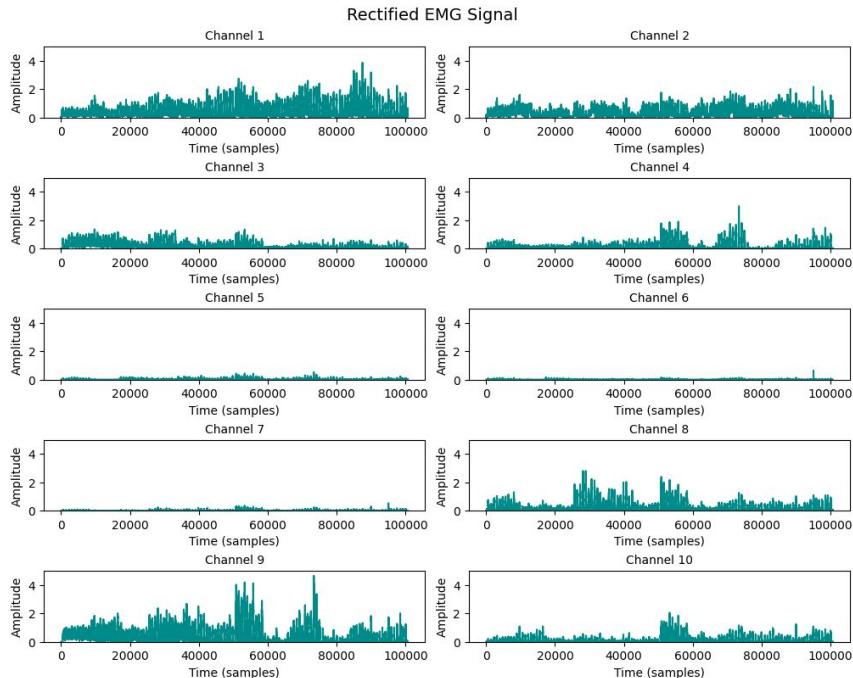
SINGLE SUBJECT CLASSIFICATION

Exercise A

1	Index flexion		7	Little finger flexion	
2	Index extension		8	Little finger extension	
3	Middle flexion		9	Thumb adduction	
4	Middle extension		10	Thumb abduction	
5	Ring flexion		11	Thumb flexion	
6	Ring extension		12	Thumb extension	

# NinaPro Dataset 1 - Subject 2

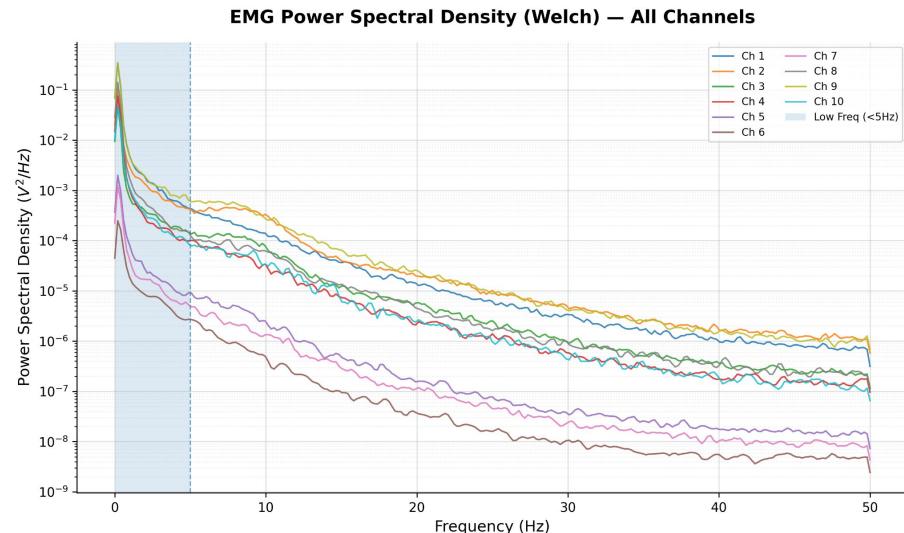
## Amplitude vs Time



We observe that all signals are positive.

- Data appears to already be **rectified**.

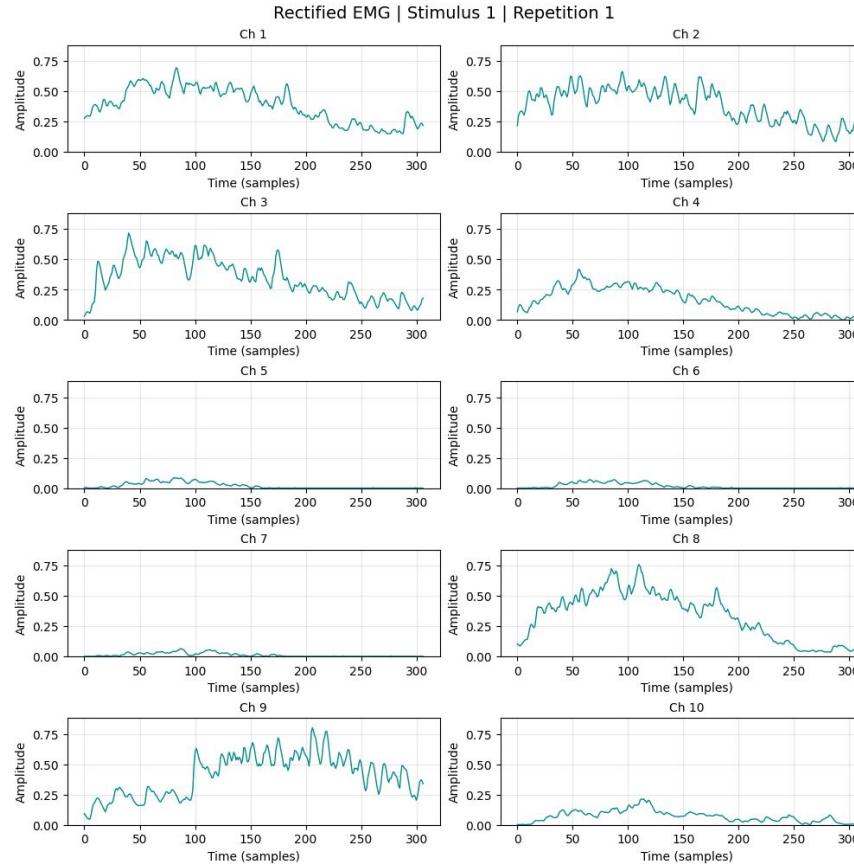
## PSD vs Frequency



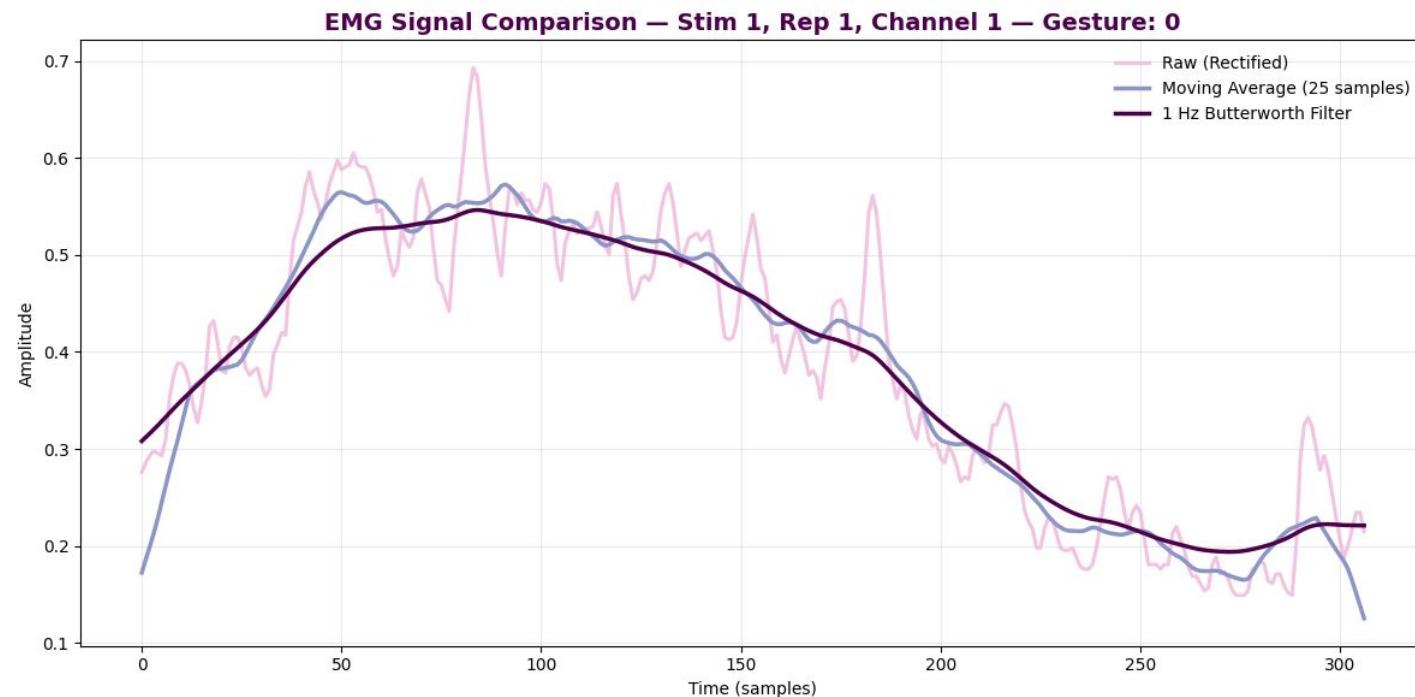
We do not observe any peaks. Data is clipped at 50Hz - line noise frequency.

Data appears to already be **filtered**.

# Visualising Data per Channel per Trial



No trials dropped!

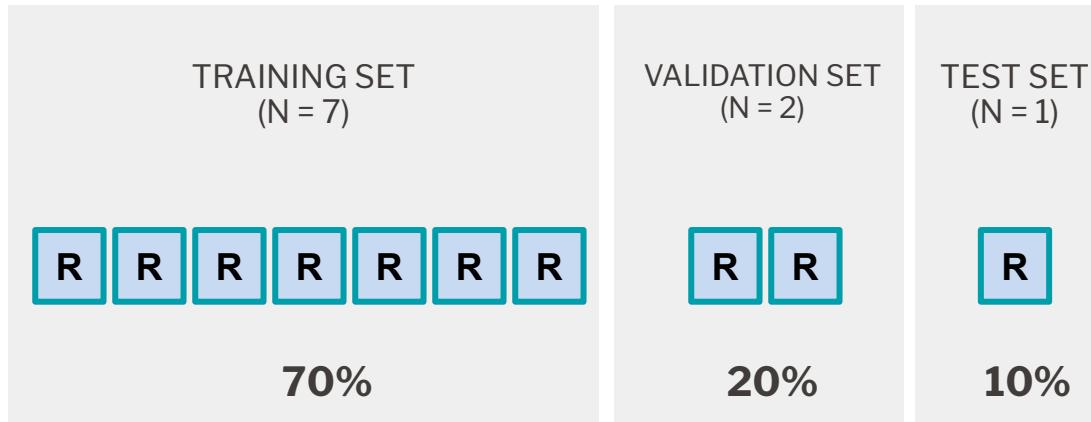


Tried different preprocessing methods based on literature and the labs.

**Stuck with Raw, rectified data** to avoid overly smoothing data.

# Splitting the Data

For each of the 12 movements:



Splitting to ensure all 12 classes are **balanced** across the training, validation and testing dataset.

# Feature Selection

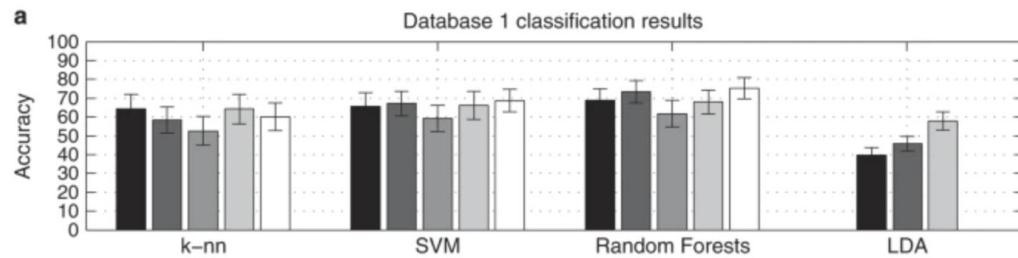
## SOURCES

ATZORI ET AL. (2014) + HEDGINS ET AL. (2002)

### TIME DOMAIN

- ROOT MEAN SQUARE (RMS)
- MEAN ABSOLUTE VALUE (MAV)
- WAVEFORM LENGTH (WL)
- SLOPE SIGN CHANGE (SSC)
- HISTOGRAM (HIST LOG ENTROPY)

RMS
TD
HIST
mDWT
All



### FREQUENCY DOMAIN

- MARGINAL DISCRETE WAVELET TRANSFORM

## COMPLEMENT WITH NEW FEATURES

### SOURCE

LECTURES + LABS

### TIME DOMAIN

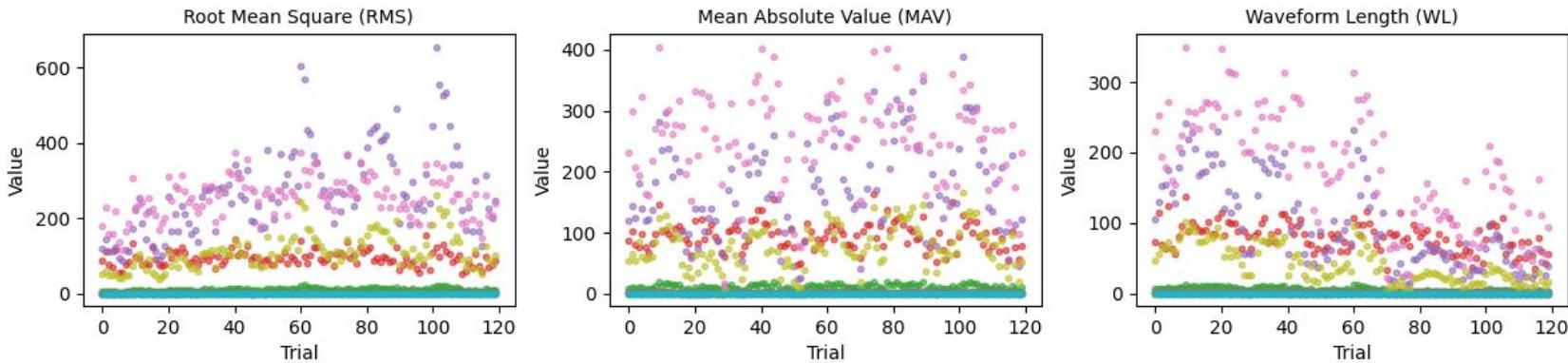
- INTEGRATED EMG (IEMG)
- VARIANCE (VAR)
- WILLISON AMPLITUDE (WAMP)

### FREQUENCY DOMAIN

- POWER SPECTRAL DENSITY (PSD)

# Feature Visualisation

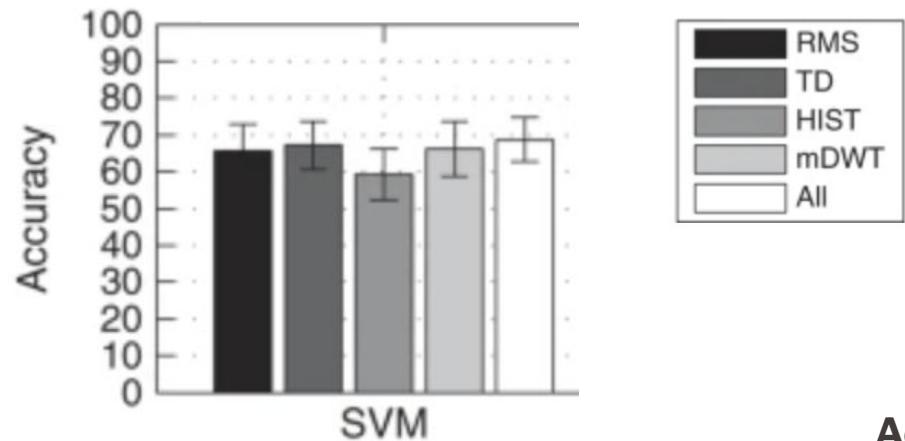
Channels
Ch 1
Ch 2
Ch 3
Ch 4
Ch 5
Ch 6
Ch 7
Ch 8
Ch 9
Ch 10



Feature values differ between channels but remain relatively consistent within each channel for repeated executions of the same movement

# Support Vector Machine Performance

Features	Best Model	Val accuracy	Test accuracy
All	RBF / C=1	0.96	0.84



Atzori et al. 2014  
Best Accuracy: ~70%  
Accuracy depends on feature set used

# Dimensionality Reduction

Features	Best Model	Val accuracy	Test accuracy
All	RBF / C=1	0.96	0.84

**Recursive  
Feature  
Elimination  
(RFE)**

**Principal  
Component  
Analysis  
(PCA)**

**Mutual  
Information**

# Dimensionality Reduction

Features	Best Model	Val accuracy	Test accuracy
All	RBF / C=1	0.96	0.84
RFE top 15	RBF / C=1	0.88	1
PCA 10 components	RBF / C=10	0.92	0.92
Mutual Info top 25	Linear / C=10	0.88	0.75

**Recursive  
Feature  
Elimination  
(RFE)**

**Principal  
Component  
Analysis  
(PCA)**

**Mutual  
Information**

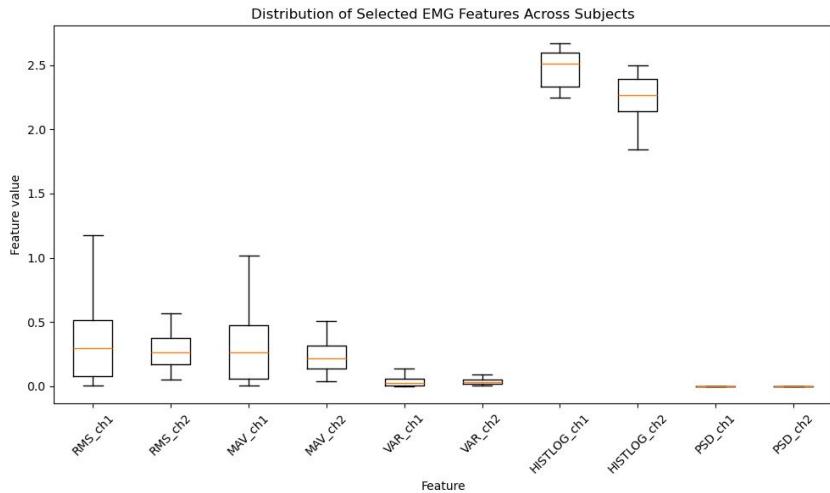
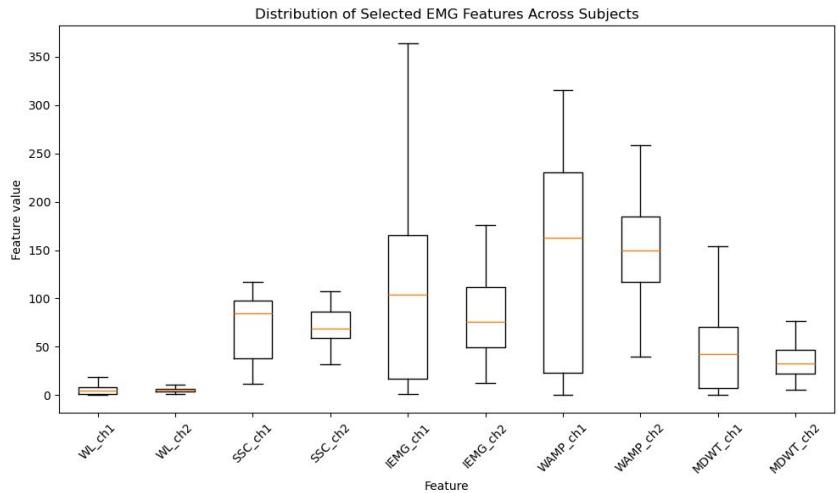
# PART 2

GENERALISATION ACROSS SUBJECTS

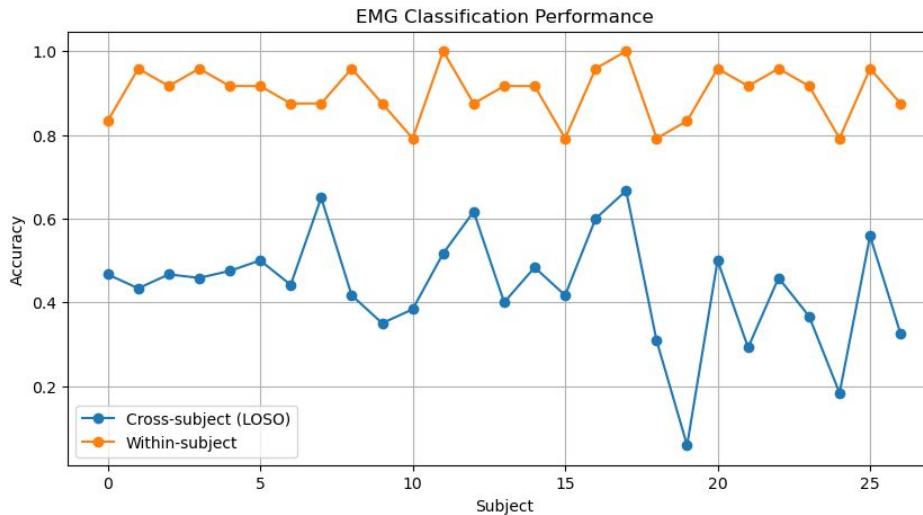
# Preprocessing + Feature Extraction

COMPLETE DATASET

27 Subjects - 10 Features

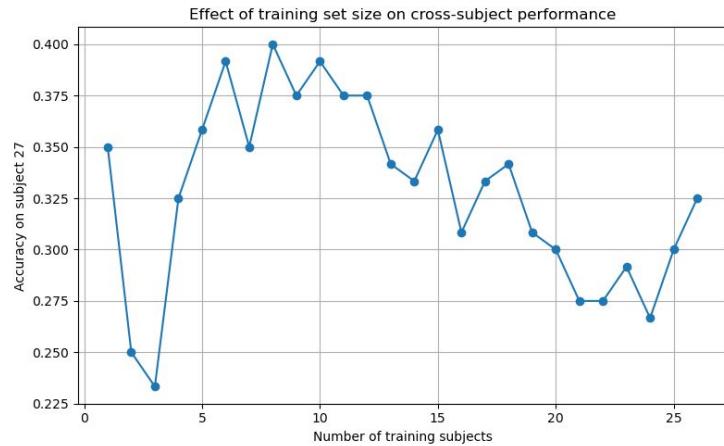


# Cross-subject Classification

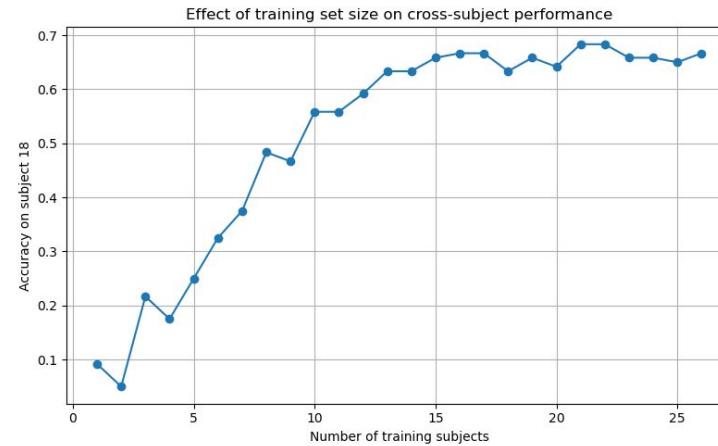


Mean cross-subject accuracy:  $0.44 \pm 0.13$   
Mean within-subject accuracy:  $0.90 \pm 0.06$

# Effect of Training Set Size

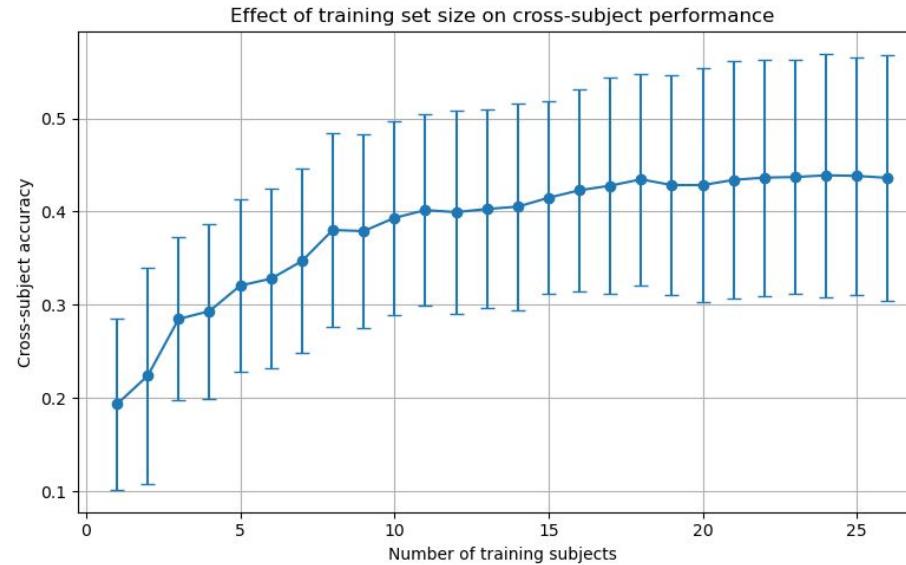


Accuracy for Subject #27



Accuracy for Subject #18

# Effect of Training Set Size

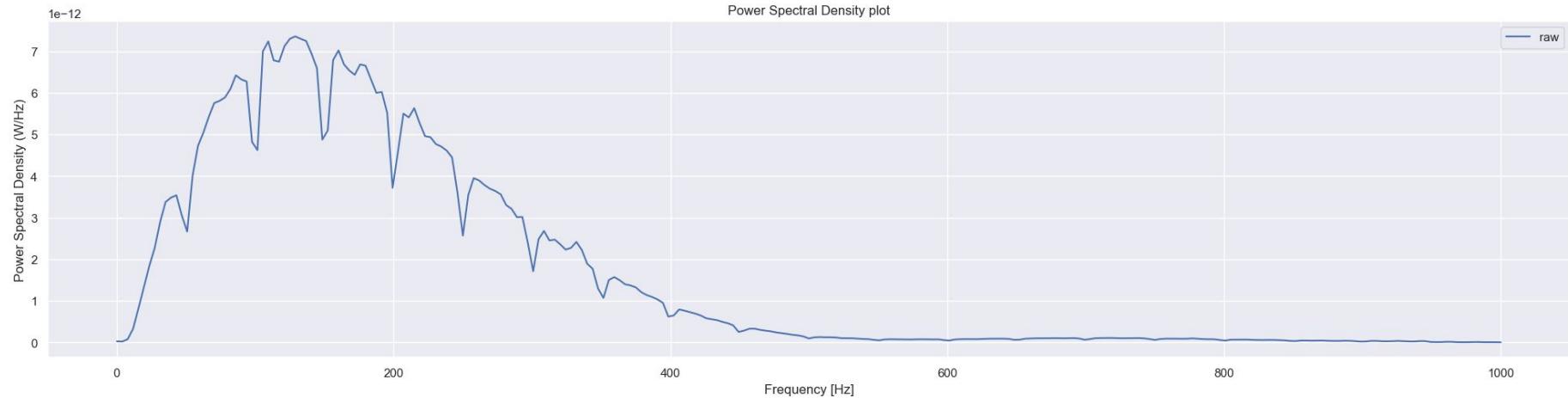


performance gains became smaller beyond a moderate number of training subjects (e.g. 15)

# PART 3

REGRESSION FOR JOINT ANGLES

# Preprocessing and Splitting



**Validation set:** repetitions 2 and 7

**Test set:** repetition 5

**Train set:** other repetitions

Sliding windows:

1. 128 ms per window ( 256 data points per window)
2. 50ms second incremental increase (100 data points increase)

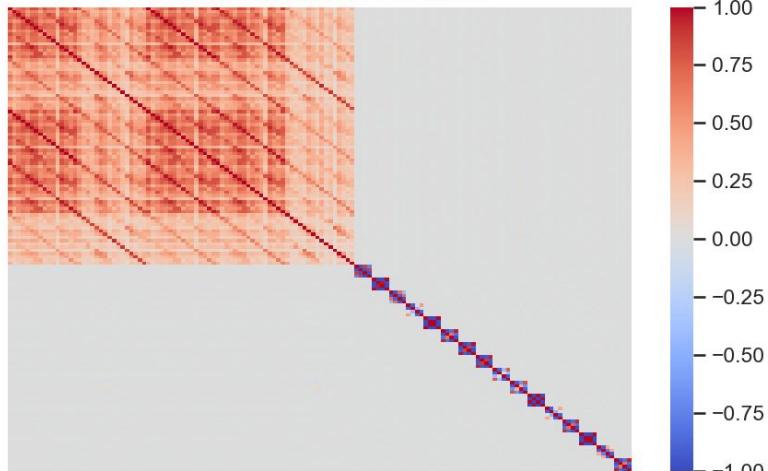
Taken from literature - [Krasoulis et al., Effect of user adaptation on prosthetic finger control with an intuitive myoelectric decoder. Frontiers in Neuroscience, 2019](#)



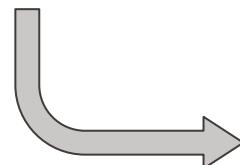
(60% overlap)

# Feature Extraction and Correlation

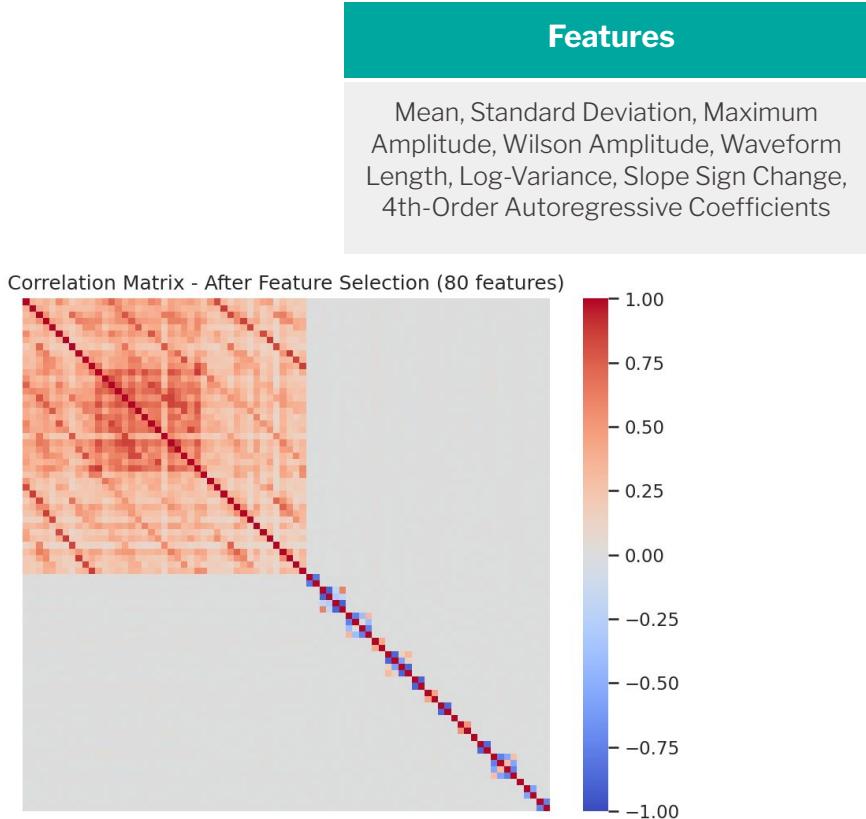
Correlation Matrix of 144 Features



16 channels x 11 features = 176 features.  
144 after removing the constant features.  
**We selected only 80 final features after  
removing one of the feature from  
feature-pairs which were the most  
correlated.**



Correlation Matrix - After Feature Selection (80 features)



# Hyperparameters optimization

Kernel / C	0.01	0.1	1	10	100
linear	694.53	586.32	579.65	578.98	584.07
rbf	1042.09	932.74	550.88	352.97	303.82

**FIGURE 3.4**  
SVR performance (MSE) comparison

We test different models to find the optimal hyperparameters

# Metric Choice and final results

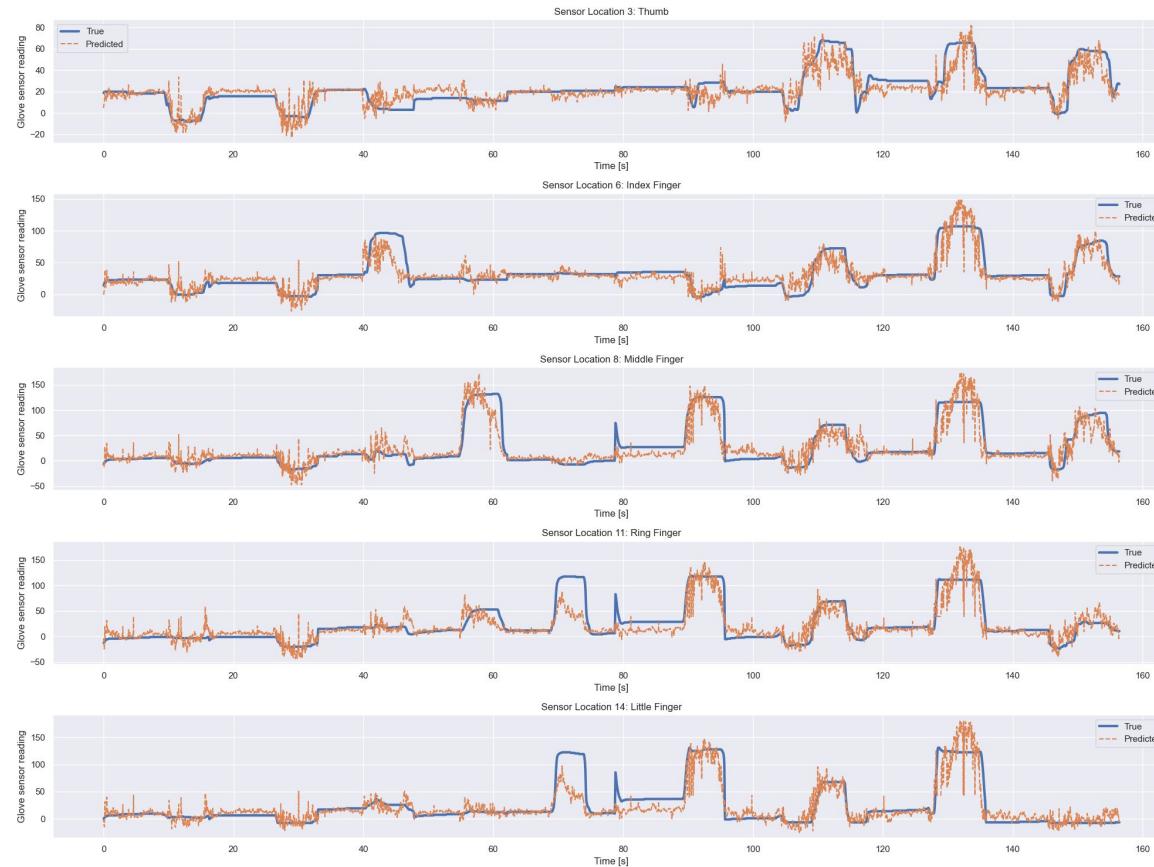
## Metric used: $R^2$

MSE penalizes large errors and is optimal for Gaussian noise assumptions, but  $R^2$  is more appropriate here as it normalizes by label variance. We use  $R^2 = 1 - \text{MSE}/\text{Var}(y)$  to assess test performance.

## Final results:

1.  $R^2 = 0.68$  on validation set
2.  $R^2 = 0.70$  on test set

# Results visualization



# Finger comparison

**FIGURE 3.6**  
 $R^2$  values for each finger sensor location.

Sensor / Finger	Thumb	Index	Middle	Ring	Little
$R^2$	0.700	0.673	0.743	0.675	0.698

Middle finger: dedicated tendon compartment.

Ring finger: biomechanically coupled to adjacent finger.

Thumb: relies on intrinsic hand muscles not captured by forearm sEMG, and extrinsic muscles overlap with wrist muscles, causing crosstalk.

# Team Contributions

Contribution	Team Member
<b>Part I</b>	Pamela van den Enden Uribe, Khushi Singh, Arnault Dominic Philippe Stähli
<b>Part II</b>	Heliya Shakeri
<b>Part III</b>	Arnault Dominic Philippe Stähli, Angana Mondal

## References

Atzori, M., Gijsberts, A., Castellini, C., Caputo, B., Hager, A.-G. M., Elsig, S., Giatsidis, G., Bassetto, F., & Müller, H. (2014). Electromyography data for non-invasive naturally-controlled robotic hand prostheses. *Scientific Data*, 1, 140053.

<https://doi.org/10.1038/sdata.2014.53>

Hudgins, B., Parker, P., & Scott, R. N. (1993). A new strategy for multifunction myoelectric control. *IEEE Transactions on Biomedical Engineering*, 40(1), 82–94.

**THANK YOU!**

# References

- Atzori, M., Gijsberts, A., Castellini, C., Caputo, B., Hager, A.-G. M., Elsig, S., Giatsidis, G., Bassetto, F., & Müller, H. (2014). Electromyography data for non-invasive naturally-controlled robotic hand prostheses. *Scientific Data*, 1, 140053.  
<https://doi.org/10.1038/sdata.2014.53>
- Hudgins, B., Parker, P., & Scott, R. N. (1993). A new strategy for multifunction myoelectric control. *IEEE Transactions on Biomedical Engineering*, 40(1), 82–94.

# Feature Selection

## TIME DOMAIN FEATURES

ROOT MEAN  
SQUARE (RMS)

MEAN ABSOLUTE  
VALUE (MAV)

WAVEFORM  
LENGTH (WL)

SLOPE SIGN  
CHANGE (SSC)

INTEGRATED  
EMG (IEMG)

VARIANCE  
(VAR)

WILLISON  
AMPLITUDE (WAMP)

HISTOGRAM

## FREQUENCY DOMAIN FEATURES

POWER SPECTRAL  
DENSITY (PSD)

MARGINAL DISCRETE  
WAVELET TRANSFORM

Sources:  
[Atzori et al. \(2014\)](#)  
NX421 lectures/labs

# Feature Selection

## TIME DOMAIN FEATURES

### ROOT MEAN SQUARE (RMS)

Overall power of the signal

### MEAN ABSOLUTE VALUE (MAV)

Average amplitude of rectified signal

### WAVEFORM LENGTH (WL)

Cumulative variation or complexity of signal.

### SLOPE SIGN CHANGE (SSC)

Number of slope changes in signal.

### INTEGRATED EMG (IEMG)

Summation |EMG| signal over time.

### VARIANCE (VAR)

Power or spread of EMG signal.

### WILLISON AMPLITUDE (WAMP)

# times the amplitude exceeds set threshold.

### HISTOGRAM

Log of amplitude histogram to quantify signal complexity

## FREQUENCY DOMAIN FEATURES

### POWER SPECTRAL DENSITY (PSD)

Mean power distribution

### MARGINAL DISCRETE WAVELET TRANSFORM

Sum of absolute wavelet coefficients across all levels per channel (3 levels)

Sources:  
[Atzori et al. \(2014\)](#)  
NX421 lectures/labs