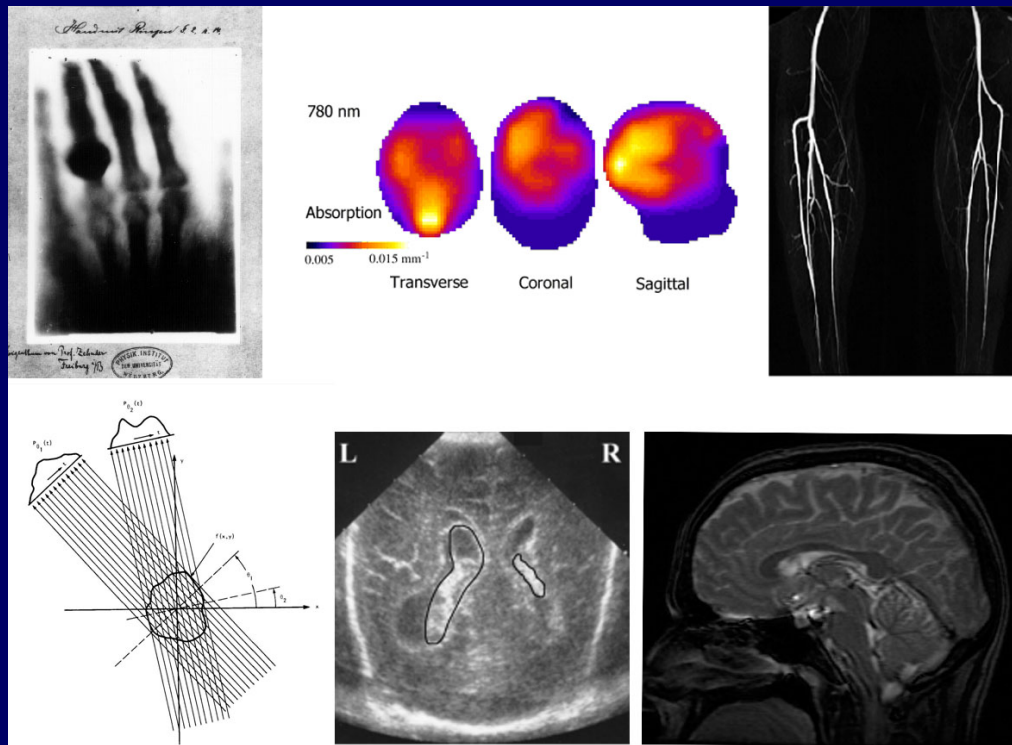


The Mathematics of Medical Imaging: What Is Essential is Invisible to the Eyes



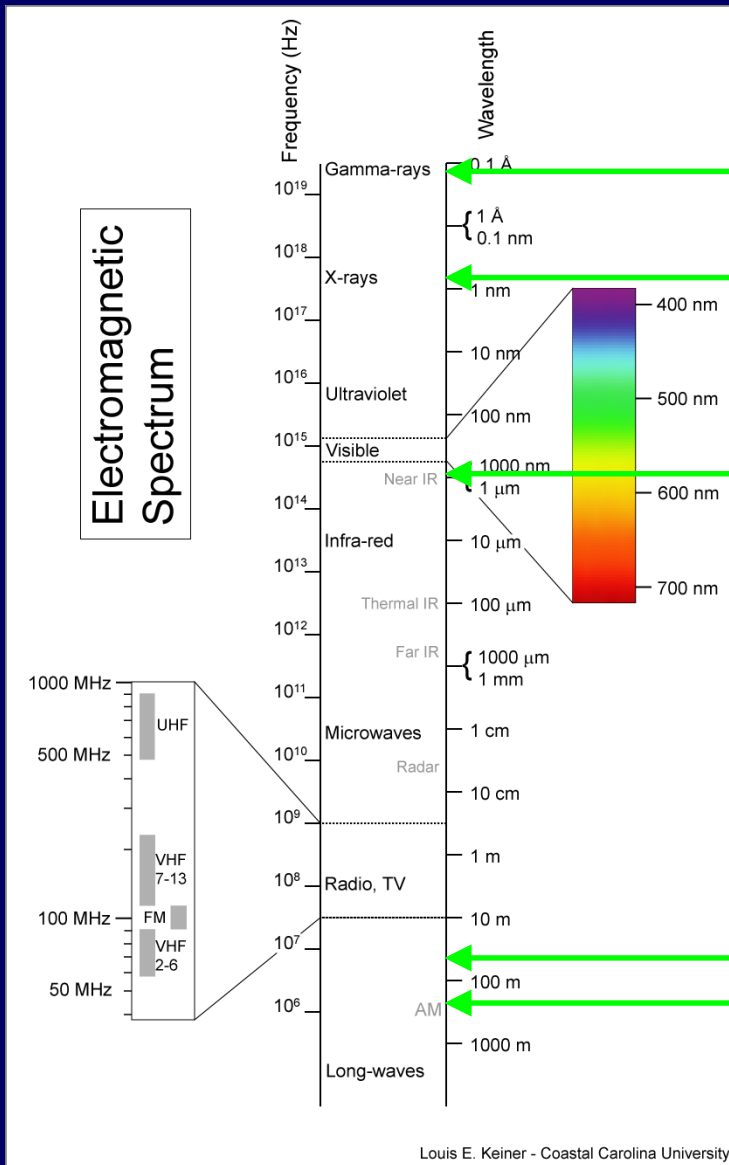
Angel R. Pineda
Manhattan College
Riverdale, NY



Monmouth Math Colloquium
Nov. 6, 2015



Imaging Using Electromagnetic Waves



Nuclear Medicine: PET, SPECT

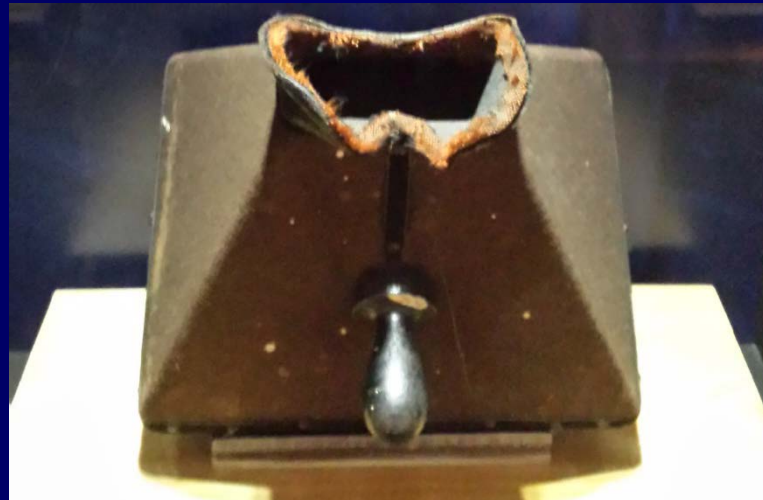
X-ray Imaging: Mammography, CT scans

Diffuse Optical Imaging

Radio Frequency Excitation in MRI
Ultrasound

Nobel History of Medical Imaging

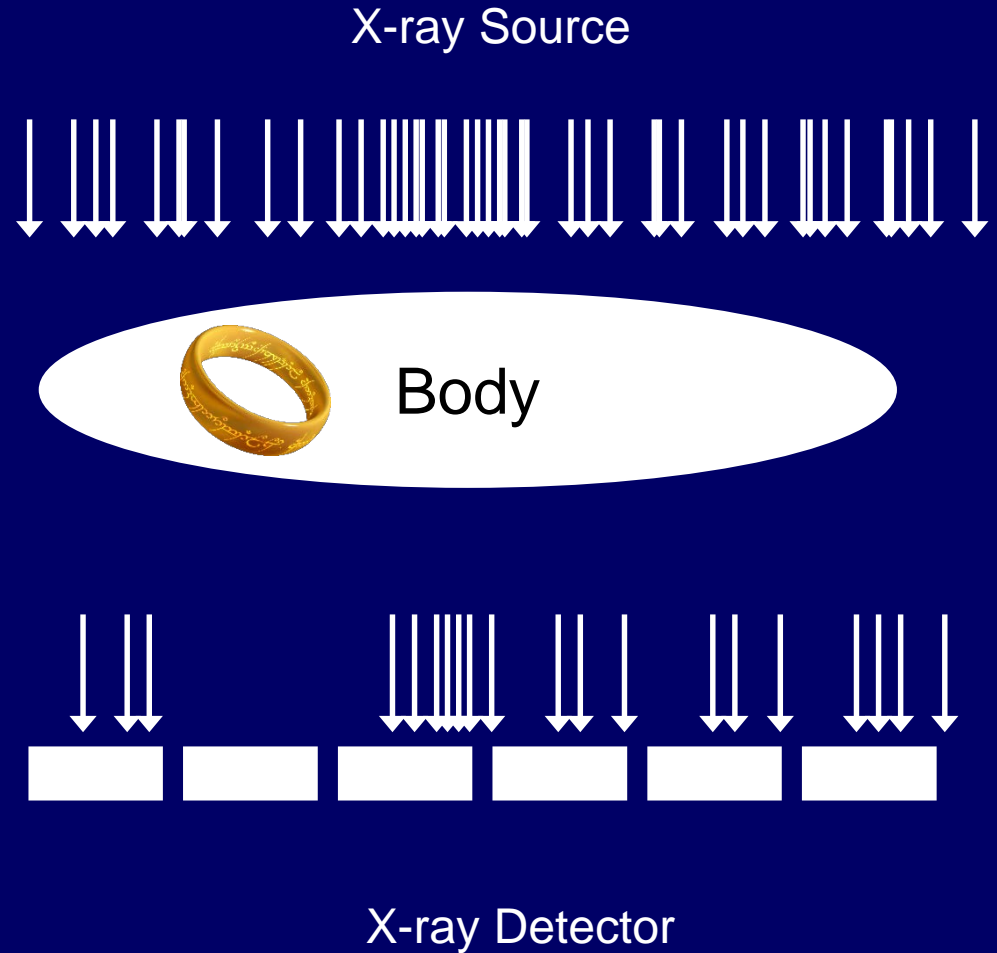
- In 1901 Roentgen gets first Nobel Prize in Physics for the discovery of x-rays. An immediate application is medical imaging.
- In 1979 Hounsfield and Cormack get Nobel Prize in Medicine for x-ray Computed Tomography (CT) which allows for cross-sectional imaging.
- In 2003 Lauterbur and Mansfield received the Nobel Prize in Medicine for magnetic resonance imaging (MRI).



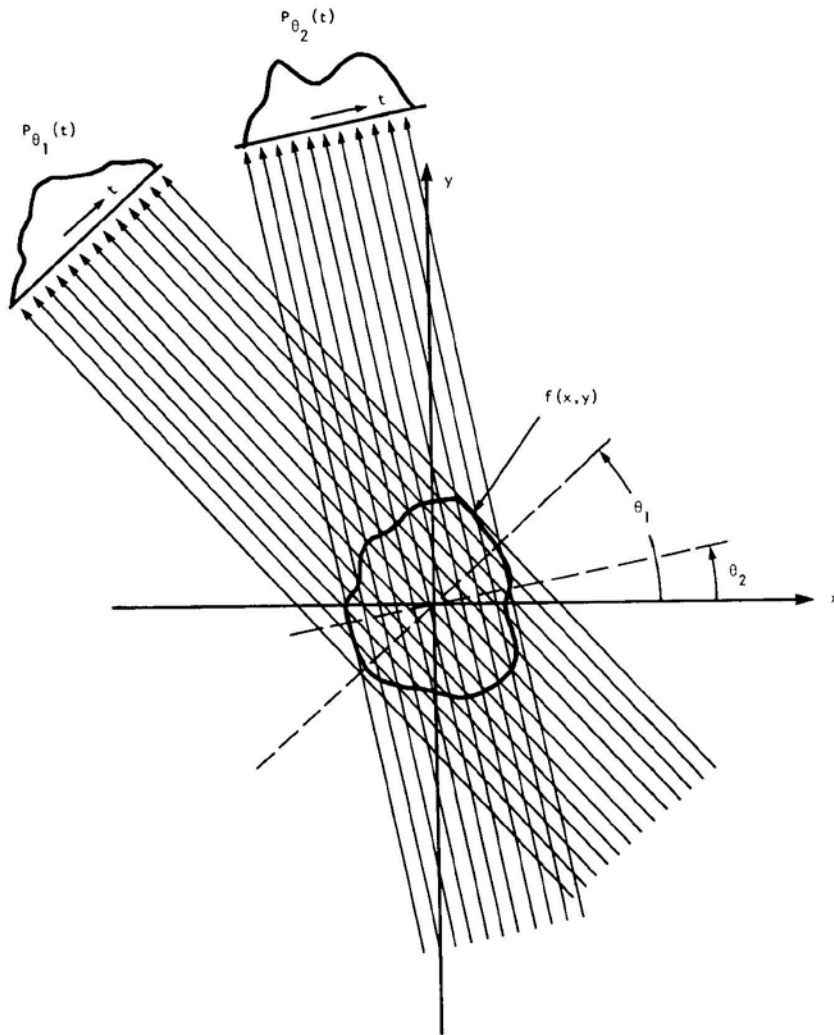
X-ray Imaging (Single Projection)



Image of Anna Bertha Ludwig's hand.
First x-ray image ever produced.



X-ray Projections (2-D Radon Transform)



$$P_{\theta}(t) = \int_{(\theta, t) \text{ line}} f(x, y) ds.$$

From Kak and Slaney, Principles of Computerized Tomographic Imaging

Inverting the Radon Transform

- Take the Fourier Transform of Projections
- Multiply by Judicious Weighting Function (Filter)
- Smear Back Filtered Projections (Backproject)
- Modern reconstruction in CT is based on Filtered Backprojection (Note: Hounsfield iteratively solved the linear system.)

Show MATLAB Simulation of CT

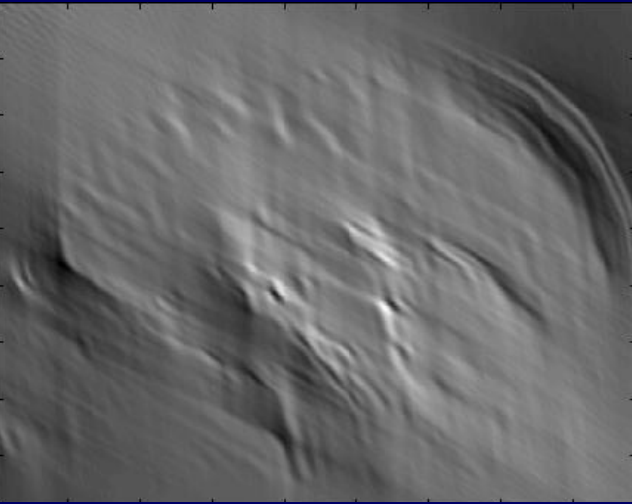


Image with 60 projections

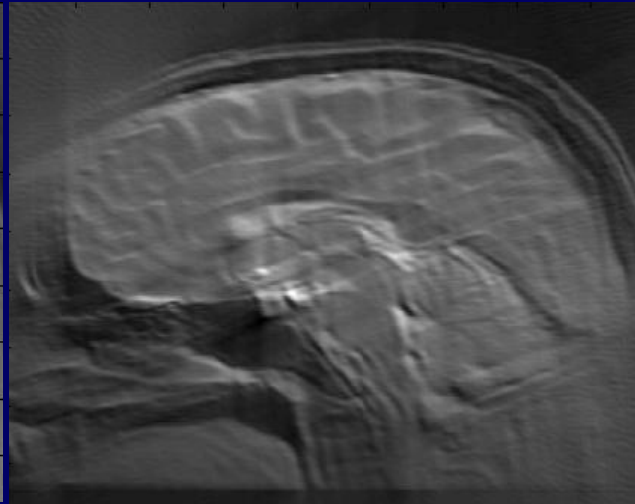


Image with 120 projections

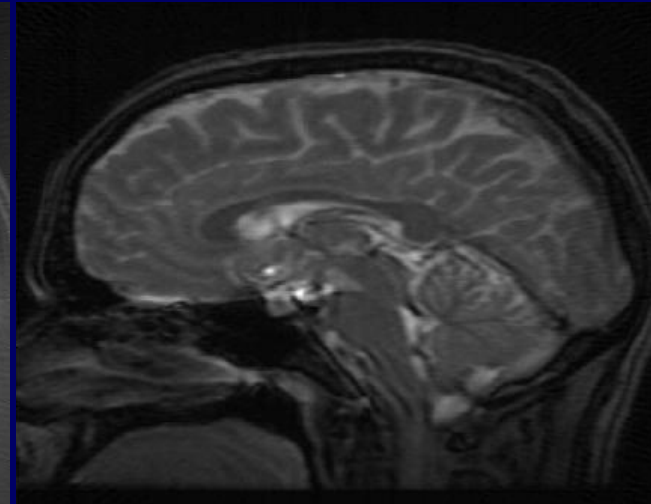
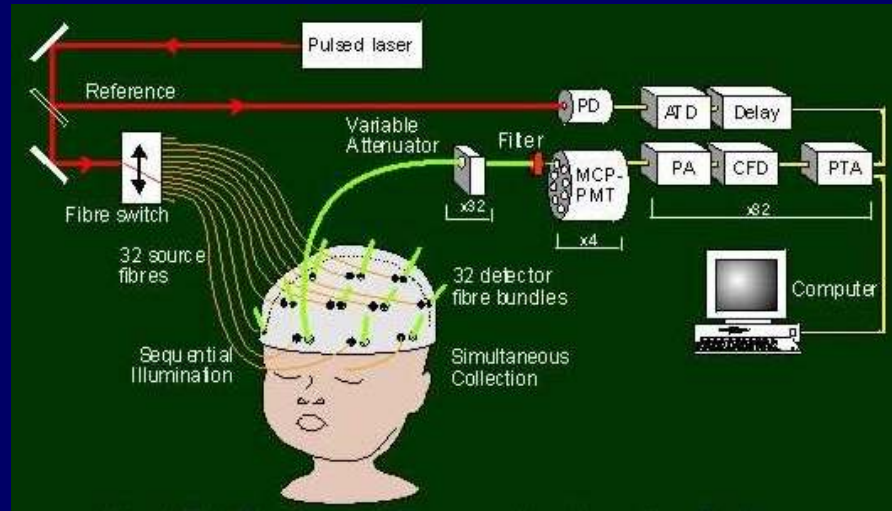


Image with 180 projections

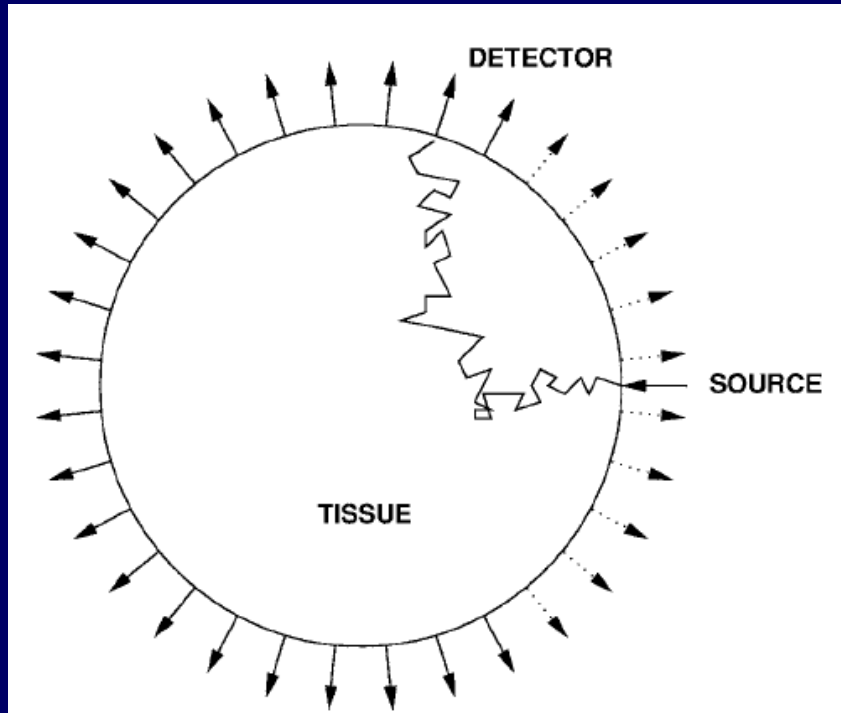
Optical Tomography: The Instrument



MONSTIR
(**M**ulti-channel **O**pto-electronic
Near-infrared **S**ystem for
Time-resolved **I**mage **R**econstruction)
at University College London.



Optical Tomography: The Model



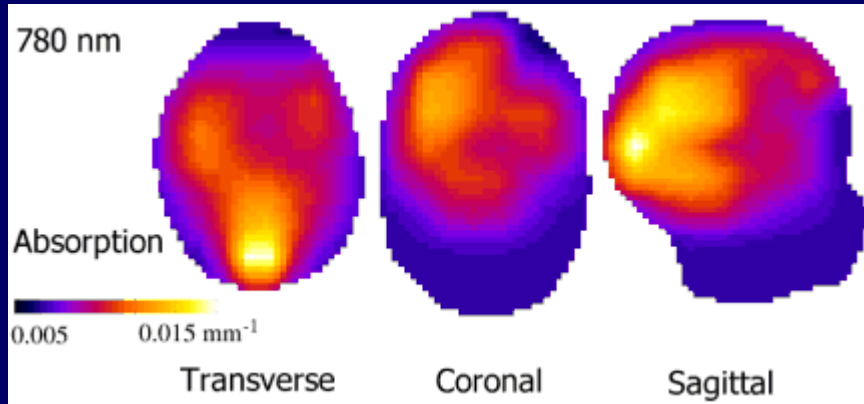
$$\frac{1}{c} \frac{\partial \Phi(\mathbf{r}, t)}{\partial t} - \nabla \cdot k(\mathbf{r}) \nabla \Phi(\mathbf{r}, t) + \mu_a(\mathbf{r}) \Phi(\mathbf{r}, t) = q_o(\mathbf{r}, t)$$

Φ is the photon density,
 μ_a is the attenuation coefficient,
 q_o is the source,
 k is the diffusion coefficient and
 c is the speed of light in the medium.

The optical parameters of tissue (k and μ_a) vary with blood volume and oxygenation.

Our goal is to estimate them from the boundary measurements.

Optical Tomography: The Images

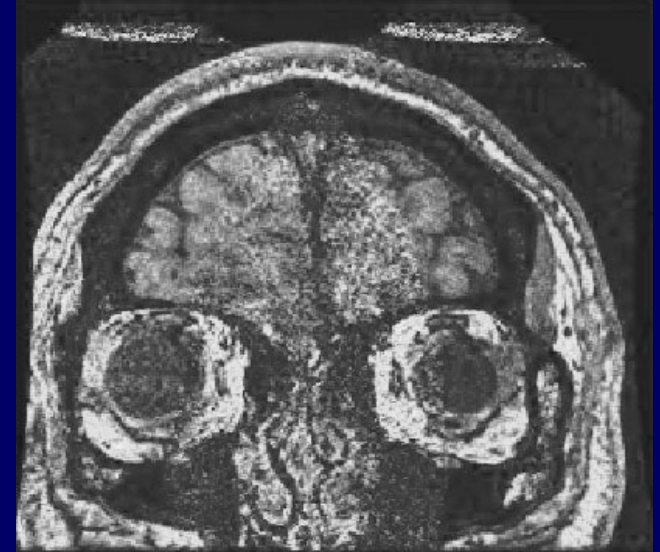
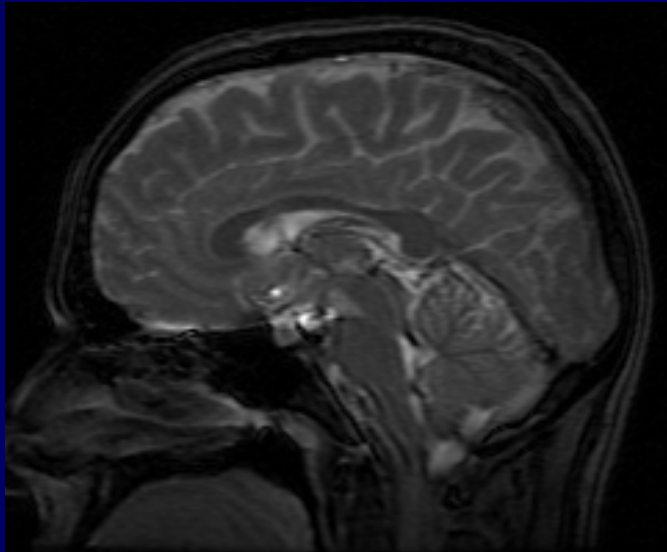
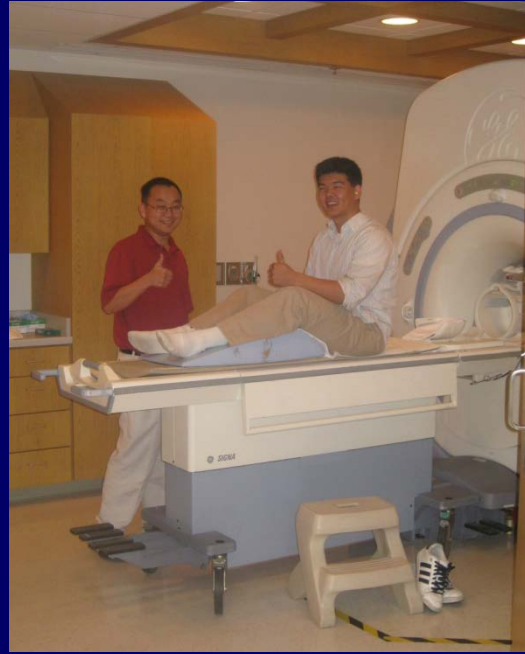


Optical Tomography



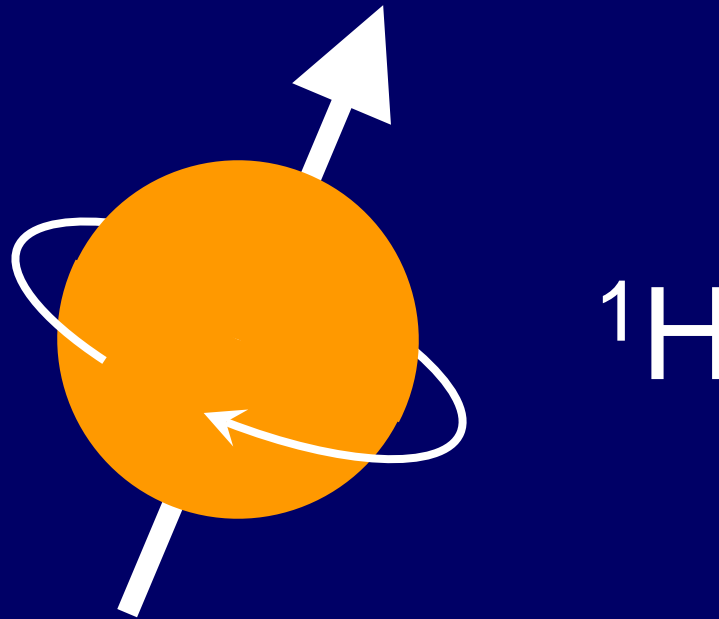
Ultrasound Image to Validate Result

Magnetic Resonance Imaging (MRI)



Magnetic Resonance

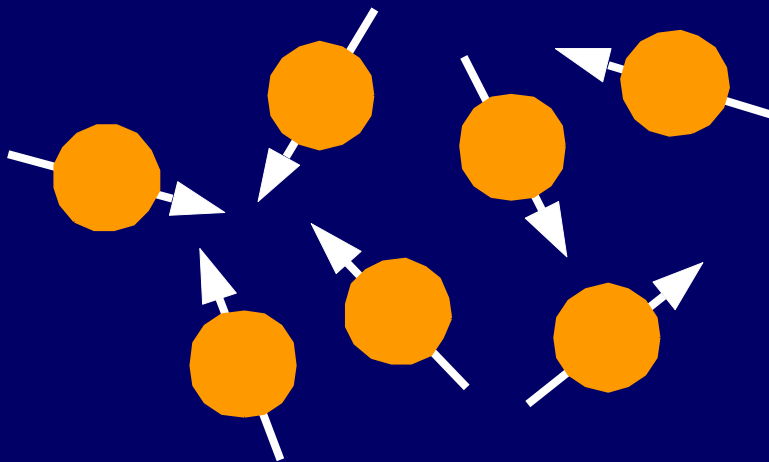
- Certain atomic nuclei including ^1H exhibit nuclear magnetic resonance.
- Nuclear “spins” are like magnetic dipoles.



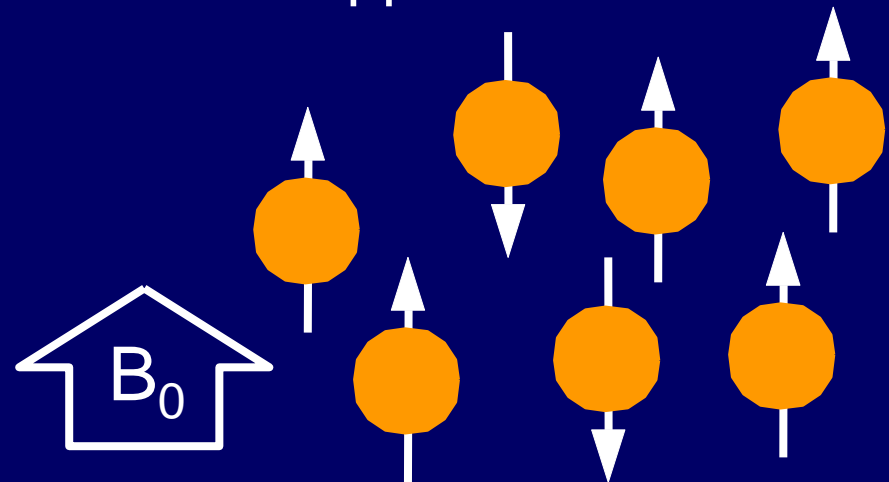
Polarization

- Spins are normally oriented randomly.
- In an applied magnetic field, the spins align with the applied field in their equilibrium state.
- Excess along B_0 results in net magnetization.

No Applied Field



Applied Field



How MRI works?

- By modifying the magnetic field we measure the Fourier Transform of the object being imaged.
- We reconstruct the images by applying the Inverse Fourier Transform.

$$F(k) = \int_{-\infty}^{\infty} f(x) e^{-2\pi i x k} dx$$
$$f(x) = \int_{-\infty}^{\infty} F(k) e^{2\pi i x k} dk$$

Statistical Estimation with Limited Data

- The less data (samples of the Fourier transform) one collects, the more sophisticated the mathematics required to create an image.
- An important application is time-resolved imaging in real time.
- Think in terms of constrained Least-Squares Estimation:

$$\hat{o} = \underset{o}{\operatorname{argmin}} \underbrace{(g - Fo)^2}_{\text{Data Agreement}} + \alpha \underbrace{|\nabla_t o|}_{\text{Total Variation Constraint}}$$

Accelerated MRI Movies



Hip Hop



Opera

Courtesy of Krishna Nayak at USC of
SPAN: Speech Production and Articulation kNowledge Group

Some of my Projects

- Noise Analysis of X-ray CT
- Chemical Species Separation in MRI
- Time-Resolved Angiography in MRI
- Uncertainty in Fat-Fraction Estimation using MRI

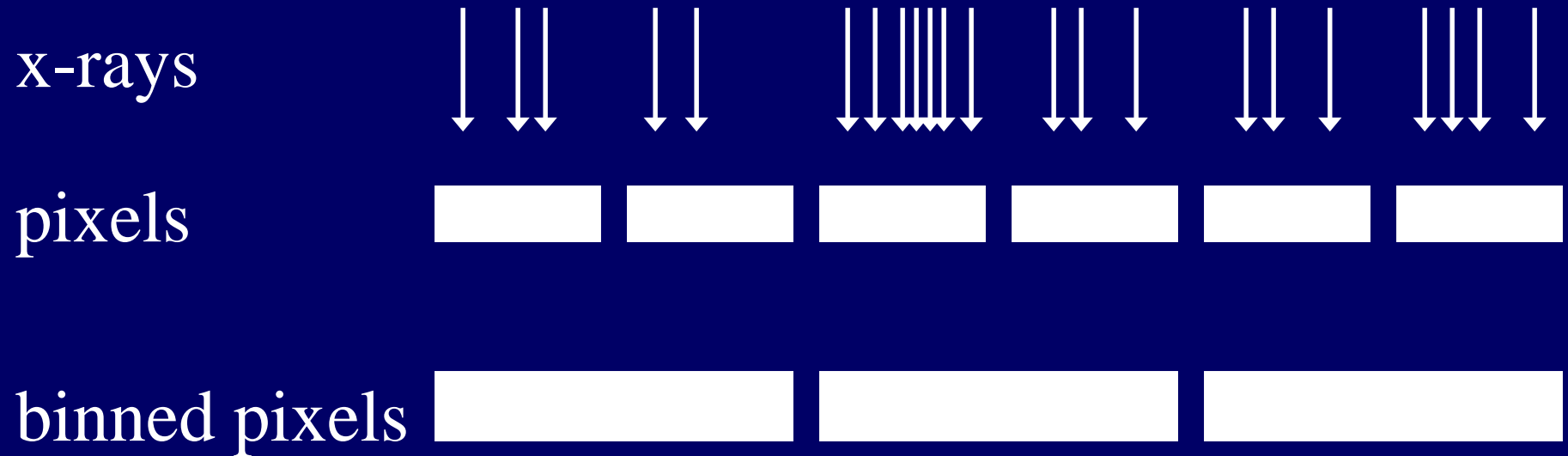
To Bin or Not to Bin in CT?

Collaboration with:

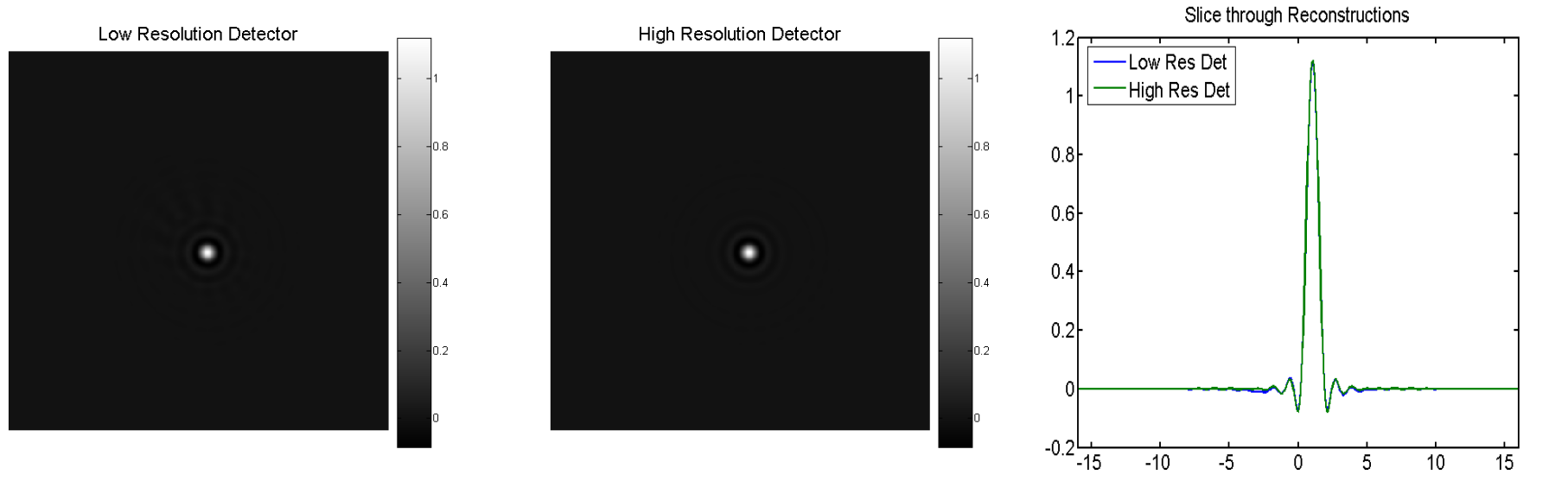
Norbert Pelc, Stanford University

Jongduk Baek, Yonsei University, Korea

Binning



Same Results for Noise-Free Data



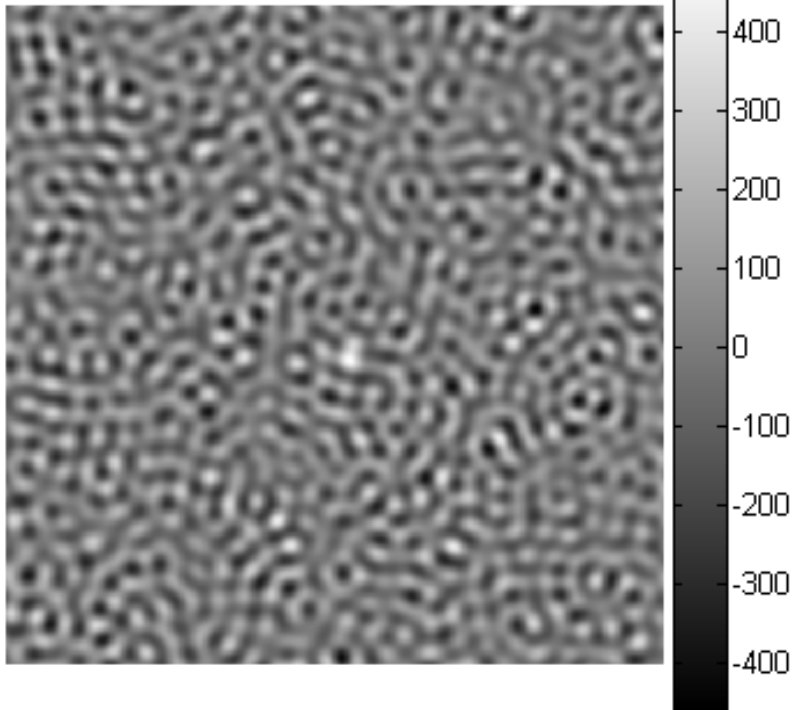
Reconstruction
With Binned Data

Reconstruction With
High Resolution Data

Slices of Both
Reconstructions

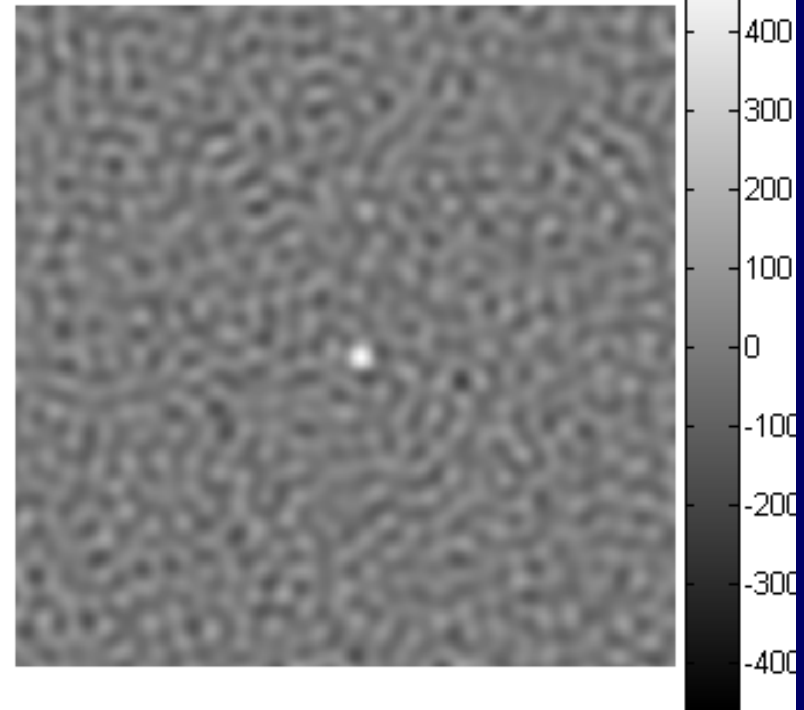
Different Results for Noisy Data!

Low Resolution Detector



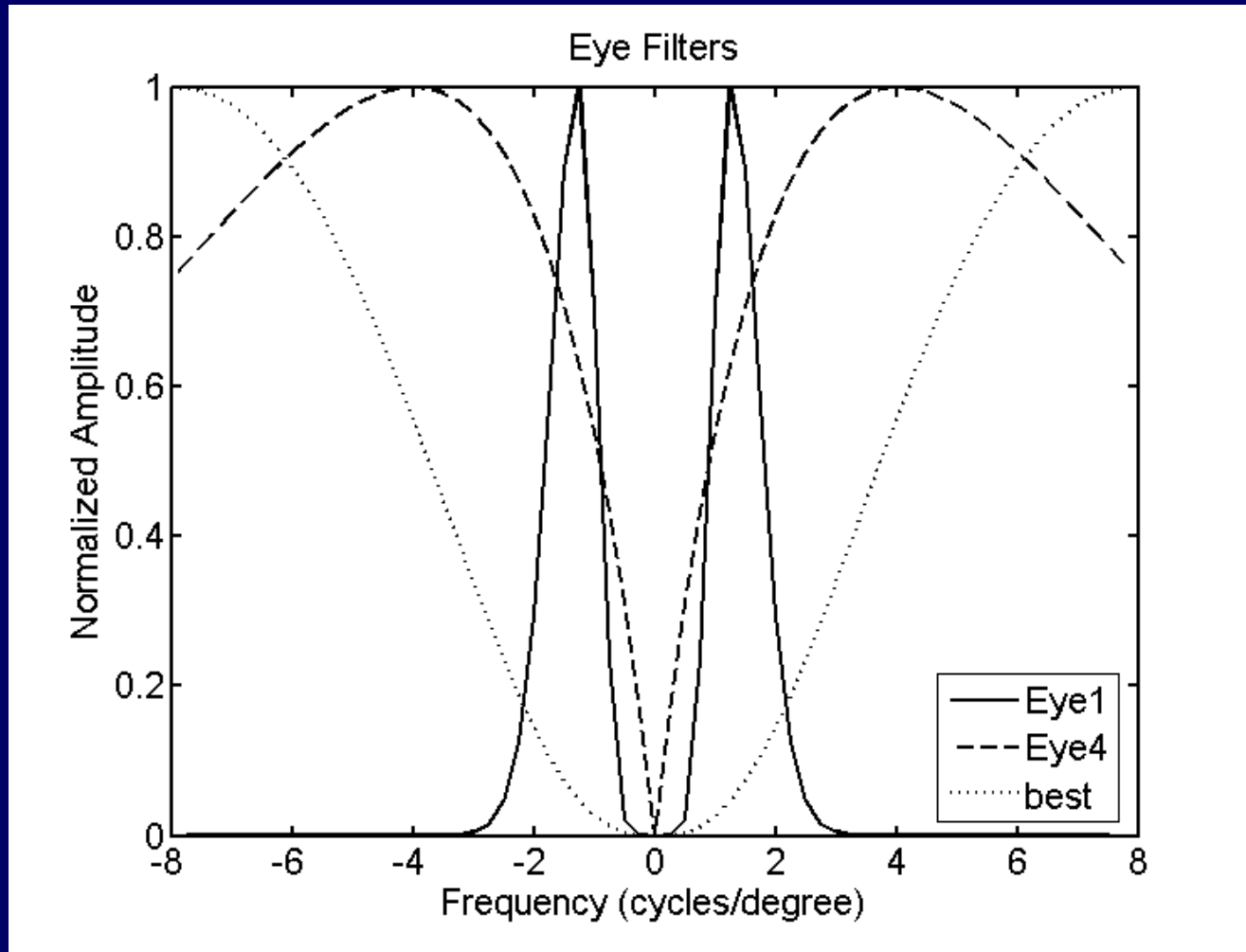
Reconstruction
With Binned Data

High Resolution Detector

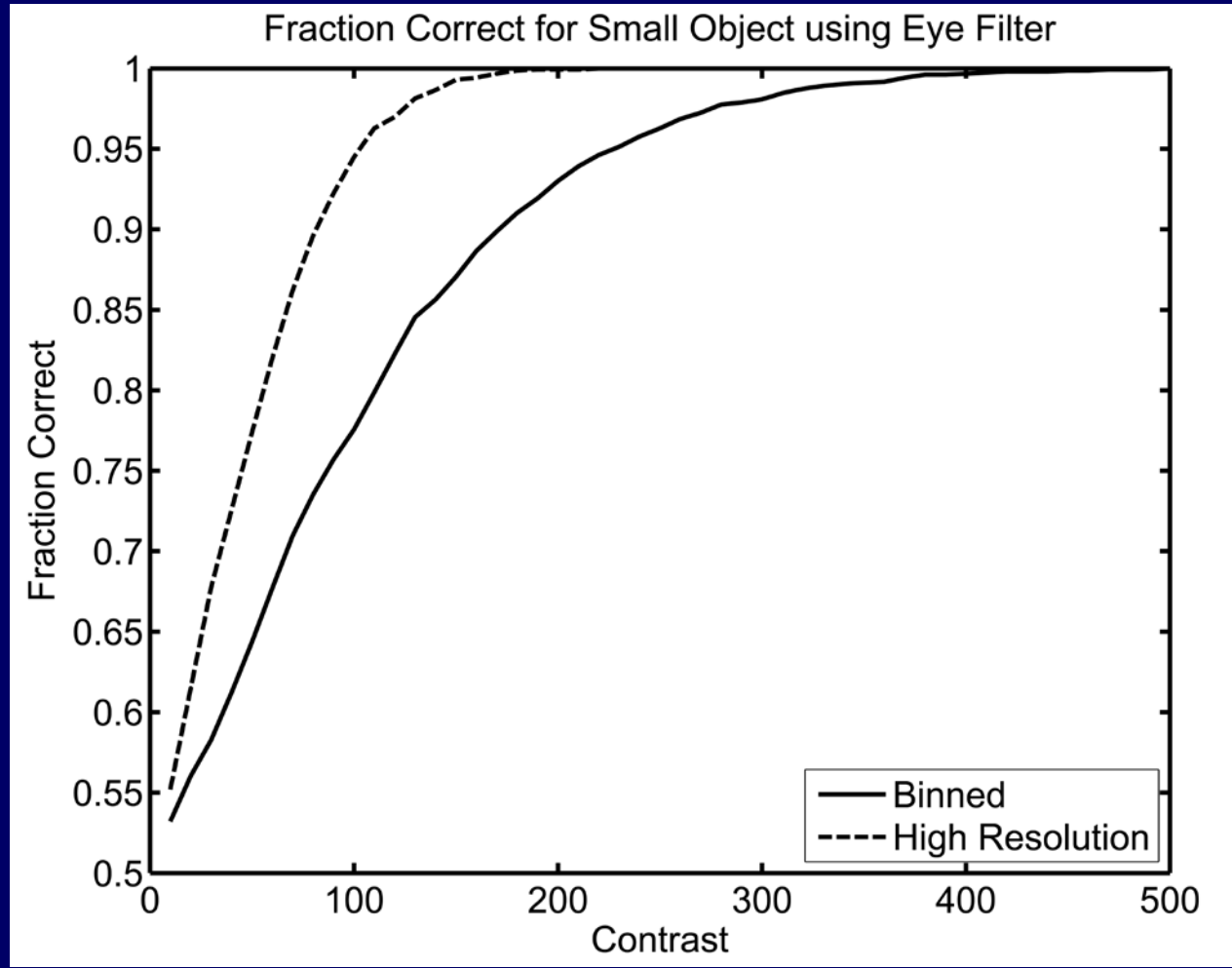


Reconstruction With
High Resolution Data

Eye Filters and Detection Theory



Results Small Object



Fat / Water Separation in MRI

Collaboration with:
UW Madison and GE Healthcare

CSUF Students Involved:
Emily Bice
Joaquin Alvarado

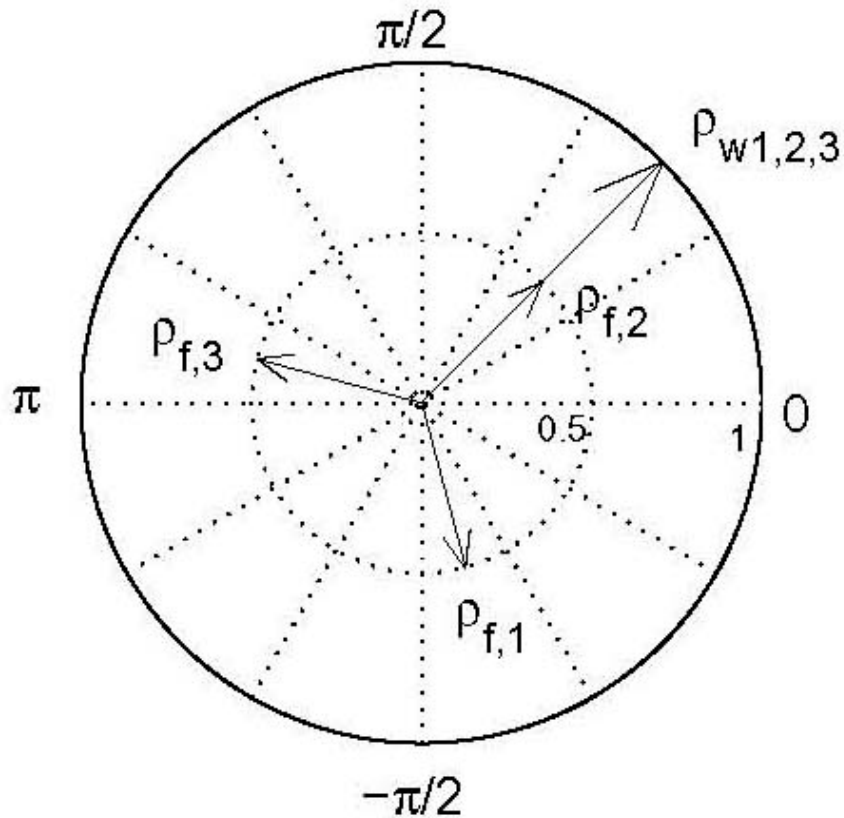
A Simple Model for the Signal

$$s(k) = \left[\rho_w e^{j\phi_w} + \rho_f e^{j(\phi_f + \Delta\phi_k)} \right] e^{j\psi TE_k} + \epsilon.$$

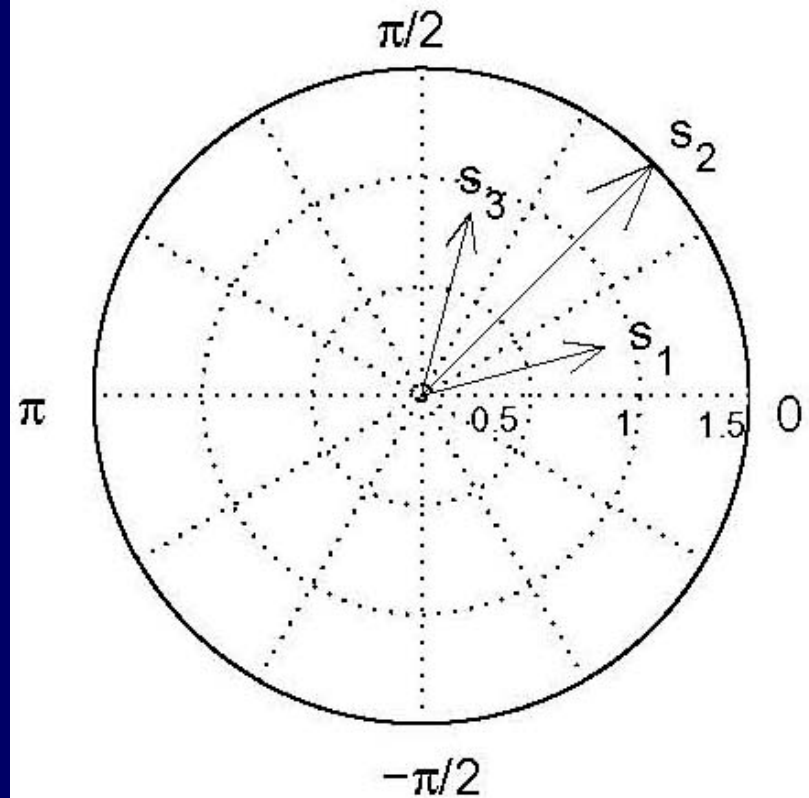
$s(k)$ is the k^{th} complex measurement,
 ρ_w and ϕ_w are the magnitude and phase of water,
 ρ_f and ϕ_f are the magnitude and phase of fat,
 $\Delta\phi_k = \Delta\omega TE_k$ is difference in phase rotation,
 TE_k is the time of the k^{th} image,
 ψ is the field inhomogeneity,
and ϵ is the noise.

Geometric View of Data

a) Fat and Water Signals



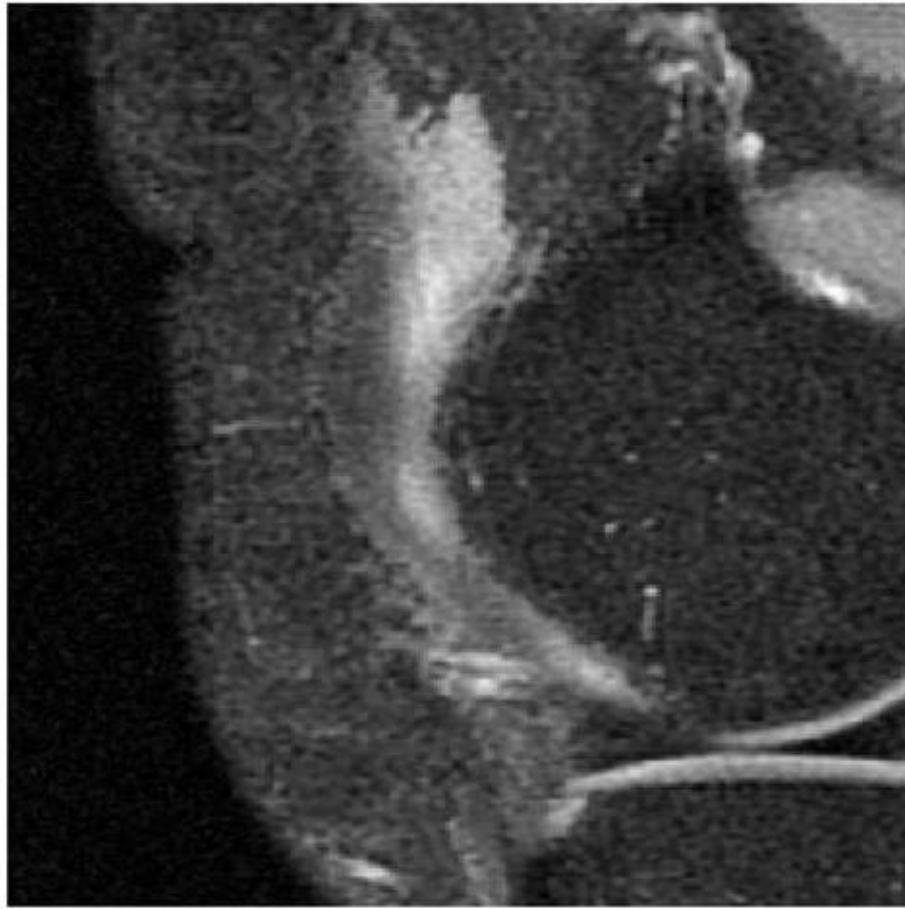
b) Observed Signals



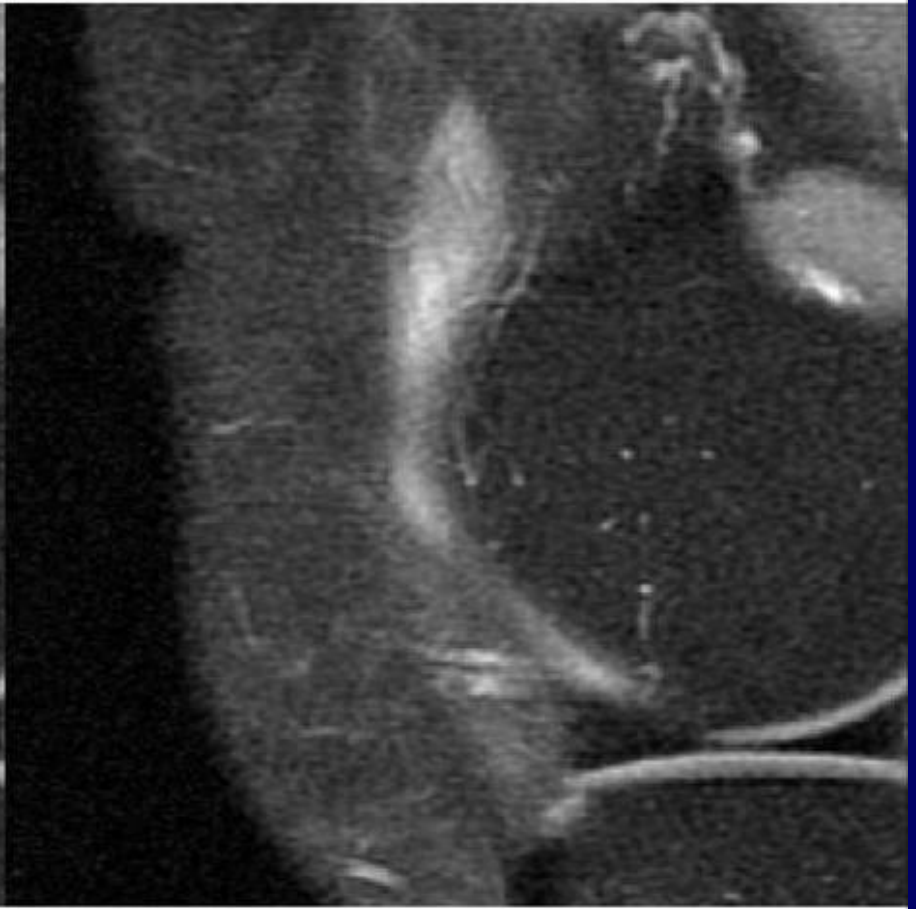
$$\Delta\phi_1 = -\frac{2\pi}{3}, \Delta\phi_2 = 0, \Delta\phi_3 = \frac{2\pi}{3}, \text{ i.e. } \left(-\frac{2\pi}{3}, 0, \frac{2\pi}{3}\right)$$

Theory and the Clinic Come Together!

Which image would you want used to diagnose your knee?



Symmetric Acquisition

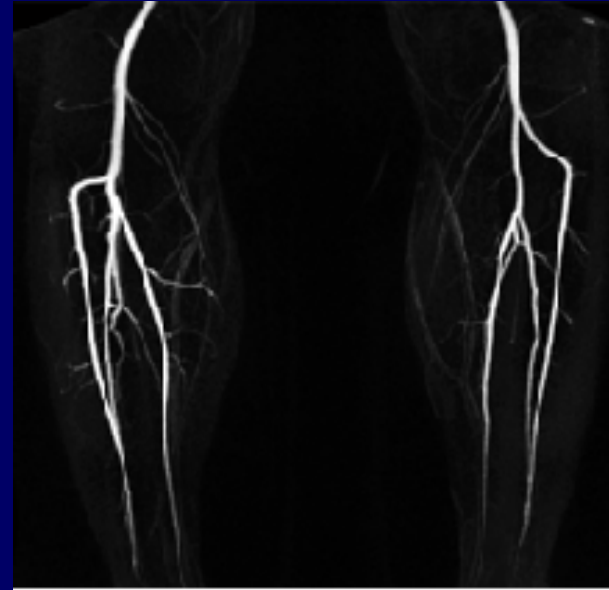


Asymmetric Acquisition

HYPR Applied Math Project (for GE)



Students Not Pictured:
Nasser Abbasi and Siavash Jalal



Leg Angiogram

Co-advisor: Bill Gearhart

Explaining HYPR!

MLEM-1 Algorithm

$$g = Hf + \varepsilon$$

$$f_n^{(1)} = f_n^{(0)} \frac{1}{z_n} \left[H^T \left[\frac{g}{(Hf^{(0)})} \right] \right]_n$$

H

H^T

z_n

g

$f^{(0)}$

HYPR

$$s_t = R_{\phi_t} [I_t]$$

$$J_n = \frac{1}{N_p} C_n \cdot R_{\phi}^u \left(\frac{s}{R_{\phi}(C)} \right)_n$$

R_{ϕ} – Radon Transform

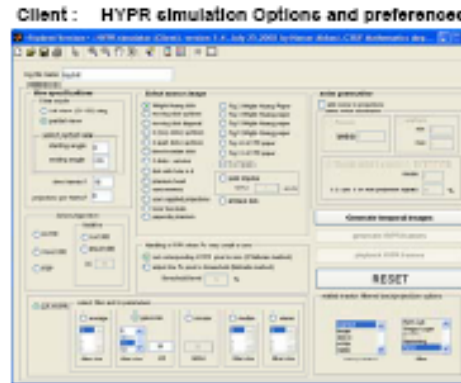
R_{ϕ}^u – Unfiltered backprojection

N_p – Projections per time frame

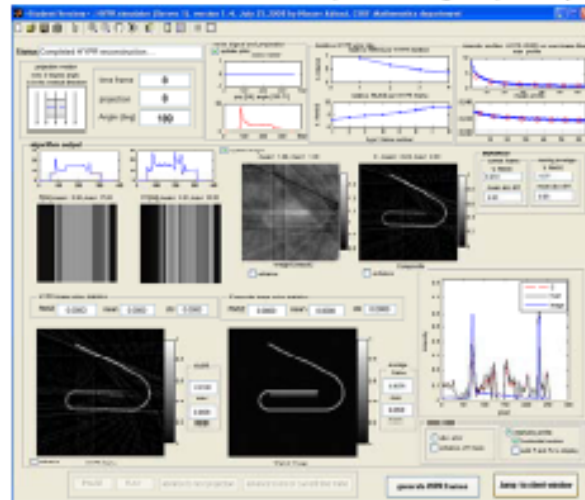
s – Original projection

C – Composite image

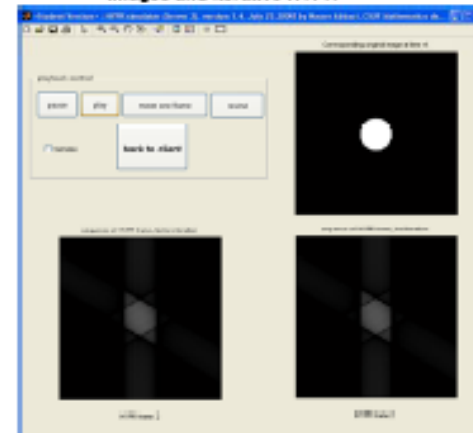
The HYPR Simulator



Server 1: HYPR simulation computation image output and plots

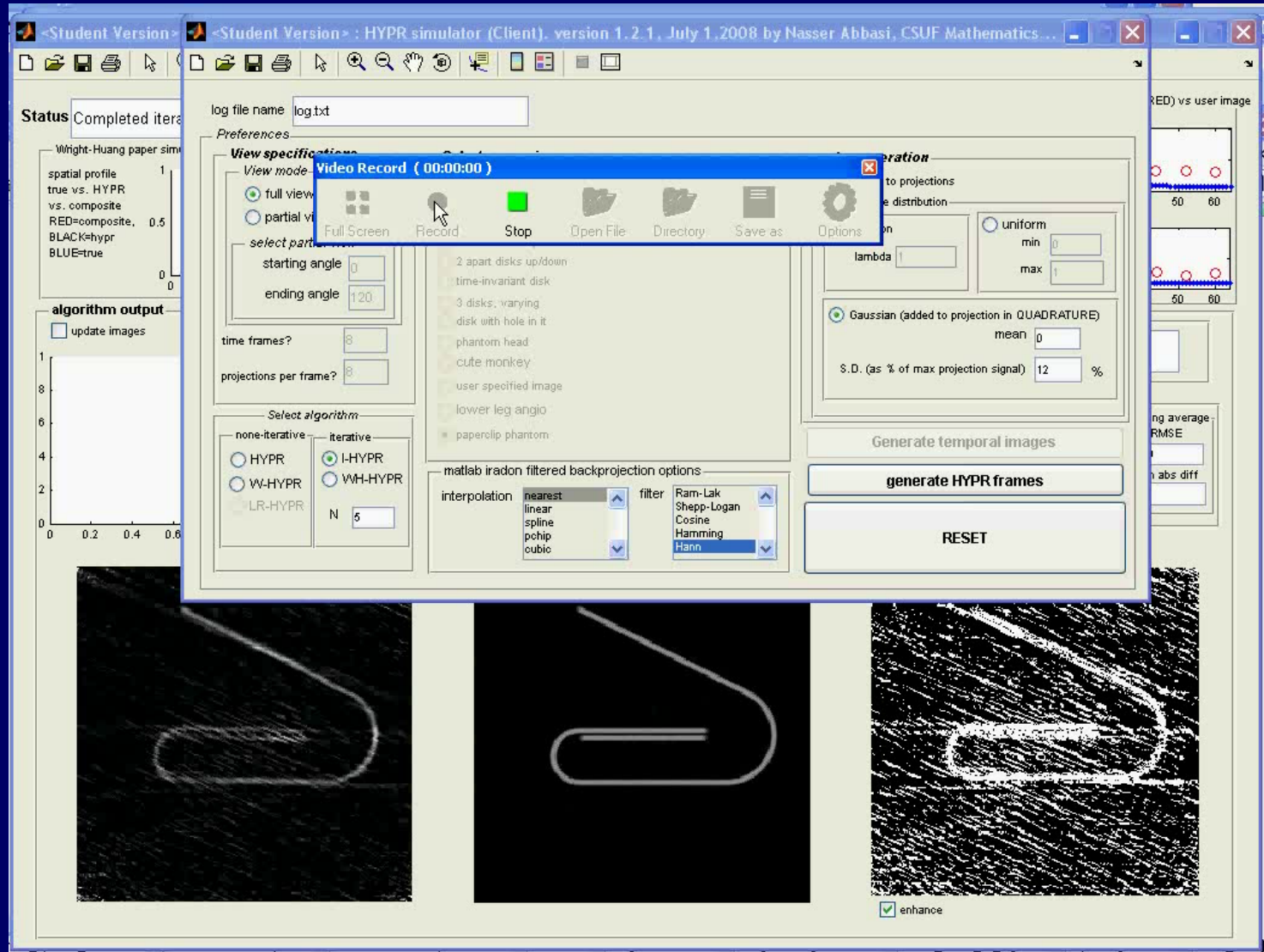


Server 2: Playback of reconstructed HYPR Images and iterative HYPR



HYPR
log file
Log.txt

The Movie



CURM project



Student Collaborators:

Anne Calder

Eden Ellis

Li-Hsuan Huang

Kevin Park

Introduction

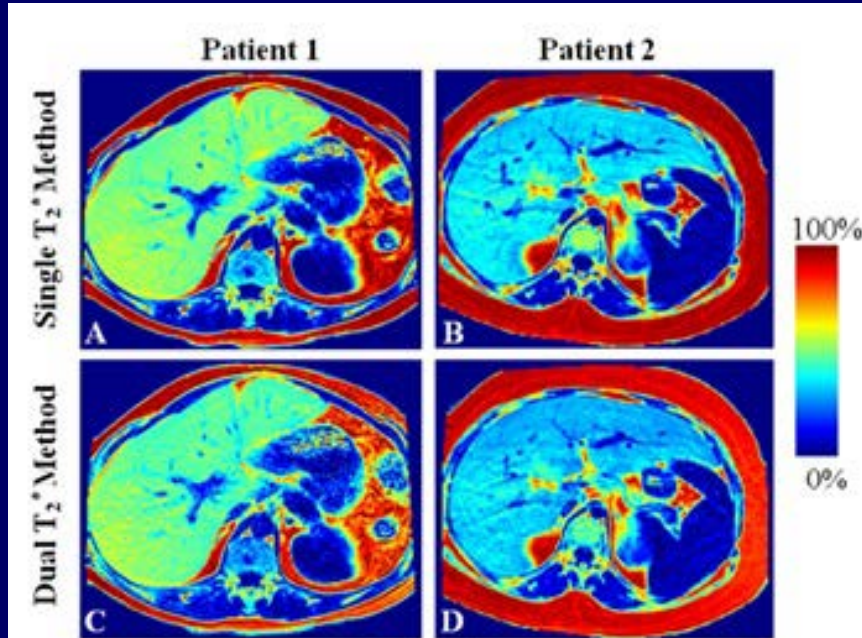
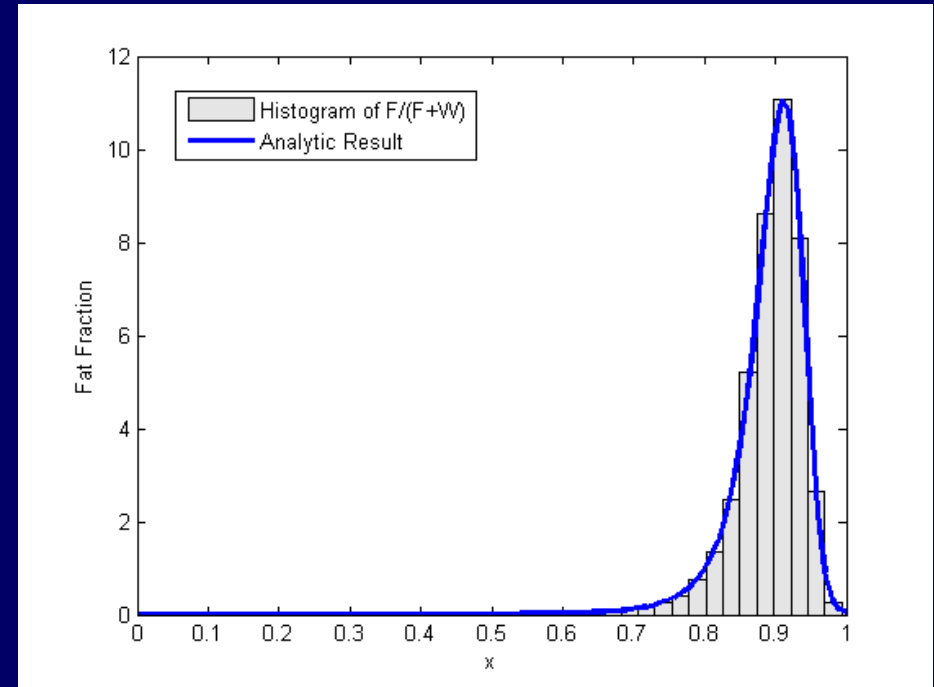
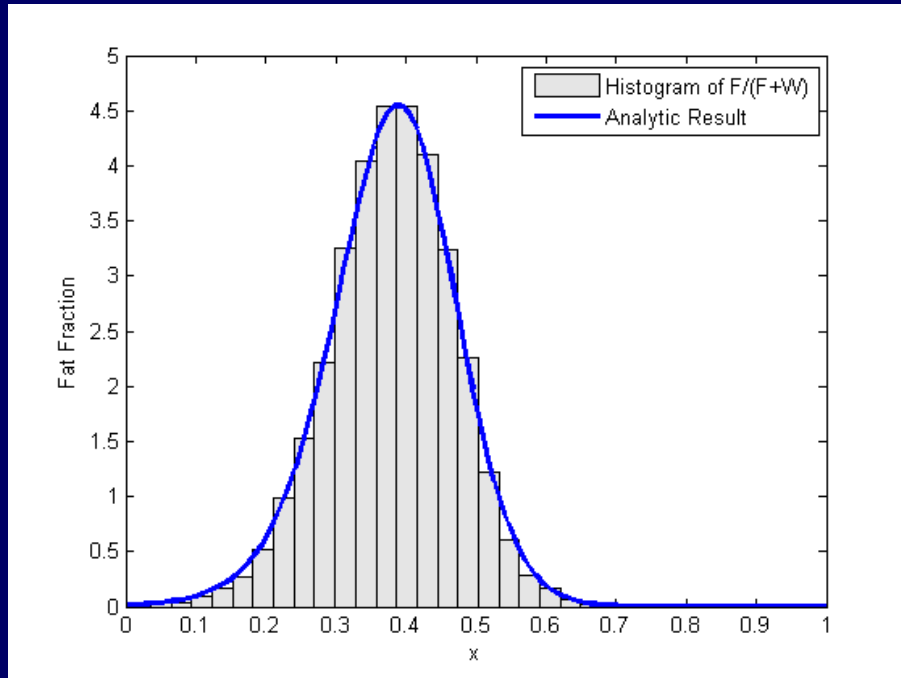


Image courtesy of Reeder, SB.

We want to characterize the uncertainty in measurements of the Fat-Fraction using MRI

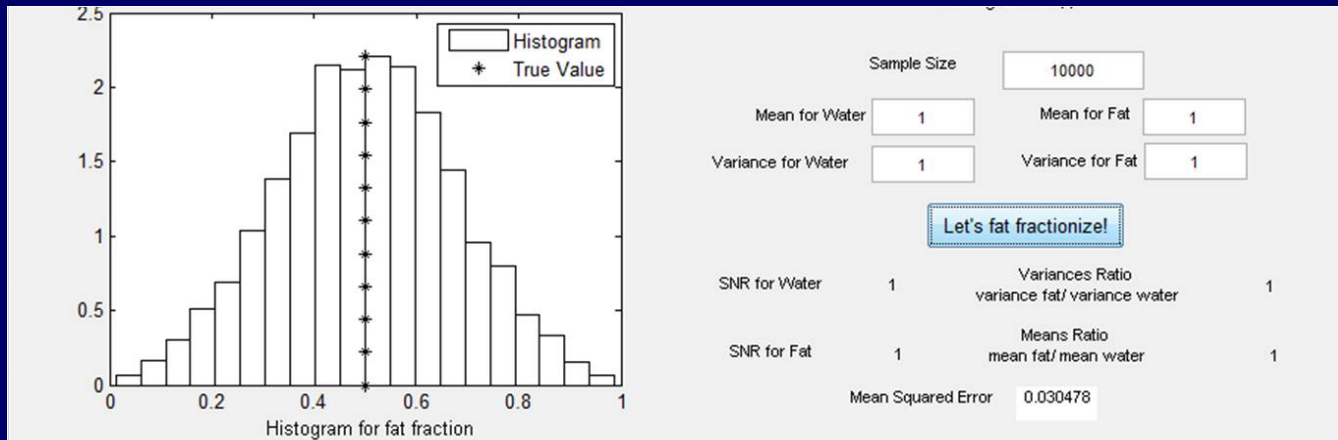
$$\frac{|F|}{|W| + |F|}$$

Theoretical Result

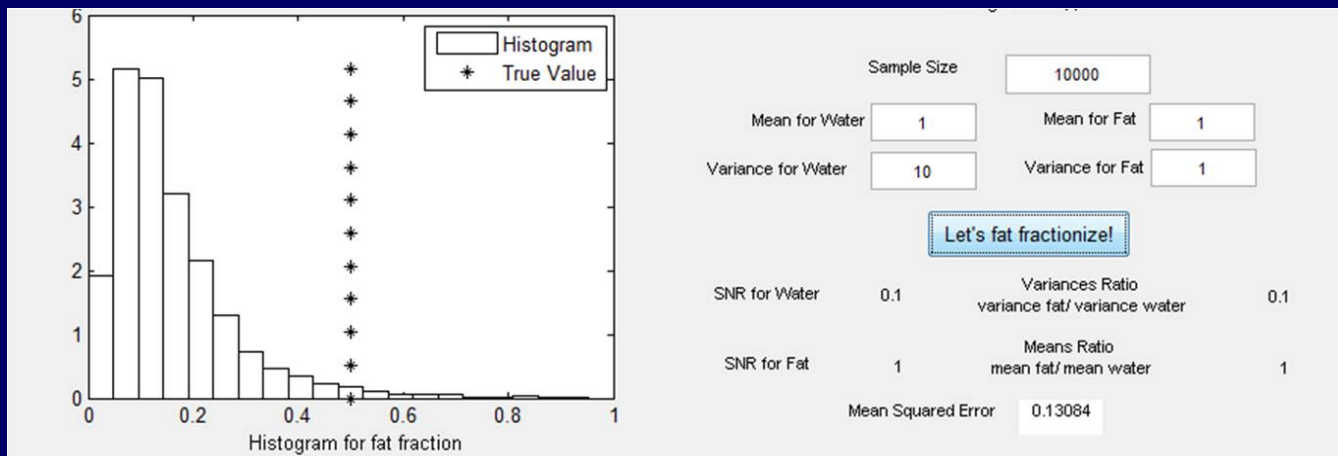


The probability density derived for the fat-fraction under the normal assumption matched simulation results:
The Huang-Park Distribution!

Simulation Result



Accurate Estimation



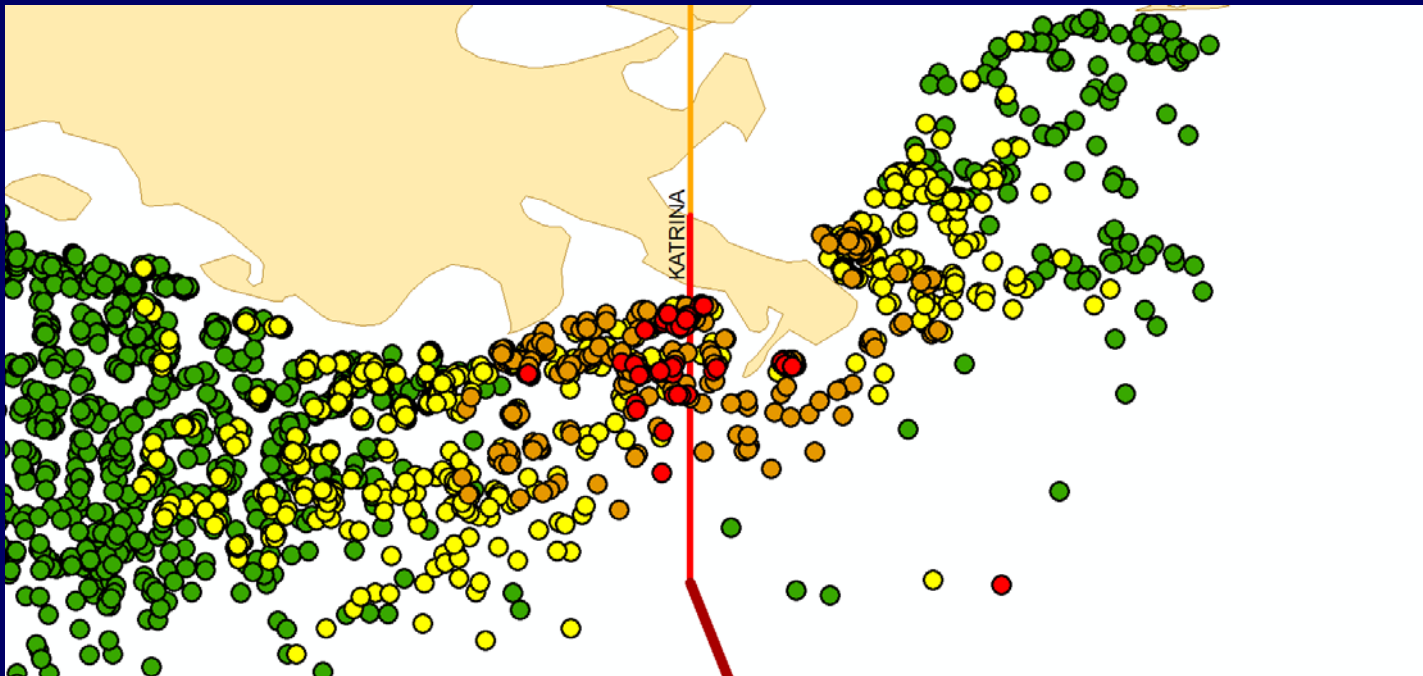
Inaccurate Estimation

Looking Back...

- Imaging data comes from a physical and biological process which we need to model. This is the “forward problem”.
- To create the images we see, we need to invert the process which created the image. This is the “inverse problem”.
- Mathematics, statistics and the sciences are naturally coupled in medical imaging.

Medicine and Hurricanes

Determining whether a patient has cancer from data is similar to deciding whether an oil platform will be destroyed by a hurricane (Applied Math Project with Earth Science Associates in 2015)



Acknowledgements and Support

Acknowledgements:

Norbert Pelc (at Stanford University)

Jongduk Baek (at Yonsei University)

Scott Reeder and Venkata Chebrolu (at UW Madison)

Jean Brittain and Huanzhou Yu (at GE)

John Grace and Scott Morris (at Earth Science Associates)

Financial Support:

CSUF, NSM, NIH, GE, CURM, LSAMP

Thank you... any questions?



The Usual Suspects...