

Lecture 7 – Image Reconstruction (图像重建)

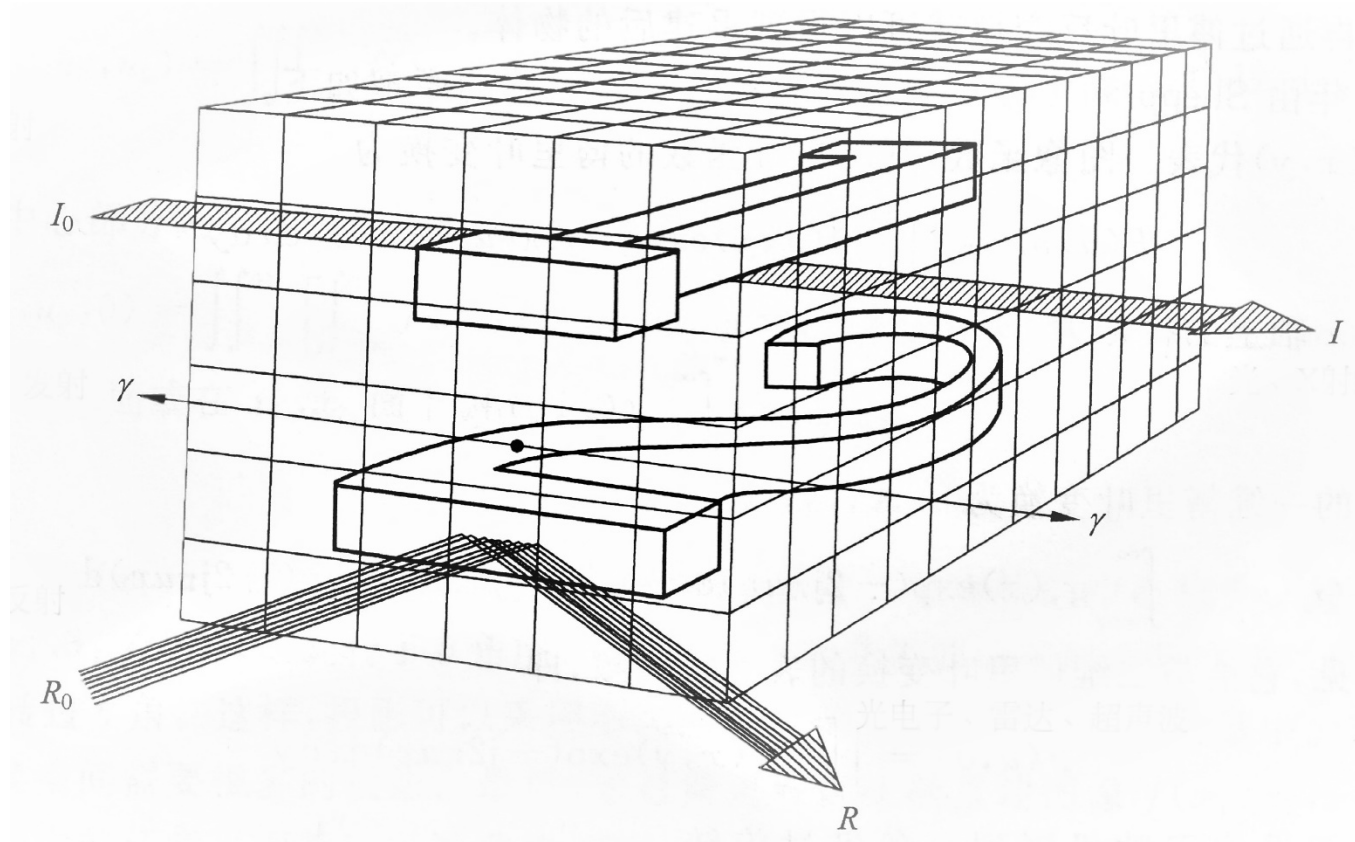
This lecture will cover:

- Reconstruction modalities (重建模式)
- Reconstruction from projection (投影重建算法)
 - Computed Tomography (计算机断层成像)
 - Radon transform (雷登变换)
 - The Fourier-Slice Theorem (傅里叶切片定理)
 - Parallel-Beam Filtered Backprojections (平行射线束滤波反投影)
 - Fan-Beam Filtered Backprojections (扇形射线束滤波反投影)
- Reflection imaging
 - Time of flight
 - Born Approximation and Inverse theory (玻恩近似与反演理论)

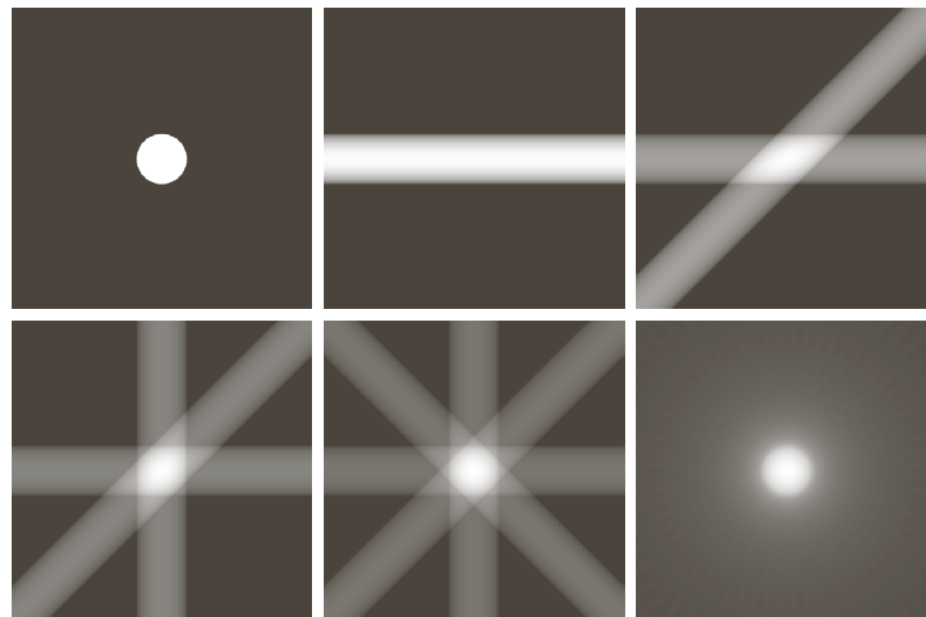
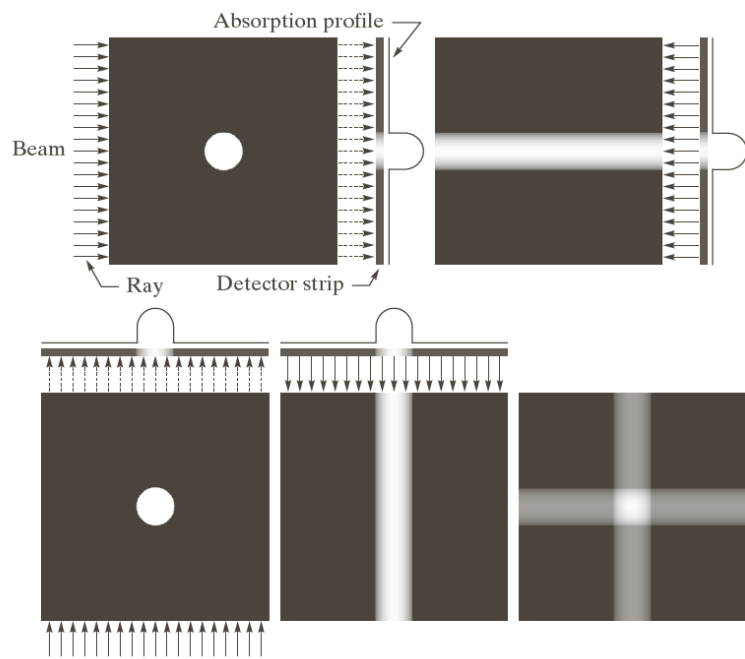


Reconstruction Modalities

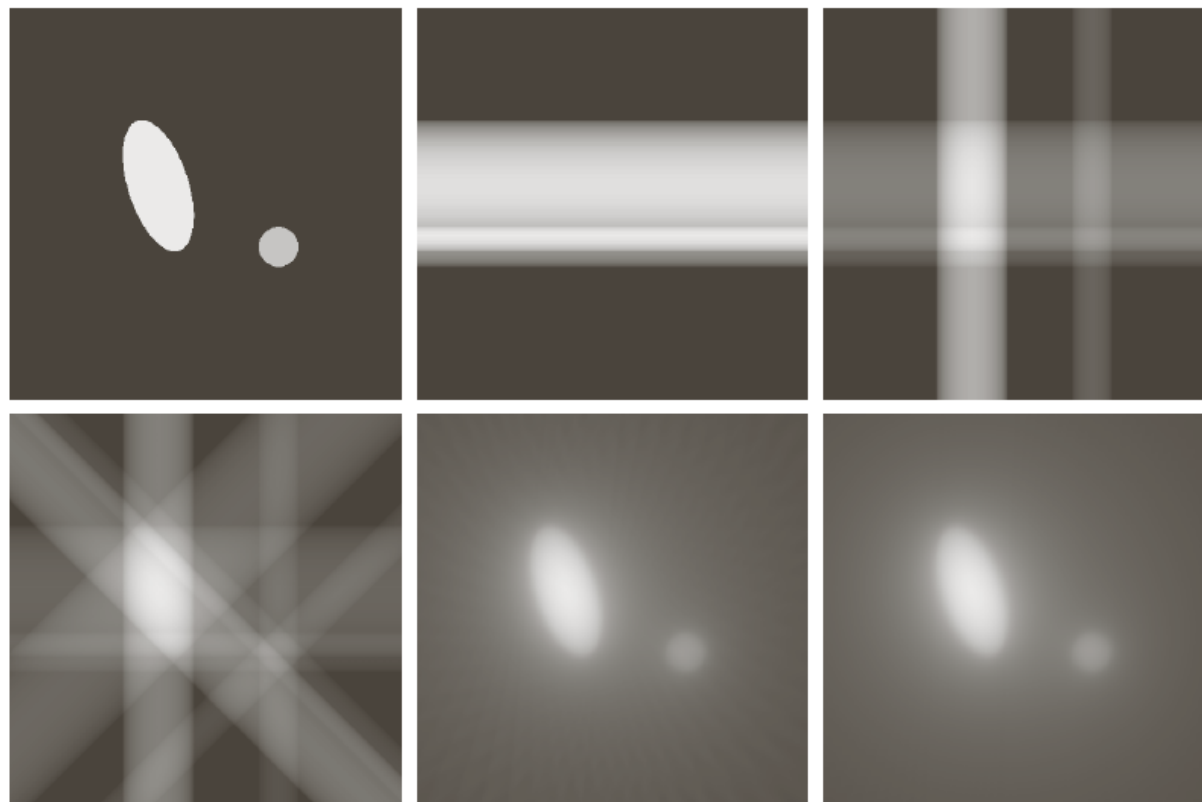
- Transmission
- Emission
- Reflection



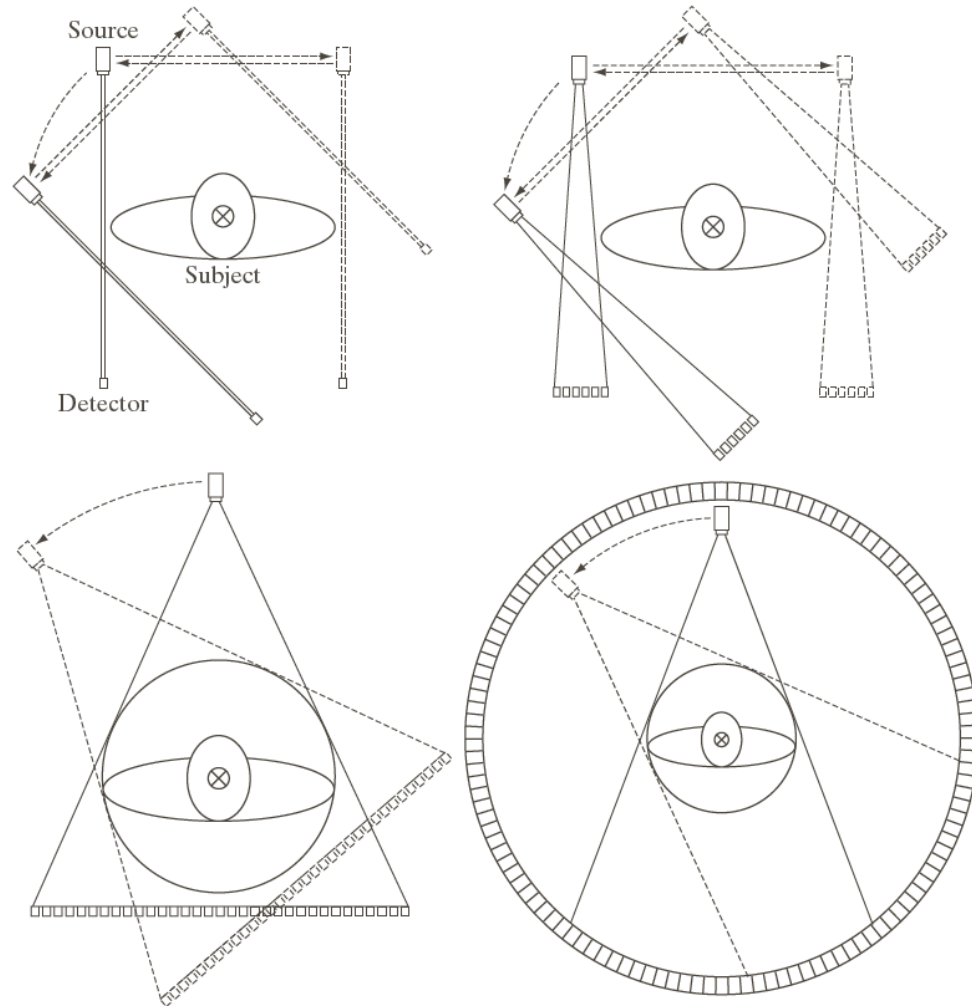
Back Projection



Back Projection



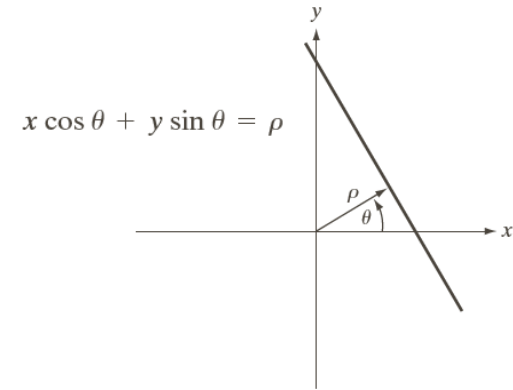
Computed Tomography



Radon Transform

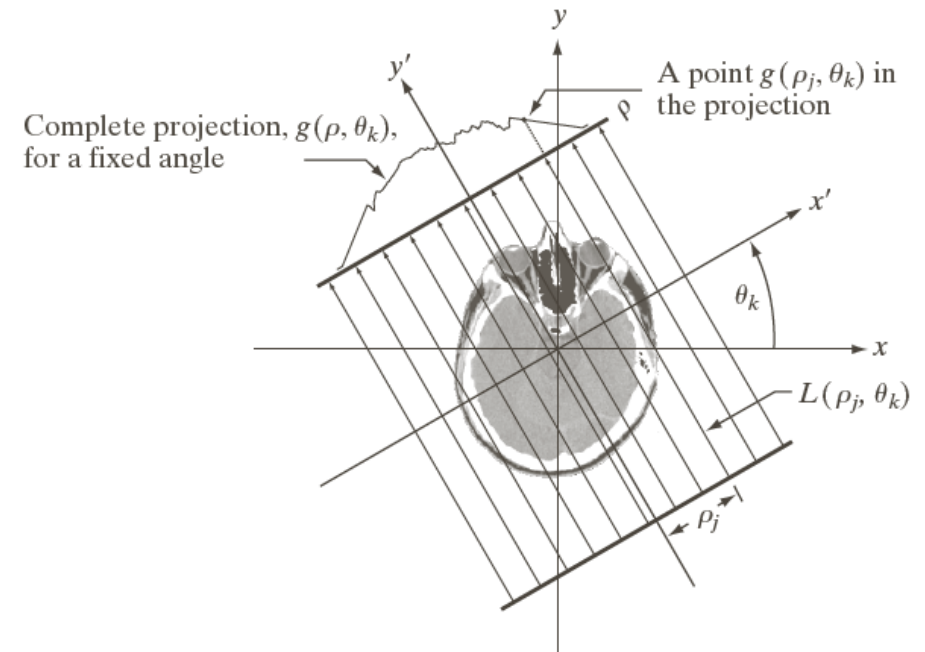
Normal representation for a line:

$$x \cos \theta + y \sin \theta = \rho$$

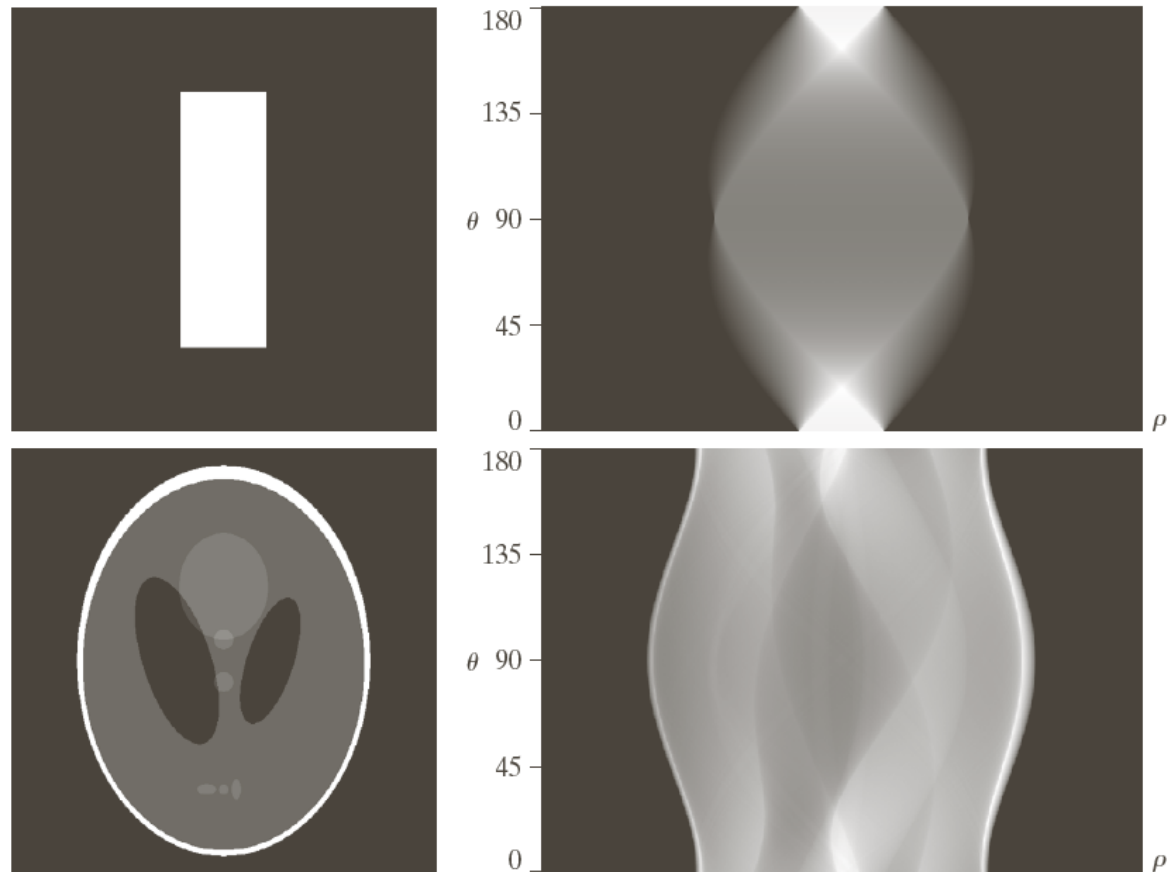


The projection of $f(x, y)$ along an arbitrary line in the xy -plane:

$$g(\rho, \theta) = \sum_{x=0}^{M-1} \sum_{y=0}^{N-1} f(x, y) \delta(x \cos \theta + y \sin \theta - \rho)$$



Sinogram (正弦图)



Back Projection from Radon Transform

For a fixed value of rotation θ_k :

$$f_{\theta_k}(x, y) = g(\rho, \theta_k) = g(x \cos \theta_k + y \sin \theta_k, \theta_k)$$

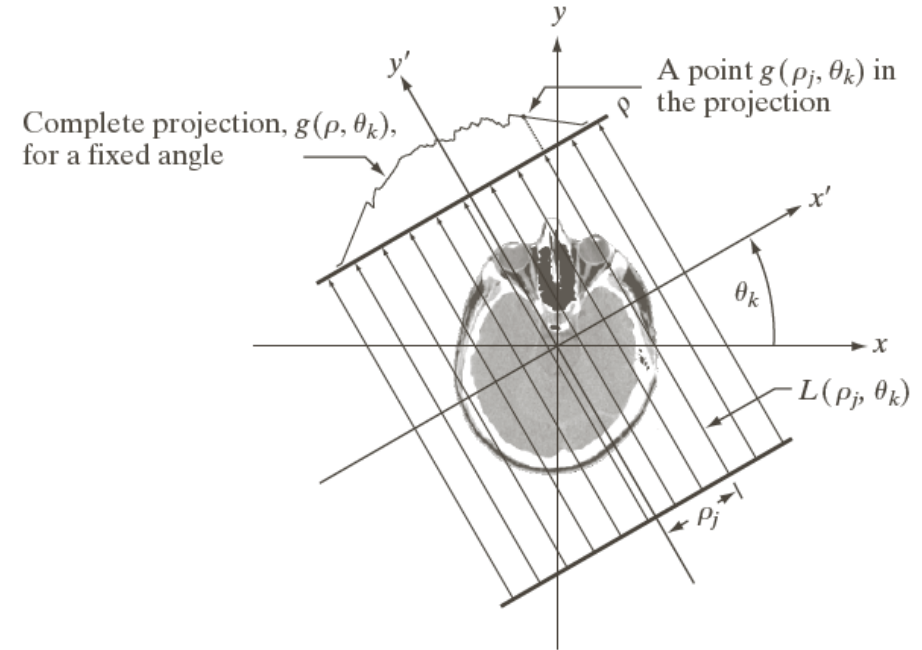
Then a single backprojection obtained at an angle θ :

$$f_{\theta}(x, y) = g(x \cos \theta + y \sin \theta, \theta)$$

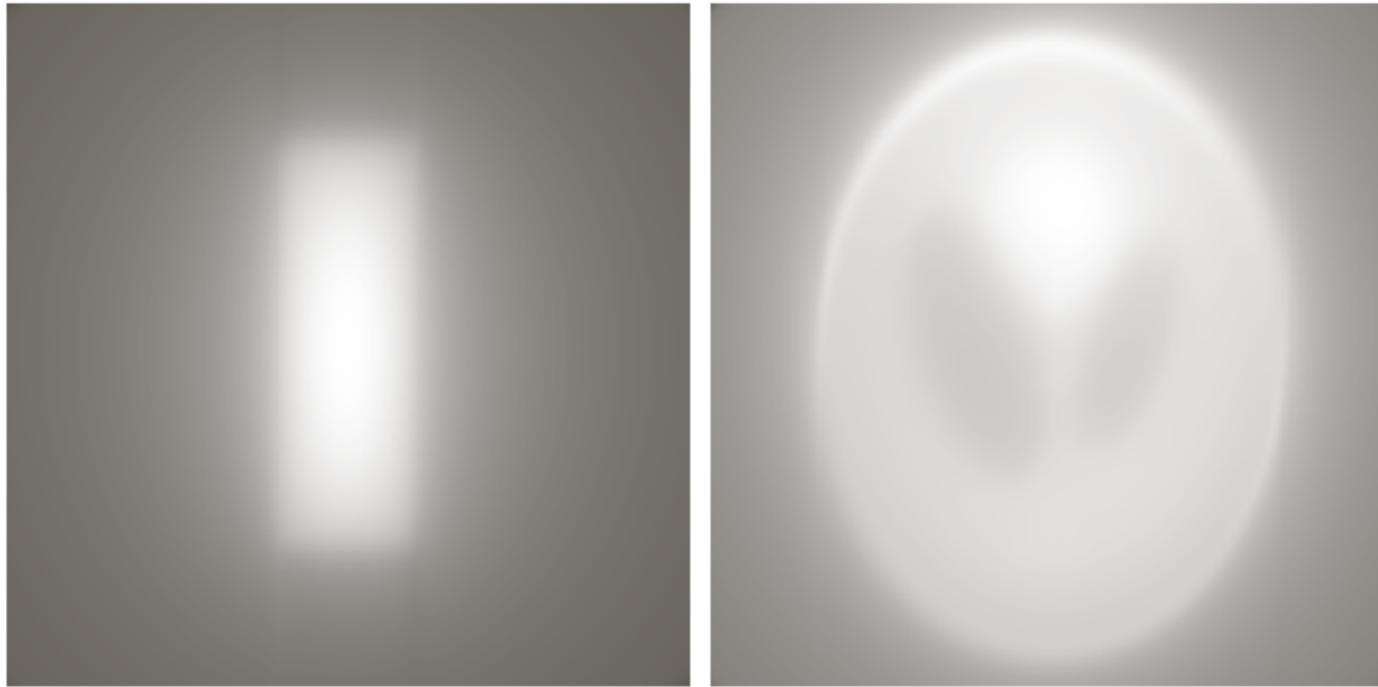
Where $g(\rho, \theta)$ is the projection value.

The final image by summing over all the back-projected images

$$f(x, y) = \sum_{\theta=0}^{\pi} f_{\theta}(x, y)$$



Back Projection from Radon Transform



The Fourier-Slice Theorem

The 1D FT of a projection with respect of ρ :

$$G(\omega, \theta) = \int_{-\infty}^{\infty} g(\rho, \theta) e^{-j2\pi\omega\rho} d\rho$$

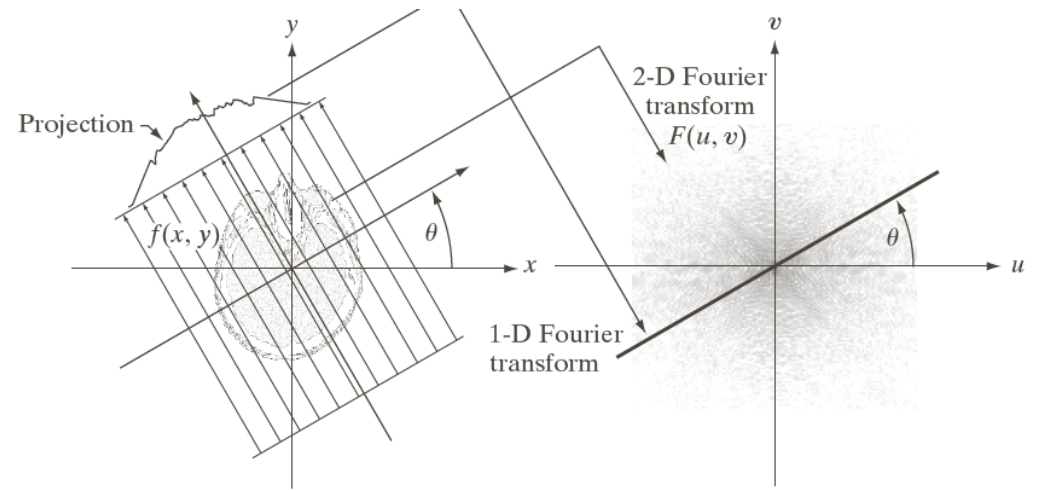
where projection $g(\rho, \theta)$ is

$$g(\rho, \theta) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} f(x, y) \delta(x \cos \theta + y \sin \theta - \rho) dx dy$$

then

$$\begin{aligned} G(\omega, \theta) &= \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} f(x, y) e^{-j2\pi\omega(x \cos \theta + y \sin \theta)} dx dy \\ &= \left[\int_{-\infty}^{\infty} \int_{-\infty}^{\infty} f(x, y) e^{-j2\pi(ux + vy)} dx dy \right]_{u=\omega \cos \theta; v=\omega \sin \theta} \end{aligned}$$

Therefore $G(\omega, \theta) = F(\omega \cos \theta, \omega \sin \theta)$



Parallel-Beam Filtered Backprojections

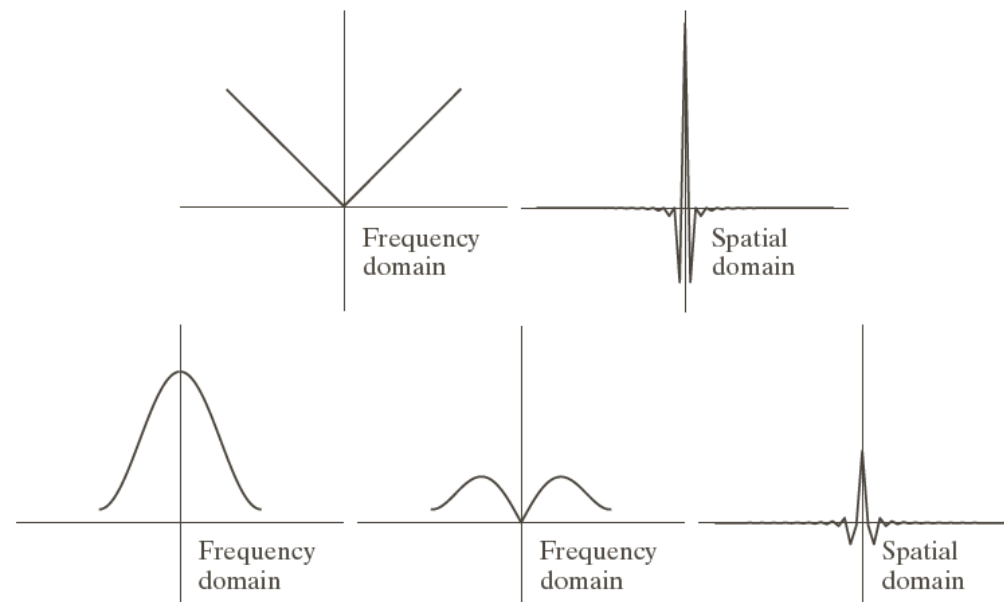
The 2D IFT of $F(u, v)$ with Fourier-slice theorem:

$$\begin{aligned}
 f(x, y) &= \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} F(u, v) e^{j2\pi(ux+vy)} du dv \\
 &= \int_0^{2\pi} \int_0^{\infty} G(\omega, \theta) e^{j2\pi\omega(x \cos \theta + y \sin \theta)} \omega d\omega d\theta \\
 &= \int_0^{\pi} \left[\int_{-\infty}^{\infty} |\omega| G(\omega, \theta) e^{j2\pi\omega\rho} d\omega \right]_{\rho=x \cos \theta + y \sin \theta} d\theta
 \end{aligned}$$

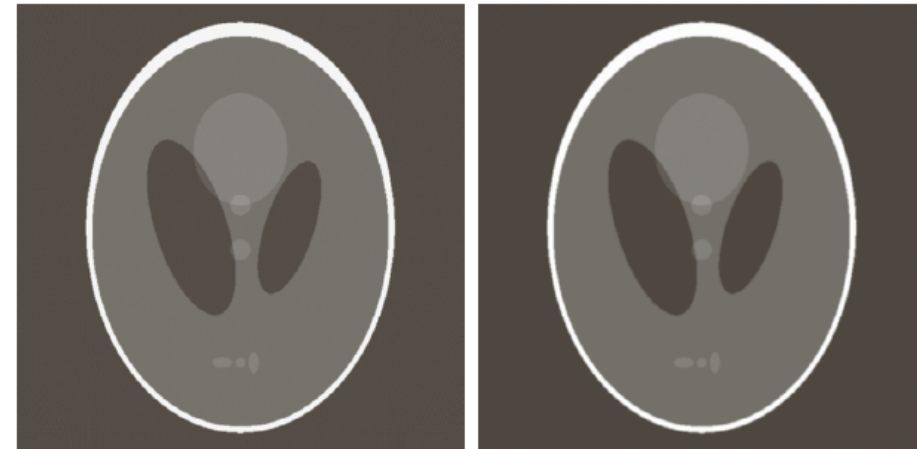
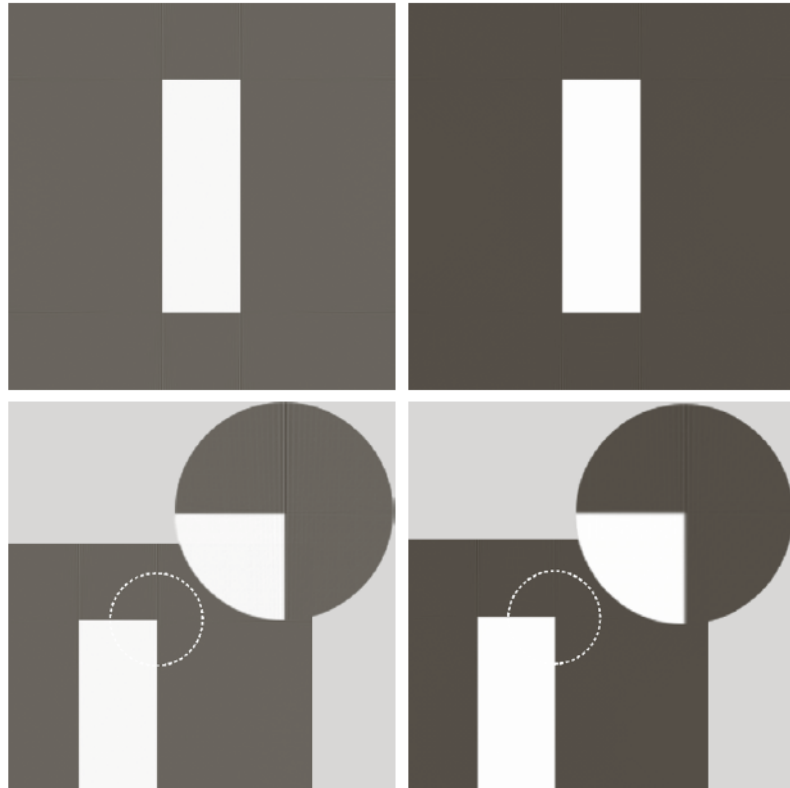
Convolution backprojection

$$f(x, y) = \int_0^{\pi} [s(\rho) \star g(\rho, \theta)]_{\rho=x \cos \theta + y \sin \theta} d\theta$$

Where $s(\rho) = \text{IFT}(|\omega|)$, $g(\rho, \theta) = \text{IFT}[G(\omega, \theta)]$



Parallel-Beam Filtered Backprojections

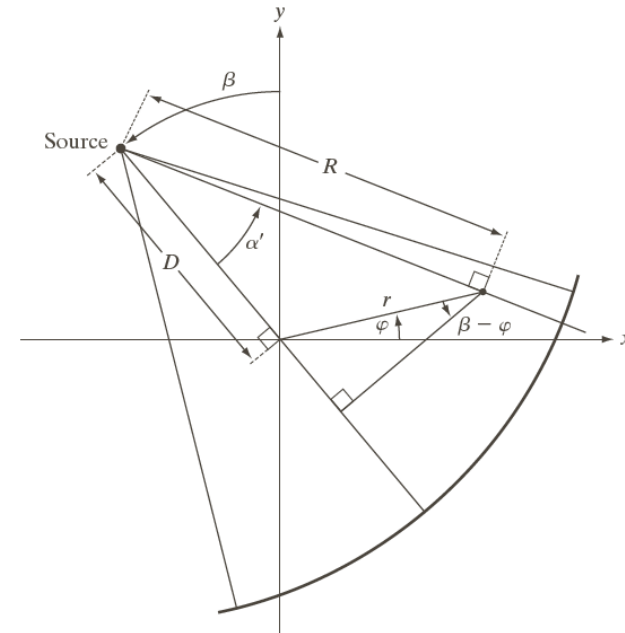
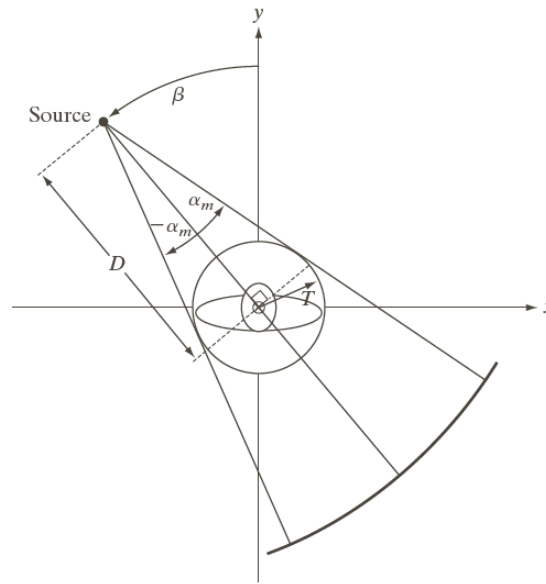
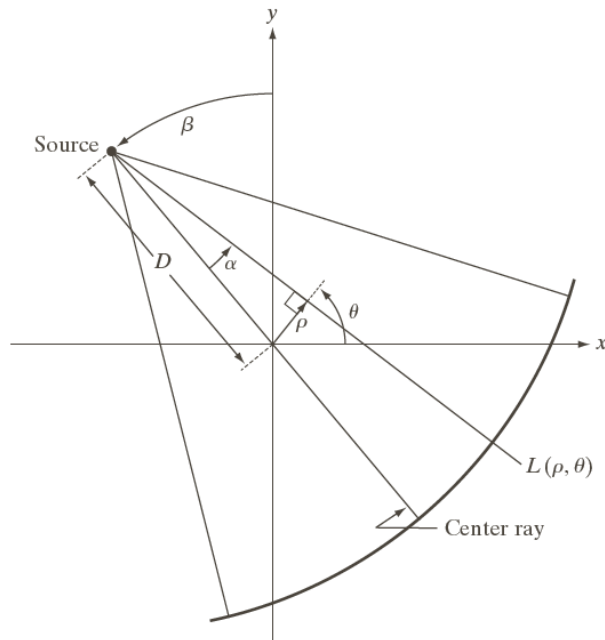


Fan-Beam Filtered Backprojections

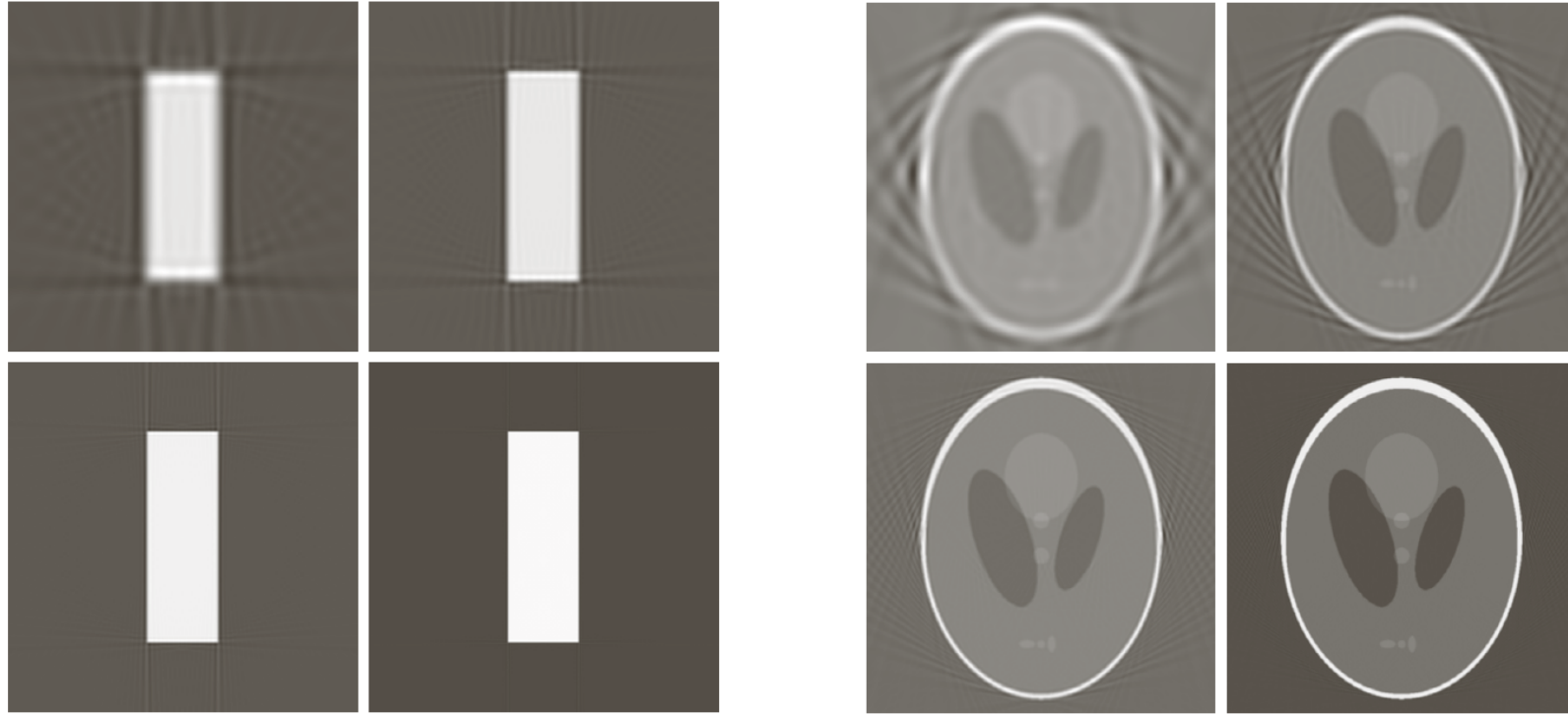
Fundamental fan-beam reconstruction based on filtered backprojection:

$$f(r, \varphi) = \int_0^{2\pi} \frac{1}{R^2} \left[\int_{-\alpha_m}^{\alpha_m} q(\alpha, \beta) h(\alpha' - \alpha) d\alpha \right] d\beta$$

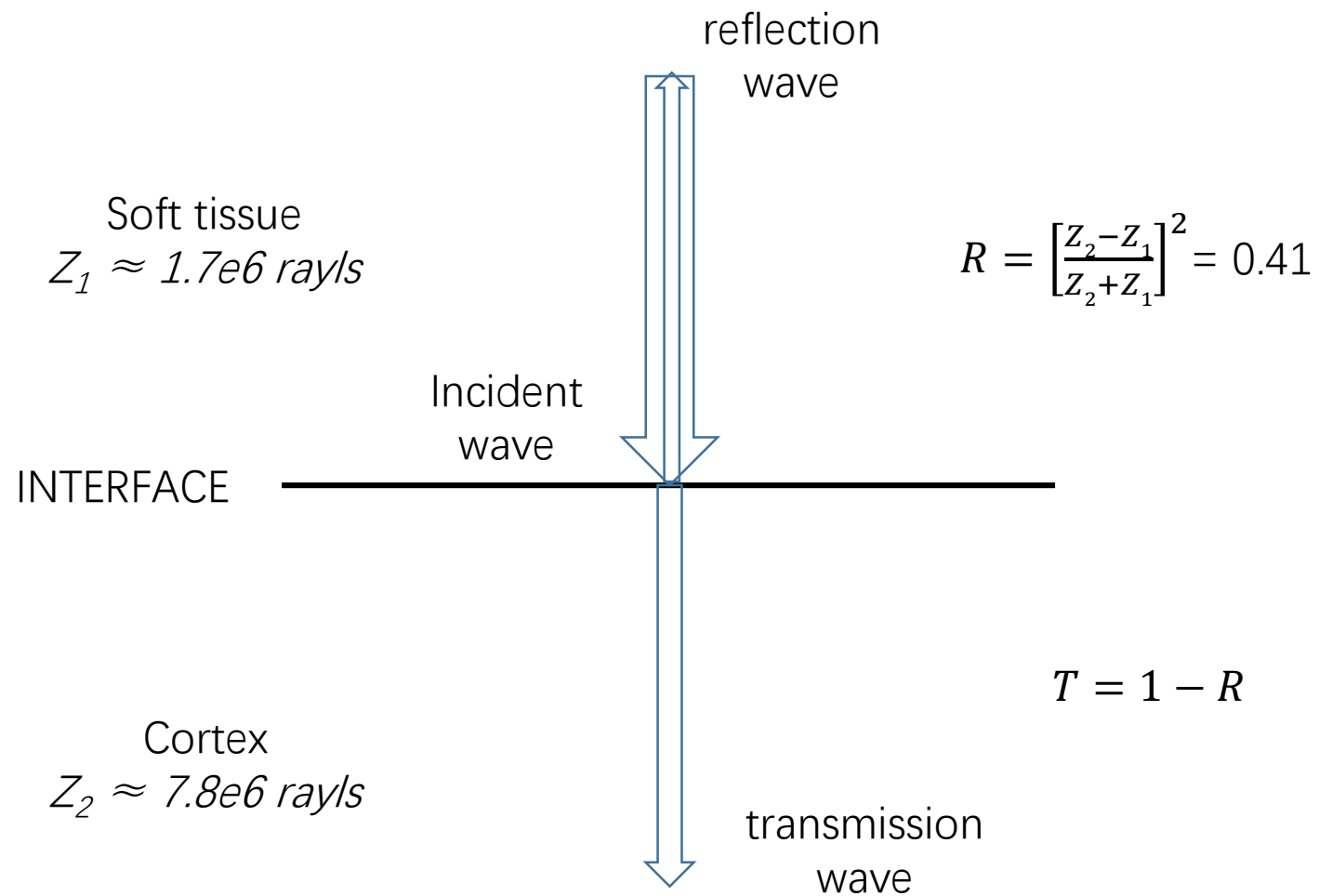
Where $h(\alpha) = \frac{1}{2} \left(\frac{\alpha}{\sin \alpha} \right)^2 s(\alpha)$, $q(\alpha, \beta) = p(\alpha, \beta) D \cos \alpha$, $p(\alpha, \beta) = g(\rho, \theta) = g(D \sin \alpha, \alpha + \beta)$



Fan-Beam Filtered Backprojections



Ultrasound wave reflection

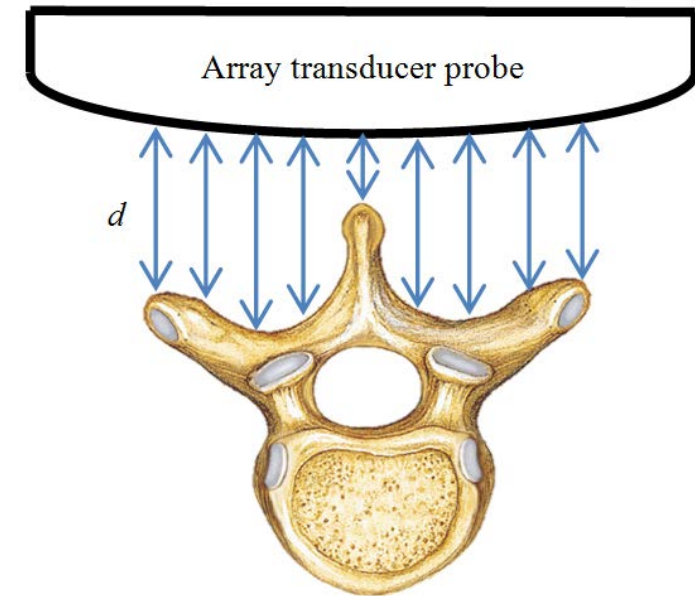


Ultrasound imaging

- Reflection from the interface between different tissues
- Using time of flight (t) to determine the distance (d) and locate the structures

$$t = \frac{2 * d}{V}$$

- Use gray level to indicate the amplitude (B mode)

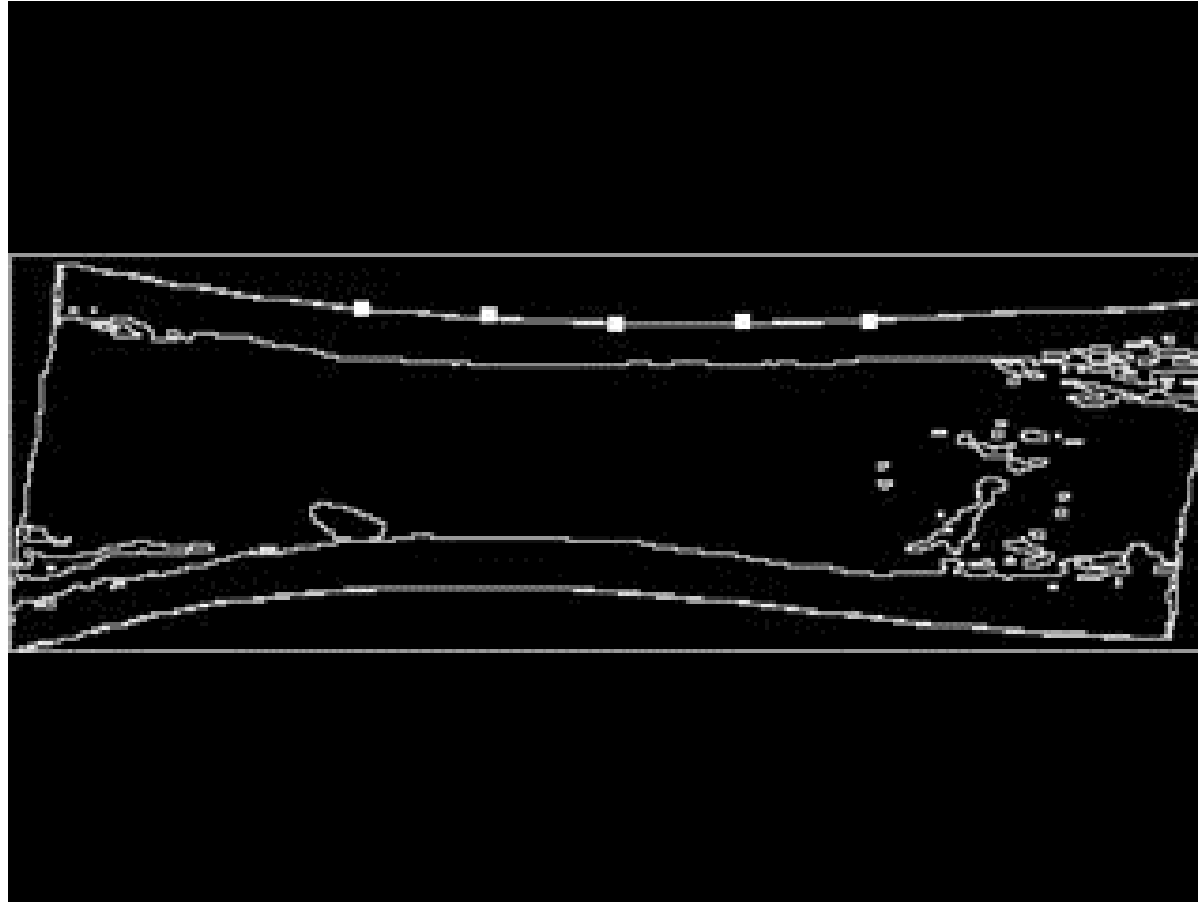


The schematic of ultrasound reflection waves from the vertebra cortex / soft tissue interface.

Ultrasound image



Wave Propagation



Born Approximation

Based on the perturbation velocity profile assumption:

$$\frac{1}{c^2(\vec{x})} = \frac{1}{c_0^2(\vec{x})} + f(\vec{x})$$

An approximate solution for acoustic wave equation (Born Approximation) is

$$d(\vec{s}, \vec{r}, \omega) = \omega^2 \int d^3x G_0(\vec{x}, \vec{r}, \omega) f(\vec{x}) G_0(\vec{s}, \vec{x}, \omega)$$

$G_0(\vec{x}, \vec{y}, \omega)$: Green function

$$G_0(\vec{x}, \vec{y}, \omega) = A(\vec{x}, \vec{y}) e^{-j\omega\tau(\vec{x}, \vec{y})}$$

Operator & cost function

Rewrite in operator form: $D(\vec{s}, \vec{r}) = L(\vec{s}, \vec{r}, \vec{x}, \omega_i) * F(\vec{x})$

Where, the cost function J $J = \left\| D - D^{obs} \right\|_2^2$

Where

D : the theoretical data D^{obs} : the observed data

Inversion is to minimize J to find the best solution of $F(\vec{x})$

Operator & cost function

- Adjoint operator: $F(\vec{x}) = L^*(\vec{s}, \vec{r}, \vec{x}, \omega) * D(\vec{s}, \vec{r})$
- Minimum norm solution (LS): $J = \|LF - D\|_2^2$
- Damped minimum norm solution (DLS): $J = \|LF - D\|_2^2 + \mu \|F\|_2^2$
- Weighted minimum norm solution (WLS): $J = \|LF - D\|_2^2 + \mu \|WF\|_2^2$



Conjugate Gradient Method

Consider a system of linear equations: $\mathbf{Lx}=\mathbf{y}$

Let $\mathbf{x}=\mathbf{x}_0$, $\mathbf{p}_0=\mathbf{r}_0=\mathbf{y}-\mathbf{Lx}_0$, and $k=0$. The following steps will be repeated until number of iterations or the tolerance limit for convergence is reached.

$$(a) \quad \alpha_k = \frac{\mathbf{r}_k^T \mathbf{r}_k}{\mathbf{p}_k^T \mathbf{Lp}_k} .$$

$$(b) \quad \mathbf{x}_{k+1} = \mathbf{x}_k + \alpha_k \mathbf{p}_k .$$

$$(c) \quad \mathbf{r}_{k+1} = \mathbf{y} - \mathbf{Lx}_{k+1} .$$

$$(d) \quad \beta_k = \frac{\mathbf{r}_{k+1}^T \mathbf{r}_{k+1}}{\mathbf{r}_k^T \mathbf{r}_k} .$$

$$(e) \quad \mathbf{p}_{k+1} = \mathbf{r}_{k+1} + \beta_k \mathbf{p}_k .$$

$$(f) \quad k = k + 1 .$$

