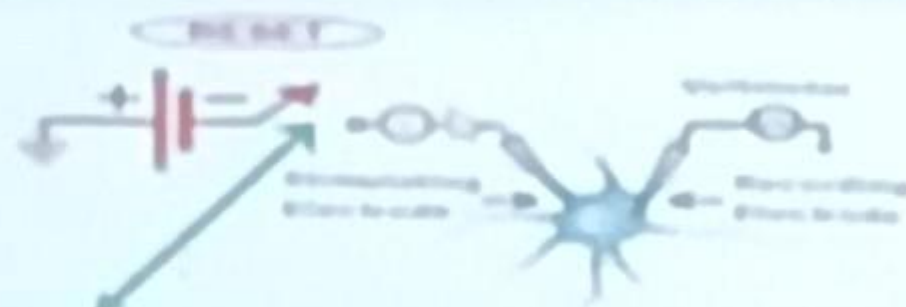


Action Potential (Electrical Viewpoint)

A. Hyperpolarizations



ELECTRONIC SWITCH

Depolarization/Hyperpolarization in the previous slides achieved using a battery

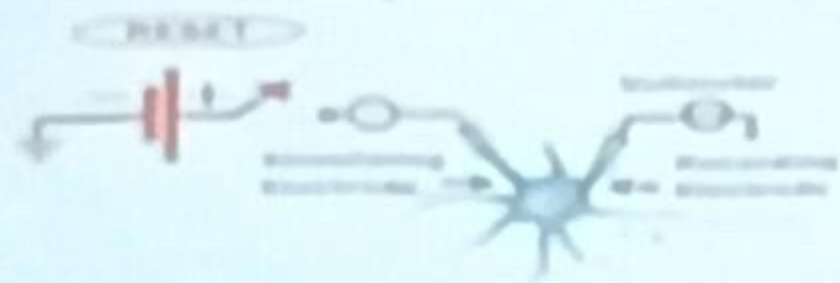
Degree of change of hyperpolarization is proportional to MAGNITUDE or AMPLITUDE of stimulus current (I)



Stimulus Current (I)

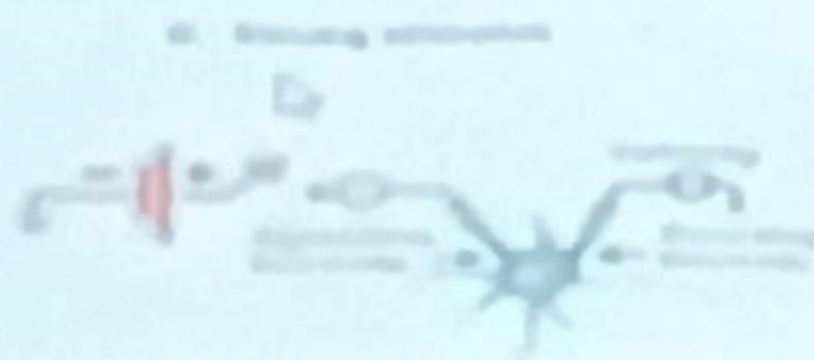
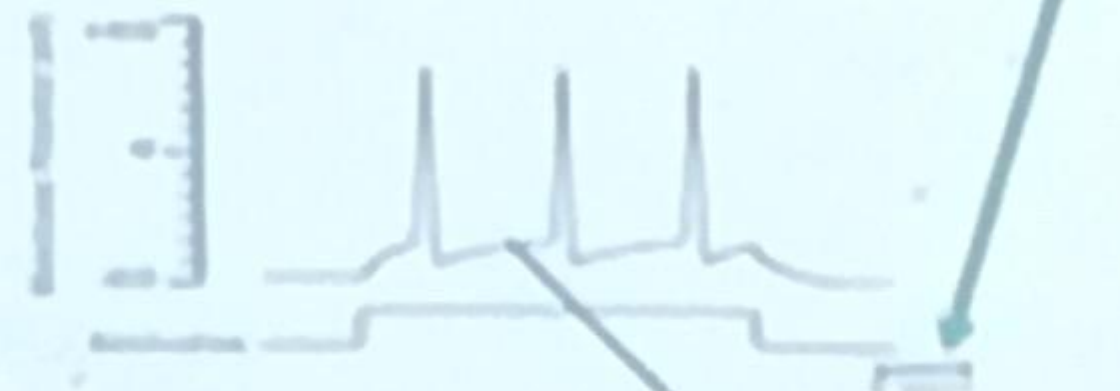
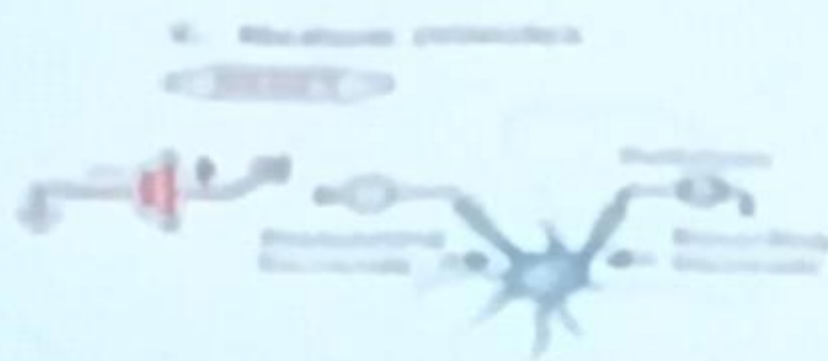
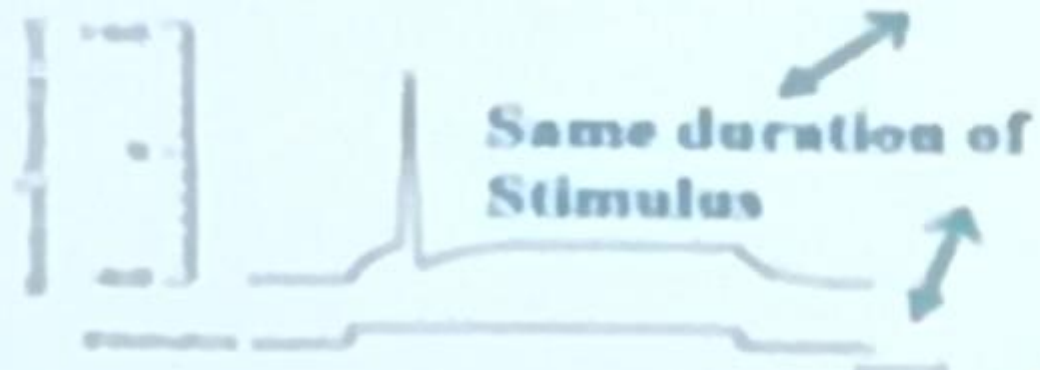
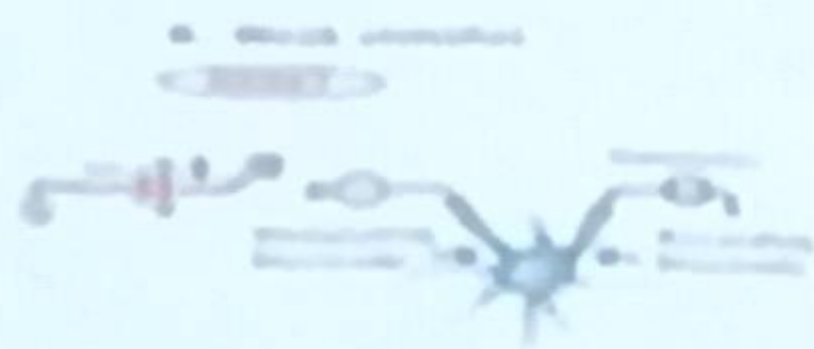
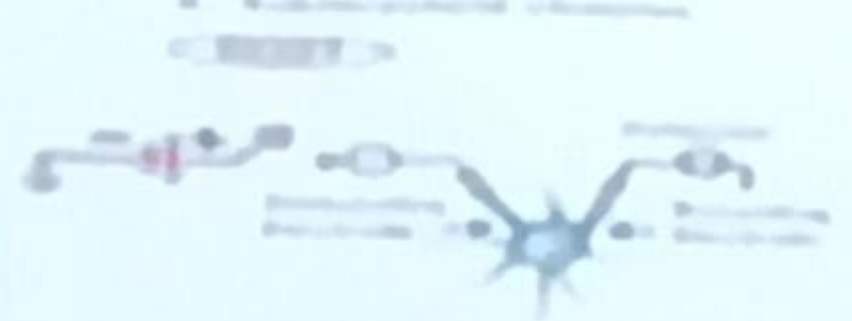
Duration of Stimulus

B. Depolarizations and the Action Potential



Stimulus Current (I)

Depolarizing current is responsible for action potential evoking.

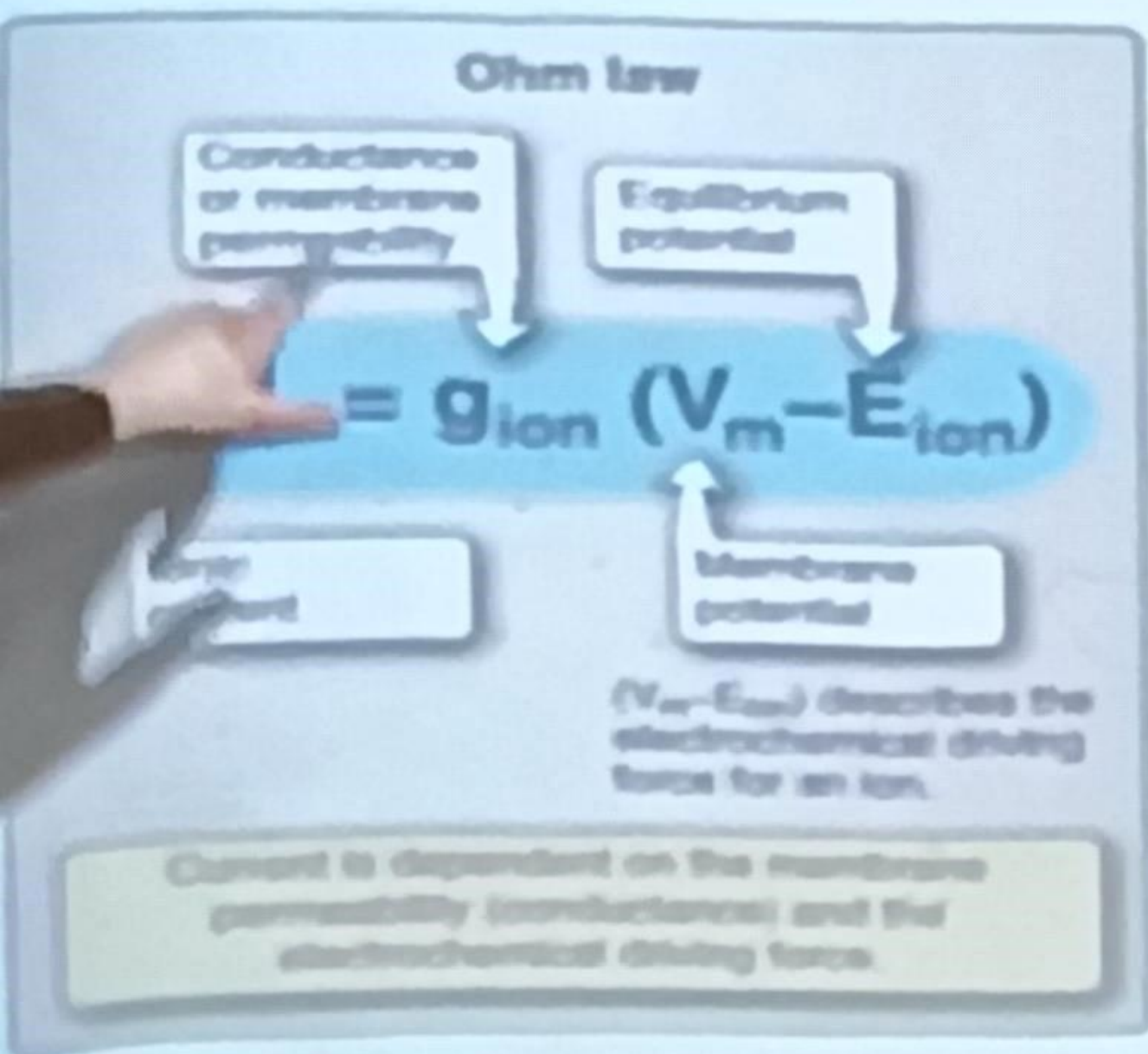


Tutorial-2 (Tomorrow)- PLEASE BRING LAPTOPS

ANY CONCERNS, EMAIL TA and ME

Ohms Law

**Current Flow (Action Potential) in Axon
Depends on ?**



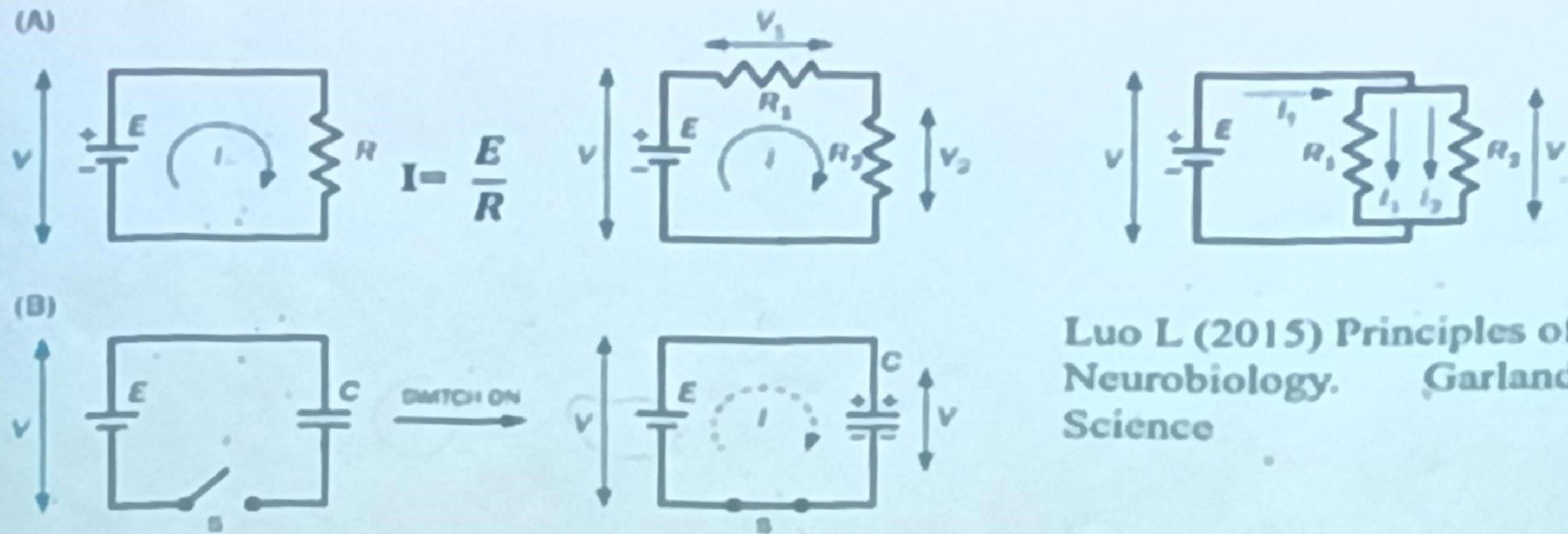
Ohms Law

Content from book: Neuroscience by Claudia Krebs

Introduction to Hodgkin Huxley Model

**Using Ohms law/Electrical Circuit Theory
(R,C and RC)**

Neuronal Plasma membrane or Biological membrane as Electrical circuits



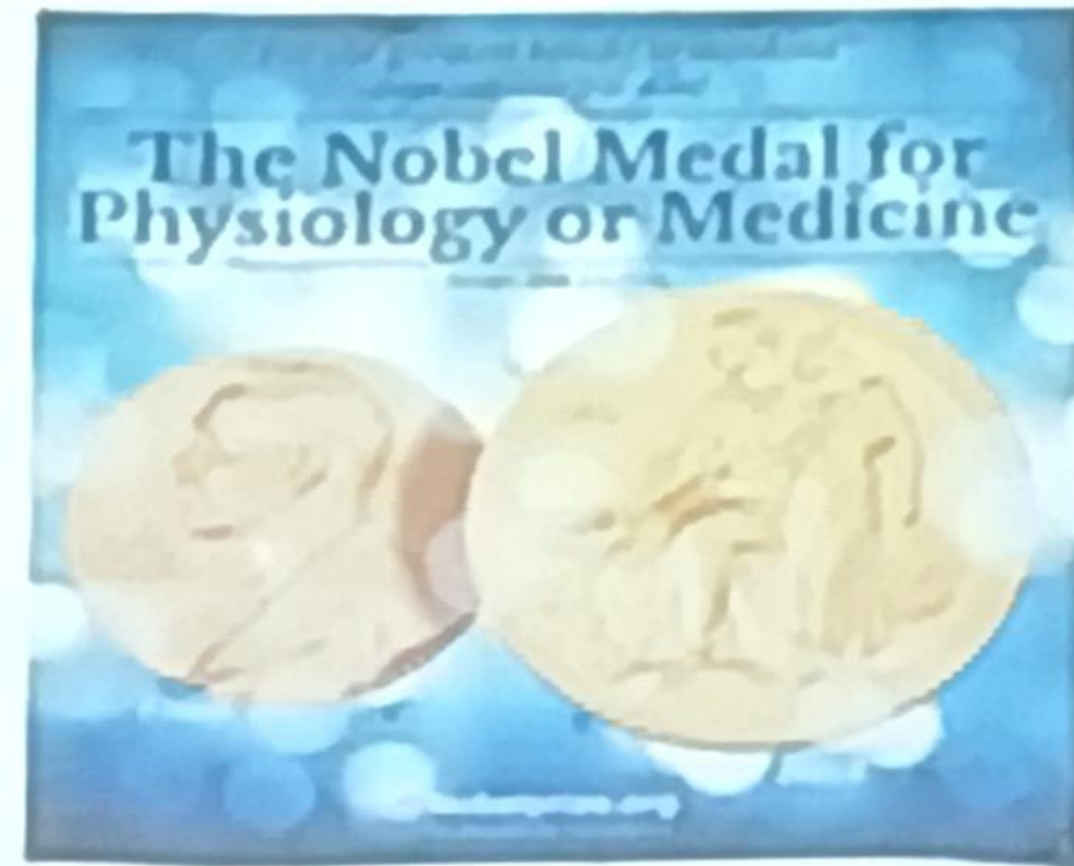
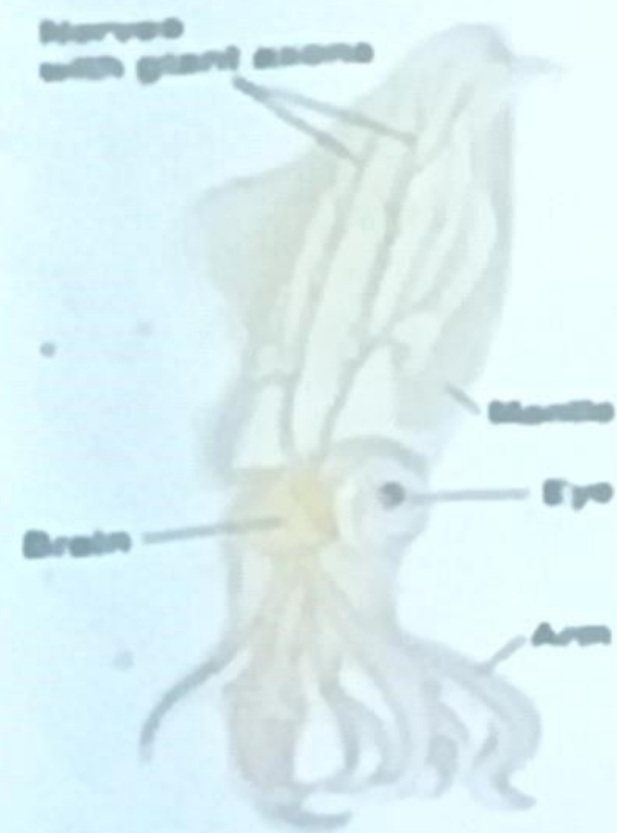
Luo L (2015) Principles of Neurobiology. Garland Science

Initially there is no charge across the Capacitor and it needs time (Current is biggest)

Over time capacitor gets charged and creates voltage same as battery E and current is zero

Neuron and Capacitor Link

Hodgkin Huxley (HH) Model



Developed in 1952 using the squid axon, which is quite large

Model was developed, tested and refined before the use of computers (1)

Awarded the 1963 Nobel Prize In Physiology/Medicine

Remains the most widely used model for the action potential

Breakthrough of HH Model

- The breakthrough of Hodgkin and Huxley was that they succeeded to measure how the cell membrane voltage or current can be modeled and represented as electrical circuits

Applications of Hodgkin Huxley Model

- **Mathematical modeling can reveal mechanisms long before they can be observed directly.**
- **Framework for studying and analyzing ion channel kinetics.**

Hodgkin and Huxley, Journal of Physiology, 1952

Why Study HH model, Applications

J. Physiol. (1952) 117, 500-544

**A QUANTITATIVE DESCRIPTION OF MEMBRANE
CURRENT AND ITS APPLICATION TO CONDUCTION
AND EXCITATION IN NERVE**

By A. L. HODGKIN AND A. F. HUXLEY

From the Physiological Laboratory, University of Cambridge

What is Hodgkin Huxley Model?

(23426 citations on Google scholar)

Nobel Prize in Physiology or Medicine, 1963

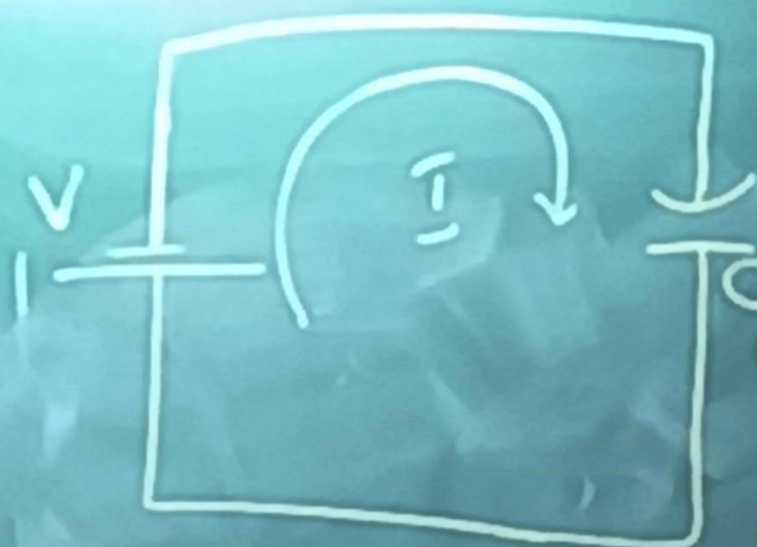
Lets Derive the HH Model

$$P_L = \frac{1}{2}$$

V_L

$$P_{NL} = \frac{1}{9}$$

V_{NL}

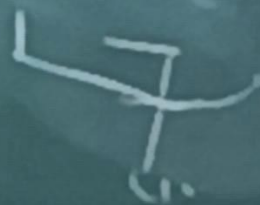


$$C = \frac{q}{V} = \frac{\text{charge}}{\text{voltage}}$$

Capacitors
(C) $q = CV$

$$\frac{dq}{dt} = C \frac{dv}{dt}$$

$$I_c = C \frac{dv}{dt}$$



t_m

membranes proteins



neuron cell which is membrane a bilayer

V_L = Voltage across leakage channel

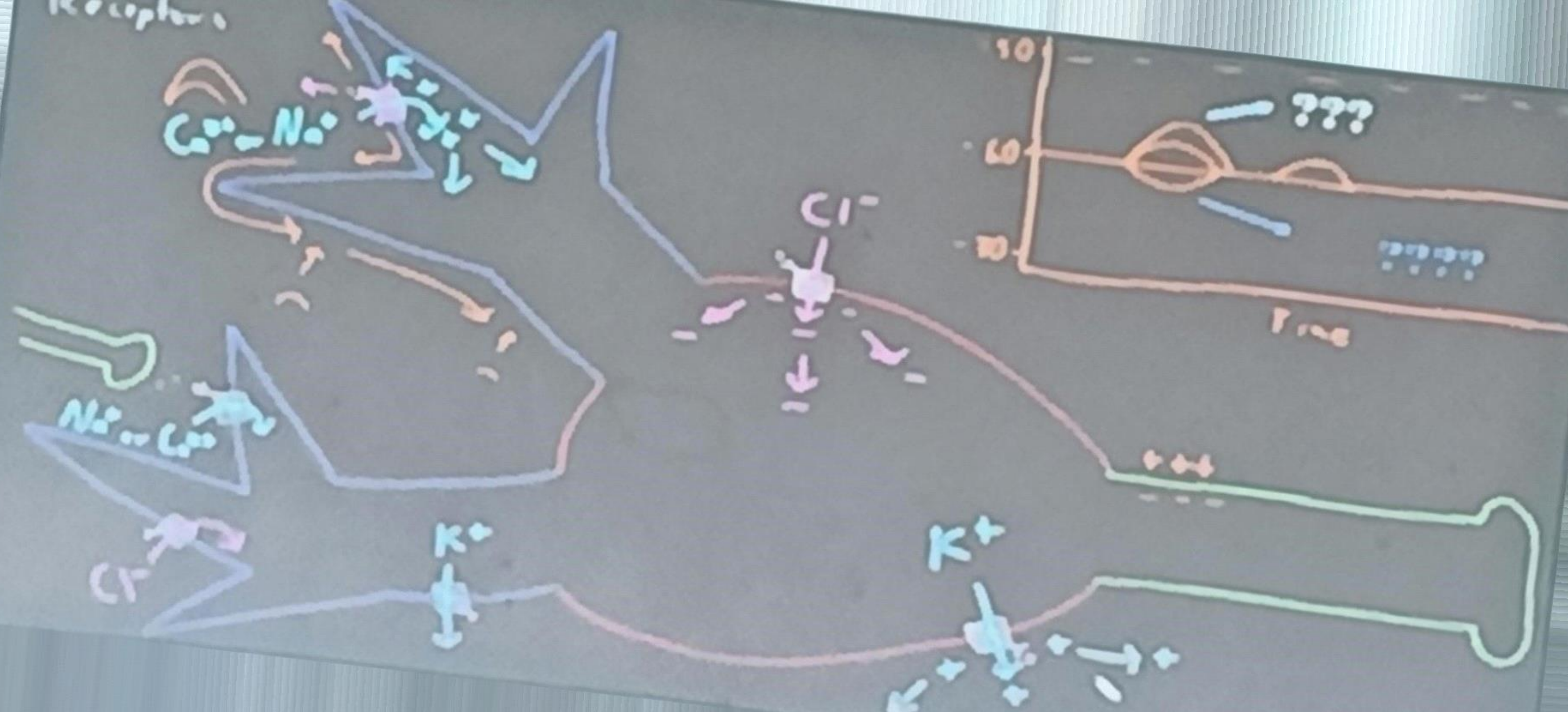
$g = \frac{1}{R}$ = conductance

All other ions contribute to leakage

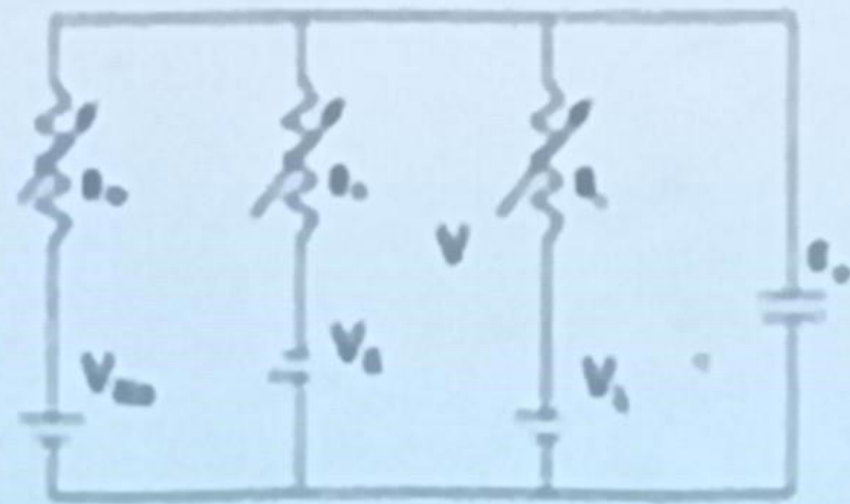
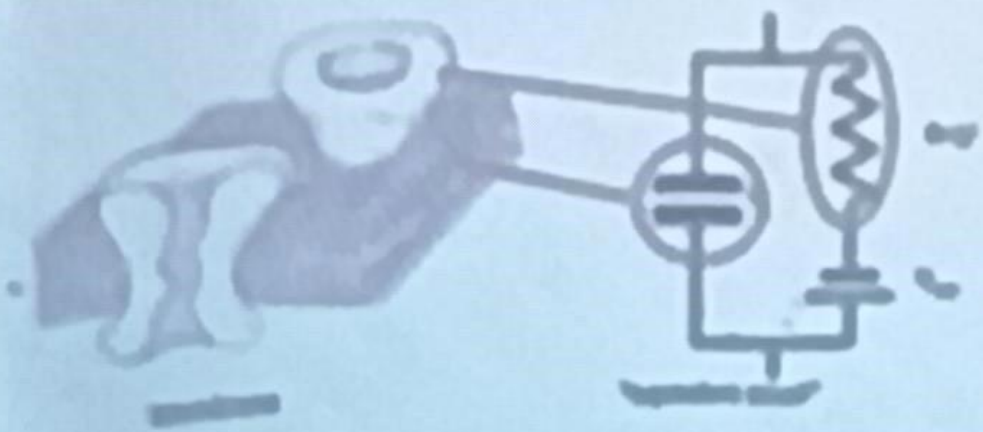


I

Receptor:



Full equations for electric circuit model



Hodgkin Huxley (HH) Model

$$I_{\text{TOT}} = I_K + I_{\text{Na}} + I_L$$

$$I_{\text{TOT}} = \frac{dQ}{dt} = C \frac{dV}{dt}$$

$$I_{\text{Na}}(V, t) = (V_{\text{Na}} - V)g_{\text{Na}}(V, t)$$

$$I_K(V, t) = (V_K - V)g_K(V, t)$$

$$I_L(V, t) = (V_L - V)g_L$$

Basic form of conductances:

$$g = g_{\text{max}} \cdot f(V, t)$$

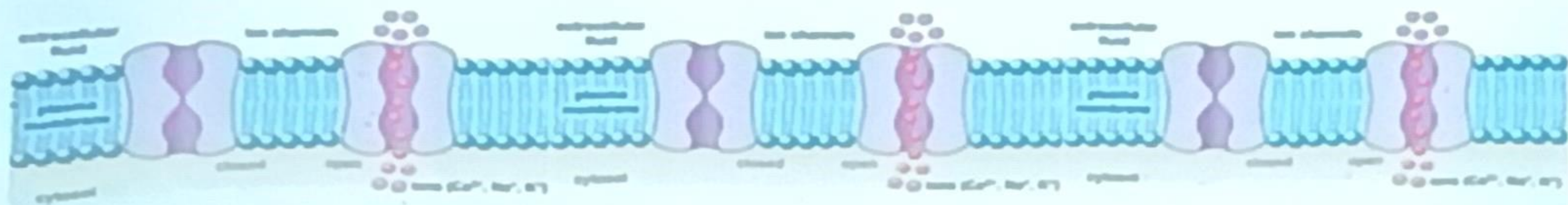
f is the fraction of channels open, which depends on V and t

$$I_{\text{TOT}} = C \frac{dV}{dt} = (V_K - V)g_K(V, t) + (V_{\text{Na}} - V)g_{\text{Na}}(V, t) + (V_L - V)g_L$$

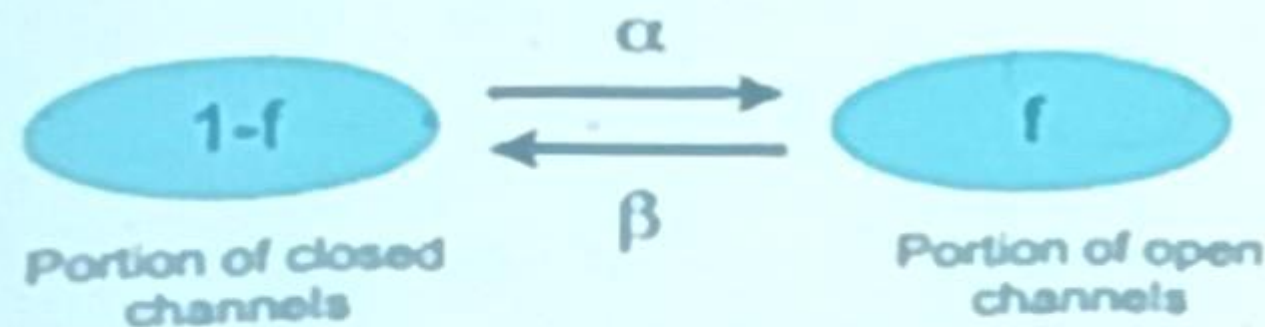
Hodgkin Huxley Model

- *Semi permeable membrane* acts as a capacitor
- Each channel type (Na^+ , K^+) is represented/characterized by a *resistor*.
- *Nernst potential* generated by differences in ion is represented by battery. E_L is leakage voltage for Cl^- and other ions
- Specific batteries since Nernst potential is different for each ion type.
- If input current $I(t)$ is injected into the neuron cell it charges the capacitor or leaks through the channels in cell membrane.

Key concept : gating variable Hodgkin Huxley (HH) Model



Rate coefficients



$$\frac{df}{dt} = \alpha_f(1 - f) - \beta_f f$$

f = Gating variable

f : fraction of open channels
a.k.a. the gating variable
(depends on V and t)

α : rate at which closed channels
open (depends on V)

β : rate at which open channels
close (depends on V)

Note: The f gating variable will be called n , m
and h for the three types of gating: K^+ activation,
 Na^+ activation, and Na^+ inactivation

Potassium current (activation)

Maximum conductivity
with all gates open
($n = 1$)

$$g_K(V, t)$$

We can write an expression for the conductivity of this ion as

$$g_K = \bar{g}_K n^4(V, t)$$

Four activation gates
result in fourth power
for gating variable n

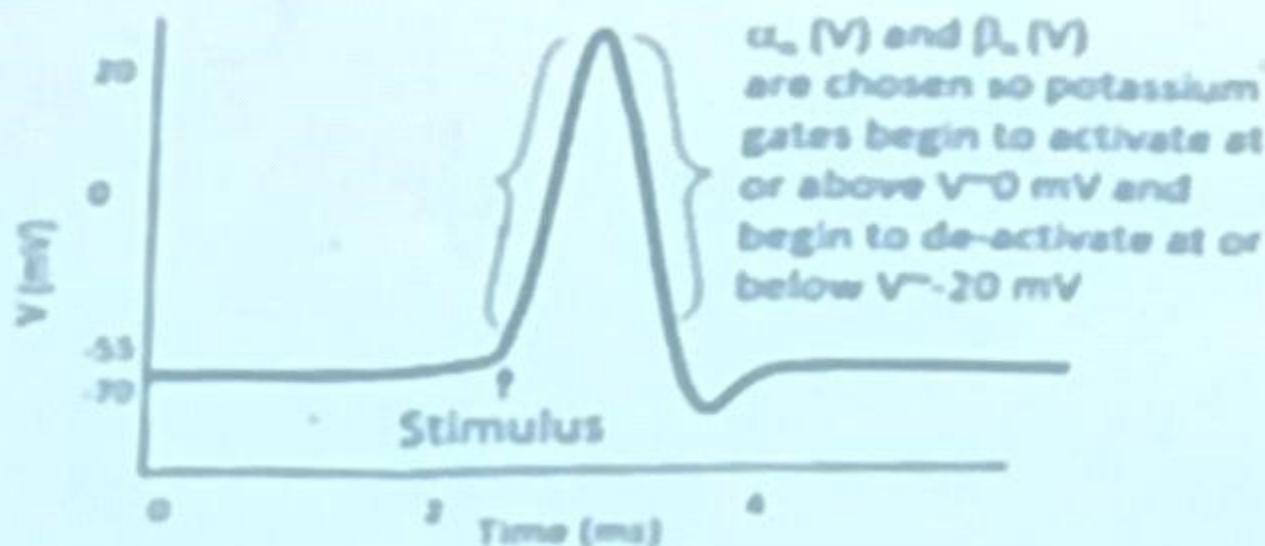
And then assume a simple first order kinetic behavior of the
gating variable n

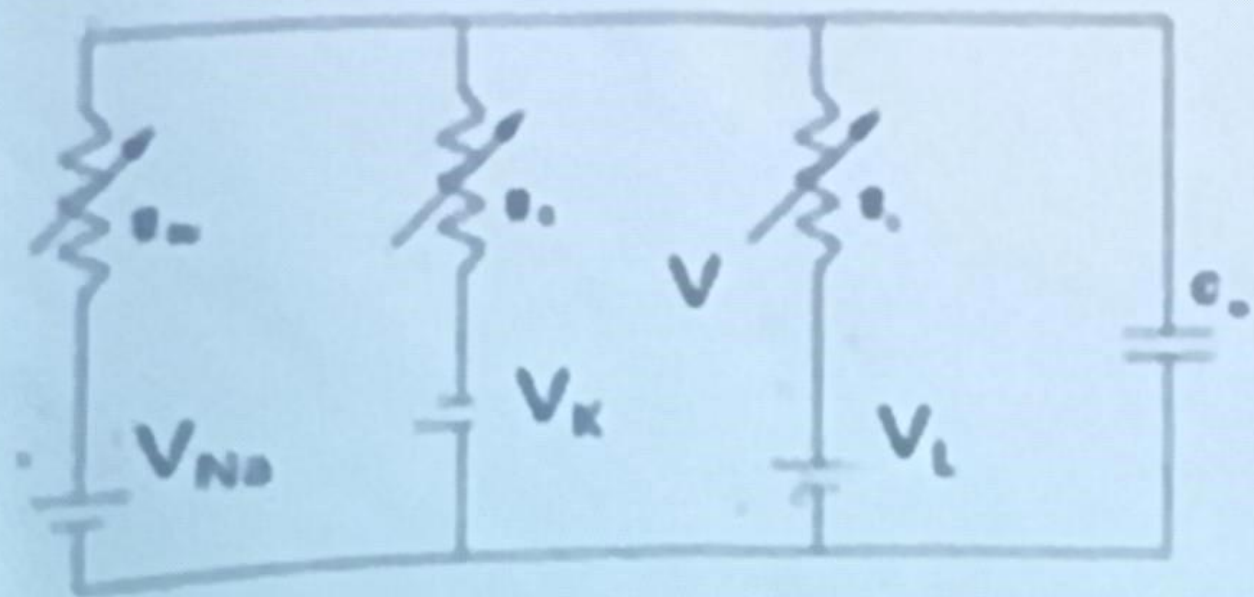
$$\frac{dn}{dt} = \alpha_n(V)(1 - n) - \beta_n(V)n$$

(same as previous slide,
with f now called n)



Potassium gate
protein with
4 identical
tetramers in a
ring shape (resulting
in the 4th power of n ,
as all gates must be
open for ion to pass)





Entire Hodgkin Huxley (HH) Model

$$I_{TOT} = C \frac{dV}{dt} = (V_K - V)g_K(V, t) + (V_{Na} - V)g_{Na}(V, t) + (V_L - V)g_L$$

Inside

$$\begin{aligned} \frac{dn}{dt} &= \alpha_n(V) (1-n) - \beta_n(V) n \\ \frac{dm}{dt} &= \alpha_m(V) (1-m) - \beta_m(V) m \\ \frac{dh}{dt} &= \alpha_h(V) (1-h) - \beta_h(V) h \end{aligned}$$

$$g_K(V, t) = \bar{g}_K (n(V, t))^4$$

$$g_{Na}(V, t) = \bar{g}_{Na} (m(V, t))^3 h(V, t)$$

$$g_L = \bar{g}_L$$

Parameters $C, V_K, V_{Na}, V_L, \bar{g}_K, \bar{g}_{Na}, \bar{g}_L$ are derived from experimental measurements

The three α and β functions are chosen so that the channel gates open at the observed membrane potentials and with the appropriate speed for a particular type of neuron

Ion channels-related diseases

Ion channels-related diseases

Neuronal disorders like Epilepsy, Alzheimer's disease, Parkinson's disease, Schizophrenia may result from dysfunction of voltage-gated sodium, potassium and calcium channels