

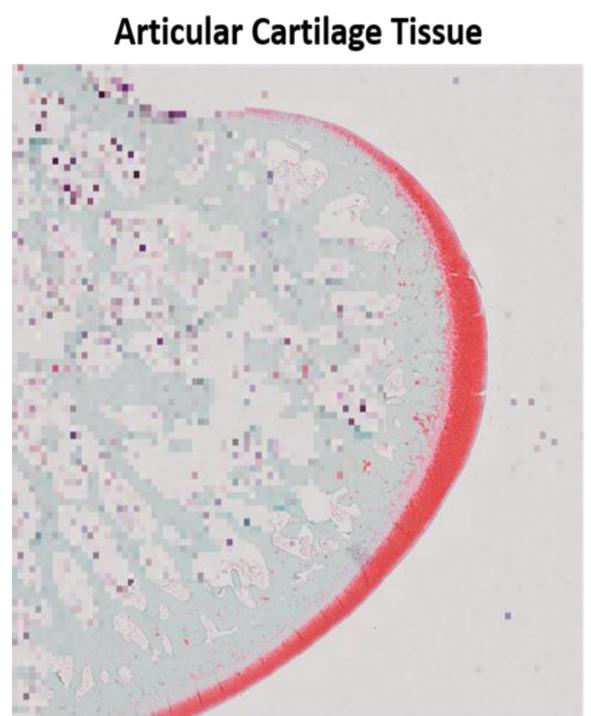
### IE:5995 Deep Learning Project: Articular Cartilage Segmentation

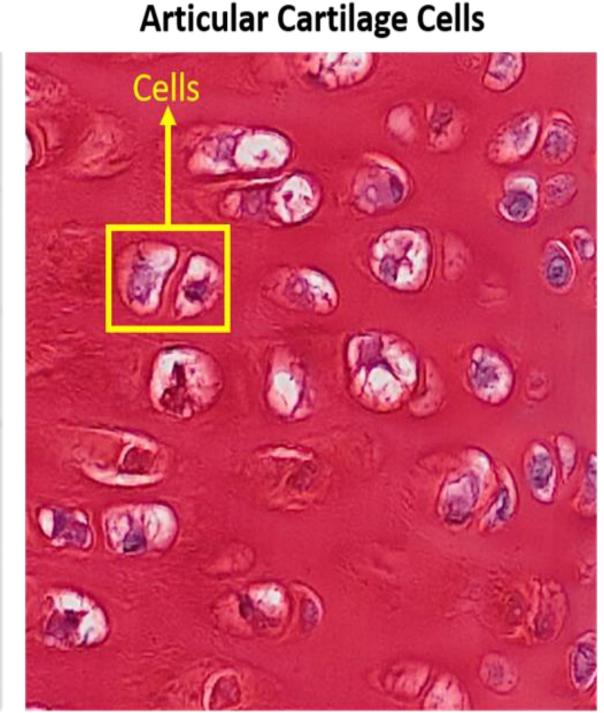


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#### **Abstract**

The gold standard for evaluating articular cartilage tissue relies heavily on human-eye observations. However, this method is not only subjective but also time consuming. In this project, we propose an automated system for evaluating microscopic cartilage tissue using state-of-art deep learning methods. Our approach consists of first segmenting stained cartilage tissue using the fully convolutional neural network, U-Net [1]. We supplement this by developing a method for segmenting the cells within the would-be segmented region. We compare two methods in this regard: (1) U-Net and (2) a Deep Convolutional Aware Network (DCAN) [2]. The resulting binary masks from this step is then used as part of a post processing technique for counting articular cartilage cells. We hope our method will alleviate histology based approaches for the evaluation of the articular cartilage.





**Articular Cartilage Cell Count** 

Figure 1. Overview of the main goals of this project. First, a method is required for segmenting the red stained articular cartilage tissue. Within this segmented area, articular cartilage cells are segmented. The resulting binary mask of the segmented cells are then counted. This cell count provides valuable insight in the health of articular cartilage tissue. An automated version of this process will reduce the time and improve the accuracy over human eye cell counting methods.

### **Setting Up the Architecture**

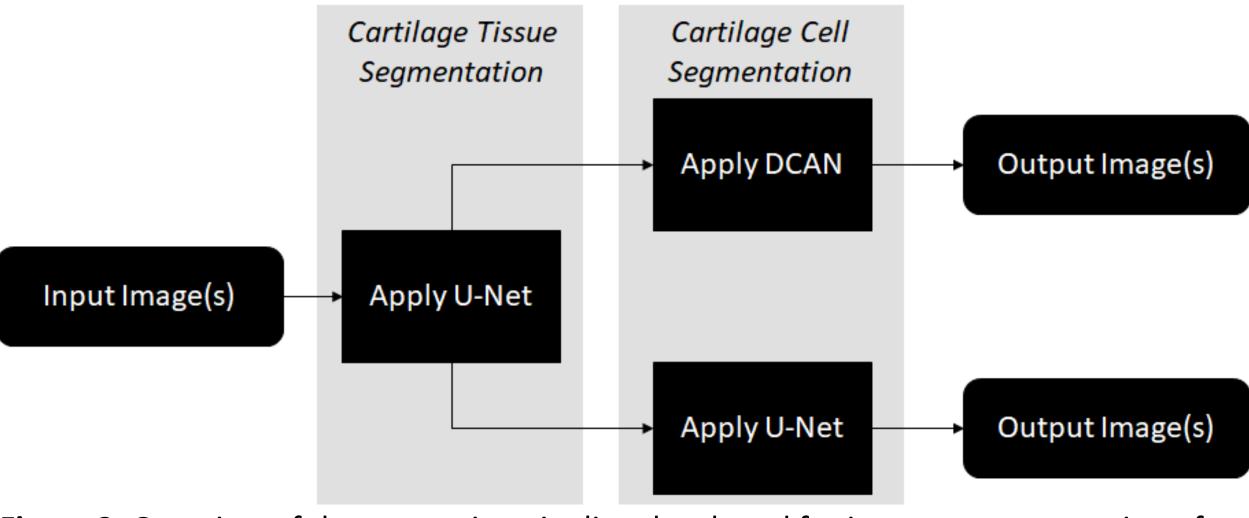


Figure 2. Overview of the processing pipeline developed for instance segmentation of articular cartilage cells. A modified U-Net neural network is trained to first segment cartilage tissue. Two different neural networks, U-Net and DCAN, were compared in order to determine the optimal cell instance segmentation method.

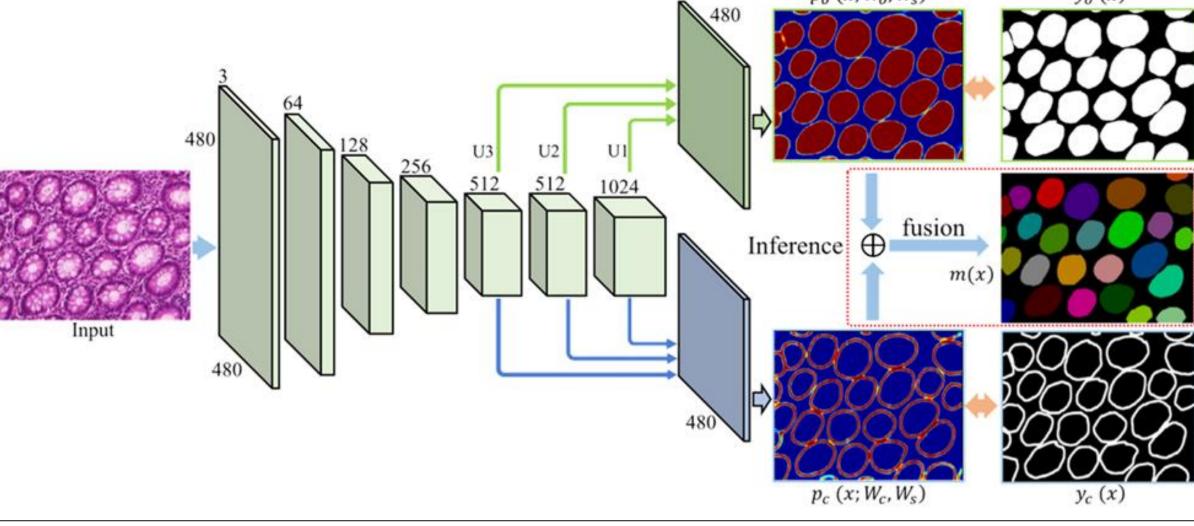
## copy and crop max pool 2x2 dup-conv 2x2 conv 1x1

Figure 3. The architecture of the neural network, U-Net, developed by Olaf et al [1]. This network is composed of a fully convolutional neural network. More specifically, an encoding path to capture context and a decoding path that enables precise localization.

clusters by incorporating both object and contour masks. DCAN uses end-to-end fully convolutional network to deal with variation in input images. In addition, auxiliary supervision is employed to help the network deal with vanishing gradients.

Figure 4. Overview of the Deep Contour Aware Network (DCAN) developed by Chen

et al [2]. This neural network has found success in identifying individual cells in



### **Tissue Segmentation**

The original U-Net architecture is retained with a several modifications. Batch normalization layer is added after convolution layer. Padding is applied to keep the image size through each convolution.

Table 1 describes the data augmentation approaches used. These include linear transformation, brightness transformation, elastic deformation as well as hue adjustment. We used a loss function combination of dice loss and cross binary entropy. Table 2 lists how images were partitioned between training, validation and testing. This function is minimized by an Adam optimizer. The final segmentation result is evaluated using the dice metric.

**Table 1.** Summary of the 7 various data augmentation methods used for both segmentation tasks. Blurring was not used for tissue segmentation.

Augmentation Type			
	Change		
Hue Adjustment	Adjust image hue in range (0.5,1.0)		
Brightness Adjustment	Adjust brightness in (0.9,1.0)  Scale images in x and y direction		
Elastic Deformation			
Image Gaussian Blurring	Convolve image with gaussian function		
Image Reflection	Flip image vertically/horizontally		
Image Rotation	Rotate image (0,90) degrees		

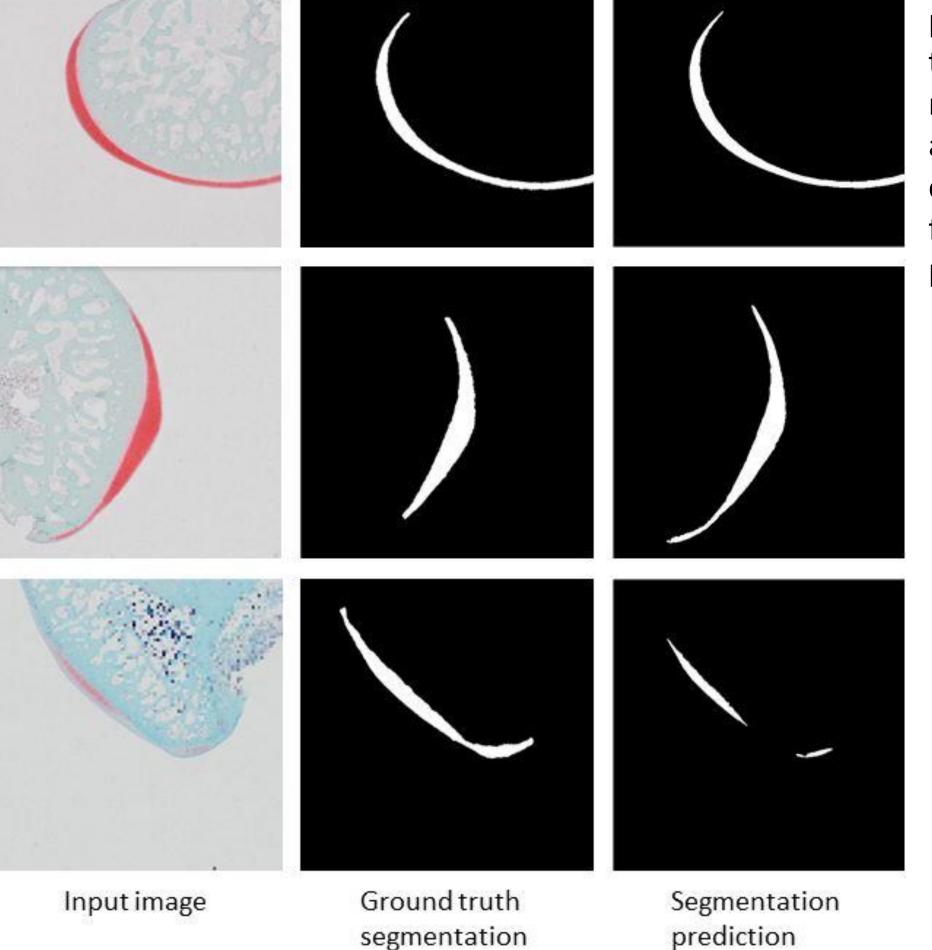


Figure 5. Examples of input images, ground truth segmented images, and predicted segmentations output from the implemented U-Net. The first two rows correspond to successful segmentation predictions. The last row corresponds to a failed segmented prediction which may be attributed to the lack of the red stain in the input image. An average dice coefficient of 0.9032 is achieved. The lowest value of 0.5285 is obtained from the image in the 3rd row in the figure 5. All other (9 images) test predictions had values above 0.9.

Table 2. The number of images input into the processing pipeline for articular cartilage tissue segmentation. A variety of healthy and injurious cartilage cross sectional images were used. More unhealthy images were used as injurious cartilage tissue does not stain as well as healthy. In addition, the average dice coefficient computed for the test images is also given.

	Training Images	Validation Images	Test Images	
Count	35	10	10	
Dice Coef.	-	-	0.9032	

### **Cell Segmentation**

In this task, two methods are applied and compared:

- 1. U-Net applied with loss weight map to account for class imbalance as well as improving its ability to differentiate adjacent cells.
- 2. DCAN: Two ground truth masks are used. One for the object (whole cell) and another of the object's contour (edges). The loss function of both are

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ummed.			Training	Validation	Test
ble 3. The number of iginal images input into e processing pipeline. A riety of images were used reflect the different tissue undaries and degree of ain. Also shown are the erage dice coefficient and scores computed for the st images of both the U-			Images	Images	Images
		Count	100	20	20
	U-Net	Dice Coef.	-	-	0.8846
		F1 Score	-	-	0.8469
	DCAN	Dice Coef.	-	-	0.6483
		F1 Score	•	-	0.6749
et and DCAN.					

# **Ground Truth** Segmentation Input Image

Segmentation

Prediction by U-Net

Figure 6. Examples of some test images, their ground truth segmentation masks, as well as the predicted segmentation from U-Net and DCAN. U-Net achieves an average dice coefficient of 0.8846 and a F1 score of 0.8469. Its prediction on some cells with certain appearance is poor and results in low metrics' value (lowest 0.4898 for F1 and 0.4809 for dice, respectively). The segmentation results for DCAN were worse, yielding an average dice loss and F1 scores of 0.6483 and 0.6749, respectively. Maximum and minimum dice loss values were 0.8761 and 0.0772. Similar metric were obtained for the F1 score: 0.9054 and 0.0645. It should be noted that auxiliary supervision was omitted in our implementation of DCAN.

### Conclusions

We have shown our method for instance segmentation of articular cartilage cells using a deep learning approach. Using U-Net is sufficient for segmenting both articular cartilage cells and tissues as it yielded high dice coefficient and F1 scores. However, we obtained worse segmentation results from the DCAN model. These results may be attributed to how we combined the results from the auxiliary supervision as well as omitting regularization in the loss function. We anticipate by optimizing these components as well as adding more training images, we may improve the performance of the DCAN model.

### **Future Work**

A number of future works remain to be done. These include the following:

- Improve the DCAN neural network implementation.
- Increase the number of training images used to train the neural networks in order to improve the performance of the segmentations.
- Apply DCAN and U-Net on the entire resulting masks from the articular cartilage tissue segmentation step.
- Incorporate a method for counting the number of cells from the final segmentation task into the processing pipeline.

### Acknowledgements

Prediction by DCAN

We would like to acknowledge and thank Professors Baek and Goetz for their invaluable assistance and feedback throughout the duration of this project.

### References

- [1] Ronneberger, Olaf et al. "U-net: Convolutional networks for biomedical image segmentation." International Conference on Medical image computing and computer-assisted intervention. Springer, Cham, 2015.
- [2] Chen, Hao et al. "DCAN: Deep contour-aware networks for object instance segmentation from histology images," Medical Image Analysis, vol. 36, pp. 135-146, 2017.