

1 Introduction

The Cerebrospinal Fluid (CSF) surrounds the brain and acts as a protection to the brain inside the skull. As a result of the cardiac cycle the CSF will flow up and down the subarachnoid space (SAS) surrounding the spinal cord. The Chiari malformation is a displacement of the cerebellar tonsils that partially blocks CSF flow entering the SAS around the spinal cord. This causes abnormal CSF flows which sometimes results in a syringomyelia inside the spinal cord filled with fluid. Treatment may include surgery to remove parts of the bones of the skull to relieve pressure. Studies have shown that the syrinx gradually vanishes after surgery. The mechanisms behind this are not yet fully understood. Many researchers have suggested Computational Fluid Dynamics (CFD) to give useful insight, as experiments are very difficult and expensive.

2 Problem definition

The model consists of a spinal cord surrounded by space filled with CSF. The cord has a diameter of 10 mm and the fluid space has a diameter of 18 mm. The model also has a inner central spinal canal, 2 mm in diameter. The central spinal canal has height 4 cm and is placed in the center of the mesh which has height 6 cm.

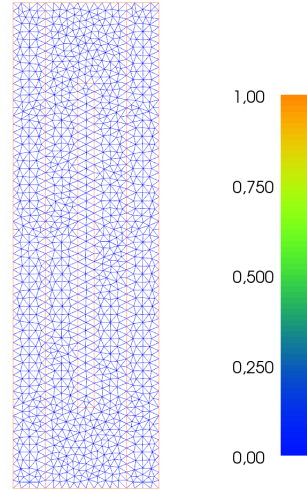


Figure 1: Coarse version of the mesh

2.1 Governing equations

Fluid Space

The fluid in the SAS as well as the central spinal canal is governed by the Navier-Stokes equations

$$\frac{\partial u_f}{\partial t} + u \cdot \nabla u = -\frac{1}{\rho_f} \nabla p_f + \frac{1}{\rho} \nabla \cdot \tau + F \quad \text{in } \Omega_f \quad (1)$$

$$\frac{\partial \rho}{\partial t} + \nabla \cdot (\rho u_f) = 0 \quad \text{in } \Omega_f \quad (2)$$

where u_f is the fluid velocity, ρ_f is the fluid density, τ is the stress tensor and F are all external volume forces. In addition to the equations (1)-(2) comes

boundary conditions at the domain boundary. When solving the equations numerically, manipulation of the coupled equations into simpler equations may lead to problems involving the boundary conditions. Therefore a proper choice of boundary conditions is crucial for stability and existence.

In this case we will consider incompressible flows, where ρ is constant and $\nabla \cdot u = 0$. The stress tensor is given by

$$\tau = 2\mu\epsilon(u_f)$$

where $\epsilon(u_f) = \frac{1}{2}(\nabla u_f + (\nabla u_f)^T)$. When taking the divergence of the stress tensor the Navier-Stokes equations for incompressible flows take the form

$$\frac{\partial u_f}{\partial t} + u \cdot \nabla u_f = -\frac{1}{\rho} \nabla p_f + \nu \nabla^2 u_f + F \quad \text{in } \Omega_f \quad (3)$$

$$\nabla \cdot u_f = 0 \quad \text{in } \Omega_f \quad (4)$$

Spinal Cord

The spinal cord is modeled as a poroelastic medium, which allows for some fluid to flow from the SAS to the central spinal canal. In this case the Biot-equations have been used to include both elasticity and flow in the spinal cord.

$$-\mu \nabla^2 u_s - (\lambda + \mu) \nabla \nabla \cdot u_s - \nabla p_s = 0 \quad \text{in } \Omega_s \quad (5)$$

$$(\nabla \cdot u_s)_t - \nabla \cdot (\kappa \nabla p_s) = 0 \quad \text{in } \Omega_s \quad (6)$$

Here, $\kappa \nabla p_s$ represents the fluid velocity in the porous medium. p_s is the pressure in the fluid occupying the pores.

2.2 Weak form

Equations (3) and (5) will be multiplied by a vector test function, v , and equations (4) and (6) with a scalar test function, q . The equations are then integrated over the entire domain. By using two different test functions the coupled equations can be written as one weak formulation each

$$\begin{aligned} \int_{\Omega_f} \frac{\partial u_f}{\partial t} \cdot v dx + \int_{\Omega_f} (u_f \cdot \nabla u_f) \cdot v dx &= \frac{1}{\rho} \int_{\Omega_f} \nabla \cdot v p_f dx - \nu \int_{\Omega_f} \nabla u : \nabla v dx \\ &- \frac{1}{\rho} \int_{\partial \Omega_f} p v \cdot n dS + \nu \int_{\partial \Omega_f} \nabla u \cdot v \cdot n dS + \int_{\Omega_f} \nabla \cdot u q dx \end{aligned} \quad (7)$$

And for the fluid and structure movement in the cord:

$$\begin{aligned}
& \mu \int_{\Omega_s} \nabla u_s : \nabla v dx + (\mu + \lambda) \int_{\Omega_s} \nabla \cdot u_s \nabla \cdot v dx - \mu \int_{\partial\Omega_s} \nabla u_s \cdot v \cdot n dS \\
& - (\lambda + \mu) \int_{\partial\Omega_s} \nabla \cdot uv \cdot n dS = \frac{1}{\rho} \int_{\Omega_s} \nabla \cdot v p_s dx - \frac{1}{\rho} \int_{\partial\Omega_f} p v \cdot n dS \\
& + \nu \int_{\partial\Omega_s} \nabla u \cdot v \cdot n dS + \int_{\Omega_s} \frac{\partial(\nabla \cdot u_s)}{\partial t} q dx + \int_{\Omega_s} k \nabla p_f \cdot \nabla q dx - \int_{\partial\Omega_s} q \kappa \nabla p_f \cdot n dS
\end{aligned} \tag{8}$$