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Project Reference 1: Hemodynamics Ali Nasimi

Hemodynamics is study of the relationship among physical factors affecting blood flow through the vessels.

Poiseuille's Law (Blood flow is a function of pressure difference and resistance)

Blood Flow (F)
pressure difference (ΔP)
resistance to blood flow (R)
through the vessel

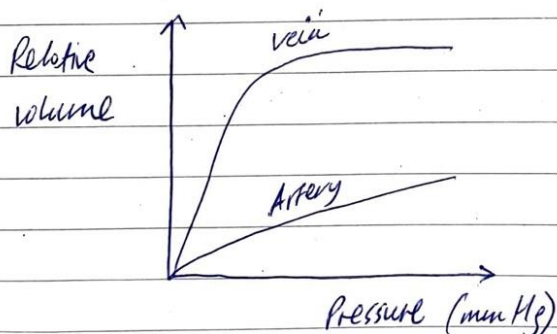
$$F = \frac{\Delta P}{R}$$

known as
Poiseuille's Law
or Ohm's Law.

Definitions from VFT2 Descriptor

$$\text{Compliance } (C = \frac{dV}{dp})$$

Compliance: sometimes called capacitance/distensibility refers to the ability of a vessel to respond to an increase in pressure by distending or swelling, and increase the volume of blood it can hold, or with decreased pressure, a decrease in volume.



Arteries : any of the muscular-walled tubes forming part of the circulation system by which blood (mainly oxygenated) is conveyed from the heart to all parts of the body

Veins : any of the tubes forming part of the blood circulation system of the body carrying (oxygen-depleted blood towards the heart,

Blood vessel wall : Shear stress is the tangential force of the flowing blood on the endothelial surface of the blood vessel.

- High shear stress (laminar flow) promotes endothelial cell survival and quiescence, alignment in the direction of flow, and secretion of substances that promote vasodilation and anticoagulation.
- Low shear stress (or changing shear stress direction as found in turbulent flow, promotes endothelial proliferation and apoptosis, shape change and secretion of substances that promote vasoconstriction, coagulation and platelet aggregation.

Rigid Walls : Rigidity is a condition when blood vessels lose elasticity. Rigidity causes blood vessels hardening of blood vessels so blood supply decreases.

Only a small amount of stroke volume is used for blood circulation, mostly only arteries are rigid due to hardening and thickening of artery walls.

Hemodynamics Ali Nbsiri (cont'd)

Darcy's Law / Ohm's Law

$$F = \frac{\Delta P}{R}$$

$$I = \frac{V}{R}$$

F (Flow) is defined as the volume of blood passing each point of the vessel in one unit time

Pressure (P) which is the force that pushes the blood through the vessel is defined as the force exerted on a unit surface of the wall of the tube perpendicular to flow. Pressure is expressed as millimeters of mercury (mmHg). As pressure changes over the course of the blood vessel there is no one value for pressure, so ΔP change in pressure is used instead.

$$\Delta P = P_1 - P_2$$

Resistance is how difficult it is for blood to flow from point 1 to point 2. The resistance equation is:

$$R = \frac{8\eta L}{\pi r^4}$$

η = fluid viscosity

L = vessel length

r = inside radius of the vessel.

Poiseuille's Law (sub in R equation into Darcy's Law)

$$F = \frac{\Delta P}{R} = \frac{\Delta P}{\left(\frac{8\eta L}{\pi r^4}\right)} = \boxed{\frac{\pi r^4 \Delta P}{8\eta L}} \quad \boxed{F = \frac{\pi \Delta P r^4}{8\eta L}}$$

Shear stress in blood vessels

Shear stress is the tangential force of the flowing blood on the endothelial surface of the blood vessel.

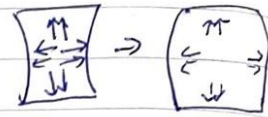
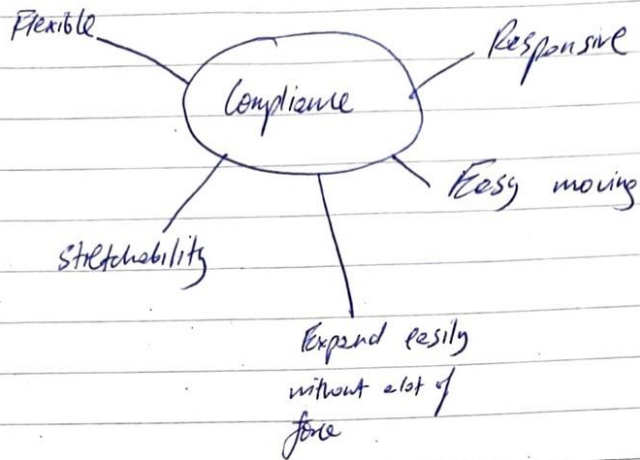
High shear stress (found in laminar flow) promotes endothelial cell survival and quiescence, alignment in the direction of flow, and secretion of substances that promote vasodilation and anticoagulation.

Simplified

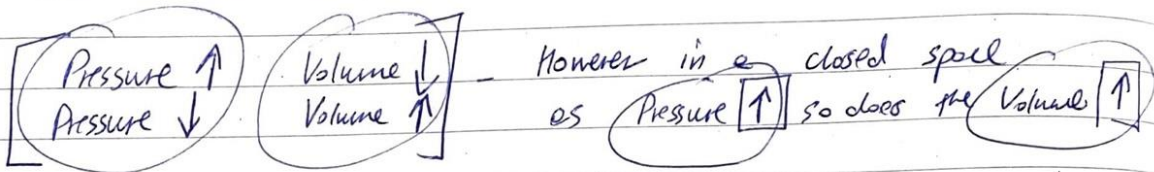
endothelial cells form a single cell layer that lines all blood vessels

- Endothelial lining of blood vessels presents a large surface area for exchange of materials between blood and tissue
- Endothelial cells are quiescent meaning that they are proliferating (~~pro~~ proliferation - rapid reproduction of a cell, part or organism)
- High shear stress in blood vessels promote vasodilation (widening of blood vessels as a result of the relaxation of the blood vessel's muscular walls.) & anticoagulation - (prevent the blood from clotting).

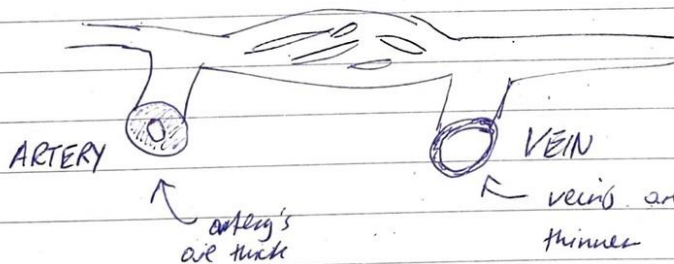
• Compliance of blood vessels



Pressure and Volume



$$\text{Compliance} = \frac{\text{Change in Volume}}{\text{Change in Pressure}} = \frac{\Delta V}{\Delta P}$$



Arteries: carry oxygenated blood from your heart to body.

Veins: carry deoxygenated blood from your organs back to your heart.

- Arteries are less compliant
- Veins are more compliant

Navier-Stokes Equations

In physics, Navier-Stokes equations are certain partial differential equations which describe the motion of viscous fluid substances.

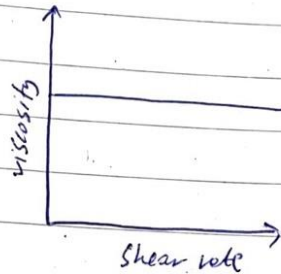
$$\nabla \cdot u = 0$$

← First Navier-Stokes Equation

$$\rho \frac{du}{dt} = -\nabla p + \mu \nabla^2 u + F$$

← Second Navier-Stokes Equation

Newtonian Fluid



← Newtonian Fluid

Assumptions: Newtonian Fluid
Incompressible
Isothermal

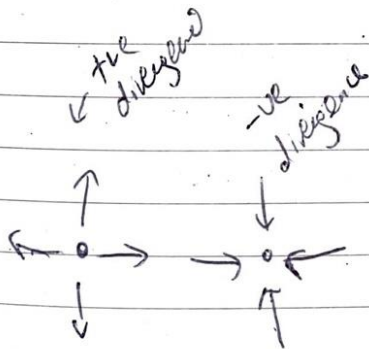
Velocity vector field

$$\nabla \cdot u = 0$$

Divergence

Divergence (Mathematical Expression)

$$\text{div } \vec{F} = \nabla \cdot \vec{F} = \begin{bmatrix} \frac{\partial}{\partial x} \\ \frac{\partial}{\partial y} \\ \frac{\partial}{\partial z} \end{bmatrix} \cdot \vec{F}$$



Divergence of vector field indicates how much or how little a point acts as a source of a fluid.

Navier-Stokes Equation

friction/viscosity

$$\rho \frac{du}{dt} = -\nabla p + \mu \nabla^2 u + F$$

← 2nd Navier-Stokes Equation

pressure

$$ma = \Sigma F$$

↓

$$\rho a = \Sigma F$$

↓

$$\rho \frac{du}{dt} = \Sigma F$$

pressure

$$\rho = \frac{m}{V}$$

density

← mass

← volume

$$a = \frac{du}{dt}$$

acceleration

$$\rho \frac{du}{dt} = -\nabla p + \Sigma F$$

$$\frac{du}{dt} = \frac{\partial u}{\partial t} + u \cdot \nabla u$$

$$\rho \frac{du}{dt} = -\nabla p + \mu \nabla^2 u + \Sigma F$$

friction/viscosity

external force
(usually gravity)

$$F = \rho g$$

gravity/external force

Navier-Stokes Equation

$$\nabla \cdot \underline{u} = 0$$

← Conservation of Mass

$$\rho \frac{d\underline{u}}{dt} = -\nabla p + \mu \nabla^2 \underline{u} + \underline{F} \leftarrow \begin{array}{l} \text{Conservation of momentum} \\ \text{(Newton's 2nd law)} \cdot (F=ma) \end{array}$$

$$\underline{u} = [u, v, w] \leftarrow \text{vector with components in } x, y \text{ and } z \text{ direction}$$

$$\nabla \cdot \underline{u} = \frac{\partial u}{\partial x} + \frac{\partial v}{\partial y} + \frac{\partial w}{\partial z} = 0$$

↑ tells us that mass is conserved

↑
change in
x-direction

↑
change in
y-direction

↑
change in
z-direction

$$\begin{array}{c} \text{velocity} \\ \downarrow \\ \rho \frac{d\underline{u}}{dt} \end{array} \rightarrow \text{acceleration} = -\nabla p + \mu \nabla^2 \underline{u} + \underline{F}$$

density ↑ time

Internal Force External Force (gravity)

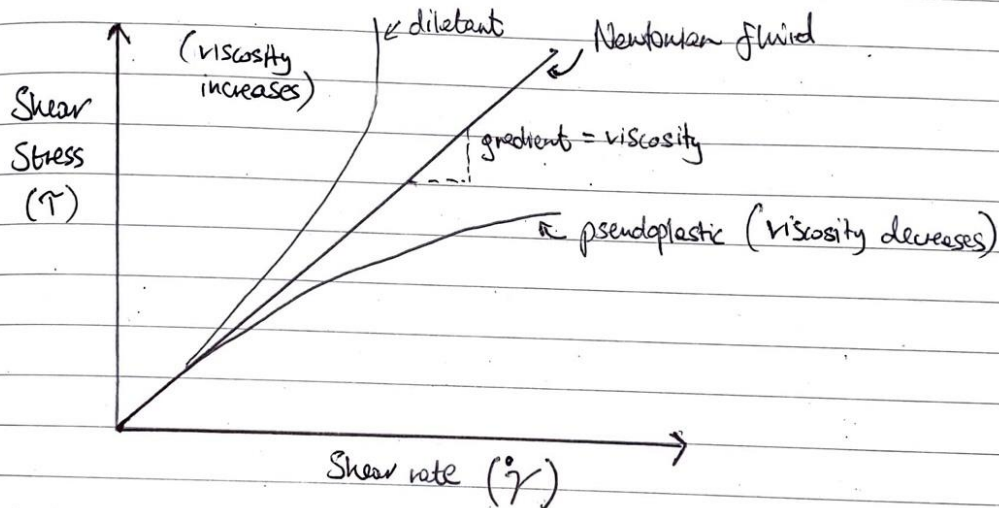
$$\nabla p = \left(\frac{\partial p}{\partial x}, \frac{\partial p}{\partial y}, \frac{\partial p}{\partial z} \right) \leftarrow \text{change in pressure. (Fluid moves from high pressure to low pressure)}$$

Internal Forces

$$\mu \nabla^2 \underline{u} \leftarrow \text{viscosity}$$

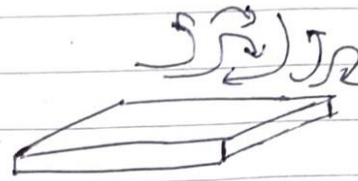
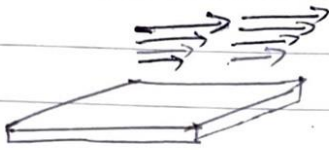
Newtonian Fluids.

Newtonian Fluids have constant viscosity. Their shear rate is directly related to the shear stress. Viscosity shows the resistance to the deformation of fluid. The more viscous a substance the greater the resistance to the deformation of the fluid. For Newtonian Fluids: in the shear stress, shear rate graph there is a linear relationship. The gradient of this graph is the viscosity. As this is a linear relationship for a Newtonian Fluid the viscosity value is constant. For the purpose of this project the blood flow is assumed to be a Newtonian Fluid.

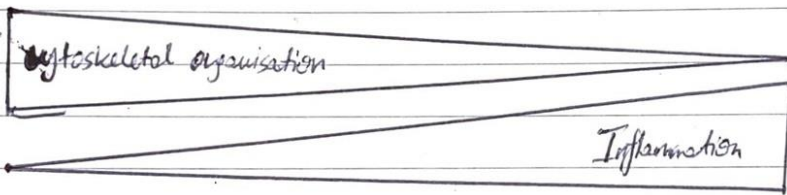
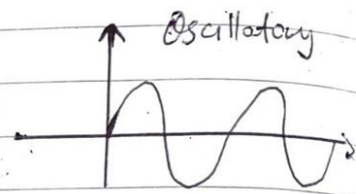
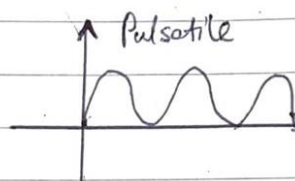
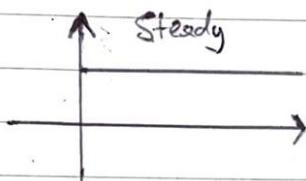


ESC (cytoskeletal)

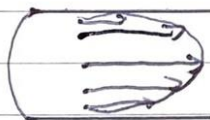
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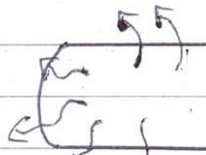
DYNAMICS



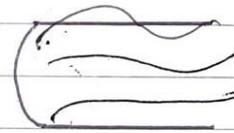
DIRECTION



Luminal



Transmural



Interstitial

Quiescence →



Angiogenesis

Blood Vessel Compliance

- We saw that pressure differences exist in arteries and veins as a result of a difference in anatomy of the two blood vessels.
- Blood pressure is not the only measurement that can be used to describe the properties of blood vessels.

Qualitative Measure of Compliance

- Compliance basically describes how easy it is to expand a blood vessel.
- If expanding the blood vessel causes it to resist this expansion and recoil back to its normal size, then the blood vessel has a low compliance.

- If the blood vessel remains expanded without much recoil, it has a high compliance.

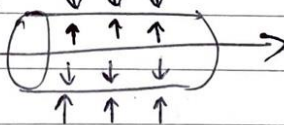
Arteries (Low compliance)

- Arteries have a thick layer of smooth muscle, which gives them the ability to recoil during expansion. This means that when the blood pushes against the walls of the arteries, they push right back. Therefore, when blood fills the large arteries, they only expand by a small amount (10%).

a)



b)



* Arteries can withstand high pressures without increasing in volume by too much.

Veins (High compliance)

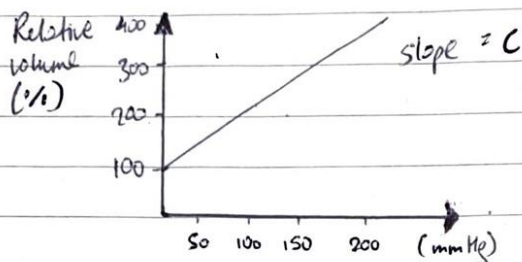
- Veins behave very differently compared to arteries. When they experience blood flow, the blood pushes on the walls but the walls cannot push back as hard. This expands the cross-sectional area and therefore increases the volume of blood that can pass inside the vein. It also ensures there is less built up pressure in the veins. Veins are stretchy therefore no build up in pressure inside them.

Quantitative Measure

$$C = \frac{\Delta V}{\Delta P}$$

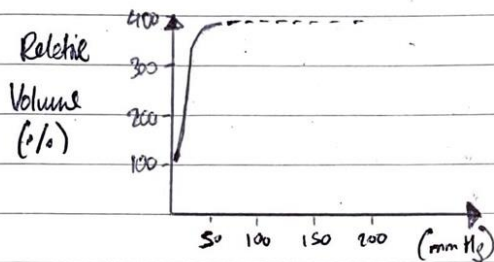
C = compliance value for blood vessel
 ΔV = change in volume of blood vessel
 ΔP = change in pressure between inside & out.

Arteries (LOW COMPLIANCE)



- For arteries, the slope is small (LOW COMPLIANCE).
- Arteries can resist high pressures without really increasing in volume by that much.

Veins (HIGH COMPLIANCE)



- For Veins, the slope is very large. (HIGH COMPLIANCE)
- Veins change in volume even when there is a tiny increase in pressure.
- Hence veins expand (distend) very well and store large volumes of blood.

Water's Newtonian Fluid
Blood is non-newtonian.

Viscosity of blood = 3.5 - 5.5 cP

Important Definitions

Arteries -



Thick wall

Veins -



Thin wall

ARTERIES

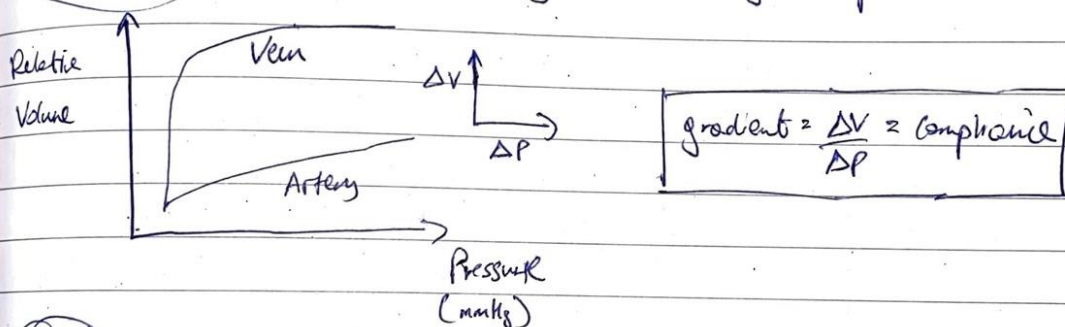
Blood vessels that deliver oxygen-rich blood from heart to the tissues of the body.

VEINS

Blood vessels that returns oxygen-depleted blood from organs back to heart.

VASCULAR COMPLIANCE

The ability of a blood vessel wall to expand and contract passively with change in pressure



WSS

- The force per unit area exerted by a solid boundary on a fluid in motion (and vice-versa) in a direction tangent to flow of the fluid. It is caused by the friction within the fluid and between the fluid and the vessel wall.

Hagen-Poiseuille Equation

$$\Delta p = \frac{8\mu L Q}{\pi R^4}$$

L = Length of pipe

Q = Volumetric flow rate

Fluid element analysis -
predict how fluid flows

R = pipe radius

μ = dynamic viscosity

