

# Photoacoustic imaging of controlled blood oxygenation within a programmable dynamic flow system

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## Introduction

- Blood oxygenation ( $sO_2$ ) is an important physiological measure to assess hemodynamics on the macro- and micro-scales.
- Established methods for estimation of  $sO_2$  include near-infrared spectroscopy<sup>1</sup> and calculation from measurements of the partial pressure of oxygen.<sup>2</sup>
- Wavelength-dependent photoacoustic (PA) signal intensities can be used to monitor  $sO_2$  values spatiotemporally in vascular structures.
- $sO_2$  measurements with PA are perturbed by processes such as spectral coloring and inhomogeneous light fluence distributions.
- $sO_2$  estimation approaches would benefit from an in-depth understanding of experimental ground truth.

## Aim

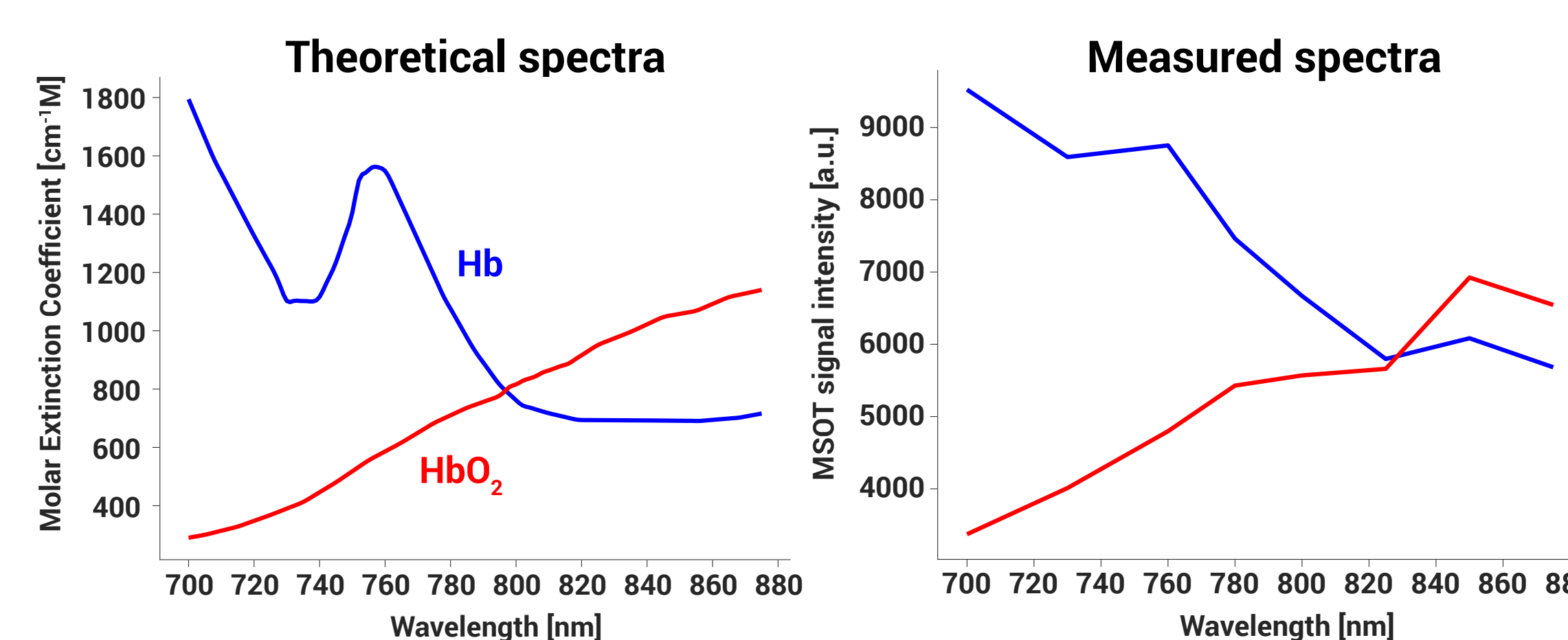
- To design and implement a phantom platform for investigation of the relationship between blood oxygenation measured using PA and ground truth oxygenation.

## Methods

- The programmable dynamic flow system was introduced into a commercial PA system (iThera Medical inVision 256-TF).
- Mouse blood (~5 mL) was 100% oxygenated with hydrogen peroxide, introduced via an injection site, and air bubbles were removed by a depressurization vent.
- Data acquisition was performed synchronously. PA signals were acquired at 7 wavelengths (700 to 875 nm, no averaging).
- After spectroscopy and  $pO_2$  readout stabilization, sodium hydrosulfite was introduced for deoxygenation.

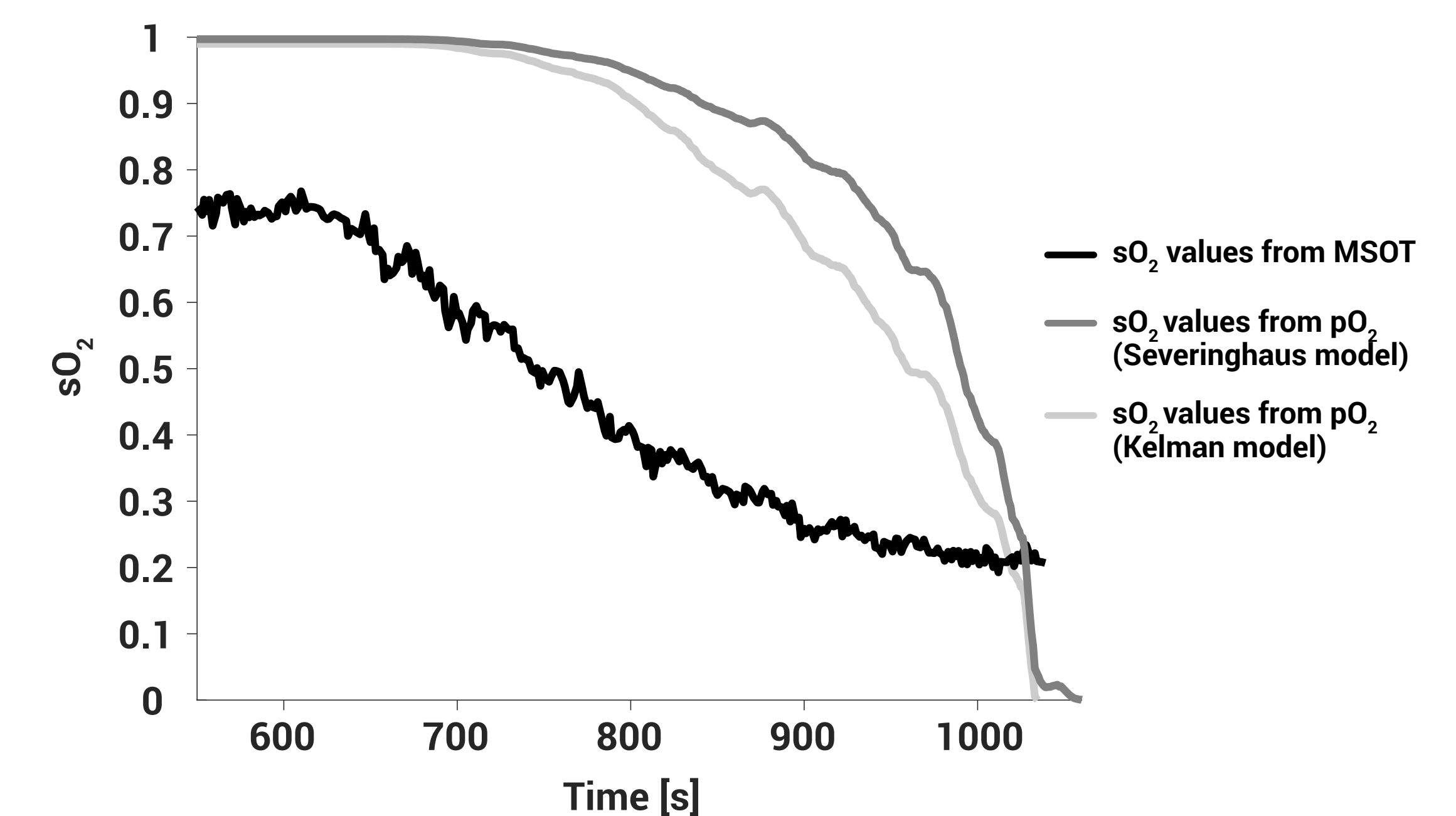
## Results

- We compared the theoretical spectra of oxygenated and deoxygenated blood with the start and end spectra measured in the MSOT (Fig. 2)



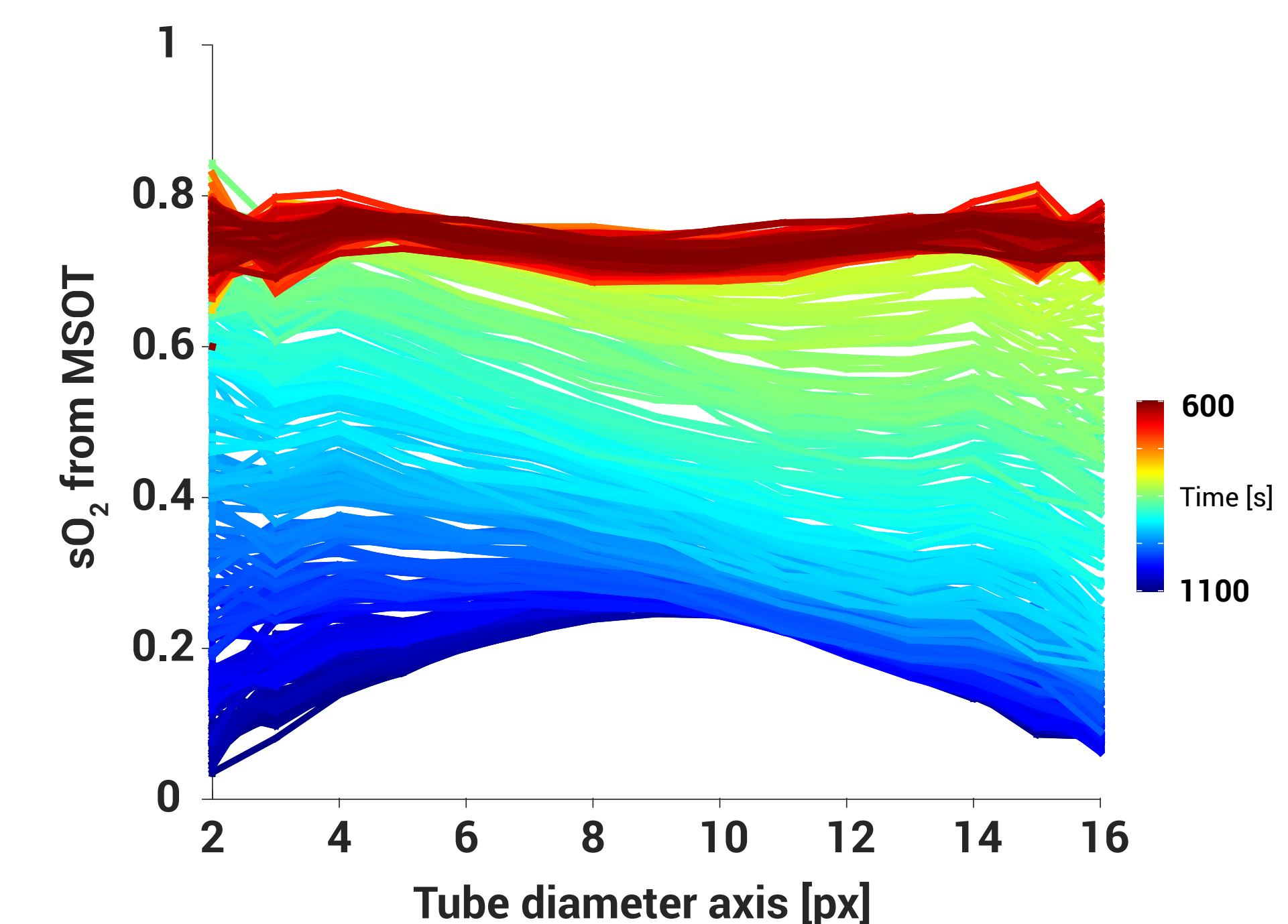
**Figure 2:** Comparison of theoretical spectra of oxyhemoglobin ( $HbO_2$ ) and deoxyhemoglobin ( $Hb$ ) with measured start and endpoint spectra from MSOT. Good agreement can be observed in general, except for dip omitted at around 725 nm.

- $sO_2$  values were calculated from  $pO_2$  values using the Severinghaus and Kelman models and plotted against MSOT-determined  $sO_2$  values (Fig. 3).



**Figure 3:** Time course of  $sO_2$  values from MSOT plotted with  $sO_2$  values from  $pO_2$  data over time. Although a similar trend can be observed between the three curves, the dynamic ranges and gradients are different.

- At lower  $sO_2$  levels, oxygenation was over-estimated in the tube center, as shown in Fig. 4.



**Figure 4:** Evolution of  $sO_2$  values measured over the course of the experiment where blood was progressively deoxygenated.  $sO_2$  values were measured in each pixel across the tube diameter.

- Inner regions of the tube are susceptible to spectral coloring: for low  $sO_2$ , high absorption by Hb reduces light penetration especially of shorter wavelengths, thus reducing the signal in the tube centre, causing elevation in the calculated proportion of  $HbO_2$ .

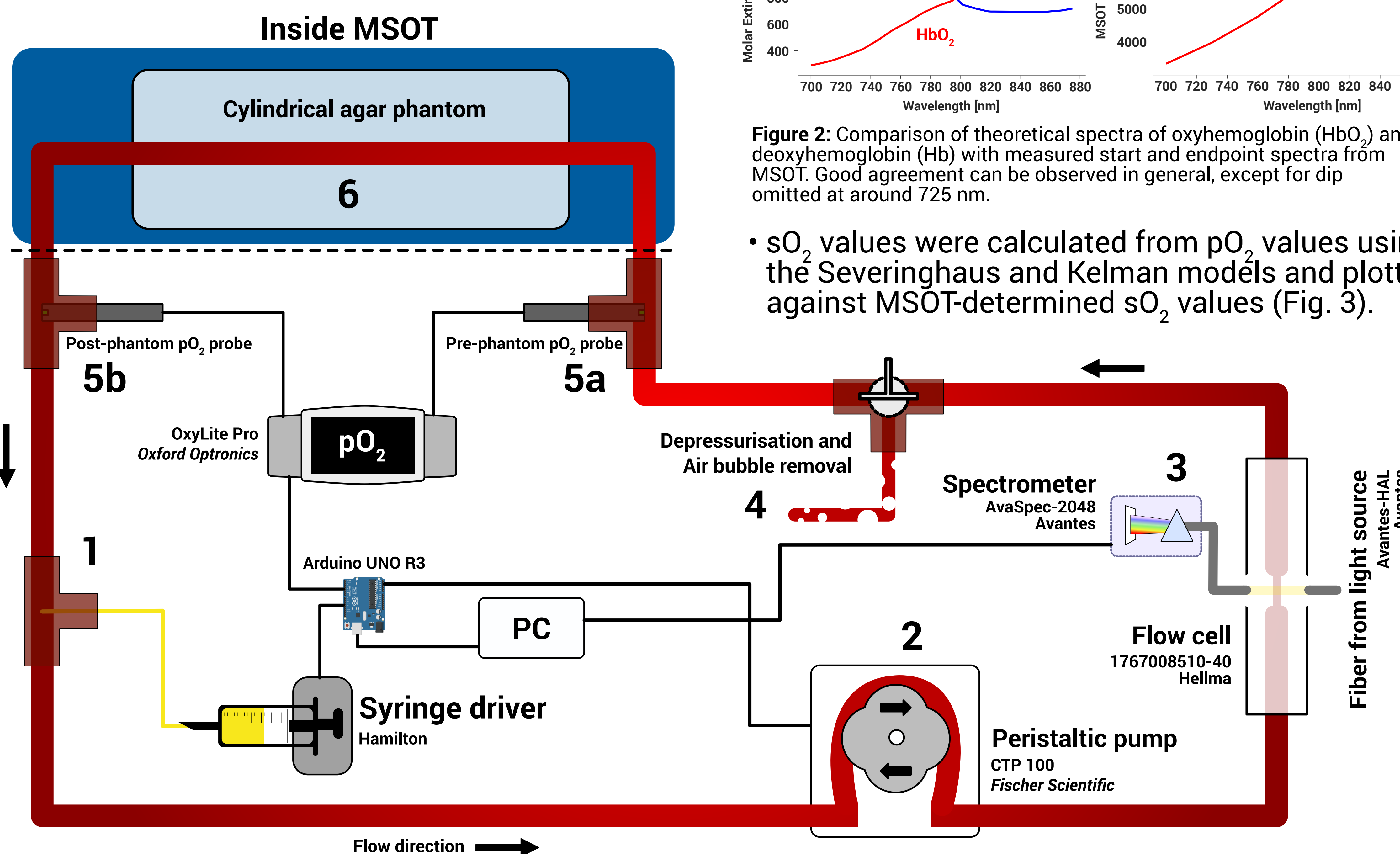
## Conclusion

- A programmable dynamic flow phantom was used to provide insights into the relationship between blood oxygenation measured using PA and ground truth oxygenation obtained by spectroscopy and/or  $pO_2$ .
- By improving the accuracy of the recovered spectra (e.g. fluence correction), we will improve the reproducibility of  $sO_2$  measurements in order to derive reliable information about blood and tissue oxygenation.

## References

- [1] Cope, M., 1991. *The development of a near infrared spectroscopy system and its application for non invasive monitoring of cerebral blood and tissue oxygenation in the newborn infants* (Doctoral dissertation, University of London).
- [2] Breuer, H.W., Groeben, H., Breuer, J. and Worth, H., 1989. Oxygen saturation calculation procedures: a critical analysis of six equations for the determination of oxygen saturation. *Intensive care medicine*, 15(6), pp.385-389.

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**Figure 1: Overview of the flow phantom.** (1) Injection site for introducing oxygenated blood into the flow system, and for subsequently deoxygenating the blood using sodium hydrosulfite delivered using the computer controlled syringe driver; (2) peristaltic pump provides blood circulation; (3) spectra are recorded as the blood passes through a flow cell; (4) air bubbles are released via a three-way tap; (5)  $pO_2$  measurements are made before (a) and after (b) the blood passes through the agar phantom immersed in the MSOT (6).