

# ICU CRAB Modeling Plan

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## 1. Modeling Overview and Objectives

### 1.1 Project Understanding

This project builds an intelligent quorum-quenching system targeting **CRAB** using engineered **EcN**. The system includes **three core layers** (sensing–amplification–execution), a **spatial targeting module** (AHL chemotaxis), a **positive feedback loop**, **multi-scenario visualization modules**, and **multi-level kill switches**, with customized delivery strategies for three infection scenarios: lung, bloodstream, and wound.

### 1.2 Modeling Objectives

ID	Modeling objective	Corresponding design module
M1	Quantify AHL sensing sensitivity and T7 amplification gain; optimize promoter/RBS strength	Core Pathway: Sensing + Amplification
M2	Analyze the bistable window of the positive feedback loop; determine activation/maintenance thresholds	Positive Feedback Loop Optimization
M3	Predict PvdQ degradation kinetics for 3-OH-C12-HSL	Execution Layer
M4	Simulate chemotaxis of engineered bacteria along AHL gradients	Spatial Enhancement
M5	Build a QS-regulated dynamic growth/dissolution model of CRAB biofilms	Background (biofilm formation mechanism)
M6	Model enzyme–probe competitive kinetics; predict the color-change time point	Visualization (lung/blood/wound)
M7	Predict timed clearance dynamics and safety window of the MazEF kill switch	Kill Switch

ID	Modeling objective	Corresponding design module
M8	Simulate targeted release of pH-sensitive liposomes in the lung	Route of Administration: Pulmonary
M9	Simulate diffusion and mass transfer of AHL/enzymes in core–shell microcarriers	Route of Administration: Wound

## 2. Model 1: ODE Model for AHL Sensing and T7 Amplification Cascade

### 2.1 Purpose

Quantify the full signal transduction from extracellular 3-OH-C12-HSL input to high intracellular PvdQ expression. Predict the system's **limit of detection**, **response time**, and **amplification gain**, and provide theoretical guidance for pAbaI\* promoter engineering and RBS optimization.

### 2.2 Biochemical Reaction Network

#### Sensing layer reactions:

1. Constitutive AbaR expression:  $\emptyset \xrightarrow{\alpha_{AbaR}} \text{AbaR}$
2. AHL transmembrane diffusion:  $\text{AHL}_{ext} \xrightleftharpoons[k_{out}]{k_{in}} \text{AHL}_{int}$
3. AbaR–AHL complex formation:  $\text{AbaR} + \text{AHL}_{int} \xrightleftharpoons[k_{off}]{k_{on}} \text{AbaR:AHL}$
4. pAbaI\* activation drives T7 RNAP expression:  $\text{AbaR:AHL} + \text{pAbaI}^* \rightarrow \text{T7 RNAP}$

#### Amplification layer reactions:

5. T7 RNAP drives PvdQ expression:  $\text{T7 RNAP} + \text{pT7} \rightarrow \text{PvdQ}$

### 2.3 ODE System

$$\begin{aligned}
 \frac{d[\text{AbaR}]}{dt} &= \alpha_{AbaR} - \gamma_{AbaR}[\text{AbaR}] - k_{on}[\text{AbaR}][\text{AHL}_{int}] + k_{off}[\text{AbaR:AHL}] \\
 \frac{d[\text{AHL}_{int}]}{dt} &= k_{in}[\text{AHL}_{ext}] - k_{out}[\text{AHL}_{int}] - k_{on}[\text{AbaR}][\text{AHL}_{int}] + k_{off}[\text{AbaR:AHL}] \\
 \frac{d[\text{AbaR:AHL}]}{dt} &= k_{on}[\text{AbaR}][\text{AHL}_{int}] - k_{off}[\text{AbaR:AHL}] - \gamma_c[\text{AbaR:AHL}] \\
 \frac{d[\text{T7}]}{dt} &= \alpha_{T7} \cdot \frac{[\text{AbaR:AHL}]^n}{K_{d,\text{pAbaI}}^n + [\text{AbaR:AHL}]^n} + \beta_{T7} - \gamma_{T7}[\text{T7}] \\
 \frac{d[\text{PvdQ}]}{dt} &= \alpha_{PvdQ} \cdot \frac{[\text{T7}]^m}{K_{d,\text{pT7}}^m + [\text{T7}]^m} + \beta_{PvdQ} - \gamma_{PvdQ}[\text{PvdQ}]
 \end{aligned}$$

Where:

- $\alpha_{AbaR}$ : constitutive AbaR expression rate (set by a weak constitutive promoter)

- $k_{on}, k_{off}$ : binding/unbinding rate constants for AbaR and AHL
- $K_{d,pAbaI}$ : half-saturation constant for pAbal\* activation by AbaR:AHL
- $n$ : Hill coefficient reflecting pAbal\* cooperativity
- $\alpha_{T7}, \alpha_{PvdQ}$ : maximal transcription rates
- $\beta_{T7}, \beta_{PvdQ}$ : basal leak expression rates
- $\gamma_x$ : degradation rates (including dilution,  $\gamma_x = \delta_x + \mu$ , with  $\mu$  the growth rate)

## 2.4 Key Parameter Estimates

Parameter	Meaning	Estimate
$k_{on}$	AbaR–AHL binding rate	$10^6 \text{ M}^{-1}\text{s}^{-1}$
$k_{off}$	AbaR–AHL unbinding rate	$10^{-2} \text{ s}^{-1}$
$K_{d,pAbaI}$	pAbal* activation threshold	10–100 nM
$n$	Hill coefficient	1.5–2.5
$\alpha_{T7}$	maximal T7 RNAP expression rate	50 nM/min
$\gamma_{T7}$	T7 RNAP degradation rate	$0.02 \text{ min}^{-1}$
Amplification gain	T7 cascade	$> 100\times$

These values can be refined from the literature; the above are internet-based estimates.

## 2.5 Analysis Methods

1. **Steady-state analysis**: set derivatives to zero and solve for the dose–response  $[\text{PvdQ}]_{ss}$  vs.  $[\text{AHL}_{ext}]$
2. **Dynamic simulation**: under step input (sudden exposure to CRAB environment), compute response time  $t_{90}$  (time to reach 90% of steady state)
3. **Parameter scanning**: scan key parameters such as  $\alpha_{AbaR}, K_{d,pAbaI}, n$ , etc., and plot heatmaps to find optimal design space

## 3. Model 2: Bistability Analysis of the Positive Feedback Loop

### 3.1 Purpose

The positive feedback loop described in the design uses T7 RNAP to drive expression of an additional AbaR copy, forming a “self-amplifying” mechanism. This model aims to:

- Determine the **activation threshold**  $[\text{AHL}]_{on}$  and **maintenance threshold**  $[\text{AHL}]_{off}$
- Quantify the **hysteresis window**  $\Delta = [\text{AHL}]_{on} - [\text{AHL}]_{off}$
- Optimize the RBS strength of the extra AbaR copy to maximize  $\Delta$

### 3.2 Extended ODE

On top of Model 1, add a positive feedback term:

$$\frac{d[\text{AbaR}]}{dt} = \underbrace{\alpha_{\text{AbaR}}}_{\text{constitutive}} + \underbrace{\alpha_{\text{AbaR},fb} \cdot \frac{[\text{T7}]^m}{K_{d,\text{pT7,AbaR}}^m + [\text{T7}]^m}}_{\text{positive feedback (T7 drives extra AbaR)}} - \gamma_{\text{AbaR}}[\text{AbaR}] - k_{on}[\text{AbaR}][\text{AHL}_{int}] + k_{off}[\text{AbaR}:\text{AHL}]$$

Where  $\alpha_{\text{AbaR},fb}$  is the maximal expression rate of the extra AbaR driven by T7 via pT7, determined by the RBS strength of the extra AbaR copy.

### 3.3 Bistability Analysis Method

**Phase plane analysis:**

Define two key variables  $x_1 = [\text{AbaR}:\text{AHL}]$ ,  $x_2 = [\text{T7}]$ , and plot the nullclines:

$$\begin{aligned} \text{Nullcline 1: } & \frac{d[\text{AbaR}:\text{AHL}]}{dt} = 0 \\ \text{Nullcline 2: } & \frac{d[\text{T7}]}{dt} = 0 \end{aligned}$$

When the two nullclines intersect at **three points**, the system exhibits bistability (two stable states + one unstable saddle point).

### 3.4 RBS Optimization Strategy

Scan  $\alpha_{\text{AbaR},fb}$  (corresponding to different RBS strengths) to find the best value that:

$$\max \Delta = [\text{AHL}]_{on} - [\text{AHL}]_{off}$$

While satisfying the constraint:

$$\text{s.t. Metabolic Burden}([\text{AbaR}]_{ss,ON}) < \text{Tolerance Threshold}$$

Metabolic burden can be approximated by total protein expression flux:

$$\text{Burden} \propto \alpha_{\text{AbaR}} + \alpha_{\text{AbaR},fb} \cdot f([\text{T7}]) + \alpha_{\text{T7}} \cdot g([\text{AbaR}:\text{AHL}]) + \alpha_{\text{PvdQ}} \cdot h([\text{T7}])$$

### 3.5 Expected Outputs

- **S-shaped bifurcation diagram** showing the bistable interval
- **Hysteresis window vs. RBS strength** curve to guide RBS library screening
- **Noise robustness analysis** via Gillespie SSA to validate single-cell bistability stability

## 4. Model 3: PvdQ Enzyme Kinetics and AHL Degradation Model

### 4.1 Purpose

Quantify PvdQ degradation efficiency on 3-OH-C12-HSL and predict, at a given engineered bacterial density, the **time required to reduce AHL below the threshold**.

### 4.2 Enzyme Kinetics

As an acyl transferase, PvdQ follows Michaelis–Menten kinetics:

$$v = \frac{V_{max}[\text{AHL}]}{K_m + [\text{AHL}]}$$

Where:

- $V_{max} = k_{cat} \cdot [\text{PvdQ}]_{total}$
- $K_m$  (PvdQ for 3-OH-C12-HSL): reported  $\sim 1\text{--}10 \mu\text{M}$
- $k_{cat}$ :  $\sim 5\text{--}50 \text{ s}^{-1}$  (to be experimentally validated)

## 4.3 Environmental AHL Dynamics

Consider competition between continuous AHL production by CRAB and degradation by PvdQ:

$$\frac{d[\text{AHL}_{ext}]}{dt} = \underbrace{r_{AHL} \cdot N_{CRAB} \cdot f(\text{QS state})}_{\text{CRAB AHL production}} - \underbrace{\frac{k_{cat}[\text{PvdQ}]_{ext}[\text{AHL}_{ext}]}{K_m + [\text{AHL}_{ext}]}}_{\text{PvdQ degradation}} - \underbrace{\delta_{AHL}[\text{AHL}_{ext}]}_{\text{natural decay/diffusion}}$$

Where:

- $r_{AHL}$ : AHL production rate per CRAB cell
- $N_{CRAB}$ : CRAB cell density
- $f(\text{QS state})$ : regulatory function for AHL synthesis under QS positive feedback
- $[\text{PvdQ}]_{ext}$ : extracellular PvdQ concentration (depends on secretion efficiency)

## 4.4 Comparison of PvdQ Secretion Strategies

The design evaluates three secretion strategies (OmpA, PelB, HlyA). In the modeling framework, assign each a secretion efficiency  $\eta_{sec}$ :

$$\frac{d[\text{PvdQ}]_{ext}}{dt} = \eta_{sec} \cdot [\text{PvdQ}]_{int} \cdot N_{EcN} - \gamma_{PvdQ,ext} \cdot [\text{PvdQ}]_{ext}$$

Secretion system	Estimated $\eta_{sec}$ range	Features
OmpA (Sec pathway)	0.1–0.3	Requires signal peptide cleavage; possible folding delay
PelB (Sec pathway)	0.1–0.4	Better suited for periplasmic secretion
HlyA (Type I)	0.3–0.7	Direct transmembrane secretion; no periplasmic transport

Simulate AHL clearance time across different  $\eta_{sec}$  to guide experimental choice.

## 4.5 Expected Outputs

- **AHL concentration–time decay curves** under different EcN densities and PvdQ levels
- **Critical EcN density** required for effective quorum quenching
- **Secretion strategy comparison plots** of AHL clearance time

## 5. Model 4: PDE Model for Chemotactic Spatial Targeting

### 5.1 Purpose

Simulate directional migration of engineered bacteria under AHL gradients, quantify how **chemotaxis efficiency** affects bacterial enrichment near CRAB biofilms, and evaluate the targeting gain of the chimeric Tar–AbaR receptor.

### 5.2 Keller–Segel Chemotaxis Model

Use the classic Keller–Segel PDE model:

$$\begin{aligned}\frac{\partial b}{\partial t} &= \underbrace{D_b \nabla^2 b}_{\text{random diffusion}} - \underbrace{\nabla \cdot (\chi(c) b \nabla c)}_{\text{chemotactic migration}} + \underbrace{\mu_b b \left(1 - \frac{b}{b_{max}}\right)}_{\text{bacterial growth}} \\ \frac{\partial c}{\partial t} &= D_c \nabla^2 c + \underbrace{r_{AHL} \cdot \rho_{CRAB}(x)}_{\text{AHL release by CRAB}} - \underbrace{\frac{k_{cat} [\text{PvdQ}(b)] \cdot c}{K_m + c}}_{\text{AHL degradation by PvdQ}} - \delta_c c\end{aligned}$$

Where:

- $b(x, t)$ : engineered EcN density (cells/volume)
- $c(x, t)$ : AHL concentration
- $D_b$ : bacterial diffusion coefficient ( $\sim 10^{-6}$  cm<sup>2</sup>/s)
- $\chi(c)$ : chemotactic sensitivity function
- $D_c$ : AHL diffusion coefficient ( $\sim 5 \times 10^{-6}$  cm<sup>2</sup>/s)
- $\rho_{CRAB}(x)$ : spatial distribution of CRAB (high density in biofilm core)

### 5.3 Chemotactic Sensitivity Function

Based on receptor occupancy theory:

$$\chi(c) = \chi_0 \cdot \frac{K_d}{(K_d + c)^2}$$

Where:

- $\chi_0$ : maximal chemotactic sensitivity (related to chimeric receptor expression level)
- $K_d$ : dissociation constant of the chimeric Tar–AbaR receptor for 3-OH-C12-HSL

This function peaks at  $c = K_d$ , meaning chemotaxis is most sensitive at intermediate AHL concentrations—consistent with the design goal of enriching near the **biofilm edge** where gradients are steepest.

### 5.4 Geometry

Infection scenario	Geometry	Boundary conditions
Wound infection	2D plane (wound surface)	No-flux boundary (hydrogel confinement)
Lung infection	quasi-1D (radial from airway lumen to wall)	Airway wall biofilm as AHL source
Bloodstream infection	3D spherical symmetry (OMV delivery)	Spherical biofilm core

## 5.5 Simulation Comparison: No Chemotaxis vs Chemotaxis

Define the **Targeting Enrichment Factor (TEF)**:

$$\text{TEF} = \frac{\int_{\Omega_{biofilm}} b(x, t_{eq}) dx}{\int_{\Omega_{total}} b(x, t_{eq}) dx} \Big/ \frac{|\Omega_{biofilm}|}{|\Omega_{total}|}$$

TEF = 1 indicates uniform distribution; TEF  $\gg 1$  indicates effective enrichment near the biofilm.

## 5.6 Expected Outputs

- **Spatiotemporal heatmaps** of engineered bacterial density and AHL concentration
- **TEF vs time curves** comparing chemotaxis vs no chemotaxis
- **Chemotactic gain factor**: the fold increase of effective PvdQ concentration near biofilms

## 6. Model 5: Dynamic Model of CRAB Biofilms

### 6.1 Purpose

Build a QS-regulated biofilm growth–maturation–dissolution model linking QS signal concentration to biofilm state, to evaluate quorum-quenching treatment efficacy.

### 6.2 Framework

Divide CRAB into three subpopulations:

- $P$ : planktonic cells
- $B$ : biofilm-embedded cells
- $E$ : EPS matrix (extracellular polysaccharides, etc.)

$$\begin{aligned}\frac{dP}{dt} &= \mu_P P \left(1 - \frac{P}{P_{max}}\right) - \underbrace{k_{attach} \cdot f_{QS}(c) \cdot P}_{\text{QS-regulated attachment}} + \underbrace{k_{detach} \cdot B}_{\text{detachment to planktonic}} - \delta_P P \\ \frac{dB}{dt} &= k_{attach} \cdot f_{QS}(c) \cdot P + \mu_B B \left(1 - \frac{B}{B_{max}}\right) - k_{detach} \cdot B - \delta_B B \\ \frac{dE}{dt} &= \underbrace{r_E \cdot f_{QS}(c) \cdot B}_{\text{QS-regulated EPS synthesis}} - \underbrace{\delta_E \cdot E}_{\text{natural EPS degradation}}\end{aligned}$$

QS regulation function:

$$f_{QS}(c) = \frac{c^{n_{QS}}}{K_{QS}^{n_{QS}} + c^{n_{QS}}}$$

When PvdQ lowers environmental AHL  $c$ ,  $f_{QS}(c) \rightarrow 0$ , leading to:

- reduced attachment of planktonic cells into biofilms
- reduced EPS synthesis
- collapse of biofilm steady state

## 6.3 Relationship Between Resistance and Biofilms

Model the biofilm-enhanced antibiotic resistance factor as:

$$\text{MIC}_{\text{effective}} = \text{MIC}_{\text{planktonic}} \cdot \left( 1 + \phi \cdot \frac{E}{E + K_E} \right)$$

Where  $\phi$  is the maximal enhancement factor (10–1000× per the design), and  $K_E$  is the EPS half-saturation constant.

## 6.4 Expected Outputs

- **Biofilm growth curves:**  $B(t)$  with vs without quorum quenching
- **Combination therapy predictions:** quorum quenching + antibiotics killing efficiency
- **Therapeutic window:** required PvdQ level to reduce MIC to clinically achievable range

## 7. Model 6: Competitive-Substrate Kinetic Model for the Visualization Module

### 7.1 Purpose

All three visualization strategies rely on **PvdQ's competitive substrate preference** between natural AHL and artificial probes. This model quantifies competition and predicts the **critical AHL concentration** and **time window** for color change.

### 7.2 Competitive Michaelis–Menten Kinetics

PvdQ faces two substrates simultaneously (natural AHL and artificial Probe):

$$v_{AHL} = \frac{k_{cat,AHL} \cdot [\text{PvdQ}] \cdot [\text{AHL}]}{K_{m,AHL} \left( 1 + \frac{[\text{Probe}]}{K_{m,Probe}} \right) + [\text{AHL}]}$$
$$v_{Probe} = \frac{k_{cat,Probe} \cdot [\text{PvdQ}] \cdot [\text{Probe}]}{K_{m,Probe} \left( 1 + \frac{[\text{AHL}]}{K_{m,AHL}} \right) + [\text{Probe}]}$$

**Key design principle:**  $K_{m,AHL} \ll K_{m,Probe}$  (PvdQ has much higher affinity for native AHL), therefore:

- At high AHL:  $v_{AHL} \gg v_{Probe}$ , probe remains intact → colorless
- At low AHL:  $v_{Probe}$  increases significantly → dye release

### 7.3 Scenario-Specific Parameters

Scenario	Probe type	Pigment product	Readout
Wound	BpsA substrate (glutamine) + cl regulatory switch	Indigoidine	Dressing turns blue
Lung	Sulfonated indoxyl probe	Indigo Carmine	Blue sputum
Bloodstream	PEG-shielded prodrug probe	Resorufin	Red urine

**Wound specialization:** includes cl repressor regulation; couple cl degradation dynamics:

$$\frac{d[\text{cI}]}{dt} = \alpha_{cI} \cdot \frac{[\text{AbaR:AHL}]^n}{K_d^n + [\text{AbaR:AHL}]^n} - \underbrace{(\gamma_{cI} + \gamma_{ssrA})}_{\text{intrinsic + ssrA-tag accelerated degradation}} \cdot [\text{cI}]$$

BpsA expression repressed by cI:

$$\frac{d[\text{BpsA}]}{dt} = \alpha_{BpsA} \cdot \frac{K_{R,cI}^{n_R}}{K_{R,cI}^{n_R} + [\text{cI}]^{n_R}} - \gamma_{BpsA}[\text{BpsA}]$$

**Bloodstream specialization:** PEG shielding removal is cleaved by CRAB biofilm-associated enzyme CpaA:

$$\frac{d[\text{Probe}_{active}]}{dt} = k_{CpaA} \cdot [\text{CpaA}] \cdot [\text{Probe}_{PEG}] - v_{Probe}$$

## 7.4 Expected Outputs

- **AHL vs pigment output dose-response curves** to determine the “color-change threshold”
- **Treatment timeline:** quantify time delay from AHL decrease to color-change trigger
- **Effect of cI ssrA tag on response speed:** parameter scan of ssrA degradation rate in the wound scenario

# 8. Model 7: Timed Clearance Model for the MazEF Kill Switch

## 8.1 Purpose

Predict the kill switch **timed clearance window** (time to arabinose depletion) and **emergency clearance response time** (kill rate after doxycycline induction), ensuring engineered bacteria survive during therapy and die completely afterward.

## 8.2 ODE Model

**Arabinose metabolism:**

$$\frac{d[\text{Ara}]}{dt} = -\frac{V_{max,Ara} \cdot [\text{Ara}]}{K_{m,Ara} + [\text{Ara}]} \cdot N_{EcN}$$

**MazE (antitoxin) expression:**

$$\frac{d[\text{MazE}]}{dt} = \alpha_{MazE} \cdot \frac{[\text{Ara}]^{n_A}}{K_{Ara}^{n_A} + [\text{Ara}]^{n_A}} - \gamma_{MazE}[\text{MazE}] - k_{bind}[\text{MazE}][\text{MazF}]$$

**MazF (toxin) expression:**

$$\frac{d[\text{MazF}]}{dt} = \underbrace{\alpha_{MazF,const}}_{\text{weak constitutive}} + \underbrace{\alpha_{MazF,Dox} \cdot \frac{[\text{Dox}]^{n_D}}{K_{Dox}^{n_D} + [\text{Dox}]^{n_D}}}_{\text{doxycycline induction}} - \gamma_{MazF}[\text{MazF}] - k_{bind}[\text{MazE}][\text{MazF}]$$

**MazEF complex (inactive):**

$$\frac{d[\text{MazE:MazF}]}{dt} = k_{bind}[\text{MazE}][\text{MazF}] - \gamma_{EF}[\text{MazE:MazF}]$$

**Cell survival:**

$$\frac{dS}{dt} = -k_{kill} \cdot \max ([\text{MazF}]_{free} - [\text{MazF}]_{threshold}, 0) \cdot S$$

Where  $[\text{MazF}]_{free} = [\text{MazF}] - [\text{MazE}:\text{MazF}]$  (killing is triggered when free MazF exceeds the threshold).

## 8.3 Key Design Parameters

Parameter	Design requirement	Constraint source
Initial $[\text{Ara}]_0$	premixed concentration in hydrogel	ensure sufficient MazE during therapy (e.g., 24 h)
$\gamma_{\text{MazE}}$	MazE is naturally unstable	MazE half-life $\sim 30$ min (literature)
$\gamma_{\text{MazF}}$	MazF is more stable	MazF half-life $\sim 2\text{--}4$ h
$\alpha_{\text{MazF},const}$	weak constitutive “baseline toxin”	cannot be too high to avoid premature killing
RBS strength (MazE)	mentioned as optimization target	ensure $\text{MazE} > \text{MazF}$ under normal conditions

## 8.4 Simulation Scenarios

### Scenario A: automatic timed clearance

- Initial: sufficient  $[\text{Ara}]_0$ ,  $[\text{Dox}] = 0$
- As time progresses, arabinose is metabolized
- Plot:  $[\text{Ara}](t)$ ,  $[\text{MazE}](t)$ ,  $[\text{MazF}]_{free}(t)$ ,  $S(t)$
- **Key outputs:** survival window  $T_{survival}$  and killing half-life  $t_{1/2,kill}$

### Scenario B: emergency doxycycline clearance

- Add doxycycline at  $t = t_{emergency}$
- MazF rapidly upregulates and overwhelms residual MazE
- **Key output:** time from dosing to 99% killing  $T_{99\%}$

### Scenario C: parameter robustness

- Scan  $[\text{Ara}]_0$  and  $\alpha_{\text{MazE}}$  (RBS strength)
- Plot “safe operating space” heatmap: x-axis survival window, y-axis killing reliability

## 8.5 Expected Outputs

- **Arabinose decay curve** and corresponding **cell survival** trajectory
- **Safe operating space plot** to guide hydrogel arabinose premix concentration
- **Emergency clearance time** to validate doxycycline override response speed

## 9. Model 8: pH-Sensitive Liposome Pulmonary Drug Release Model

### 9.1 Purpose

The design states that pH-sensitive liposomes (CHEMS/DOPE) remain stable in healthy lung tissue (pH 7.0–7.4) but rapidly destabilize and release drug in the acidic microenvironment of CRAB infection sites (pH 5.5–6.5). This model quantifies the **pH-**

dependent release rate.

## 9.2 Model Equations

Liposome membrane stability vs pH:

CHEMS protonation determines membrane stability. Let liposome integrity be  $I(t) \in [0, 1]$ :

$$\frac{dI}{dt} = -k_{release}(\text{pH}) \cdot I$$

Model the pH dependence of  $k_{release}$  as a sigmoidal function:

$$k_{release}(\text{pH}) = k_{max} \cdot \frac{1}{1 + 10^{n_{pH}(\text{pH} - \text{pH}_{crit})}}$$

- $\text{pH}_{crit}$ : critical pH (~6.0–6.5, near CHEMS pKa)
- $n_{pH}$ : transition steepness
- $k_{max}$ : maximal release rate constant

PvdQ release dynamics:

$$\frac{d[\text{PvdQ}]_{released}}{dt} = k_{release}(\text{pH}) \cdot I(t) \cdot [\text{PvdQ}]_{encap,0}$$

## 9.3 Spatial Distribution Model

Combine lung anatomy with a 1D reaction–diffusion model (from airway center to wall):

$$\frac{\partial [\text{PvdQ}]}{\partial t} = D_{PvdQ} \frac{\partial^2 [\text{PvdQ}]}{\partial r^2} + \text{Source}(r, \text{pH}(r))$$

Where  $\text{pH}(r)$  is acidic near CRAB biofilms (inner layer) and gradually returns to neutral toward the airway lumen.

## 9.4 Expected Outputs

- **pH-release curves**: PvdQ release time course at different pH values
- **Therapeutic efficiency comparison**: pH-sensitive vs conventional liposomes in healthy vs infected tissue (selective release ratio)
- Recommendations for optimal liposome composition parameters

# 10. Model 9: Diffusion Model for Core–Shell Microcarriers in Wound Hydrogels

## 10.1 Purpose

The dual-layer hydrogel system must ensure:

1. External AHL can **diffuse in** to the core–shell microcarrier and trigger the gene circuit
2. Produced PvdQ and pigments can **diffuse out** to function
3. Engineered bacteria ( $1\text{--}2 \mu\text{m}$ ) are **physically retained** and cannot escape

This model quantifies mass transfer in the core–shell structure.

## 10.2 Modeling Framework

**Spherically symmetric diffusion model** (three-layer structure):

$$\frac{\partial C_i}{\partial t} = \frac{1}{r^2} \frac{\partial}{\partial r} \left( D_{i,j} \cdot r^2 \frac{\partial C_i}{\partial r} \right) + R_i(r)$$

Where  $i$  denotes different species (AHL, PvdQ, pigment), and  $j$  denotes different regions:

Region	Radius range	Diffusion coefficient	Reaction term
Core (Ca-alginate + EcN)	$0 < r < R_{core}$	$D_{i,core}$	gene circuit expression
Shell (QCS-alginate PEC)	$R_{core} < r < R_{shell}$	$D_{i,shell}$ (dense membrane; low permeability for macromolecules)	none
External hydrogel matrix	$r > R_{shell}$	$D_{i,gel}$	none

### Size selectivity:

Model the effective MWCO of the PEC shell via:

$$D_{i,shell} = D_{i,0} \cdot \exp \left( -\lambda \cdot \frac{R_{H,i}}{R_{pore}} \right)$$

- $R_{H,i}$ : hydrodynamic radius of species  $i$
- $R_{pore}$ : pore size of the PEC membrane
- AHL ( $M_W \approx 300$  Da,  $R_H \sim 0.5$  nm) → passes freely
- PvdQ ( $M_W \approx 80$  kDa,  $R_H \sim 3$  nm) → passes slowly (needs validation for sufficient diffusion)
- EcN ( $\sim 1-2$   $\mu\text{m}$ ) → fully retained

## 10.3 Expected Outputs

- **AHL penetration time** from outside to core to ensure sensing is not overly delayed
- **PvdQ release kinetics** from core to outside to evaluate onset of therapeutic action
- **Bacterial escape risk assessment**: quantitative validation of PEC membrane retention for micron-scale particles

## Key Performance Indicators (KPIs)

KPI	Definition	Target
<b>Sensing sensitivity</b>	minimum $[\text{AHL}_{ext}]$ to trigger the system	< 100 nM
<b>Response time <math>t_{90}</math></b>	time for PvdQ to reach 90% steady state	< 2 h
<b>AHL clearance time <math>t_{clear}</math></b>	time for AHL to drop below QS threshold	< 6 h
<b>Hysteresis window <math>\Delta</math></b>	difference between maintenance and activation thresholds	> 50 nM

KPI	Definition	Target
<b>Targeting enrichment factor TEF</b>	local concentration enhancement due to chemotaxis	> 5×
<b>Color-change delay</b>	time from treatment completion to color change	< 1 h
<b>Self-destruction window <math>T_{survival}</math></b>	engineered bacteria survival time	24–72 h (tunable)
<b>Emergency clearance time <math>T_{99\%}</math></b>	time to 99% killing after Dox	< 4 h