



General Linear Model for fMRI: bases of statistical analyses

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Objectives

- Intuitive understanding of the GLM
- Get an idea how t-tests, ANOVA, regressions, etc .. are instantiation of the GLM
- Learn key concepts: linearity, model, design matrix, collinearity and orthogonalization

Overview

- What is linearity?
- Why do we speak of models?
- A simple fMRI model
- A more complex model
- Issues with regressors

What is linearity?

Linearity

- Means created by lines
- In maths it refers to equations or functions that satisfy 2 properties: additivity (also called superposition) and homogeneity of degree 1 (also called scaling)
- Additivity $\rightarrow y = x_1 + x_2$ (output is sum of inputs)
- Scaling $\rightarrow y = \beta x_1$ (output is proportional to input)

Examples of linearity / non linearity

`X = sort(randn(10,1))`

- Linear correlation

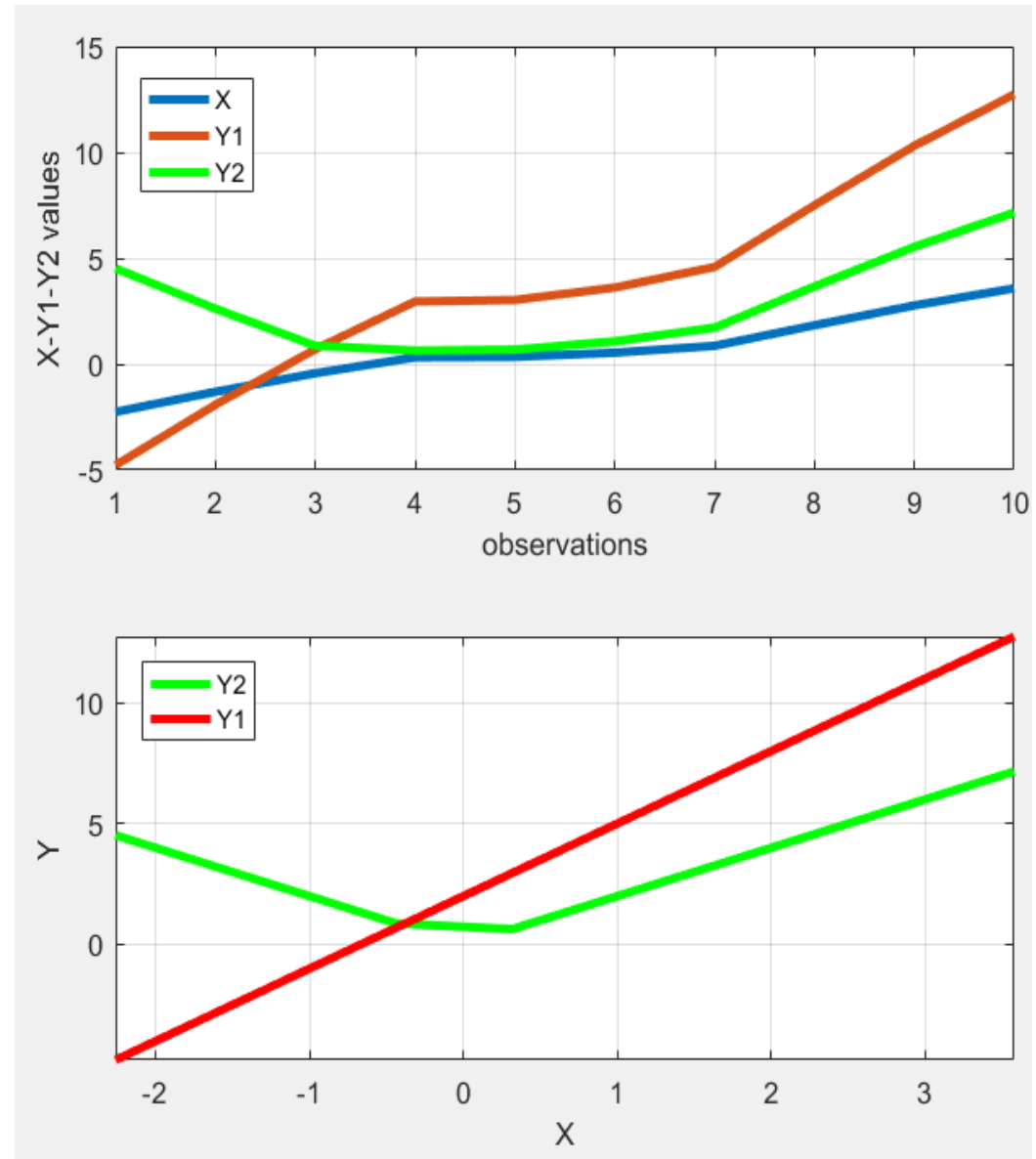
$$Y1 = 3 * X + 2$$

Pearson $r = 1$

- Non linear correlation

$$Y2 = \text{abs}(2 * X)$$

Pearson $r = 0.5$



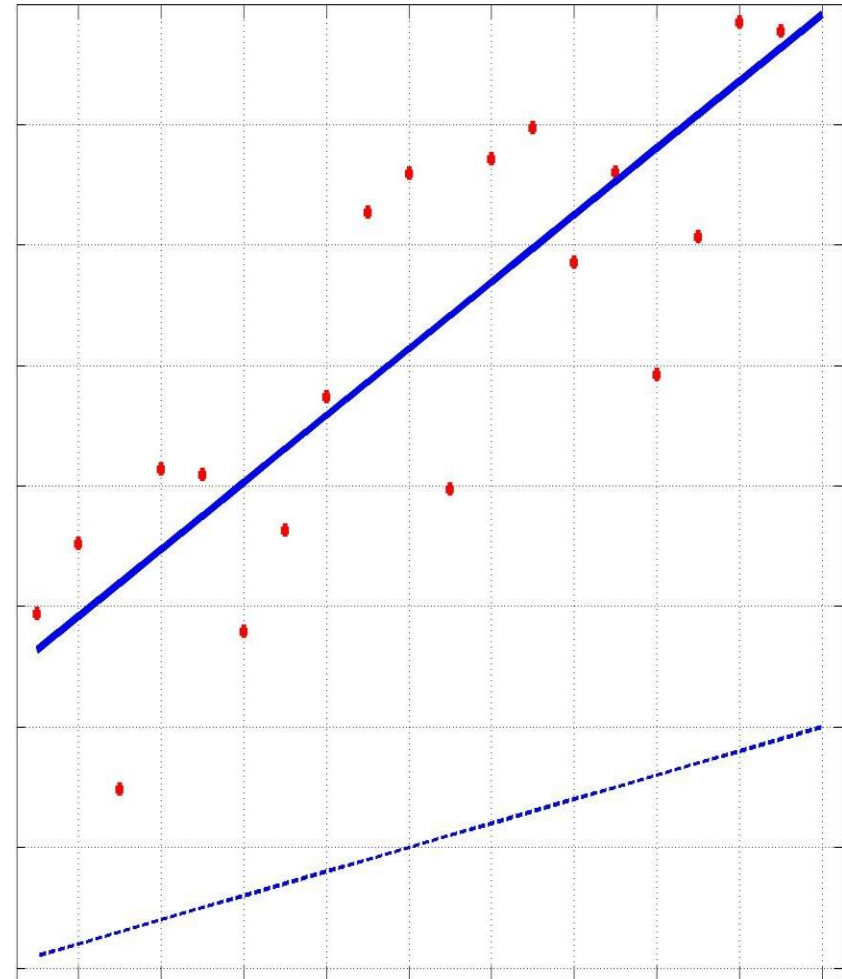
What is a linear model?

What is a linear model?

- An equation or a set of equations that models data and which corresponds geometrically to straight lines, plans, hyperplans and satisfy the properties of additivity and scaling.
- Simple regression: $y = \beta_1 x_1 + \beta_2 + \varepsilon$
- Multiple regression: $y = \beta_1 x_1 + \beta_2 x_2 + \beta_3 + \varepsilon$
- One way ANOVA: $y = \mu + \alpha_i + \varepsilon$
- Repeated measure ANOVA: $y = u + S_i + \alpha_i + \varepsilon$
- ...

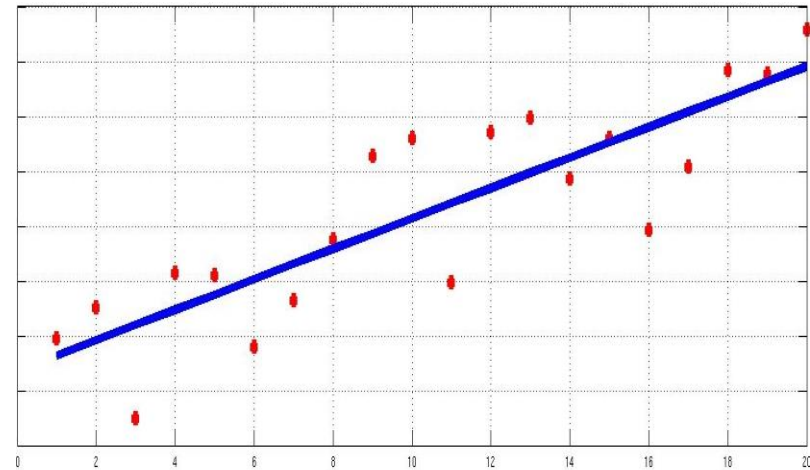
A regression is a linear model

- We have an experimental measure x (e.g. stimulus intensity from 0 to 20)
- We then do the expe and collect data y (e.g. RTs)
- Model: $y = \beta_1 x + \beta_2$
- Do some maths / run a software to find β_1 and β_2
 $\hat{y} = 2.7x + 23.6$

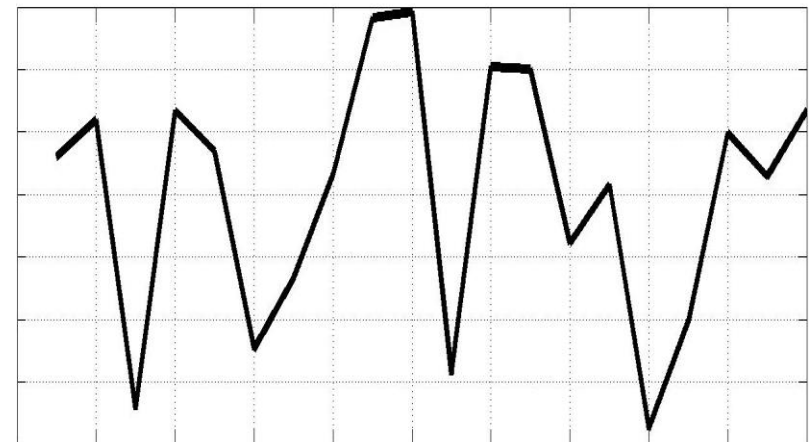


A regression is a linear model

- The error is the distance between the data and the model
- $F = (SS_{\text{effect}} / df) / (SS_{\text{error}} / df_{\text{error}})$
- $SS_{\text{effect}} = \text{norm}(\text{model} - \text{mean}(\text{model}))^2;$
- $SS_{\text{error}} = \text{norm}(\text{residuals})^2;$

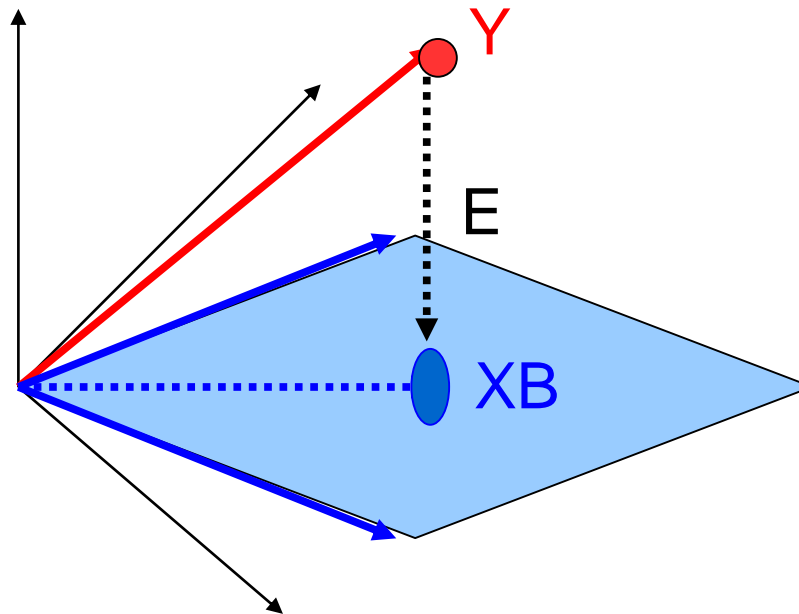


$$\text{Error} = Y - XB$$



Summary

- Linear model: $y = x_1\beta_1 + x_2\beta_2$ (output = additivity and scaling of input)

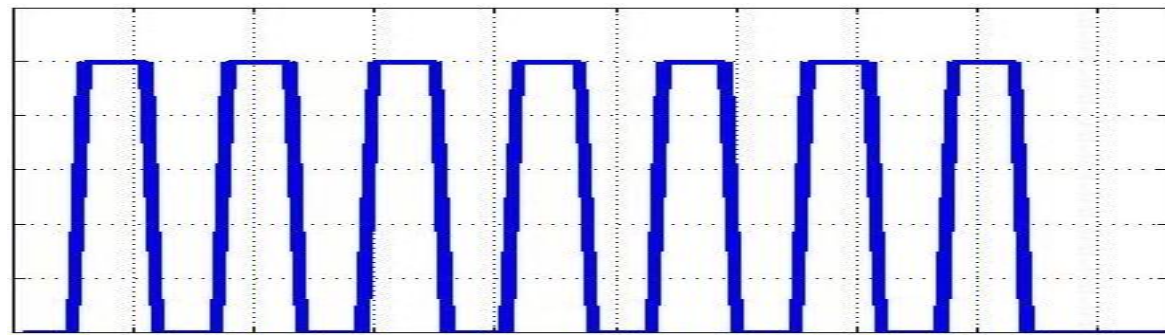


A simple fMRI model

<http://www.fil.ion.ucl.ac.uk/spm/data/auditory/>

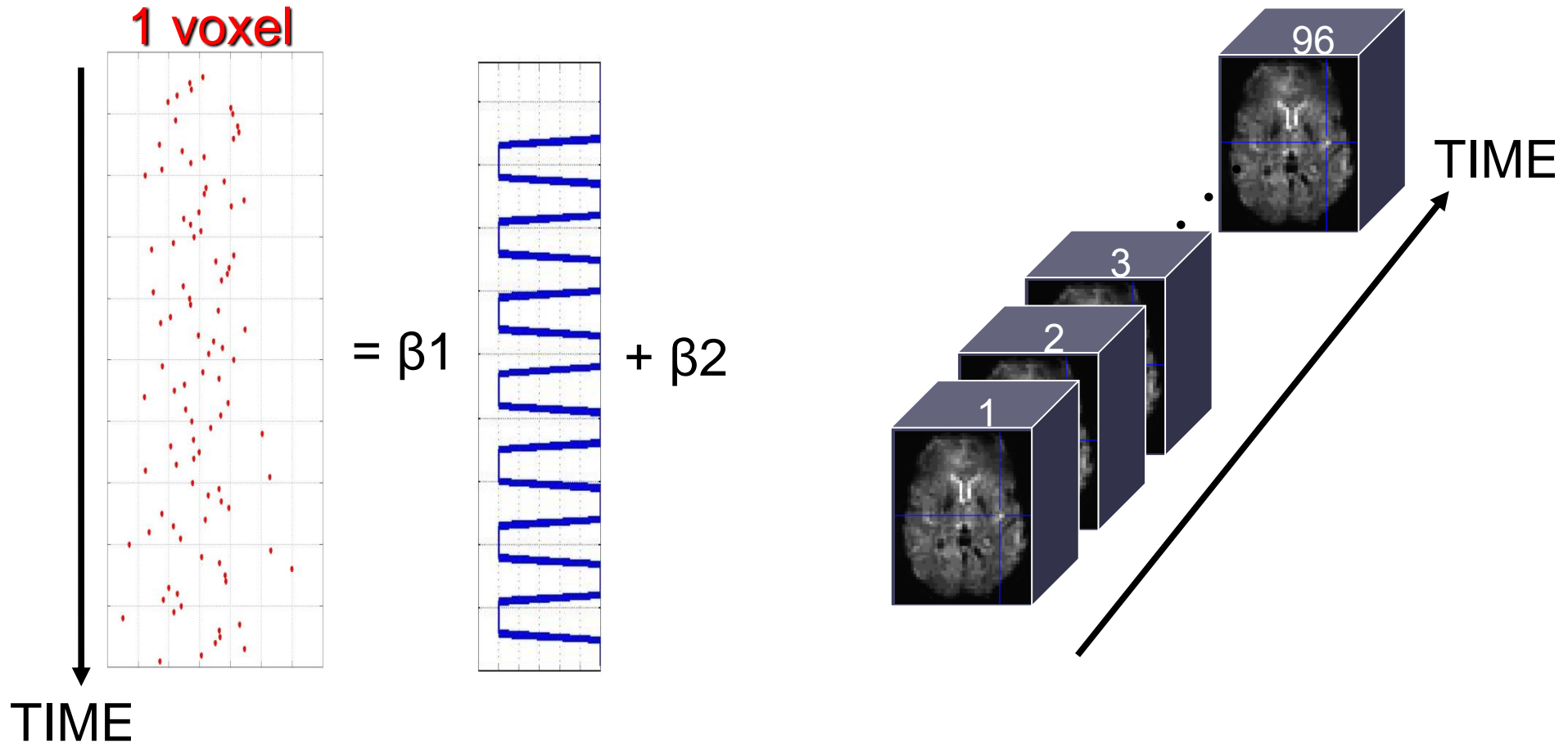
FMRI experiment

- *SPM auditory data set*: which areas are activated by the presentation of bi-syllabic words presented binaurally (60 per minute)
- Experimental measure **x**: 7 blocks of 42 sec of stimulation

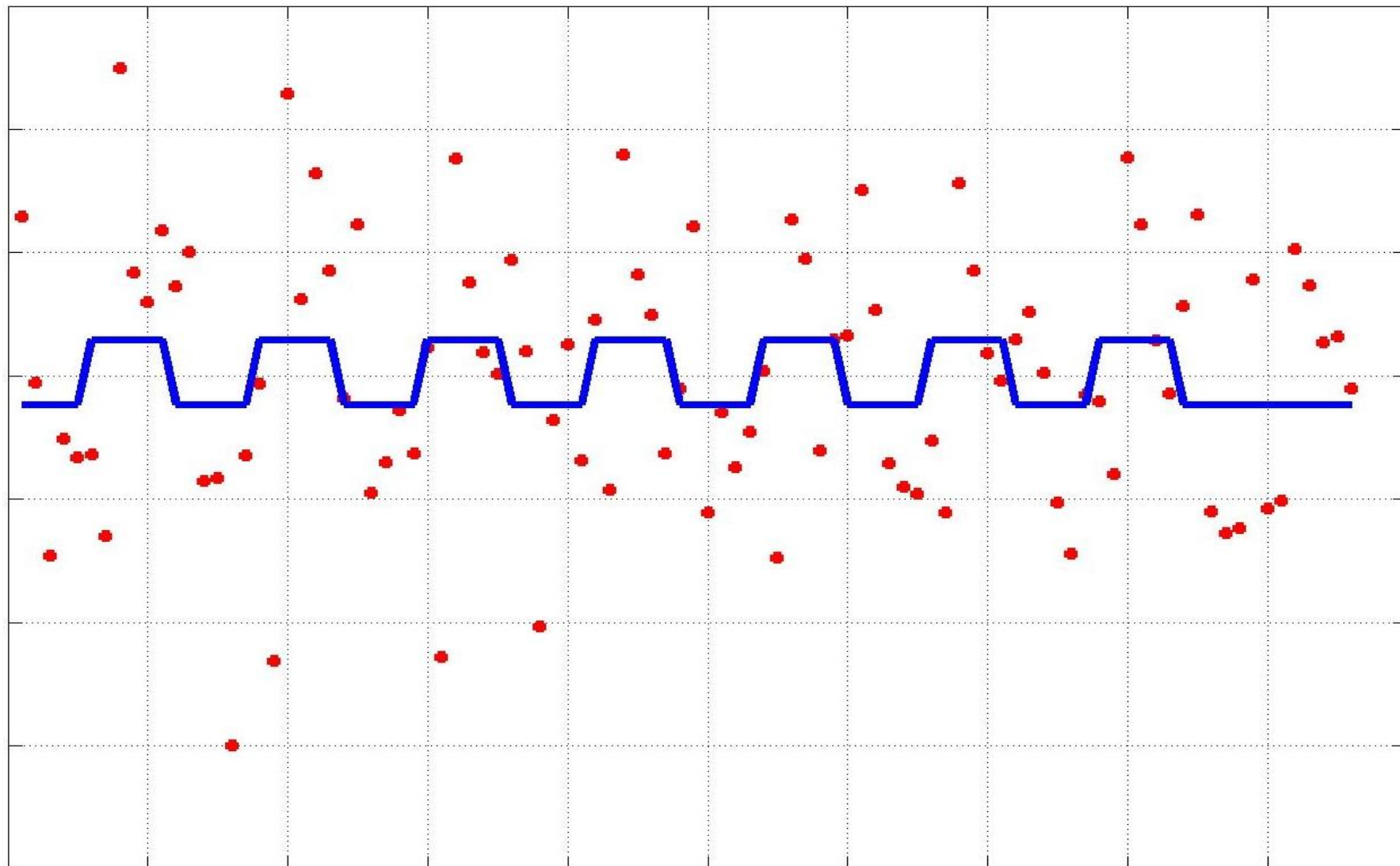


FMRI experiment

- Collect the data : 96 fMRI volumes (TR=7s)
- Model: $y = \beta_1 x + \beta_2$

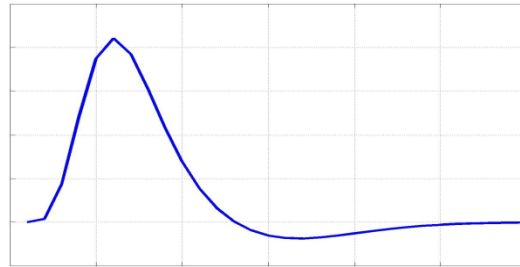


FMRI experiment

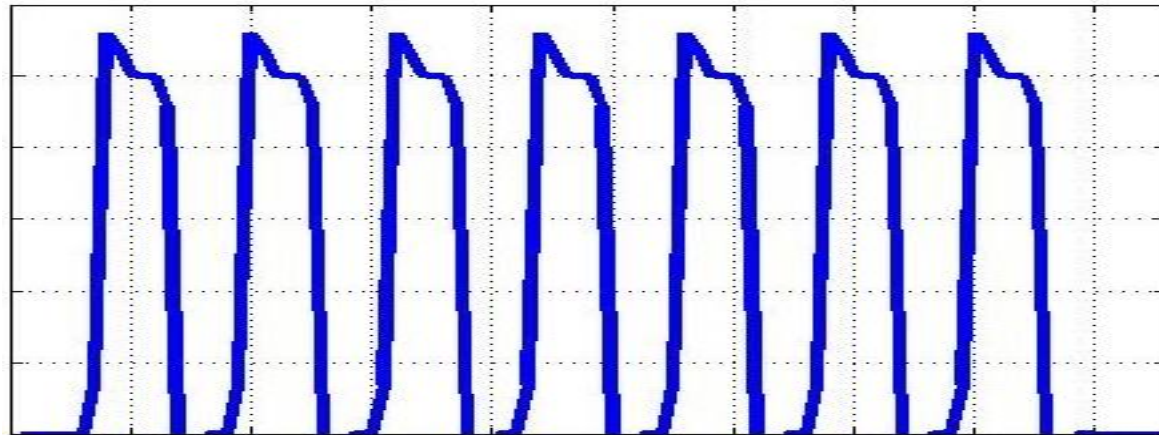


FMRI experiment

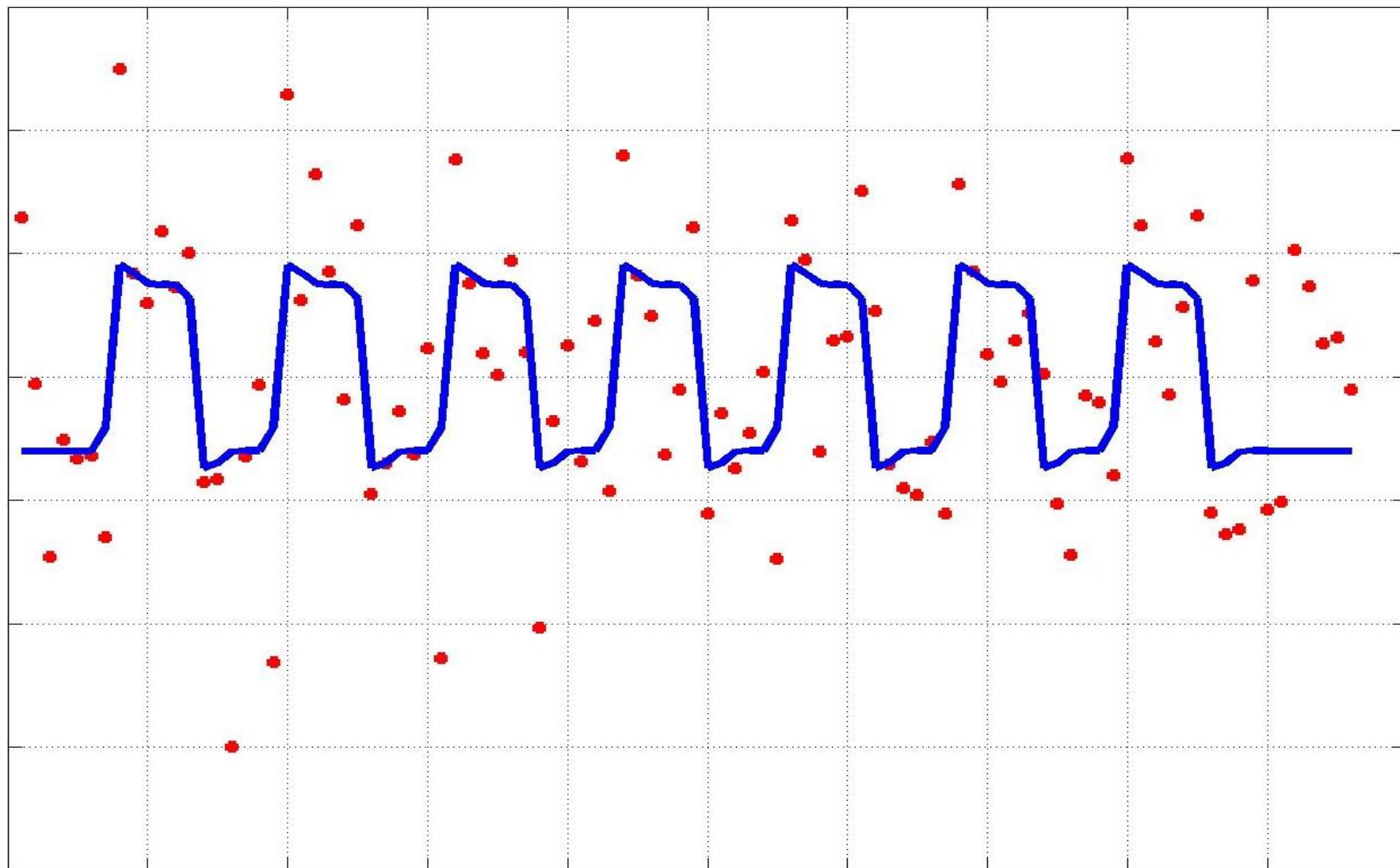
- A better model: we know the shape of the BOLD response



- Convolution by the hrf: $x \otimes \text{hrf}$



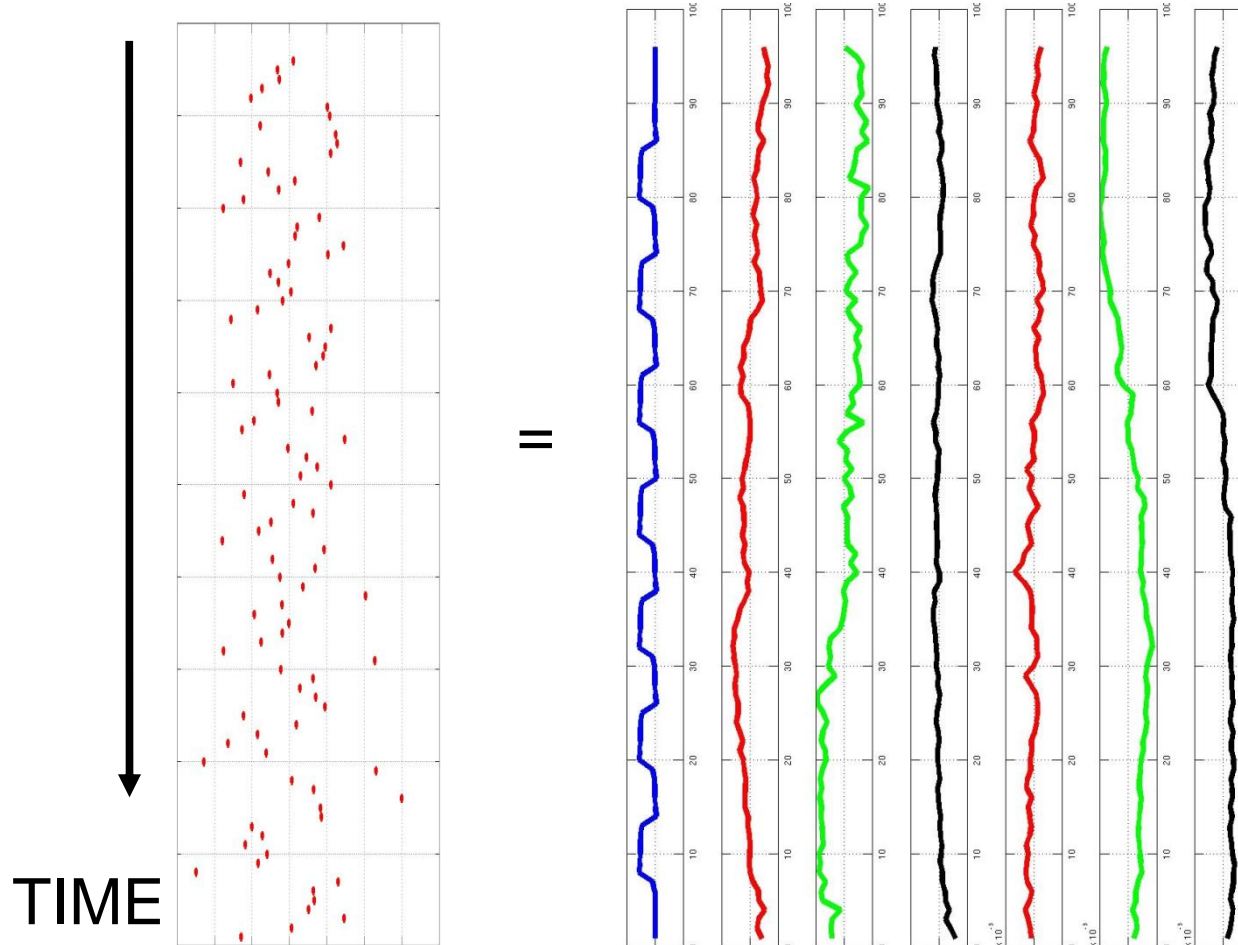
FMRI experiment



FMRI experiment

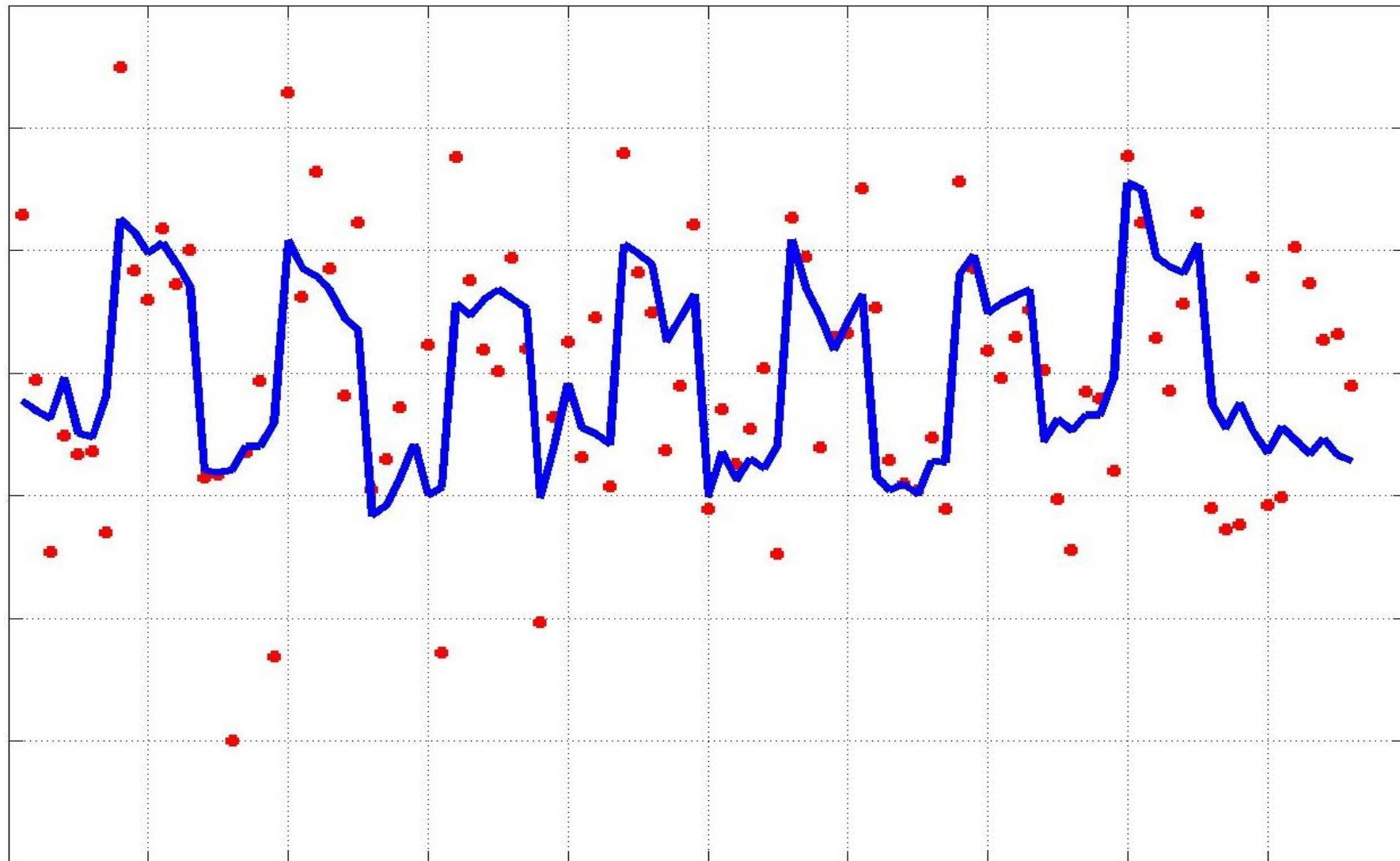
- An even better model: add motion parameters

1 voxel



$$* [\beta_1 \ \beta_2 \ \beta_3 \ \beta_4 \ \beta_5 \ \beta_6 \ \beta_7 \ \beta_8] + \beta_8$$

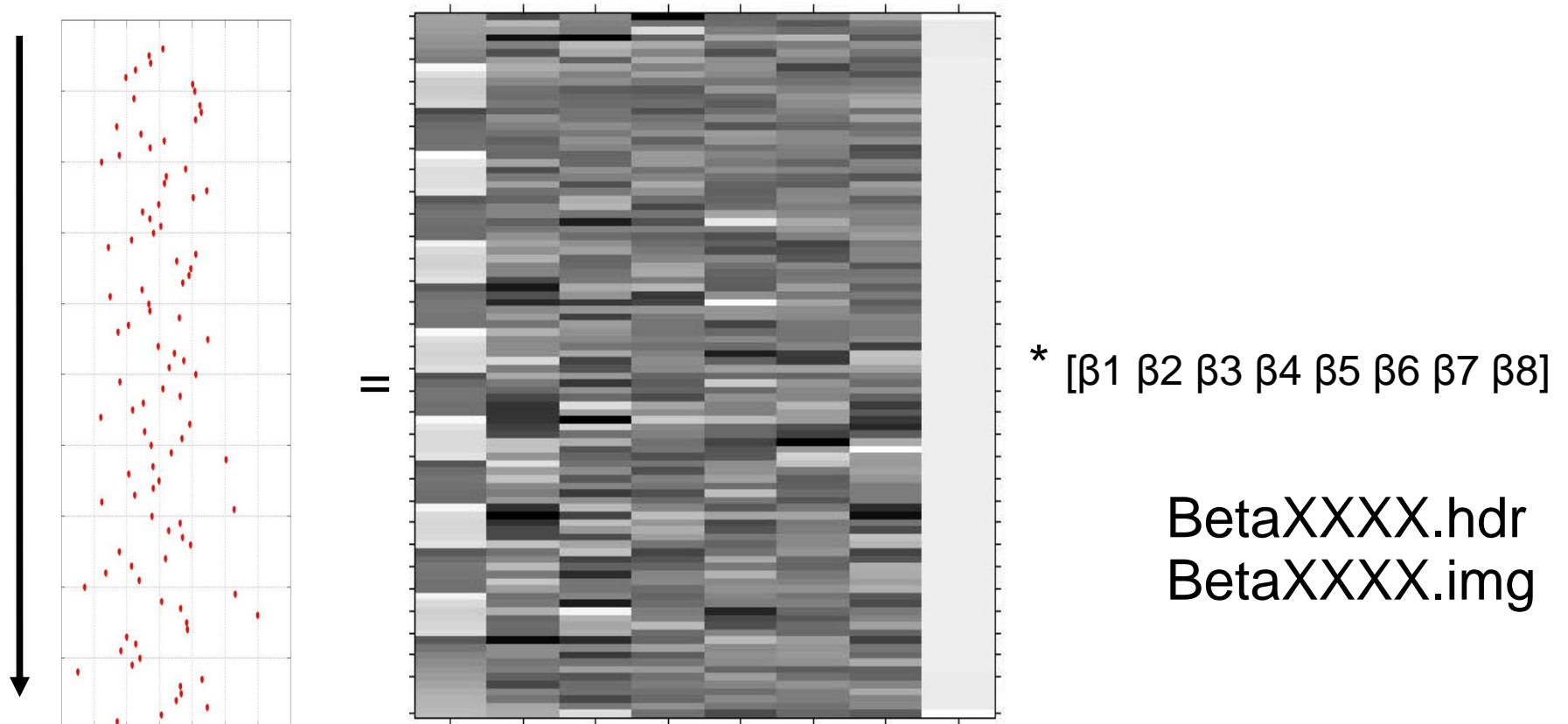
FMRI experiment



FMRI experiment

- Matrix formulation and SPM colour coding

1 voxel



$$\text{FMRI data (Y)} = \text{Design matrix (X = SPM.mat)} * B + E \text{ (ResMS)}$$

Noise modelling

- GLM: $Y = XB + E$ with $E \sim N(0, V)$
- Because of scanner issue, data often have a drift, that we can incorporate into the model X (high pass filter)
- V is the covariance matrix whose depends on your model – in SPM we use an AR(1) model + white noise to remove dependencies related to physiological artefacts (e.g. cardiac aliasing) and model residual noise

FMRI experiment

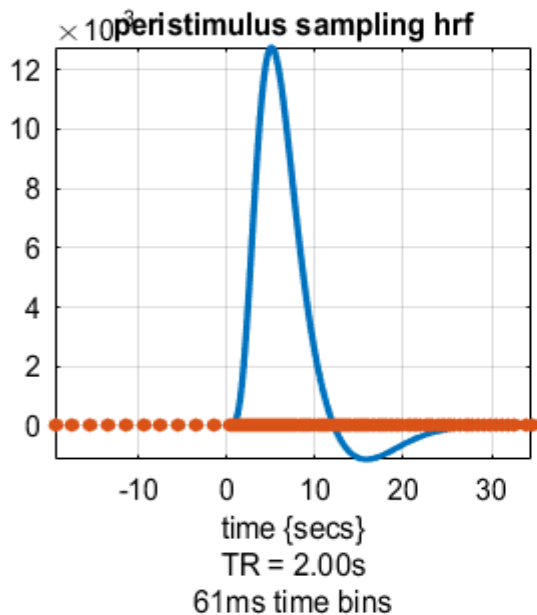
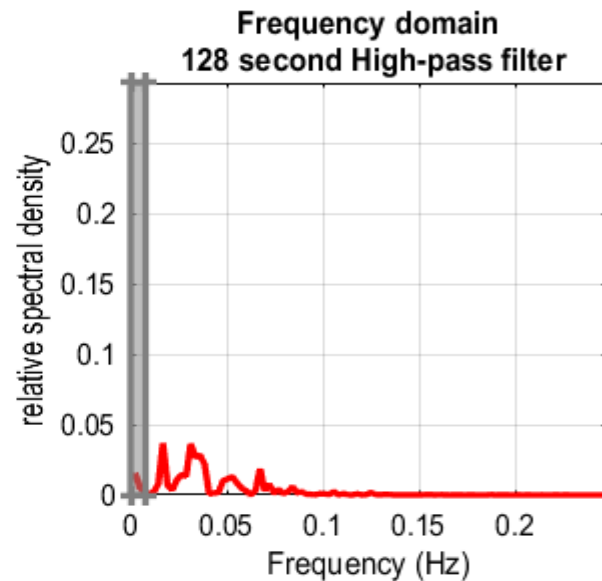
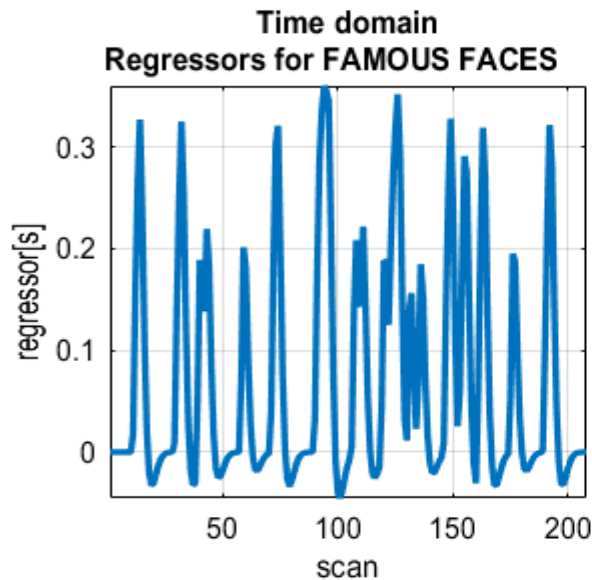
Current Module: fMRI model specification

Timing parameters	
. Units for design	<-X
. Interscan interval	<-X
. Microtime resolution	16
. Microtime onset	8
Data & Design	
. Subject/Session	
. . Scans	<-X
. . Conditions	
. . Multiple conditions	
. . Regressors	
. . Multiple regressors	
. . High-pass filter	128
Factorial design	
Basis Functions	
. Canonical HRF	
. . Model derivatives	No derivatives
Model Interactions (Volterra)	Do not model Interactions
Global normalisation	None
Masking threshold	0.8
Explicit mask	
Serial correlations	AR(1)

Current Item: Data & Design

Note: High pass filter in seconds $1/128 \text{ sec} = 0.007 \text{ Hz}$
The hrf itself peaks at $\sim 0.04 \text{ Hz}$

When you specify a design you can check it !



What should be your filter?

- the old rule of thumb (a la SPM99) is to take the highest freq (longest periods between repeats) and multiply by 2 (to have a filter away from your peak) – ideally toward high frequencies
- Because noise is low frequency – e.g. resting is 0.01 Hz - 0.1Hz \rightarrow 100sec / 10sec \rightarrow can't really get much lower than the 128 sec (0.007Hz)

Summary

- Linear model: $y = \beta_1 x_1 + \beta_2 x_2$ (output = additivity and scaling of input)
- GLM: $Y = XB + E$ (matrix formulation, works for any statistics, express the data Y as a function of the design matrix X)

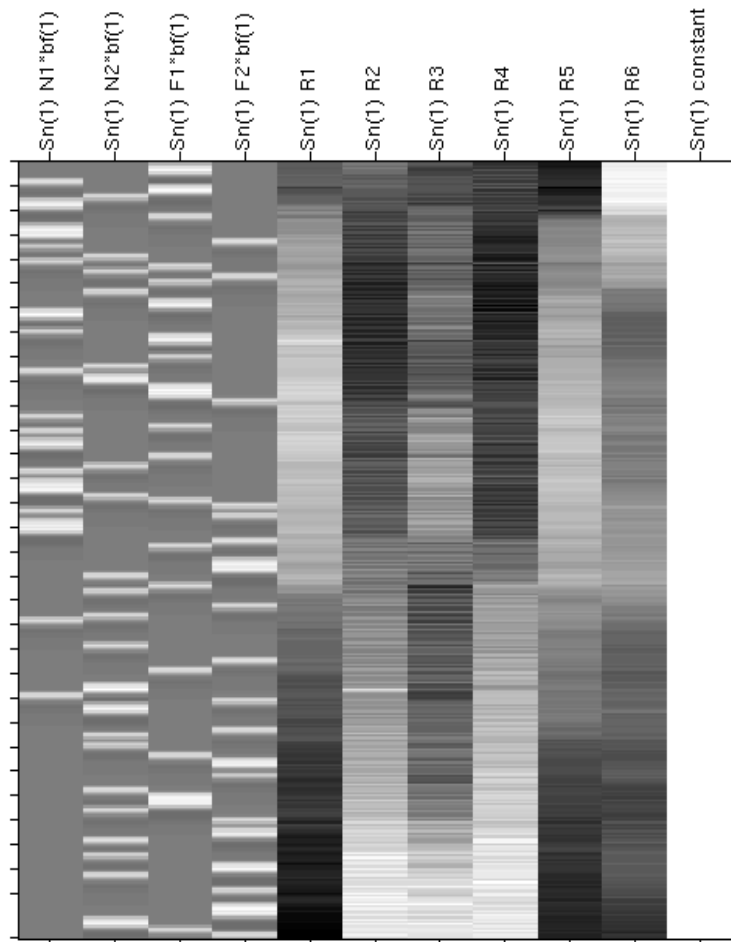
A more complex model

2 x 2 factorial design

- New experiment: (Famous vs. Nonfamous) x (1st vs 2nd presentation) of faces against baseline of chequerboard
- 2 presentations of 26 Famous and 26 Nonfamous Greyscale photographs, for 0.5s, randomly intermixed, for fame judgment task (one of two right finger key presses).

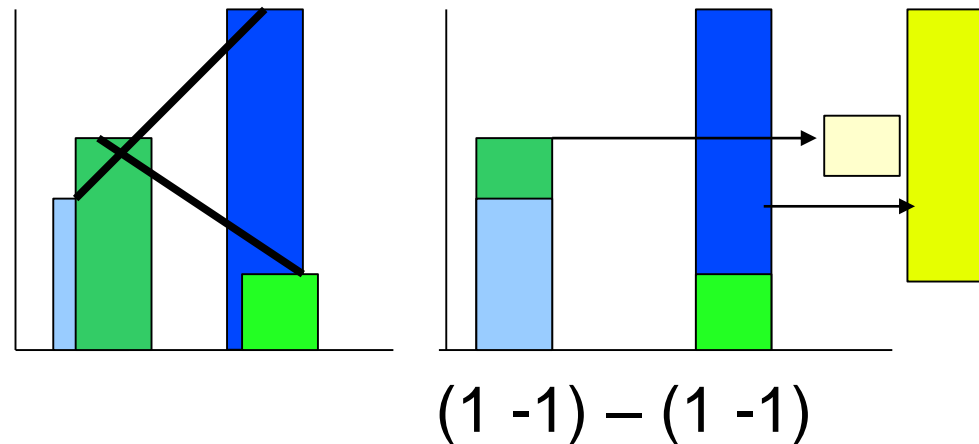
Contrasts (more tomorrow)

- SPM design matrix

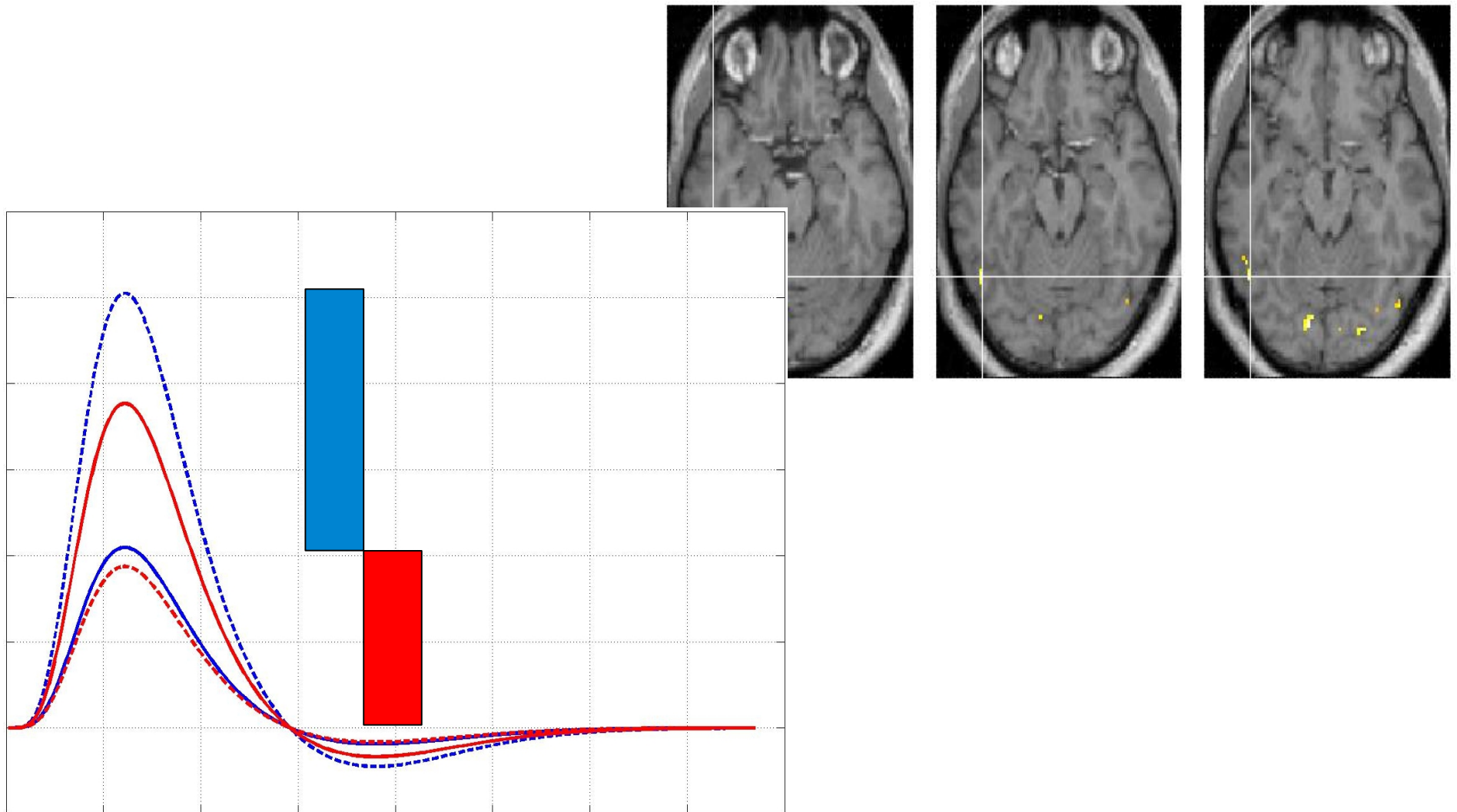


Use contrasts

- Main effects
- Fame: $[1 \ 1 \ -1 \ -1 \ 0 \ 0 \ \dots]$
- Rep: $[1 \ -1 \ 1 \ -1 \ 0 \ 0 \ \dots]$
- Interaction $[1 \ -1 \ -1 \ 1 \ 0 \ 0 \ \dots]$

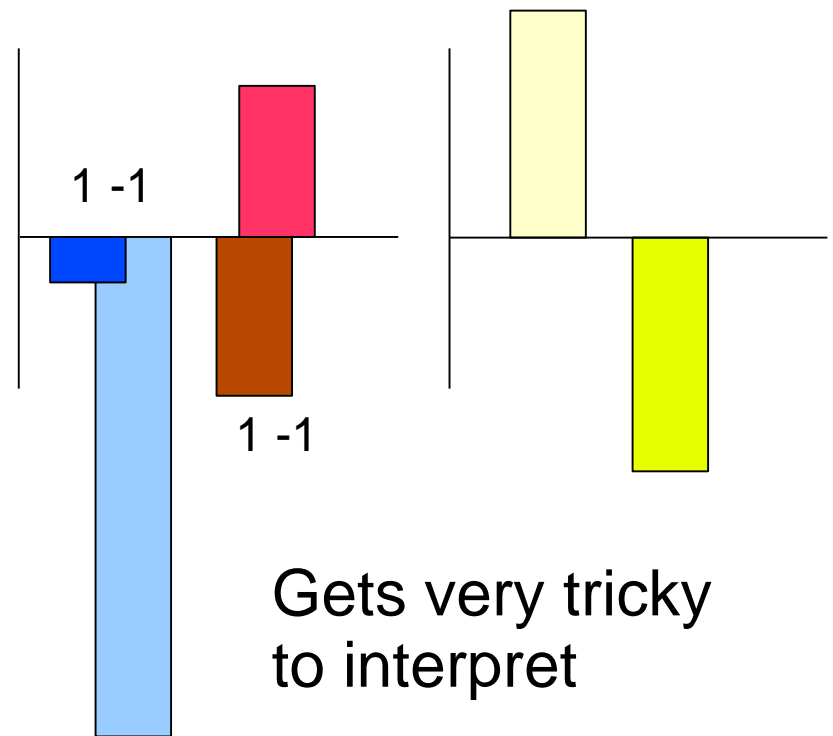
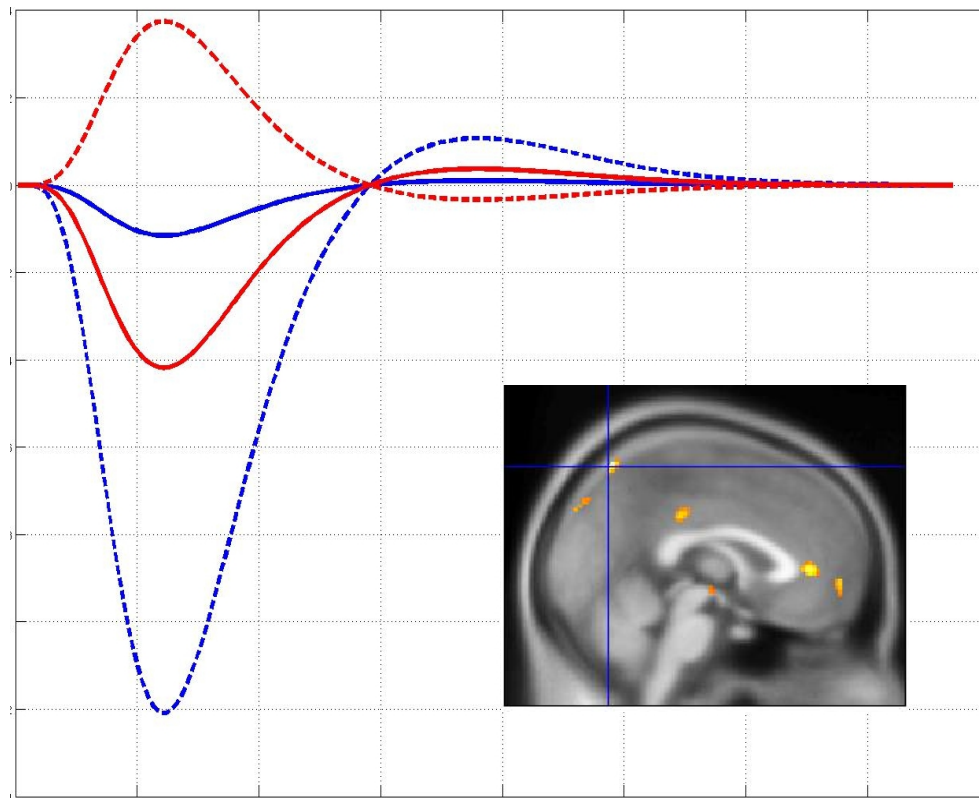


Always check interactions



Always check interactions

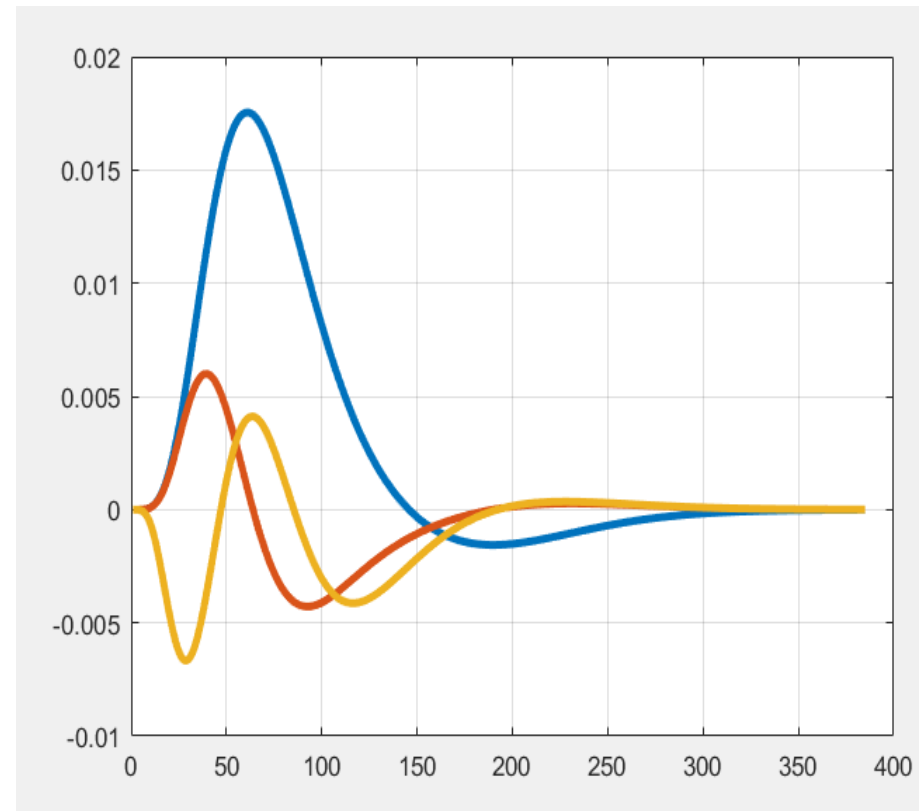
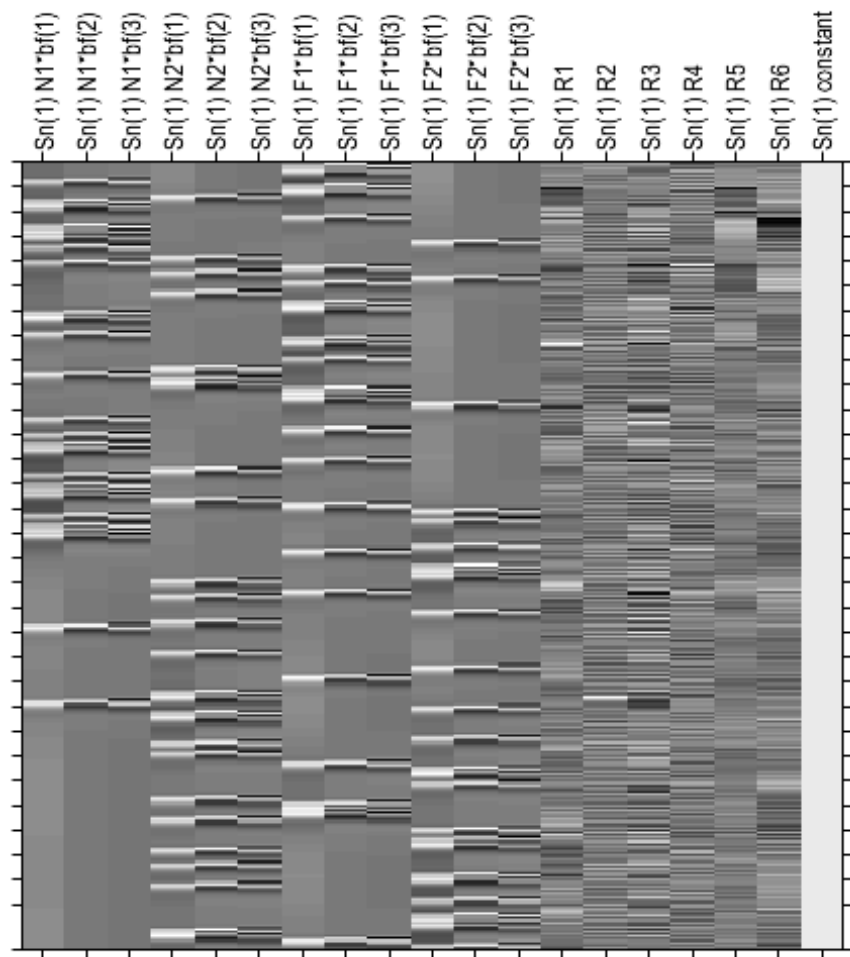
- Search in areas where all regressors are positive or all negative (i.e. use masking) otherwise ...



Plot the results !

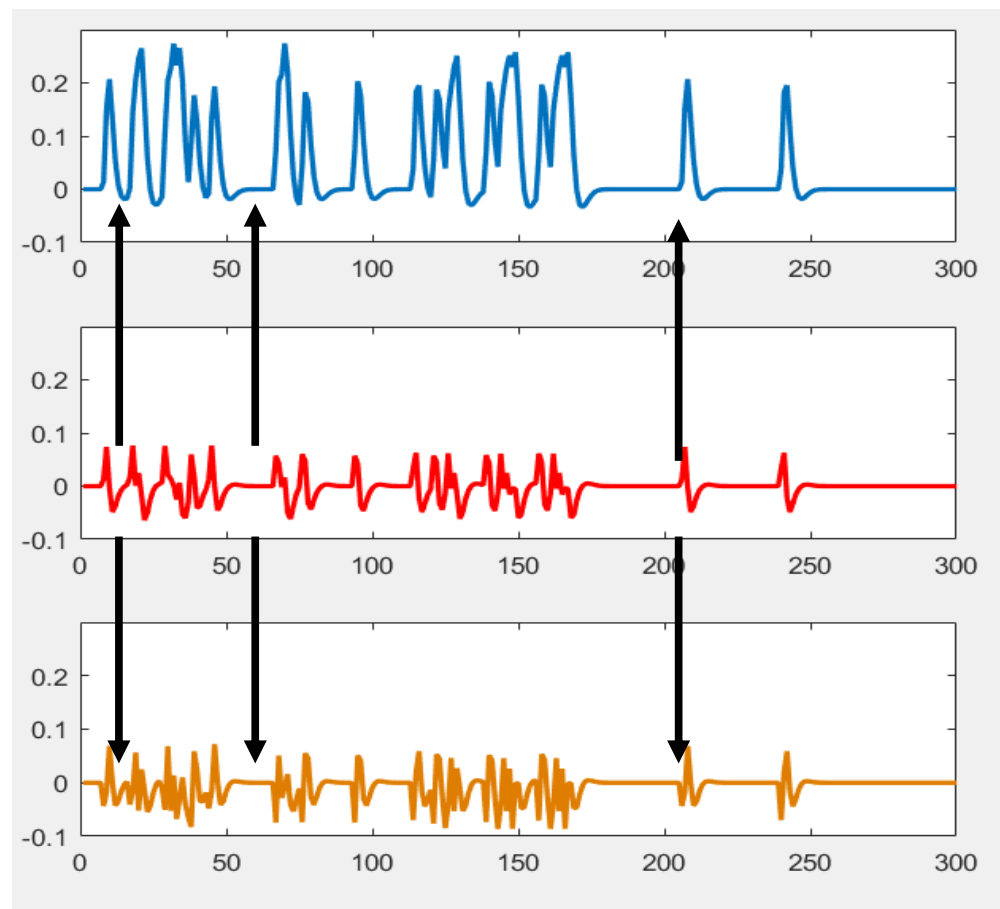
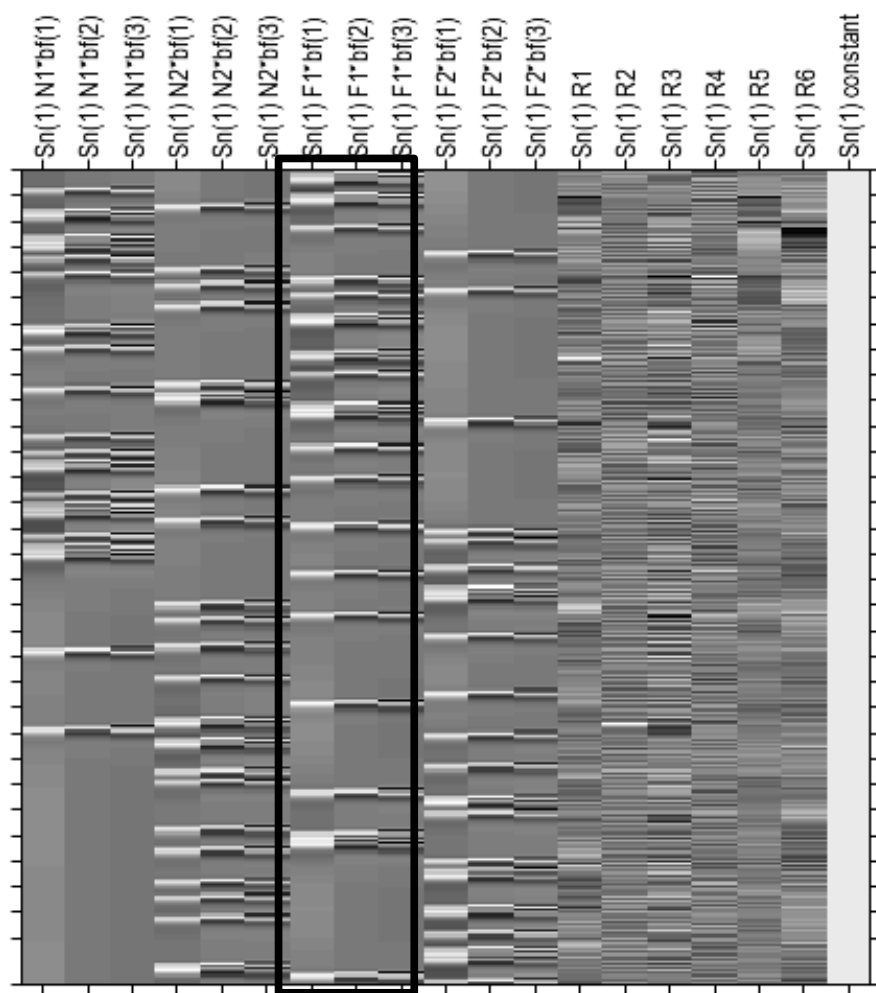
A more complete model

- Same design as before but added hrf derivatives.



A more complete model

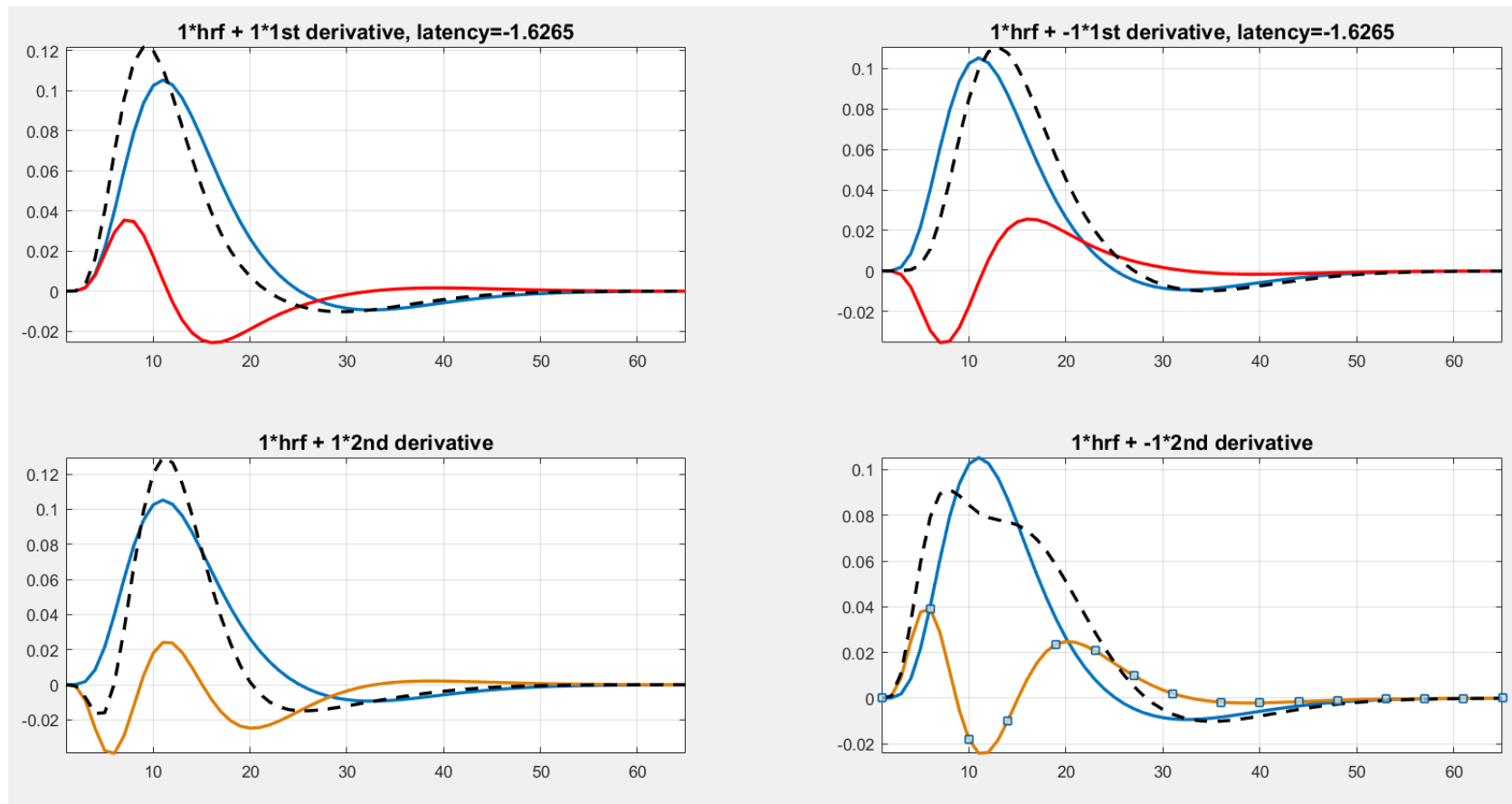
- Same design as before but added hrf derivatives.



3 regressors all at the same time (diff. values)

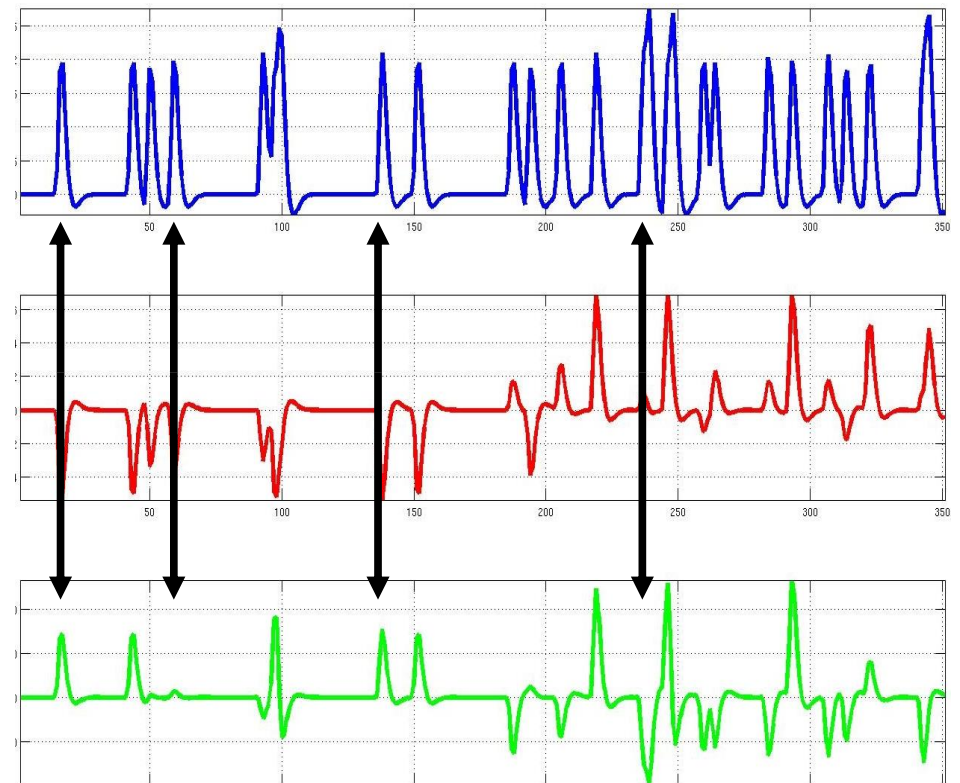
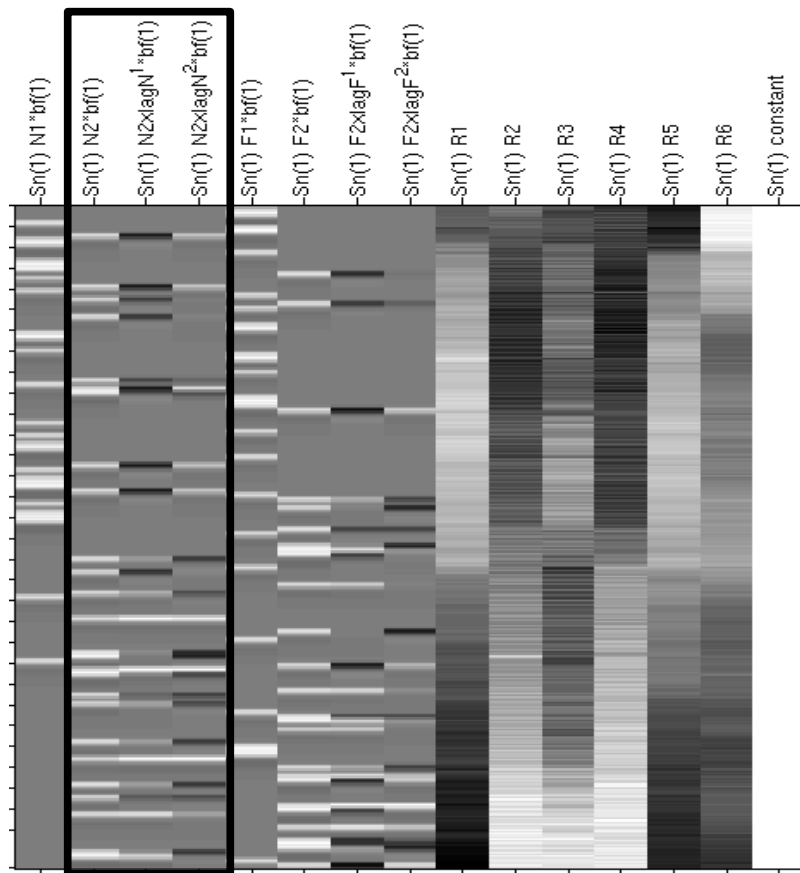
A more complete model

- What's a linear model already?
- We simply have to add the columns * coefficients betas



A more complex model

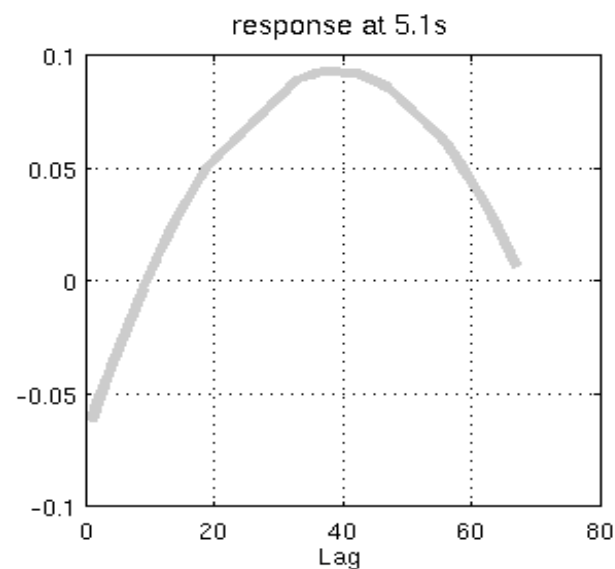
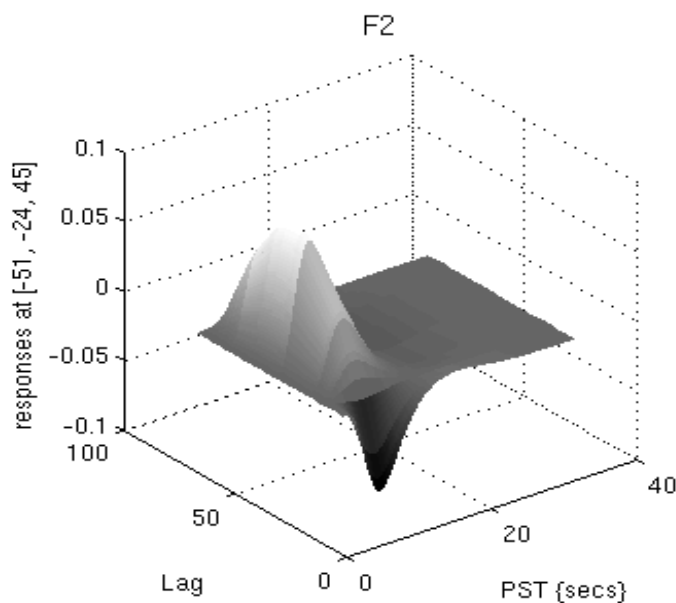
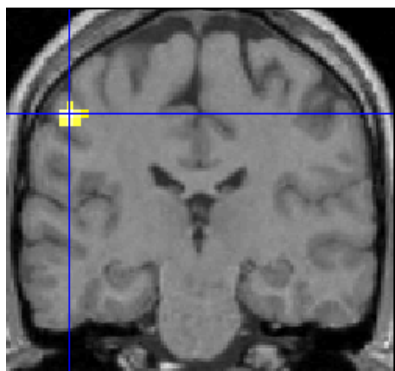
- Same design as before but added a 'parametric' regressor – here the lag and lag² between presentations



3 regressors all at the same time (diff. values)

A more complex model

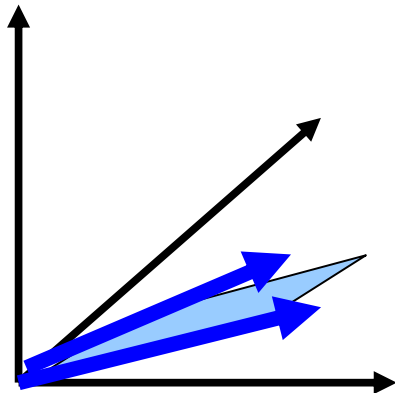
- The parametric regressors express the amplitude of signal as a function of the lag, i.e. the signal amplitude changes from trial to trial



Issues with regressors

More Regressors: collinearity

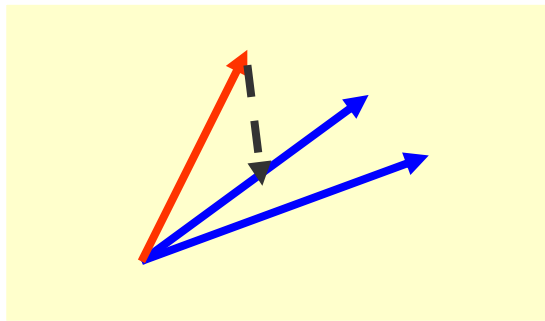
- By default, SPM orthogonalizes parametric regressors making the regressors non collinear (but you can disable that)
- Three or more points are said to be collinear if they lie on a single straight line.
- Regressors are collinear if they are perfectly correlated (note $\text{corr of 2 vectors} = \cos\theta$)



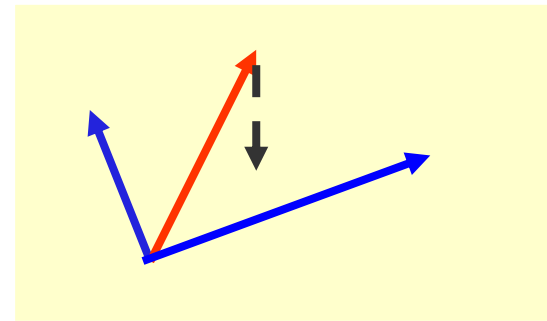
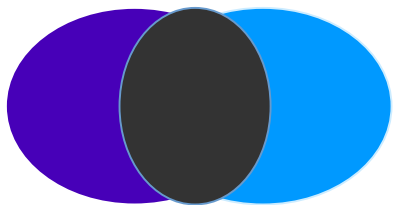
- Can make solution impossible
- Often make the model ok but individual regression values unstable
- Classical height and weight regression pblm

<http://en.wikipedia.org/wiki/Multicollinearity>
<http://mathworld.wolfram.com/Collinear.html>

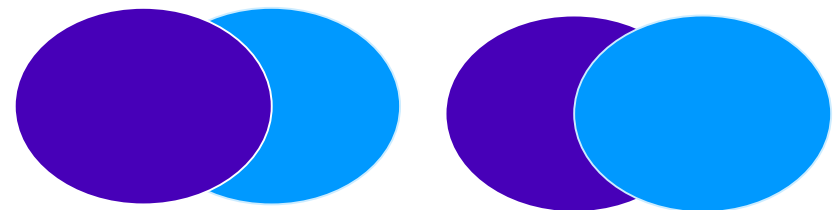
More Regressors: orthogonalization



Lot of variance shared –
because we look for the unique
part of variance, the shared
part goes into the error

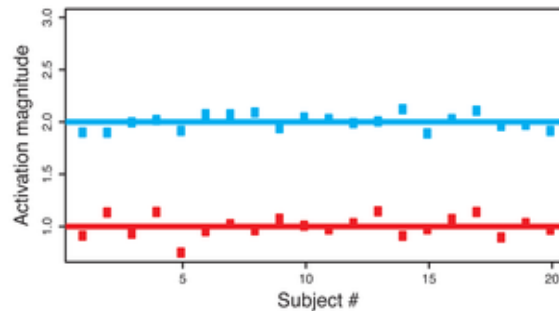


Orthogonalization ($\theta = 90^\circ$) removes shared
variance BUT order
matters !

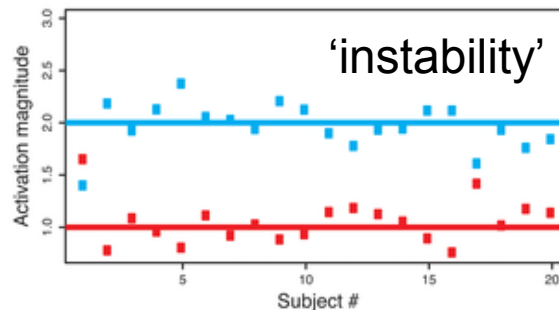


More Regressors: orthogonalization

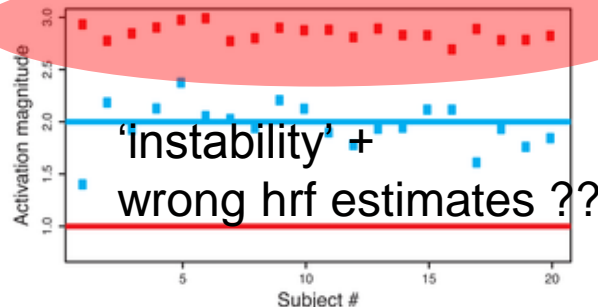
Low collinearity
ISI=3s



High collinearity
ISI=1s



Feedback
orthogonalized
with respect to
Stimulus



It's an interpretation issue,
what do we want to look at ?

$$Y = x_1b_1 + x_2b_2$$

→ b_1 is the 'baseline'
activation

→ b_2 is the modulation above
baseline

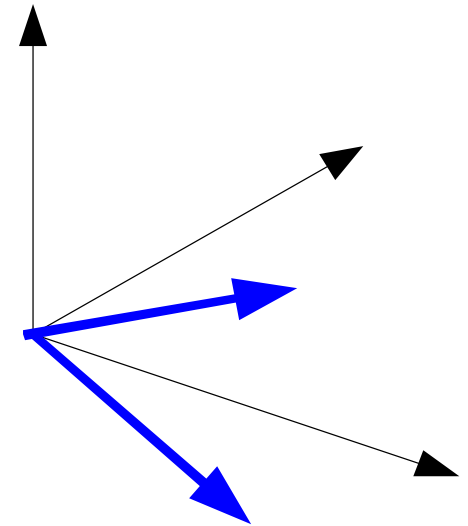
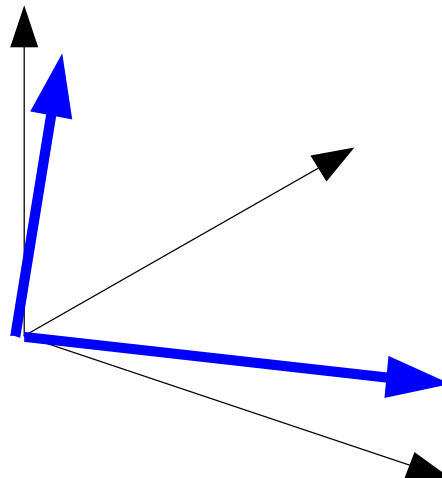
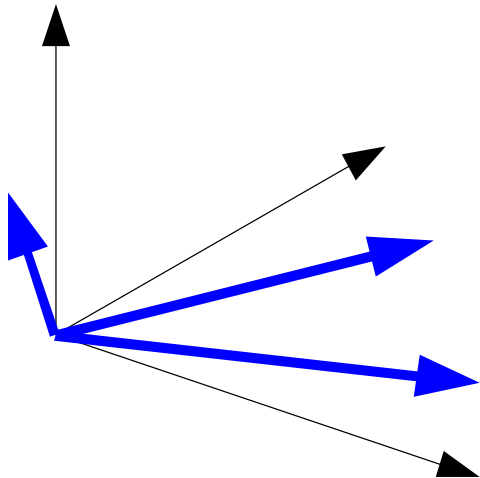
$$Y = x_1b_1 + \perp x_2b_2$$

→ b_1 is the mean activation

→ b_2 is the modulation around
the mean

More regressors

- Linearly independent ($X_2 \neq aX_1$), orthogonal ($X_1'Y_2 = 0$) and uncorrelated ($(X_1 - \text{mean}(X_1))'(X_2 - \text{mean}(X_2)) = 0$) variables



More regressors

- Linearly independent ($X_2 \neq aX_1$), orthogonal ($X_1'Y_2 = 0$) and uncorrelated ($(X_1 - \text{mean}(X_1))'(X_2 - \text{mean}(X_2)) = 0$) variables

[1 1 2 3] and [2 3 4 5]

Independent, correlated, not orthogonal

[1 -5 3 -1] and [5 1 1 3]

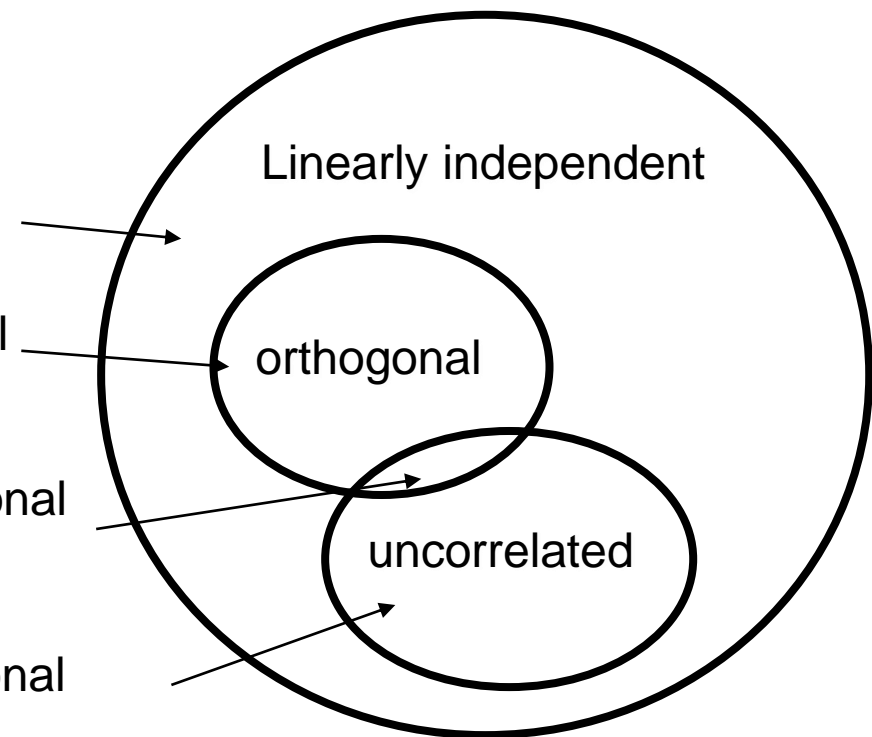
Independent, correlated and orthogonal

[-1 -1 1 1] and [1 -1 1 -1]

Independent, uncorrelated and orthogonal

[0 0 1 1] and [1 0 1 0]

Independent, uncorrelated, not orthogonal



Summary

- Linear model: $y = \beta_1 x_1 + \beta_2 x_2$ (output = additivity and scaling of input)
- GLM: $Y = XB + E$ (matrix formulation, works for any statistics, express the data Y as a function of the design matrix X)
- More regressors is better as it captures more of the signal but it may bring instability if regressors are collinear (and cost df). Orthogonalization makes sense for parametric regressors but not always.

Selected References

- Friston, K. J., Holmes, A. P., Worsley, K. J., Poline, J.-P., Frith, C. D., and Frackowiak, R. S. (1994). Statistical parametric maps in functional imaging: a general linear approach. *Hum. Brain Mapp.* 2, 189–210. doi: 10.1002/hbm.460020402
- Friston, K. J., Holmes, A., Poline, J.-B., Grasby, P., Williams, S., Frackowiak, R. S. J., et al. (1995). Analysis of time-series revised. *Neuroimage* 2, 45–53. doi: 10.1006/nimg.1995.1007
- Worsley, K. J., and Friston, K. (1995). Analysis of fMRI time-series revised - again. *Neuroimage* 2, 173–181. doi: 10.1006/nimg.1995.1023
- Poline, J.-B., and Brett, M. (2012). The general linear model and fMRI: does love last forever? *Neuroimage* 62, 871–880. doi: 10.1016/j.neuroimage.2012.01.133
- Pernet CR (2014) Misconceptions in the use of the General Linear Model applied to functional MRI: a tutorial for junior neuro-imagers. *Front. Neurosci.* 8:1. doi: 10.3389/fnins.2014.00001
- Mumford JA, Poline JB, Poldrack RA (2015) Orthogonalization of Regressors in fMRI Models. *PLOS ONE* 10(4): e0126255. doi: 10.1371/journal.pone.0126255
- Rodgers, J. L., Nicewander, W. A., and Toothaker, L. (1984). Linearly independent, orthogonal, and uncorrelated variables. *Am. Stat.* 38, 133–134.