

# Correction for multiple comparisons

Cyril Pernet, PhD

SBIRC/SINAPSE – University of Edinburgh

# Overview

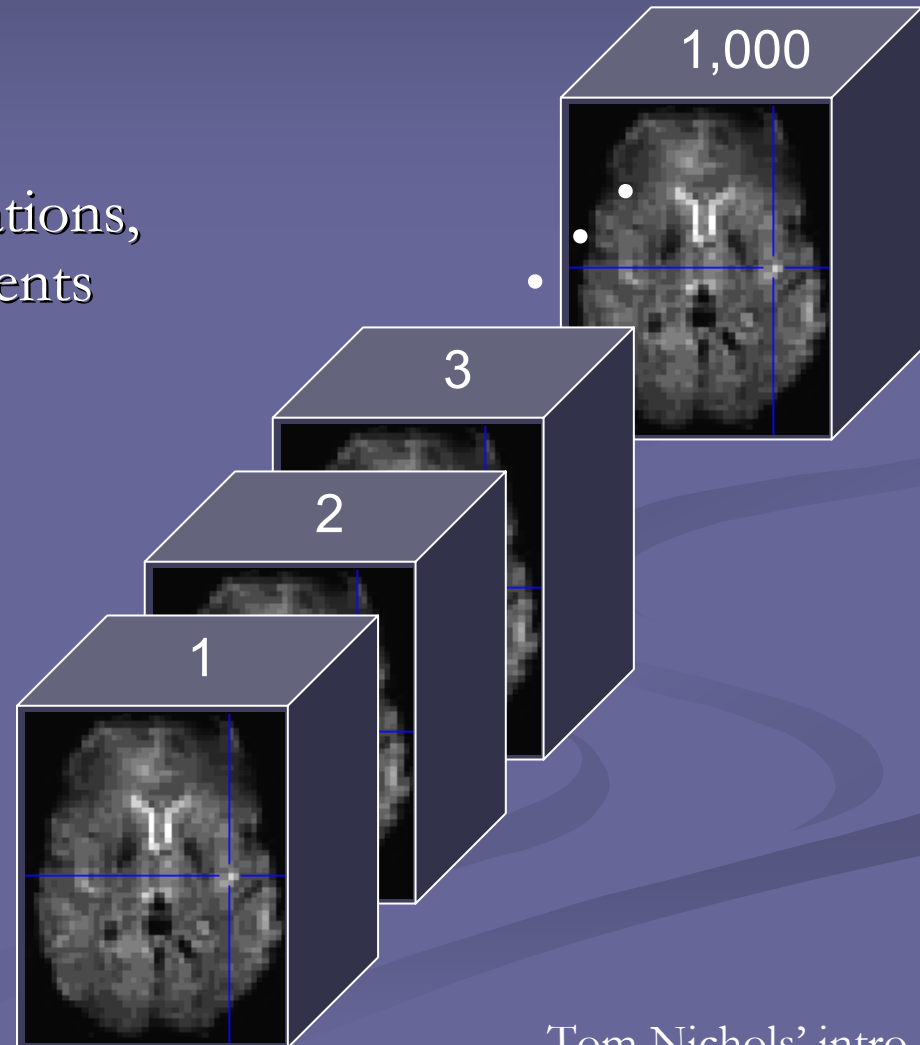
- Multiple comparisons correction procedures
- Levels of inferences (set, cluster, voxel)
- Circularity issues

# Multiple comparison correction

Avoiding false positives

# What Problem?

- 4-Dimensional Data
  - 1,000 multivariate observations, each with  $> 100,000$  elements
  - 100,000 time series, each with 1,000 observations
- Massively Univariate Approach
  - 100,000 hypothesis tests
- Massive MCP!



Tom Nichols' intro

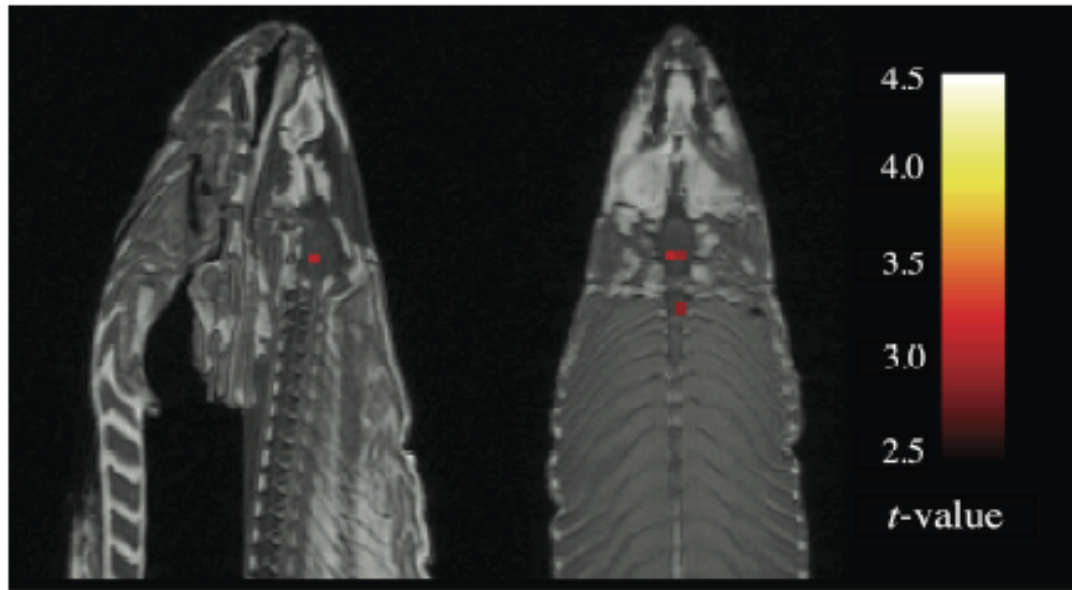
# What Problem?

- Typical brain  $\sim 130000$  voxels
- @  $p = .05$ , it is expected = 6500 false positives!
- @ a more conservative value like  $p = .001$  we still expect 130 false positives.
- Using extend threshold  $k$  without correction is not enough as it, by chance, can cluster as well.

# What Problem?

- Bennet et al., 2009
- Task: take a decision about emotions on pictures
- Design: blocks of 12 sec activation/rest
- Analysis: standard data processing with SPM
- Subject: a dead salmon!

# What Problem?



A  $t$ -contrast was used to test for regions with significant BOLD signal change during the photo condition compared to rest. The parameters for this comparison were  $t(131) > 3.15$ ,  $p(\text{uncorrected}) < 0.001$ , 3 voxel extent threshold.

- The cluster was  $81\text{mm}^3$  ! – after multiple comparison corrections all false activations were removed.

# Solutions for MCP

- Height Threshold
- Familywise Error Rate (FWER)
  - Chance of *any* false positives; Controlled by Bonferroni & Random Field Methods
- False Discovery Rate (FDR)
  - Proportion of false positives *among* rejected tests
- Bayes Statistics



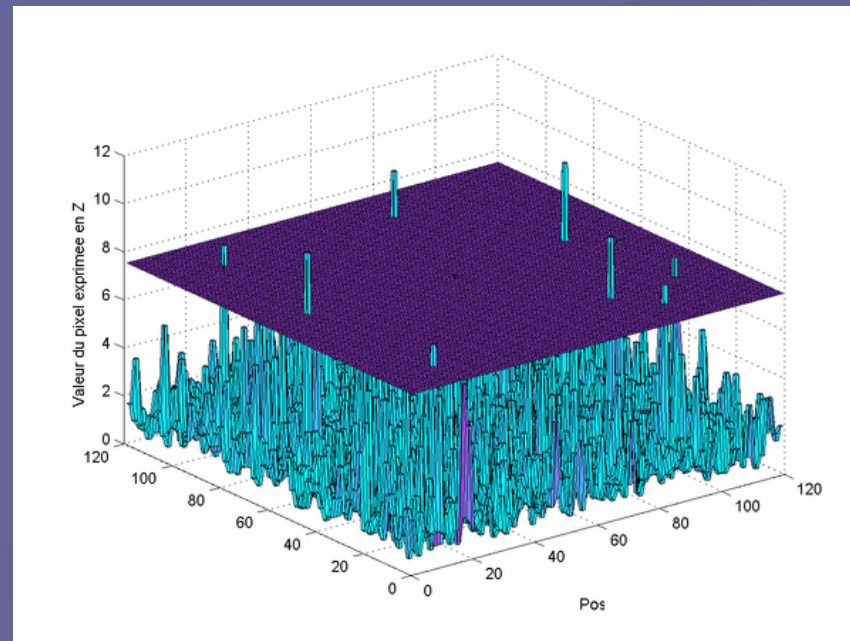
# From single univariate to massive univariate

Univariate stat	Functional neuroimaging
1 observed data	Many voxels
1 statistical value	Family of statistical values
Type 1 error rate (chance to be wrong rejecting $H_0$ )	Family-wise error rate
Null hypothesis	Family-wise null hypothesis

# Height Threshold

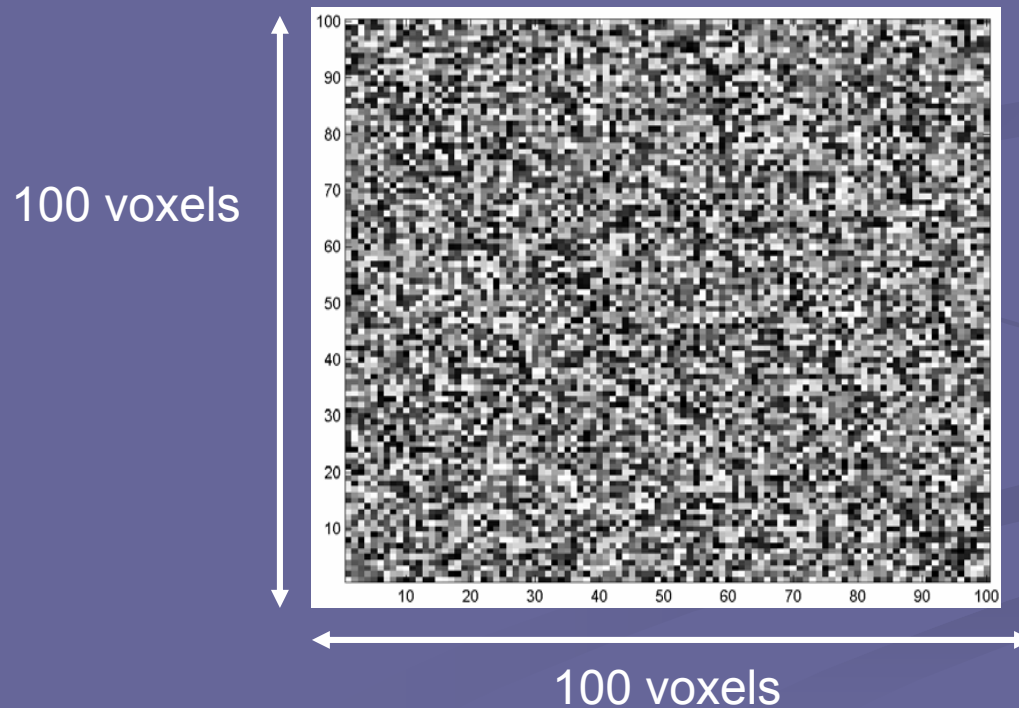
- Choose locations where a test statistic  $Z$  (T, F, ...) is large to threshold the image of  $Z$  at a height  $z$
- The problem is how to choose this threshold  $z$  to exclude false positives with a high probability (e.g. 0.95)?

To control for family wise error on must take into account the nb of tests



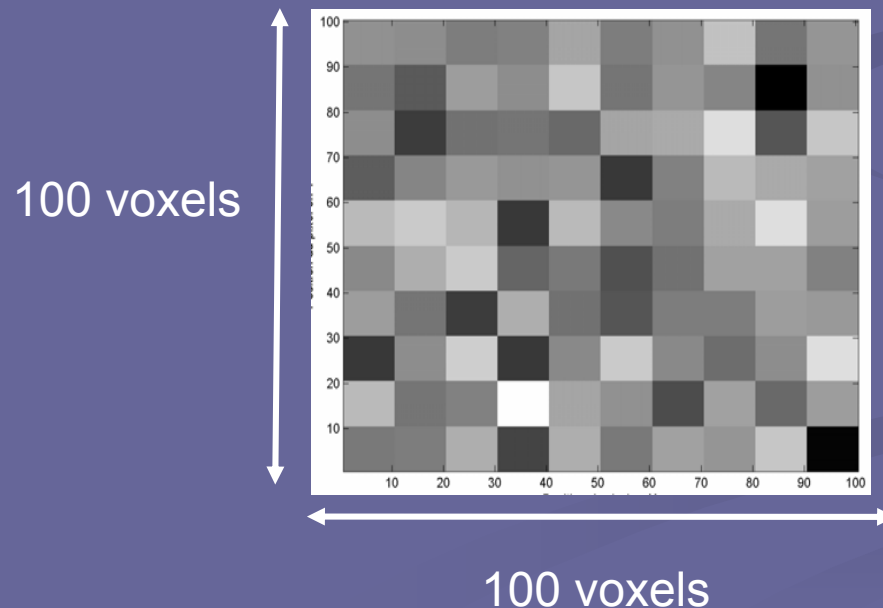
# Bonferroni

- 10000 Z-scores ;  $\alpha = 5\%$
- $\alpha \text{ corrected} = .000005$  ;  $z\text{-score} = 4.42$



# Bonferroni

- 10000 Z-scores ;  $\alpha = 5\%$
- 2D homogeneous smoothing – 100 independent observations
- $\alpha \text{ corrected} = .0005$  ;  $z\text{-score} = 3.29$

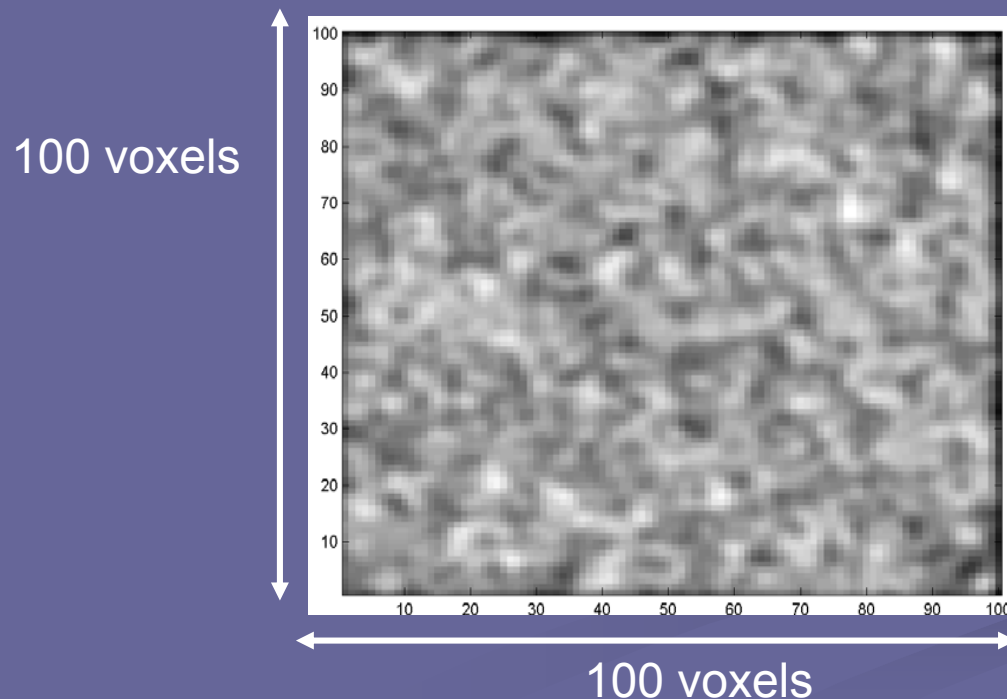


# Solutions for MCP

- An important feature of neuroimaging data is that we have a family of stat values that has topological features (Bonferroni for instance consider tests as independent)
- Why considering data as a smooth lattice? (Chumbley et al., 2009 NeuroImage 44)
  - fMRI/PET are projection methods of data points onto the whole space – MEEG forms continuous functions in time and are smooth by the scalp (space)
  - Neural activity propagate locally through intrinsic/lateral connections and is distributed via extrinsic connections / Hemodynamic correlates are initiated by diffusing signals (e.g. NO)

# Random Field Theory

- 10000 Z-scores ;  $\alpha = 5\%$
- Gaussian kernel smoothing –
- How many independent observations ?

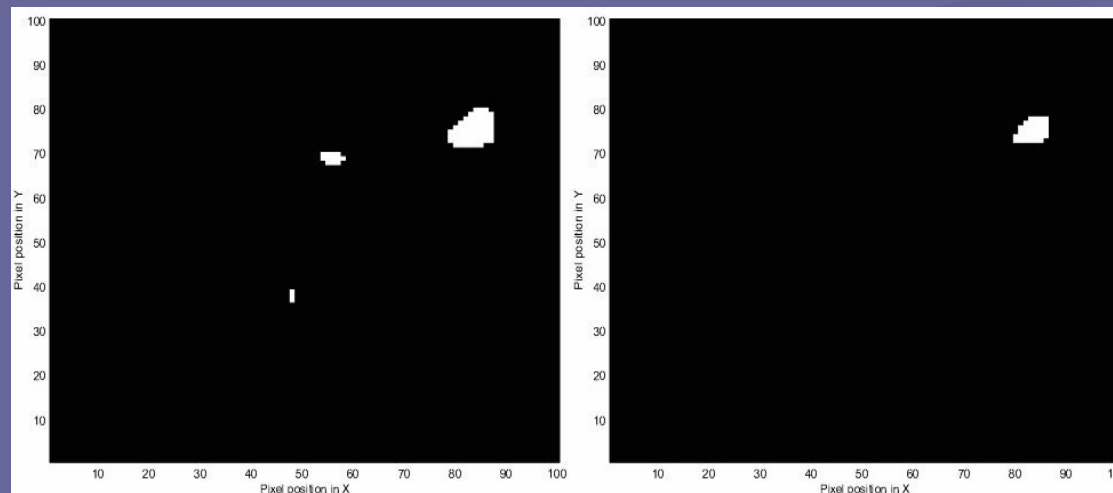


# Random Field Theory

- RFT relies on theoretical results for smooth statistical maps (hence the need for smoothing), allowing to find a threshold in a set of data where it's not easy to find the number of independent variables. Uses the expected Euler characteristic (EC density)
- 1 Estimation of the smoothness = number of resel (resolution element) =  $f(\text{nb voxels}, \text{FWHM})$
- 2 expected Euler characteristic = number of clusters above the threshold
- 3 Calculation of the threshold

# Random Field Theory

- The Euler characteristic can be seen as the number of blobs in an image after thresholding (p value that you select in SPM)
- At high threshold,  $EC = 0$  or  $1$  per resel:  $E[EC] \approx p^{\text{FWE}}$

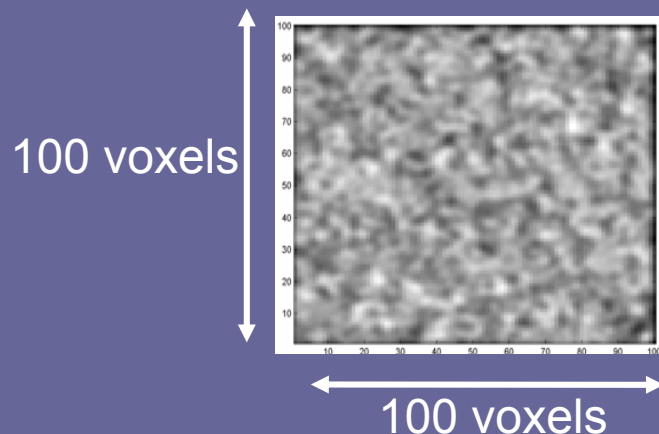


$E[EC] = R \cdot (4 \log_e 2) \cdot (2\pi)^{-2/3} \cdot Z_t \cdot e^{-1/2 Z_t^2}$  for a 2D image, more complicated in 3D



# Random Field Theory

- For 100 resels, the equation gives  $E[EC] = 0.049$  for a threshold  $Z$  of 3.8, i.e. the probability of getting one or more blobs where  $Z$  is greater than 3.8 is 0.049



$\alpha$	number of resels in the image	Bonferroni		RFT
		threshold	score $Z$	score $Z$
0.05	100	$\frac{0.05}{100}$	3.3	
				3.8

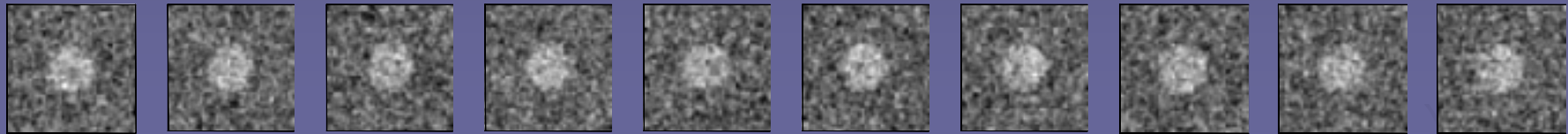
- If the resel size is much larger than the voxel size then  $E[EC]$  only depends on the nb of resels otherwise it also depends on the volume, surface and diameter of the search area (i.e. shape and volume matter)

# False discovery Rate

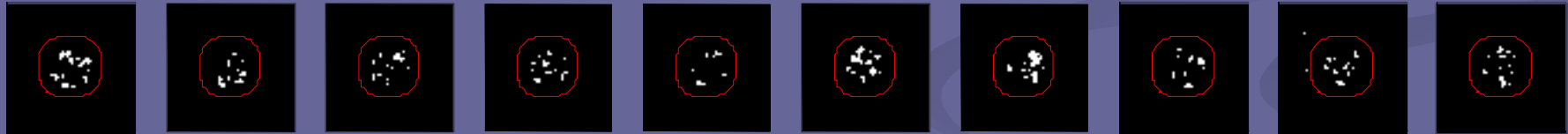
- Whereas family wise approach corrects for any false positive, the FDR approach aim at correcting among positive results only.
1. Run an analysis with  $\alpha = x\%$
  2. Sort the resulting positive data
  3. Threshold to remove the false positives

# False discovery Rate

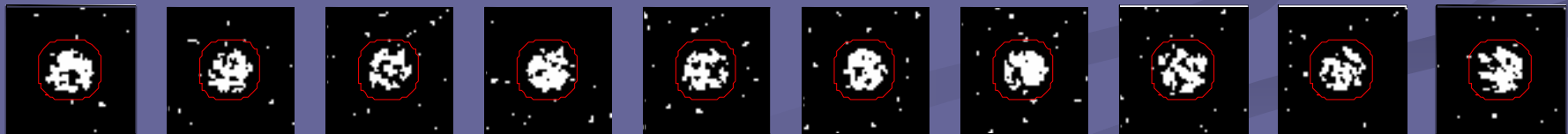
Signal+Noise



FEW correction



FDR correction

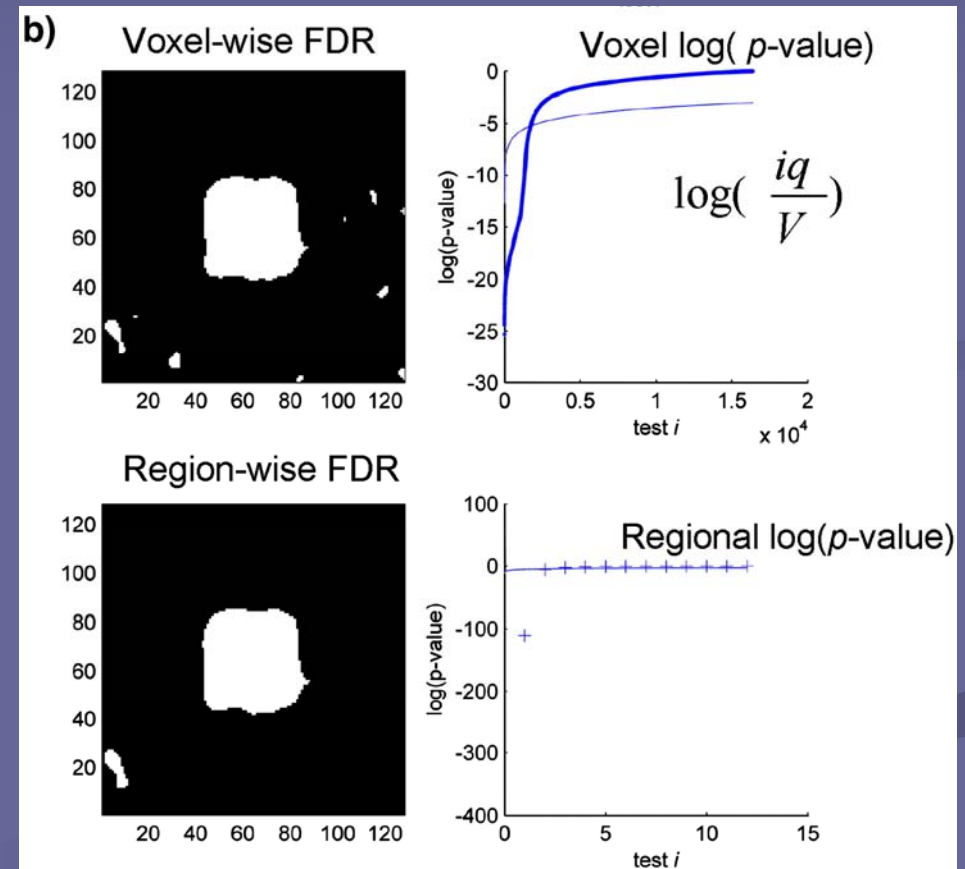


# False discovery Rate

takes the spatial structure into account

Under  $H_0$  the nb of voxels per cluster is known  $\rightarrow$  uncorrected p value for clusters  $\rightarrow$  apply FDR on the clusters (volume-wise correction)

Assumes that the volume of each cluster is independent of the number of clusters



# Levels of inference

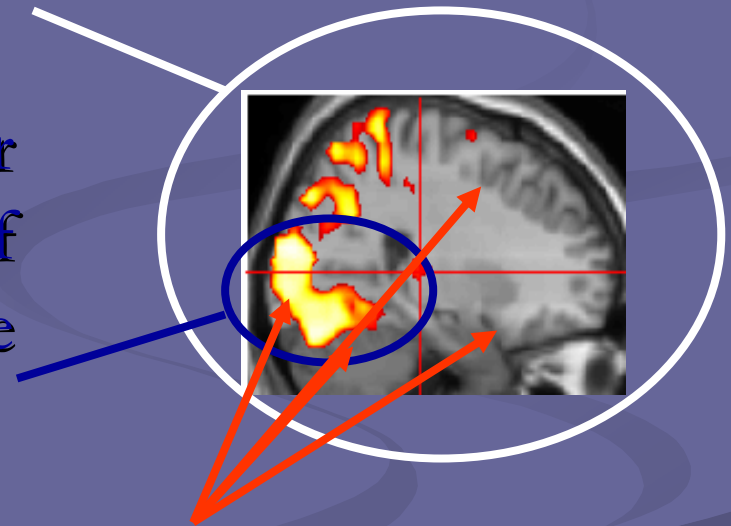
Voxel, cluster and set

# Levels of inference

- 3 levels of inference can be considered:
  - Voxel level (prob associated at each voxel)
  - Cluster level (prob associated to a set of voxels)
  - Set level (prob associated to a set of clusters)
- The 3 levels are nested and based on a single probability of obtaining  $c$  or more clusters (set level) with  $k$  or more voxels (cluster level) above a threshold  $u$  (voxel level):  
 $P_w(u, k, c)$

# Levels of inference

- Set level: we can reject  $H_0$  for an omnibus test, i.e. there are some significant clusters of activation in the brain.
- Cluster level: we can reject  $H_0$  for an area of a size  $k$ , i.e. a cluster of 'activated' voxels is likely to be true for a given spatial extend.
- Voxel level: we can reject  $H_0$  at each voxel, i.e. a voxel is 'activated' if exceeding a given threshold



# Levels of inference

- Each level of inference is valid, but the inferences are different – e.g. a set might be enough to check that subjects activated regions selected a priori for a connectivity analysis – clusters might be good enough if hypotheses are about the use of different brain areas between groups
- Both voxel and cluster levels need to address the multiple comparison problem. If the activated region is predicted in advance, the use of corrected p values is unnecessary and inappropriately conservative – a correction for the number of predicted regions (Bonferroni) is enough



# Level of inference

Statistics: *p-values adjusted for search volume*

set-level		cluster-level				peak-level					mm mm mm		
<i>D</i>	<i>C</i>	<i>D</i> <sub>FWE-corr</sub>	<i>q</i> <sub>FDR-corr</sub>	<i>k</i> <sub>E</sub>	<i>D</i> <sub>uncorr</sub>	<i>D</i> <sub>FWE-corr</sub>	<i>q</i> <sub>FDR-corr</sub>	<i>T</i>	( <i>Z</i> <sub>E</sub> )	<i>D</i> <sub>uncorr</sub>			
0.000	22	0.000	0.000	317	0.000	0.000	0.000	8.66	Inf	0.000	43	-30	-32
						0.000	0.000	7.48	7.16	0.000	51	-21	-13
						0.000	0.000	7.37	7.06	0.000	40	-10	-14
		0.103	0.048	22	0.017	0.000	0.000	6.75	6.51	0.000	-16	91	-22
						0.525	0.178	3.88	3.83	0.000	-1	96	-17
						0.000	0.000	6.71	6.47	0.000	-13	-51	-11
		0.005	0.003	52	0.001	0.000	0.000	6.37	6.17	0.000	13	-47	-11
						0.008	0.004	6.22	6.03	0.000	-39	-20	-9
						0.000	0.000	0.022	0.010	4.83	4.73	0.000	-39
		0.001	0.001	72	0.000	0.000	0.000	6.18	5.99	0.000	-42	-32	-58
						0.042	0.017	4.68	4.59	0.000	-24	-40	-62
						0.125	0.039	4.38	4.31	0.000	-12	-36	-62
		0.000	0.000	191	0.000	0.001	0.001	5.58	5.44	0.000	6	-23	7
						0.001	0.001	5.40	5.27	0.000	-2	-15	17
						0.022	0.010	4.83	4.74	0.000	9	-33	18
		0.000	0.000	91	0.000	0.005	0.004	5.14	5.03	0.000	-46	93	-7
						0.017	0.009	4.89	4.80	0.000	-35	93	-2
						0.045	0.017	4.66	4.57	0.000	2	109	7
		0.435	0.182	10	0.091	0.006	0.004	5.09	4.99	0.000	-46	-15	-39
						0.130	0.054	4.63	4.55	0.000	33	-32	-57
0.147	0.056					3.97	3.92	0.000	43	70	0		
0.549	0.215	8	0.127	0.453	0.151	3.94	3.89	0.000	47	67	11		
				0.457	0.151	3.94	3.89	0.000	28	-1	1		
				0.489	0.196	9	0.107	0.628	0.228	3.79	3.74	0.000	-39

*table shows 3 local maxima more than 8.0mm apart*

Height threshold:  $T = 3.12$ ,  $p = 0.001$  (0.998)  
 Extent threshold:  $k = 0$  voxels,  $p = 1.000$  (0.998)  
 Expected voxels per cluster,  $\langle k \rangle = 3.583$   
 Expected number of clusters,  $\langle c \rangle = 6.27$   
 FWEp: 4.633, FDRp: 4.334, FWEc: 47, FDRc: 22

Degrees of freedom = [1.0, 303.0]  
 FWHM = 13.1 13.0 12.7 mm mm mm; 3.5 3.5 2.5 (voxels)  
 Volume: 1429734 = 20334 voxels = 558.0 resels  
 Voxel size: 3.8 3.7 5.0 mm mm mm; (resel = 30.96 voxels)  
 Page

RFT

Using  $p=.001$  this creates an excursion set  
 Prob clusters of that size  
 Prob peak that height  
 → after FDR correction

Uncorrected (bad)

# Circularity issues in fMRI

# Definition

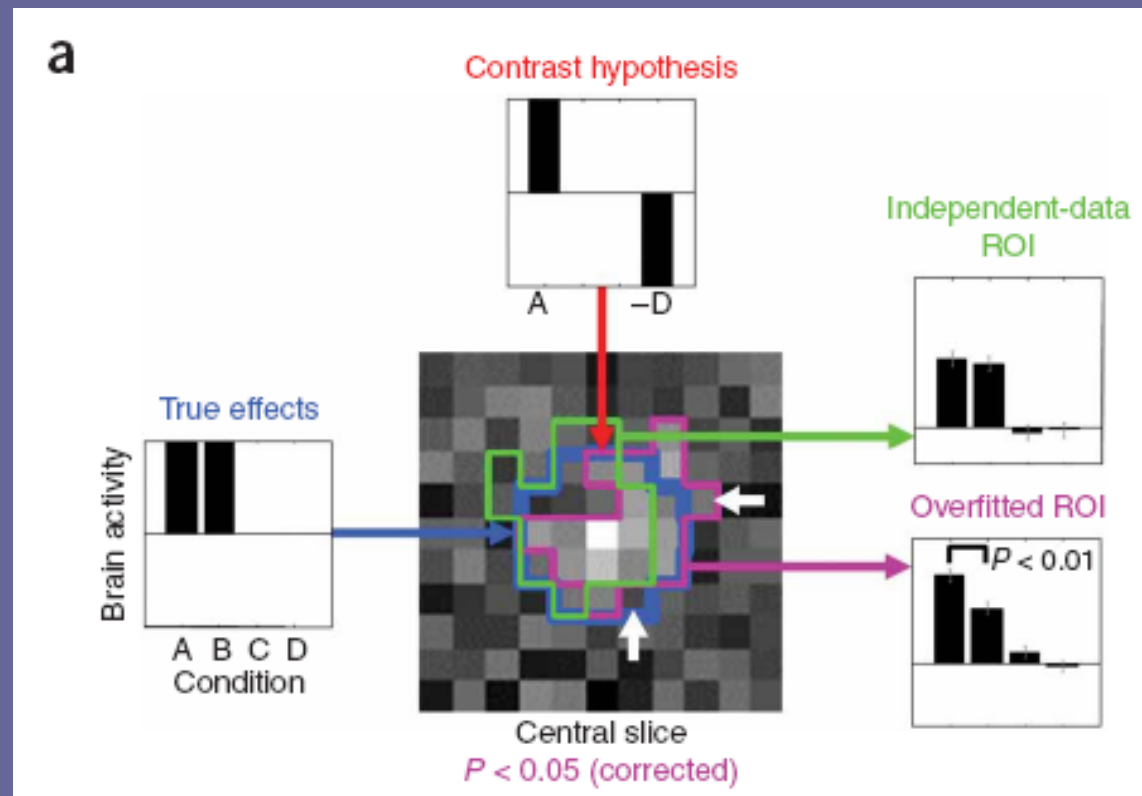
- Refers to the problem of selecting data for analysis
- How data (areas usually) are selected, analysed and sorted is key to avoid circularity
- Put forward by Vul et al. 2009, *Perspectives on Psychological Science*. 4
- Better explained in Kriegeskorte et al., 2009 *Nat. Neuroscience* 12

# Circularity

- Double dipping pblm: “data are first analyzed to select a subset and then the subset is reanalyzed to obtain the results. In this context, assumptions and hypotheses determine the selection criterion and selection can, in turn, distort the results.”
- Take a gp of subjects and measures RTs, then take 2 subgroups from the same subjects and re-do some analysis?? → increases the diff.
- Take fMRI data and get activated areas, extract ROI and re-do some analyses??

# Circularity

- Selection and tests must be independent – non independence create spurious effects



# Circularity

- Independence of the selection and tests
  1. Anatomic ROI, analysis of fMRI
  2. SPM, minimal requirement is orthogonality of the contrasts (e.g. find regions using  $A+B>0$   $C=[1 \ 1]$  and test  $A$  vs  $B$   $C=[1 \ -1]$ ) but if  $N_A$  and  $N_B$  are different there is still a bias when testing  $A-B$  (across subjects independence is ensured by  $C_{\text{selection}}^T (X^T X)^{-1} C_{\text{test}}$ )
  3. Select using a subset of data, test with another one

# Enough for today ☺



Thanks for your attention