

U-Net: Convolutional Networks for Biomedical Image Segmentation

Ronneberger, et al, 2015

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Outline

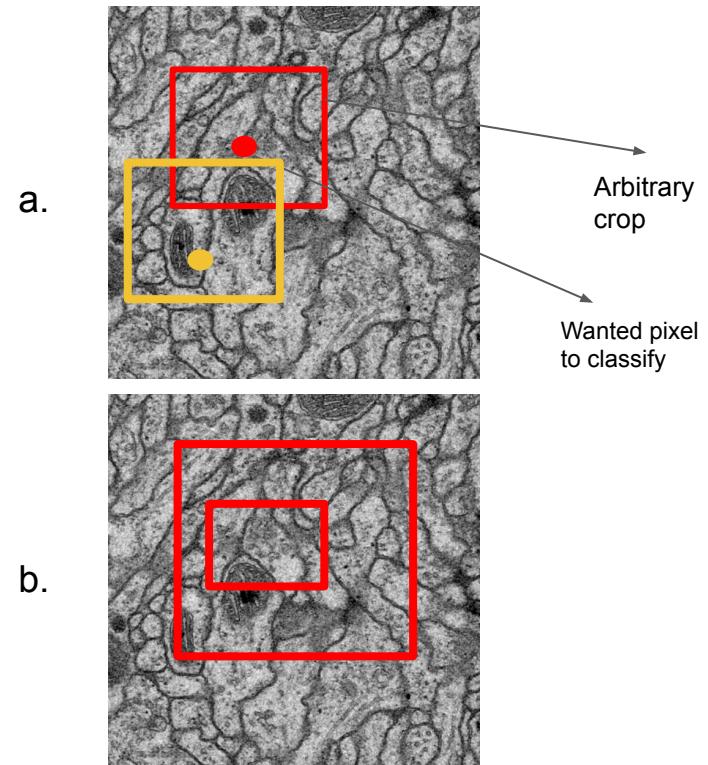
- Previous works lead to U-Net
 - Deep Neural Networks Segment Neuronal Membranes in Electron Microscopy Images, Ciresan et al, 2012
 - Fully Convolutional Networks for Semantic Segmentation, Long et al, 2014
- U-Net Architecture
- Training Strategies
- Results
- U-Net Variations
- Summary and Limitations



Deep Neural Networks Segment Neuronal Membranes in Electron Microscopy Images, Ciresan et al, 2012

Sliding Window Setup

- Advantage:
 - Improve localization
 - Increase number of data training
- Drawbacks:
 - slow to run
 - Redundancy due to overlap (a)
 - Tradeoff on localization and use of context (b)

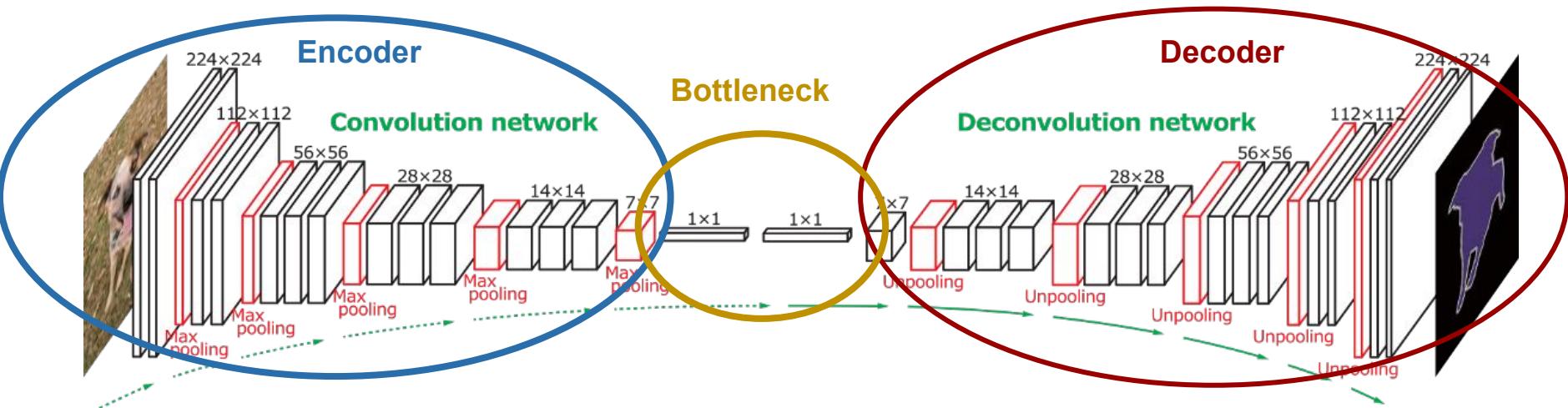


Sample slice of a dataset, Figure 5,
Ciresan et al, 2012

Fully Convolutional Networks for Semantic Segmentation, Long et al, 2014

- Architecture:

- Capable of being trained on arbitrary size of input (no fully connected layer in network)
- Consists of Use upsampling / transposed convolution
- Skip connection



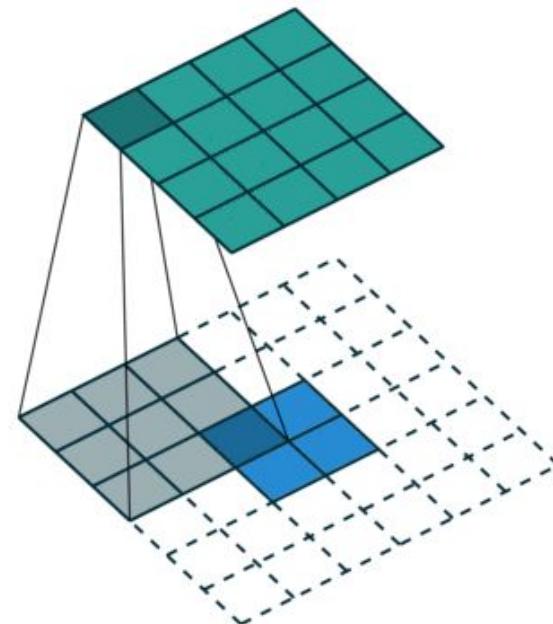
<https://medium.com/@wilburdes/semantic-segmentation-using-fully-convolutional-neural-networks-86e45336f99b>

Transposed Convolution (Deconvolution/ Unpooling)

Convolution (3*3 kernel)



Transposed Conv (3*3 kernel)



<https://towardsdatascience.com/intuitively-understanding-convolutions-for-deep-learning-1f6f42faee1>

<https://datascience.stackexchange.com/questions/6107/what-are-deconvolutional-layers>

Skip Connections

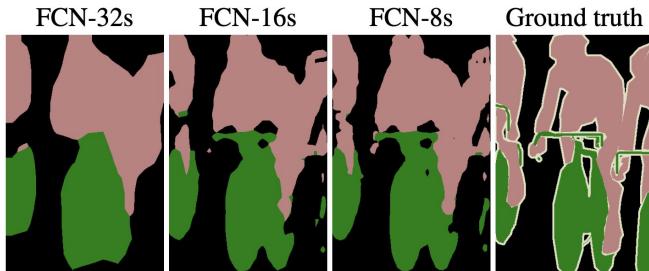


Figure 4, Long et al, 2014

To go up from the bottleneck layer and construct the segmentation labels

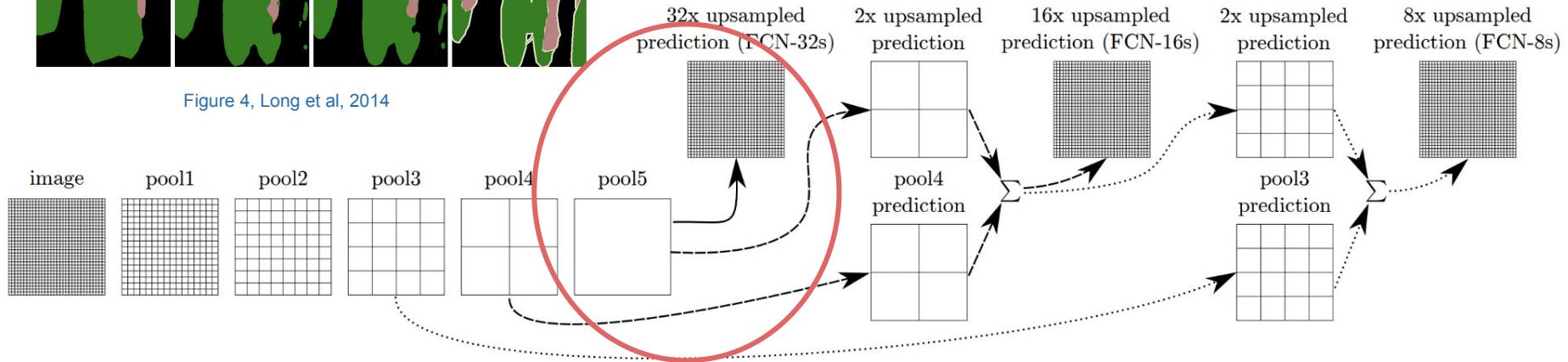


Figure 3, Long et al, 2014

Figure 2, Ronneberger, et al, 2015

Number of feature channels per layer

Input size of each layer

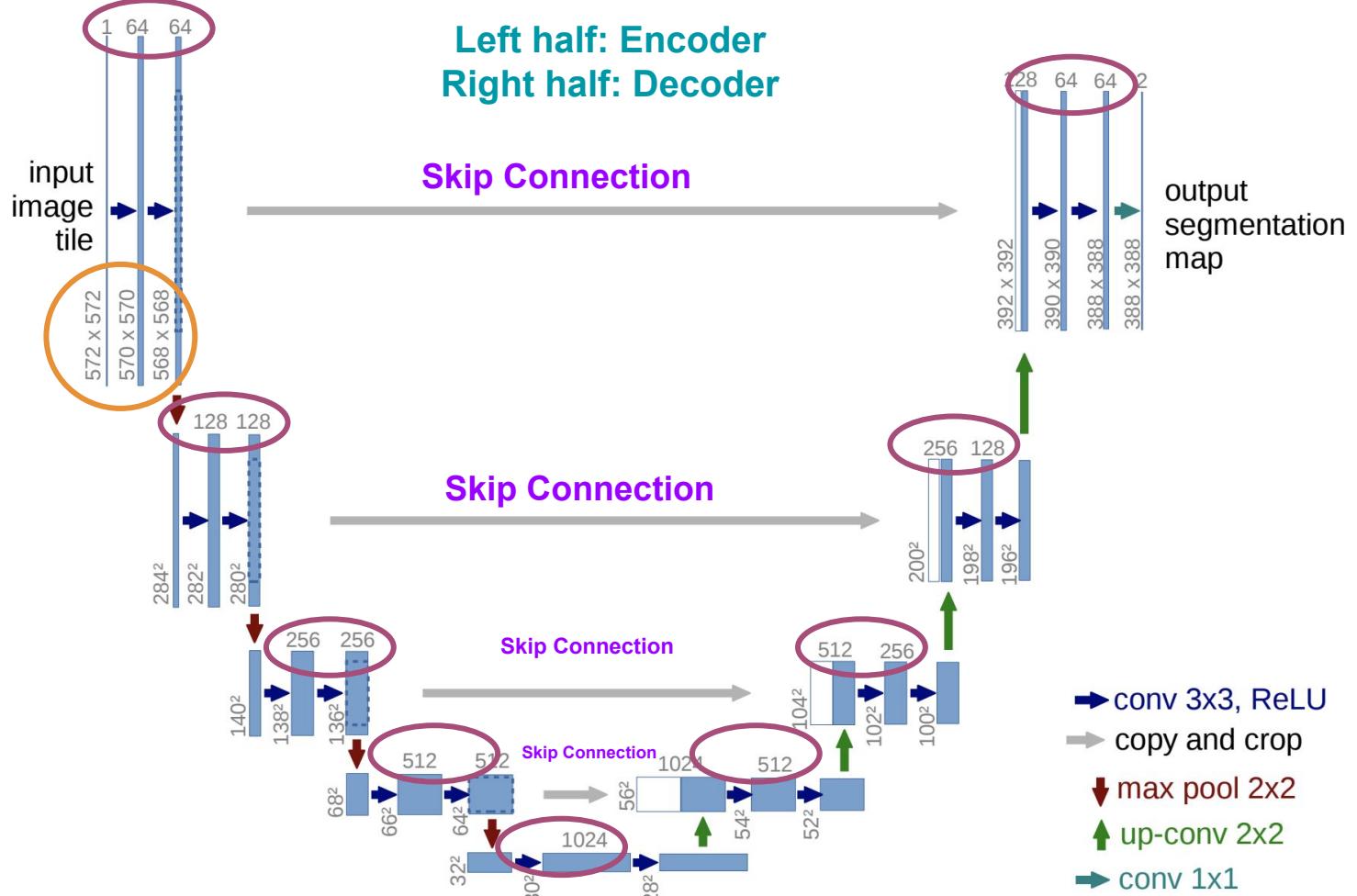
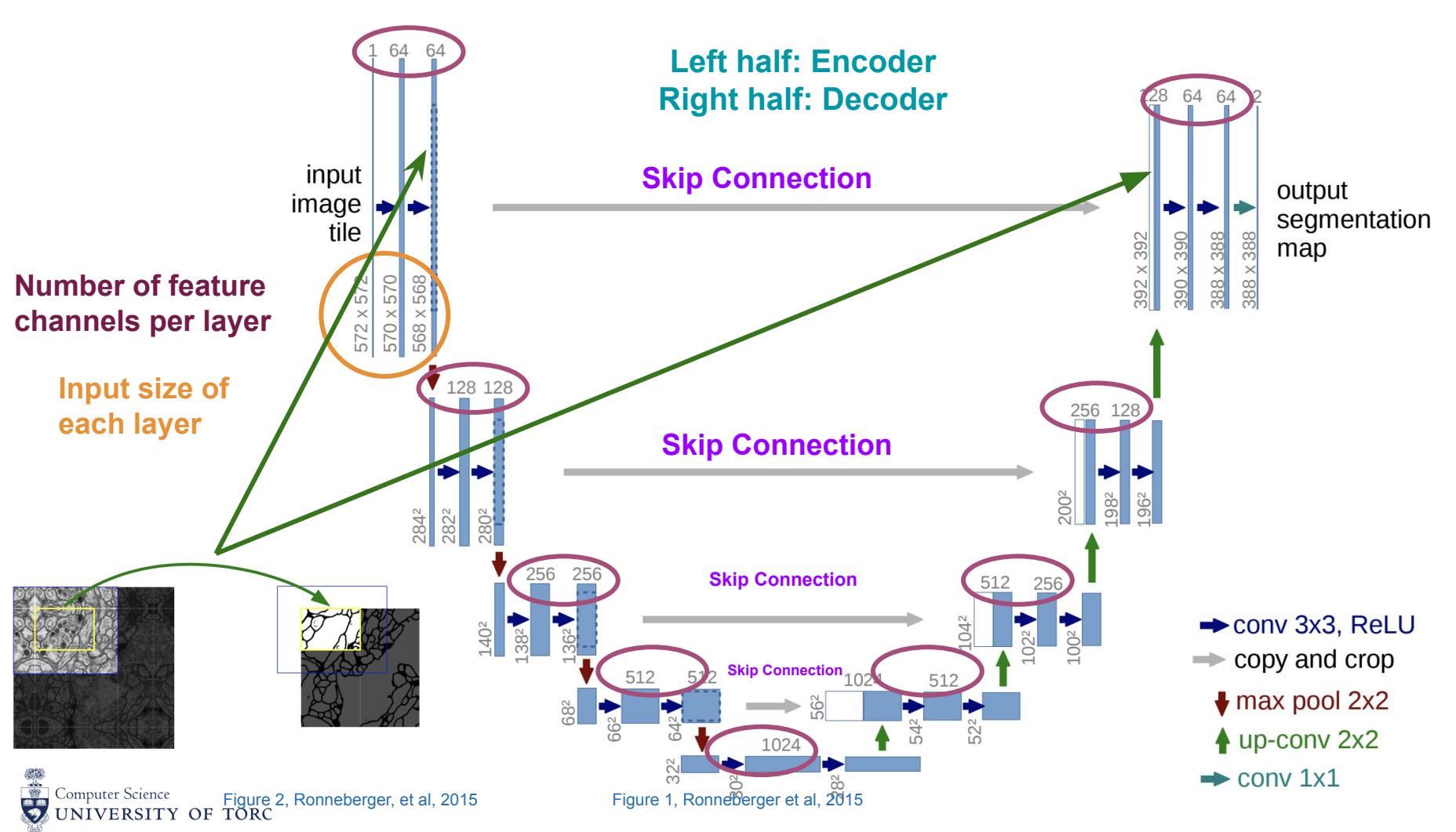
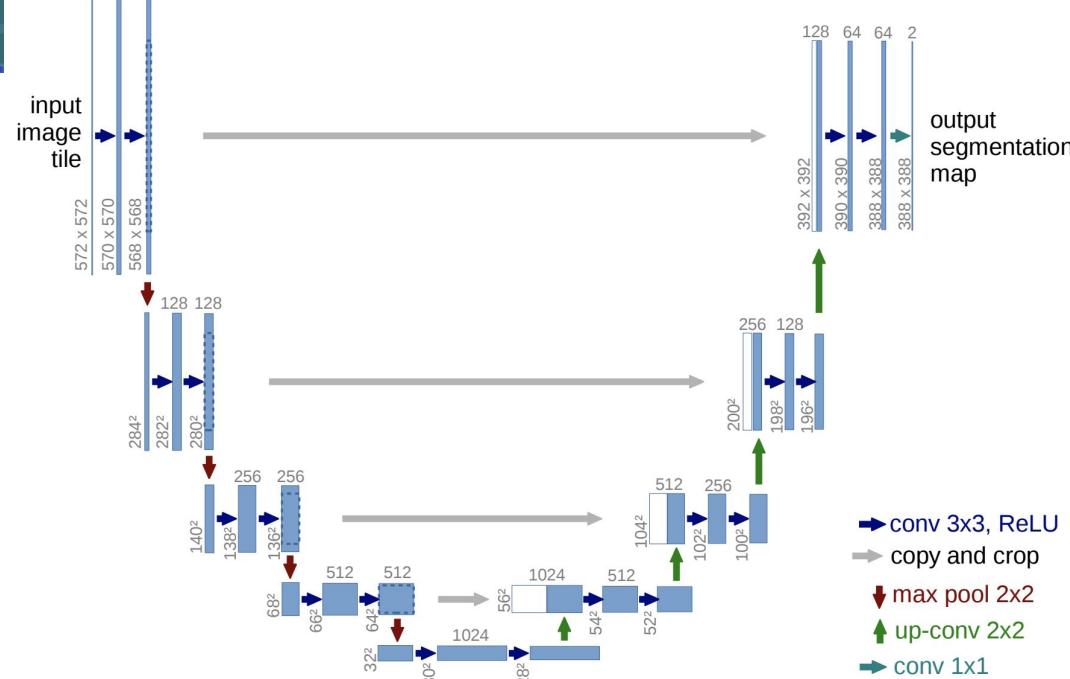
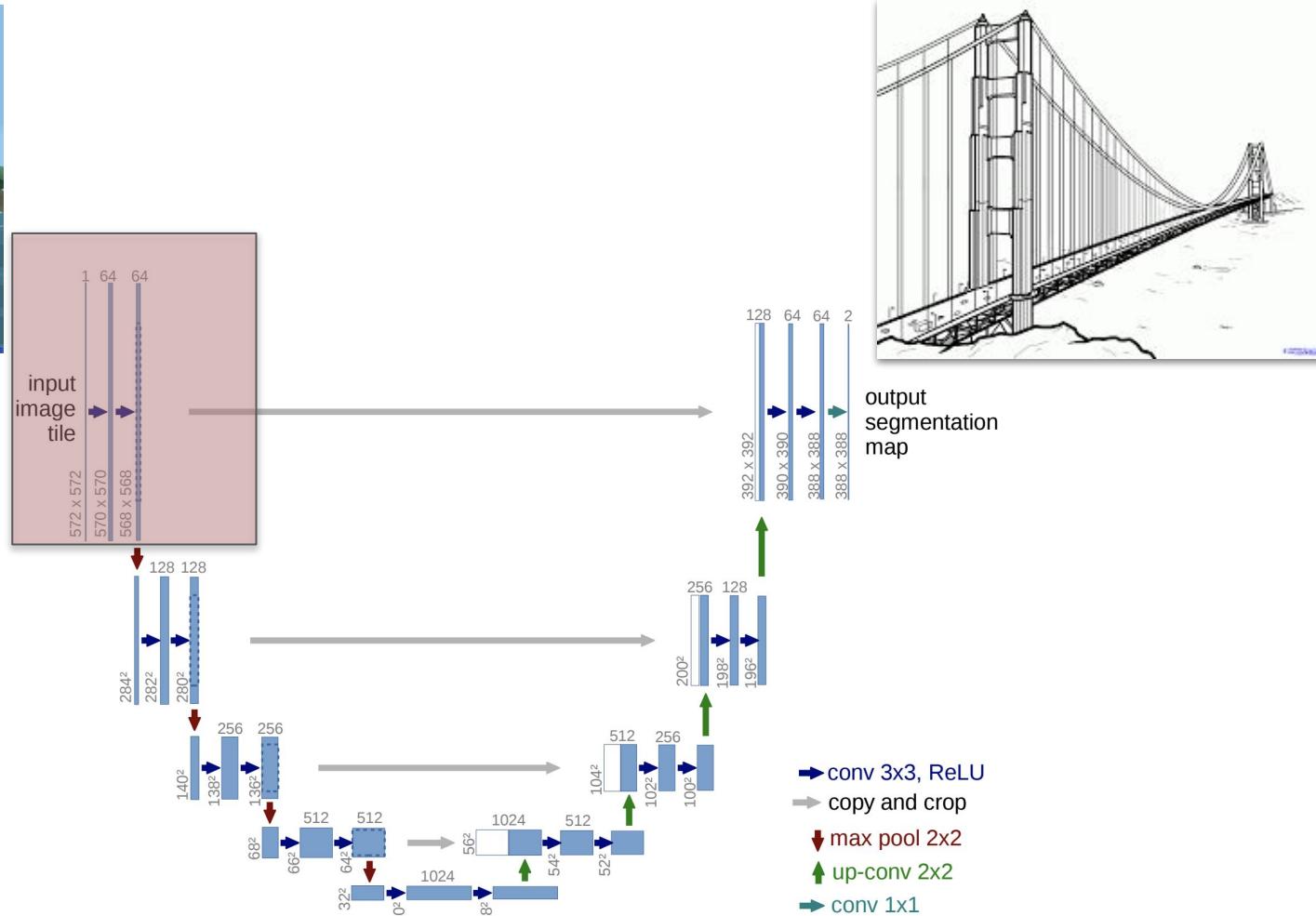
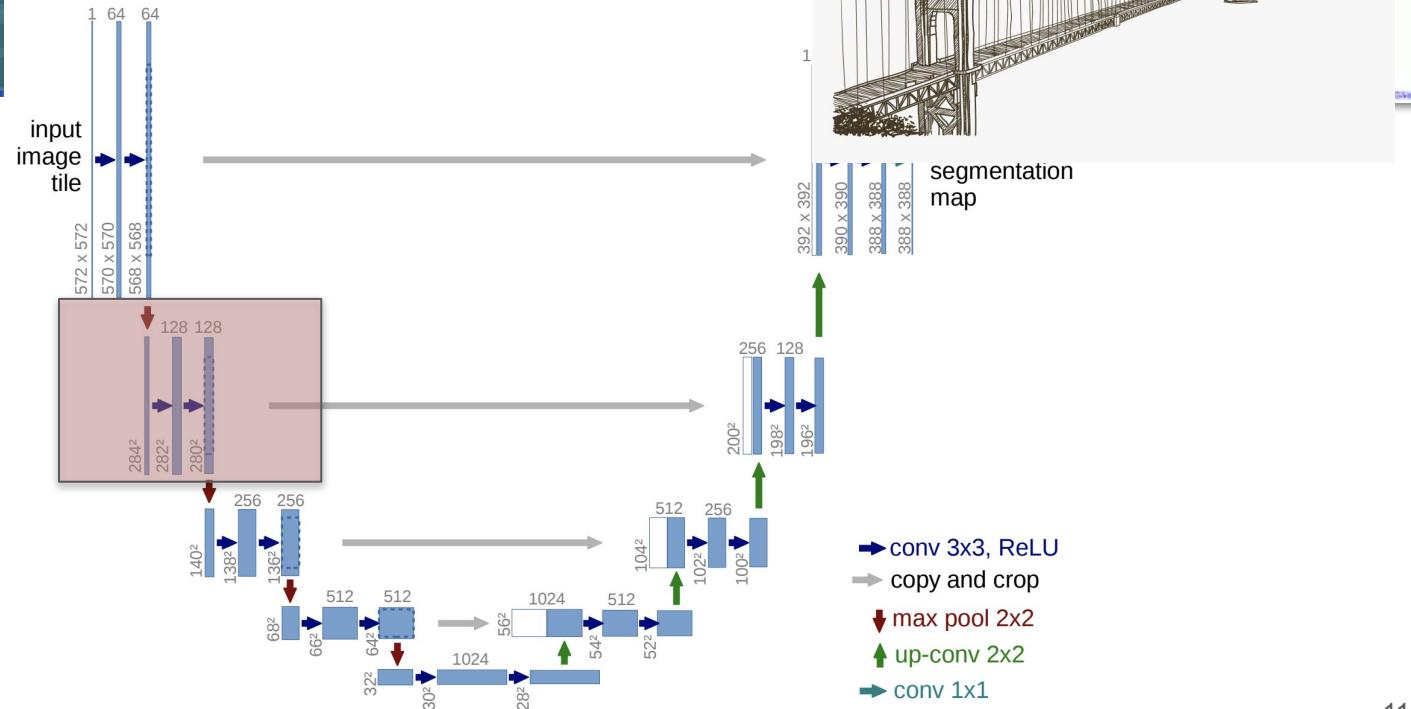


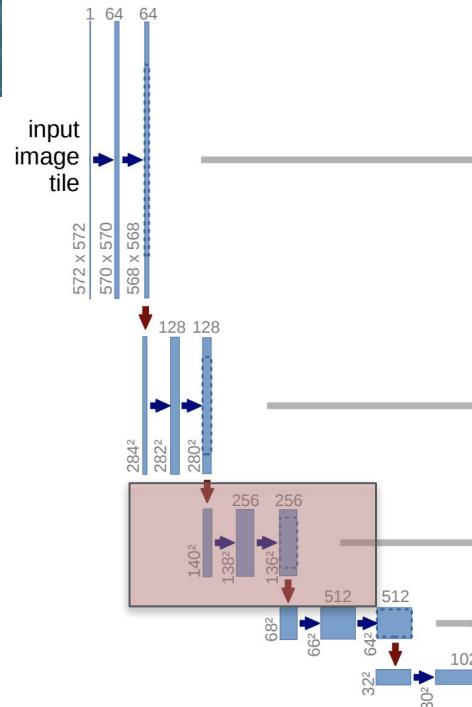
Figure 1, Ronneberger et al, 2015

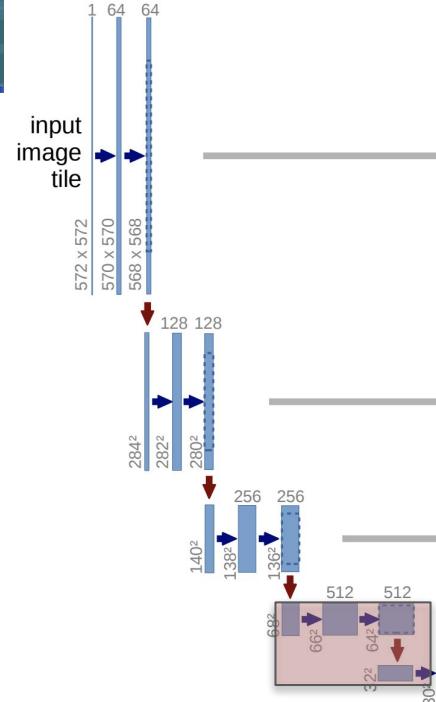




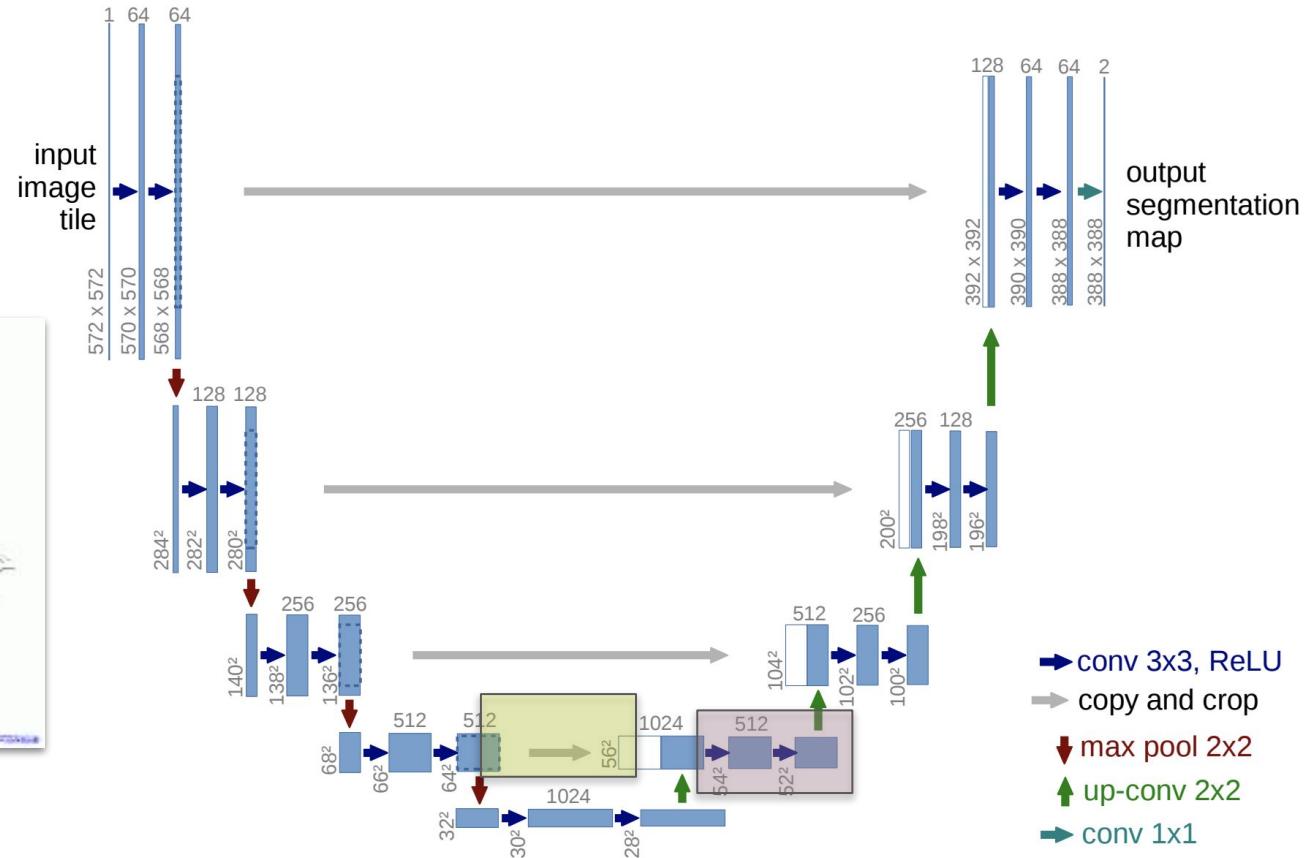
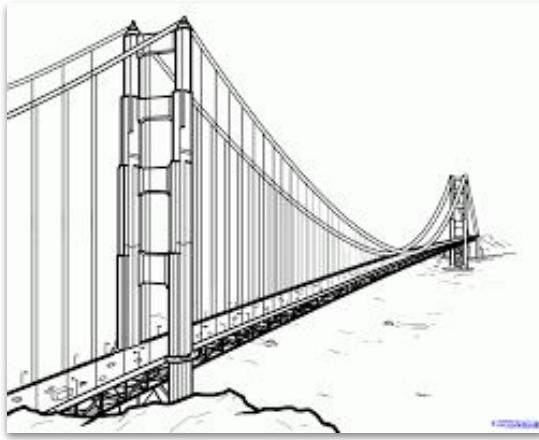


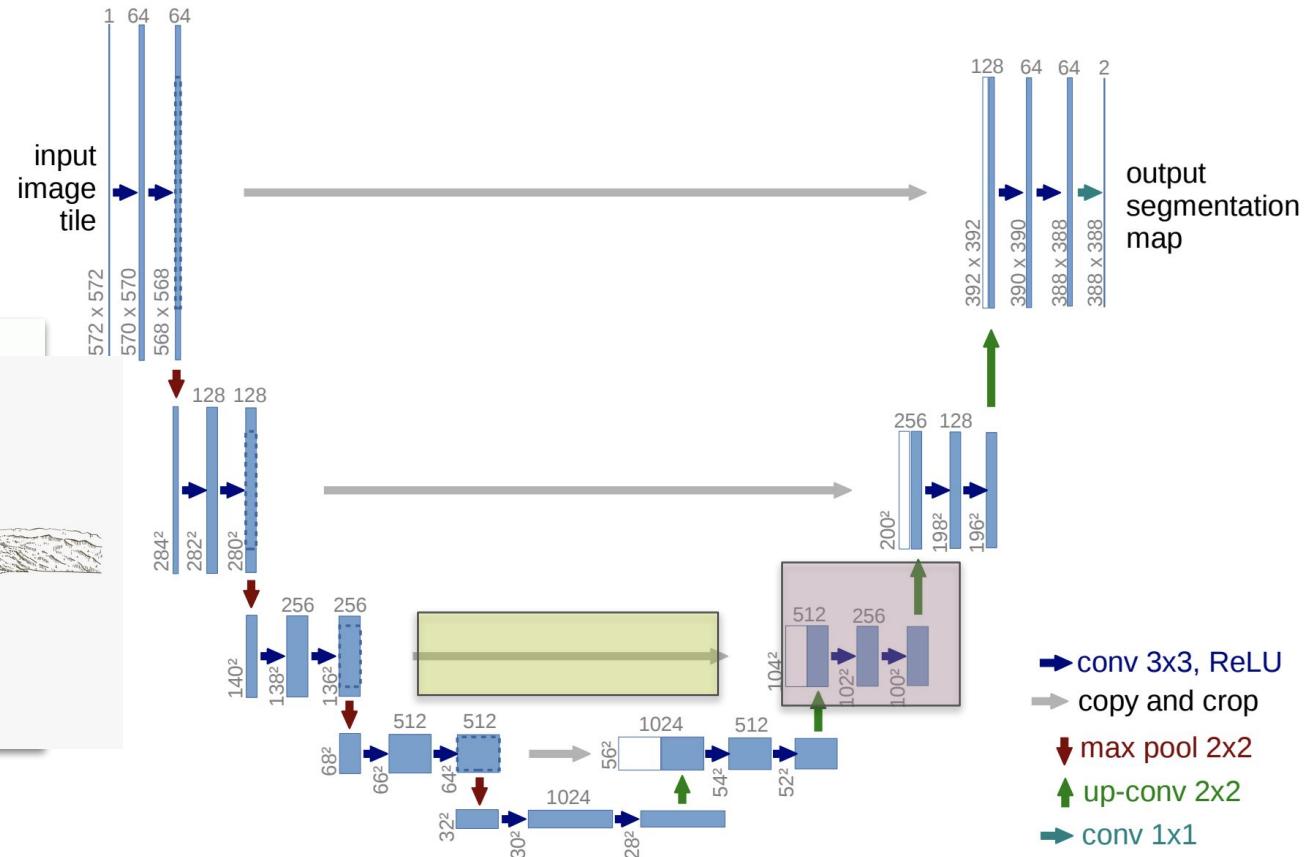
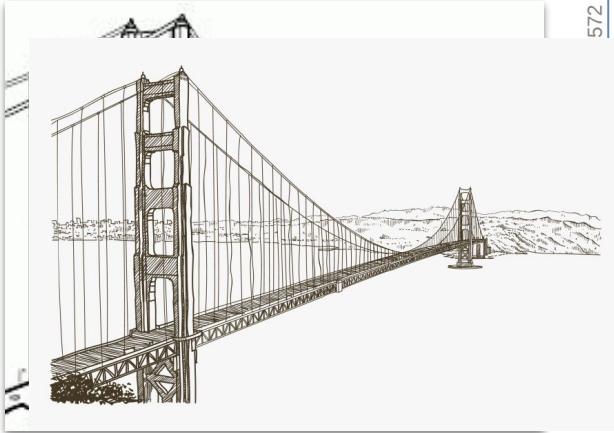


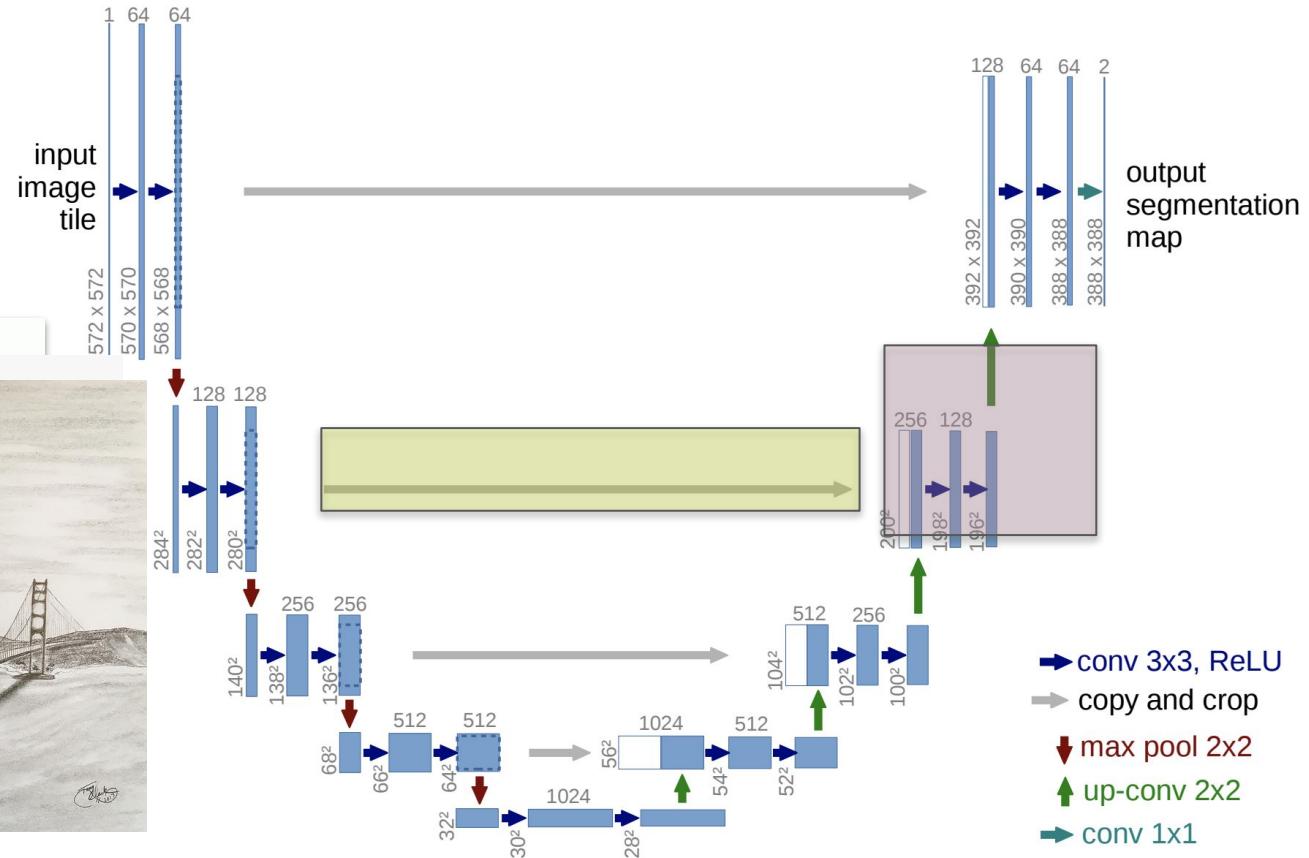


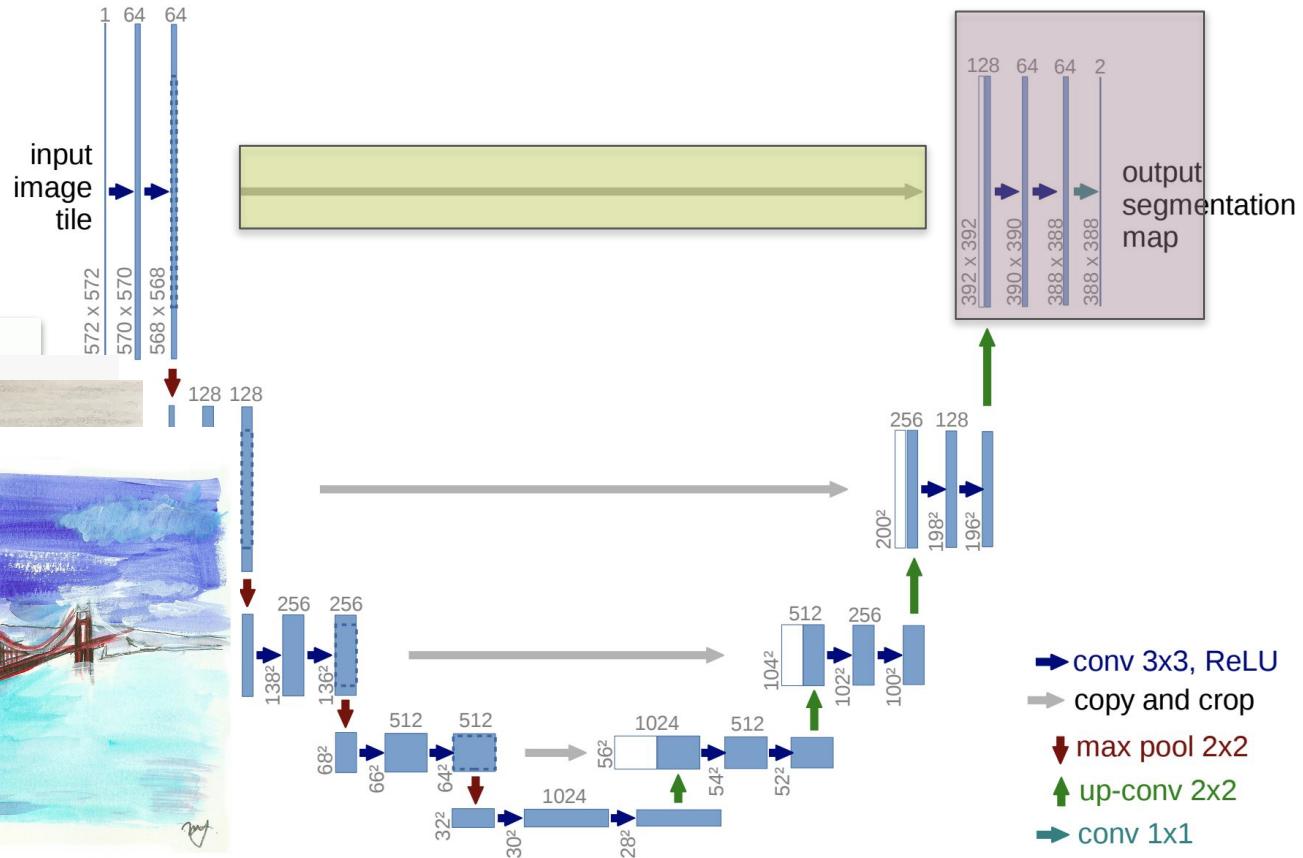
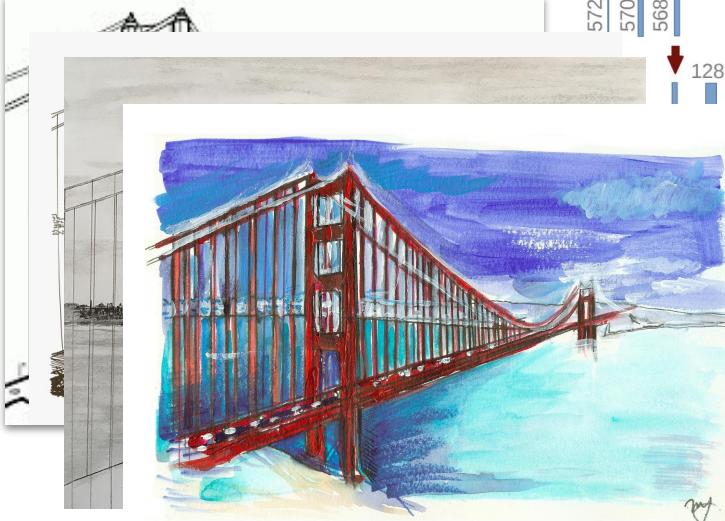










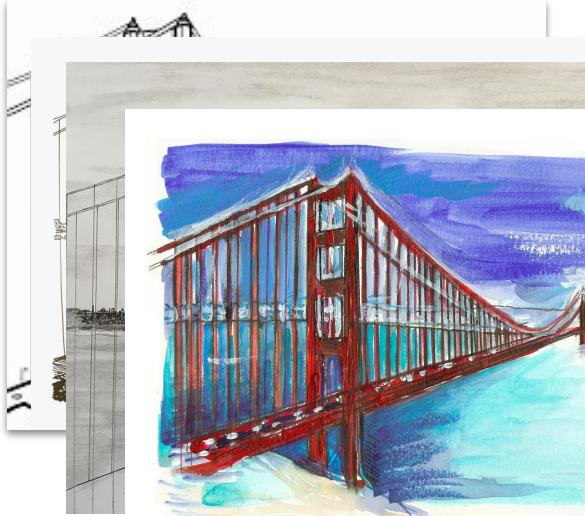




input
image
tile



n

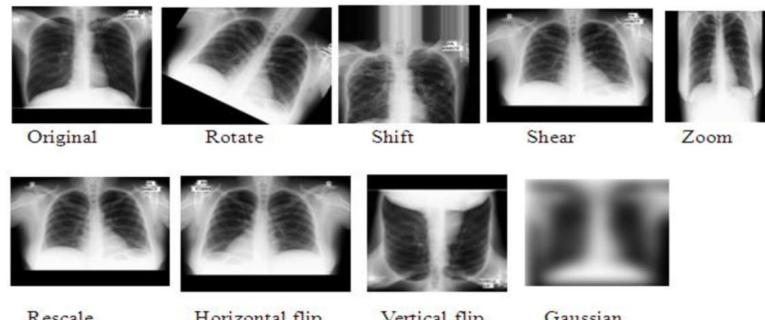


DragoArt.com



Training strategy: Data Augmentation

Teach model invariance and robustness properties

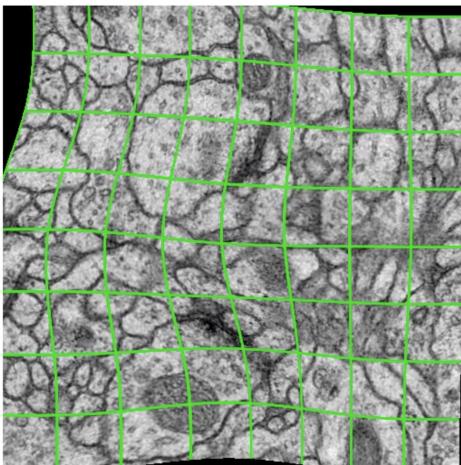


Data augmentations applied on a Chest X-ray image

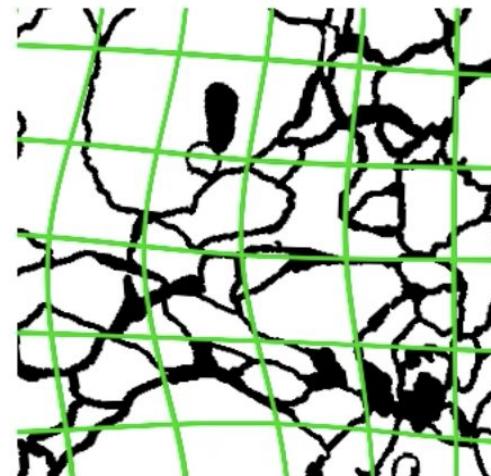
Microscopy Images: very less images in Unet paper

- **Shift and rotation invariance**
- Robustness to **deformation and gray value variations**

Data Augmentation: Random Elastic Deformation



Elastic transformation on raw image

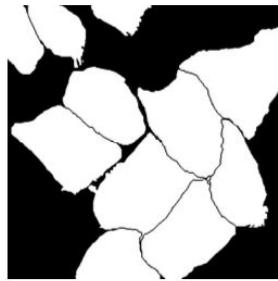


Elastic transformation on corresponding mask.

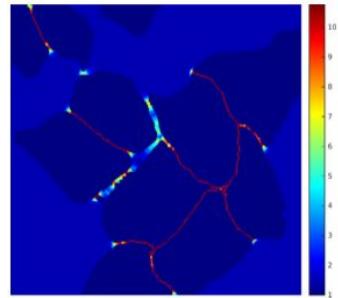


Other training strategies

- i) Touching cells: pixel-wise weighted loss



*Segmentation mask:
White(cells) and Black
(background)*



*Loss weight for each
pixel*

- ii) Favour larger input tiles over larger batch size
- iii) Good weight initialization

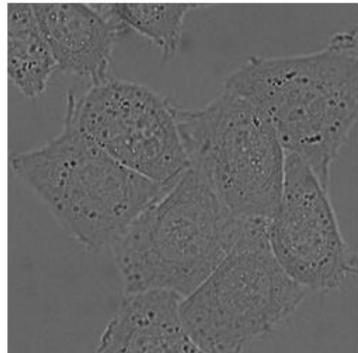


Experimental Results: Segmentation of Neuronal Structures in EM stacks

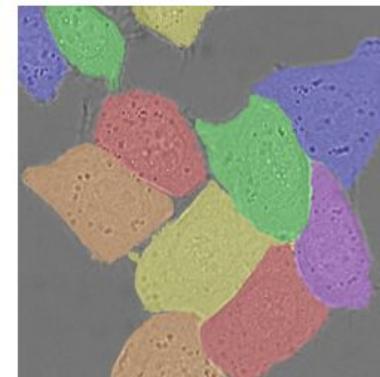
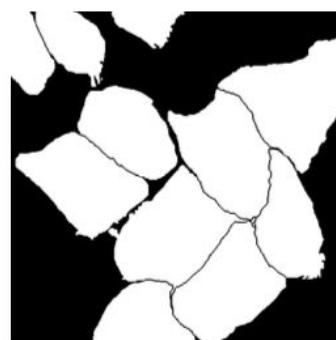
Dataset: EM Segmentation Challenge(ISBI 2012)

30 images (512x512 pixels)

Transmission electron microscopy (**TEM**) of Drosophila first instar larva ventral nerve cord (**VNC**)



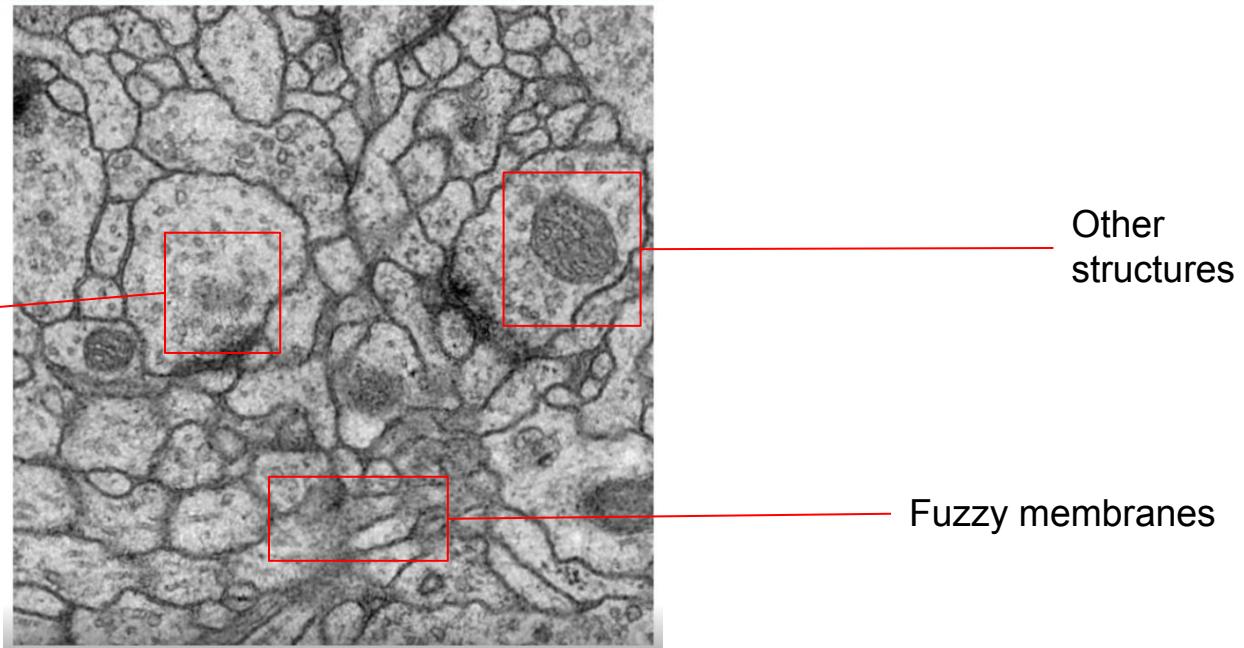
*Raw TEM
sample image*



*Overlay of ground truth on raw
image*



Challenges in the dataset



Structures with
very low
contrast

Other
structures

Fuzzy membranes

Raw image

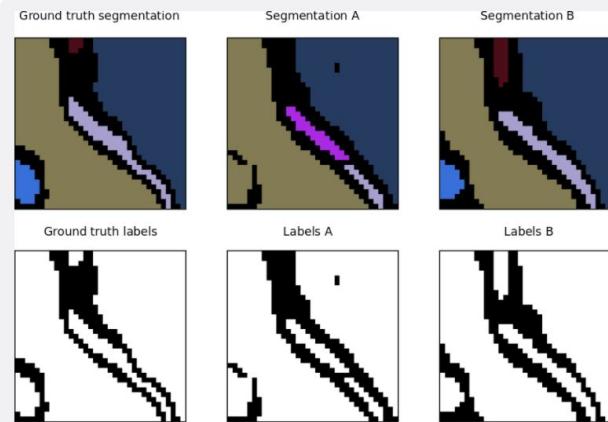


Evaluation: EM stacks

Penalizes **topological disagreements**, and used to compare the performance of boundary labellings

Rank	Group name	Warping Error	Rand Error	Pixel Error
	** human values **	0.000005	0.0021	0.0010
1.	u-net	0.000353	0.0382	0.0611
2.	DIVE-SCI	0.000355	0.0305	0.0584
3.	IDSIA [1]	0.000420	0.0504	0.0613
4.	DIVE	0.000430	0.0545	0.0582
:				
10.	IDSIA-SCI	0.000653	0.0189	0.1027

Ranking in EM segmentation challenge, sorted by warping error



Application of the topology-preserving warping error.
Example A and B have almost the same amount of pixel error with respect to the ground truth, however, example B has no topological error.

Evaluation: EM stacks

Penalizes **connectivity errors**

Compares segmentations in which regions are non-contiguous clusters of pixels

Rank	Group name	Warping Error	Rand Error	Pixel Error
	** human values **	0.000005	0.0021	0.0010
1.	u-net	0.000353	0.0382	0.0611
2.	DIVE-SCI	0.000355	0.0305	0.0584
3.	IDSIA [1]	0.000420	0.0504	0.0613
4.	DIVE	0.000430	0.0545	0.0582
:				
10.	IDSIA-SCI	0.000653	0.0189	0.1027

Ranking in EM segmentation challenge, sorted by warping error

Given 2 segmentations: S1 and S2 of image \mathbf{I} with n pixels:

$$RI = \frac{a+b}{\binom{n}{2}}$$

$$RE = 1 - RI$$

a = number of pixel pairs in \mathbf{I} that are in the **same** object in S1 as in **same** object of S2 (same label)

b = number of pixel pairs in \mathbf{I} that are in the **different** object in S1 as in **different** object of S2 (different labels)



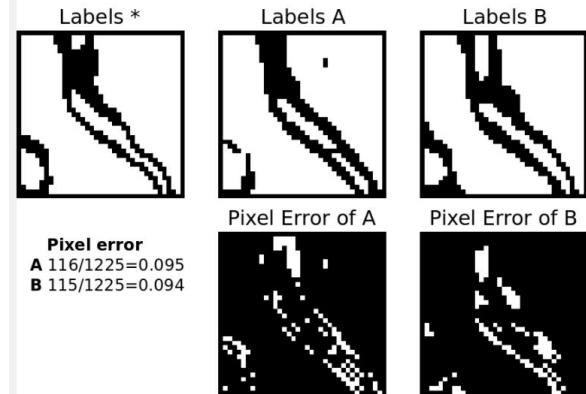
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Ranking in EM segmentation challenge, sorted by warping error

Focuses of **pixel level disagreement**

Measures pixel differences between the segmented and original image



Pixel error between two different segmentations labels (A and B) with respect to the original labels (*, ground truth).



Results: ISBI cell Tracking challenge (2014 and 2015)

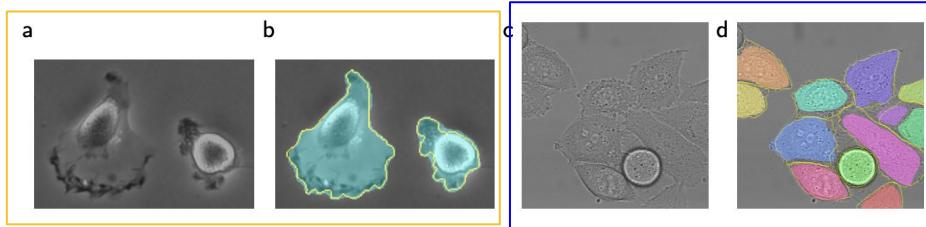


Fig. 4. Result on the ISBI cell tracking challenge. **(a)** part of an input image of the “PhC-U373” data set. **(b)** Segmentation result (cyan mask) with manual ground truth (yellow border). **(c)** input image of the “DIC-HeLa” data set. **(d)** Segmentation result (random colored masks) with manual ground truth (yellow border).

Name	PhC-U373	DIC-HeLa
IMCB-SG (2014)	0.2669	0.2935
KTH-SE (2014)	0.7953	0.4607
HOUS-US (2014)	0.5323	-
second-best 2015	0.83	0.46
u-net (2015)	0.9203	0.7756

*Segmentation results - IOU
(Intersection over union) on ISBI*

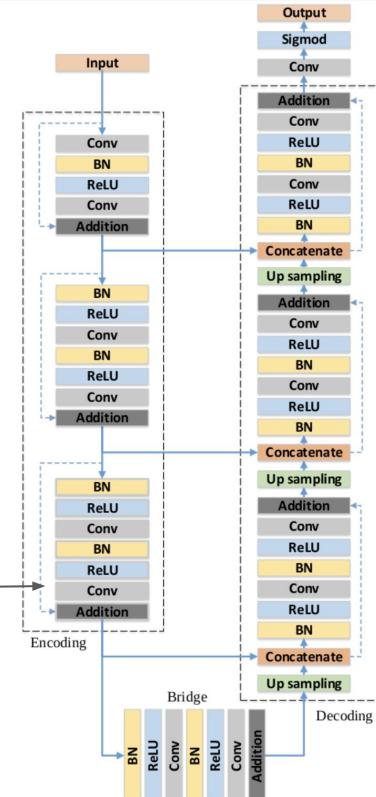
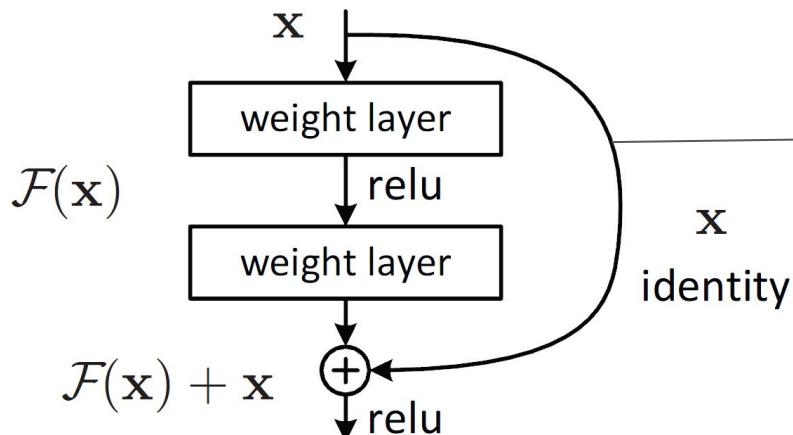
- **DIC-HeLa - 20 partially annotated training images** (DIC - Differential Inference Contrast) microscope
- **PhC-U373 - 35 partially annotated training images**, phase contrast microscopy

Limitations: U-Net's variants



a) Residual U-Net

- Residual networks are proposed to overcome the problem of Deep CNN's (vanishing gradients)
 - Residual U-Net borrows residual blocks from ResNet¹ paper
 - Train deeper networks, leading to faster convergence



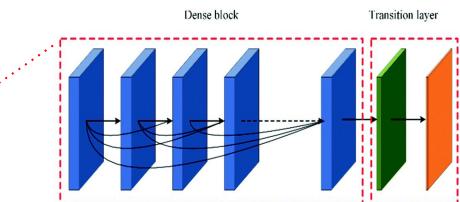
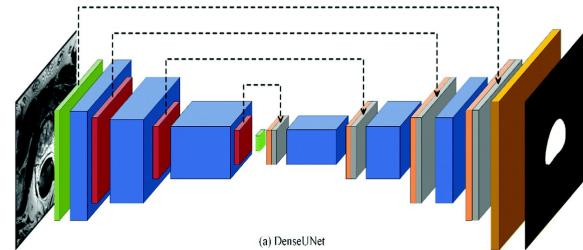
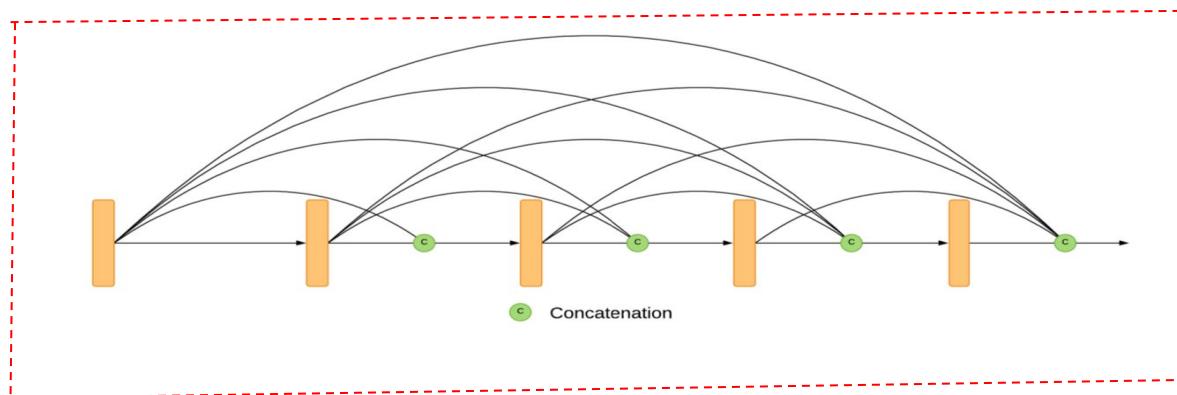
[1]: <https://arxiv.org/abs/1512.03385>

b) Dense-Unet

Dense blocks instead of Conv blocks

Dense-UNet = UNet backbone + 2 modifications

- a) Every layer receives features from previous layers
- b) Identity maps combined with channel wise concatenation



(b) Dense block and Transition layer

Operation of (a)	Operation of (b)
Conv	BN + Relu + Conv + Drop
Dense Block	2 × (BN + Relu + Conv + Drop)
Transition	AvgPooling
BN + Relu + Deconv + Drop	BN + Relu + Deconv + Sigmoid
Concat	

Summary

- Unet makes accurate biomedical semantic segmentations feasible with few training examples
- Encoder captures context, while decoder helps in maintaining localization
 - (localization and use of context at same time)
- Fast inference (1s per image)
- Training strategies
 - data augmentations
 - pixel-wise weighted loss (seems to be key concepts to train network with few images)



Limitations (addressed by other architectures):

- Residual Unet: Train larger models (skip connections)
- Dense Unet: Every layer has contextual information, better segmentation accuracy

Limitations (Our point of view)

- a) Determining the **depth** of the network **apriori** is difficult (ablation study was missing)
- b) Data Augmentation: how to select the transformation that are suited for a given task?
- c) Missing ablation studies for the pre-processing / post processing in EM stacks evaluation
- d) Why not dice loss for training the network?

Thank You :)

Questions?!

