

Outline:

- Problem setup
- Data processing Efrén
- Classification Denny
- Future Work Yonghua

Study Team

Initially Sponsored By Dr. Benzi Kluger Of UCH-Neurology

Keeran Maharaj - Research

Part Of Larger Study To Improve Parkinson's Treatment

Recently Joined By Debashis Ghosh Of UCH Bioinformatics

Efren Cruz Cortés - Machine Learning

Yonghua Zhuang - Machine learning - Biostatistics PhD student

Dennis Graham - Data Science - Programmer

Introduction

Goal Is To Develop An Inexpensive And Reliable Parkinson's Disease Diagnostic

Parkinson's Difficult To Diagnose Because Of Imposters

Mild Cognitive Impairment MCI

Essential Tremor ET

Parkinson's Dementia PD+

Parkinson's PD

What is MEG?

Measures magnetic fields of the brain

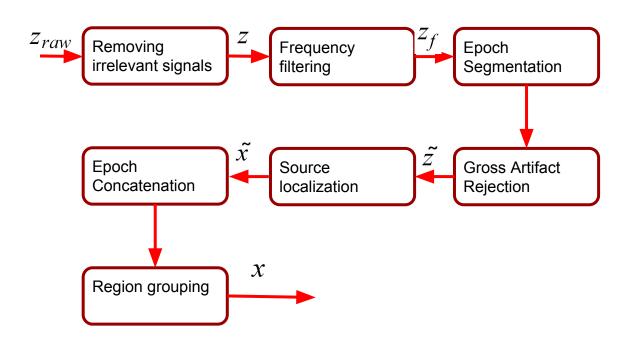
Array of magnetometers outside skull

Similar to EEG



Image from Wikimedia

Preprocessing flowchart



Removing Irrelevant Signals That May Be Relevant

- Independent Component Analysis
- Eyeblink and heartbeat signatures are examples but 'temporal muscle activity' is included.
- Software: EEGLAB

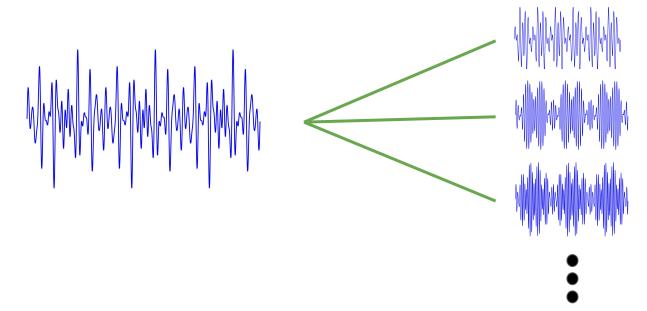
Comments:

Eyeblink and temporal muscle activity patterns will differ from PD to non-PD patients. Make sure relevant signal is not removed or do not use.

From EEGLAB documentation: The quality of the data is critical for obtaining a good ICA decomposition. ICA can separate out certain types of artifacts -- only those associated with fixed scalp-amp projections. These include eye movements and eye blinks, temporal muscle activity and line noise.

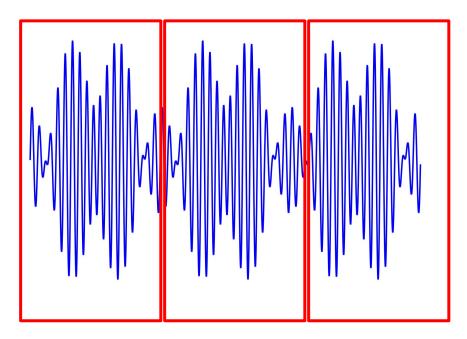
Frequency Filtering

- Bandpass filter over 5 frequency bands:
- [4,8], [8,10], [10-13], [13-30], [30-56] ("brain waves"- delta, alpha, etc.)



Epoch segmentation

- Segment into 5 second epochs
- Allows for removal of artifacts

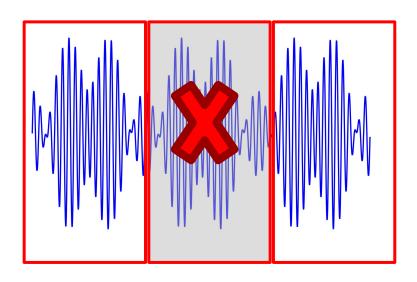


Gross artifact rejection

Delete epochs where gross artifacts (e.g. head bump) are identified

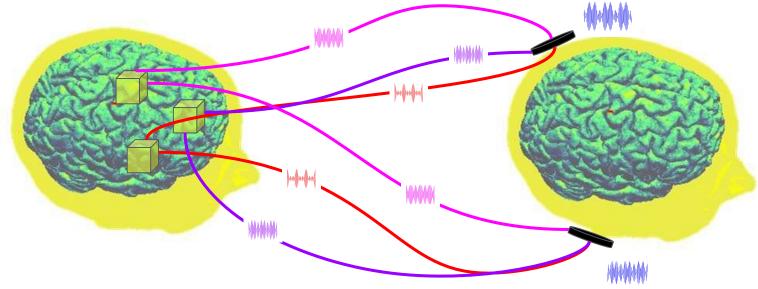
Questions:

Deleted epochs are replaced by ?



Source localization

- Blind Source Separation Problem (similar to ICA)
- Recover brain region signals from sensor signals



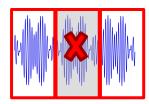
Brain Image Courtesy of Luis Gomez, Duke University

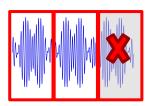
Epoch concatenation

Concatenate surviving epochs

Questions:

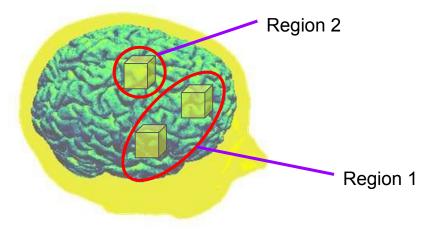
How are patients commensurate after asynchronous concatenation?





Region grouping

- From source localization obtain MNI coordinates
- From MNI coordinates obtain brain region (e.g. premotor gyrus)
- 87 neural regions



Preprocessed data - final form

For each patient, 5 sets of 87 matrices, each corresponding to a neural region, with time signal of points in that region. Each set is a frequency band.



Development Process

Small Sample Of 90 Including PD,PD+,ET,MCI Plus Control Samples

Initially The MEG Data Was Processed Using EEGLAB

No Classification Results Could Be Achieved

Decision To Apply Machine Learning

SVM, Random Forests, Logistic Regression Failed To Classify

Decision To Apply Neural Networks

Results Achieved With Dense ANN

Preprocessing Inhibits AI Processing

Inherent Part Of This Study But To Be Deleted In Future Study

Uses Standard Signal Processing Based On Frequency

Preprocessing Removed Data That Could Be Used By Al Techniques

Al Uses Time Dependent Events

PD IS A MOVEMENT DISORDER THAT IS ERRATIC

Expectation Should Be That Symptoms Generate Time Dependent Signals

In Different Brain Regions

That Are Random And Appear As Irrelevant Artifacts

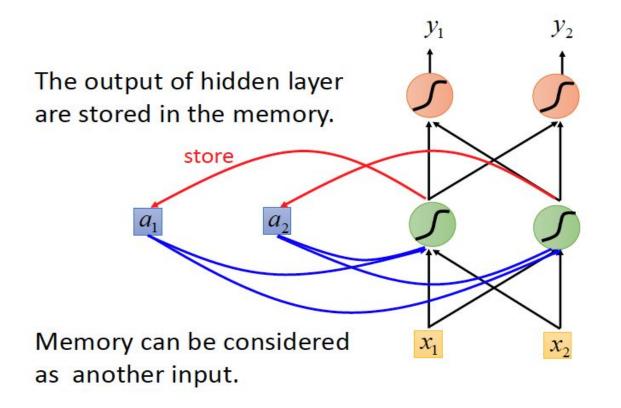
Future directions

> Long short-term memory Neural Network (LSTM)

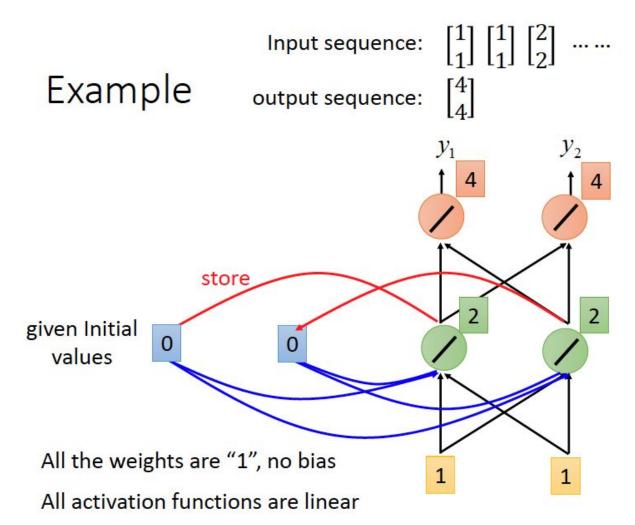
> CNN with LSTM

➤ LSTM with Soft Attention model

Recurrent Neural Network (RNN)

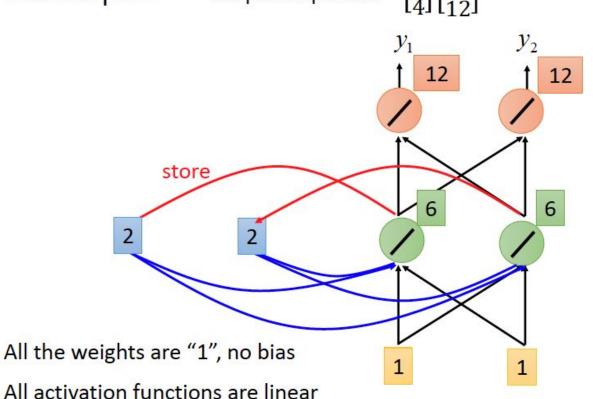


Hung-yi Le. Deep learning Tutorial. 2017.



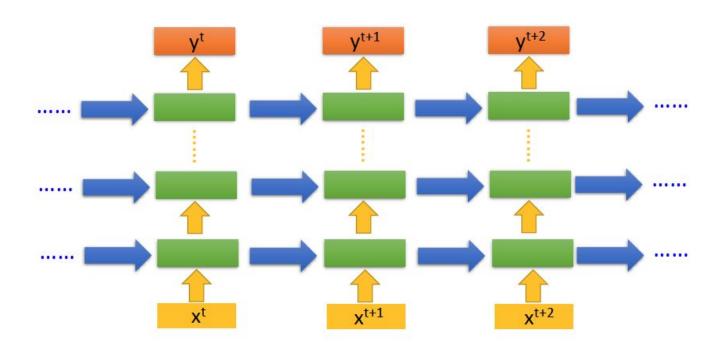
Example

Input sequence: $\begin{bmatrix} 1\\1 \end{bmatrix} \begin{bmatrix} 1\\1 \end{bmatrix} \begin{bmatrix} 2\\2 \end{bmatrix} \dots \dots$ output sequence: $\begin{bmatrix} 4\\4 \end{bmatrix} \begin{bmatrix} 12\\12 \end{bmatrix}$

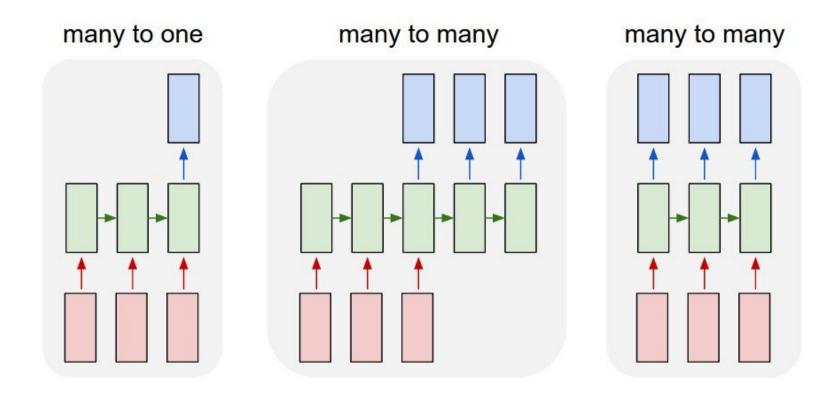


 $\begin{bmatrix} 1 \\ 1 \end{bmatrix} \begin{bmatrix} 1 \\ 1 \end{bmatrix} \begin{bmatrix} 2 \\ 2 \end{bmatrix}$ Input sequence: Example output sequence: Changing the sequence 12 12 order will change the output. store All the weights are "1", no bias All activation functions are linear

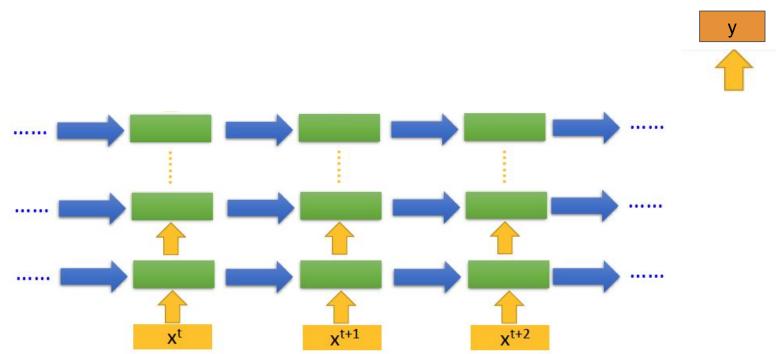
Of course it can be deep ...



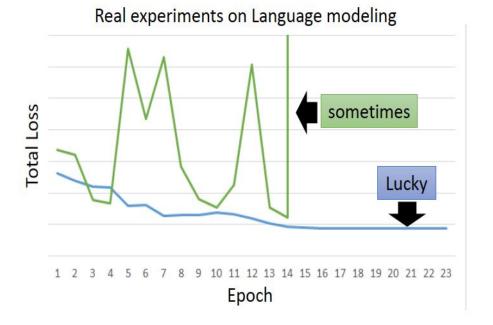
Recurrent Neural Networks



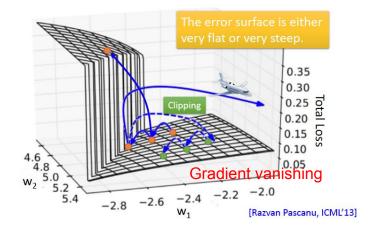
Recurrent Neural Networks (Many to one)



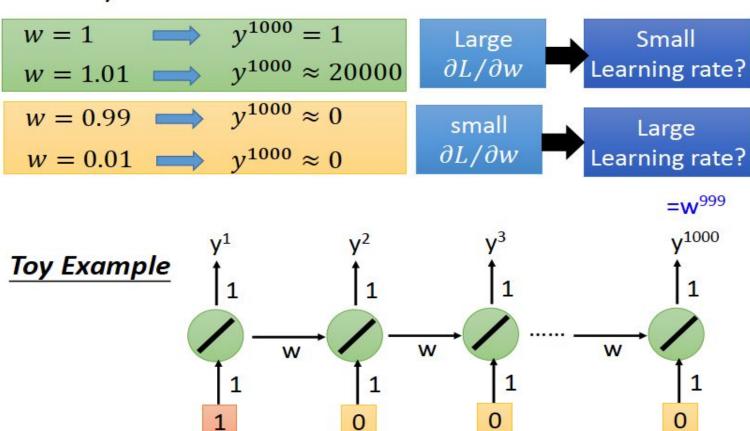
RNN-based network is not always easy to learn



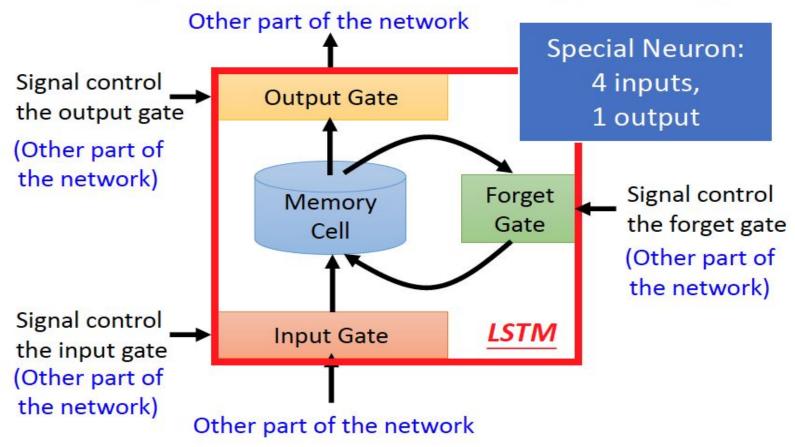
The error surface is rough.

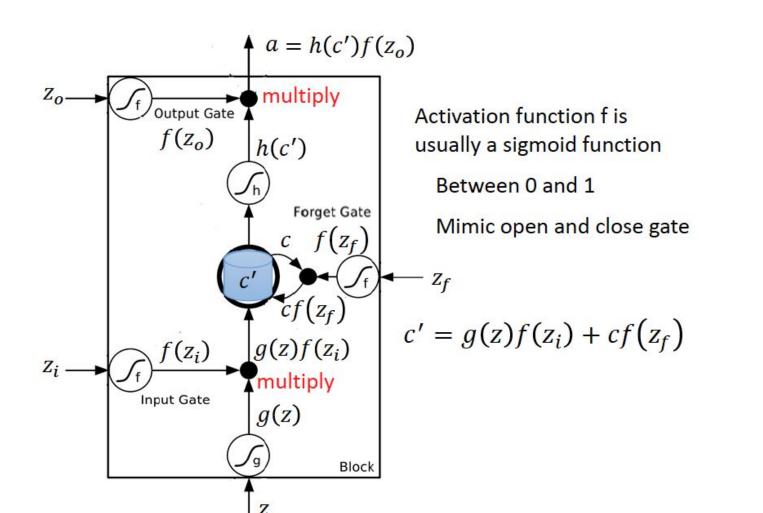


Why?

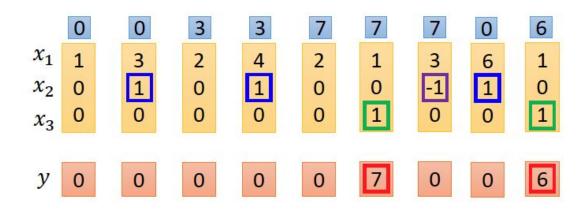


Long Short-term Memory (LSTM)

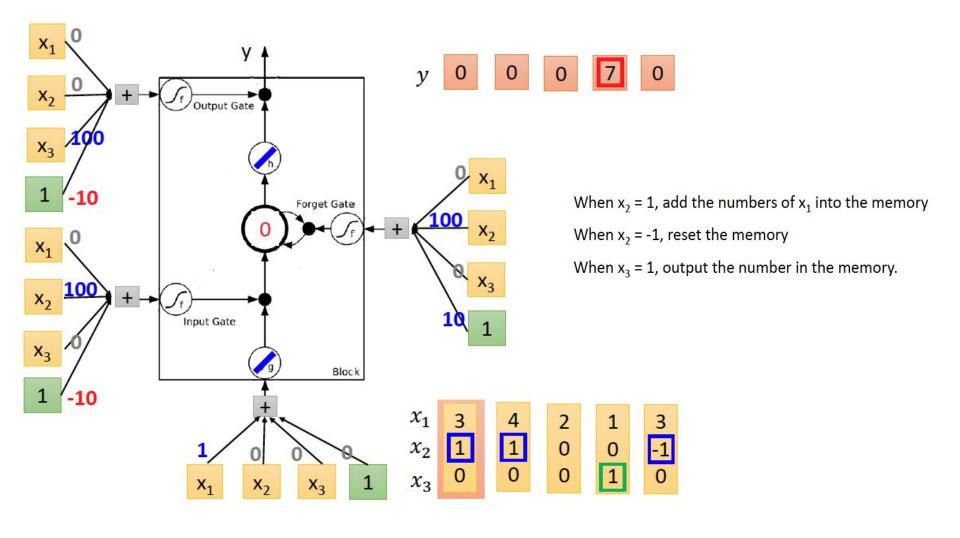


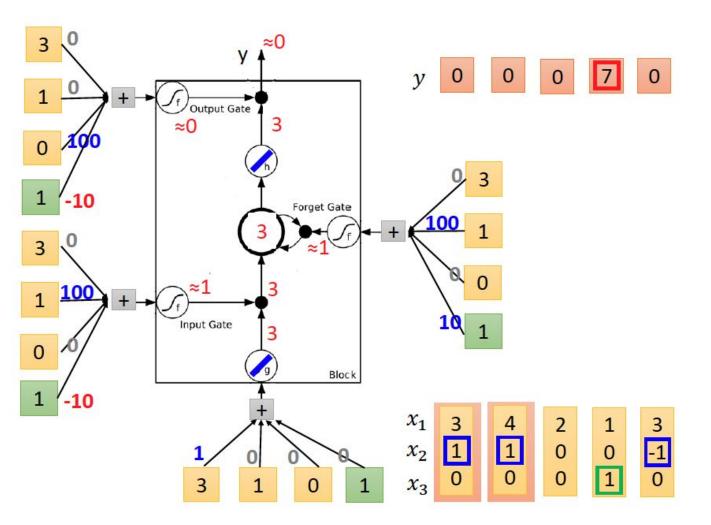


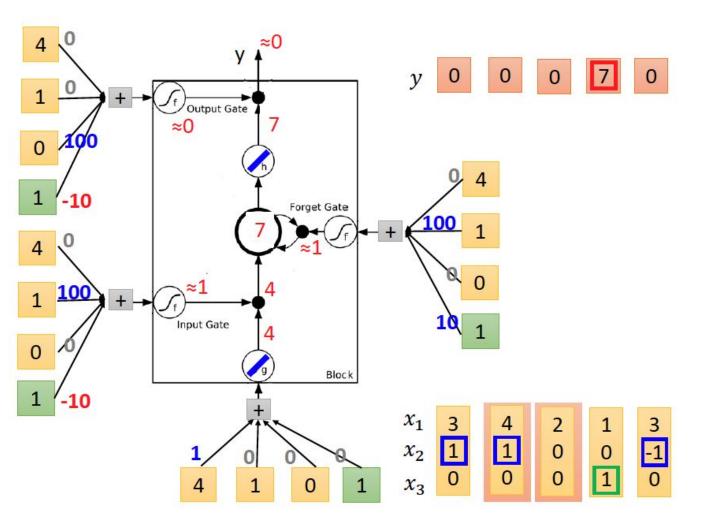
LSTM - Example

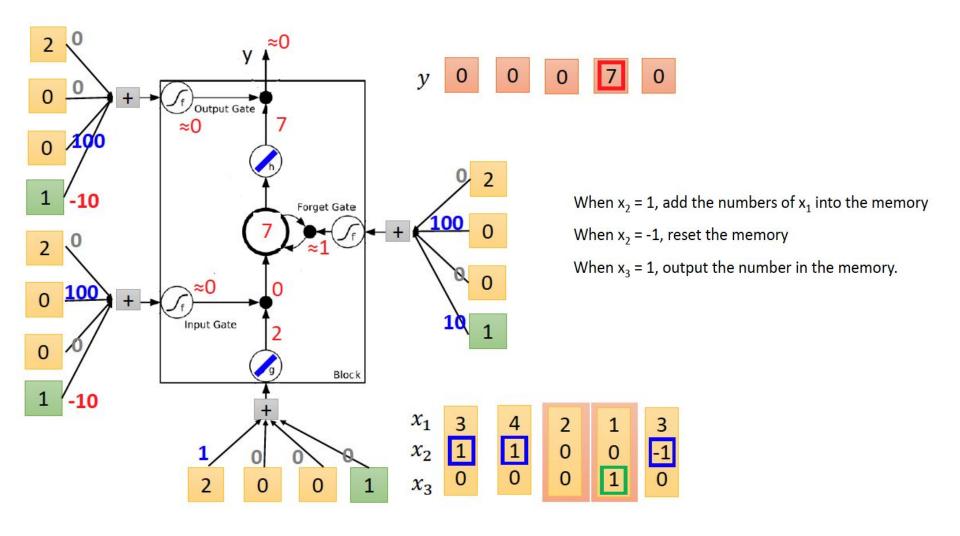


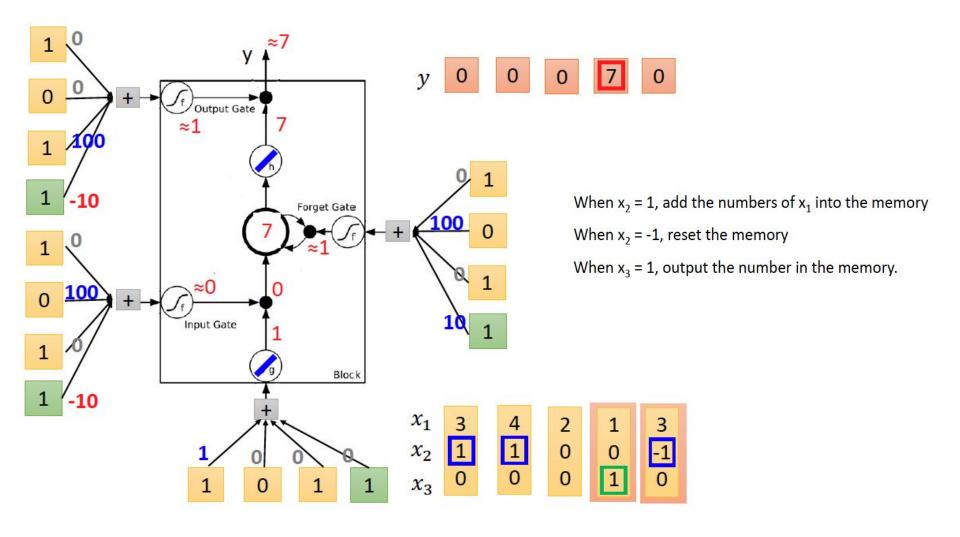
When $x_2 = 1$, add the numbers of x_1 into the memory When $x_2 = -1$, reset the memory When $x_3 = 1$, output the number in the memory.

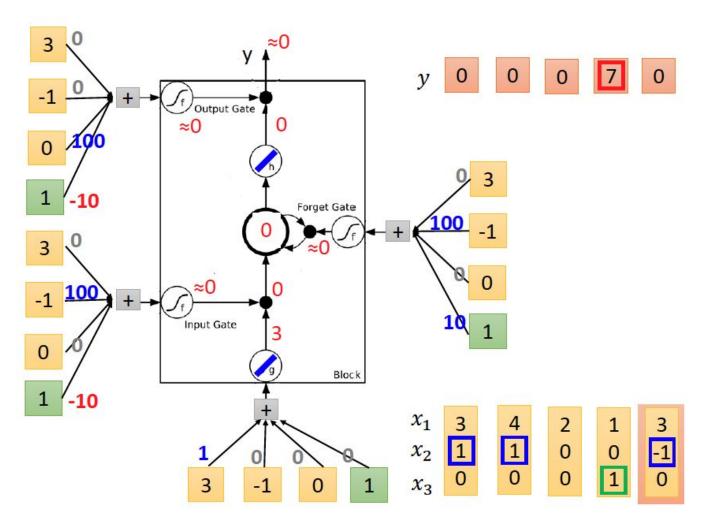


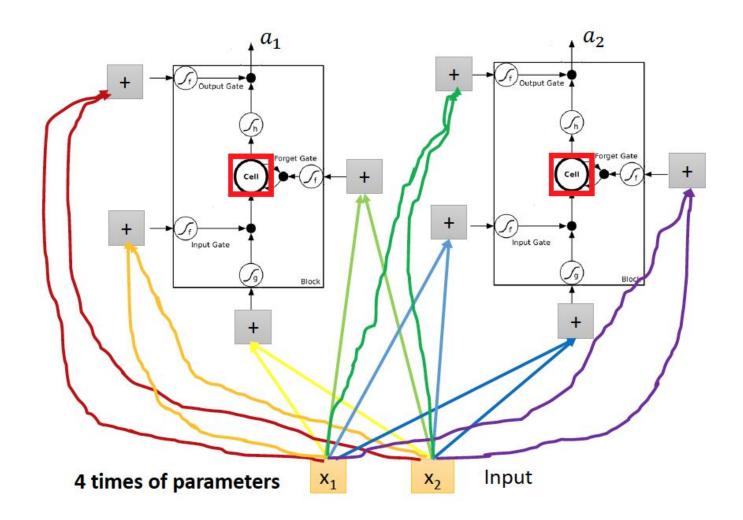












Long Short-term Memory (LSTM)

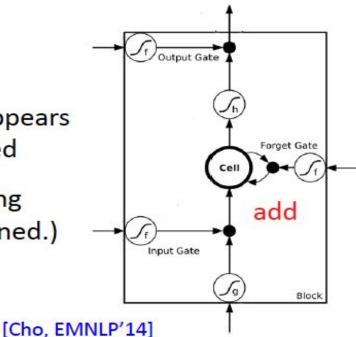
Can deal with gradient vanishing (not gradient explode)

- Memory and input are added
- ➤ The influence never disappears unless forget gate is closed



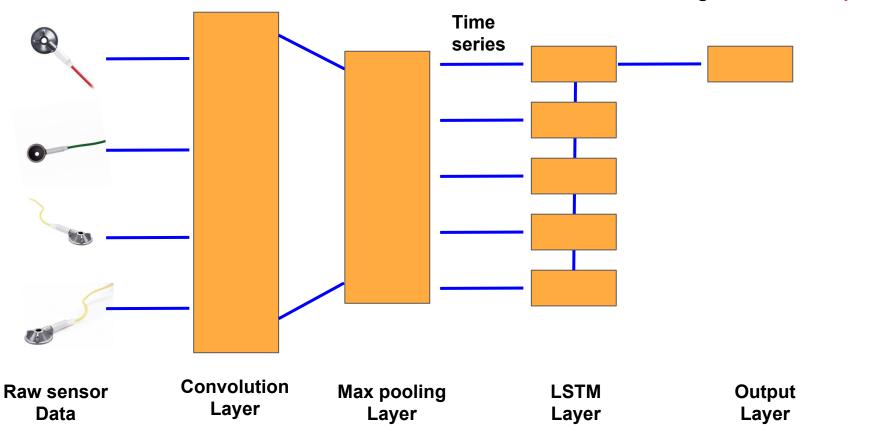
No Gradient vanishing (If forget gate is opened.)

Gated Recurrent Unit (GRU): simpler than LSTM



CNN with LSTM

Regularization: dropout



A few words about attention model

- Attention involves focus of certain parts of input;
- > Types of attention: soft/hard attention;
- ➤ Models:

LSTM with soft attention (add extra attention layer);

Simple attention model.