

X-Ray Fokker-Planck Equation

Fundamentals

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Conventional X-Ray Imaging

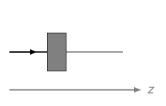


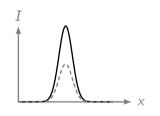
[American Society for Surgery of the Hand, 2015]



Conventional X-Ray Imaging

Attenuation of the X-Ray beam







adapted from [Morgan et al., 2019]

[Bech et al., 2013]



X-Ray Imaging: Complementary Modalities

Attenuation Image



[Bech et al., 2013]

Phase-Contrast Image



[Bech et al., 2013]

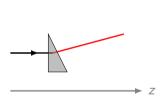
Dark-Field Image

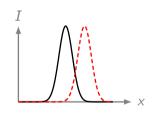


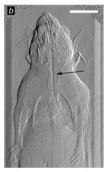
[Bech et al., 2013]



Phase Shift caused by soft tissues





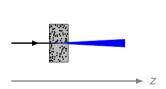


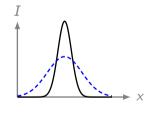
adapted from [Morgan et al., 2019]

[Bech et al., 2013]



Dark-Field Signal resulting from unresolved, sub-pixel structures



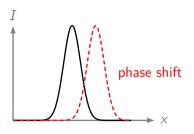


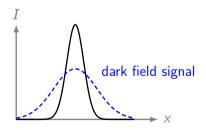
adapted from [Morgan et al., 2019]

[Bech et al., 2013]



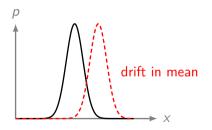
- detector can only measure intensities
- mathematical model required to extract phase shift and dark-field signal

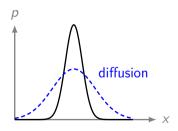






- integrated intensity conserved post sample
- analogous to a probability distribution







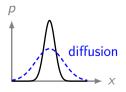
Fokker-Planck Equation

Time-evolution of probability distribution p(x, t):

$$\partial_t p = \boxed{-\partial_x \left[D_1 p\right]} + \boxed{\partial_x^2 \left[D_2 p\right]}$$

- drift velocity $D_1(x, t)$
- diffusion coefficient $D_2(x, t)$







Fokker-Planck Equation

Applications:

- Brownian motion
- hydrodynamics
- electron and photon transport in biological tissues
- gaseous micro-flows
- droplet nucleation
- X-ray imaging

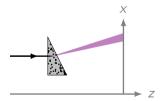


X-Ray Fokker-Planck Equation

Modification from time-evolution $\partial_t p$ to intensity change $\partial_z I$:

$$\partial_t p = \boxed{-\partial_x \left[D_1 p\right]} + \boxed{\partial_x^2 \left[D_2 p\right]} \longrightarrow \boxed{\partial_z I = \boxed{-\frac{1}{k} \partial_x \left[I \partial_x \phi\right]} + \boxed{\partial_x^2 \left[D(z)I\right]}}$$

- t: change over propagation distance z
- p: beam intensity I
- D_1 : phase shift $\frac{1}{k}\partial_x\phi$
- D_2 : "linear" diffusion coefficient D(z)





X-Ray Fokker-Planck Equation

1-dimensional detector signal:

$$\partial_z I = \boxed{-rac{1}{k}\partial_x \left[I\partial_x\phi
ight]} + \boxed{\partial_x^2 \left[D(z)I
ight]}$$

2-dimensional detector signal:

$$\partial_z I = \boxed{-rac{1}{k}
abla_\perp \left[I
abla_\perp \phi
ight]} + \boxed{
abla_\perp^2 \left[D(z) I
ight]}$$

- Transport-of-intensity equation
- diffusion term



Transport-of-Intensity Equation

Homogeneous **Helmholtz-Equation** for a monochromatic wave ψ_{ω} :

$$\left(\nabla^2+k^2\right)\psi_\omega=0$$

Paraxial Approximation:

$$\psi_{\omega} = \Phi e^{ikz}$$

- $\Phi(x, y, z)$: complex envelope with slow z-variation such that $\partial_z^2 \Phi = 0$
- e^{ikz} : oscillatory plane wave behaviour



Paraxial Wave Equation:

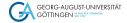
$$\left(2ik\partial_z^2 + \nabla_\perp^2\right)\Phi = 0$$

Projection Approximation:

$$\Phi = \sqrt{I}e^{i\phi}$$

- no diffraction / scattering within the (thin) sample
- $\sqrt{I(x, y, z)}$: amplitude
- $\phi(x, y, z)$: phase

$$\partial_z I = -rac{1}{k}
abla_\perp \left[I
abla_\perp \phi
ight]$$



X-Ray Fokker-Planck Equation

Transport-of-Intensity Equation

$$\partial_z I = \boxed{-rac{1}{k}
abla_\perp \left[I
abla_\perp \phi
ight]}$$

• energy conservation under coherent x-ray energy transport

Diffusion Term

$$\partial_z I = \nabla^2_{\perp} [D(z)I]$$

 energy conservation under diffusive x-ray energy transport

Constant (Noether) Charge: integrated intensity

$$\mathfrak{N} = \iint I(x, y, z) \, \mathrm{d}x \, \mathrm{d}y$$



Transport-of-Intensity Equation

$$\partial_{\mathsf{z}} I = igc| -rac{1}{k}
abla_{\perp} \left[I
abla_{\perp} \phi
ight]$$

Diffusion Term

$$\partial_z I = \boxed{
abla_\perp^2 \left[D(z) I \right] }$$

Conserved (Noether) Current:

transverse Poynting vector

Fick's first law of diffusion

$${f J}_{ot}^{(1)}\equivrac{1}{k}I
abla_{ot}\phi$$

$$\mathbf{J}_{\perp}^{(2)}\equiv-
abla_{\perp}\left[D(z)I
ight]$$

Continuity Equation:

$$\partial_z I = -
abla_\perp \left(\mathbf{J}_\perp^{(1)} + \mathbf{J}_\perp^{(2)}
ight) = -
abla_\perp \mathbf{J}_\perp$$

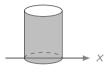
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Application to Forward Problems

Phase-Contrast Image

$$\partial_{\mathsf{z}} I = iggl[-rac{1}{k} \partial_{\mathsf{x}} \left[I \partial_{\mathsf{x}} \phi
ight]$$



Transport-of-intensity equation: finite difference

$$I(z=\Delta) = I(z=0) - rac{\Delta}{k} \Big(\partial_{\mathsf{x}} I \cdot \partial_{\mathsf{x}} \phi + I \cdot \partial_{\mathsf{x}}^2 \phi \Big)$$

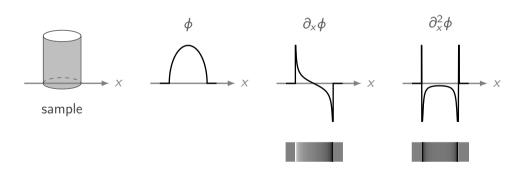
• intensity at small distance Δ from sample



Phase-Contrast Image

$$I(z = \Delta) = I(z = 0) - \frac{\Delta}{k} \left(\partial_{\mathsf{x}} I \cdot \boxed{\partial_{\mathsf{x}} \phi} + I \cdot \boxed{\partial_{\mathsf{x}}^2 \phi} \right)$$

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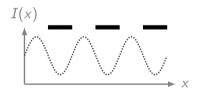
Phase Effects

$$I(z=\Delta)=I(z=0)-rac{\Delta}{k}\Big(\partial_{x}I\cdot\partial_{x}\phi+I\cdot\partial_{x}^{2}\phi\Big)$$

Detector image: sinusoidal illumination

$$I(x) = a \sin\left(\frac{x}{p}\right) + b$$

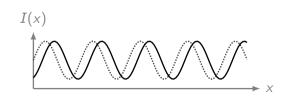
- prism effects
- focusing effects
- edge effects





Prism Effect





$$\partial_{\mathsf{x}}\phi>0$$

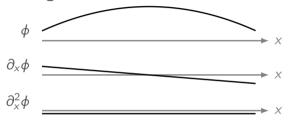
ullet Shift o

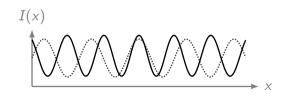
$$\partial_x^2 = 0$$

- Mean unchanged
- Period unchanged



Focusing Effect





$$\partial_{\mathsf{x}}\phi>0$$

$$\partial_{\mathsf{x}}\phi<0$$

$$ullet$$
 Shift o

• Shift
$$\leftarrow$$

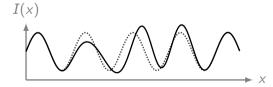
$$\partial_x^2 < 0$$

- Mean ↑
- Period J



Edge Effect





$$\partial_x < 0$$

• Shift \rightarrow

$$\partial_x^2 \phi > 0$$

$$\partial_x^2 \phi < 0$$

Mean ↓

Mean ↑

Period ↑

• Period J

➤ X



Dark-Field Effects

Scattering Edge

$$\partial_z I = \left[\partial_x^2 \left[D(z)I\right]\right]$$

sample



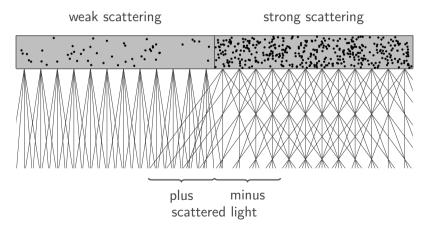
Diffusion equation: finite difference

$$I(z = \Delta) = I(z = 0) + \Delta \left(\partial_x^2 [D(z)I]\right)$$

• intensity at small distance Δ from sample



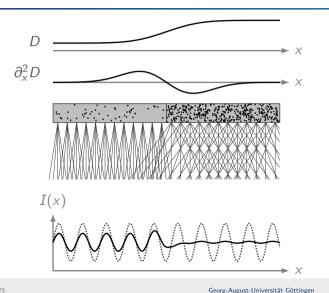
Scattering Edge



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Visibility ↓

$$\partial_x^2 = 0$$

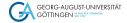
• Mean unchanged

$$\partial_x^2 > 0$$

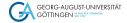
$$\partial_x^2 < 0$$

Mean ↑

Mean ↓



Thank you for your attention!



References I



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References II



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References III



Morgan, K. S. and Paganin, D. M. (2019).

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