

# Super-Resolution of Degraded Low-Resolution X-Ray Images Using a Novel Patch-Based Generative Adversarial Network

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In this work, we propose a patch-based generative adversarial network for super-resolution of degraded low-resolution X-ray images. The generated super-resolution X-ray images showed a structural similarity of 0.85 to the source X-ray images. Our model, XPGAN, outperforms interpolation techniques in reconstructing image detail and shows promise in recovering edges in degraded images. It also allows for memory efficient computation without sacrificing image fidelity. The network was trained and tested for X-ray images which were smoothed and downsampled by a factor of 4, corresponding to a 16x reduction in radiation dose. This method allows for the reconstruction of high-resolution X-rays from lower dose X-ray images. This could help reduce the cost of X-rays while minimizing radiation exposure.

# Background



Left: High-resolution (HR) X-ray; Right: Low-resolution (LR) X-ray

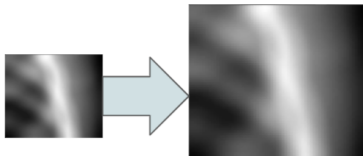
- Lower the resolution, lower the pathological detail
- Higher resolution requires higher radiation dose
- Need a way to increase resolution of low-dose X-rays

## Another Problem - Converting CT data to X-Rays

- CT resolution -  $1 \times 1 \times 1$  mm
- X-ray resolution -  $100 \times 100$  microns
- Conversion of CT data to X-ray projections gives lower resolution degraded X-ray images
- Conversion of LR X-ray projections to HR is required.

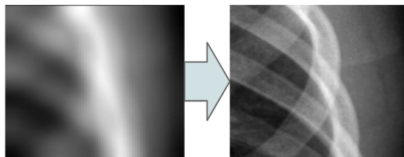
1

Increase resolution



2

Reconstruct lost detail

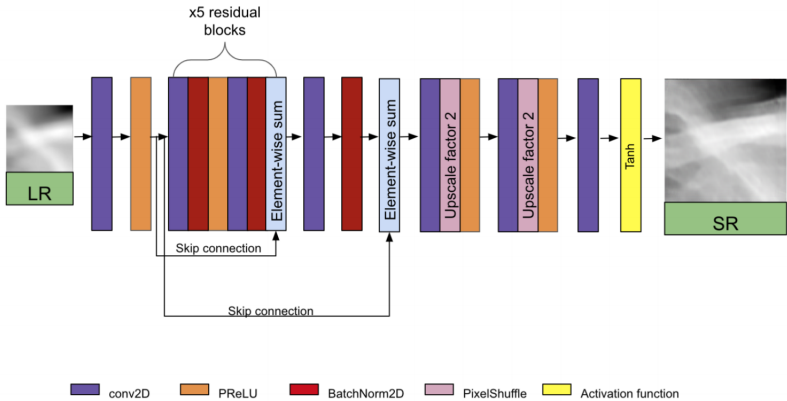


# Motivation Behind XPGAN Design

The goals behind our generative adversarial network, XPGAN's design are:

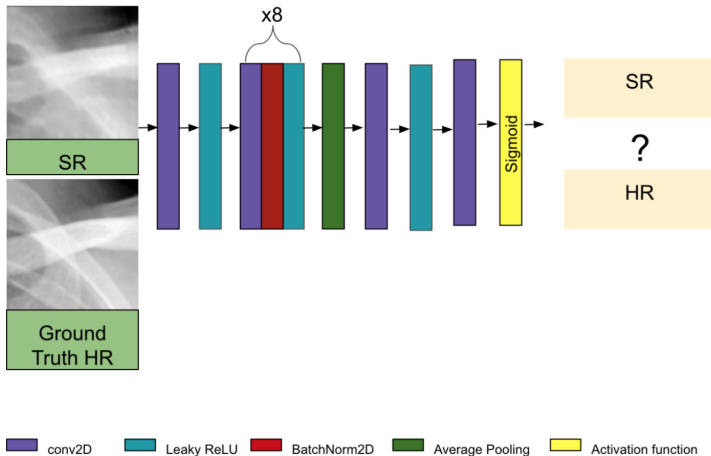
- Recovery of fine structural details
- High Penalty placed on artifacts
- Memory-efficient computation
- Robust model which works for X-rays of varied degradation levels.

# Generator Architecture



<sup>1</sup>Ledig et al. Photo-Realistic Single Image Super-Resolution Using a Generative Adversarial Network

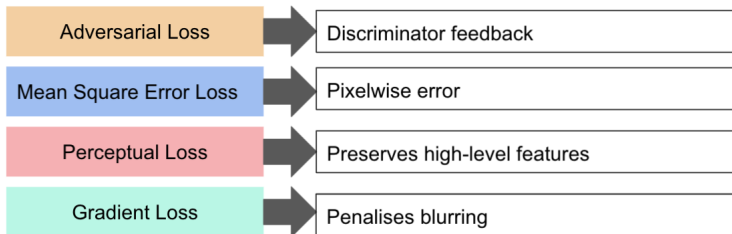
# Discriminator Architecture



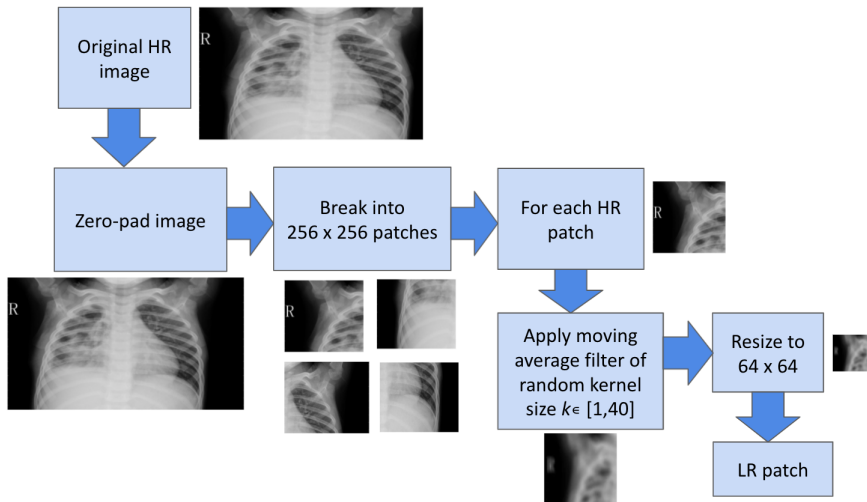


# Losses

$$L_{gen} = \alpha(L_{adv}) + \beta(L_{mse}) + \gamma(L_{vgg/i,j}) + \delta(L_{gra})$$

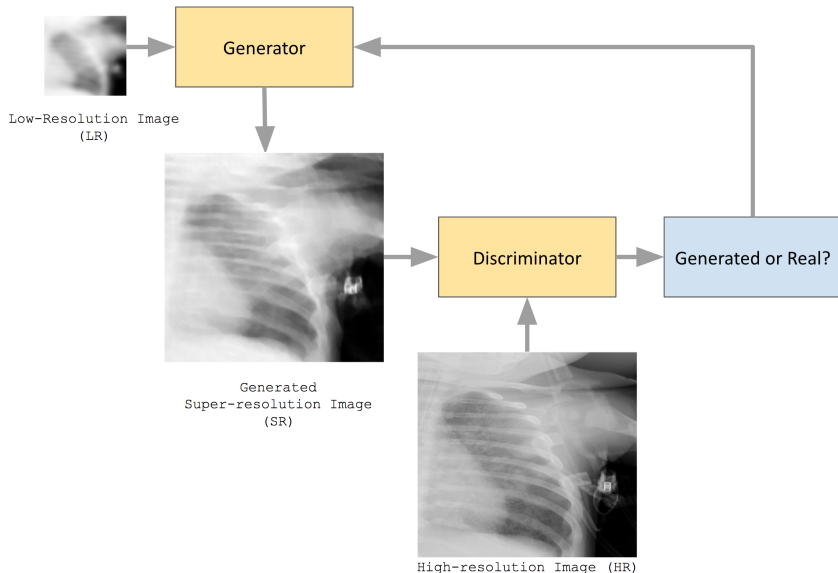


# Image Processing Pipeline During Training

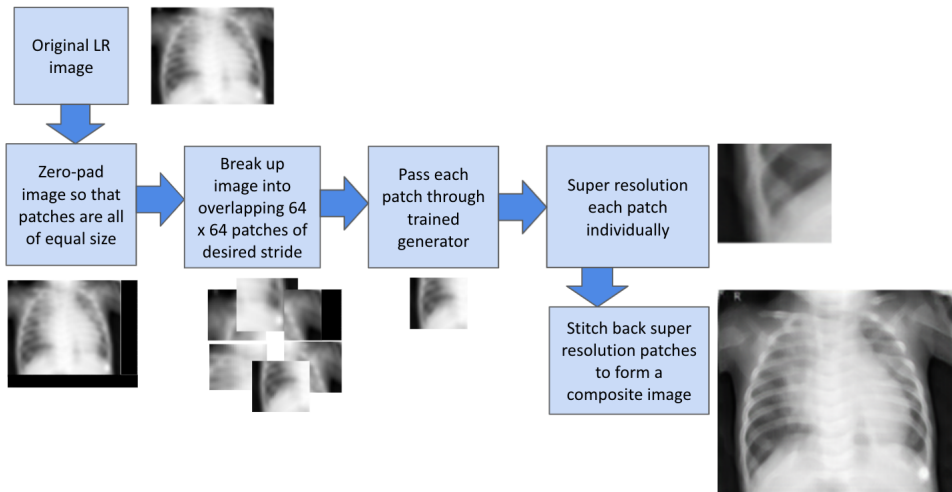


# Training XPGAN

XPGAN is trained on LR-HR pairs of patches



# Inference pipeline after training



# Testing Methodology

- 5 test datasets; each with 3000 LR patches
- Dataset 1: simple moving average(SMA) filter of kernel size  $k \in [1, 40]$  applied
- Datasets 2-5:  $40 \times 40$  SMA,  $30 \times 30$  SMA,  $20 \times 20$  SMA,  $10 \times 10$  SMA applied respectively
- Comparison of XPGAN's performance with bicubic interpolation

# Results: Structural Similarity Index Measure (SSIM)

Dataset	XPGAN	Bicubic Interpolation
Randomly chosen $k \in [1, 40]$	0.85	0.81
$k = 40$	0.80	0.72
$k = 30$	0.83	0.74
$k = 20$	0.85	0.79
$k = 10$	0.89	0.86

SSIM comparison of XPGAN with bicubic interpolation on testing set

## Results: Variance of the Laplacian

Dataset	XPGAN	Bicubic Interpolation
Randomly chosen $k \in [1, 40]$	30.58	1.72
$k = 40$	14.65	0.94
$k = 30$	23.85	0.99
$k = 20$	28.38	1.10
$k = 10$	31.08	1.69

Variance of the Laplacian comparison of XPGAN with bicubic interpolation on testing set

- Laplacian measure shows that edges reconstructed and sharpness recovered
- SSIM shows that feature detail is recovered and there are fewer artifacts.
- Tested on datasets with varying filters; model is robust and can be used in practical settings

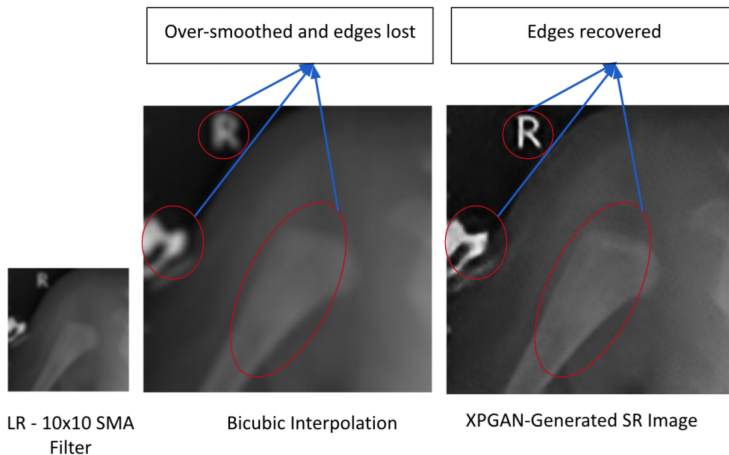


# Example Test Image: Real HR Image

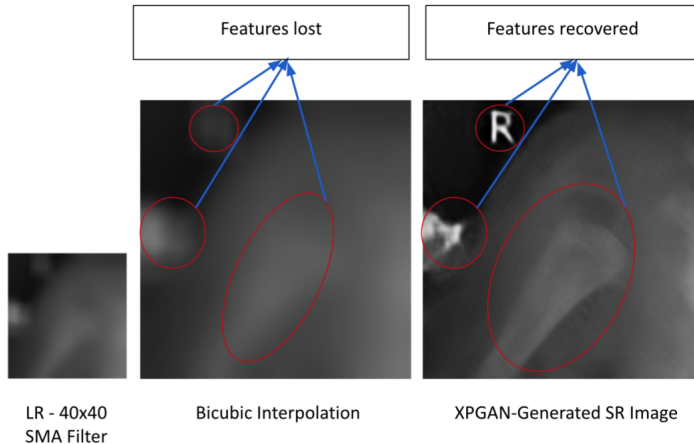


Real HR

# Example Test Image: 10 x 10 filter



# Example Test Image: 40 x 40 filter



- Implement on CT based simulations of x-rays
- Perform radiologist reader study to check for acceptability of super-resolution X-ray images (ongoing)

- Smaller patches  $\rightarrow$  preserve fidelity of original image as no resizing is required; memory-efficient
- Outperforms interpolation methods in
  - image sharpness
  - perceptual similarity to real HR images.
- Trained and tested for an upscaling factor of  $4\times$  which corresponds to  $16\times$  reduction in radiation dose.