

API Documentation

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April 28, 2014

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1 Package meet

This is the Modular EEg Toolkit (MEET) for Python 2.

```
*****
***Disclosure:***
***-----***
***This software comes as it is - there might be errors at runtime ***
***and results might be wrong although the code was tested and did ***
***work as expected. Since results might be wrong you must ***
***absolutely not use this software for a medical purpose - decisions***
***concerning diagnosis, treatment or prophylaxis of any medical ***
***condition mustn't rely on this software.***
*****
```

Only Python 2 is supported at the moment, however modifications should be easy to do.

Dependencies:

```
-----
-Python 2
-Numpy
-Scipy
-Matplotlib
```

Installation:

```
-----
```

Using the usual procedure:

```
python setup.py build
python setup.py install (be sure that the python executable is Python 2)
```

Uninstallation:

```
-----
```

if you use pip you can uninstall doing:

```
pip uninstall meet
```

Version Compatibility:

```
-----
```

I try to avoid incompatibilities when updating functions, this however cannot be totally avoided from time to time. However functions are thoroughly tested.

Citation:

```
-----
```

If you use this software for scientific publications please give proper citation.

In the moment please cite as (or similar)

G. Waterstraat, 2014. Modular EEg toolkit (MEET) for Python.

<https://github.com/neurophysics/meet>. Retrieved on <date>

There is a properly citable publication on the way as well which may be cited additionally.

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1.1 Modules

- **_cSPoC**: Implements canonical Source Power Correlation analysis (cSPoC)
(Section 2, p. 6)
- **_dot_new**: A drop in replacement for numpy.dot
(Section 3, p. 10)
- **_interp**: hidden functions for interpolating EEG
(Section 4, p. 11)
- **basic**: Basic functions for reading binaries and EEG manipulation
(Section 5, p. 12)
- **cSPoC**: Implements canonical Source Power Correlation analysis (cSPoC)
(Section 6, p. 18)
- **eeg_viewer**: Simple interactive EEG viewer
(Section 7, p. 22)
- **elm**: Extreme Learning Machine Classification
(Section 8, p. 24)
- **iir**: IIR Filtering
(Section 9, p. 32)

- **spatfilt**: Spatial Filters
(Section 10, p. 34)
- **sphere**: Spherical spline interpolation and CSD
(Section 11, p. 39)
- **tf**: S transform (time-frequency transformation)
(Section 12, p. 49)

2 Module meet._cSPoC

Implements canonical Source Power Correlation analysis (cSPoC)

Reference:

Dahne, S., et al., Finding brain oscillations with power dependencies in neuroimaging data, NeuroImage (2014),
<http://dx.doi.org/10.1016/j.neuroimage.2014.03.075>

Hidden submodule of the Modular EEG Toolkit - MEET for Python.
 (Imported by spatfilt module)

This module implements some spatial filters such as CSP, CCA, CCAvReg, bCSTP and QCA.

2.1 Functions

pattern_from_filter(*filter*, *X*)

Get a an activation pattern from the filter matrix and the input data X.

Input:

filter - is a p (x k) numpy array, where p is the dimensionality of the data and k is the number of filters (if k == 1, the array may be 1-dimensional)

X - is an p x N (x tr) numpy array, where p is the dimensionality of the data, N is the number of datapoints (per trial, and tr is the number of trials)

If X is 3d, the patterns are computed by collapsing the last 2 axes

Output:

pattern - is a (k x) p numpy array of activation patterns, where p is the dimensionality of the data and k is the number of filters
 If the input filter array is 1d so will be this array

```
cSPoC(X, Y, opt='max', num=1, log=True, bestof=15)
```

canonical Source Power Correlation analysis (cSPoC)

For the datasets X and Y, find a pair of linear filters wx and wy, such that the correlation of the amplitude envelopes wx.T.dot(X) and wy.T.dot(Y) is maximized.

Reference:

Dahne, S., et al., Finding brain oscillations with power dependencies in neuroimaging data, NeuroImage (2014),
<http://dx.doi.org/10.1016/j.neuroimage.2014.03.075>

Notes:

Datasets X and Y can be either 2d numpy arrays of shape (channels x datapoints) or 3d array of shape (channels x datapoints x trials). For 3d arrays the average envelope in each trial is calculated. If log == True, then the log transform is taken before the average inside the trial

The filters are in the columns of the filter matrices Wx and Wy, for 2d input the data can be filtered as:

```
np.dot(Wx.T, X)
```

for 3d input:

```
np.tensordot(Wx, X, axes=(0,0))
```

Input:

```
-- X numpy array - the first dataset of shape px x N (x tr), where px
                      is the number of sensors, N the number of data-
                      points, tr the number of trials
-- Y is the second dataset of shape py x N (x tr)
-- opt {'max', 'min'} - determines whether the correlation coefficient
                      should be maximized - seeks for positive
                      correlations ('max', default);
                      or minimized - seeks for anti-correlations
                      ('min')
-- num int > 0 - determine the number of filter-pairs that will be
                      derived. This depends also on the ranks of X and Y,
                      if X and Y are 2d the number of filter pairs will be:
                      min([num, rank(X), rank(Y)]). If X and/or Y are 3d the
                      array is flattened into a 2d array before calculating
                      the rank
-- log {True, False} - compute the correlation between the log-
                      transformed envelopes, if datasets come in
                      epochs, then the log is taken before averaging
                      inside the epochs, defaults to True
-- bestof int > 0 - the number of restarts for the optimization of the
                      individual filter pairs. The best filter over all
                      these restarts with random initializations is
                      chosen, defaults to 15.
```

Output:

```
cSPoAC(X, tau=1, opt='max', num=1, log=True, bestof=15)
```

canonical Soure Power Auto-Correlation analysis (cSPoAC)

For the dataset X, find a linear filters wx, such that the correlation of the amplitude envelopes $wx.T.dot(X[:, :-tau])$ and $wx.T.dot(X[:, tau:])$ is maximized, i.e. it seeks a spatial filter to maximize the auto-correlation of amplitude envelopes for a shift of tau.

The solution is inspired by and derived by the original cSPoC-Analysis

Reference:

Dahne, S., et al., Finding brain oscillations with power dependencies in neuroimaging data, NeuroImage (2014),
<http://dx.doi.org/10.1016/j.neuroimage.2014.03.075>

Notes:

Dataset X can be either a 2d numpy array of shape (channels x datapoints) or 3d a array of shape (channels x datapoints x trials). For 2d array tau denotes a lag in the time domain. For a 3d array the average envelope in each trial is calculated and tau denotes a trial-wise lag.
 If log == True, then the log transform is taken before the average inside the trial

The filters are in the columns of the filter matrices Wx and Wy, for 2d input the data can be filtered as:

```
np.dot(Wx.T, X)
```

for 3d input:

```
np.tensordot(Wx, X, axes=(0,0))
```

Input:

```
-- X numpy array - the dataset of shape px x N (x tr), where px is the
                        number of sensors, N the number of data-points, tr
                        the number of trials
-- tau int - the lag to calculate the autocorrelation , if X.ndim==2,
                        this is a time-wise lag, if X.ndim==3, this is a trial-
                        wise lag.
-- opt {'max', 'min'} - determines whether the correlation coefficient
                        should be maximized - seeks for positive
                        correlations ('max', default);
                        or minimized - seeks for anti-correlations
                        ('min')
-- num int > 0 - determine the number of filters that will be derived.
                        This depends also on the rank of X, if X is 2d, the
                        number of filter pairs will be: min([num, rank(X)]).
                        If X is 3d, the array is flattened into a 2d array
                        before calculating the rank
-- log {True, False} - compute the correlation between the log-
                        transformed envelopes, if datasets come in
                        epochs, then the log is taken before averaging
```


2.2 Variables

Name	Description
__package__	Value: 'meet'

3 Module `meet._dot_new`

A drop in replacement for `numpy.dot`

Avoid temporary copies of non C-contiguous arrays

The code is available here: <http://pastebin.com/raw.php?i=M8TfbURi> In future this will be available in numpy directly: <https://github.com/numpy/numpy/pull/2730>

3.1 Functions

<code>dot(A, B, out=None)</code>

A drop in replacement for <code>numpy.dot</code> Computes A.B optimized using fblas call
--

<code>test_dot()</code>

<code>test_to_fix()</code>

1d array, complex and 3d

3.2 Variables

Name	Description
<code>__package__</code>	Value: <code>'meet'</code>

4 Module `meet._interp`

hidden functions for interpolating EEG

Hidden submodule of the Modular EGg Toolkit - MEET for Python.

Author:

Gunnar Waterstraat

gunnar[dot]waterstraat[at]charite.de

4.1 Functions

akima (x , y)

mchi (x , y)

Monotone cubic hermite interpolation

4.2 Variables

Name	Description
<code>__package__</code>	Value: <code>'meet'</code>

5 Module meet.basic

Basic functions for reading binaries and EEG manipulation

Submodule of the Modular EEG Toolkit - MEET for Python.

Author:

Gunnar Waterstraat

gunnar[dot]waterstraat[at]charite.de

5.1 Functions

```
readBinary(fname, num_channels, channels='all', readnum_dp='all',
data_type='float4', buffermem=512)
```

Read EEG from a binary file and output as numpy array.

The binary of a signal with k channels and n datapoints must be of the type:

	t0	t1	...	tn-1
ch_0	0	k	...	(n-1)*k
ch_1	1	k+1	...	(n-1)*k+1
...
ch_k-1	k-1	2*k-1	...	n*k-1

The endianness of the runtime system is used.

Input:

```
-----
-- fname - (str) - input file name
-- num_channels - int - total number of channels in the file
-- channels - numpy array OR 'all' - iterable of channels to read
              (starting with 0) if 'all', all channels are read
-- readnum_dp - int OR 'all' - number of datapoints to read
-- data_type - str - any of 'int2', 'int4', 'int8', 'float4',
                  'float8', 'float16' where the digit determines
                  the number of bytes (= 8 bits) for each element
-- buffermem - float - number of buffer to us in MegaBytes
```

Output:

```
-----
-- data - numpy array - data shaped k x n where k is number of
                  channels and n is number of datapoints
```

Example:

```
-----
>>> readBinary(_path.join(_path.join(_packdir, 'test_data'),
array([[0, 2, 4, 6, 8],
       [1, 3, 5, 7, 9]])
'sample.dat'), 2, data_type='float4')
```

```
interpolateEEG(data, markers, win, interpolate_type='mchs')
```

Interpolates segemnets in the data

Input:

```
-- data - one or two dimensional array
      1st dimension: channels (can be ommitted if single channel)
      2nd dimension: datapoints
-- markers - marker positions arranged in 1d array
-- win - iterable of len 2 - determining the window in datapoints to
      be interpolated (win[0] is in, win[1] is out of the window)
-- interpolate_type: ['linear', 'mchs', 'akima'] - linear or
      Monotone Cubic Hermite Spline
      or Akima interpolation
```

Output:

interpolated dataset

Examples:

```
>>> data = _np.arange(20, dtype=float).reshape(2,-1)
>>> interpolateEEG(data, [5], [-1,2], 'linear')
array([[ 0.,  1.,  2.,  3.,  4.,  5.,  6.,  7.,  8.,  9.],
       [10., 11., 12., 13., 14., 15., 16., 17., 18., 19.]])
>>> interpolateEEG(data, [5], [-1,2], 'mchs')
array([[ 0.,  1.,  2.,  3.,  4.,  5.,  6.,  7.,  8.,  9.],
       [10., 11., 12., 13., 14., 15., 16., 17., 18., 19.]])
>>> interpolateEEG(data, [5], [-1,2], 'akima')
array([[ 0.   ,  1.   ,  2.   ,  3.   ,  3.625,  5.   ,  6.375,
        7.   ,  8.   ,  9.   ],
       [10.   , 11.   , 12.   , 13.   , 13.625, 15.   , 16.375,
        17.   , 18.   , 19.   ]])
```

```
epochEEG(data, marker, win)
```

Arrange the dataset into trials (=epochs) according to the marker and window.

markers and the window borders are sorted in ascending order.

Input:

```
-- data - numpy array - 1st dim channels (can be omitted if single
                           channel)
                           2nd dim datapoints
-- marker - iterable - the marker
-- win - iterable of len 2 - determining the start and end of epochs
        in dp (win[0] is in, win[1] is out of the window)
```

Output:

```
-- epochs - numpy array - dimension one more than data input
                  - 1st dim: channel (might be omitted - see
                                above)
                  - 2nd dim: epoch length = win[1] - win[0]
                  - 3rd dim: number of epochs
```

Example:

```
>>> data = _np.arange(20, dtype=float).reshape(2,-1)
>>> epochEEG(data, [3,5,7], [-2,2])
array([[[ 1.,  3.,  5.],
        [ 2.,  4.,  6.],
        [ 3.,  5.,  7.],
        [ 4.,  6.,  8.]],
       <BLANKLINE>
        [[ 11., 13., 15.],
        [ 12., 14., 16.],
        [ 13., 15., 17.],
        [ 14., 16., 18.]])
```

calculateRMS(*data*, *axis=-1*)

Calculate rms value of the input data along the indicated axis

Input:

```
-- data - numpy array - input data
-- axis - int - axis along which the rms is calculated; if None, the
              flattened array is used
```

Output:

```
-- rms value along the indicated axis
```

Example:

```
>>> data = _np.arange(20, dtype=float).reshape(2,-1)
>>> calculateRMS(data, None)
11.113055385446435
>>> calculateRMS(data, 0)
array([ 7.07106781,  7.81024968,  8.60232527,  9.43398113,
        10.29563014, 11.18033989, 12.08304597, 13.          ,
        13.92838828, 14.86606875])
>>> calculateRMS(data, 1)
array([ 5.33853913, 14.7817455 ])
```

getMarker(*marker*, *width=50*, *mindist=100*)

Gets position of markers from the trigger channel

GetMarkerPosFromData(marker)

input:

```
-- marker - one-dimensional array with trigger channel - each
              impulse or zero crossing is treated a marker
--width - int - calculates the local mean in window of size width
              - defaults to 50
--mindist - int - minimal distance between triggers in dp
              - defaults to 100
```

output:

```
-- marker - one-dimensional array containing trigger positions
```

Example:

```
>>> x = _np.ones(1000)
>>> x[200:400] = -1
>>> x[600:800] = -1
>>> getMarker(x)
array([200, 400, 600, 800])
```


5.2 Variables

Name	Description
<code>--package--</code>	Value: <code>'meet'</code>

6 Module meet.cSPoC

Implements canonical Source Power Correlation analysis (cSPoC)

Reference:

Dahne, S., et al., Finding brain oscillations with power dependencies
in neuroimaging data, NeuroImage (2014),
<http://dx.doi.org/10.1016/j.neuroimage.2014.03.075>

6.1 Functions

```
cSPoC(X, Y, opt='max', num=1, log=True, bestof=15)
```

canonical Soure Power Correlation analysis (cSPoC)

For the datasets X and Y, find a pair of linear filters wx and wy, such that the correlation of the amplitude envelopes wx.T.dot(X) and wy.T.dot(Y) is maximized.

Reference:

Dahne, S., et al., Finding brain oscillations with power dependencies in neuroimaging data, *NeuroImage* (2014),
<http://dx.doi.org/10.1016/j.neuroimage.2014.03.075>

Notes:

Datasets X and Y can be either 2d numpy arrays of shape (channels x datapoints) or 3d array of shape (channels x datapoints x trials). For 3d arrays the average envelope in each trial is calculated. If log == True, then the log transform is taken before the average inside the trial

The filters are in the columns of the filter matrices Wx and Wy, for 2d input the data can be filtered as:

```
np.dot(Wx.T, X)
```

for 3d input:

```
np.tensordot(Wx, X, axes=(0,0))
```

Input:

```
-- X numpy array - the first dataset of shape px x N (x tr), where px
                      is the number of sensors, N the number of data-
                      points, tr the number of trials
-- Y is the second dataset of shape py x N (x tr)
-- opt {'max', 'min'} - determines whether the correlation coefficient
                      should be maximized - seeks for positive
                      correlations ('max', default);
                      or minimized - seeks for anti-correlations
                      ('min')
-- num int > 0 - determine the number of filter-pairs that will be
                      derived. This depends also on the ranks of X and Y,
                      if X and Y are 2d the number of filter pairs will be:
                      min([num, rank(X), rank(Y)]). If X and/or Y are 3d the
                      array is flattened into a 2d array before calculating
                      the rank
-- log {True, False} - compute the correlation between the log-
                      transformed envelopes, if datasets come in
                      epochs, then the20log is taken before averaging
                      inside the epochs, defaults to True
-- bestof int > 0 - the number of restarts for the optimization of the
                      individual filter pairs. The best filter over all
                      these restarts with random initializations is
```

pattern_from_filter(*filter*, *X*)

Get a an activation pattern from the filter matrix
and the input data X.

Input:

filter - is a p (x k) numpy array, where p is the dimensionality of the
data and k is the number of filters (if k == 1, the array may
be 1-dimensional)

X - is an p x N (x tr) numpy array, where p is the dimensionality of
the data, N is the number of datapoints (per trial, and tr is the
number of trials)

If X is 3d, the patterns are computed by collapsing the last 2 axes

Output:

pattern - is a (k x) p numpy array of activation patterns, where p is
the dimensionality of the data and k is the number of filters
If the input filter array is 1d so will be this array

6.2 Variables

Name	Description
<code>__package__</code>	Value: 'meet'

7 Module `meet.eeg_viewer`

Simple interactive EEG viewer

Submodule of the Modular EEG Toolkit - MEET for Python.

Author:

Gunnar Waterstraat

`gunnar[dot]waterstraat[at]charite.de`

7.1 Variables

Name	Description
<code>--package--</code>	Value: <code>'meet'</code>

7.2 Class plotEEG

7.2.1 Methods

```
__init__(self, signals, ylabels, t, t_res=30, title=False)
```

Function to Plot EEG-Signals in of several channels

```
Def: PlotEEG(signals, ylabels, t, t_res, title = False)
```

Interaction:

PageUp -> Go backward a big step

PageDown -> Go forward a big step

Up -> Go backward a small step

Down -> go forward a small step

i -> Zoom in (show smaller temporal window)

o -> Zoom out (show larger temporal window)

+ -> increase gain

- -> decrease gain

Pos1 -> Go to start

End -> Go to end

LeftMouseClicked -> saves the x coordinate in self.clicks

Input:

-signals: 2d array of input data

-ylabels: list of channel names in same order as in
 'signals' (unit is presumed to be mikro V)

-t: array of time values in s

-t_res: mm per second (standard: 30 mm / s)

-title: title string

Output:

-EEG_viewer class: plot with EEG.show()

clicks are saved in self.clicks

```
change_gain(self, new_offset)
```

```
change_t(self, new_t0, new_t_show)
```

```
show(self)
```

8 Module *meet.elm*

Extreme Learning Machine Classification

Submodule of the Modular EEG Toolkit - MEET for Python.

This module implements regularized Extreme Learning Machine Classification and Weighted Extreme Learning Machine Classification.

Classification is implemented in the `ClassELM` class

For faster execution of dot product the module `dot_new` is imported since it avoids the need of temporary copy and calls `fblas` directly.

The code is available here: <http://pastebin.com/raw.php?i=M8TfbURi>

In future this will be available in `numpy` directly:

<https://github.com/numpy/numpy/pull/2730>

1. Extreme Learning Machine for Regression and Multiclass Classification

Guang-Bin Huang, Hongming Zhou, Xiaojian Diang, Rui Zhang

IEEE Transactions of Systems, Man and Cybernetics - Pat B: Cybernetics,

Vol. 42, No. 2. April 2012

2. Weighted extreme learning machine for imbalance learning.

Weiwei Zong, Guang-Bin Huang, Yiqiang Chen

Neurocomputing 101 (2013) 229-242

Author & Contact

Written by Gunnar Waterstraat

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8.1 Functions

`accuracy(conf_matrix)`

Measure of the performance of the classifier.

The Accuracy is the proportion of correctly classified items in relation to the total number of items.

You should be aware that this is very sensitive to imbalanced data (data with very unequal sizes of each class):

Imagine a sample with 99% of the items belonging to class 0 and 1% of items belonging to class 1. A classifier might have an accuracy of 99% by just assigning all items to class 0. However, the sensitivity for class 1 is 0% in that case. It depends on your needs if this is acceptable or not.

Input:

`conf_matrix` - shape `ny x ny`, where `ny` is the number of classes
the rows belong to the actual, the columns to the
predicted class: item `ij` is hence predicted as class
`j`, while it would have belonged to class `i`

Output:

float - the accuracy

`G_mean(conf_matrix)`

The G-mean is the geometric mean of the per-class-sensitivities. It is much more stable to imbalance of the dataset than the global accuracy. However it depends on your needs, which measure of performance of the classifier to use.

Input:

`conf_matrix` - shape `ny x ny`, where `ny` is the number of classes
the rows belong to the actual, the columns to the
predicted class: item `ij` is hence predicted as class `j`,
while it would have belonged to class `i`

Output:

the geometric mean of per-class sensitivities

Matthews(*conf_matrix*)

The Matthews correlation coefficient is used in machine learning as a measure of the quality of binary (two-class) classifications. It takes into account true and false positives and negatives and is generally regarded as a balanced measure which can be used even if the classes are of very different sizes. The MCC is in essence a correlation coefficient between the observed and predicted binary classifications; it returns a value between -1 and +1. A coefficient of +1 represents a perfect prediction, 0 no better than random prediction and -1 indicates total disagreement between prediction and observation.

Source: Wikipedia (2013-09-25)

Input:

`conf_matrix` - shape 2 x 2, where 2 is the number of classes
 the rows belong to the actual, the columns to the
 predicted class: item `ij` is hence predicted as class `j`,
 while it would have belonged to class `i`
 AN ERROR IS THROWN IF THE SHAPE OF THE MATRIX IS NOT
 CORRECT

Output:

float - the the Matthews Correlation Coefficient

PPV(*conf_matrix*)

Calculate the Positive Predictive Value

Input:

`conf_matrix` - shape 2 x 2, where 2 is the number of classes
 the rows belong to the actual, the columns to the
 predicted class: item `ij` is hence predicted as class `j`,
 while it would have belonged to class `i`
 AN ERROR IS THROWN IF THE SHAPE OF THE MATRIX IS NOT
 CORRECT

Output:

float - the PPV

```
ssk_cv(data, labels, folds=3)
```

Cut data into folds with method:
shuffled, stratified, k-folds cross-validation

Input:

data - numpy array - shape n x p, with n items and p features

Output:

returns a list, with each list-element including the indices of one fold

```
get_conf_matrix(true, pred)
```

Get a confusion matrix

Input:

true - the true labels

pred - the predicted labels

Output:

conf_matrix - shape ny x ny, where ny is the number of classes
the rows belong to the actual, the columns to the
predicted class: item ij is hence predicted as class j,
while it would have belonged to class i

8.2 Variables

Name	Description
__package__	Value: 'meet'

8.3 Class ClassELM

Class for Extreme Learning Machine Classification

Input:

L - (int) - dimensionality of the feature space (defaults to 1000)

change_alg - (int) - number of samples to change from implementation

```

                                I to II
kernel - (str) - any of: 'sigmoid' - Sigmoid function
                                - more functions not implemented yet
-----

use self.cv() for cross-validation
use self.train() for training

after cross-validation or training use

self.classifiy()
```

8.3.1 Methods

<code>__init__(self, L=1000, kernel='sigmoid')</code>

```
cv(self, data, labels, method='ssk_cv', C_array=None, folds=3,
precision_func='accuracy', scale=True, weights=True, mem_size=512, verbose=True)
```

Perform Cross-Validation of Extreme Learning Machine parameter C

Input:

data - numpy array - shape (n x p) with n being sample number
and p being number of features

labels - numpy array - shape (n) with the class labels
0,1,...,ny-2,ny-1, where ny is the number of classes

method - string - cross-validation method
- 'ssk_cv' - shuffled stratified k-folds
cross-validation

C_array - numpy array - default is None - the C's which are
cross-validated
- if None from $2^{*(-25)}$, $2^{*(-24)}$, ..., $2^{*(24)}$, $2^{*(25)}$

folds - integer - default 3 - number of folds

precision_func - string or function - standard is 'accuracy' -
Measure of performance
- as string implemented: 'accuracy' -
proportion of
correctly classified
to total number of
samples
'G_mean' - geometric
mean of per-class
accuracies
'Matthews' - Matthews
Correlation
Coefficient - Only
for binary
classification
'PPV' - Positive
Predictive Value -
Only for binary
classification
- if function: with confusion matrix as single
input and float (0,1) as single output

scale - bool (True | False) - whether data should be scaled to
range (-1,1)

weights - can be: - bool (True | False): - standard is True
if True, data is
re-weighted to a
class ratio of 1.0
if False, data is not
re-weighted
- float in half-open interval [0,1)
- data is re-weighted such that the
minority / majority ratio is this
float
- minority classes are the ones having
less members than on average, majority
classes have more than average
- Zong et al. proposed to use the golden
ratio (approx. 0.618 -
scipy.constants.golden) as a good

```

train(self, data, labels, C, scale=True, weights=True, mem_size=512)

Train the ELM Classifier
-----

Input:
-----
data - (numpy array) - shape n x p
            n - number of observations
            p - number of dimensions
            if data.ndim > 2, the array is reshaped as (n,-1)
labels - array with integer labels
C - regularization parameter
scale - bool (True | False) - standard is True
            - switch, if the features of the
              dataset should be scaled
              to the interval (-1,1)
weights - can be: - bool (True | False): - standard is True
            if True, data is re
            weighted to a class
            ratio of 1.0 if
            False, data is not
            re-weighted
            - float in half-open interval [0,1)
            - data is re-weighted such that the
              minority / majority ratio is this
              float
            - minority classes are the ones having
              less members than on average, majority
              classes have more than average
            - Zong et al. proposed to use the golden
              ratio (approx. 0.618 -
              scipy.Constants.golden) as a good value
            - numpy array with weights for each sorted
              unique class in labels, each class weight is
              expected to be in half-open interval [0,1)
mem_size - number - memory size of temporary array in Mb -
            default to 512

Output:
-----
No user output (Weights are generated and stored in the Class as
self._beta) self.istrained is set to True

```

```
classify(self, data, mem_size=512, scale=True)
```

Classify a dataset.

Input:

data - numpy array, shape N x p, where N is number of items, p
is number of features

mem_size - number - memory size of temporary array in Mb -
default to 512

scale - bool (True | False) - if the input should be scaled
by the network with parameters obtained during training

Output:

labels - the predicted class labels: 0, 1, ..., ny-2, ny-1,
where ny is the total number of classes

Internally the method `_run()` is used

9 Module meet.iir

IIR Filtering

Submodule of the Modular EEG Toolkit - MEET for Python.

So far only butterworth filtering is implemented

Author:

Gunnar Waterstraat

gunnar[dot]waterstraat[at]charite.de

9.1 Functions

```
butterworth(data, fp, fs, s_rate, gpass=3, gstop=8, axis=-1, zero_phase=True,
return_param=False)
```

Apply a butterworth filter to the data.

fp is the passband frequency in Hz

fs is the stopband frequency in Hz

Example of Notations:

For fs = 10, fp = 15 a high-pass filter is applied with the transition band between 10-15 Hz

For fs = 15, fp = 10 a low-pass filter is applied with the transition band between 10-15 Hz

For fs = [10, 40], fp = [20,30] a bandpass-filter with the passband 20-30 Hz and transitions between 10-20 Hz and 30-40 Hz is applied

For fs = [20, 30], fp = [10,40] a bandstop-filter with the stopband 20-30 Hz and transitions between 10-20 Hz and 30-40 Hz is applied

Input:

```
-- data - numpy array
-- fp - float - pass-band frequencies
-- fs - float - stop-band frequencies
-- s_rate - float - the sampling rate in Hz
-- gpass - float - maximal attenuation in the passband (in dB)
-- gstop - float - minimal attenuation in the passband (in dB)
-- axis - int -along which axis the filter is applied
-- zero_phase - bool - if zero phase filter is applied by filtering
                    in both directions
-- return_param - bool - if the order, b, and a should be returned
```

Output:

```
-- data - numpy array - the filtered data array
if return_param:
    -- data
    -- ord - int - filter order (this must be doubled for the
                    zero_phase implementation)
    -- (b, a) - Numerator ('b') and denominator ('a') polynomials of
                    the IIR filter.
```

9.2 Variables

Name	Description
<code>--package--</code>	Value: 'meet'

10 Module meet.spatfilt

Spatial Filters

Submodule of the Modular EEG Toolkit - MEET for Python.

This module implements some spatial filters such as CSP, CCA, CCAvReg, bCSTP and QCA.

Author & Contact

Written by Gunnar Waterstraat
email: `gunnar[dot]waterstraat[at]charite.de`

10.1 Functions

```
CSP(data1, data2, center=True)
```

Common Spatial Pattern (CSP)

This takes the multivariate data in two conditions and finds the spatial filters which minimize the variance in condition 2, while simultaneously maximizing the variance in condition one.

The algorithm uses Singular Value Decomposition since this is more stable than the Eigenvalue Decomposition of the Covariance Matrices

The filters are scaled such, that $\text{Var}(\text{cond1}) + \text{Var}(\text{cond2}) = 1$. The eigenvalues give the variance in condition 1.

The filters are in the columns of the filter matrix. Patterns can be obtained by inverting the filter matrix and are located in the rows of the inverted filter matrix.

```
filter, eigval = CSP(data1, data2)
filtered_data = filter.T.dot(data1)
```

Input:

-- data1 - 2d array - data in condition 1 (variables in rows,
 observations in columns)

-- data2 - 2d array - data in condition 2 (variables in rows,
 observations in columns)

 The number of variables in data1 and data2 must be equal

-- center - bool - if data should be centered, defaults to True

Output:

-- filter - where the individual filters are in the columns of the
 matrix (in order of decreasing eigenvalues)

-- eigvals - eigenvalues in decreasing order

CCA_data(X, Y)

Cannonical Correlation Analysis - by a combination of QR decomposition and Singular Value Decomposition

The filters are scaled to give unit variance in the components and are given in the order of decreasing canonical correlations.

Patterns can be obtained by inverting the filter matrices.

Inputs:

X - shaped p1 x N - variables in rows, observations in columns

Y - shaped p2 x N - variables in rows, observations in columns

Outputs:

a - filters for X (shape p1 x d), where d is min(rank(X), rank(Y)), each filter is in one column

b - filters for Y (shape p2 x d), where d is min(rank(X), rank(Y)), each filter is in one column

s - canonical correlations in non-increasing order, each corresponding to the respective column in a and b

CCAvReg(*trials*)

Canonical Correlation Average Regression

Calculate the CCA between trials and their average across trials

The filters are scaled to give unit variance in the components and are given in the order of decreasing canonical correlations.

Patterns can be obtained by inverting the filter matrices.

notably, all single trials can be filtered at once by:

```
np.tensordot(a, trials, axes=(0,0))
```

the filtered average can be obtained as:

```
np.dot(b.T, trials.mean(-1))
```

Input:

```
-- trials - 3d numpy array - 1st dim: channels
                             - 2nd dim: epoch length
                             - 3rd dim: number of epochs
```

Output:

```
-- a - 2d numpy array (channel x channel) - spatial filters for
      single trials, each filter is in one column
-- b - 2d numpy array (channel x channel) - spatial filters for
      average, each filter is in one column
-- s - the canonical correlations between single trials and averages
```

```

bCSTP(trials1, trials2, num_iter=30, s_keep=2, t_keep=2, verbose=True)

```

bilinear Common Spatial-Temporal Patterns

In each iteration the number of kept patterns is reduced by one,
in the last 5 iterations the finally desired number of patterns is
kept.
The minimal number of iterations must therefor be > 10

Filter matrices won't be square if the data was rank deficient,
patterns can then be obtained by using the pseudo-inverse
(`numpy.linalg.pinv`)

Input:

```

-- trials1 - 3d numpy array - 1st dim: channels
                                - 2nd dim: epoch length
                                - 3rd dim: number of epochs
    variance in condition 1 is maximized
-- trials2 - 3d numpy array - 1st dim: channels
                                - 2nd dim: epoch length
                                - 3rd dim: number of epochs
    variance in condition 2 is minimized
-- num_iter - int - number of iterations to do, defaults to 30
                    (minimum 10)
-- s_keep - int - number of spatial patterns to keep, defaults to 2
-- t_keep - int - number of temporal patterns to keep, defaults to 2
-- verbose - bool - if number of iterations should be printed during
                    execution

```

Output:

```

-- W - list of 2d arrays - spatial filter matrix for each iteration,
    the final spatial filters are in W[-1]
-- V - list of 2d arrays - temporal filter matrix for each iteration,
    the final temporal filters are in V[-1]
-- s_eigvals - list of 1d array - spatial eigenvalues,
    the final spatial eigenvalues are in s_eigvals[-1]
-- t_eigvals - list of 1d array - temporal eigenvalues, the final
    temporal eigenvalues are in s_eigvals[-1]

```

10.2 Variables

Name	Description
<code>__package__</code>	Value: 'meet'

11 Module *meet.sphere*

Spherical spline interpolation and CSD

Submodule of the Modular EEG Toolkit - MEET for Python.

Algorithm from Perrin et al., *Electroenceph Clin Neurophysiol* 1989, 72:184-187, Corrigenda in 1990, 76: 565-566

While the implementation was done independently, the code was tested using the sample data of the CSD Toolbox for Matlab (<http://psychophysiology.cpmc.columbia.edu/Software/CSDtoolbox/>) and results are the same. Thanks a lot to Juergen Kayer for sharing his work there.

Example:

For Plotting a scalp map:

```
>>> import numpy as _np
>>> coords = getStandardCoordinates(['Fp1', 'Fp2', 'C1', 'C2', 'C3', 'C4', 'P2', 'P4'])
>>> coords = projectCoordsOnSphere(coords) # be sure that these coords are on the surface of a
>>> data = _np.random.random(coords.shape[0]) # just create a random vector for testing
>>> X, Y, Z = potMap(coords, data) # interpolate using spherical splines
```

For Calculating current source densities:

```
>>> import numpy as _np
>>> coords = getStandardCoordinates(['Fp1', 'Fp2', 'C1', 'C2', 'C3', 'C4', 'P2', 'P4'])
>>> coords = projectCoordsOnSphere(coords) # be sure that these coords are on the surface of a
>>> data = _np.random.random([coords.shape[0], 1000]) # just create a random vector for testing
>>> CSD = calcCSD(coords, data) # get CSD using spherical splines - output is in data-unit/m**2
```

Author:

Gunnar Waterstraat

`gunnar[dot]waterstraat[at]charite.de`

11.1 Functions

```
addHead(ax, lw=2.0, ec='k', **kwargs)
```

Add a path representing a a head consisting of a circle with center (0,0) and r = 1 to the axis.

Input:

--ax - a matplotlib axes instance into which the head will be drawn
--lw - linewidth - defaults to 2.0
--ec - edgecolor - defaults to black ('k')

Output:

Nothing

Notes:

Kwargs are matplotlib patches kwargs and are passed to `matplotlib.patches.PathPatch`

Parts of the code (for drawing the circle) are from:

<https://sourcegraph.com/github.com/matplotlib/matplotlib/symbols/python/lib/matplotlib/path/Path/c>


```

getStandardCoordinates(elecnames, fname='standard')

```

Read (cartesian) Electrode Coordinates from tab-seperated text file

The standard is plotting_1005.txt obtained from:
http://robertoostenveld.nl/electrode/plotting_1005.txt (however 1st
and 2nd column were exchanged to get x,y,z order)

Thanks to Robert Oostenveld for sharing these files!!!

Input:

```

-- elecnames - iterable - list of Electrode names
-- fname - str - filename from which positions should be read
                  - this is a tab delimeed file with the UPPERCASE
                    electrode names in first column
                    x,y,z in subsequent columns
                    T7, T8, Oz, Fpz and Cz must be included!

```

Output:

```

-- coords - 2D array containing the cartesian coordinates in rows
              - 1st column: x
              - 2nd column: y
              - 3rd column: z

```

Example:

```

>>> getStandardCoordinates(['fc3', 'FC1', 'xx']) # 'xx' is not a
array([[ -0.6638      ,  0.3610691 ,  0.6545      ],
       [ -0.3581      ,  0.37682936,  0.8532      ],
       [          nan,           nan,           nan]])

```

valid electrode

getChannelNames(*fname*)

Read Names of Electrodes from text file

Input:

-- fname - str - tab-delimited textfile containing electrode number
and electrode-names

example:

1 C1

2 C3

output:

-- elecnames - List of electrode names in ascending order as
determined by the electrode numbers in fname

Example:

```
>>> getChannelNames(_path.join(_path.join(_packdir, 'test.data'),
['C1', 'C3']
```

'elecnames.txt'))

projectCoordsOnSphere(*coords*)

The input coordinates are projected onto a sphere with center
(0,0,0) and radius 1.

For the input coordinates it is believed that they lie on a
sphere with center (0,0,0) and radius $r = x^2 + y^2 + z^2$.
Subsequently this radius is scaled to 1, preserving altitude
and azimuth of the original coordinates.

Input:

--coords - 3D array containing the points in rows

- 1st column: x

- 2nd column: y

- 3rd column: z

Output:

-- out_coords - 3D array containing the coordinates in rows

Examples:

```
>>> coords = _np.array([[0,0,1], [0,1,0], [1,1,1]]) # the last one
```

is not on a sphere

```
>>> projectCoordsOnSphere(coords)
```

```
array([[ 0.          ,  0.          ,  1.          ],
       [ 0.          ,  1.          ,  0.          ],
       [ 0.57735027,  0.57735027,  0.57735027]])
```

```
projectCircleOnSphere(coords, projection='stereographic')
```

Project 2d coordinates inside a unit circle on a sphere with center (0,0) and radius 1.

Stereographic projection:

Where the given circle is believed to be the on the plane crossing the equator ($z=0$) and the perspective point is the southpole (0,0,-1). Points inside the circle are projected onto the northern hemisphere, points outside the circle on the souther hemisphere.

Orthographic projection:

All points have to lie inside the circle and are projected on the northern hemisphere by keeping the xy coordinates and adding a z coordinate to result in a radius of 1.

Point outside the circle result in nans.

Input:

```
-- coords - 2D array containing the coordinates in rows
           - 1st column: x
           - 2nd column: y
-- projection - str - 'stereographic' (standard) or 'orthographic'
                   (explanations see above)
```

Output:

```
-- sphere_coords - masked 3D array containing the coordinates in
                  rows
                  - 1st column: x
                  - 2nd column: y
                  - 3rd column: z
(all coordinates outside a unit sphere are masked)
```

```
projectSphereOnCircle(sphere_coords, projection='stereographic')
```

Project coordinates that lie on the surface of a unit sphere with center $(0,0,0)$ and radius 1 into a unit circle

```
If projection == 'stereographic':
```

The vertex of the sphere is $(0,0,1)$. The projection is done from the "southpole" $(0,0,-1)$ onto the plane with $z=0$.

The northern hemisphere is hereby projected into the unit circle, the southern hemisphere outside the unit circle.

```
If projection == 'orthographic':
```

Only the northern hemisphere is mapped onto a plane through the equator by keeping the xy-coordinates. For coordinates on the southern hemisphere nan is returned.

Input:

```
-- sphere_coords - 2D array containing the coordinates in rows
```

- 1st column: x

- 2nd column: y

- 3rd column: z

```
-- projection - str - 'stereographic' (standard) or 'orthographic'
                        (explanations see above)
```

Output:

```
-- coords - 2D array containing the coordinates in rows
```

- 1st column: x

- 2nd column: y

```
potMap(RealCoords, data, diameter_samples=200, n=(7, 7), m=4, smooth=0,
projection='stereographic')
```

Get a scalp map of potentials interpolated on a sphere.

If *projection* == 'stereographic':

The vertex of the sphere is (0,0,1). The projection is done from the "southpole" (0,0,-1) onto the plane with z=0.

The northern hemisphere is hereby projected into the unit circle, the southern hemisphere outside the unit circle.

If *projection* == 'orthographic':

Only the northern hemisphere is mapped onto a plane through the equator by keeping the xy-coordinates. For coordinates on the southern hemisphere nan is returned.

Input:

```
-- RealCoords - array of shape channels x 3 - (x,y,z) cartesian
                  coordinates of physical electrodes on a sphere with
                  center (0,0,0) and radius 1
-- data - array of shape channels x datapoints - containing values
          at electrodes in same order as in 'RealCoords'
-- diameter_samples - int - number of points along the diameter of
                        the scalp to interpolate
-- n - tuple of ints - how many terms of the Legendre-Polynomial
          should be calculated, defaults to (7,7)
-- m - int - order of the spherical spline interpolation, defaults
          to 4
-- smooth - float - amount of smoothing, defaults to 0
-- projection - str - 'stereographic' (standard) or 'orthographic'
                    (explanations see above)
```

Output:

```
-- X, Y, Z - grid containing the X and Y coordinates and the
                interpolated values where everything outside the unit
                circle is masked.
```

```
csdMap(RealCoords, data, diameter_samples=200, n=(7, 20), m=4, smooth=1e-05,
projection='stereographic')
```

Get a scalp map of CSDs calculated from spherical splines.

If *projection* == 'stereographic':

The vertex of the sphere is (0,0,1). The projection is done from the "southpole" (0,0,-1) onto the plane with z=0.

The northern hemisphere is hereby projected into the unit circle, the southern hemisphere outside the unit circle.

If *projection* == 'orthographic':

Only the northern hemisphere is mapped onto a plane through the equator by keeping the xy-coordinates. For coordinates on the southern hemisphere nan is returned.

Input:

```
-- RealCoords - array of shape channels x 3 - (x,y,z) cartesian
                  coordinates physical electrodes on a sphere with
                  center (0,0,0) and radius 1
-- data - array of shape channels x datapoints - containing values
          at electrodes in same order as in 'RealCoords'
-- diameter_samples - int - number of points along the diameter of
                      the scalp to interpolate
-- n - tuple of ints - how many terms of the Legendre-Polynomial
          should be calculated, defaults to (7,20)
-- m - int - order of the spherical spline interpolation,
          defaults to 4
-- smooth - float - amount of smoothing, defaults to 1E-5
-- projection - str - 'stereographic' (standard) or 'orthographic'
                    (explanations see above)
```

Output:

```
-- X, Y, Z - grid containing the X and Y coordinates and the
               interpolated values where everything outside the unit
               circle is masked. the unit of z is data.unit / m**2
```

```
calcCSD(Coords, data, n=(7, 20), m=4, smooth=1e-05, buffersize=64)
```

Calculate current source densities at the same electrode positions as in the original data set

Input:

```
-----
-- Coords - 2d array - channels x (x,y,z) cartesian coordinates of
              physical electrodes
-- data - array containing values at electrodes in same order as in
          'Coords'
          -- 1st dim: channels
          -- 2nd dim: datapoints
-- n - tuple of ints - How many terms of the Legendre-Polynomial
          should be calculated, defaults to (7, 20) - 7 for the first
          and 20 for the 2nd polynomial
-- m - order of the spherical spline interpolation, defaults to 4
-- smooth - float - amount of smoothing, defaults to 1E-5
-- buffersize - float - determine the size of a buffer in MB to do
                  the calculations
```

Output:

```
-----
-- pot - array containing CSD-values in data-unit / m**2
```

Example:

```
-----
>>> Coords = getStandardCoordinates(['C1', 'C3'])
>>> Coords = projectCoordsOnSphere(Coords) # be sure that the points are on a sphere
>>> data = _np.arange(6, dtype=float).reshape(2,-1)
>>> calcCSD(Coords, data)
array([[ -3.5474569 , -3.5474569 , -3.5474569 ],
       [ 3.60884286,  3.60884286,  3.60884286]])
```

```
smoothSP(Coords, data, n=(7, 7), m=4, smooth=1e-05, buffersize=64)
```

Calculate spatially smoothed potential values at the same electrode positions as in the original data set

Input:

```
-- Coords - 2d array - channels x (x,y,z) cartesian coordinates of
           physical electrodes
-- data - array containing values at electrodes in same order as in
         'Coords'
         -- 1st dim: channels
         -- 2nd dim: datapoints
-- n - tuple of ints - How many terms of the Legendre-Polynomial
      should be calculated, defaults to (7, 7) - 7 for the first
      and 7 for the 2nd polynomial
-- m - order of the spherical spline interpolation, defaults to 4
-- smooth - float - amount of smoothing, defaults to 1E-5
-- buffersize - float - determine the size of a buffer in MB to do
                  the calculations
```

Output:

```
-- pot - array containing the spatially smoothed potentials
```

Example:

```
>>> Coords = getStandardCoordinates(['C1', 'C3'])
>>> Coords = projectCoordsOnSphere(Coords) # be sure that the
>>> data = _np.arange(6, dtype=float).reshape(2,-1)
>>> smoothSP(Coords, data)
array([[ 0.01220571,  1.01220571,  2.01220571],
       [ 2.98778429,  3.98778429,  4.98778429]])
```

points are on a sphere

11.2 Variables

Name	Description
--package--	Value: 'meet'

12 Module meet.tf

S transform (time-frequency transformation)

Submodule of the Modular EEG Toolkit - MEET for Python.

the 'standard' S transform:

 Stockwell, Robert Glenn, Lalu Mansinha, and R. P. Lowe. "Localization of the complex spectrum: the S transform." Signal Processing, IEEE Transactions on 44.4 (1996): 998-1001.

as well as

the fast dyadic S transform:

 Brown, Robert A., M. Louis Lauzon, and Richard Frayne. "A general description of linear time-frequency transforms and formulation of a fast, invertible transform that samples the continuous S-transform spectrum nonredundantly." Signal Processing, IEEE Transactions on 58.1 (2010): 281-290.

Author:

 Gunnar Waterstraat
 gunnar[dot]waterstraat[at]charite.de

Example for a standard S transform:

 >>> import matplotlib.pyplot as plt
 >>> import numpy as np
 >>> data = np.random.random(1000) # generate a random 1000 dp signal
 >>> tf_coords, S = gft(data, sampling='full')
 >>> S = S.reshape(-1, data.shape[0]) # for the full transform no
 >>> plt.imshow(np.abs(S), aspect='equal', origin='lower') #plot the

interpolation is needed -> j
 result

Example for a dyadic S transform:

 >>> import matplotlib.pyplot as plt
 >>> import numpy as np
 >>> data = np.random.random(1000) # generate a random 1000 dp signal
 >>> tf_coords, S = gft(data, sampling='dyadic')
 >>> t, f, S_interp = interpolate_gft(tf_coords, S, (data.shape[0]//2,
 >>> plt.imshow(np.abs(S_interp), aspect='equal', origin='lower',

data.shape[0]), data.shap
 extent=[t[0], t[-1], f[0], f

12.1 Functions

```
gft(sig, window='gaussian', axis=-1, sampling='full', full=False, hanning=True)
```

Calculate the discrete general fourier family transform

Inputs:

- sig - signal of interest - 1 or 2 dimensional
- window - window function, standard is gaussian
- axis - axis along which transform should be performed
- sampling - 'full'/'dyadic' - should the S-domain be sampled completely, i.e. redundant or dyadic
- full - True|False - return also negative frequencies, standard is False
- hanning - True|False - Apply a hanning window to 5% first and last datapoints

Outputs:

- Coords - (frequency, time) Coordinates of each point in S
- S - complex S transform array
 - if sampling is dyadic interpolate.gft should be used to interpolate the result onto a regular grid
 - if sampling is full, this can be easily done by reshaping each S transform to the shape (-1, sig.shape[axis])

```
interpolate_gft(Coords, S, IM_shape, data_len, kindf='nearest', kindt='nearest')
```

Interpolate the result of a gft-transform - standard is nearest neighbor interpolation

Input:

```
-- Coords, Coords as output by the gft command
-- S - A gft result list
-- IM_shape - requested shape of the interpolated matrix
    1st axis frequency
    2nd axis time
-- data_len - length of initial data
-- kindf - interpolation method along frequency axis - any of
    ['nearest', 'linear']
-- kindt - interpolation method along time axis - any of
    ['nearest', 'linear']
```

Output:

```
-- wanted times - time point array
-- wanted freqs - frequency array
-- IM - interpolated matrix
```

12.2 Variables

Name	Description
<code>--package--</code>	Value: 'meet'

Index

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