

Thesis Proposal

September 11, 2021

1 Introduction

Background overview

Tracheal intubation (usually called intubation) is an operation to put the tract tube into the tracheal by passing the upper respiratory tract. It can keep the patient's airway unobstructed. In general anesthesia surgery, patients lost consciousness and can't breath themselves. Tracheal intubation becomes the principal method to build the artificial breath channel which can maintain the breath of patients. Under normal circumstances, anesthetist is responsible for inserting the intubation tube from the mouth into the trachea. However, the patients with poor airway evaluation result need to be intubated through the nasal cavity. If the operation failed several times or in emergency situations, anesthetist will cut off the cricothyroid cartilage to expose trachea, and then the tracheal tube through the wound. If failed over three times, the tracheal spasm will be caused. The difficulty of intubation increases exponentially, which may delay the time of ventilation and cause suffocation. At this time, more professional anesthesiologists are required to continue the tracheal intubation.

Significance and difficulties

We want to reduce the work burden of the anesthesiologists. According to the researches, the current number of anesthesiologists in China is 76,000 and the number of hospitals (including private hospitals) is 34,534. There is currently a shortage of 300,000 professional anesthesiologists. Many departments share an anesthesiologist and the hard work burden leads to the death of them. And Down's syndrome patients, patients with facial tumors, with natural throat exposed, are difficult to successfully insert the tracheal tube. They need an efficient method. About the patients with loose tongue muscles or obesity, the tongue tends to droop and block the throat. Patients with poor grades of difficult airways cannot insert a laryngoscope during intubation.

Methodological Design

The key of endotracheal intubation lies in the positioning and control of the end. In the aspect of localization, this project plans to use the magnetic dipole to locate the terminal. In the aspect of control, the pneumatic muscle can achieve this goal well.

2 Design

The robot consists of two parts. One is the expander part, responsible for expanding the trachea. Another is the locator part, responsible for locating the location in trachea.

Expander part

Pneumatic muscle

Figure 1 shows the structure of the pneumatic muscle. As air is pumped out of the muscle, it becomes compressed, and the support is compressed. As air is pumped into the muscle, it becomes stretched, and extends the support part. We will use silicone injection molding or 3D printing to print the muscle. When it is compressed, its length should not be longer than $\pi \text{ cm}$, which is the size for operation with these special patients allowed. As it is stretched, its length should not be less than $2\pi \text{ cm}$.



Figure 1: muscle structure

Support

As show in Figure 2, this part include four TPU cylinders with length of 40 cm and diameter of 3 mm. The part is responsible for enlarging the passage from the mouth to the trachea, which can make sure the tracheal tube can be put into tracheal correctly, and take out the locator part.

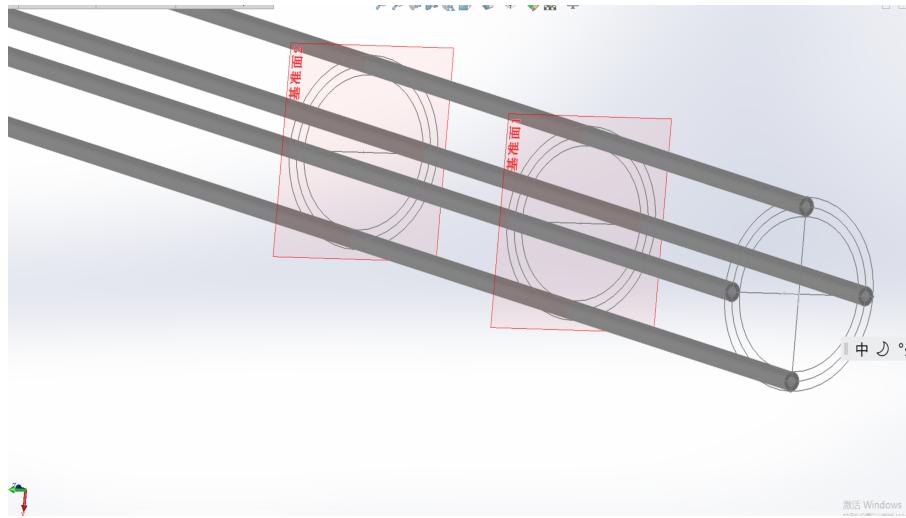


Figure 2: support part to enlarge the tracheal

Locator part

Mathematical Model

As shown in Figure 3, the system uses three-axis generating coils and the 3-axis sensor coils, which are along with the related electronic circuitry. The signals from the three-axis generating coils can be detected by the three-axis sensor coils by using time-sharing or frequency-coupling methods. By defining the

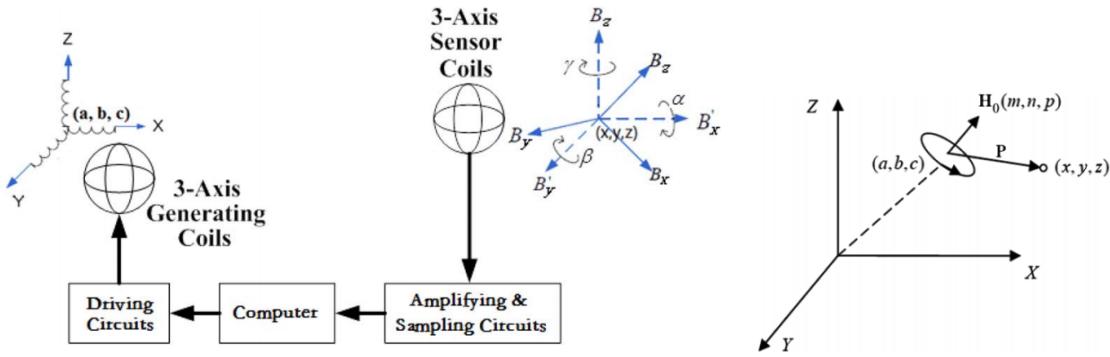


Figure 3: mathematical model of electronic dipole

coordinate frame, the position of the three-axis generating coils can be defined by (a, b, c) ; the position and orientation of the three-axis sensor coils can be defined by $(x, y, z, \alpha, \beta, \gamma)$, where (x, y, z) is the center position of the sensor coils and (α, β, γ) represents the rotation angle of the sensor coils with respect to the global coordinate frame.

And after a series of mathematical and physical deductions, finally we reach this.

$$x = \pm \frac{\sqrt{B_1^2/B_T^2 - B^2/(6B_T^2)}}{\sqrt{3[B^2/(6B_T^2)]^{2/3}}}$$

$$y = \pm \frac{\sqrt{B_2^2/B_T^2 - B^2/(6B_T^2)}}{\sqrt{3[B^2/(6B_T^2)]^{2/3}}}$$

$$z = \pm \frac{\sqrt{B_3^2/B_T^2 - B^2/(6B_T^2)}}{\sqrt{3[B^2/(6B_T^2)]^{2/3}}}$$

Where M_T is a constant defining the magnetic intensity of the dipole, and

$$B_T = \mu_r \mu_0 M_T / 4\pi$$

$$B = \frac{6B_T^2}{R^6}$$

$$R = \sqrt{(x - a)^2 + (y - b)^2 + (z - c)^2}$$

Structure Design

In order to achieve this goal, we designed a positioning shuttle and a set of receivers.

As shown in Figure 4 the khaki-colored part is a shuttle-shaped main body made of engineering plastics, used for coil support. The body is wound with a two-dimensional coil to position the shuttle from two dimensions (the third dimension is controlled by the depth of the tube insertion).

An optical camera can be mounted on the front of the positioning shuttle, with a speculum function.

When working, the positioning shuttle sends out signals, and four external positioning coils receive signals, and the positioning is completed by reference to the algorithm mentioned above.

After positioning, the system finds the trachea by controlling the pneumatic muscles of the expanded part to move in a direction.

Schedule

Figure 5 shows the schedule of our project.

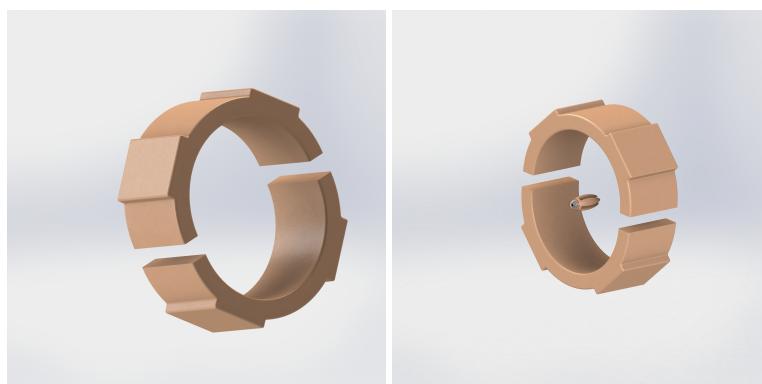


Figure 4: Structure design of locator part



Figure 5: schedule of project

References

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