



# Magnetically Enhanced Microflow Cytometer for Bead-based Immunoaffinity Measurements in Blood Samples

Master Thesis Presentation

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Munich, 31.03.2021

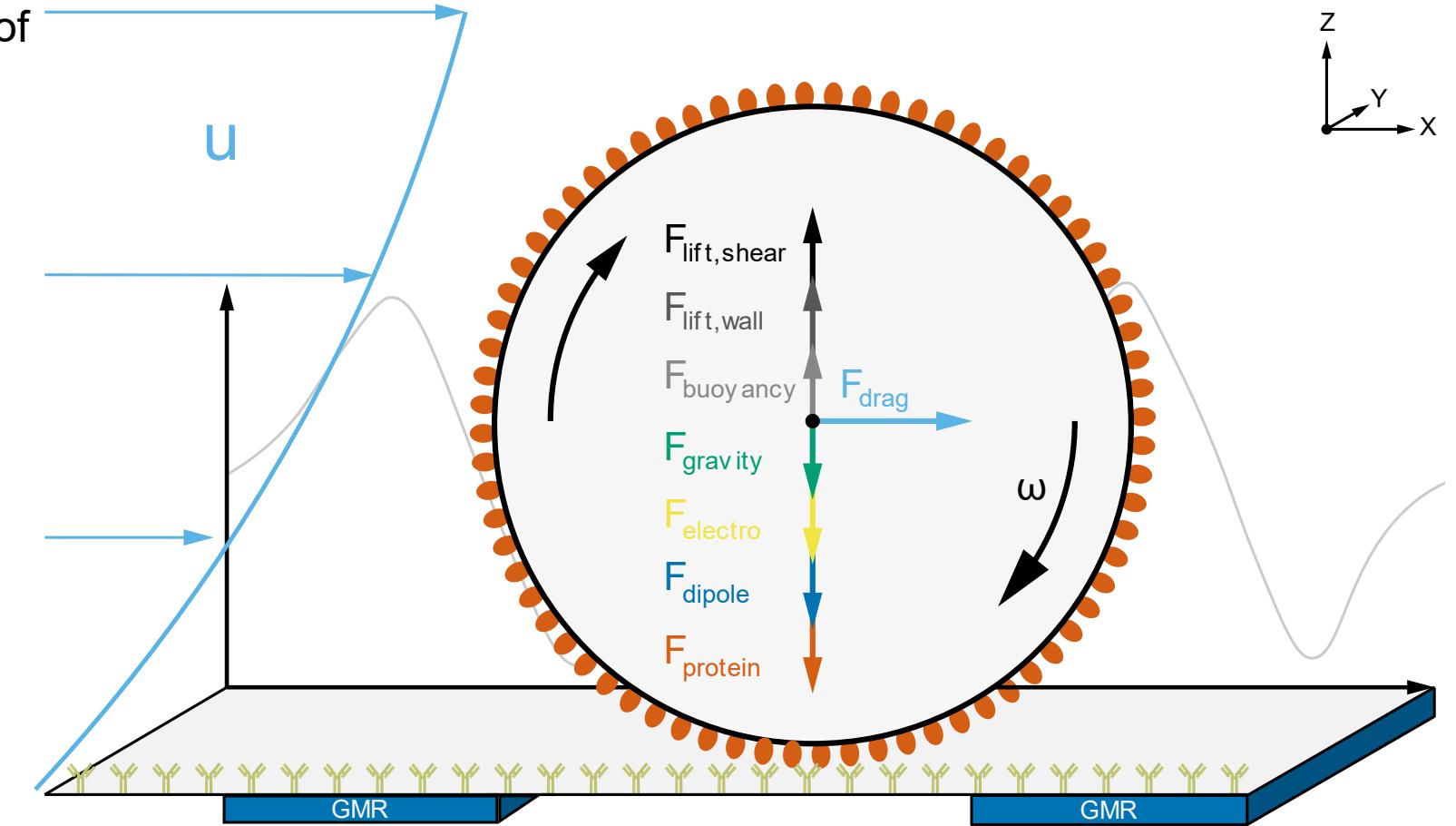
# Outline

- Theory
  - Immuno-Affinity Measurements in the Magnetic Flow Cytometer
  - Surface Chemistry Methods
- Results
  - Simulation
    - Virtual Prototyping of Cell Signals
    - Calculus Estimation of the Force-Equilibrium in a Microchannel
  - Experimental
    - Magnetic Concentration Measurements
    - Development of a Differential Counting Setup
    - Established Reference Model for Surface Marker Expression Densities
    - Affinity-based Concentration Measurements in the Magnetic Flow Cytometer
- Conclusion

# Theory

## Immuno-Affinity Measurements in the Magnetic Flow Cytometer

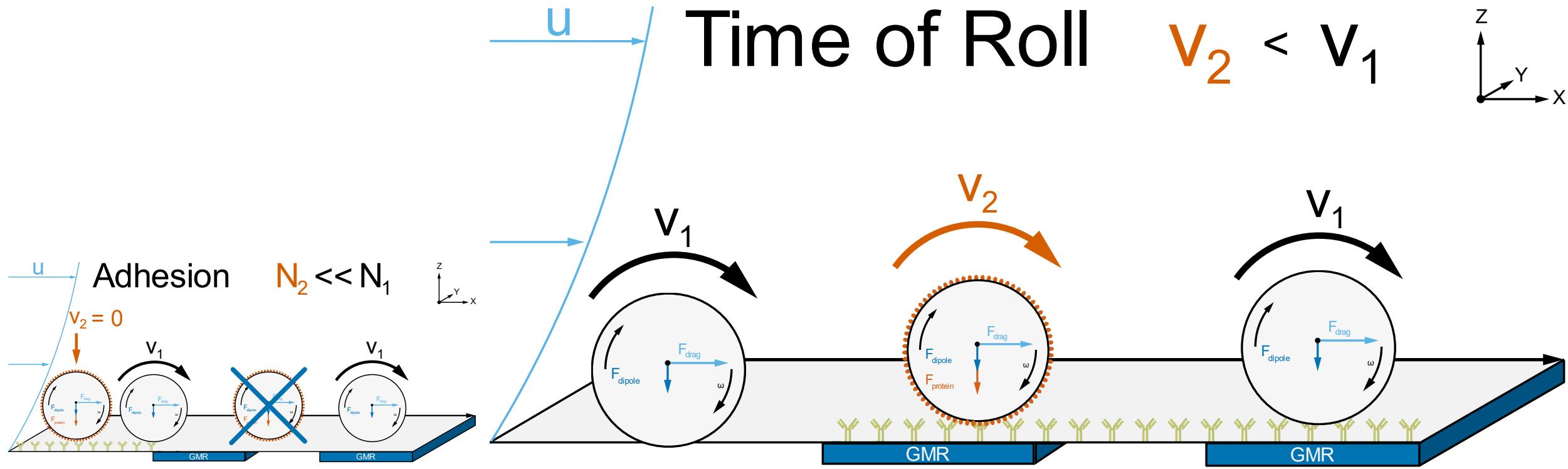
- Magnetic bead rolling on the floor of a microchannel
  - Biofunctionalized Channel
  - Force-Equilibrium:
    - Hydrodynamics
    - Volume Forces
    - Electro-Magnetism
- Change in Velocity or Adhesion





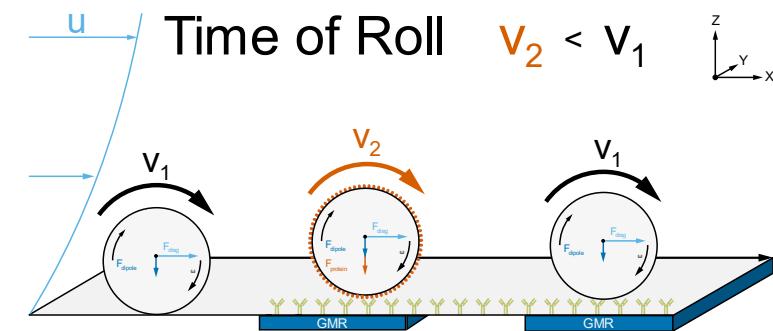
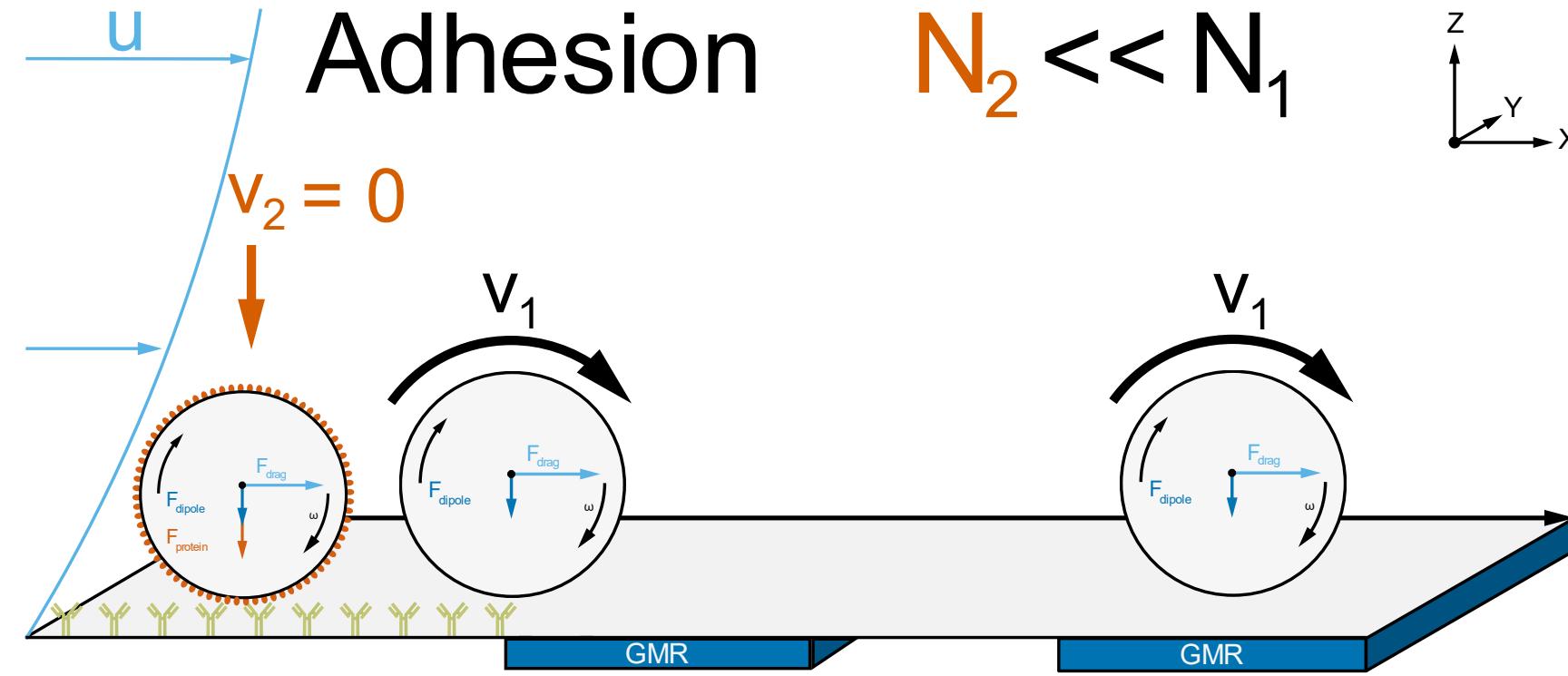
# Theory

## Immuno-Affinity Measurements in the Magnetic Flow Cytometer



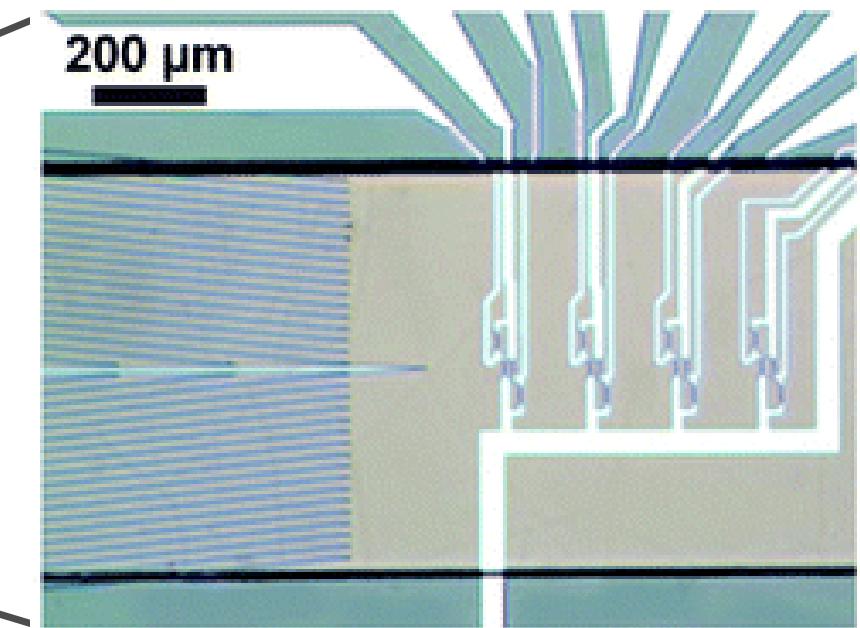
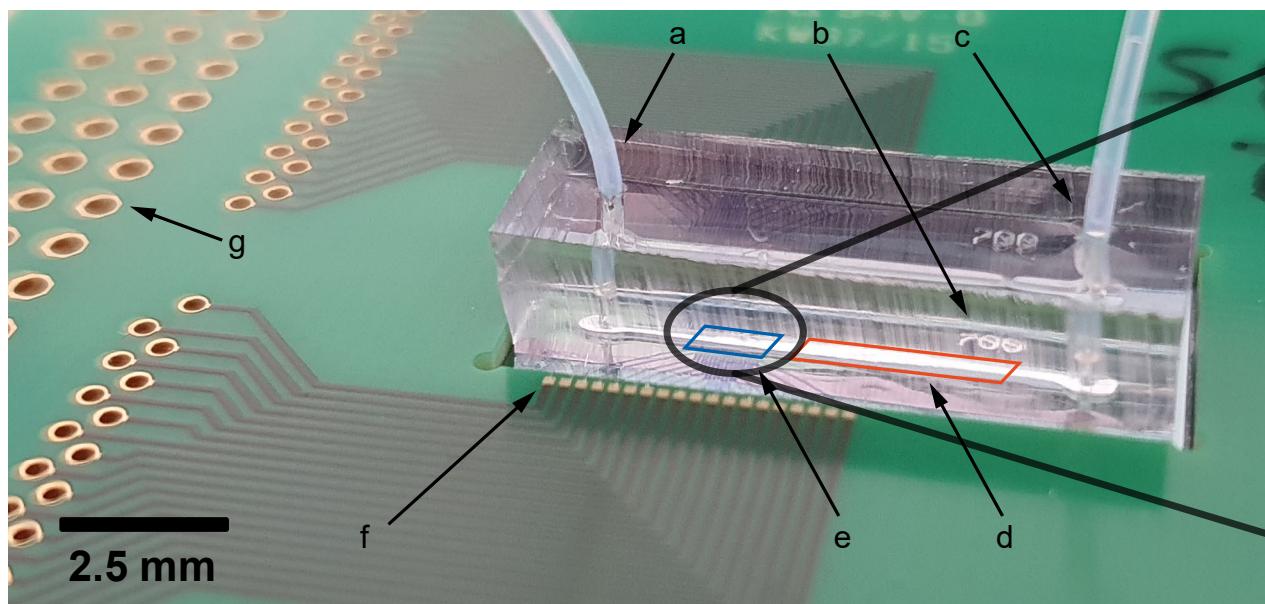
# Theory

## Immuno-Affinity Measurements in the Magnetic Flow Cytometer



# Theory

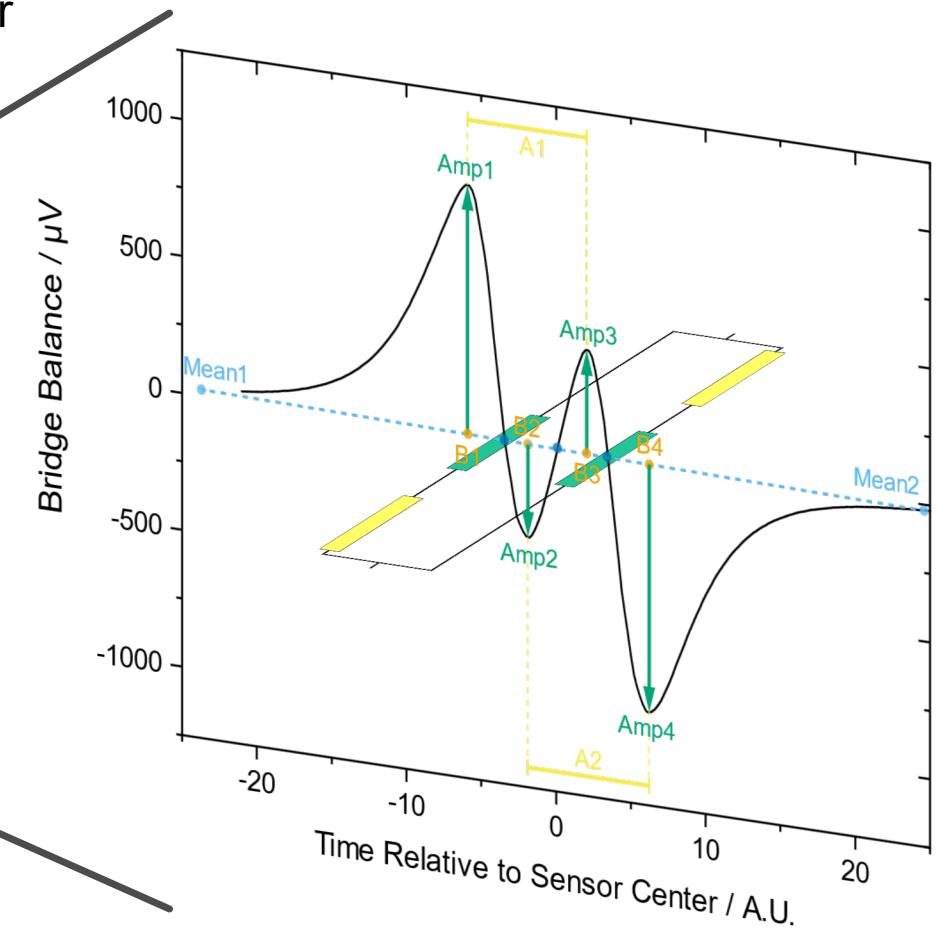
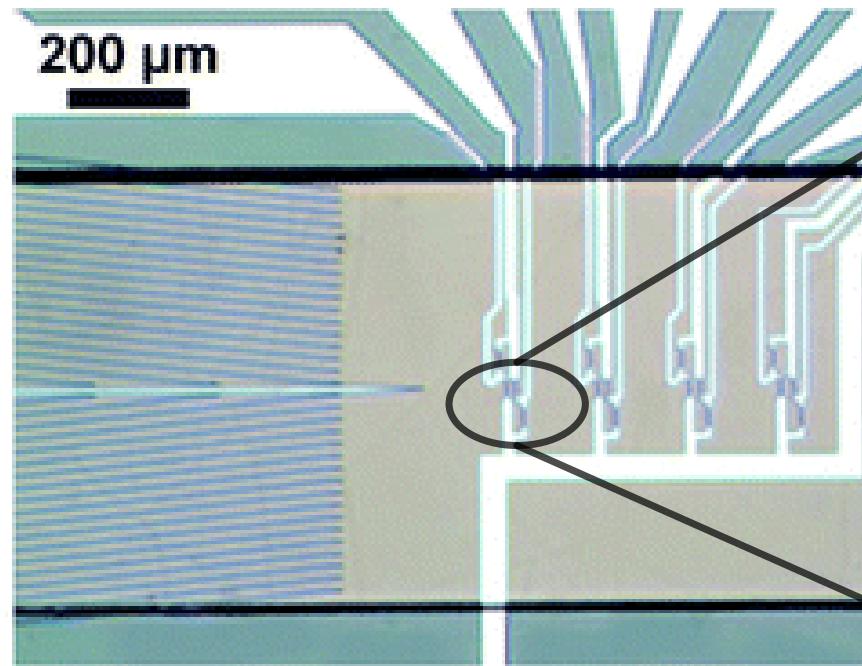
## Immuno-Affinity Measurements in the Magnetic Flow Cytometer



Helou et al. (2013) *Lab on a Chip*, 13(6)

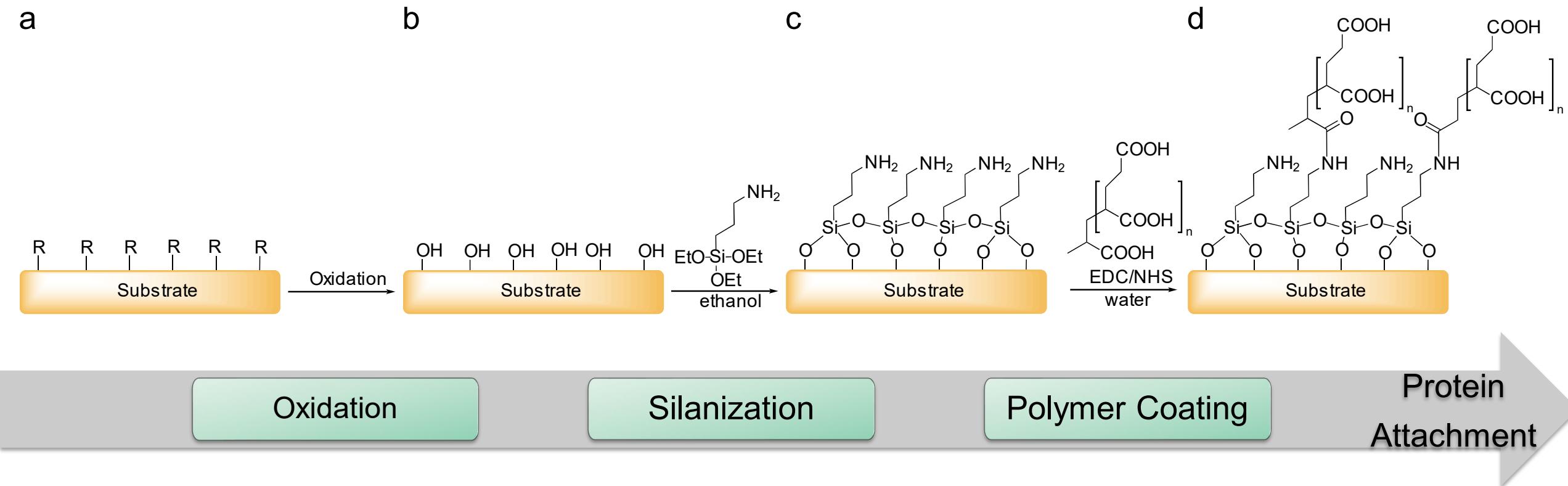
# Theory

## Immuno-Affinity Measurements in the Magnetic Flow Cytometer



## Theory

Surface Chemistry Methods – Covalent Modification

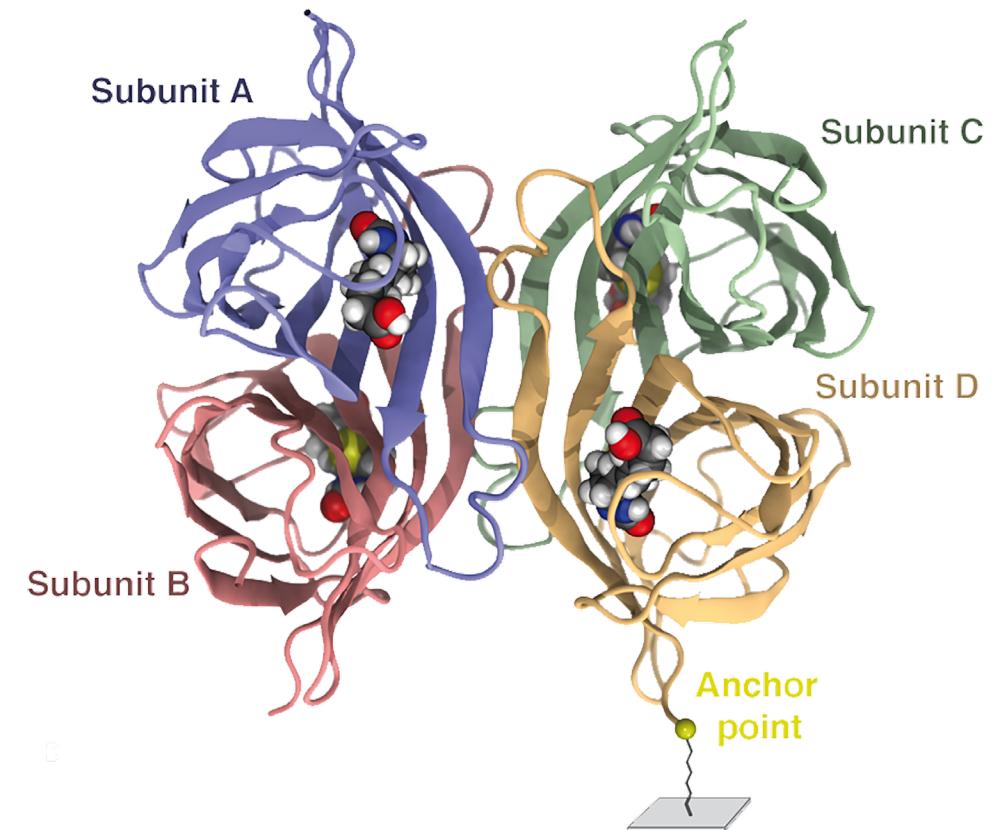
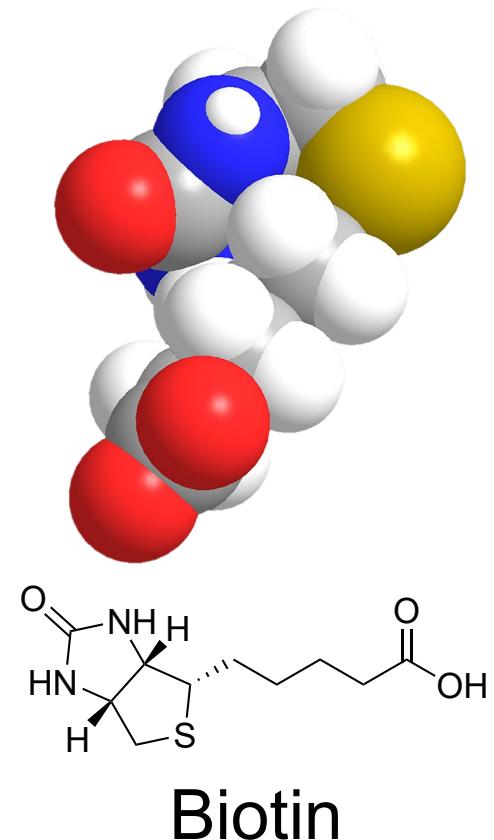


# Theory

## Surface Chemistry Methods – Biotin-Streptavidin

- Biotin-Streptavidin Interaction
- One of the strongest known non-covalent bonds
- Affinity:  $K_d = 10^{-13} - 10^{-15}$
- Release force: 100 – 400 pN

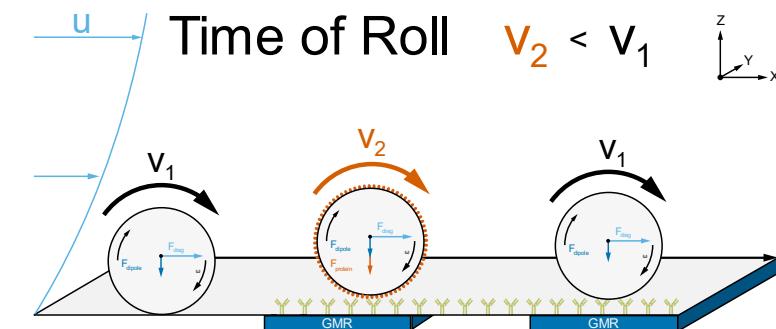
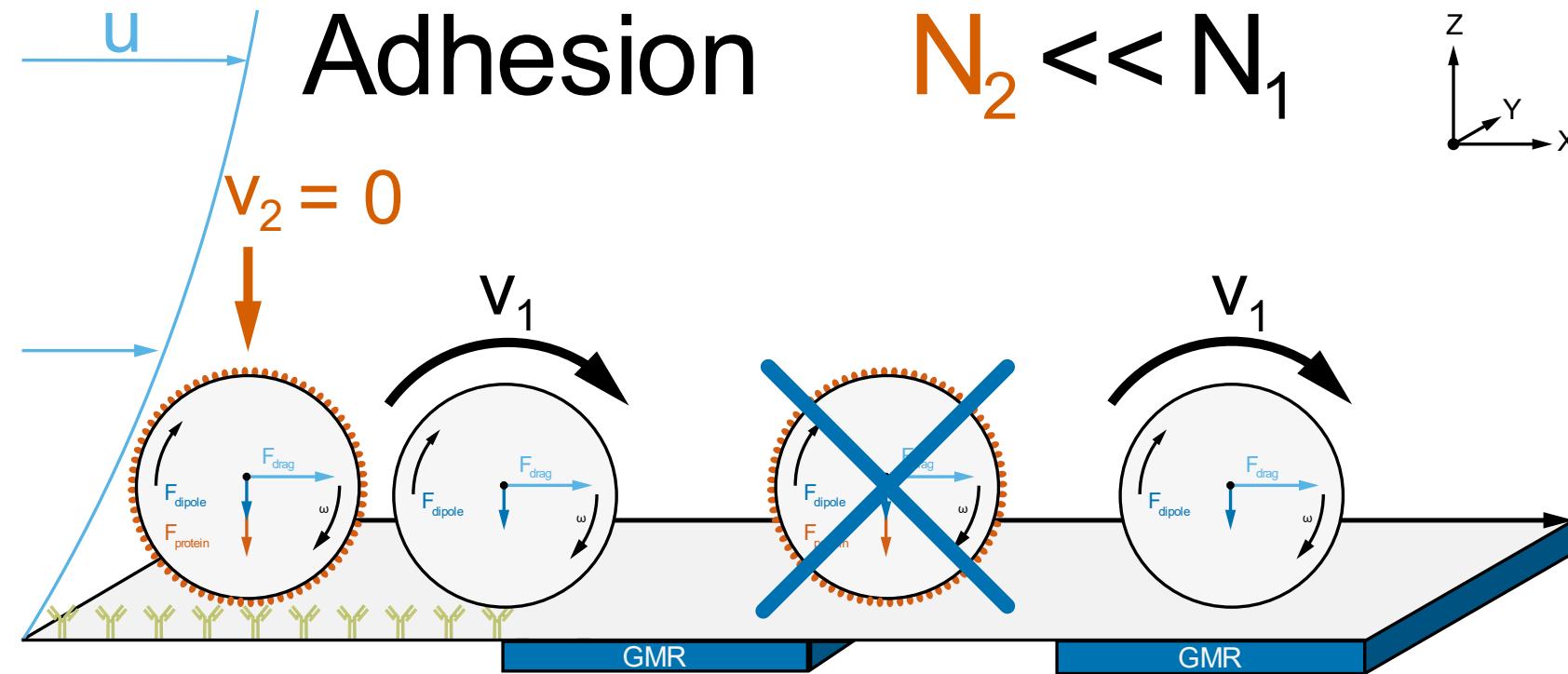
→ Adhesion



Sedlak et al. (2020) *Sci Adv*, 6(13)

# Theory

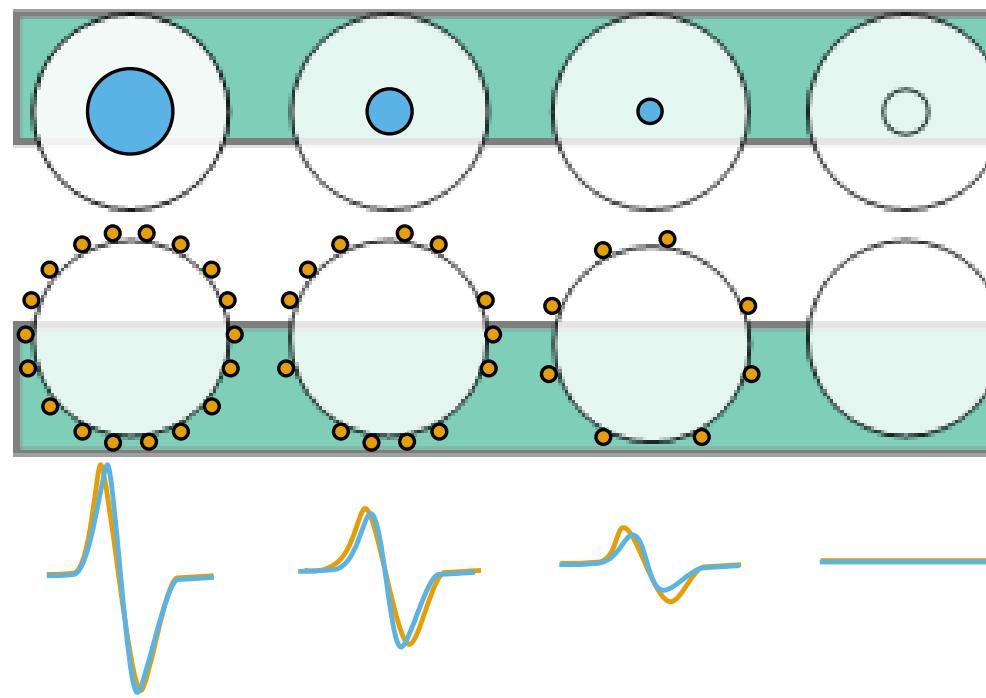
## Surface Chemistry Methods – Biotin-Streptavidin





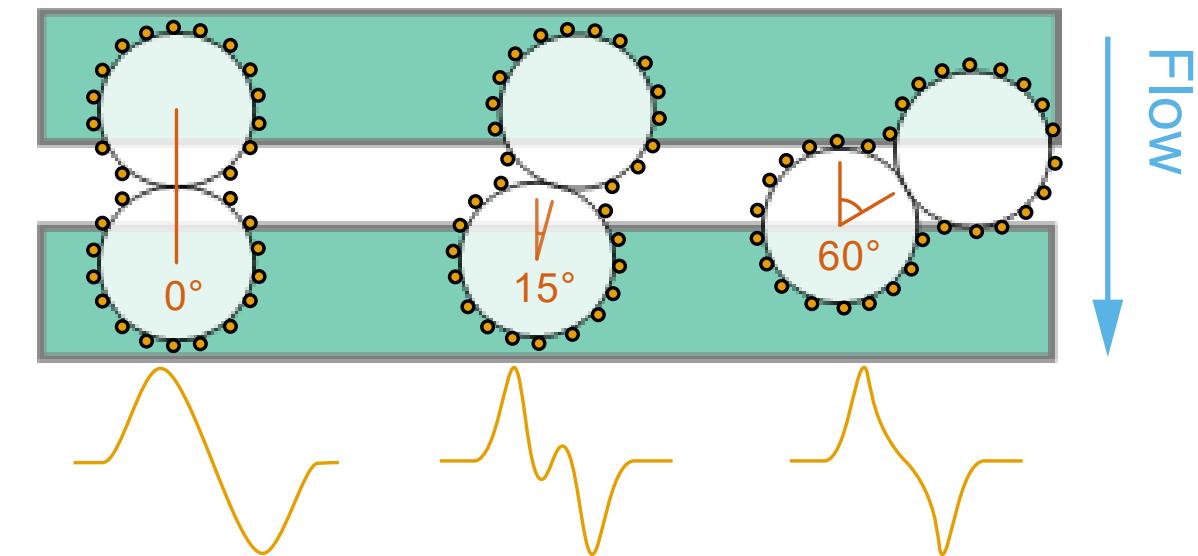
# Results

Simulation – Virtual Prototyping of Cell Signals



MNP-Coverage Evaluation

FLOW

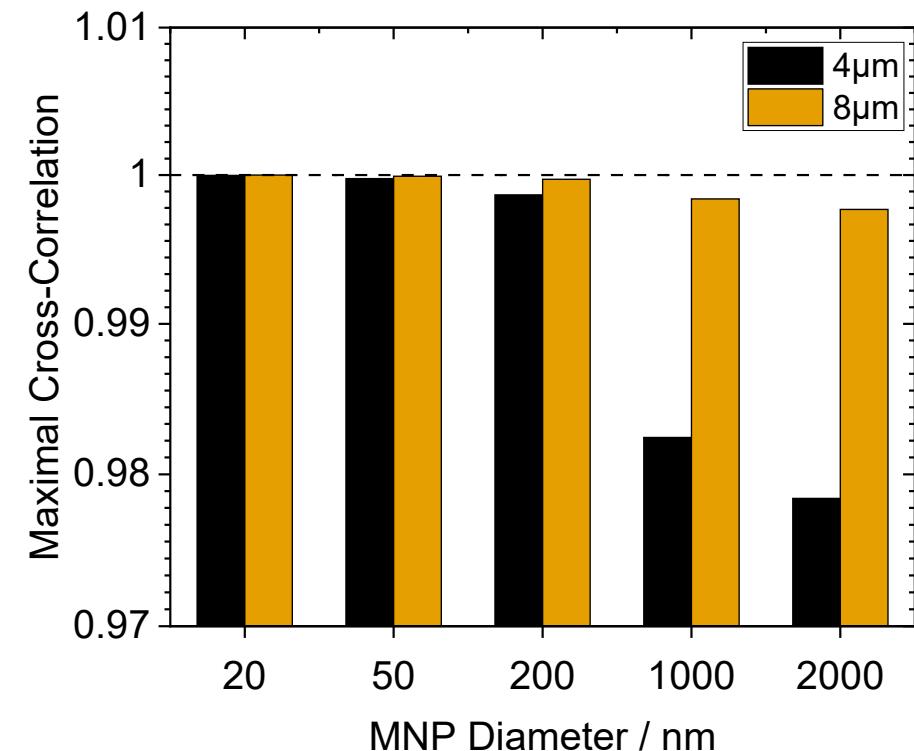
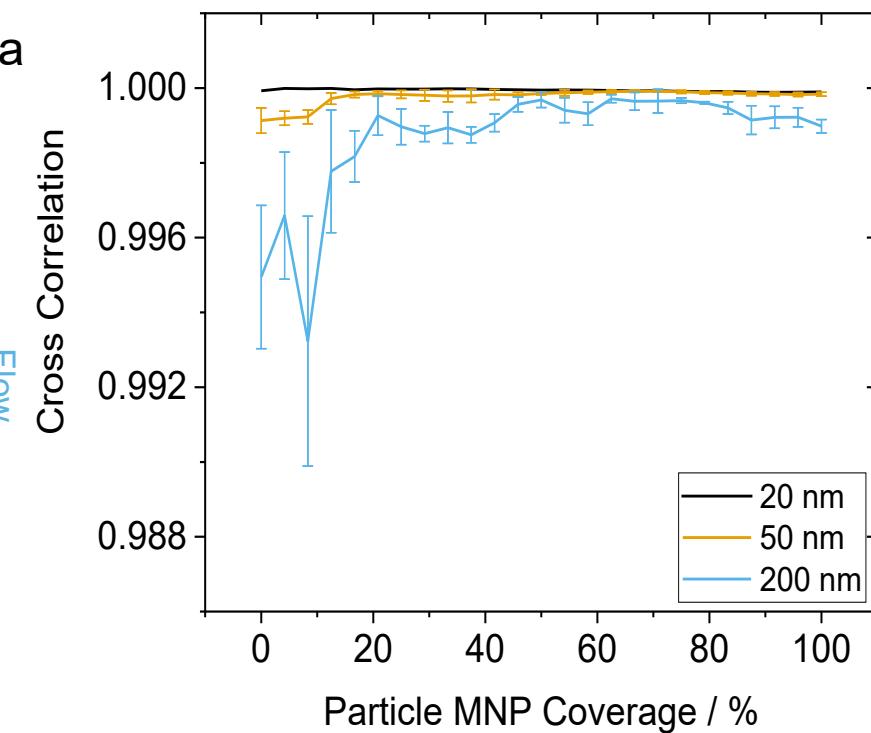
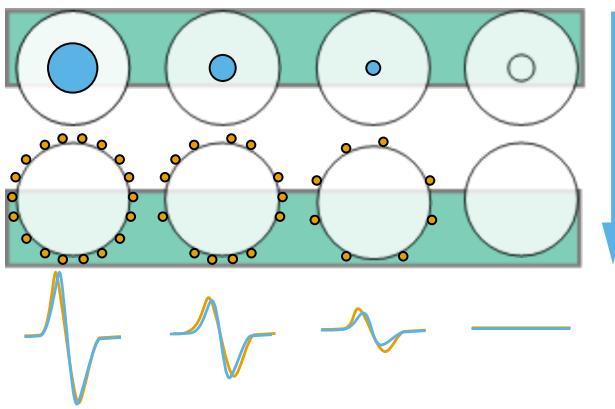


Aggregate Angle Evaluation

# Results

## Simulation – Virtual Prototyping of Cell Signals

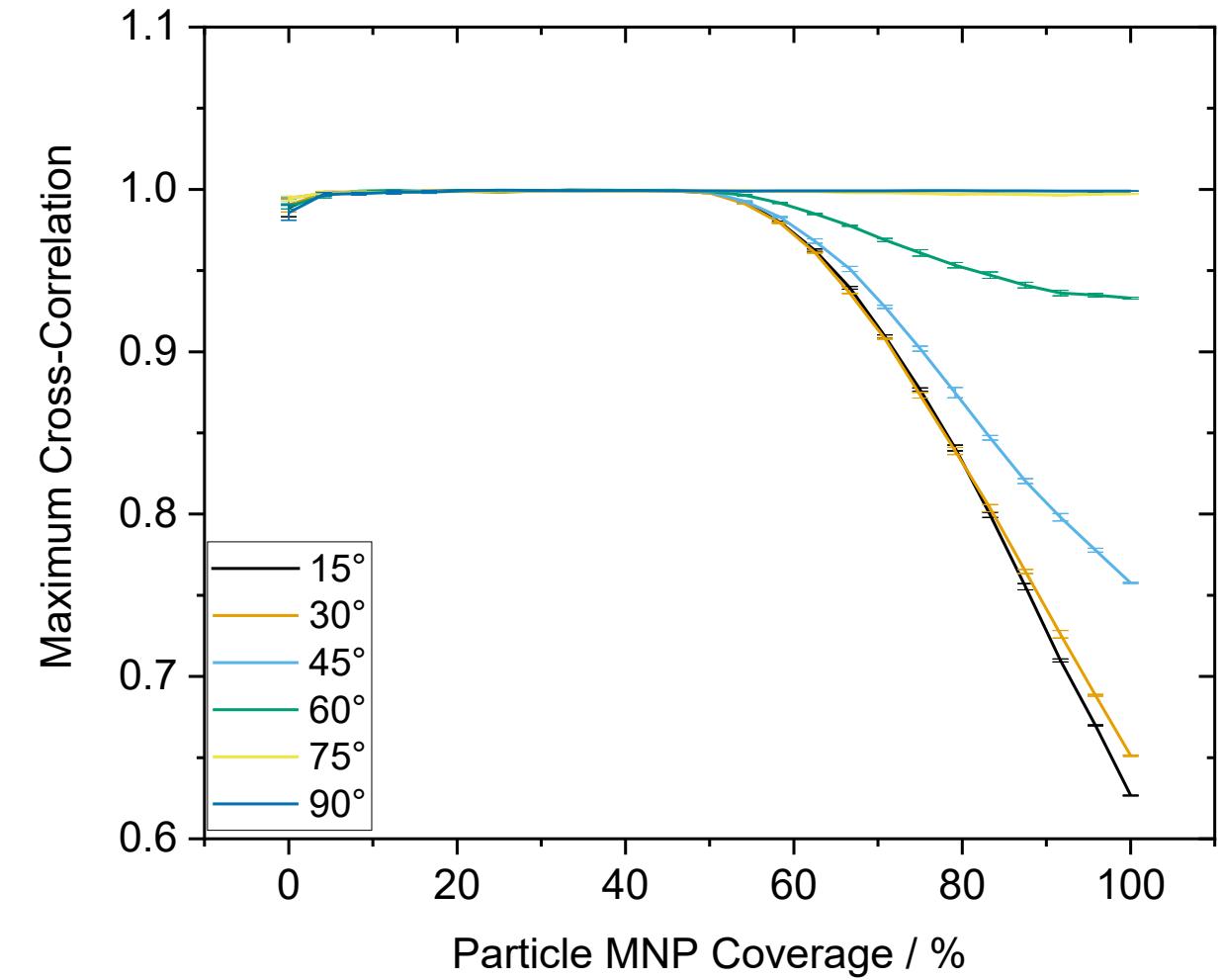
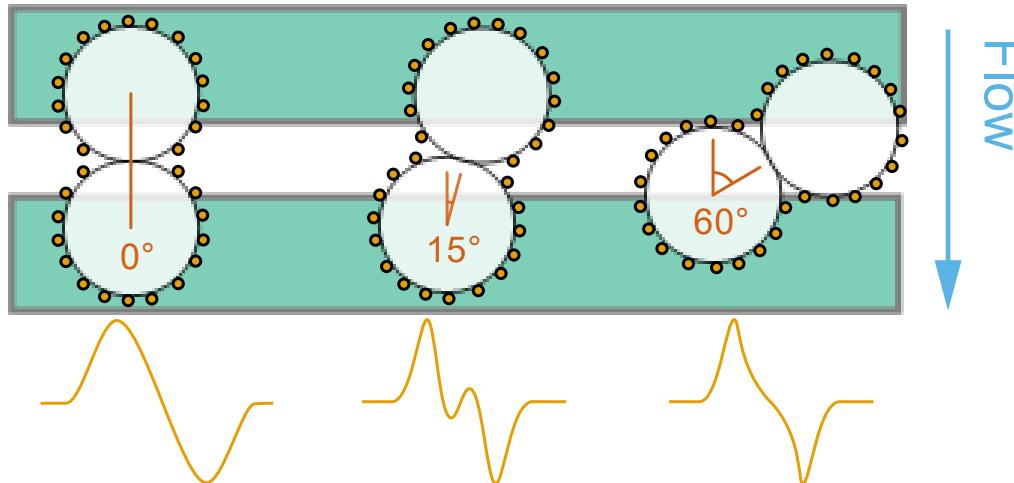
- Low Coverage:
  - Single Magnetic Momenta cause field inhomogeneity
  - Signal deterioration for larger MNP diameters



# Results

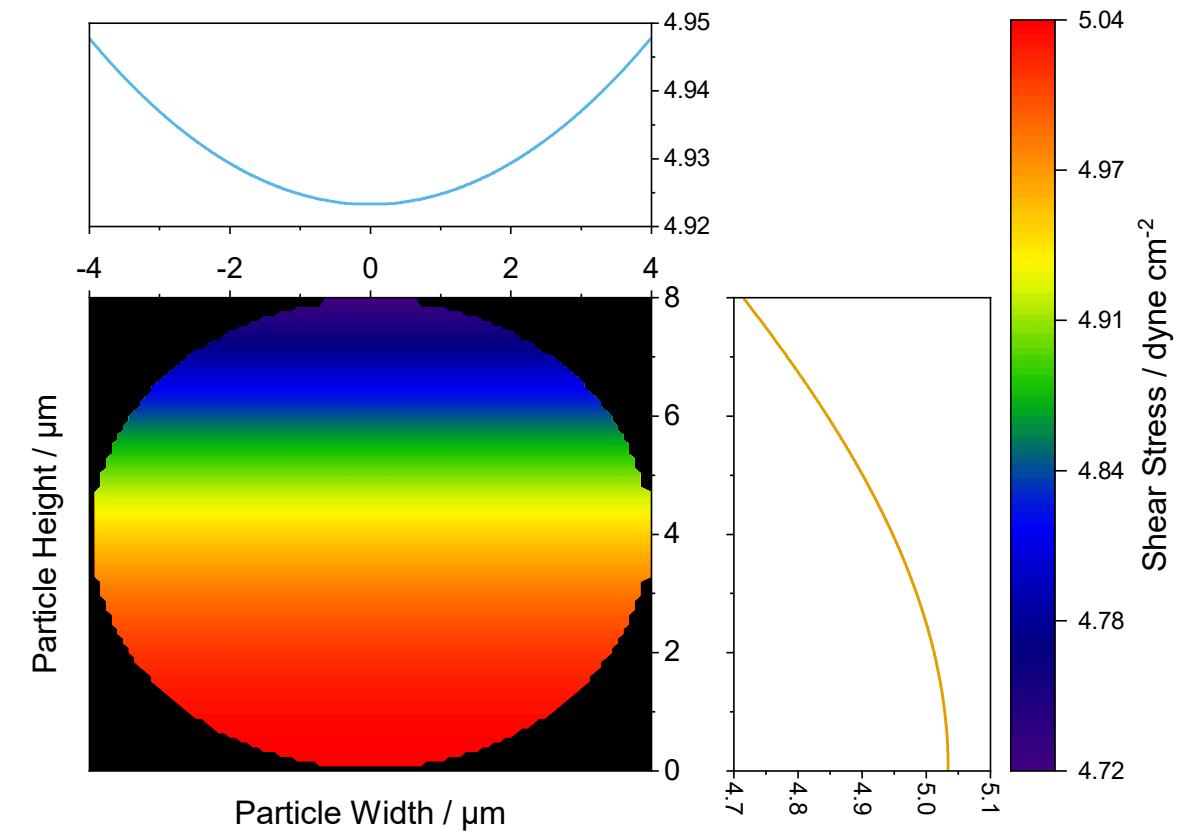
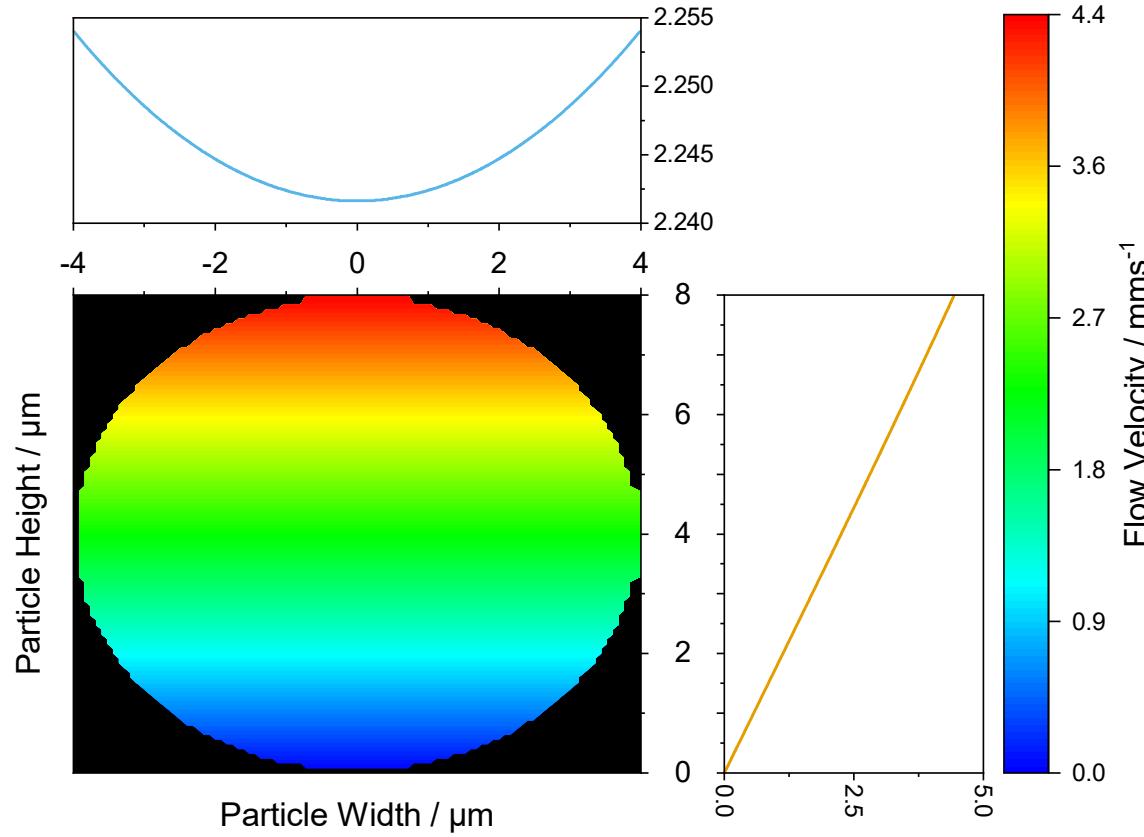
## Simulation – Virtual Prototyping of Cell Signals

- High correlation in the medium coverage regime due to inhomogeneous field
- Low yaw and high coverage → Two dipoles in superposition
- High yaw and coverage → Aggregate cannot be discriminated by the sensor



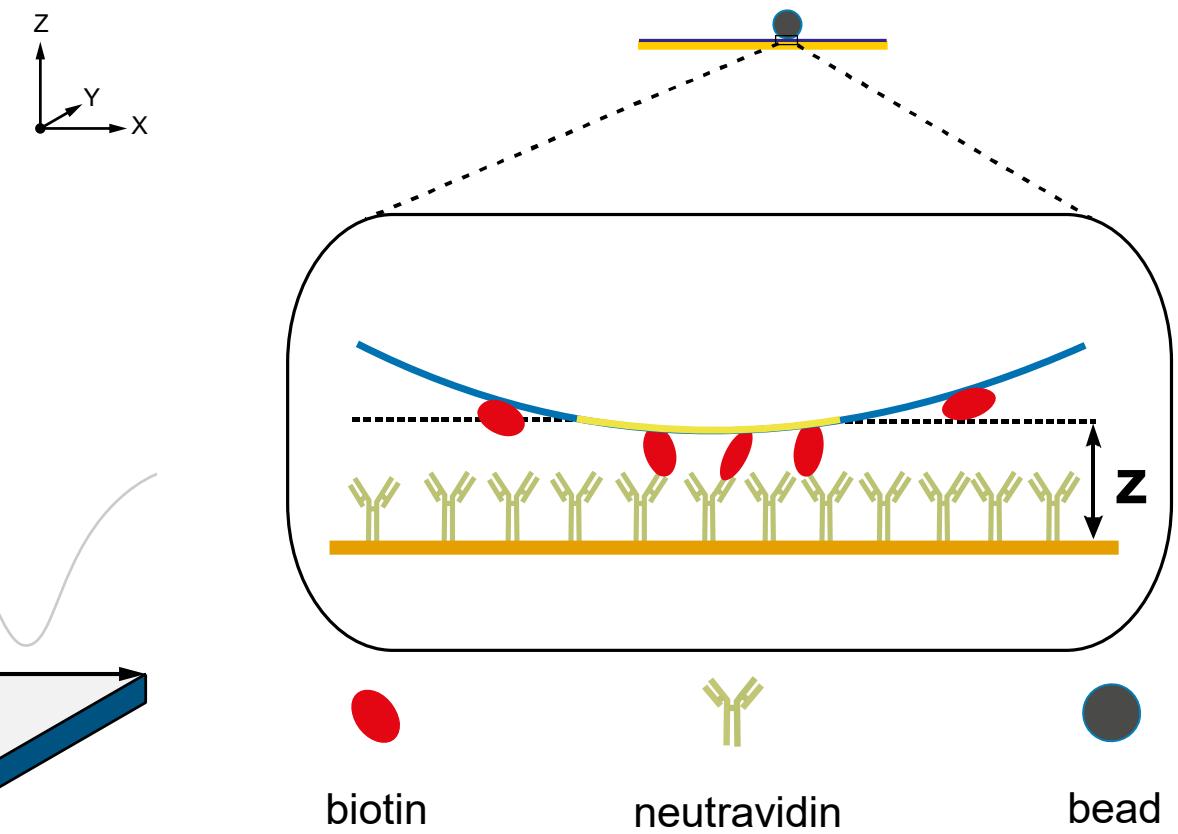
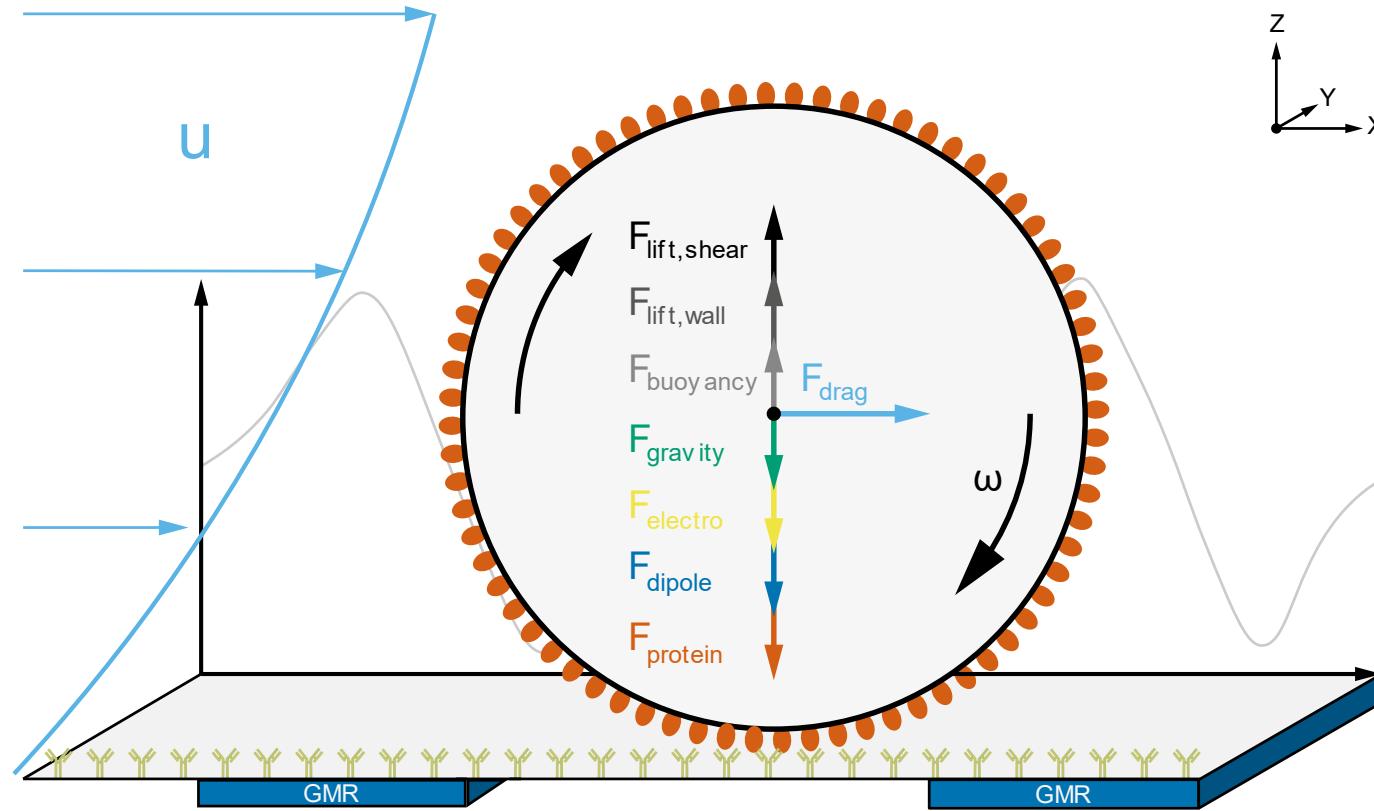
# Results

Simulation – Calculus Estimation of the Force-Equilibrium in a Microchannel



# Results

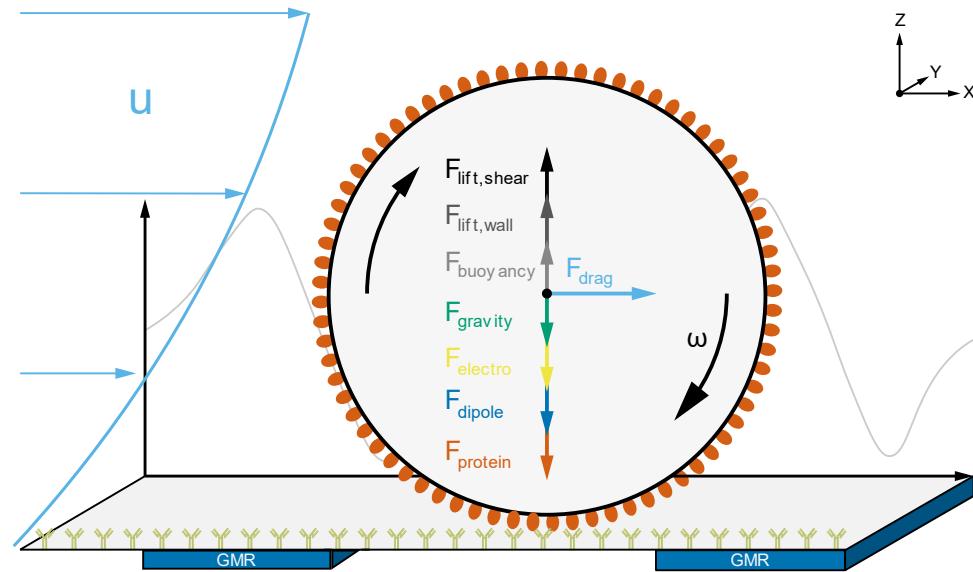
## Simulation – Calculus Estimation of the Force-Equilibrium in a Microchannel



Adopted from Wu and Voldman (2020) *Biosensors and Bioelectronics*, 154, 112070.

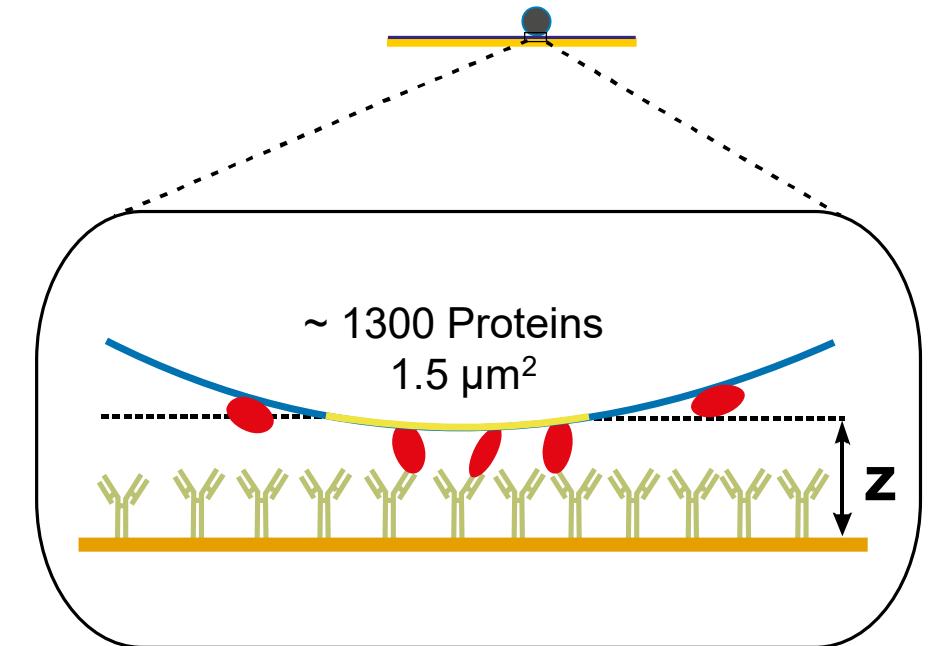
# Results

## Simulation – Calculus Estimation of the Force-Equilibrium in a Microchannel



$$F_{||} = F_{\text{drag}} - C_{rr} \cdot (F_{\text{mag}} + F_{\text{protein}} + F_{\text{grav}} - F_{\text{shear}})$$

$$C_{rr} = \sqrt{\frac{z}{d}} = \sqrt{\frac{30 \text{ nm}}{8 \mu\text{m}}} = 0.0612$$



biotin

neutravidin

bead

Adopted from Wu and Voldman (2020) *Biosensors and Bioelectronics*, 154, 112070.

# Theory

## Surface Chemistry Methods – Biotin-Streptavidin

### Predominant Forces

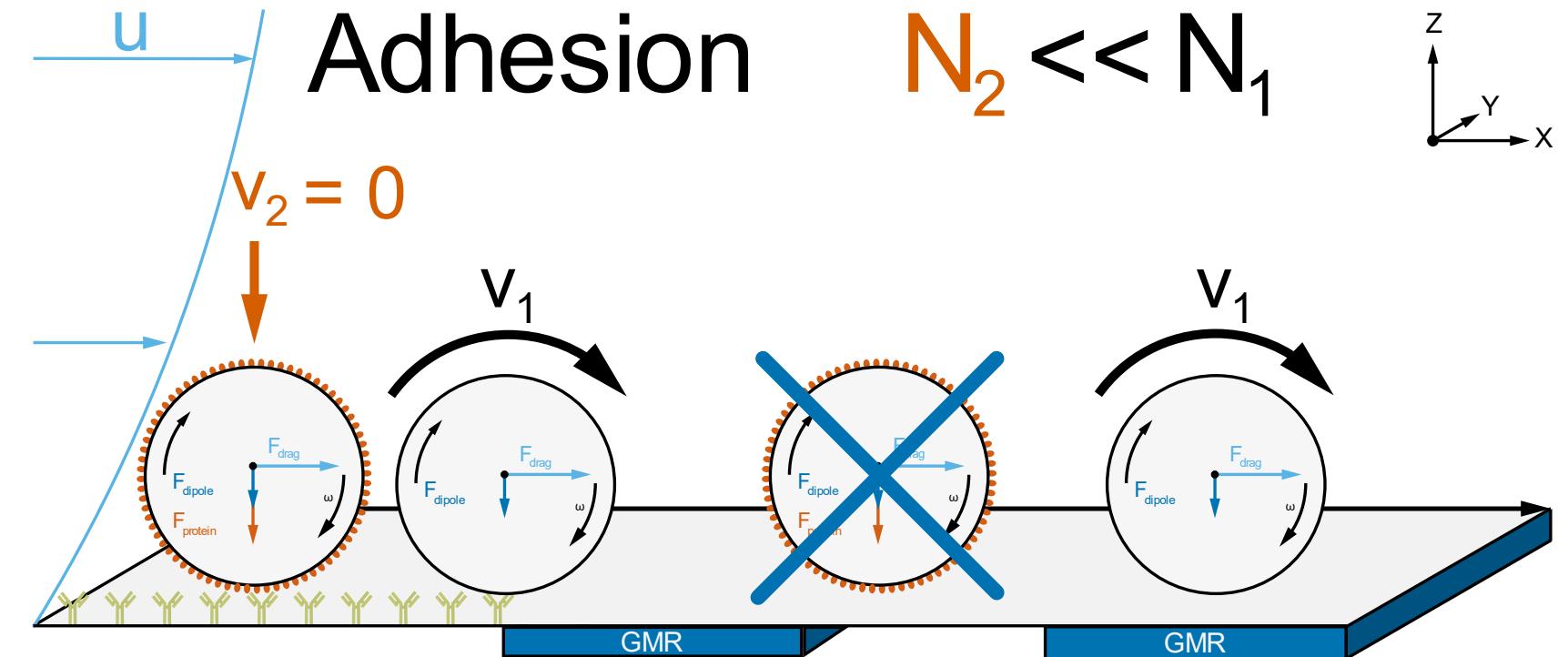
- Stoke's Drag: 460 pN
- Dipolar Force: 5 nN
- Protein Force: 5-200 nN

### Unfunctionalized Bead

- 150 pN Drag

### Bio-Functionalized Bead

- Adhesion caused by 16 - 500 molecules of neutravidin



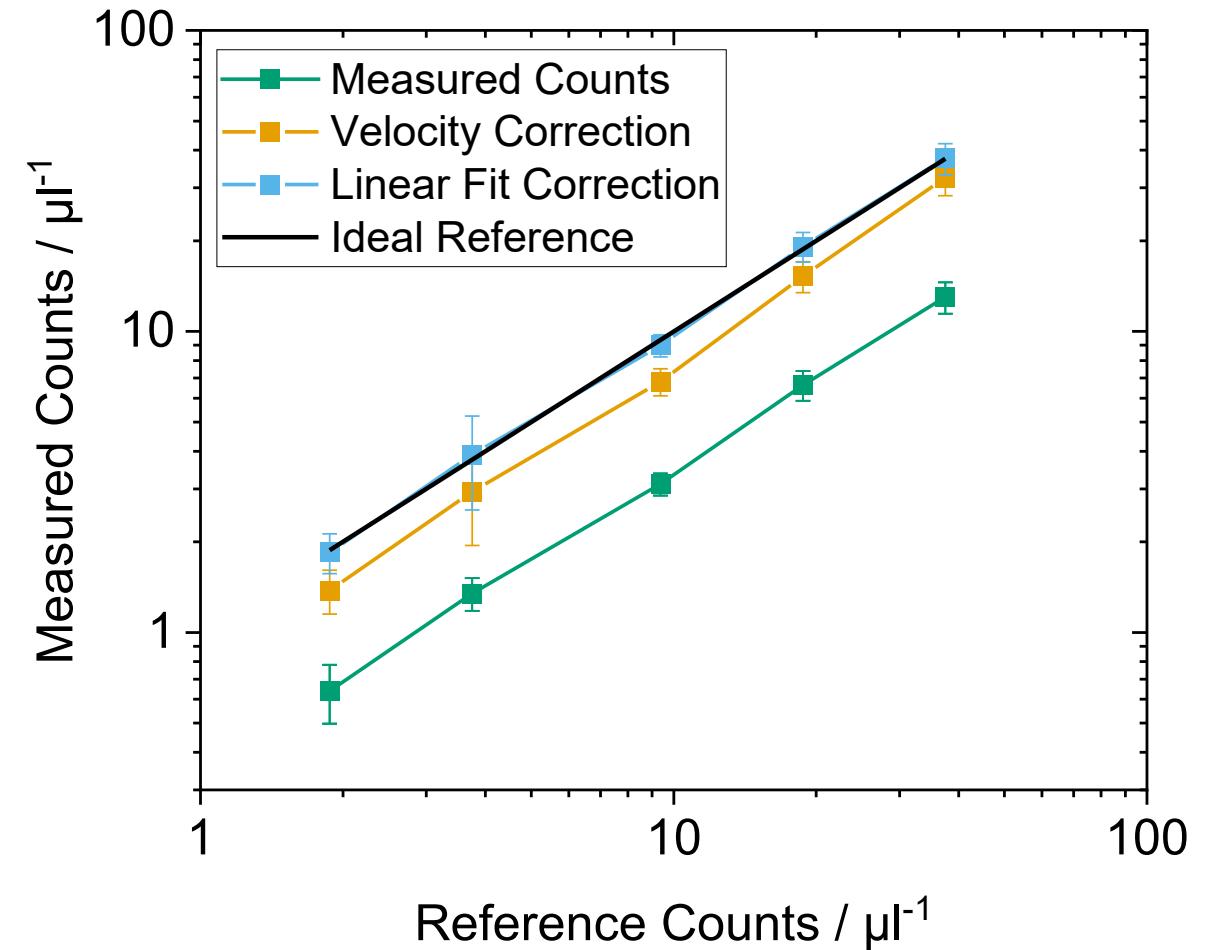
# Results

## Experimental – Magnetic Concentration Measurements

- Bead stocks characterized in the flow cytometer precisely
- Empirical correction factors to account for bead losses in interconnections and flow profile:

$$C_{\text{const}} = \frac{c_{\text{beads, standard procedure}}}{c_{\text{beads, MRCyte}}}$$

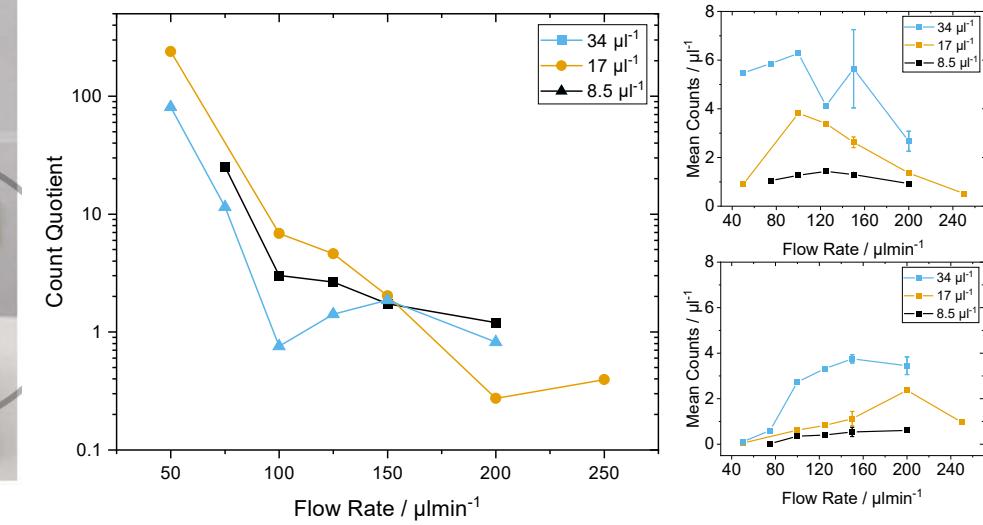
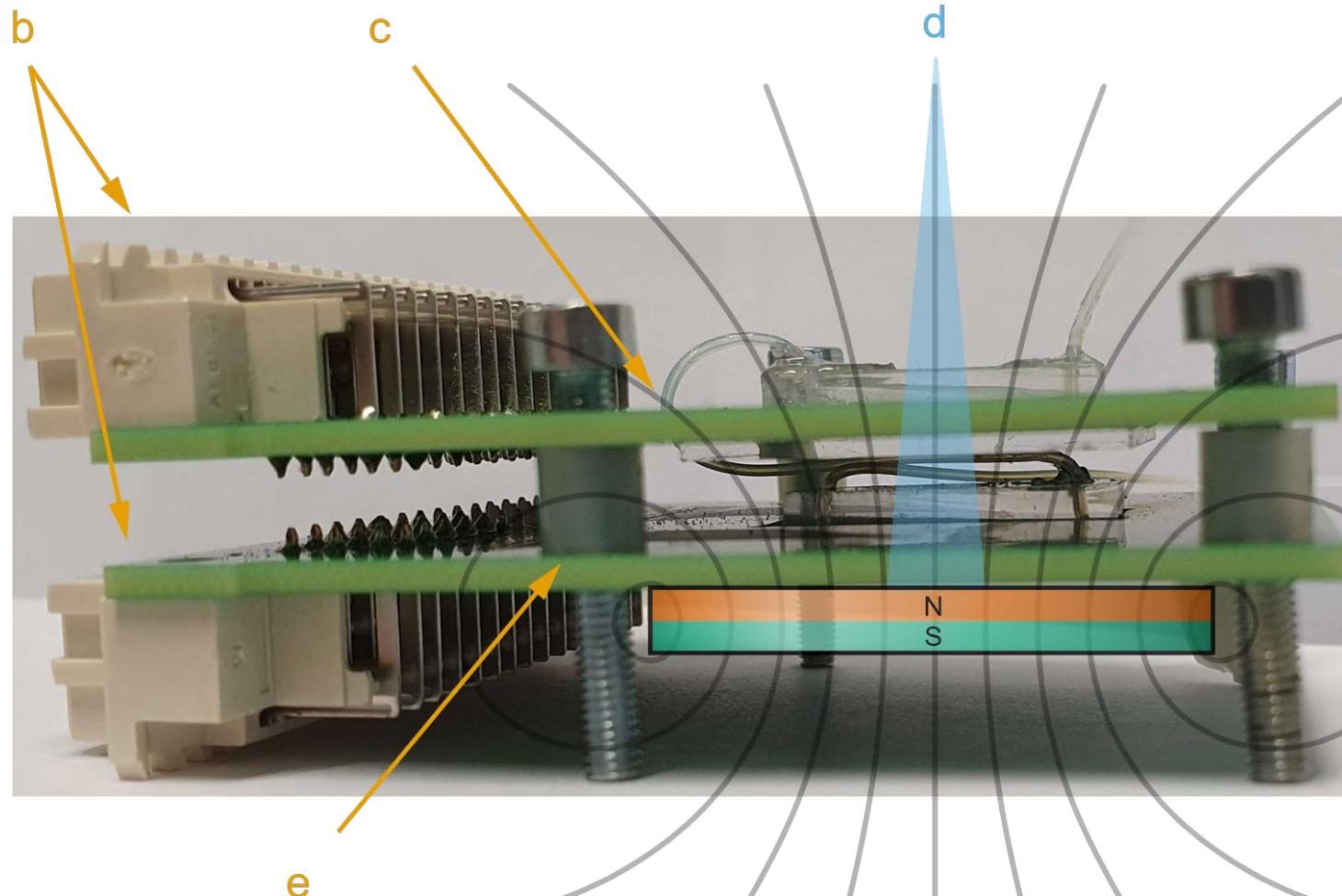
$$C_{\text{velocity}} = \frac{\bar{u}}{v_c} = \frac{Q}{A \cdot v_c}$$





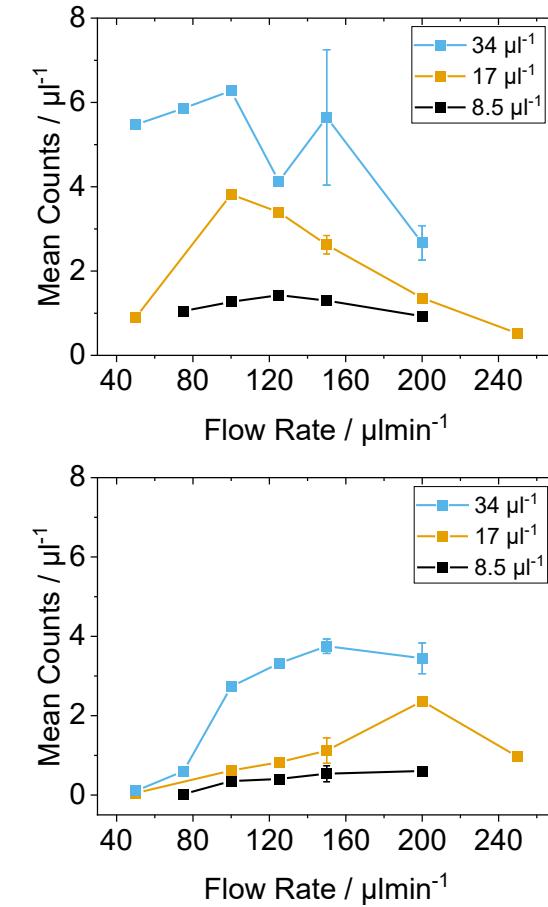
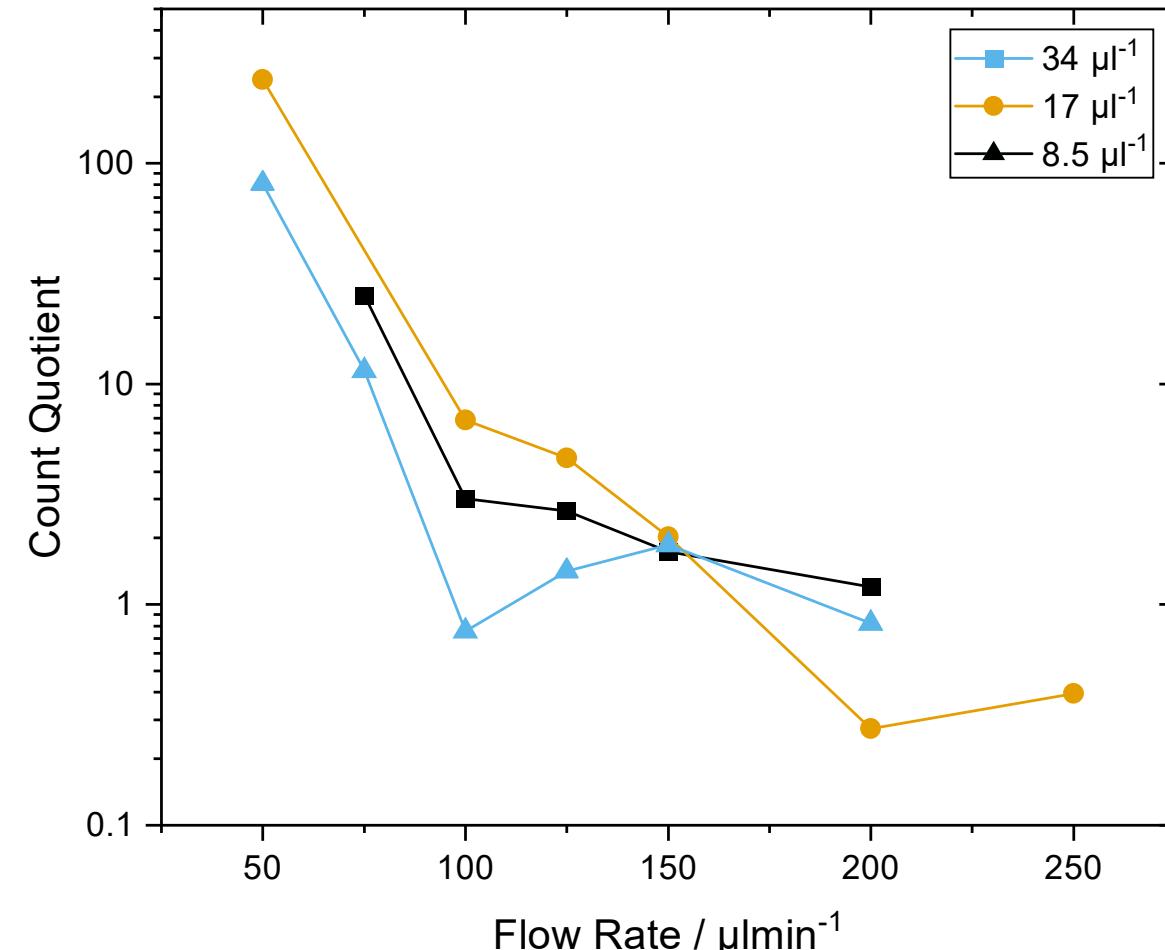
# Results

## Experimental – Development of a Differential Counting Setup



# Results

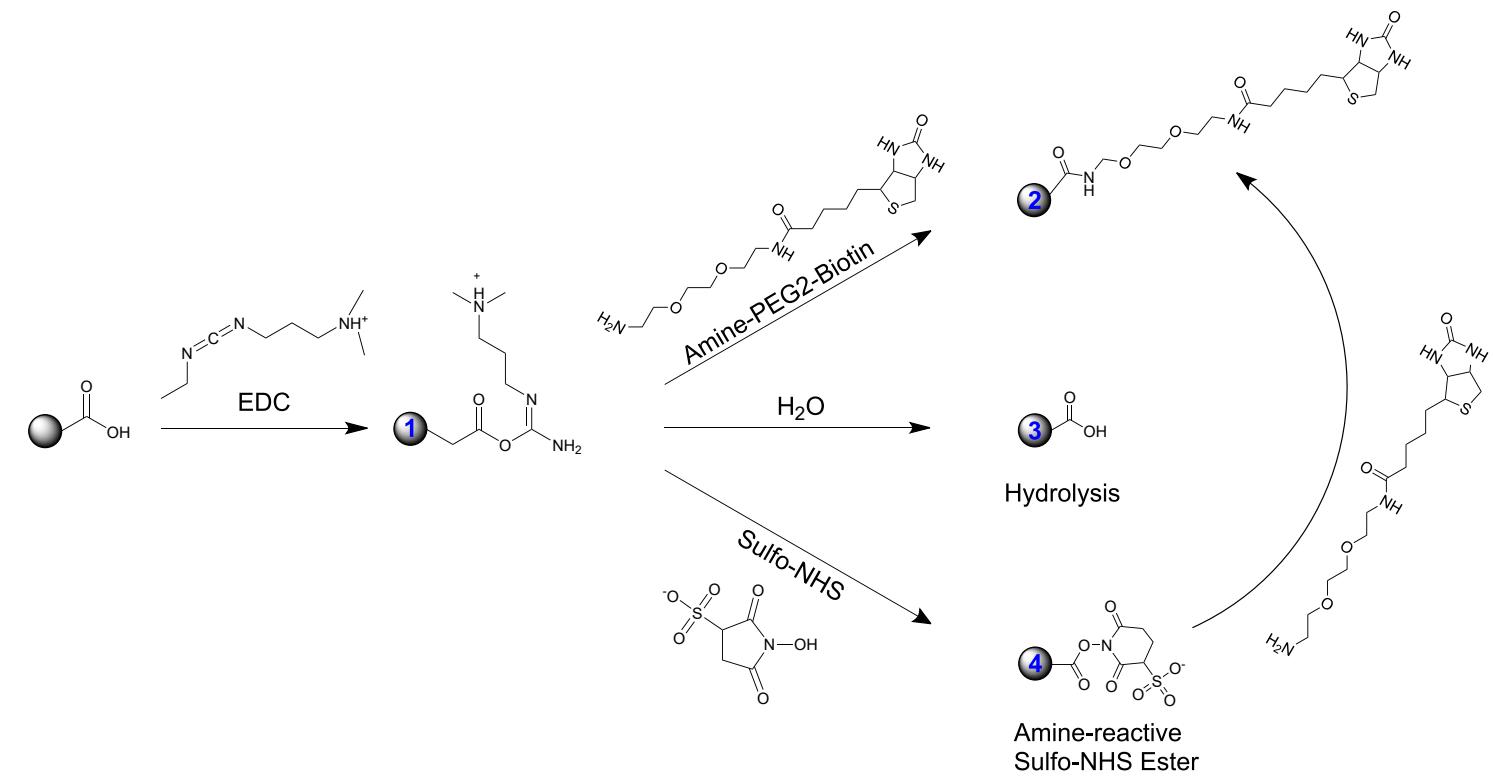
## Experimental – Development of a Differential Counting Setup

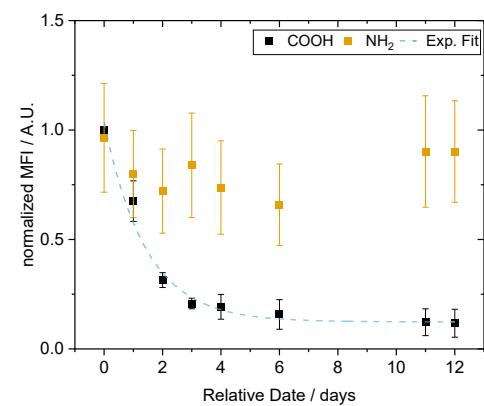
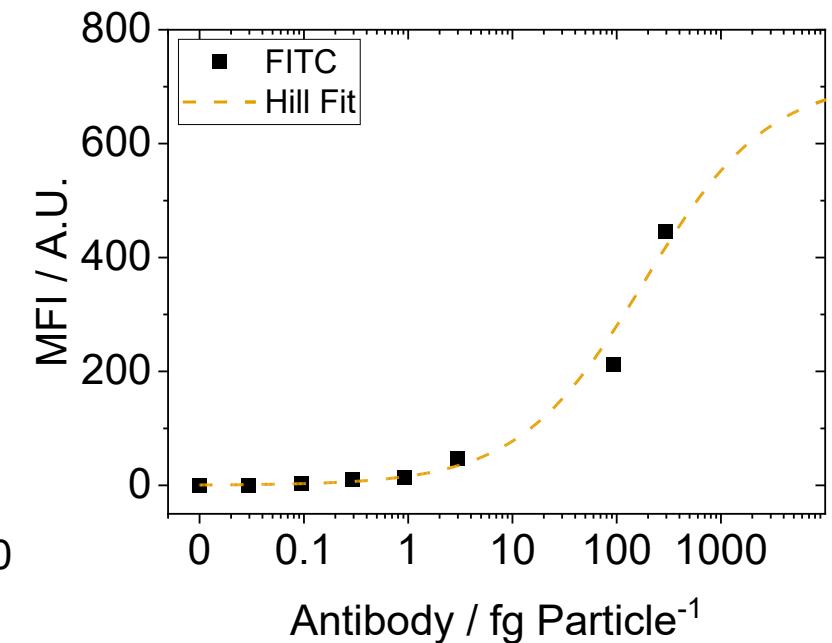
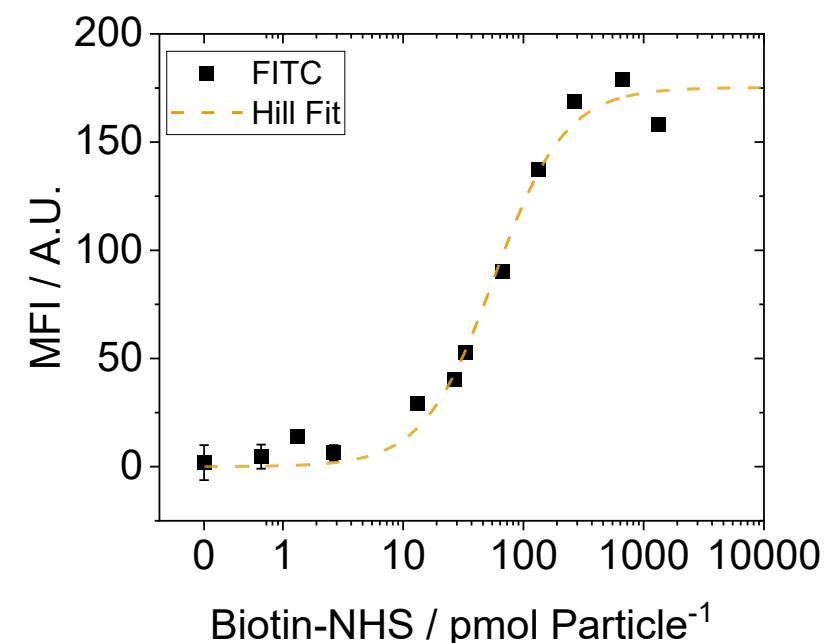
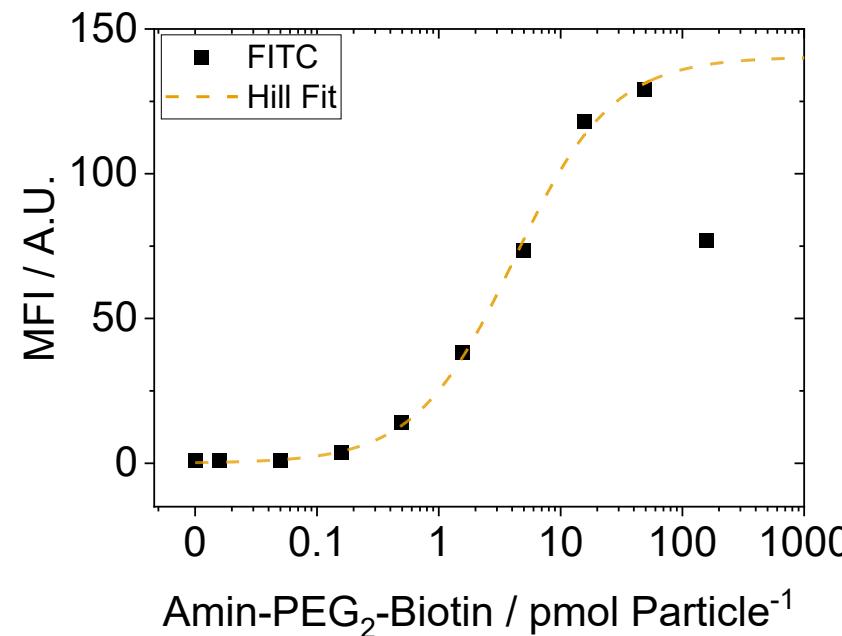


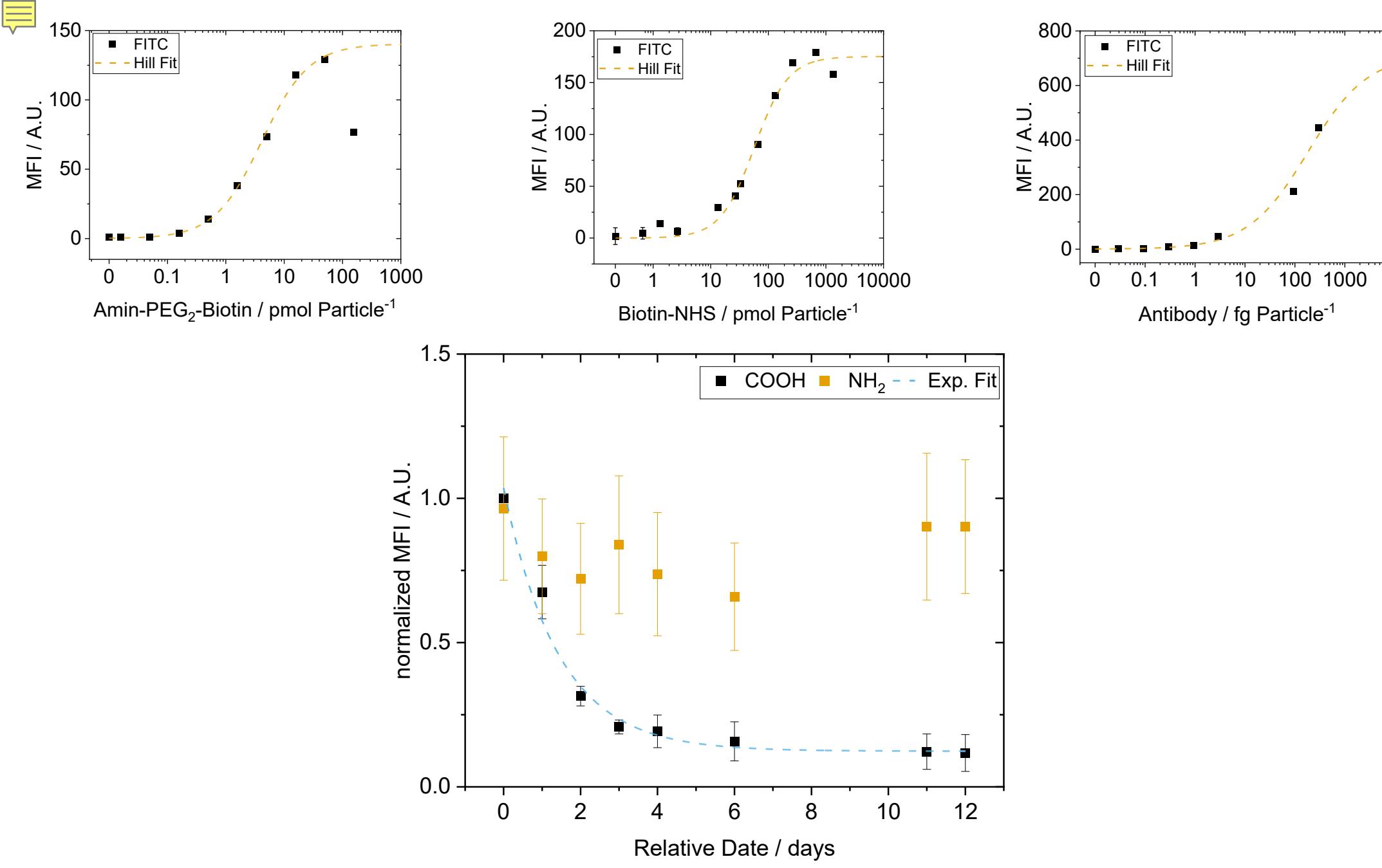
# Results

## Experimental – Established Reference Model for Surface Marker Expression Densities

- Proof of concept for the simulations in the magnetic flow cytometer
- **Epitope Density on a cell has to be modulated**
- Development of a methodology to coat beads with highly defined surface markers
- Universally applicable to proteins
- **Carbodiimide Chemistry**

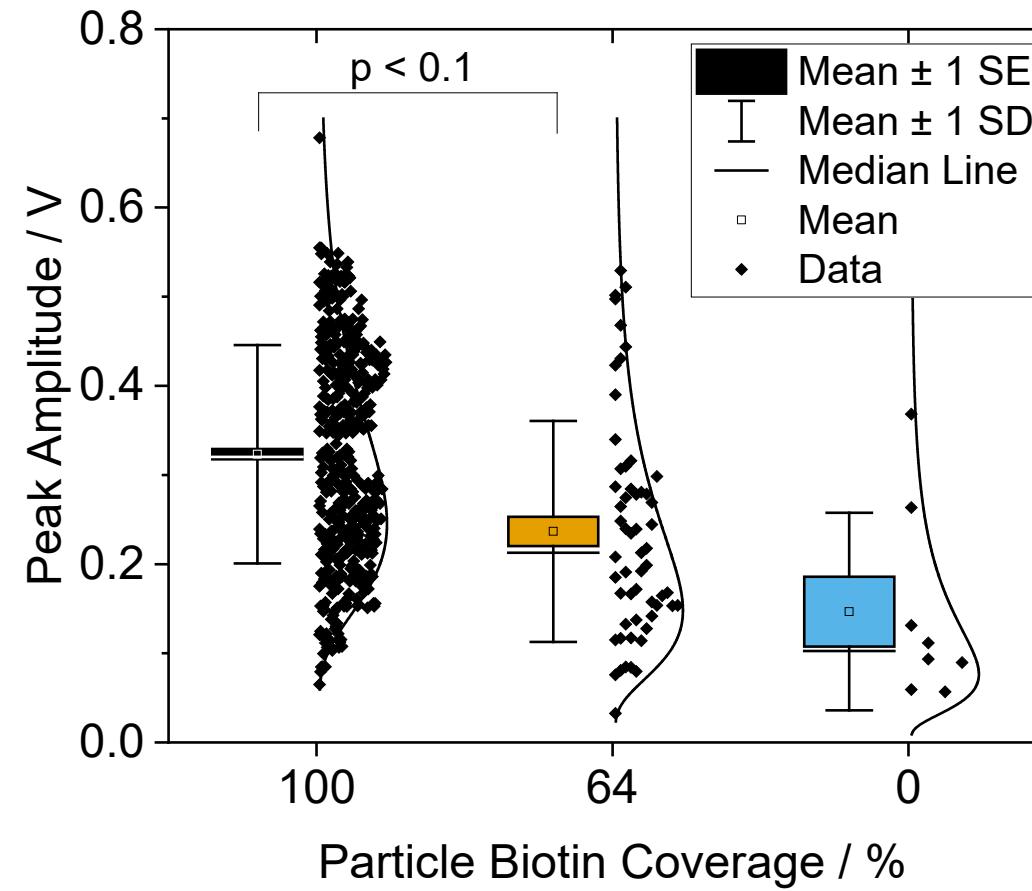




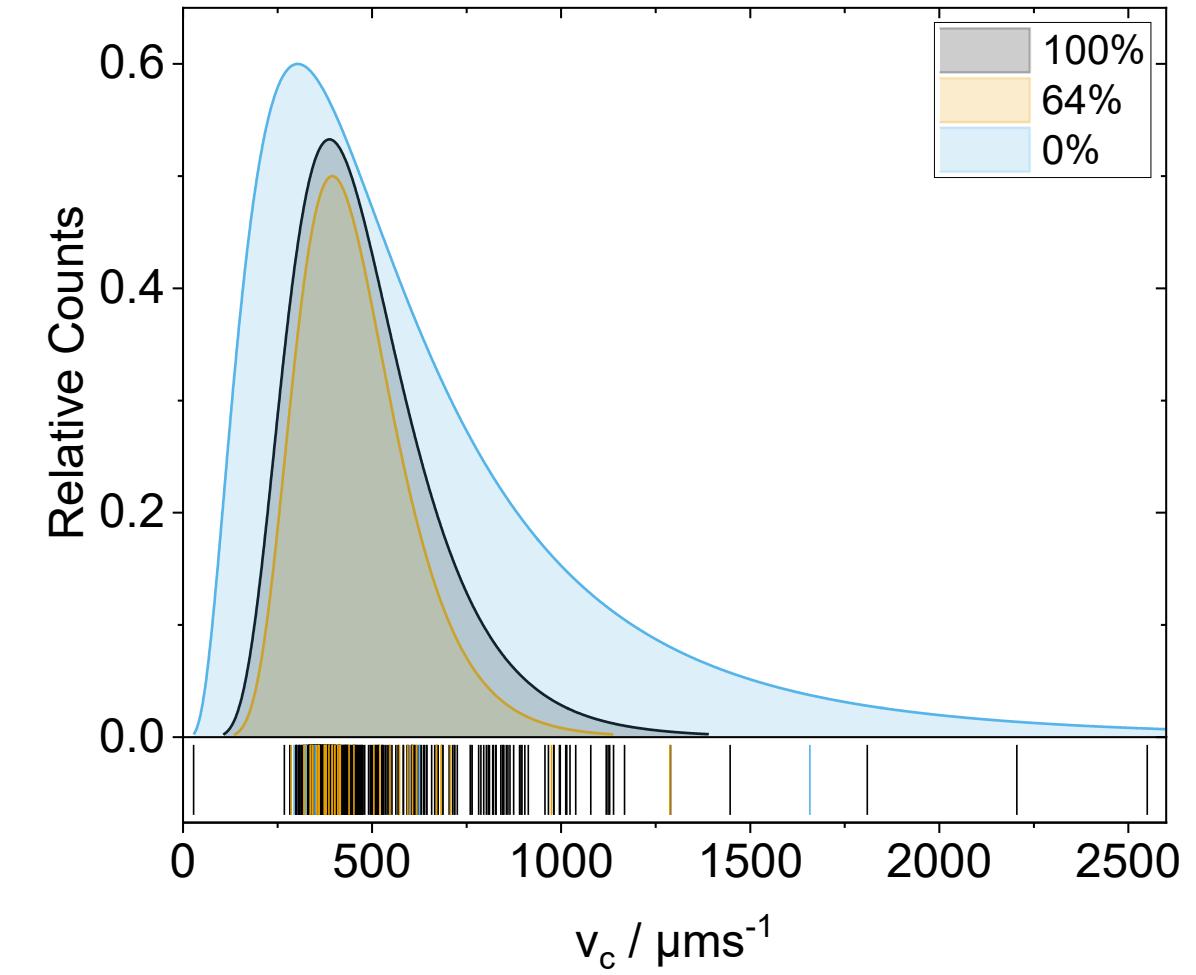


# Results

## Experimental – Established Reference Model for Surface Marker Expression Densities

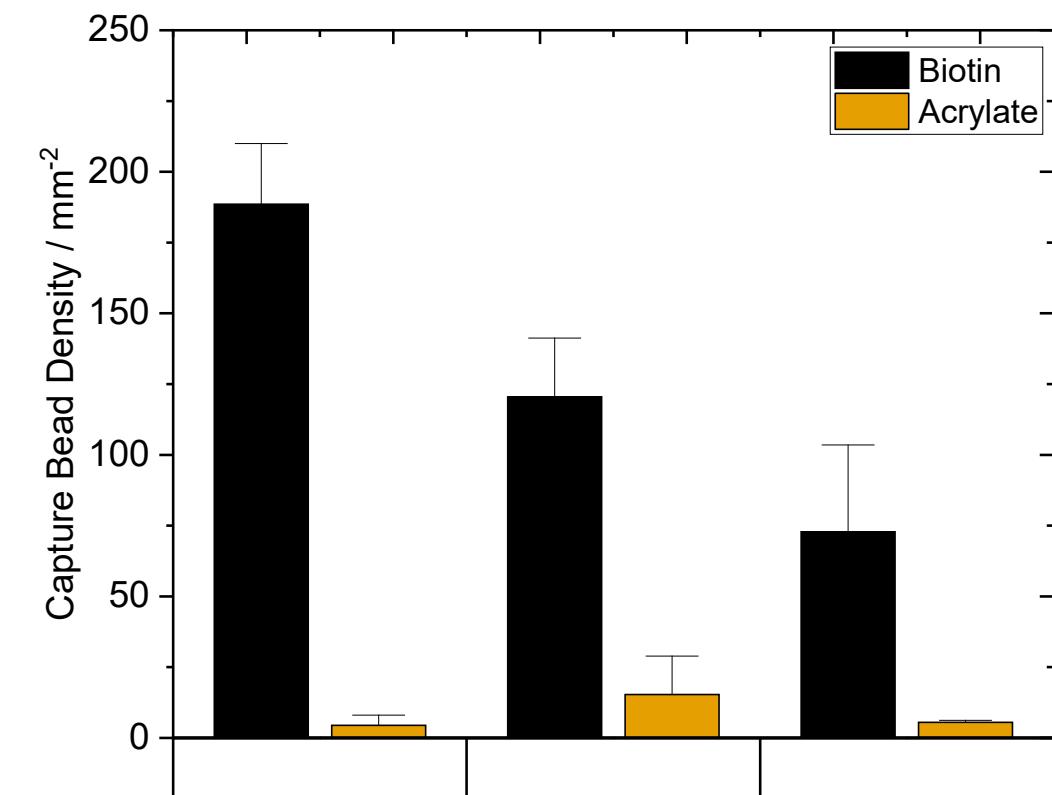
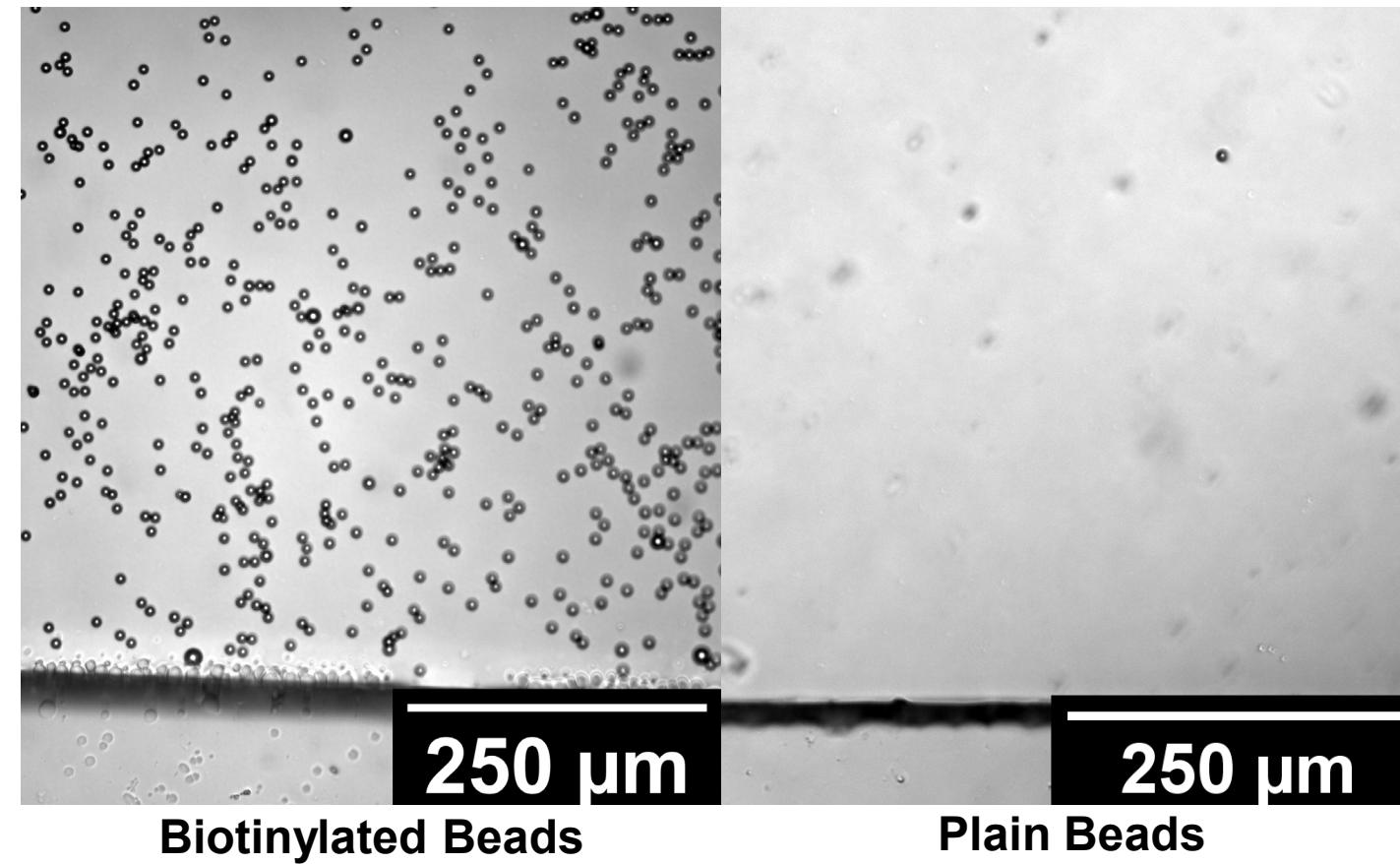


Concenctratoin measurement of magnetized polystyrene beads



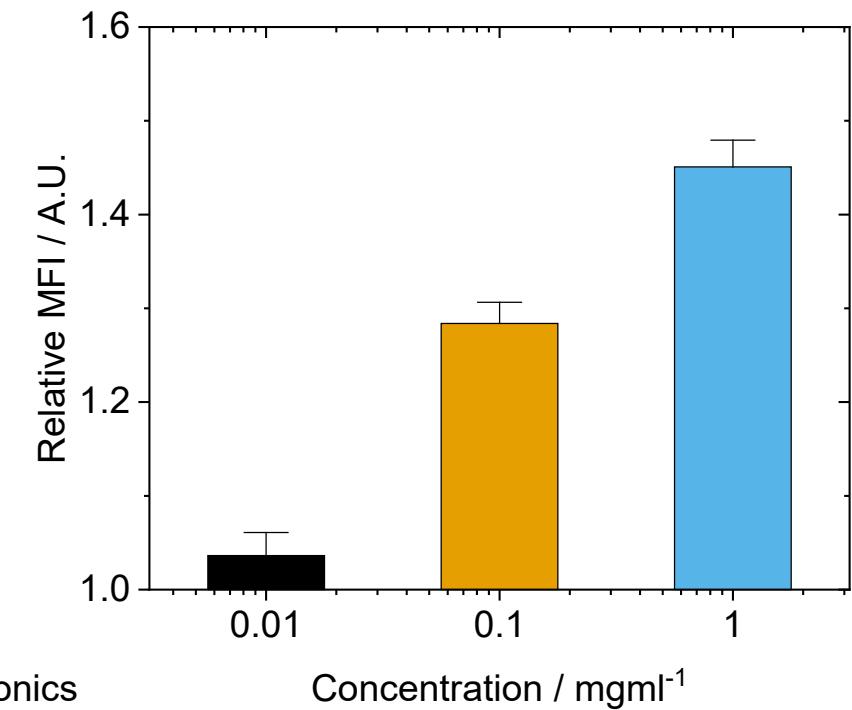
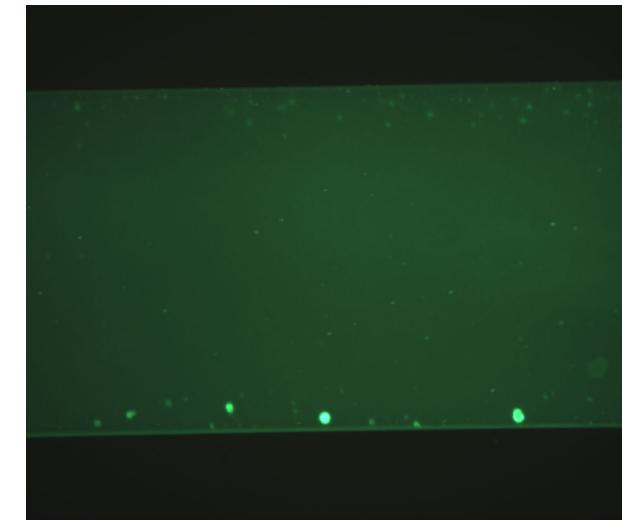
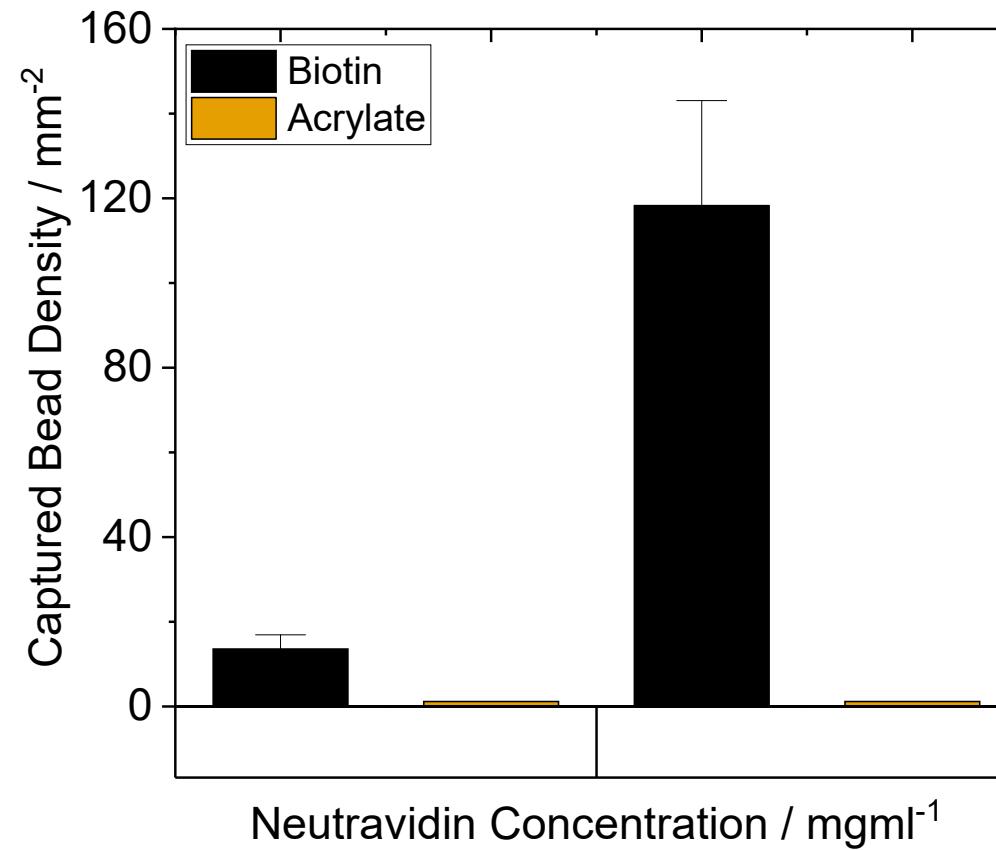
# Results

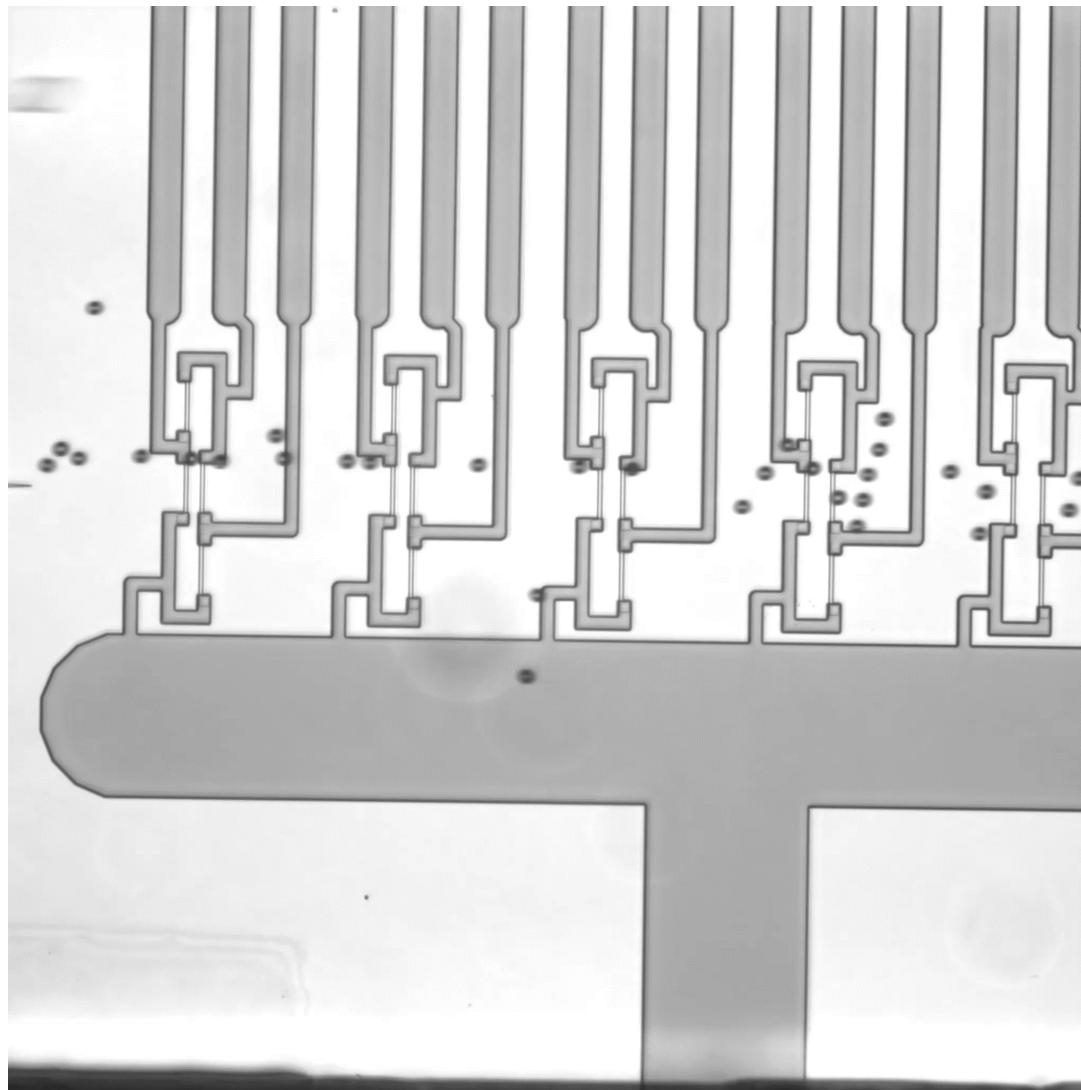
## Experimental – Affinity-based Concentration Measurements in the Magnetic Flow Cytometer



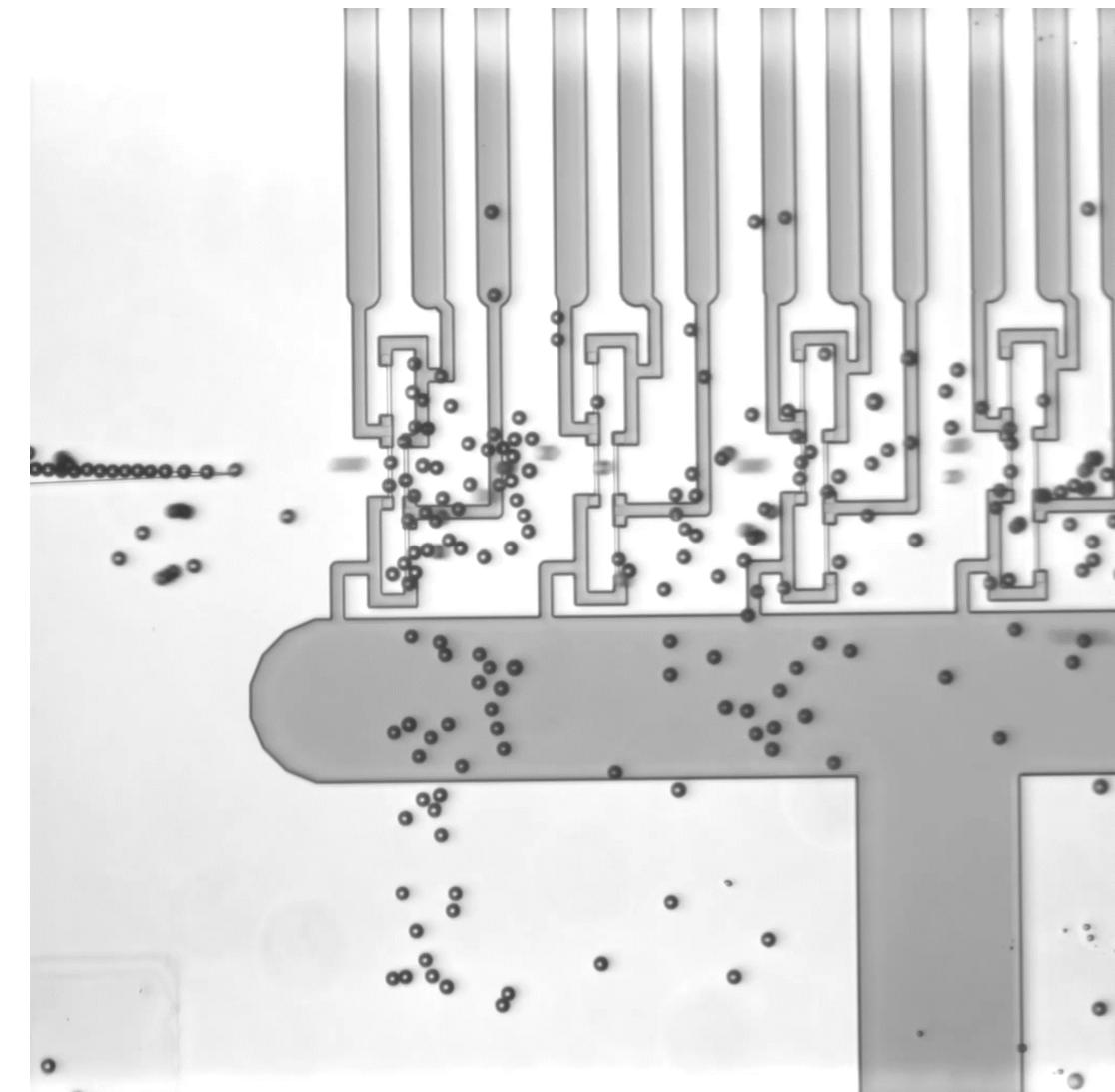
# Results

Experimental – Affinity-based Concentration Measurements in the Magnetic Flow Cytometer





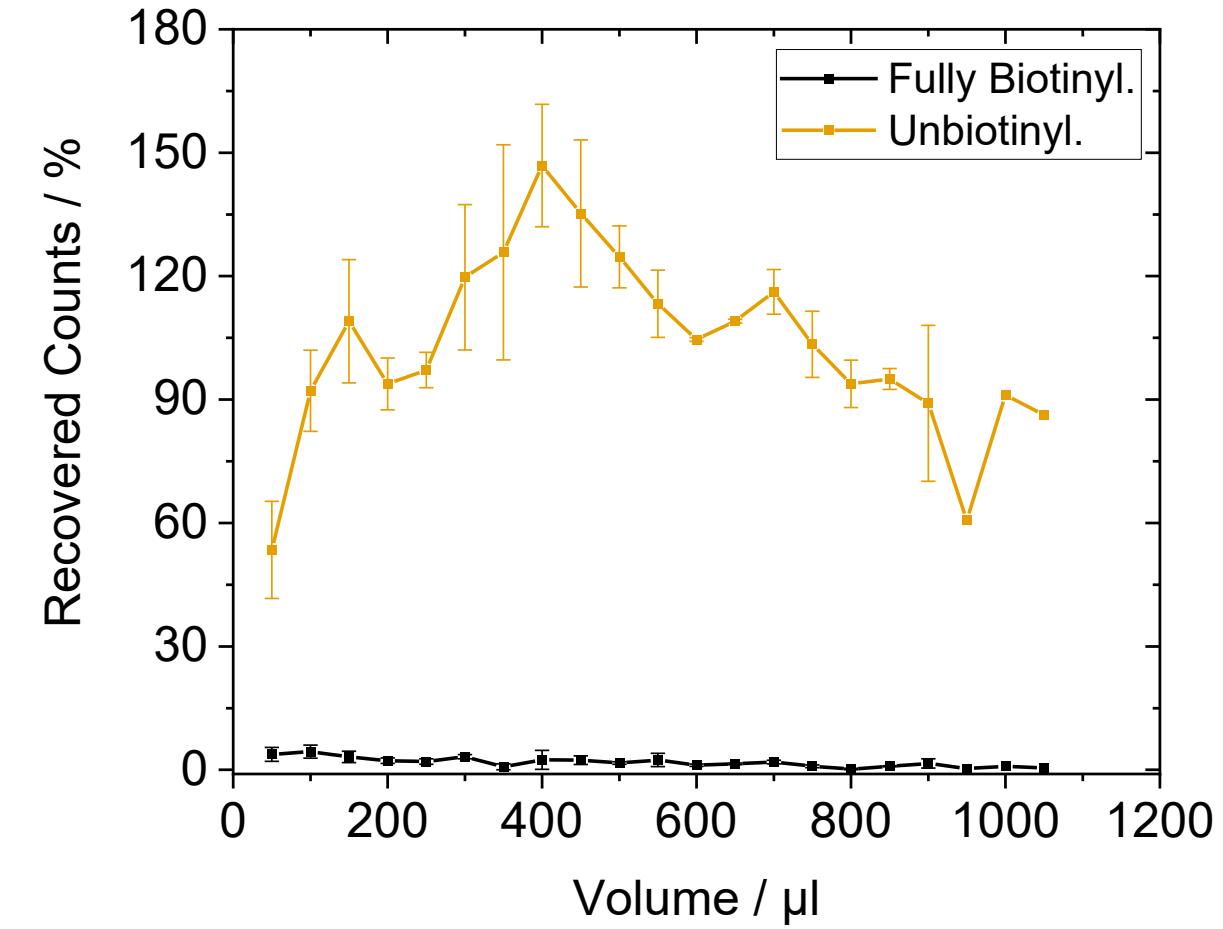
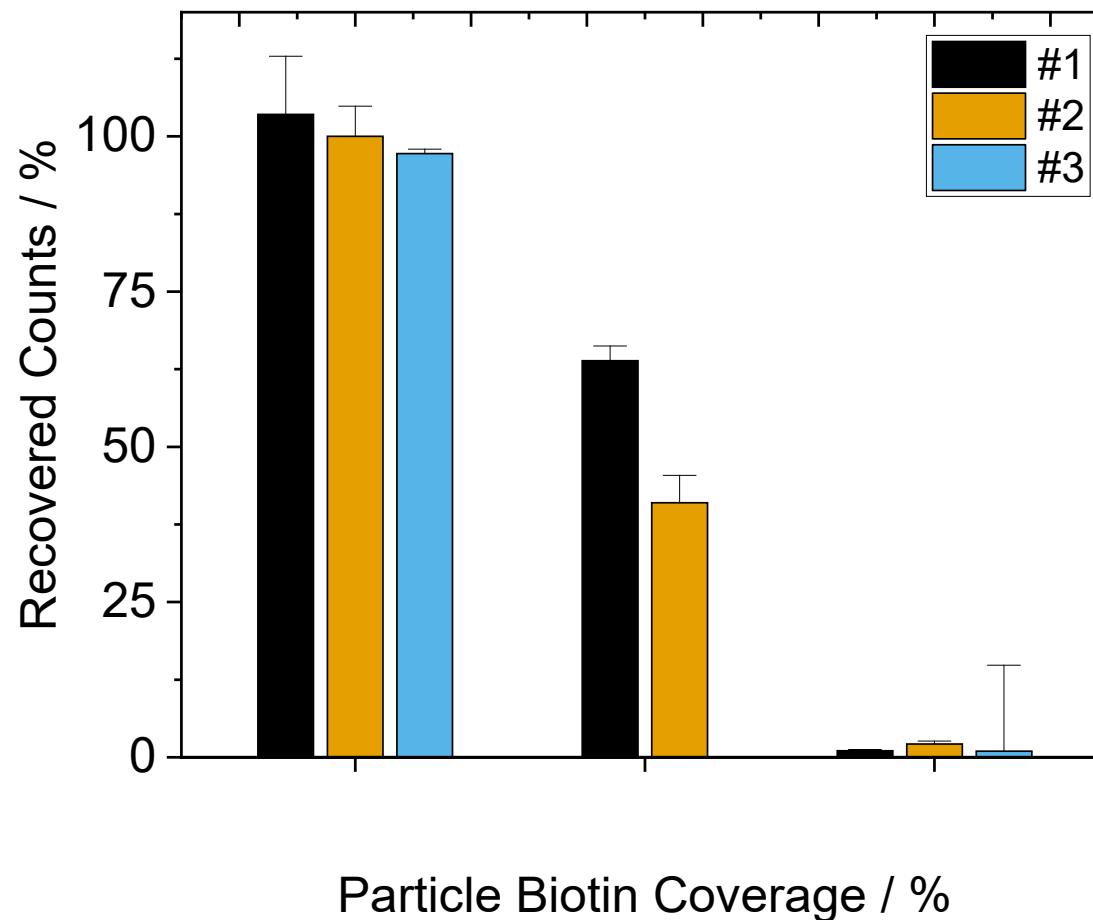
**Plain Particles**



**Biotinylated Particles**

# Results

## Experimental – Affinity-based Concentration Measurements in the Magnetic Flow Cytometer





# Conclusion

Outcomes of this thesis

1. Established **hydrodynamic and magnetic simulations** for physical phenomena of rolling cells
2. Benchmarked **absolute and differential concentration measurements** for the magnetic flow cytometer
3. Developed a **reference system** for the variation of the surface receptor density
4. Demonstrated **an affinity-dependent assay** in the magnetic flow cytometer

# Thank you, LBE!



# Magnetic Field Computations

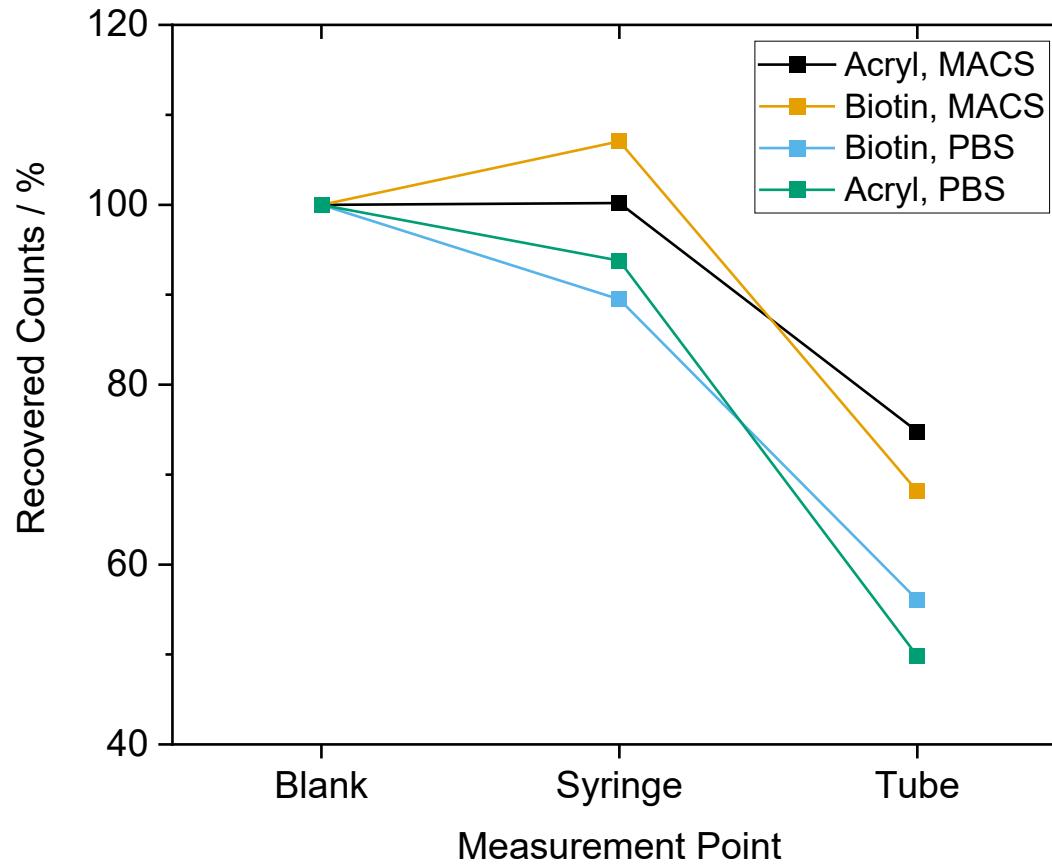
$$\mathbf{B}(t) = \sum_{i=1}^N \frac{1}{A_{\text{Sensor}}} \int_{-\frac{l}{2}}^{\frac{l}{2}} \int_{-\frac{w}{2}}^{\frac{w}{2}} \frac{\mu_o}{4\pi} \left( \frac{3\mathbf{r}_i(t) (\mathbf{r}_i(t) \cdot \mathbf{m}_i)}{|\mathbf{r}_i(t)|^5} - \frac{\mathbf{m}_i}{|\mathbf{r}_i(t)|^3} \right) dx dy \quad 1.1$$

$$\mathbf{R}_{\text{sig}}(t) = -\mathbf{B}(t) \times \frac{S}{100} \times R + R \quad 1.2$$

$$\mathbf{V}_{\text{sig}}(t) = \frac{\mathbf{R}_{\text{sig}}(t)}{R + \mathbf{R}_{\text{sig}}(t)} \times V_p - \frac{V_p}{2} \quad 1.3$$

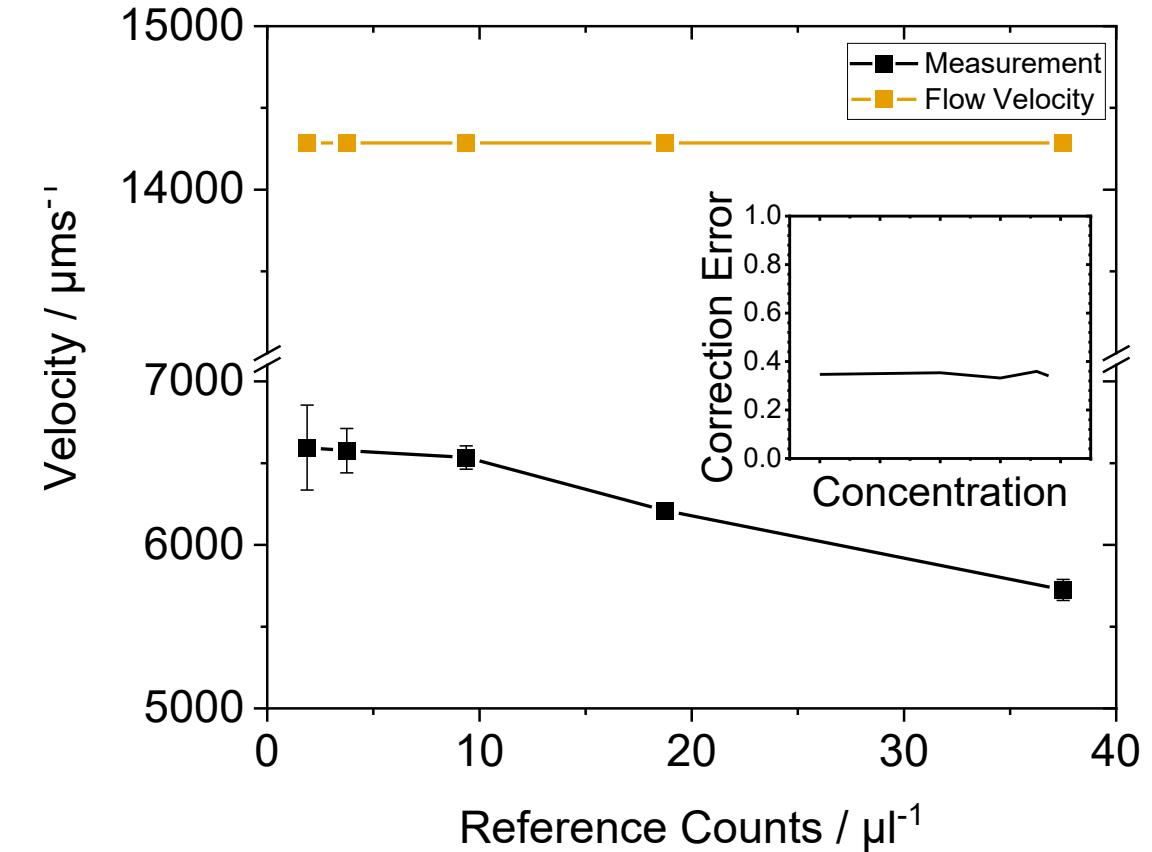
$$\max\{R_{x,y}(\tau)\} = \max \left\{ \int \mathbf{V}_{\text{ref}}^*(t) \mathbf{V}_{\text{sig}}(t + \tau) dt \right\} \quad 1.4$$

# Error Sources in the Magnetic Flow Cytometer



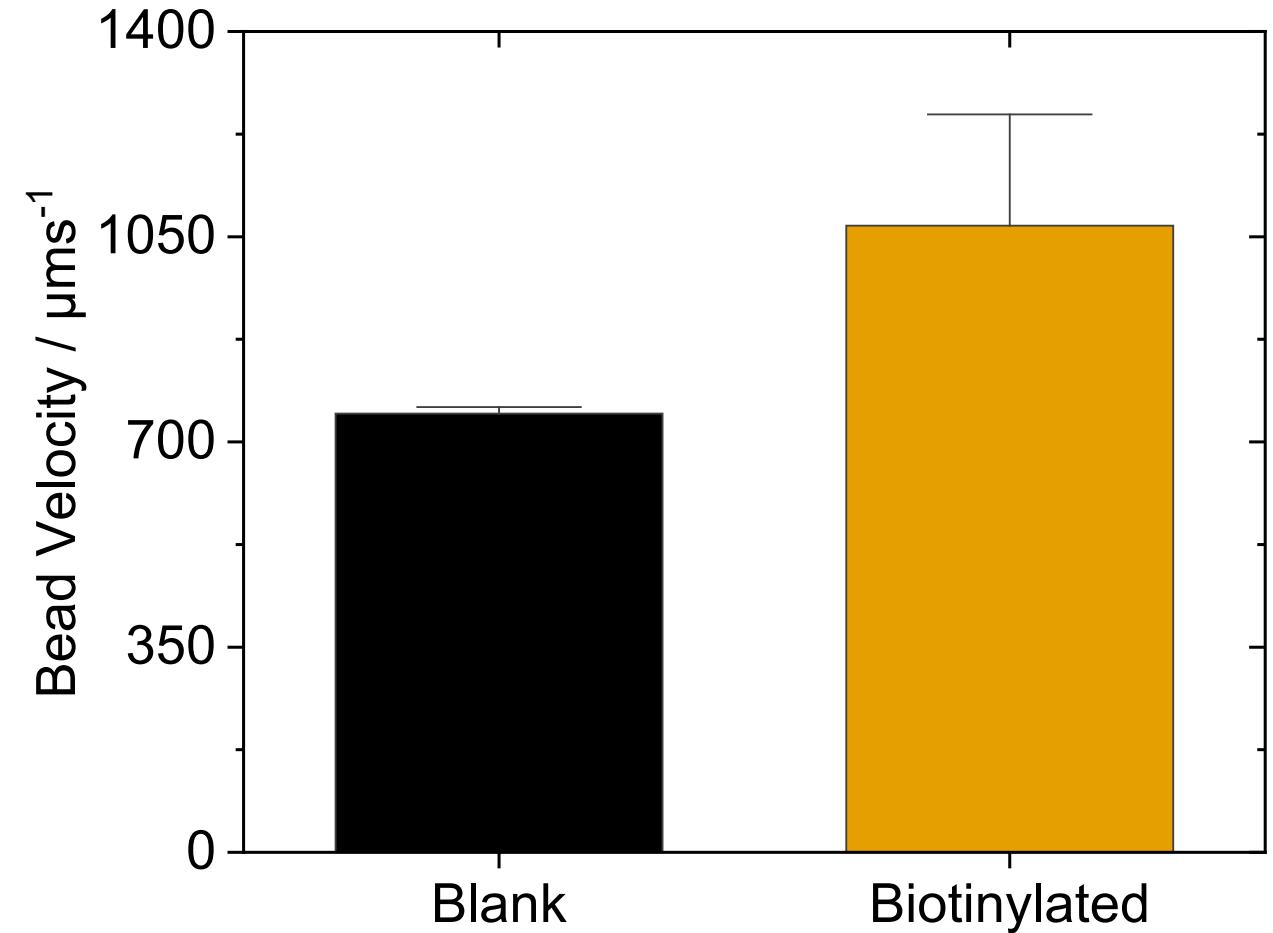
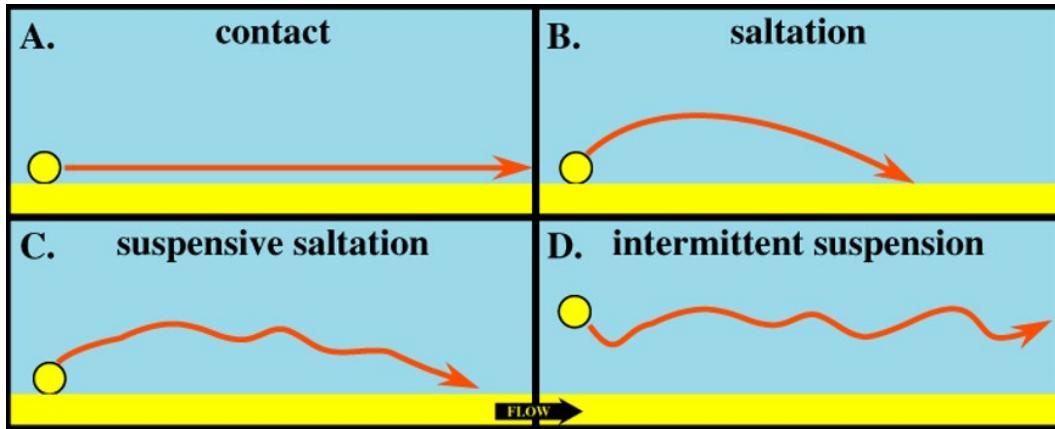
## Losses in Interconnections

## Systematic Error in Velocity Measurements at High Concentrations

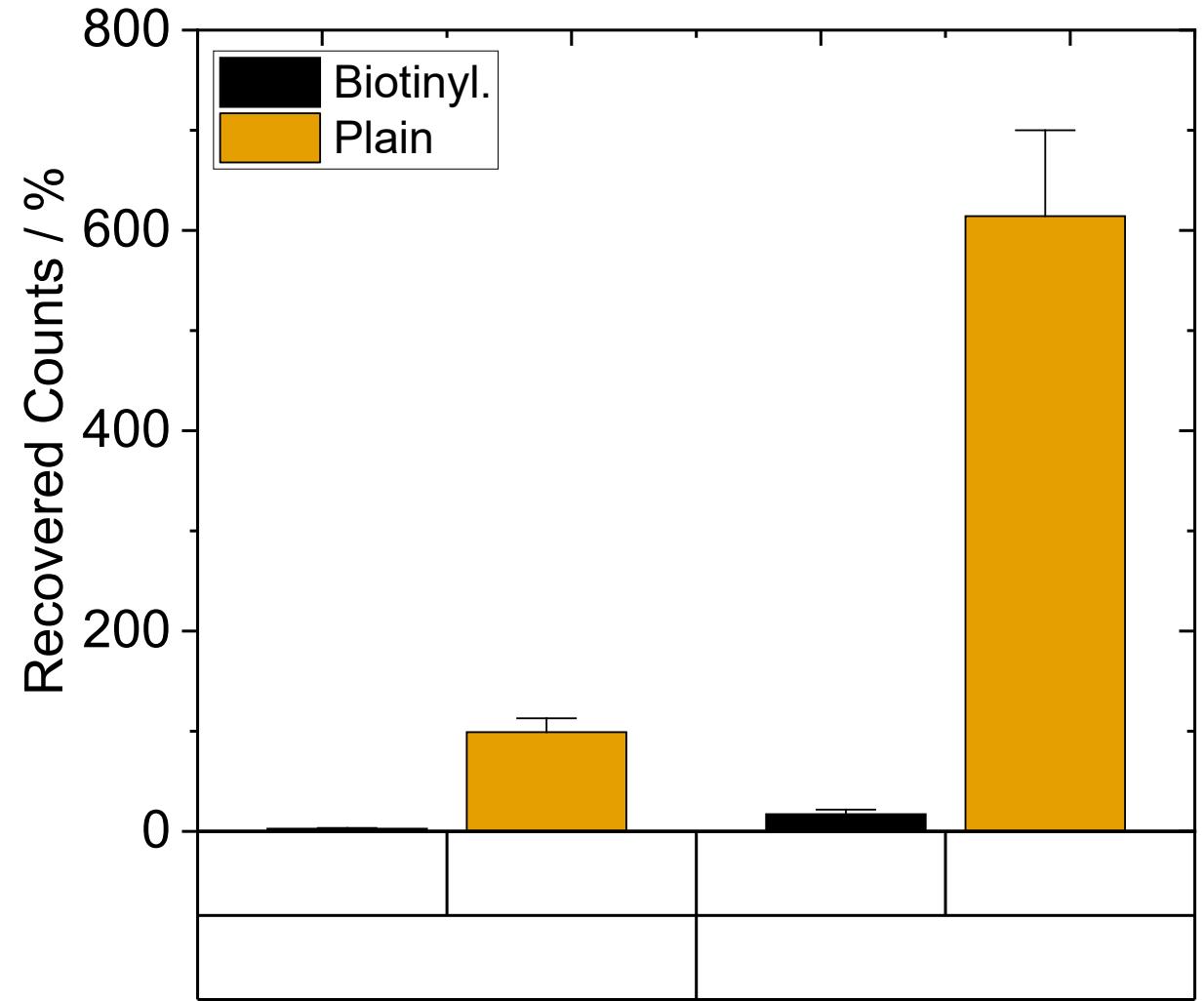


# Affinity-dependent Bead Velocity

- Magnetically measured bead velocity of biotinylated bead is statistically higher
- Probably attributed to a saltatory movement after adhesion to the channel (**B,C**)
- After adhesion, a wake forms behind the bead thus causes increasing pressure on the back

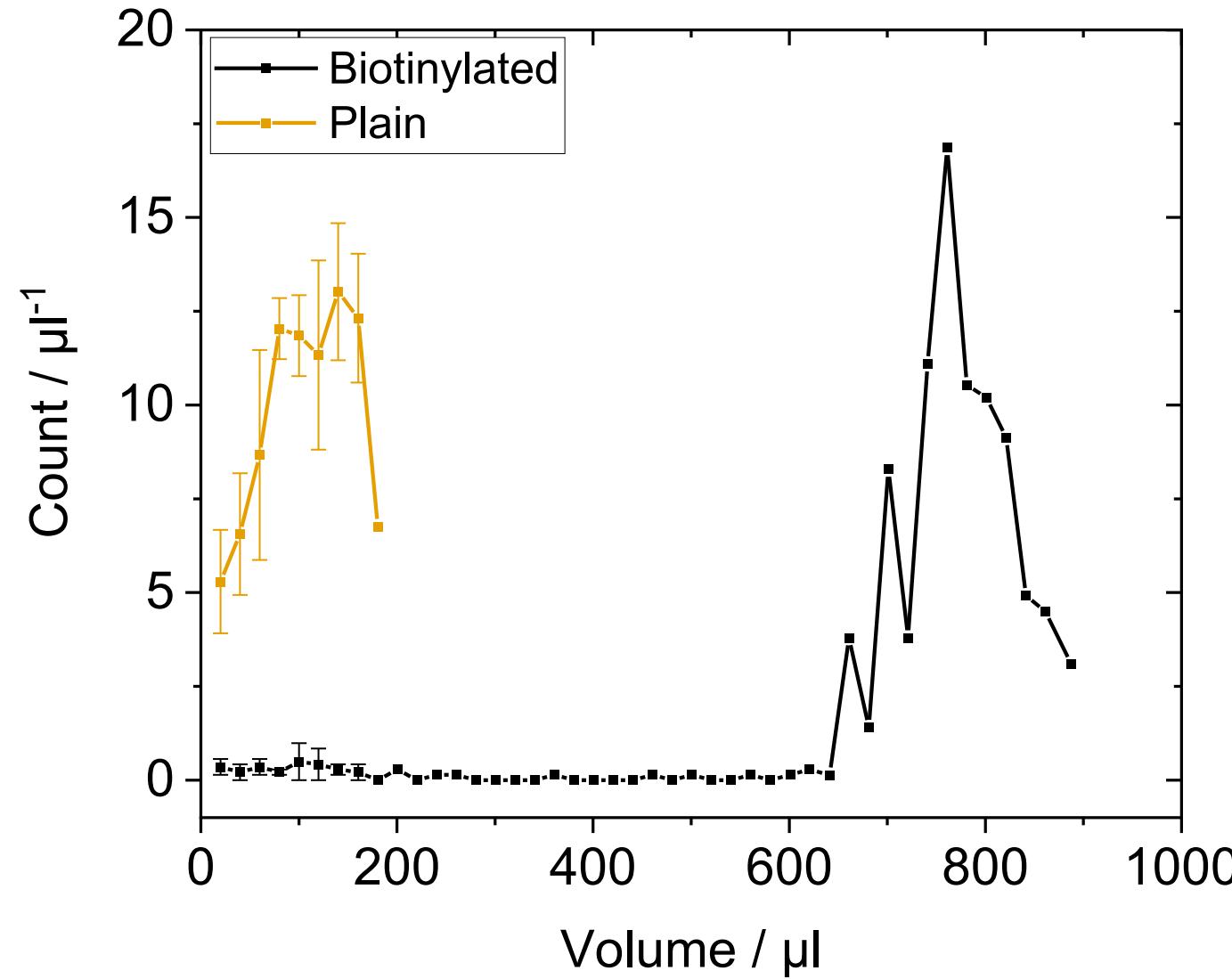


## Errors in Affinity-Based Measurements

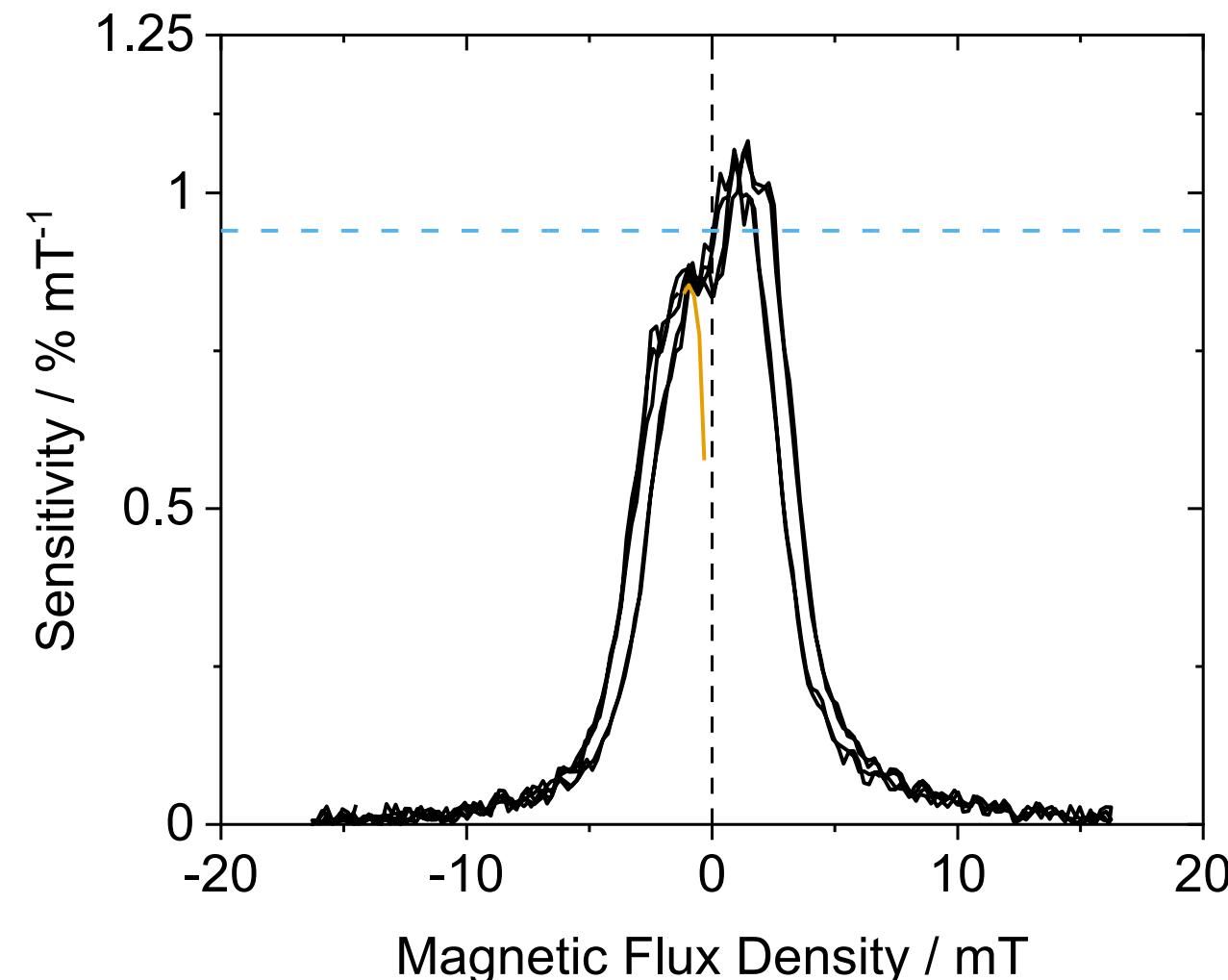
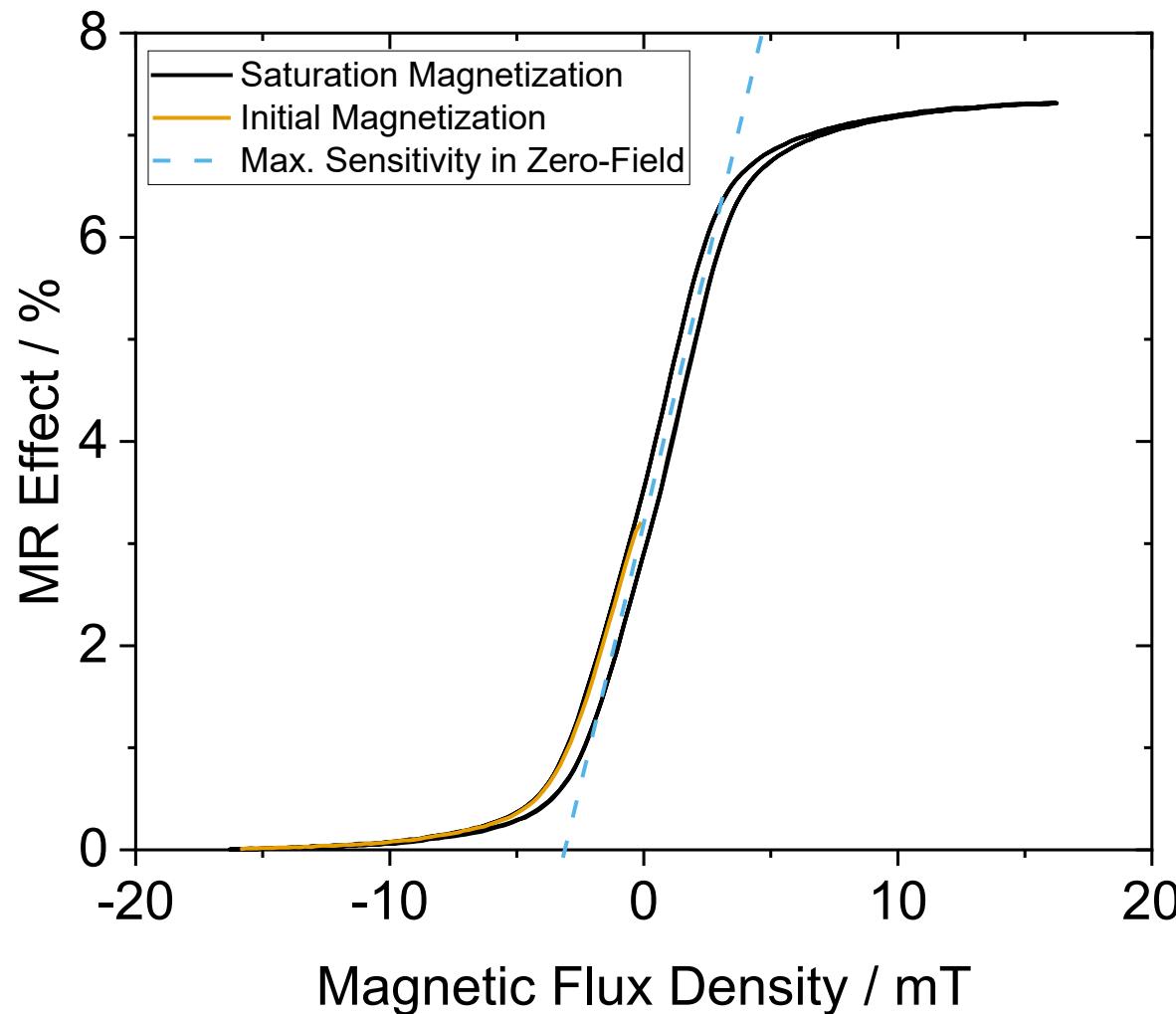


# Error Sources Affinity-Dependent Concentration Measurement

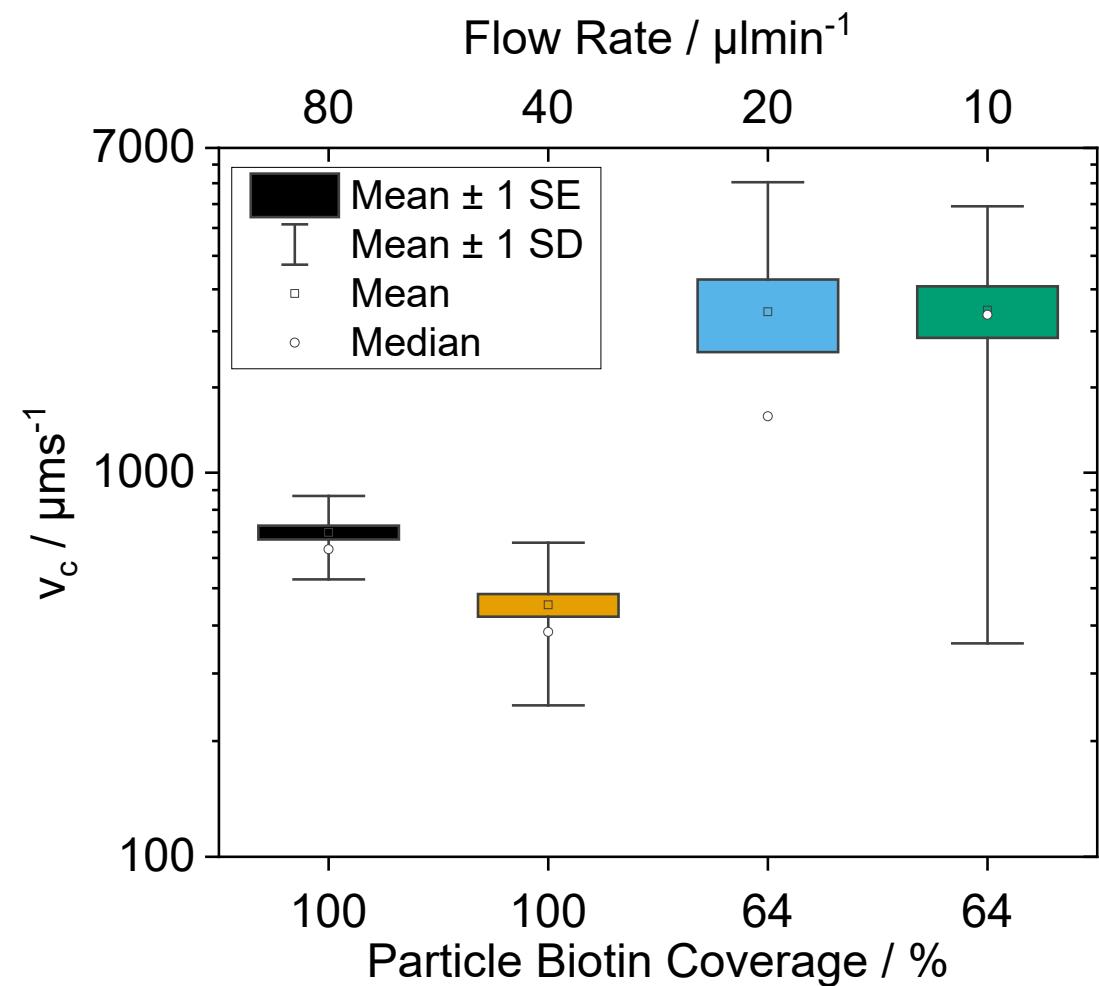
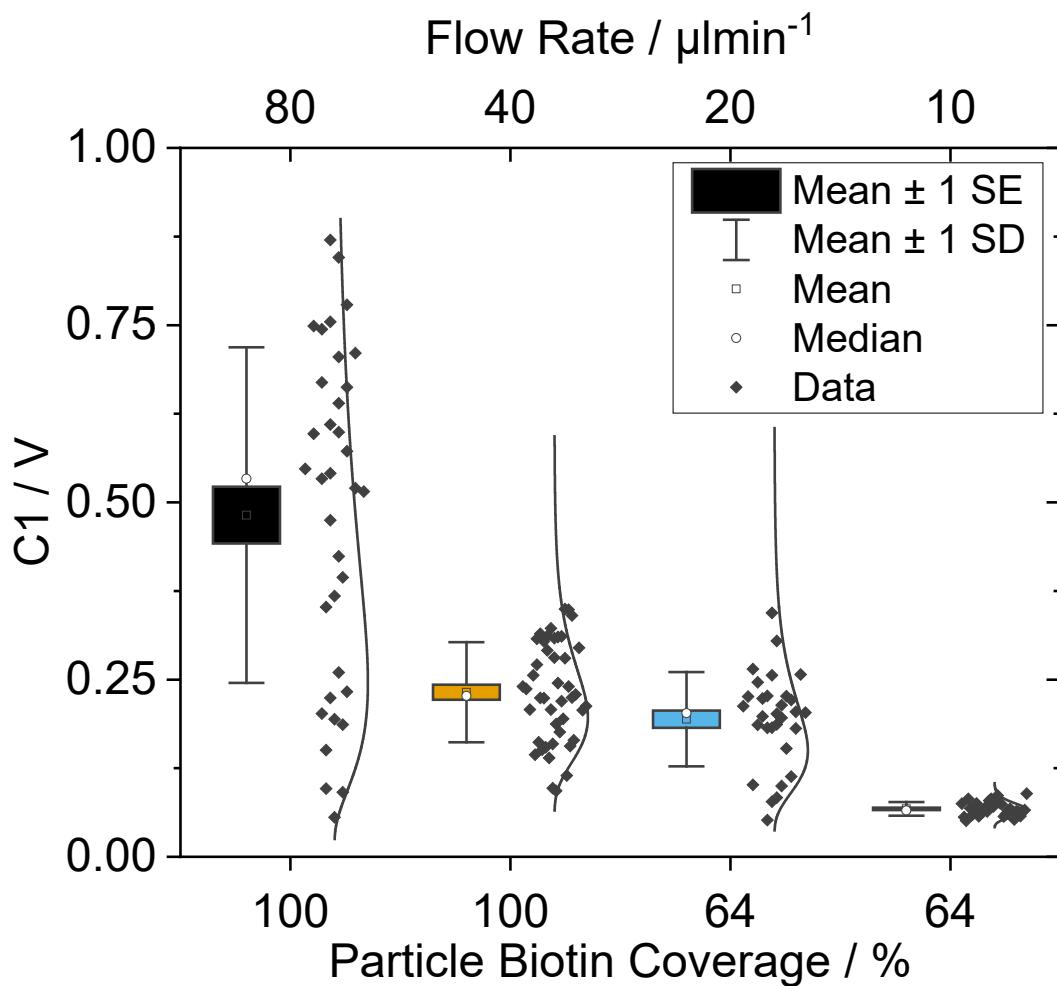
- Initial 100  $\mu\text{l}$ :
  - magnetophoretic structures are filled  
→ Steep rise
- After 700  $\mu\text{l}$ :
  - Surface is saturated with biotinylated beads  
→ Burst-Like Measurement of beads
- After 800  $\mu\text{l}$ :
  - Empty Syringe and Sedimentation Effects play a role  
→ Less beads than expected are measured



# Hysteresis Calibration of the Sensor

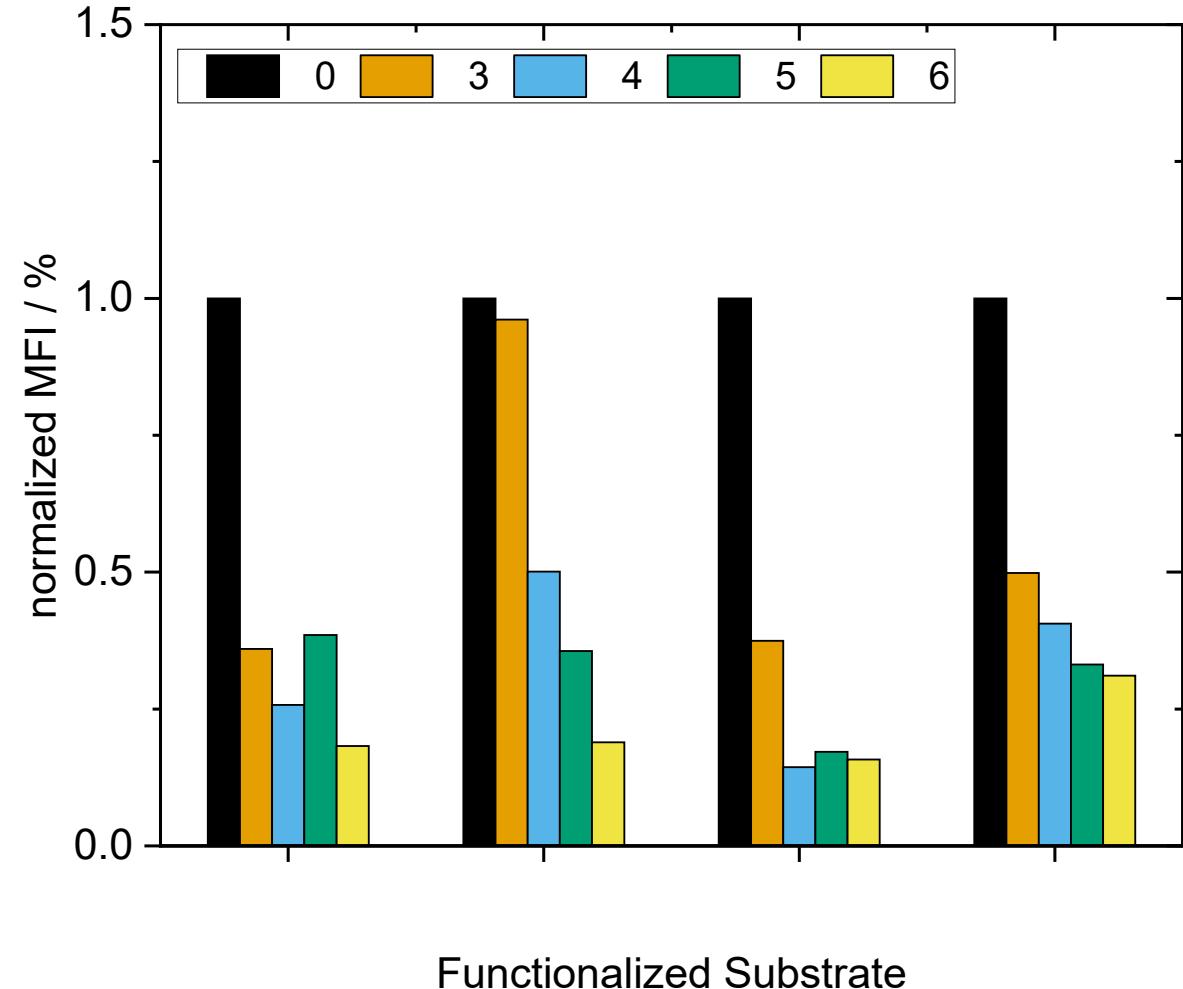


# Micromod BNF-Dextran

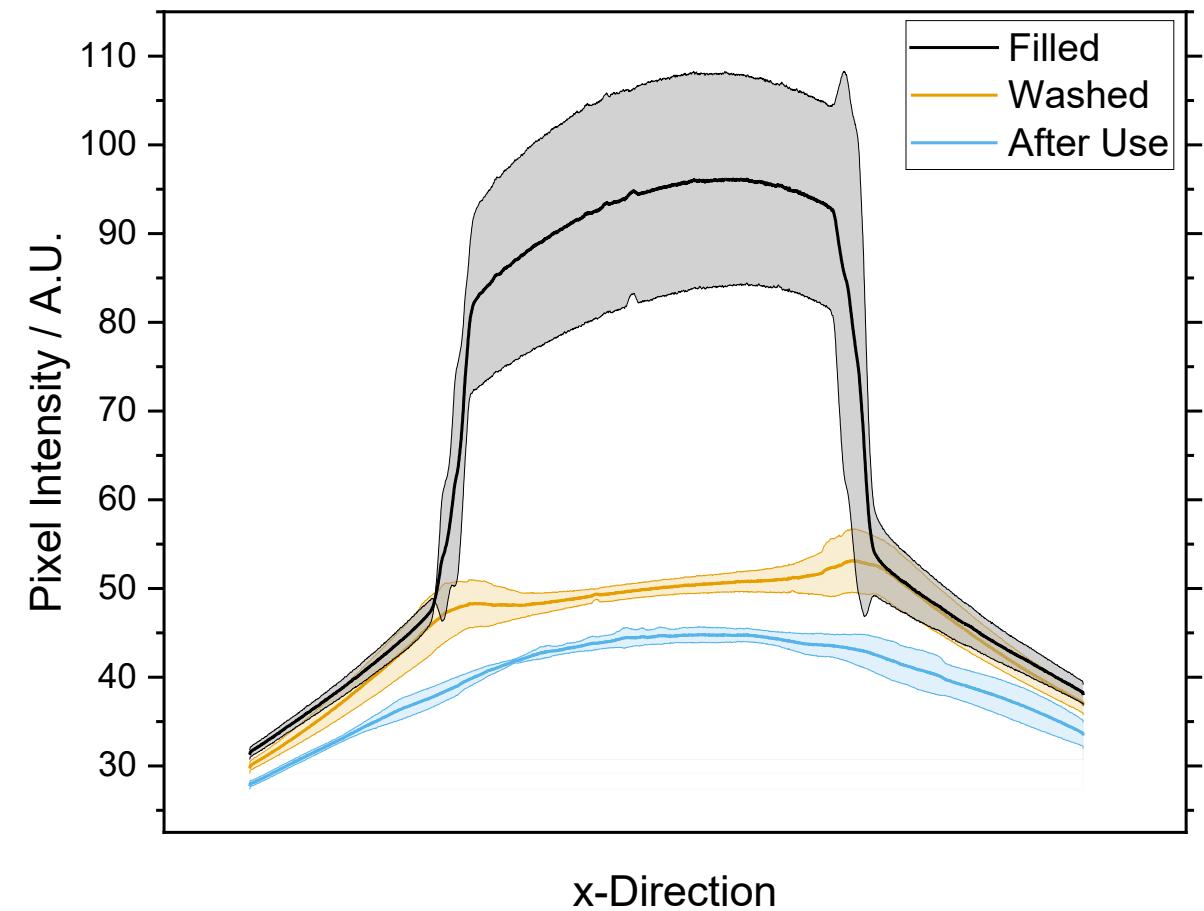
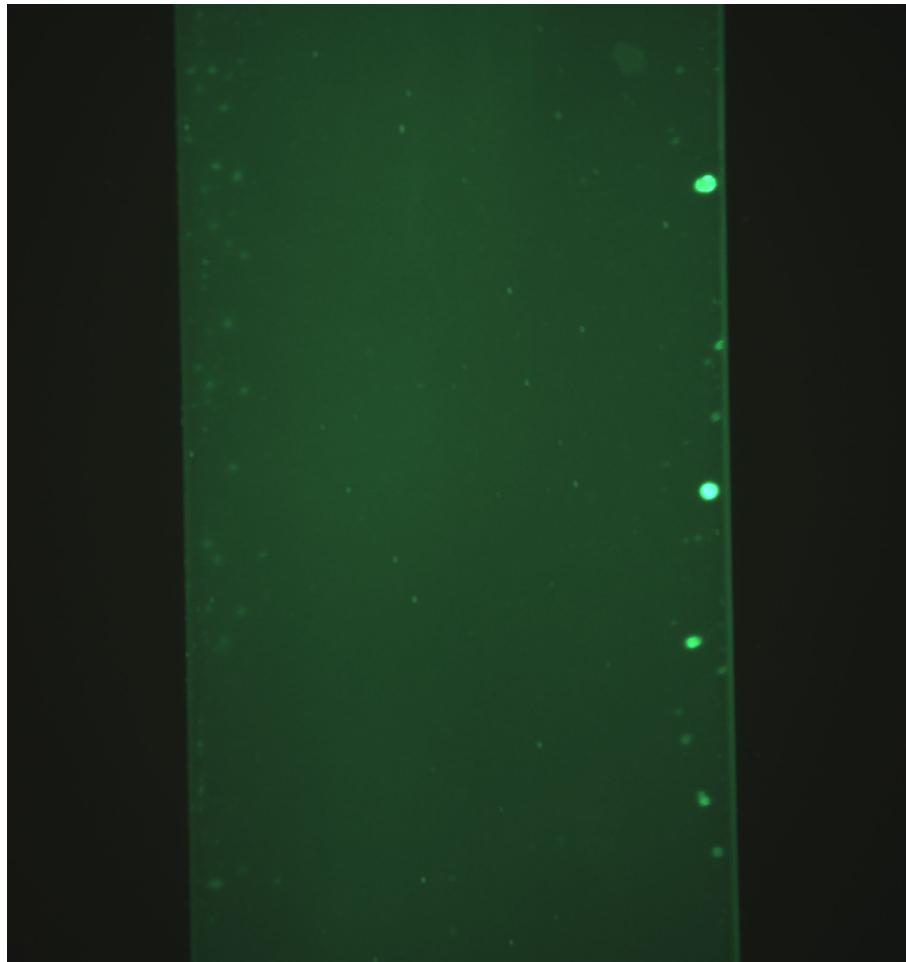


# Assessment of Physisorbed Biofunctionalization

- Platereader Experiment with AlOx and SiN surfaces
  - Coverage with fluorescent streptavidin
  - Washing by 200 µl of buffer with a micropipette
- No stability over multiple washing steps  
→ SiN superior to AlOx



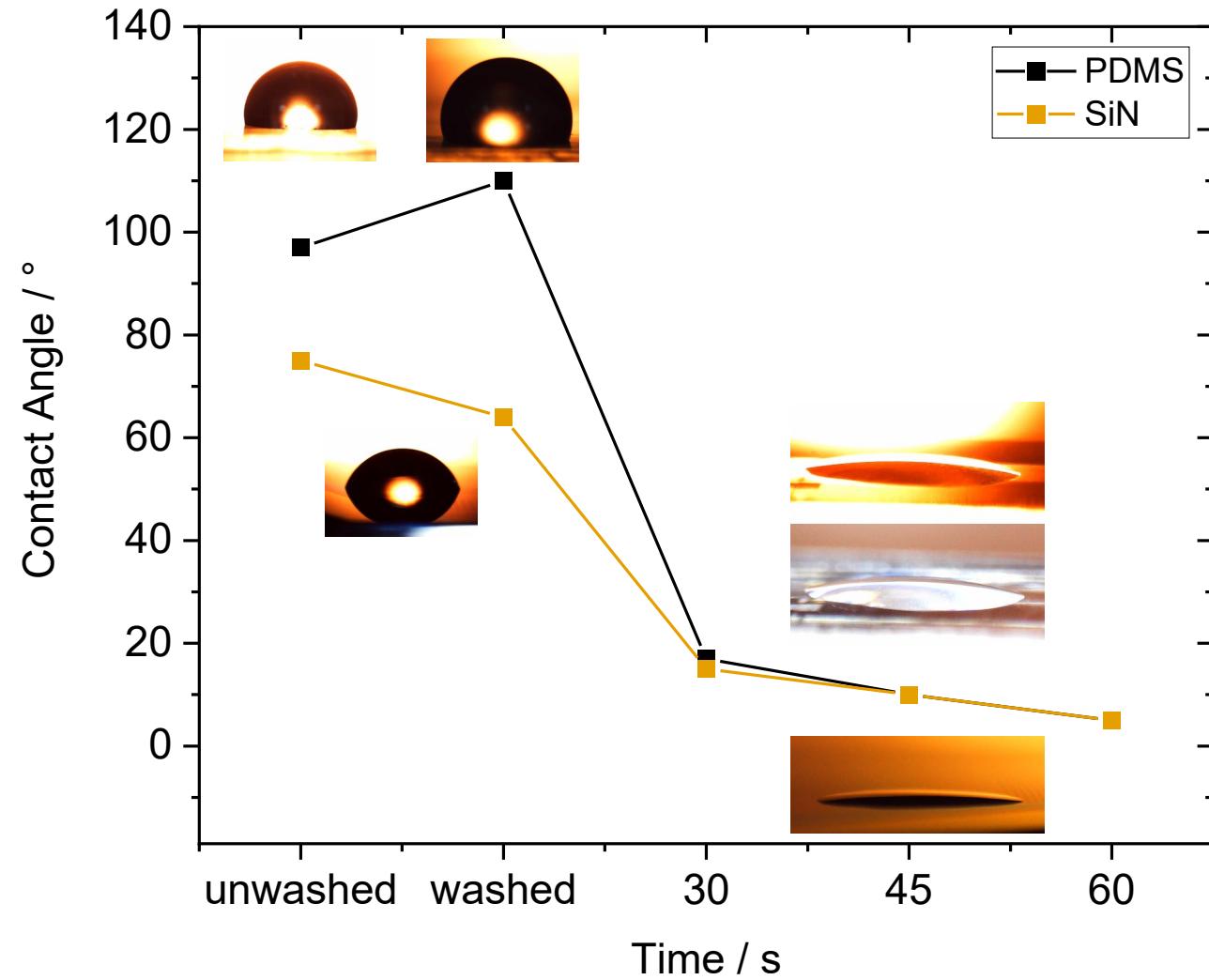
# Fluorescent Evaluation of the Biofunctionalization



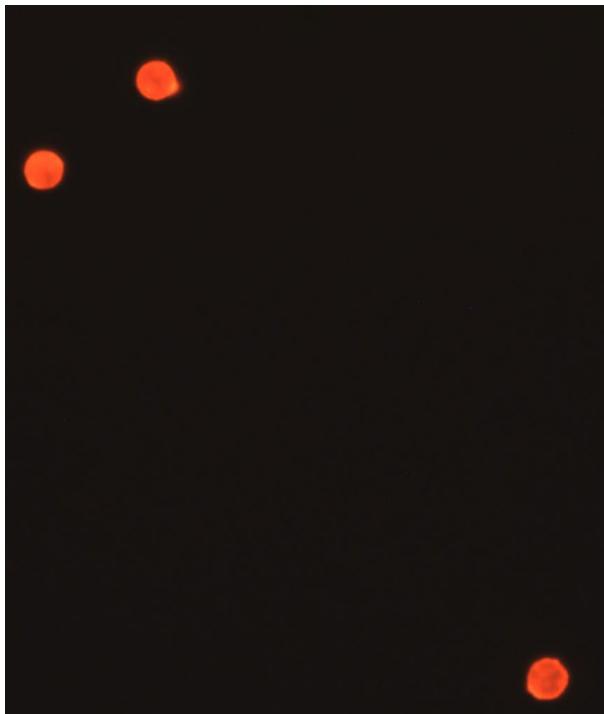
**Image Analysis: Integration over vertical Axis  
Tool: ImageJ**

# Surface Activation with Plasma

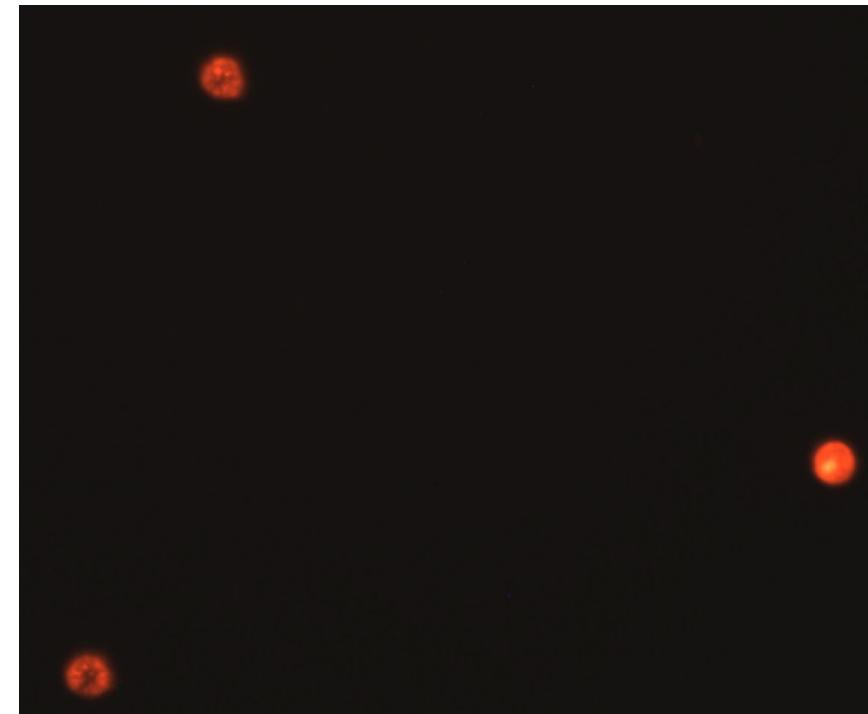
Difference to Piranha not measurable in contact angle, but in functionalization operation



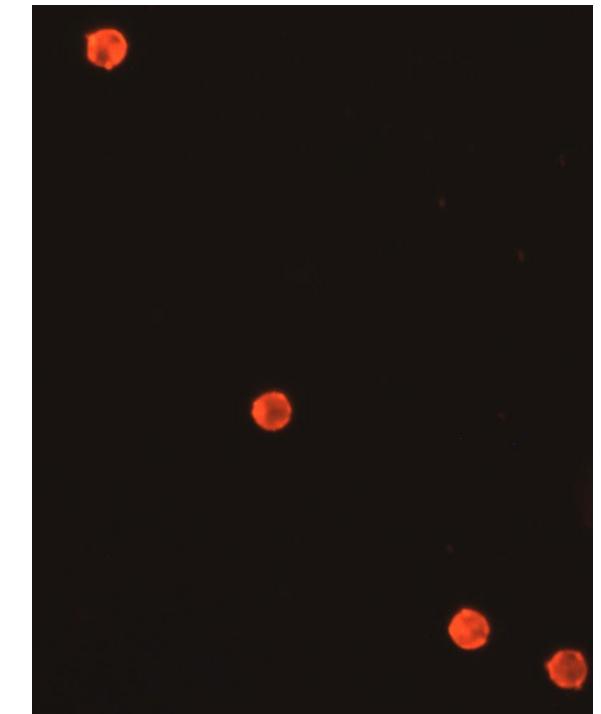
# 8 $\mu$ m Beads coated with streptavidin-redF-Dextran



Maximum Biotin Coverage



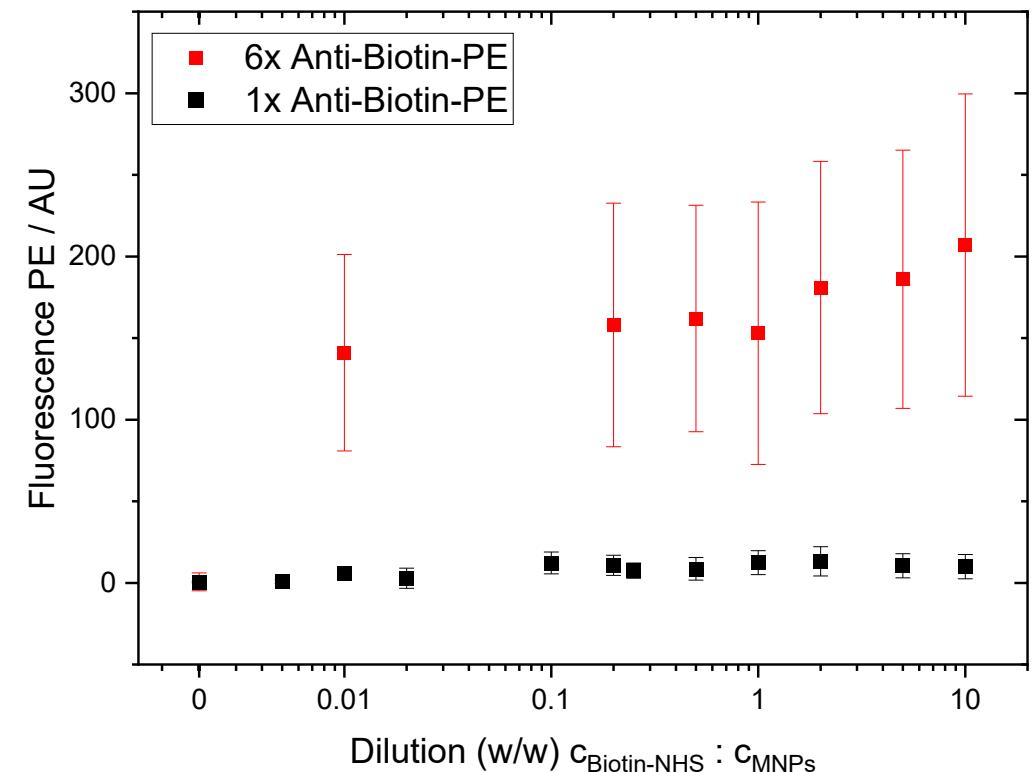
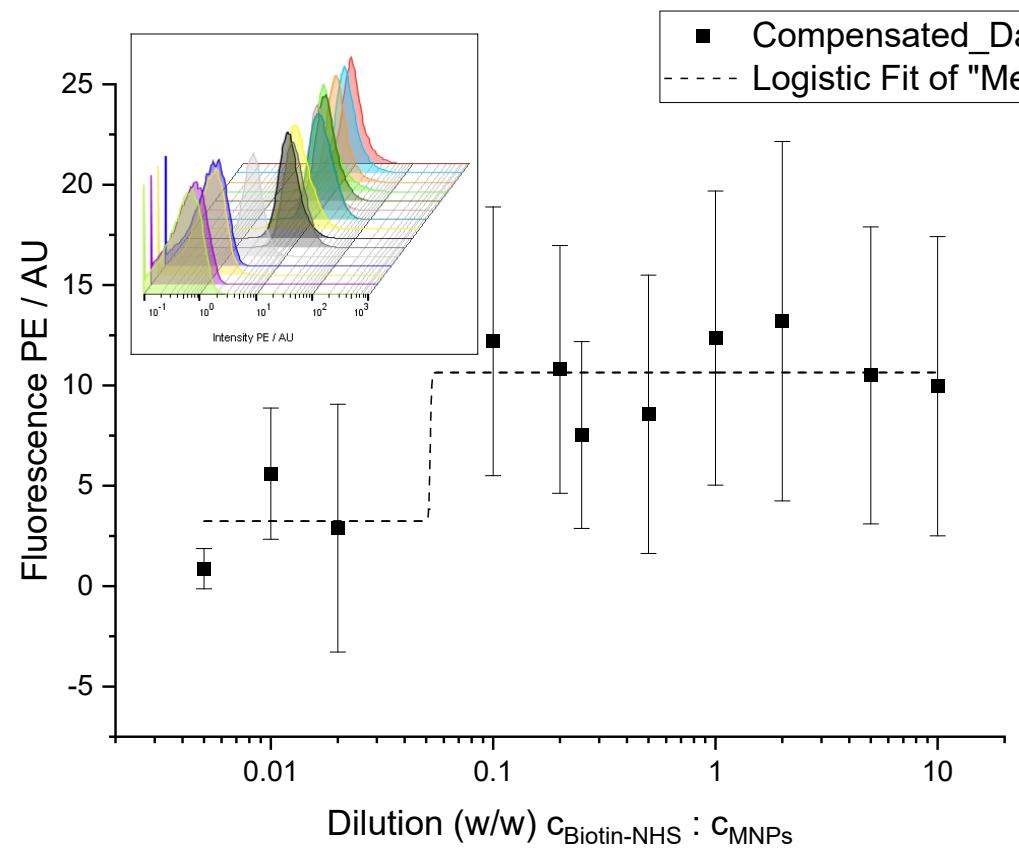
Approx 16% Coverage



Blank

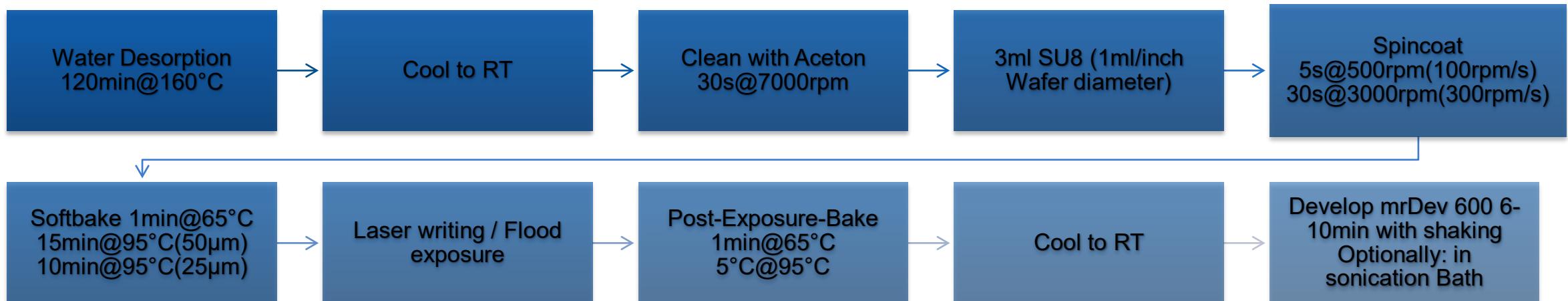
## Unspecific Binding

# Anti-Biotin-PE Assessment Not Working



# Wafer - Spincoating

- 17.07 3" SU8-3050 @ 3000 rpm written same day → ~ 98 µm
- 23.07 3" SU8-3050 @ 3000 rpm written after one week → ~ 94 µm
- 27.07 3" SU8-3050 @ 3000 rpm written same day → ~ 53 µm
- 29.07 3" SU8-3025 @ 3000 rpm written two days after → ~ 44 µm
- 4" desired 150µm Layer → ~ 115µm



# Wafer – Laserwriting

Parameter	Value
Spot size	0.01 mm
Overlap	80%
Modulation	100%
Z-Position	-6.782
velocity	40 mm/s (omitted lines in dialog)