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# Quantitative EEG reflects non-dopaminergic disease severity in Parkinson's disease



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## HIGHLIGHTS

- EEG parameters correlate to measures of disease severity in patients with Parkinson's Disease.
- Both EEG slowing and reduced connectivity correlate to non-dopaminergic disease severity.
- The proposed markers may be useful in the screening process for Deep Brain Stimulation.

### ABSTRACT

*Objective:* In Parkinson's Disease (PD), measures of non-dopaminergic systems involvement may reflect disease severity and therefore contribute to patient-selection for Deep Brain Stimulation (DBS). There is currently no determinant for non-dopaminergic disease severity. In this exploratory study, we investigated whether quantitative EEG reflects non-dopaminergic disease severity in PD.

Methods: Sixty-three consecutive PD patients screened for DBS were included (mean age  $62.4 \pm 7.2$  years, 32% females). Relative spectral powers and the Phase-Lag-Index (PLI) reflecting functional connectivity were analysed on routine EEGs. Non-dopaminergic disease severity was quantified using the SENS-PD score and its subdomains; motor-severity was quantified using the MDS-UPDRS III.

Results: The SENS-PD composite score correlated with a spectral ratio  $((\delta + \theta)/(\alpha 1 + \alpha 2 + \beta))$  powers) (global spectral ratio Pearson's r = 0.4, 95% Confidence Interval (95%CI) 0.1–0.6), and PLI in the  $\alpha 2$  band (10–13 Hz) (r = -0.3, 95%CI -0.5 to -0.1). These correlations seem driven by the subdomains cognition and psychotic symptoms. MDS-UPDRS III was not significantly correlated with EEG parameters.

Conclusions: EEG slowing and reduced functional connectivity in the  $\alpha 2$  band were associated with non-dopaminergic disease severity in PD.

Significance: The described EEG parameters may have complementary utility as determinants of non-dopaminergic involvement in PD.

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# 1. Introduction

Parkinson's Disease (PD) is a multisystem neurodegenerative disorder, caused by progressive degeneration of both dopaminergic and non-dopaminergic neurons (Jellinger, 2012). Dopaminergic neurons account primarily for the characteristic motor symptoms of PD, whilst non-dopaminergic neurons account for non-motor

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symptoms such as impaired cognition, psychiatric manifestations or sleep disturbances. PD is typically treated with oral dopaminergic medication, which alleviates motor symptoms. However, medication-related motor complications occur in the majority of patients within 10 years of disease (Ahlskog et al., 2001). Patients refractory to oral treatment may be eligible for Deep Brain Stimulation (DBS), which ameliorates motor complications and improves quality of life (Deuschl et al., 2013). DBS is particularly effective in patients perceiving substantial motor improvement upon dopaminergic treatment (Moldovan et al., 2015). However, non-dopaminergic symptoms such as cognitive impairment,

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(Contarino et al., 2007) depression (Weaver et al., 2009), speech intelligibility (Tripoliti et al., 2011) and axial symptoms (Russmann et al., 2004) may deteriorate post-DBS. This indicates the need for accurate assessment of non-dopaminergic disease severity during the preoperative selection process.

Clinical, neuropsychological and psychiatric evaluations are used to rule out severe cognitive decline or psychiatric comorbidity. However, several factors including intelligence, education, and personality limit the interpretability of clinimetric assessments (Duncan, 1993). Moreover, questionnaires and performance tasks are susceptible to misinterpretation, social desirability bias, or fatigue (Duckworth et al., 2015). Therefore, there is a need for complementary measures reflecting disease severity in PD to aid the identification of DBS candidates.

Ouantitative Electroencephalography (gEEG) is an inexpensive and widely available tool which measures brain activity directly. Previous studies applied gEEG to examine clinical domains in PD. such as cognition (Caviness et al., 2015; Cozac et al., 2016), response to treatment (George et al., 2013) or motor impairment (Babiloni et al., 2011; George et al., 2013). Global oscillatory slowing of the EEG spectrogram is a highly suitable biomarker for cognitive impairment in PD (Caviness et al., 2015). Recent advances in neurophysiology have provided more complex markers such as connectivity parameters and graph theory estimations, which quantify brain network disorganization. The Phase-Lag Index (PLI), which reflects functional connectivity, was suggested as a potential biomarker of PD dementia (Utianski et al., 2016). To our knowledge the relation of qEEG parameters to measures of non-dopaminergic severity in PD has not been investigated so far. We aimed to investigate whether qEEG correlates with clinical measures of disease severity, in order to ultimately provide neurophysiological determinants of disease severity.

# 2. Methods

# 2.1. Study participants

All consecutive PD patients who were referred for preoperative screening to the DBS center of Leiden University Medical Center (LUMC) and Haga Teaching Hospital between September 2015 and July 2017 were included in the study. All patients fulfilled the Movement Disorders Society PD criteria for clinically established PD (Postuma et al., 2015). Written informed consent was obtained from all patients. A formal ethical evaluation of this study was waived by the local medical ethics committee.

#### 2.2. Outcome measures

Motor function was assessed with the Movement Disorders Society Unified Parkinson's Disease Rating Scale (MDS-UPDRS) part III (Goetz et al., 2007) (range 0–132), whereas the SEverity of Nondopaminergic Symptoms in Parkinson's Disease (SENS-PD) scale quantified non-dopaminergic disease severity (van der Heeden et al., 2016) (range 0-54). The SENS-PD scale is a composite score comprising three items with four response options (range 0-3) from each of the following six predominantly non-dopaminergic domains: postural instability and gait difficulty (PIGD), psychotic symptoms, excessive daytime sleepiness (EDS), autonomic dysfunction, cognitive impairment and depressive symptoms (van der Heeden et al., 2016). These six domains represent a coherent complex of symptoms that is already present in early disease stages and increases in severity with age and advancing disease. The SENS-PD scale is a recently developed, short, reliable and valid scale that includes symptoms that do not improve with dopaminergic medication and may therefore more accurately reflect severity and progression of the underlying disease than currently used dopamine-sensitive measures. Higher scores on both the MDS-UPDRS III and SENS-PD scale reflect more severe impairment.

Patients were subdivided a posteriori into three groups of comparable size, according to the tertile in which their SENS-PD score fell: low disease severity (range 4–10), intermediate severity (range 11–14) and high severity (range 15–24).

# 2.3. EEG recording and pre-processing

EEGs were recorded with patients lying supine, with eyes closed, during a state of relaxed wakefulness. Light was kept at moderate intensity. Ag/AgCl EEG electrodes were placed on the scalp using 21 standard 10–20 EEG electrode positions. Additional ECG and horizontal eye movement leads were added for identification of artifacts. Data were acquired online using a Nihon Kohden EEG-1200 system, with a 500 Hz sampling rate, a 16-bit analog-to-digital converter, and band-filtered between 0.16 and 70 Hz. An EEG technician monitored signal quality throughout the entire recording; patients were alerted by acoustic stimuli upon drowsiness. All patients used dopaminergic medication according to their individual schedule.

#### 2.4. EEG analysis

EEG data were re-referenced towards a source derivation which approaches the surface Laplacian derivation (Hjorth, 1980). Five consecutive, non-overlapping 4096-point epochs lasting 8.192 s were selected for further analysis after an artifact-free signal was visually confirmed. The individual epochs were offline converted to American Standard Code for Information Interchange (ASCII) format and further analysed using Brainwave software (BrainWave version 0.9.152.4.1, C.J. Stam; available at <a href="http://home.kpn.nl/stam7883/brainwave.html">http://home.kpn.nl/stam7883/brainwave.html</a>). Recordings with less than five artifact-free epochs were excluded from analysis. Analyses were performed in signal space to allow for direct analysis of the raw EEG data in Brainwave software, which is easily reproducible for most clinicians and may increase the utility of our findings.

Spectral analysis was performed off-line by processing each epoch with a Fast Fourier Transform (FFT) and averaged to produce a power spectrum for each individual electrode. The frequency bands were defined as  $\delta$  (0.5–4.0 Hz),  $\theta$  (4.0–8.0 Hz),  $\alpha$ 1 (8.0-10.0 Hz),  $\alpha 2 (10.0-13.0 \text{ Hz})$  and  $\beta (13.0-30.0 \text{ Hz})$ .  $\gamma$  band power was not analysed due to frequent contamination with muscle artifacts. Relative bandpower was calculated by dividing the absolute bandpower of each frequency band by the total absolute bandpower from the FFT average per channel. Regional band powers were defined as: frontal for F3, F4, F7, F8 and Fz, temporal for T3, T4, T5 and T6, parietal for P3, P4 and Pz, central for C3, C4 and Cz, and occipital for O1 and O2. Global bandpower was defined as the average of all regional band powers. A spectral ratio was calculated by dividing the sum of the relative power in the  $\delta$  and  $\theta$ bands by the sum of the relative power in the  $\alpha$  and  $\beta$  bands. These spectral bands were selected a priori to incorporate as much of the EEG spectrum as possible, without contaminating the results with possible artefacts that may be present in the fast frequency bands.

Functional connectivity was assessed by calculating the PLI in each frequency band. The PLI quantifies phase coupling (range 0–1) whilst being insensitive to common sources and volume conduction. PLI = 0 indicates either no phase synchronization or equal in both leading and lagging throughout the epoch, PLI = 1 indicates perfect phase-locking (Stam et al., 2007).

# 2.5. Statistical analysis

Baseline demographic, clinical, and test variables were notnormally distributed and were thus compared between the three groups with Kruskal-Wallis H tests for continuous variables and Pearson's  $\chi^2$  tests for dichotomous variables. Included and excluded patients were compared using Mann-Whitney U tests. QEEG parameters were compared across SENS-PD tertiles using Kruskal-Wallis H tests; Mann-Whitney U tests compared the high- and low-disease severity tertiles.

The association between the SENS-PD composite score, SENS-PD subdomains, MDS-UPDRS III score and qEEG parameters was assessed by calculating partial Pearson's r correlation coefficients, with an additional correction for age and usage of psychoactive medication, which may influence EEG parameters. Bias-corrected and accelerated bootstrapping was performed with 7000 samples to normalize the data; further increasing the amount of samples did not improve statistical accuracy.

Given the exploratory nature of our study, to avoid type II errors, no further correction for multiple testing was applied. Missing values were imputed using multiple imputation with five iterations, if no more than 15% of the data was missing.

All analyses were performed using IBM Statistical Package for the Social Sciences 23 Software (SPSS Inc., Chicago, Illinois, USA). Significance was set at the 0.05 level. Graphical visualization of results was performed in either MATLAB R2016A (The MathWorks Inc., Natick, Massachusetts, USA) or GraphPad Prism 7.02 (GraphPad Software Inc., La Jolla, California, USA).

### 3. Results

#### 3.1. Patient characteristics

Eighty patients underwent DBS screening during the study period. Seventeen patients were excluded due to gross artifacts during EEG recordings (low disease severity: n = 8, intermediate severity: n = 3, high disease severity: n = 6); analysis was thus performed on 63 patients (32% female). There were no significant differences in demographic and clinical variables between included and excluded patients. Mean (SD) age was 62.4 (7.2) years, and disease duration 11.9 (6.3) years (Table 1). There were no significant differences in age, sex, disease duration, psychoactive drug usage and MDS-UPDRS III score between the three SENS-PD tertiles. By design, both the SENS-PD score and all six subdomains differed significantly between tertiles, with higher scores for the high-disease-severity group.

# 3.2. Spectral analyses

Slower EEG frequency bandpowers (i.e.  $\delta$  and  $\theta$ ) were higher in the high-disease-severity group, whereas faster frequency

bandpowers (i.e.  $\alpha 1$ ,  $\alpha 2$  and  $\beta$ ) were higher in the low-disease-severity group (Fig. 1).

Mean spectral ratios (Supplementary Table 1) differed significantly between the high and low tertiles, both globally and over the frontal, central, parietal and occipital regions. The high-disease-severity group demonstrated a higher spectral ratio, indicating a greater proportion of slow EEG power.

The SENS-PD composite score showed a significant positive correlation with the spectral ratio: a higher ratio, reflecting a greater proportion of slow EEG power, correlated with more severe non-dopaminergic impairment, across all brain regions. The subdomains cognition and psychotic symptoms showed significant correlations for all regions, whilst the subdomains PIGD and depression showed a non-significant positive trend. The subdomains EDS, autonomic dysfunction and the MDS-UPDRS III score did not correlate with EEG parameters (Fig. 2).

# 3.3. Functional connectivity

Global PLI in the  $\alpha 2$  band was significantly different between the three tertiles, while differences in the other frequency bands were non-significant (Supplementary Table 2). Regional mean  $\alpha 2$  PLI values (Supplementary Table 3) differed significantly between the tertile groups over the frontal, central, temporal and occipital regions. Patients in the high-disease-severity group had a lower connectivity density, i.e. number of connections per threshold PLI value, than patients in the low-disease-severity group (Fig. 3), indicating that higher disease severity was associated with lower functional connectivity.

Global, frontal, central, parietal and occipital PLI in the  $\alpha 2$  band was significantly negatively associated with the SENS-PD composite score and with the cognitive subdomain (Supplementary Figs. 1 and 2). The subdomain 'psychotic symptoms' showed a significant negative correlation over the central electrodes and a negative trend over all brain regions. In all instances, reduced functional connectivity correlated with higher disease severity.

# 4. Discussion

Several qEEG parameters were found to have potential as neurophysiological determinants of advanced non-dopaminergic disease severity in PD. As high non-dopaminergic disease severity is a relative contra-indication for DBS, qEEG analysis may ultimately complement clinimetric evaluations to optimize the screening process of DBS candidates.

**Table 1**Demographic and clinical characteristics.

	Overall	Low SENS-PD	Intermediate SENS-PD	High SENS-PD	P
N	63	17	25	21	
EEG data, seconds	516.1	139.3	204.8	172.0	
Age, years	62.4 (7.2)	61.6 (6.4)	62.2 (7.5)	63.3 (7.5)	0.825
Female sex	20 (32)	6 (35)	8 (32)	6 (29.0)	0.906
Disease duration, years	11.9 (6.3)	10.6 (3.0)	12.0 (6.7)	12.9 (7.6)	0.718
Use of psychoactive drugs	15 (31)	3 (18)	5 (20)	7 (33)	0.448
MDS-UPDRS III total score	24.0 (10.1)	20.7 (9.2)	24.3 (11.1)	26.4 (9.1)	0.167
SENS-PD total score	13.1 (4.9)	7.6 (1.8)	12.0 (0.8)	18.8 (2.9)	<0.001 <sup>a</sup>
PIGD subscore	1.2 (1.0)	0.7 (0.8)	1.0 (1.0)	1.8 (0.8)	0.001 <sup>b,c</sup>
EDS subscore	2.7 (1.8)	1.8 (1.3)	2.1 (1.5)	4.1 (1.6)	<0.001 <sup>b,c</sup>
Depression subscore	2.4 (2.0)	1.1 (1.6)	2.1 (1.7)	3.6 (2.1)	0.001 <sup>b,c</sup>
Autonomic dysfunction subscore	2.1 (1.2)	1.4 (1.1)	2.0 (1.0)	2.8 (1.2)	0.002 <sup>c</sup>
Psychotic symptoms subscore	1.0 (0.9)	0.5 (0.5)	0.9 (0.7)	1.5 (1.1)	<0.001 <sup>b,c</sup>
Cognition subscore	4.0 (1.6)	3.0 (1.6)	4.0 (1.2)	4.8 (1.6)	0.002 <sup>c</sup>

Results are expressed as mean (SD) for continuous variables, n (%) for categorical variables.

PIGD: postural instability and gait difficulty; EDS: excessive daytime sleepiness.

<sup>&</sup>lt;sup>a</sup> Sig. difference between all three groups.

<sup>&</sup>lt;sup>b</sup> Sig. difference between intermediate and high tertiles.

<sup>&</sup>lt;sup>c</sup> Sig. difference between low and high tertiles.

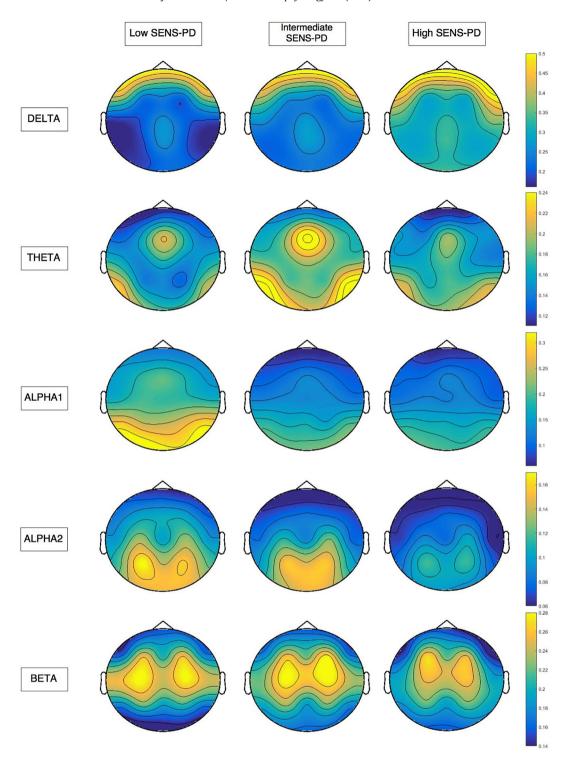


Fig. 1. Distribution of the mean spectral powers per tertile of disease severity. The high SENS-PD group demonstrated higher power in the slow EEG frequency bands (i.e.  $\delta$  and  $\theta$ ); the low SENS-PD group demonstrated higher power in the faster EEG frequency bands (i.e.  $\alpha$ 1,  $\alpha$ 2 and  $\beta$ ), indicating a global slowing of EEG frequency with increasing disease severity (yellow: high power, blue: low power). (For interpretation of the references to colour in this figure legend, the reader is referred to the web version of this article.)

Slower EEG oscillatory activity was associated with more advanced non-dopaminergic disease severity measured by the SENS-PD score and, in particular, with the subdomains cognition and psychotic symptoms, with a trend towards a correlation with PIGD and depressive symptoms. Conversely, the subdomains EDS and autonomic dysfunction did not show a clear pattern of

correlation. Motor impairment did not significantly correlate with spectral parameters.

Previous literature confirms the association between cortical slowing and cognitive impairment in PD (Caviness et al., 2015). The consistent EEG slowing both on a global level and across all the different brain areas indicates diffuse dysfunction. It has been

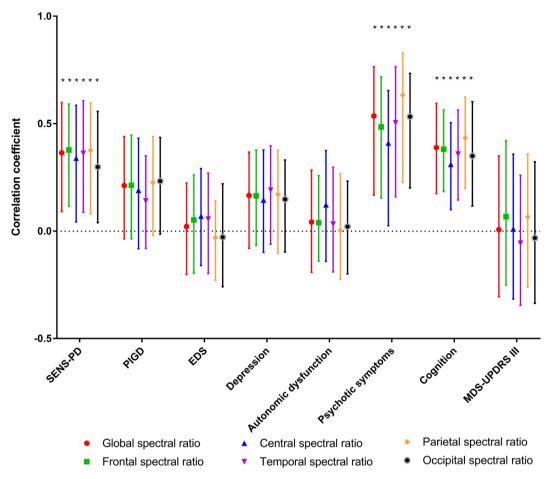


Fig. 2. Correlation of slow-over-fast spectral ratio and disease severity. Asterisks indicate significant correlations. A spectral ratio of slow-over-fast EEG power correlated significantly with the SENS-PD composite score (i.e. more slow EEG power correlated with increased non-dopaminergic disease severity). The subdomains psychotic symptoms and cognition correlated significantly with the spectral ratio, whilst a trend could be observed for the subdomains PIGD and depression. Error bars reflect 95% confidence intervals.

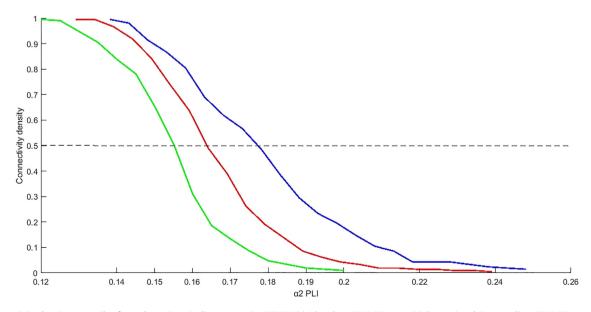
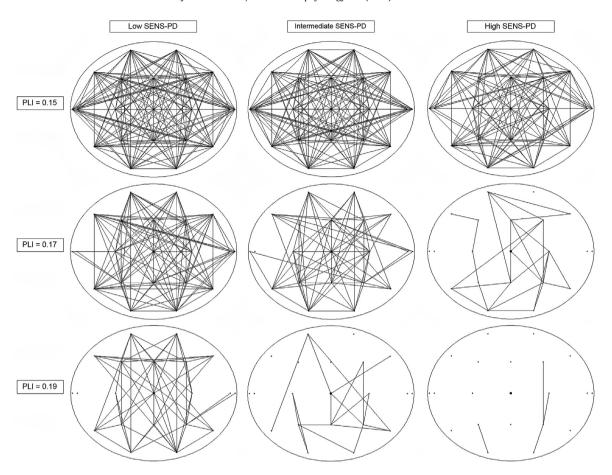


Fig. 3A. Connectivity density per tertile of non-dopaminergic disease severity (SENS-PD). Blue: low SENS-PD group (rightmost), red: intermediate SENS-PD group, green: high SENS-PD group (leftmost). The high SENS-PD group demonstrated lower  $\alpha 2$  PLI density than the low SENS-PD group, indicating a reduction of functional connectivity with increasing disease severity. Network maps of the mean PLI at three thresholds, i.e. PLI = 0.13, 0.15 and 0.17 are shown in Fig. 3B. (For interpretation of the references to colour in this figure legend, the reader is referred to the web version of this article.)



**Fig. 3B.** Average network maps of the mean PLI in the  $\alpha$ 2 band per tertile of disease severity. The  $\alpha$ 2 PLI network maps are plotted at three thresholds: PLI = 0.15, 0.17 and 0.19. A line indicates a level of functional connectivity of at least the threshold-value. With higher SENS-PD scores, the threshold for functional connectivity is lowered, indicating a greater degree of cortical desynchronization with increased disease severity.

previously suggested that diffuse cortical slowing in PD reflects a degeneration of a non-dopaminergic system with ascending cortical projections (Olde Dubbelink et al., 2013), which seems compatible with the observed correlation between clinical measures of non-dopaminergic disease severity and EEG slowing.

Cortical slowing has been associated with severity of psychiatric symptoms also in other conditions. In schizophrenic patients, auditory hallucinations were associated with task-related  $\theta$  slowing (Zheng et al., 2015) and in cases with a delirium, visual hallucinations were associated with  $\theta\text{-}\delta$  slowing (Teeple et al., 2009). Although results of these studies based on other diseases may not be directly comparable with PD, we speculate that these findings suggest a more general cortical desynchronization, rather than network alterations that are specific to PD.

Reduced functional connectivity in the  $\alpha 2$  band significantly correlated with higher non-dopaminergic disease severity, particularly with cognition, with a similar trend for the subdomains psychotic symptoms, depression, PIGD and EDS. Motor impairment did not correlate with functional connectivity. Only one EEG-study previously investigated PLI in PD, reporting reduced  $\alpha 1$  PLI values in demented PD patients relative to cognitively normal PD patients.  $\alpha 1$  PLI likewise correlated with the MMSE scale (Utianski et al., 2016). Reduced  $\alpha 1$  PLI values were also found to correlate with increased severity in Alzheimer's Disease (AD) (Engels et al., 2015). Our results indicate a non-significant trend for  $\alpha 1$  PLI, whereas we found  $\alpha 2$  PLI to be significantly reduced. This discrepancy can be explained by a difference in population, as previous studies investigated patients with more advanced cognitive deterioration while our population did not include

demented PD patients, being this a contra-indication for the DBS screening procedure. However, these findings suggest that desynchronization of a similar  $\alpha$ -band (either  $\alpha 1$  or  $\alpha 2$ ) network might underlie cognitive deterioration in both PD and AD.

The described qEEG parameters, both oscillatory slowing and functional connectivity, demonstrate discriminative ability at a group-level and may be further investigated to determine their potential as biomarkers at an individual level.

Strengths of our study are the large sample size of consecutively included patients, standardized examinations and use of a novel and validated clinimetric scale (SENS-PD). A limitation of the SENS-PD scale is that the different subdomains may reflect different systems-at-risk, indicating that similar scores between patients may reflect altogether different phenotypes, although this holds true for any multidimensional scale including the MDS-UPDRS III. From a clinical perspective, not all symptoms may be equally important, therefore the correlations with the SENS-PD scale were studied both for the composite scores and its subdomains. Our study population consisted of potential candidates for DBS. Typically, these patients had severe motor symptoms without obvious clinical signs of cognitive dysfunction or psychotic symptoms. This homogeneity constitutes both a limitation and a strength: although it is currently unknown whether our results can be generalised to all PD patients, we show that qEEG is capable of quantifying subtle differences in patients with cognitive and psychiatric symptoms that might go unnoticed in a global clinical impression. Investigations in a wider range of PD patients at different disease stages are likely to show even more pronounced correlations. Consequently, qEEG biomarkers for non-dopaminergic disease severity at different disease-stages could have clinical applicability beyond DBS screening, such as monitoring of disease progression.

The two applied methods of qEEG analysis do not show identical correlations with non-dopaminergic domains, suggesting that they address different functional aspects. The negative association of cortical connectivity in the  $\alpha 2$  band with cognitive impairment but the lack of correlation with the other non-motor domains may reflect the subcortical nature of the latter. Whereas  $\alpha$ -band connectivity is associated with cognition, it is not specifically limited to cognition as evidenced by a non-significant trend in the domain 'psychotic symptoms.' Although subcortical networks influence cortical processes (Boon et al., 2017), the exact subcortical alterations are not properly visualized by EEG which accounts for the different results. Likewise, the lack of correlation between motor functioning and EEG slowing provides further evidence that severity of motor impairment as assessed by the MDS-UPDRS III is not reflected by cortical slowing (Babiloni et al., 2011). Indeed, oscillatory alterations in the (subcortical) basal ganglia, which correlate with motor dysfunction (Brittain et al., 2014), cannot be captured by EEG. Magnetoencephalography (MEG) could investigate these subcortical networks (Boon et al., 2017), however MEG is not widely available and is less applicable for routine DBS screening purposes. Previous longitudinal studies using MEG have identified slowing of oscillatory brain activities to be correlated with global disease progression in PD (Olde Dubbelink et al., 2013).

A limitation of the applicability of EEG as a biomarker is the proportion of excluded patients due to EEG artifacts. These artifacts are partly inherent to the disease itself, such as altered muscle tone, increased ocular movements, tremor, dyskinesias, and sleepiness. As baseline characteristics, both motor and non-motor severity, did not differ between included and excluded patients, we expect that the incidence of artifacts is not associated with disease severity. This is also confirmed by the fact that in our cohort the number of recordings excluded because of artefacts was comparable in the low disease severity group and high disease severity group.

Several factors might influence EEG activity, such as aging or use of psychoactive medication. For this reason we corrected our results for both factors. Careful consideration of normal agerelated alterations cannot be neglected when assessing individual FEGs

Changes of spectral and connectivity parameters have also been found in epilepsy (Liang et al., 2010), AD (Engels et al., 2015), and schizophrenia (John et al., 2009) but it remains unclear whether these disorders have a common cortical denominator or whether there are different disease-specific network alterations.

EEG is available in every hospital, readily accessible and cheaper than other functional neuroimaging measures such as MEG, fMRI, PET or SPECT (Lystad et al., 2009). Moreover, source referencing amplified the spatial resolution, overcoming criticism of EEG's limited resolution (Burle et al., 2015). Whereas the 21-channel EEG setup could be enhanced by using a high-density setup, we demonstrated that conventional routine EEG is sufficient to provide parameters of non-dopaminergic disease severity. Advanced setups do not seem necessary to achieve sufficient discriminative ability on a group-level. In this study we demonstrate that disease severity is accurately reflected by both functional connectivity and simpler EEG spectral measures, which are calculated with relative ease by neurophysiologists. Future research could focus on validation in larger and more heterogeneous cohorts to investigate whether gEEG may serve as biomarkers at an individual level, and determine its accuracy in estimating disease severity. The use of EEG parameters to aid the selection process of DBS candidates should also be further investigated.

In conclusion, we have demonstrated that both EEG slowing and reduced functional connectivity in the  $\alpha 2$  band are associated with increased non-dopaminergic disease severity in PD, particularly with cognitive impairment and psychotic symptoms. These EEG alterations were apparent both globally and over separate brain regions. The studied qEEG parameters may have the potential to ultimately serve as complementary biomarkers of non-dopaminergic disease severity in PD.

# **Conflict of interest**

This work was supported by a grant from the 'Stichting ParkinsonFonds' and the 'Stichting Alkemade-Keuls'. The funding sources had no role in the study design, data collection, analysis, interpretation, writing or decision to submit the manuscript for publication. None of the authors has potential conflicts of interest that relate to this manuscript.

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# Appendix A. Supplementary material

Supplementary data associated with this article can be found, in the online version, at https://doi.org/10.1016/j.clinph.2018.04.752.

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