

ECE 441 Interfacing & Modulating the Nervous System

Fall 2023

Lecture 06 Electrical Neural Interface



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Today's Agenda

- Neural signals
- Neural Signal Amplification
- Model of Electrode Interface
- Noise and Interferences
- Instrumentation Amplifiers

About Me

- **Experience**

- Assistant Professor – University of Toronto
- Affiliated Scientist – University Health Network
- Qualcomm Inc. (2016 – 2021)
- Ph.D. University of Pennsylvania

- **Research Interests**

- Integrated Circuits and Systems
- Brain Machine Interfaces
- Edge Artificial Intelligence

About Me

- **More about my research**

<https://www.eecg.utoronto.ca/~xilinliu/>

- **Contact**

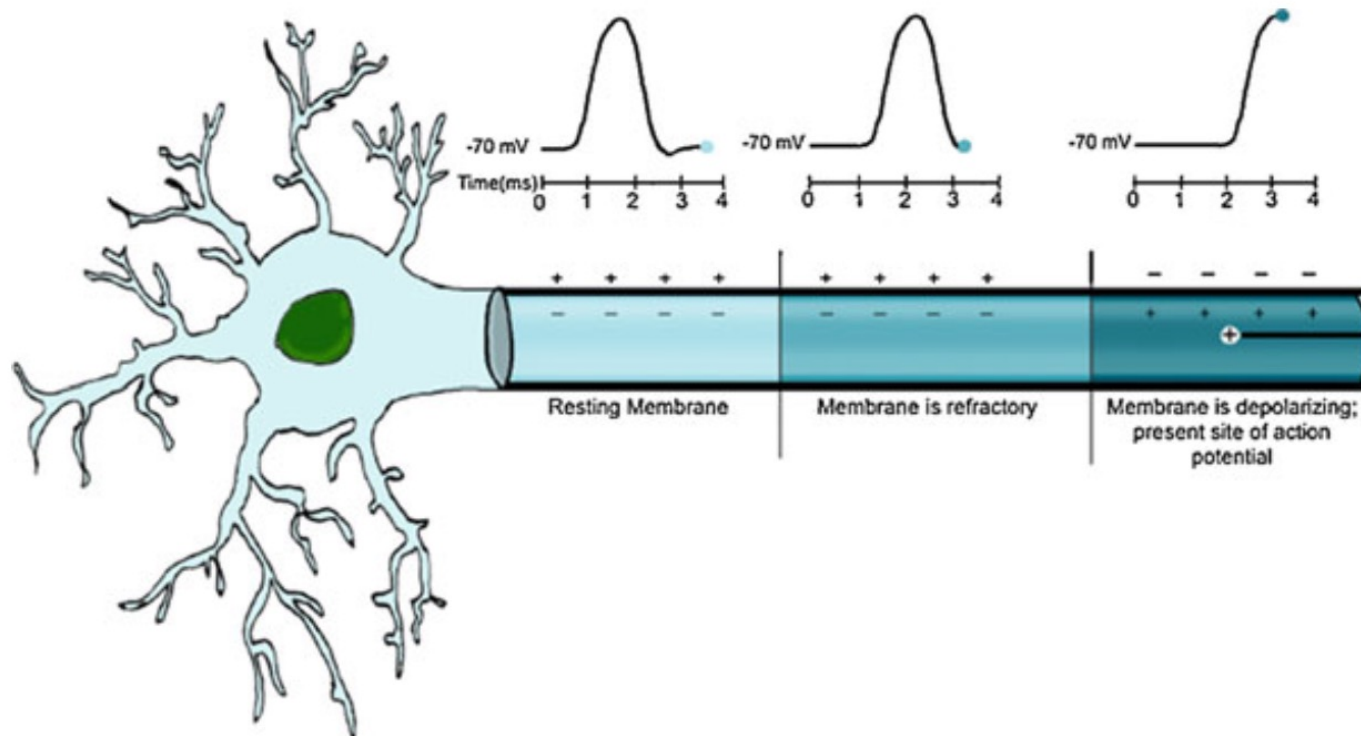
- Email: xilinliu@ece.utoronto.ca
- Office: BA5108

- **Office Hours**

- After lecture or by appointment

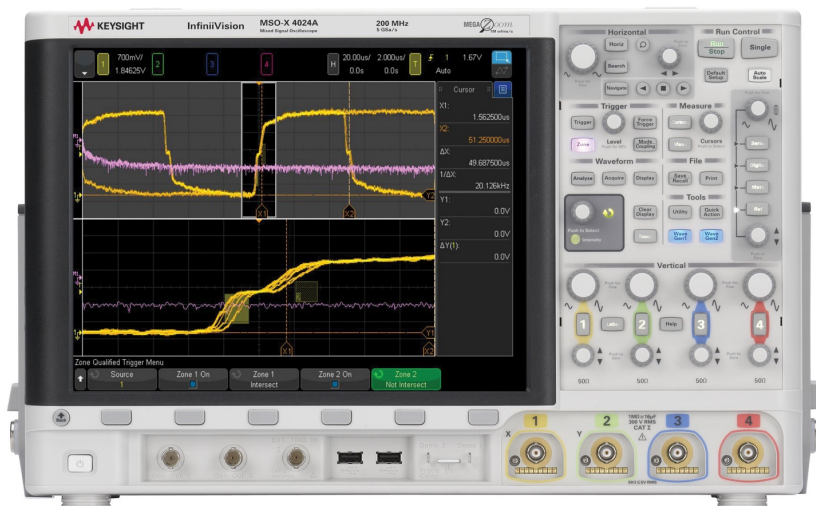
Neural Signals

Neural signals are essentially electrical and electrochemical signals

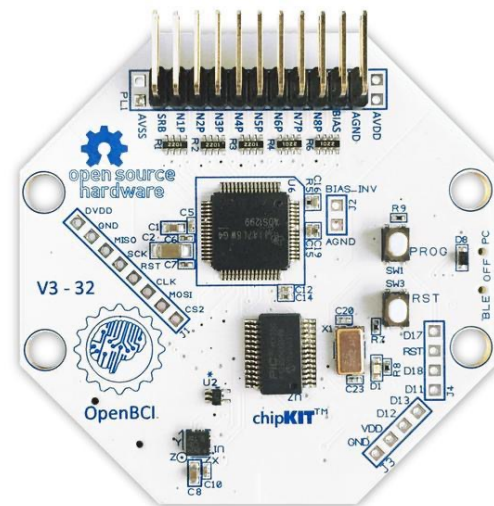


Neural Signals

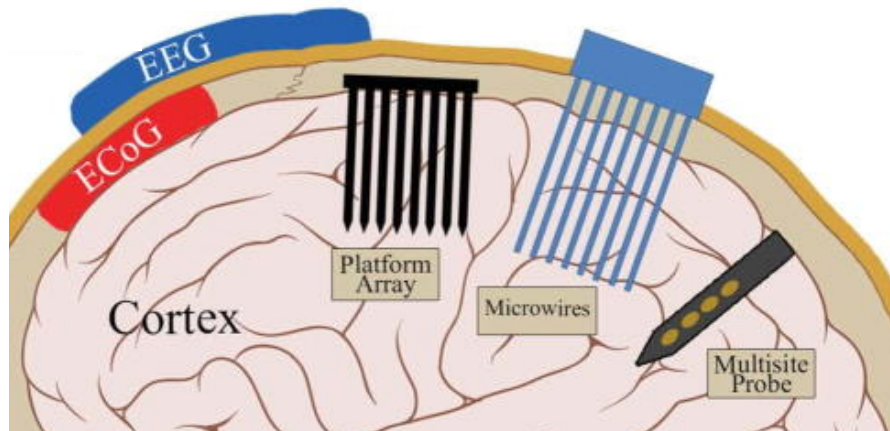
Can we use an oscilloscope to measure brain signals?



V.S.



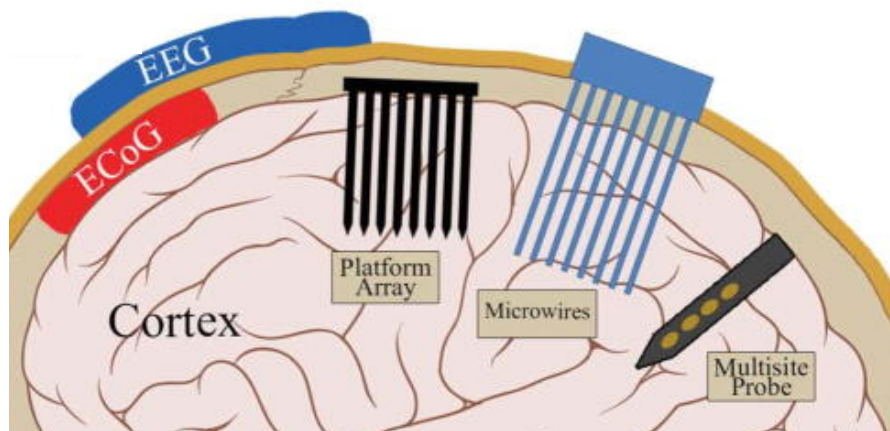
Neural Signals: EEG



EEG
5-300uV
< 100Hz

- **EEG:** Electroencephalogram

Neural Signals: ECoG

**EEG**5-300 μ V

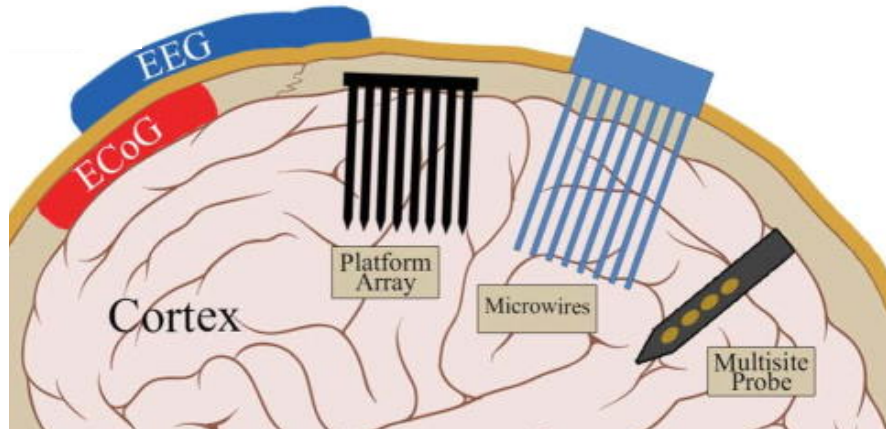
< 100Hz

**ECoG**10 μ V – 1mV

< 200Hz

- **EEG**: Electroencephalogram
- **ECoG**: Electrocorticography

Neural Signals: LFP & AP

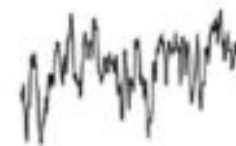


- **EEG**: Electroencephalogram
- **ECoG**: Electrocorticography
- **LFP**: Local Field Potential
- **AP**: Action Potential



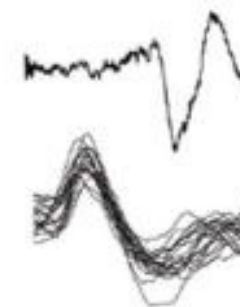
EEG

5-300uV
< 100Hz



ECoG

10uV – 1mV
< 200Hz



LFP

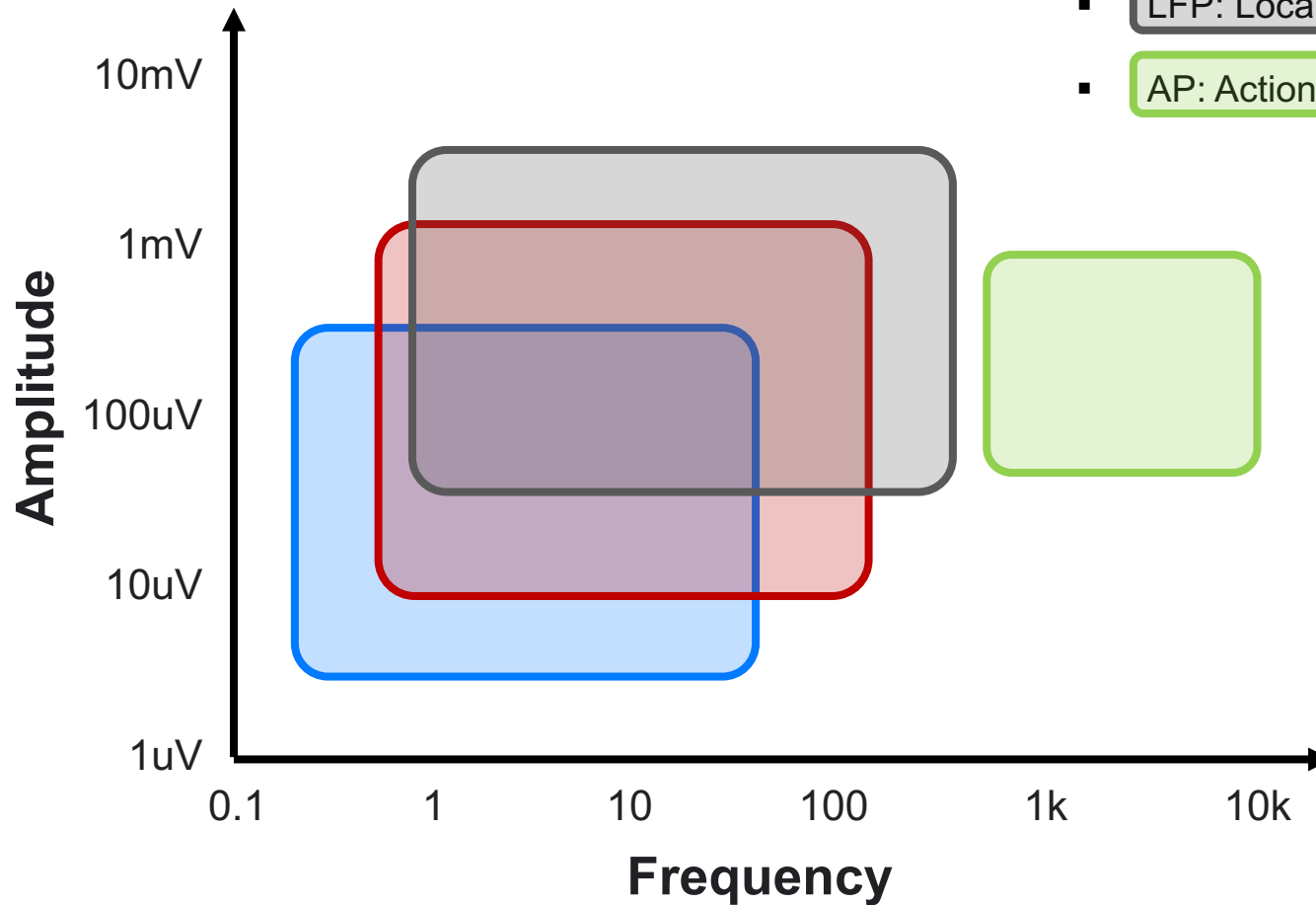
20uV – 2mV
< 500Hz

AP

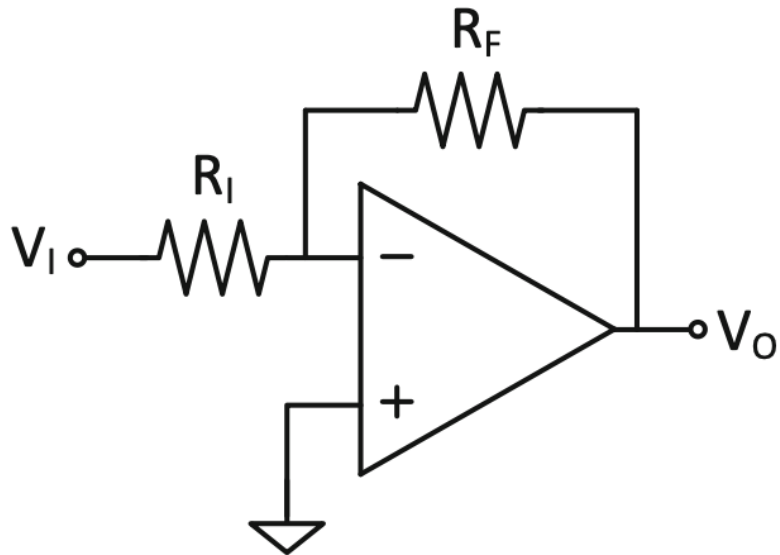
100uV – 1mV
100 – 7kHz

Neural Signals

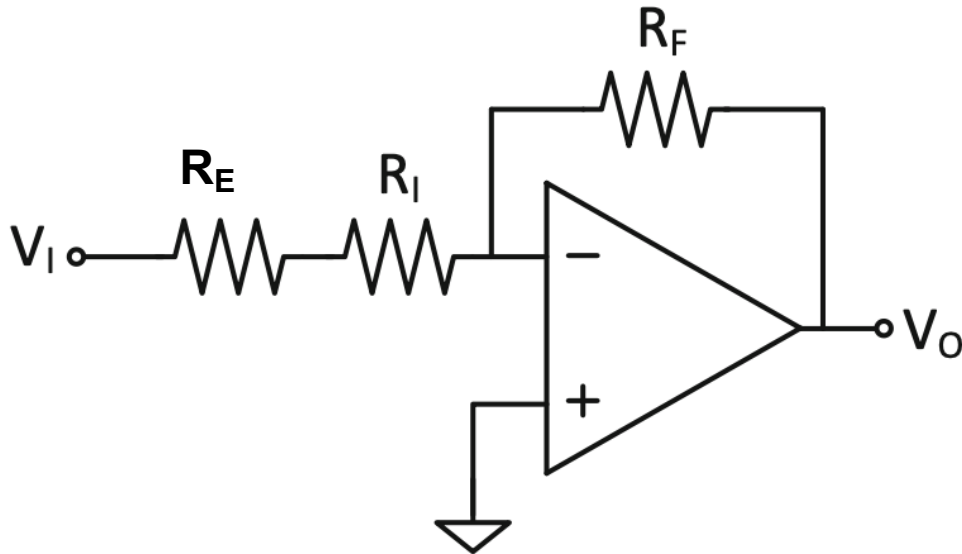
- EEG: Electroencephalogram
- ECoG: Electrocorticography
- LFP: Local Field Potential
- AP: Action Potential



Neural Signal Amplification



Neural Signal Amplification with Electrode



Neural Electrodes: EEG

Wet EEG Electrodes



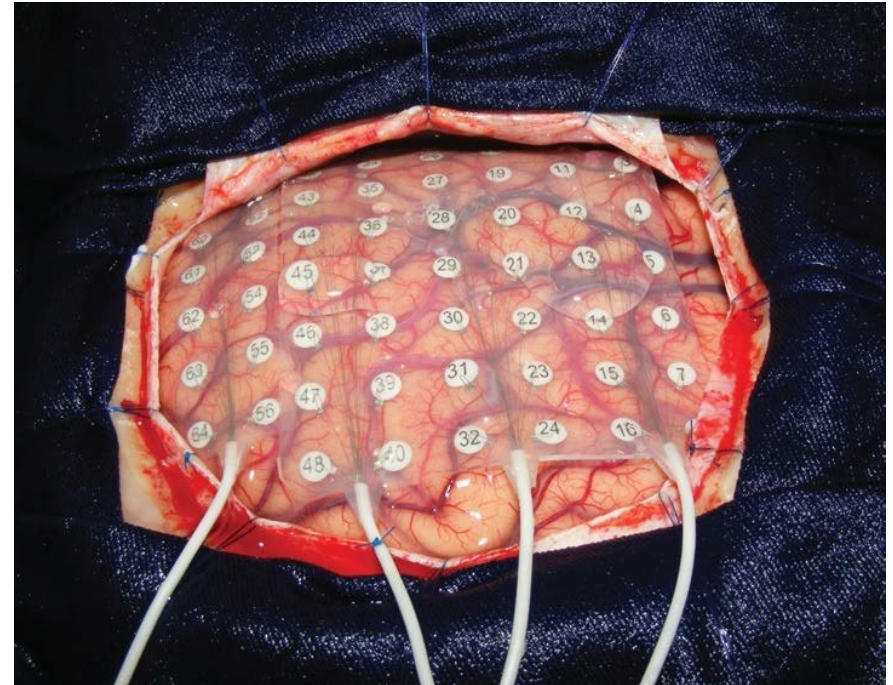
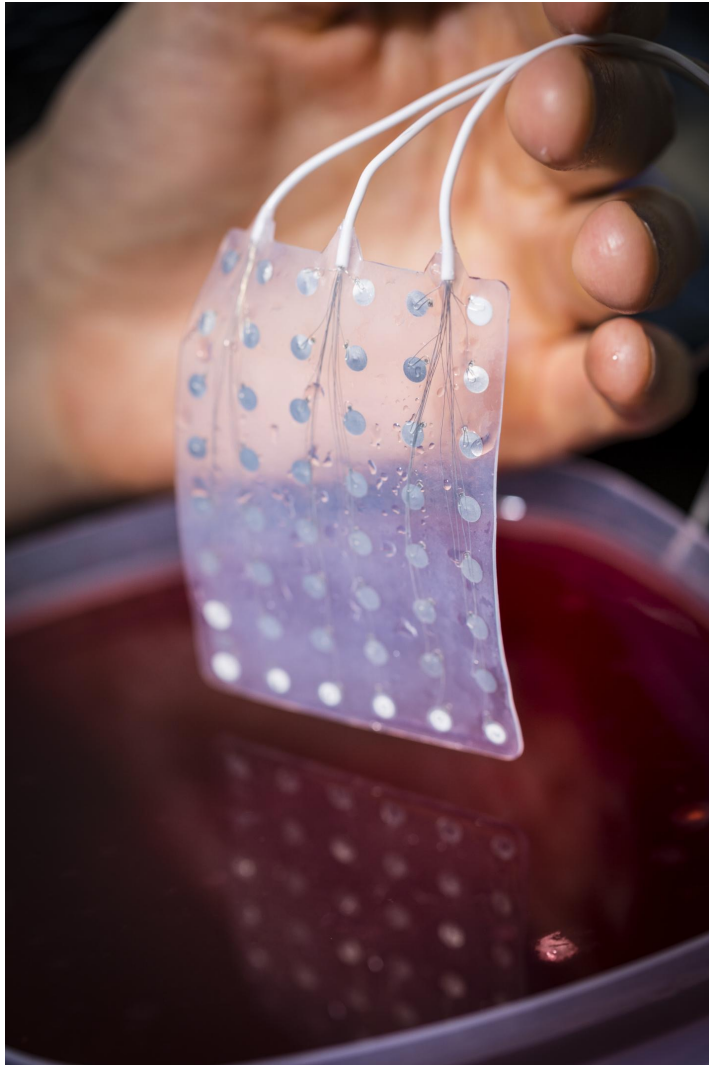
Impedance:
 $< 10\text{k}\Omega$

Dry EEG Electrodes



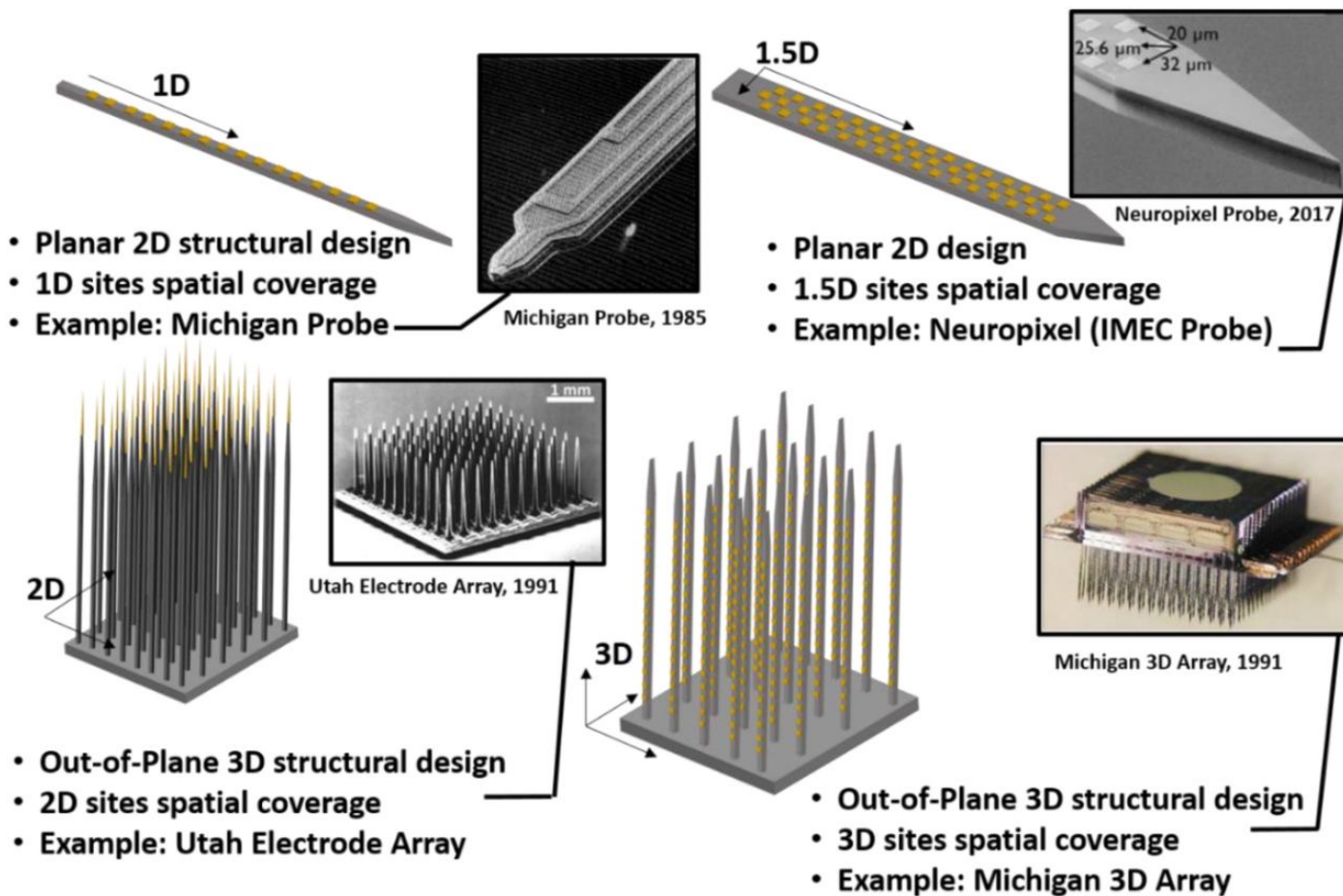
Impedance:
 $500\text{k}\Omega - 1\text{M}\Omega$

Neural Electrodes: ECoG



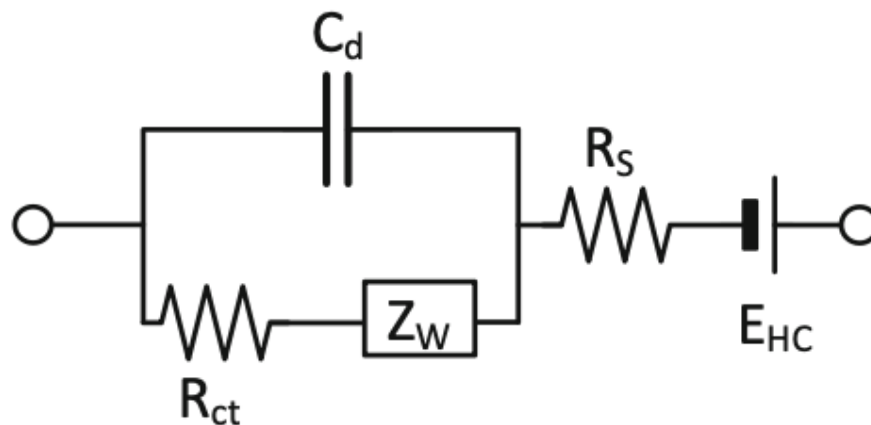
Impedance:
5-10kohm

Neural Electrodes: AP



Impedance: 300kohm – 5Mohm

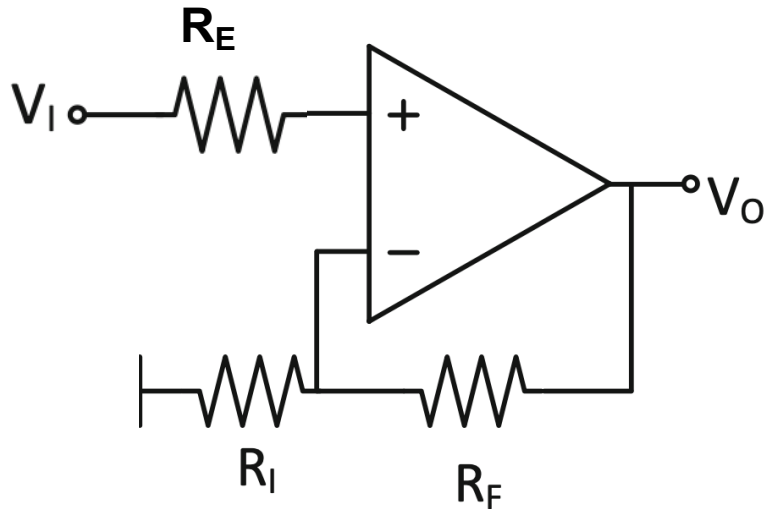
Model of Electrode Interface



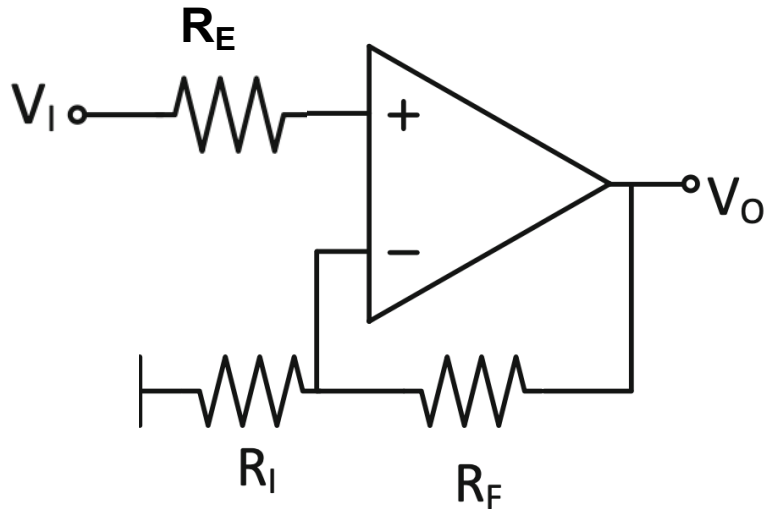
Metal and Reaction	Potential E^0 (V)
$\text{Al} \rightarrow \text{Al}^{3+} + 3\text{e}^-$	-1.706
$\text{Zn} \rightarrow \text{Zn}^{2+} + 2\text{e}^-$	-0.763
$\text{Cr} \rightarrow \text{Cr}^{3+} + 3\text{e}^-$	-0.744
$\text{Fe} \rightarrow \text{Fe}^{2+} + 2\text{e}^-$	-0.409
$\text{Cd} \rightarrow \text{Cd}^{2+} + 2\text{e}^-$	-0.401
$\text{Ni} \rightarrow \text{Ni}^{2+} + 2\text{e}^-$	-0.230
$\text{Pb} \rightarrow \text{Pb}^{2+} + 2\text{e}^-$	-0.126
$\text{H}_2 \rightarrow 2\text{H}^+ + 2\text{e}^-$	0.000 by definition
$\text{Ag} + \text{Cl}^- \rightarrow \text{AgCl} + \text{e}^-$	+0.223
$2\text{Hg} + 2\text{Cl}^- \rightarrow \text{Hg}_2\text{Cl}_2 + 2\text{e}^-$	+0.268
$\text{Cu} \rightarrow \text{Cu}^{2+} + 2\text{e}^-$	+0.340
$\text{Cu} \rightarrow \text{Cu}^+ + \text{e}^-$	+0.522
$\text{Ag} \rightarrow \text{Ag}^+ + \text{e}^-$	+0.799
$\text{Au} \rightarrow \text{Au}^{3+} + 3\text{e}^-$	+1.420
$\text{Au} \rightarrow \text{Au}^+ + \text{e}^-$	+1.680

SOURCE: Data from *Handbook of Chemistry and Physics*, 55th ed., Cleveland, OH: CRC Press, 1974-1975, with permission.

Neural Signal Amplification with Electrode

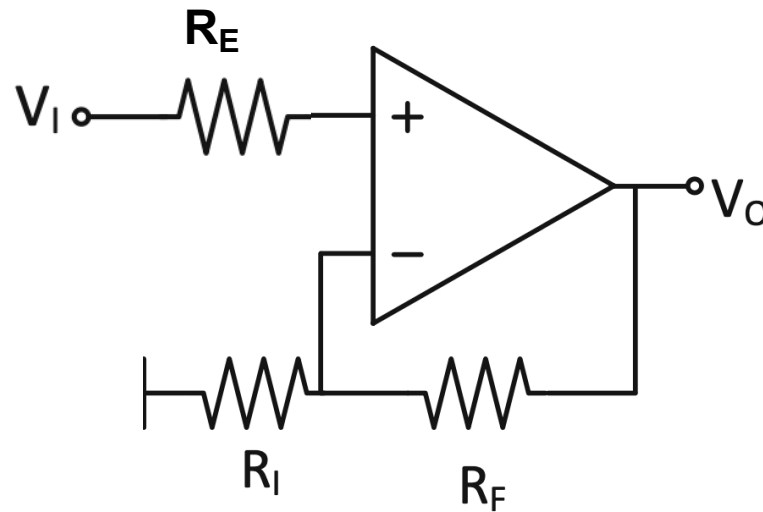


Neural Signal Amplification with Electrode



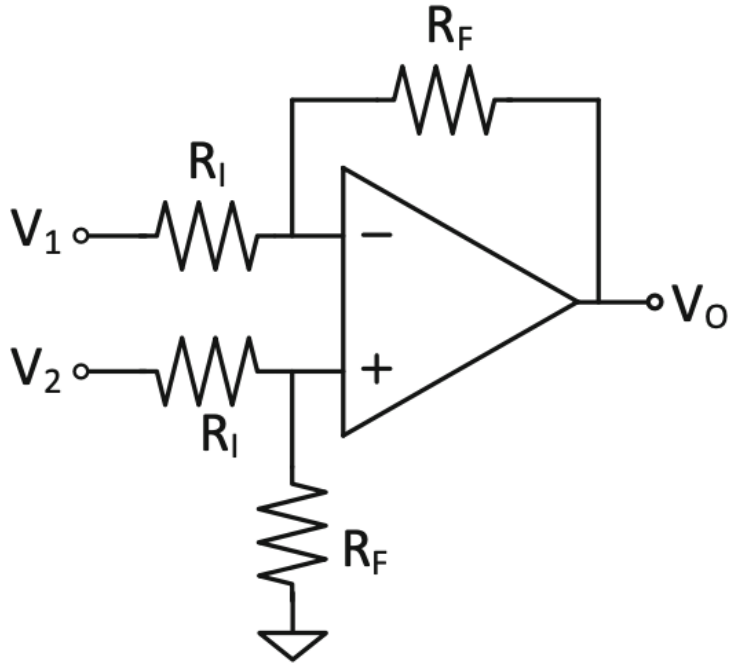
If we consider the non-idealities of the amplifier...

Noise and Interference

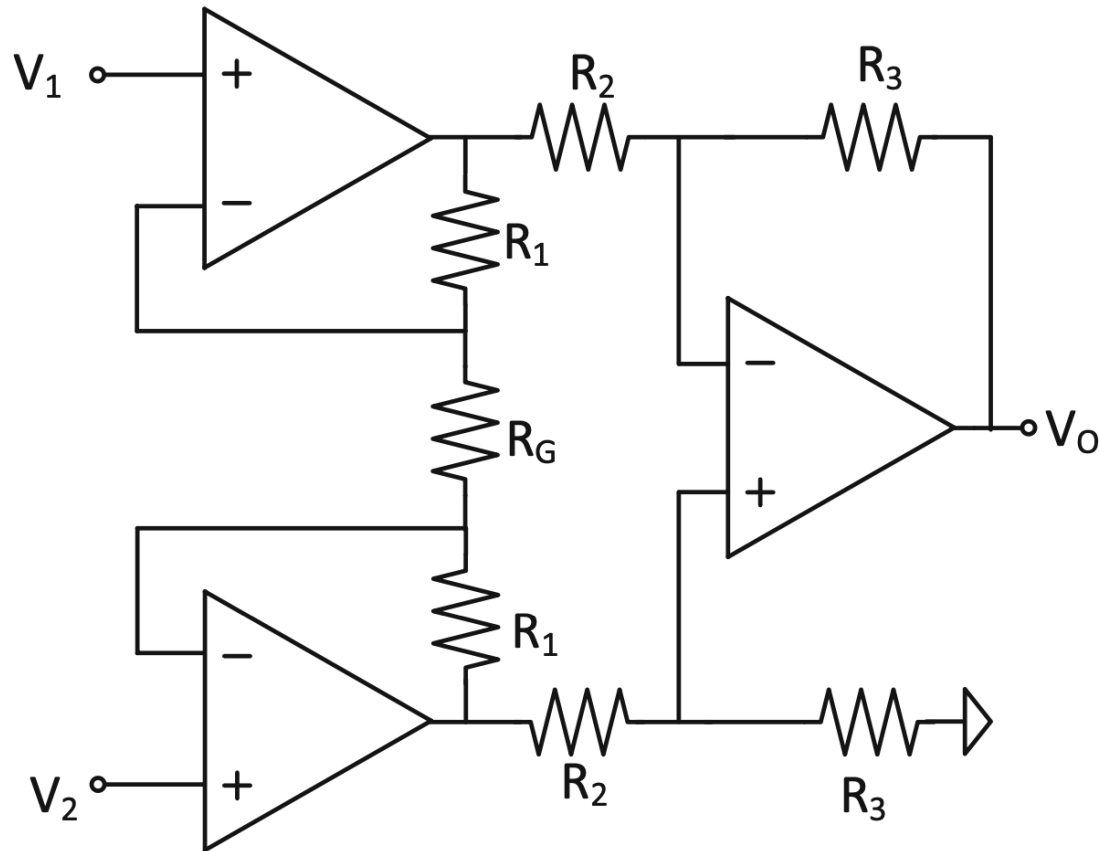


Common Mode Rejection

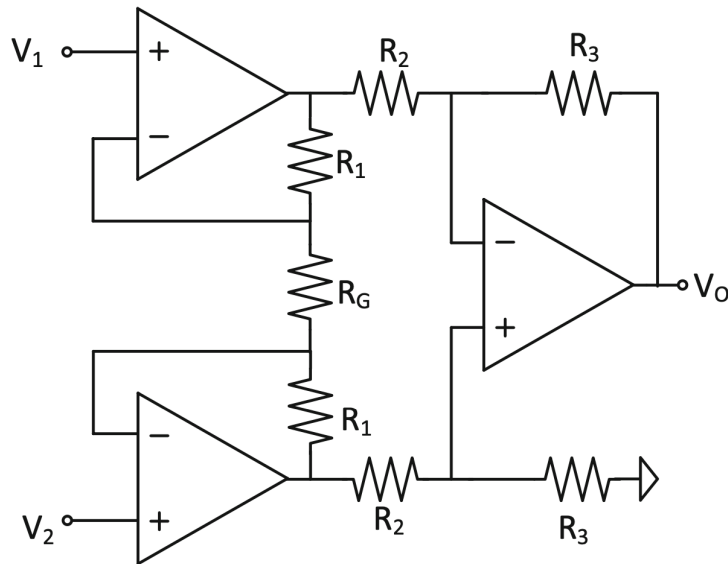
Differential Amplifier



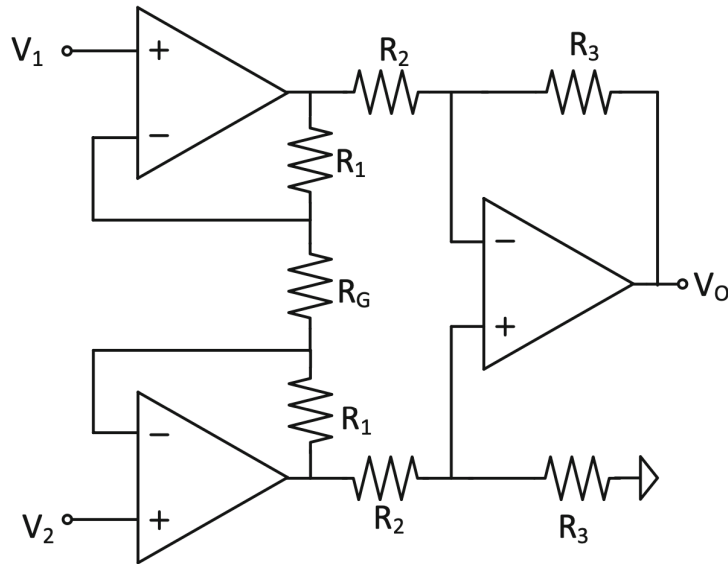
Instrumentation Amplifier (3 Op-amp Circuit)



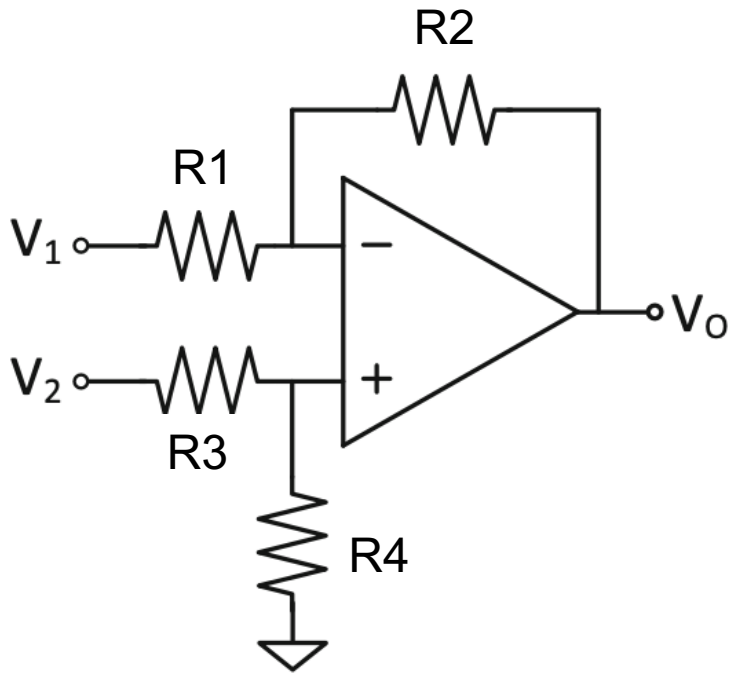
Instrumentation Amplifier (3 Op-amp Circuit)



Instrumentation Amplifier (3 Op-amp Circuit)



... with Resistor Mismatches

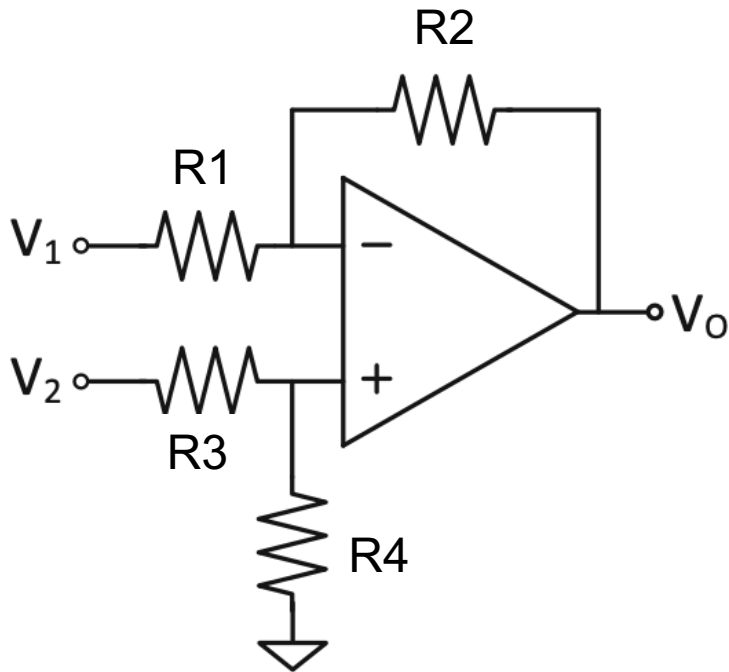


Let's assume resistors have 1% mismatch

$R1 = 10.1\text{k}\Omega$, $R3 = 9.9\text{k}\Omega$

$R2 = 0.99\text{M}\Omega$, $R4 = 1.01\text{M}\Omega$

... with Resistor Mismatches

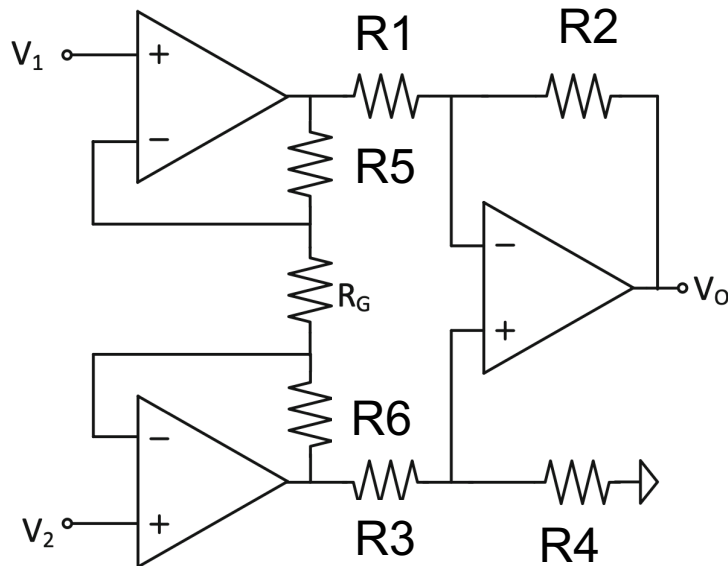


Let's assume resistors have 1% mismatch

$R1 = 10.1\text{k}\Omega$, $R3 = 9.9\text{k}\Omega$

$R2 = 0.99\text{M}\Omega$, $R4 = 1.01\text{M}\Omega$

... with Resistor Mismatches



Let's assume resistors have 1% mismatch

$R1 = 10.1\text{kohm}$, $R3 = 9.9\text{kohm}$

$R2 = 0.99\text{Mohm}$, $R4 = 1.01\text{Mohm}$

$R5 = 505\text{kohm}$, $R6 = 495\text{kohm}$

$R_G = 10\text{kohm}$



ADS1299, ADS1299-4, ADS1299-6

SBAS499C – JULY 2012 – REVISED JANUARY 2017

ADS1299-x Low-Noise, 4-, 6-, 8-Channel, 24-Bit, Analog-to-Digital Converter for EEG and Biopotential Measurements

1 Features

- Up to Eight Low-Noise PGAs and Eight High-Resolution Simultaneous-Sampling ADCs
- Input-Referred Noise: $1 \mu\text{V}_{\text{PP}}$ (70-Hz BW)
- Input Bias Current: 300 pA
- Data Rate: 250 SPS to 16 kSPS
- CMRR: -110 dB

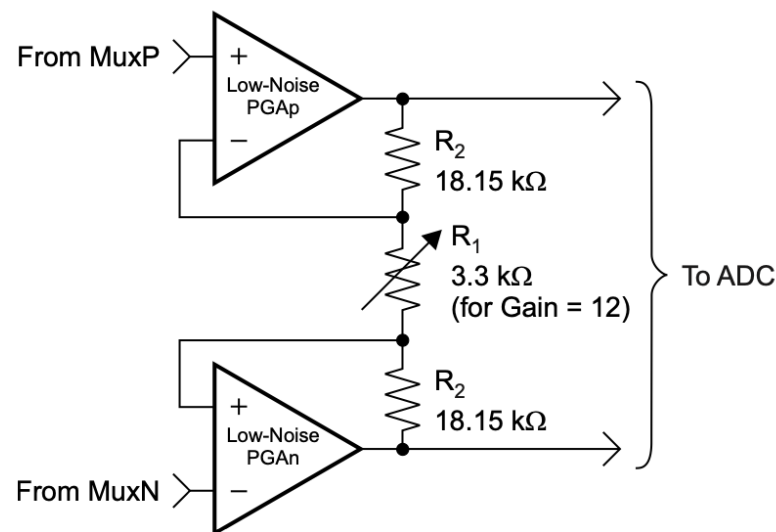
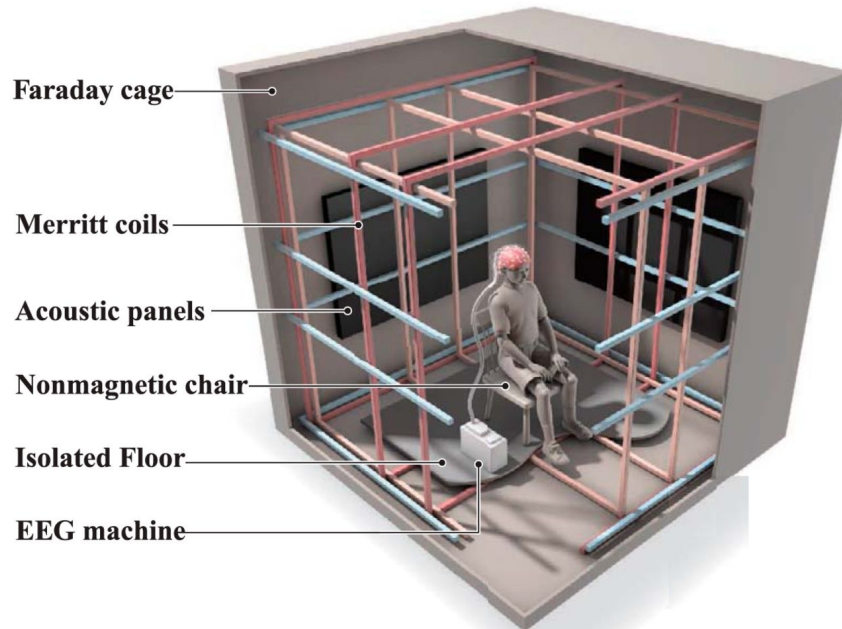


Figure 23. PGA Implementation

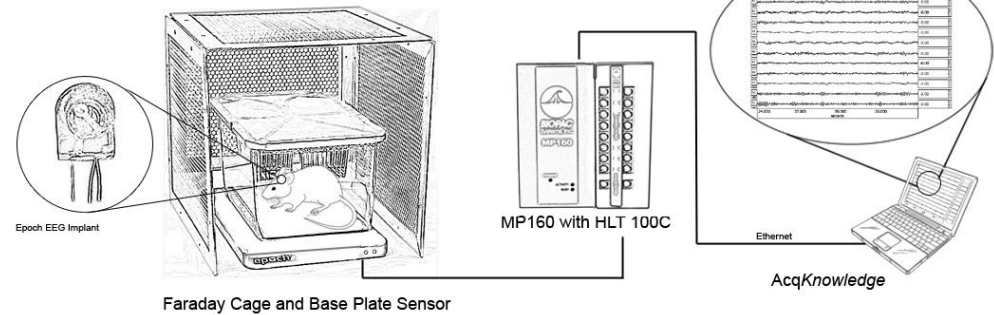
Faraday Cabin



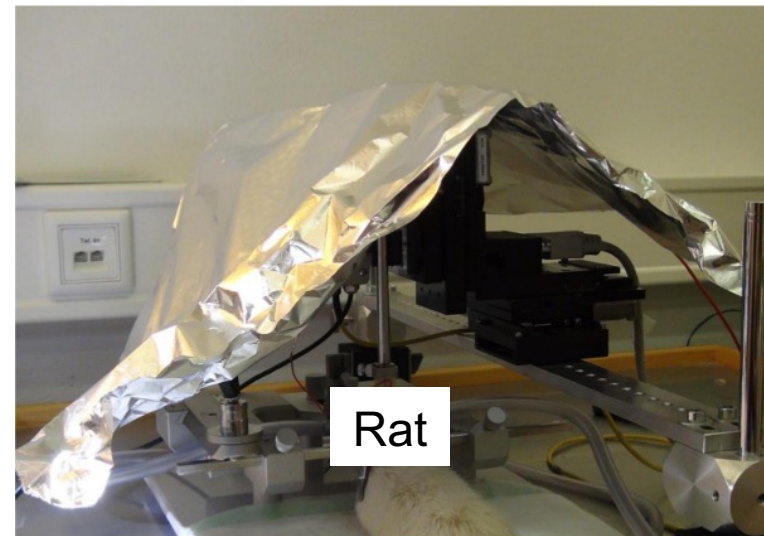
Faraday Cabin for Animal Studies



Sample System Overview
Epoch Animal EEG



or home-made...



Noise and Interference

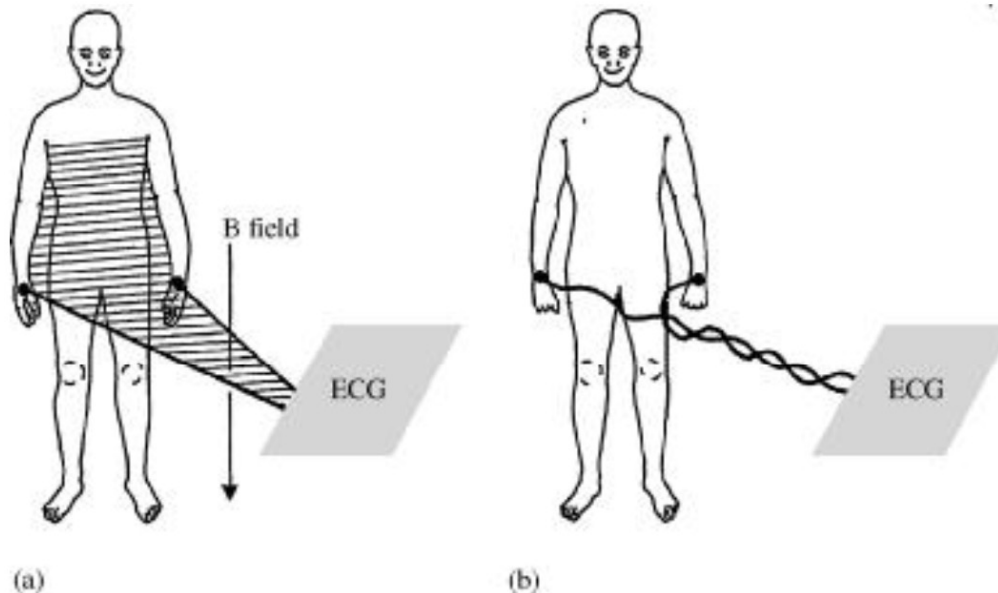
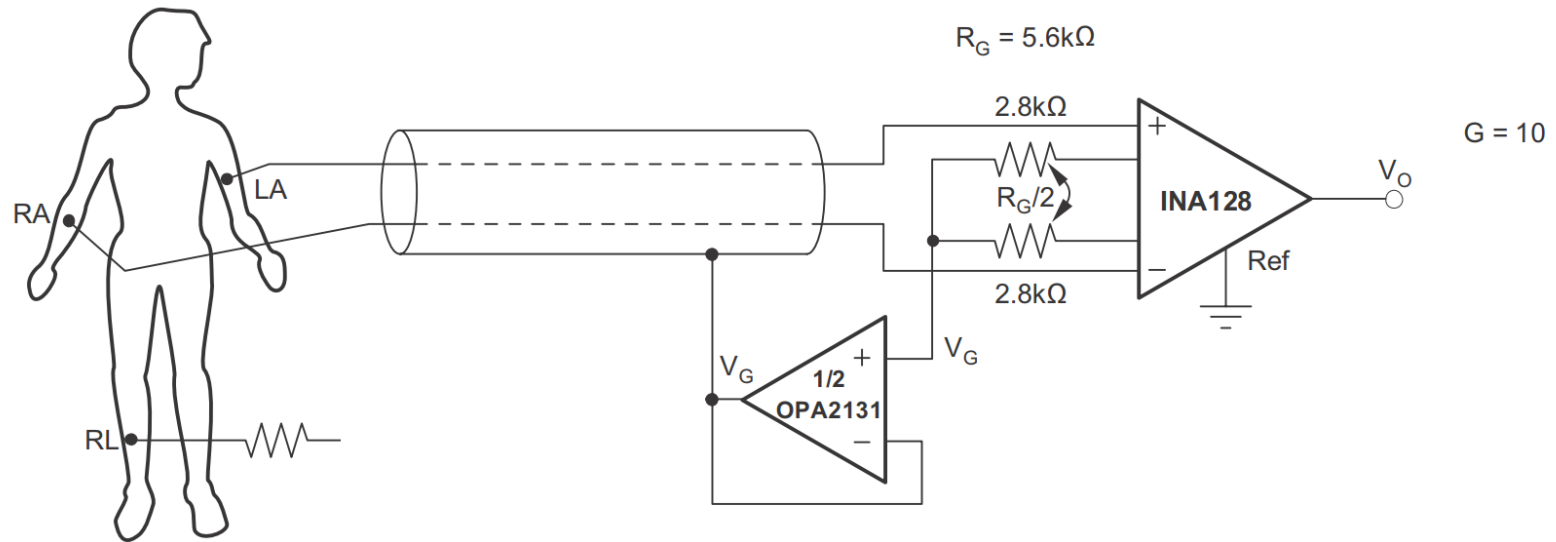


Figure 6.12 Magnetic-field pickup by the electrocardiograph (a) Lead wires for lead I make a closed loop (shaded area) when patient and electrocardiograph are considered in the circuit. The change in magnetic field passing through this area induces a current in the loop. (b) This effect can be minimized by twisting the lead wires together and keeping them close to the body in order to subtend a much smaller area.

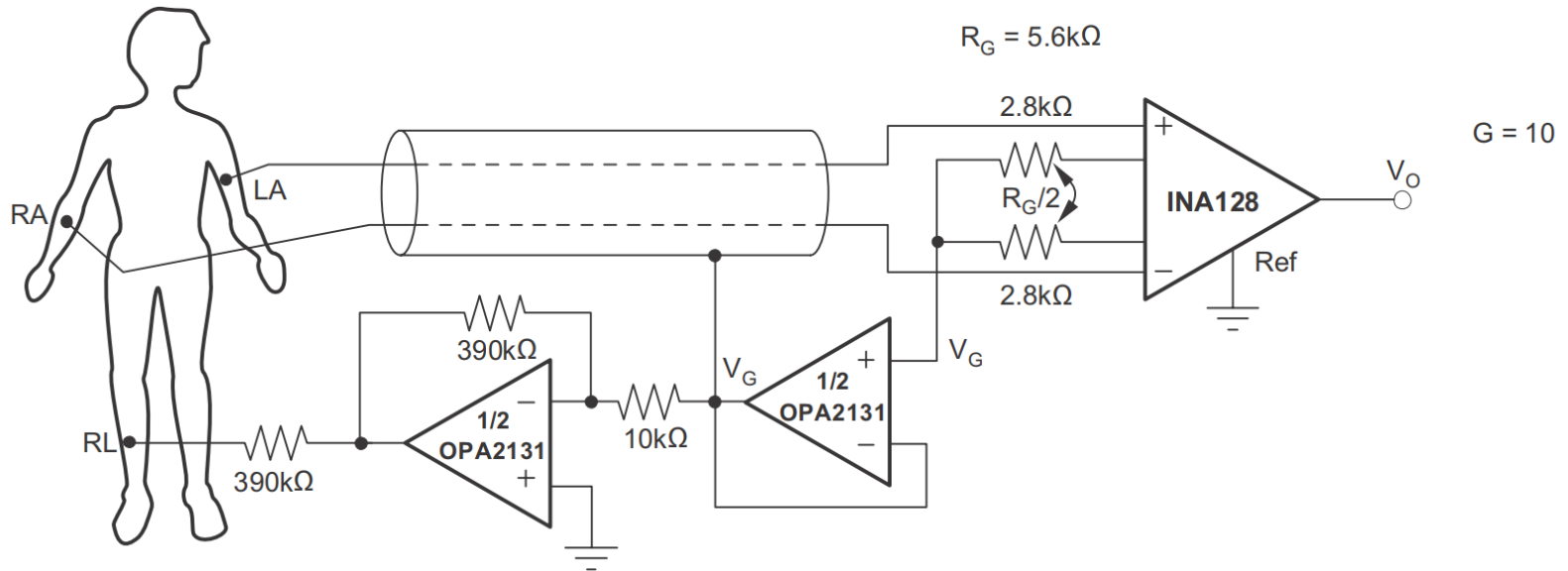
PCB routing for differential signal



Active Shielding



Active Shielding with DRL



Summary

- Neural recording is challenging because:
 - Signals are weak
 - Electrodes have high and complex impedance
 - Strong interference and noise in the environment
 - Non-idealities in amplifiers
- Challenges that we didn't discuss:
 - Channel scaling (there are sooooo many neurons...)
 - Noises and power of electronics, heating
 - Electrode drifting, degradation, foreign body rejection
 - etc.