1. Registration

Rigid registration function from SimpleITK

```
imtype=16,
p12=None,
rescale_intensity=True,
centre_tfm_model='geometry',
tfm_type = 'rigid',
metric='Matte',
metric_numberOfHistogramBins=16,
sampling_intensity_method='random',
smooth_displacement_field = True,
MetricSamplingPercentage=0.1,
shrink_factors = [1],
smoothing_sigmas = [0],
optimizer='gradient',
optimizer_params=None,
eps=1e-12):
        import SimpleITK as sitk
        def imadjust(vol, p1, p2):
   import numpy as np
                      om skimage.exposure import rescale_intensity
                # this is based on contrast stretching and is used by many of the biological image processing algorithms.
p1_, p2_ = np.percentile(vol, (p1,p2))
vol_rescale = rescale_intensity(vol, in_range=(p1_,p2_))
return vol_rescale
                 return vol_rescale
         import numpy as np
        if p12 is None:
    im1_ = vol1.copy()
    im2_ = vol2.copy()
                # no contrast stretching
if rescale_intensity == False:
   im1_ = im1_ / (2**imtype - 1)
   im2_ = im2_ / (2**imtype - 1)
                         im1_ = (im1_ - im1_.min()) / (im1_.max() - im1_.min() + eps)
im2_ = (im2_ - im2_.min()) / (im2_.max() - im2_.min() + eps)
                im1_ = imadjust(vol1, p12[0], p12[1])
im2_ = imadjust(vol2, p12[0], p12[1])
                 if rescale_intensity == False:
    im1_ = im1_ / (2**imtype - 1)
    im2_ = im2_ / (2**imtype - 1)
                         im1_ = (im1_ - im1_.min()) / (im1_.max() - im1_.min() + eps)
im2_ = (im2_ - im2_.min()) / (im2_.max() - im2_.min() + eps)
        v1 = sitk.GetImageFromArray(im1_, isVector=False)
v2 = sitk.GetImageFromArray(im2_, isVector=False)
        if centre_tfm_model=='geometry':
    translation_mode = sitk.CenteredTransformInitializerFilter.GEOMETRY
if centre_tfm_model=='moments':
    translation_mode = sitk.CenteredTransformInitializerFilter.MOMENTS
```

```
transform_mode = sitk.TranslationTransform(3)
these are the built in transforms without additional modification.
tfm_type == 'rigid':
      transform_mode = sitk.Euler3DTransform()
tfm_type == 'iso_similarity':
    tfm_type
   transform_mode = sitk.Similarity3DTransform()
tfm_type == 'aniso_similarity':
      trm_type == 'aniso_similarity':
transform_mode = sitk.ScaleVersor3DTransform() # this version allows anisotropic scaling
tfm_type == 'affine':
# transform_mode = sitk.AffineTransform(3) # this is a generic that requires setting.
transform_mode = sitk.ScaleSkewVersor3DTransform() # this is anisotropic + skew
initial_transform = sitk.CenteredTransformInitializer(v1,
                                                                                transform_mode, # this is where we change the transform
translation_mode)
registration_method = sitk.ImageRegistrationMethod()
registration\_method. Set \texttt{MetricASM} attes \texttt{MutualInformation} (\textit{numberOfHistogramBins} = \texttt{metric\_numberOfHistogramBins})
# key for making it fast. (subsampling, don't use all the pixels)
if sampling_intensity_method == 'random':
    registration_method.SetMetricSamplingStrategy(registration_method.RANDOM)
registration_method.SetMetricSamplingPercentage(MetricSamplingPercentage)
registration_method.SetInterpolator(sitk.sitkLinear) # use this to help resampling the intensity at each iteration.
    Optimizer settings. # put
optimizer == 'gradient':
      registration_method.SetOptimizerScalesFromIndexShift()
registration_method.SetShrinkFactorsPerLevel(shrinkFactors = shrink_factors) # use just the one scale.
registration_method.SetSmoothingSigmasPerLevel(smoothingSigmas=smoothing_sigmas) # don't filter.
registration_method.SetInitialTransform(initial_transform, inplace=False)
```

return tfm

```
ii in tqdm(np.arange(len(imfiles)-1)[:]):
 if ii == 0:
   imfile1 = imfiles[ii]
         im1 = skio.im1eao(im1rle), multivire=raise) # multivire is required to prevent loading of all associated fi
im1 = im1[x1:x2,y1:y2,z1:z2].copy()
im1 = np.uint16(ndimage.zoom( im1, [z_scale, 1, 1], order=1, mode='reflect')) # pad the image symmetrically.
         savefile = os.path.join(saveoutfolder, 'rigid_'+os.path.split(imfiles[ii])[-1])
skio.imsave(savefile, np.uint16(im1))
         print(ii, ii//n_ref*n_ref)
         # read the registered.

file_ind_ii = ii//n_ref*n_ref
im1 = read_tiff(os.path.join(saveoutfolder, 'rigid_'+os.path.split(imfiles[file_ind_ii])[-1])) # reinitialise from the already registered.
 im1_raw = im1.copy() # visualisation only.
imfile2 = imfiles[ii+1]
# im2 = skio.imread(imfile2, multifile=False) # multifile is required to prevent loading of all associated files.
# im2 = skid.imread.imrire, motterferance,
im2 = read_tiff(imfile2)
im2 = im2[x1:x2,y1:y2,z1:z2].copy()
im2 = np.uint16(ndimage.zoom( im2, [z_scale, 1, 1], order=1, mode='reflect'))
im2_raw = im2.copy() # make a copy for transformation later.
 # replace all 0 intensity pixels by the average of the volume.
im1[im1 == 0] = np.nanmean(im1)
im2[im2 == 0] = np.nanmean(im2)
 rigid_optimizer_params = params.gradient_descent_affine_reg()
rigid_tfm = registration.SITK_multiscale_affine_registration(im1,
im2,
                                                                                                                                 im2,
imtype=16,
pnl2=(2,99.8), # percentage scaling to enhance contrast.
rescale_intensity=True,
centre_tfm_model='geometry',
tfm_type = 'rigid', # how to do affine?
metric='Matte',
metric_numberOfHistogramBins=16,
sampling_intensity_method='random',
smooth_displacement_field = True, # remove this.
MetricSamplingPercentage=0.1,
shrink_factors = [1],
smoothing_sigmas = [0],
optimizer='gradient',
optimizer_params=rigid_optimizer_params,
eps=1e-12)
 # save this transform
savetformfile = os.path.join(saveoutfolder, 'Euler3D_'*os.path.split(imfiles[ii+1])[-1].replace('.tif', '.tfm'))
sitk.WriteTransform(rigid_tfm, savetformfile)
# apply the transform to im2
im2_tfm = registration.transform_img_sitk(im2_raw, rigid_tfm) # apply to image 2.
savefile = os.path.join(saveoutfolder, 'rigid_'-os.path.split(imfiles[ii+1])[-1])
skio.imsave(savefile, np.uint16(im2_tfm)) # save the transformed.
```

Non-rigid demons registration function modified from SimpleITK

```
imtype=16,
p12=None,
rescale_intensity=True,
centre_tfm_model='geometry',
demons_type='diffeomorphic',
n_iters = 25,
smooth_displacement_field = True,
smooth_alpha=.8,
shrink_factors = [2.,1.],
smoothing_sigmas = [1.,1.],
ens=1e-12.
                                                                            eps=1e-12,
multiscale_iters=None,
intensity_diff_thresh=None):
        import SimpleITK as sitk
        def imadjust(vol, p1, p2):
               pl_s pased on contrast stretching and is used by many of the biological image processing algorithms.

pl_s p2_ = np.percentile(vol, (p1,p2))

vol_rescale = rescale_intensity(vol, in_range=(p1_,p2_))

return vol_rescale
        import numpy as np
        if p12 is None:
    im1_ = vol1.copy()
    im2_ = vol2.copy()
                if rescale_intensity == False:
    im1_ = im1_ / (2**imtype - 1)
    im2_ = im2_ / (2**imtype - 1)
                      im1_ = (im1_ - im1_.min()) / (im1_.max() - im1_.min() + eps)
im2_ = (im2_ - im2_.min()) / (im2_.max() - im2_.min() + eps)
               im1_ = imadjust(vol1, p12[0], p12[1])
im2_ = imadjust(vol2, p12[0], p12[1])
               if rescale_intensity == False:
    im1_ = im1_ / (2**imtype - 1)
    im2_ = im2_ / (2**imtype - 1)
                       im1 = (im1 - im1..min()) / (im1..max() - im1..min() + eps)
im2 = (im2 - im2..min()) / (im2..max() - im2..min() + eps)
       v1 = sitk.GetImageFromArray(im1_, isVector=False)
v2 = sitk.GetImageFromArray(im2_, isVector=False)
       if centre_tfm_model=='geometry':
    translation_mode = sitk.CenteredTransformInitializerFilter.GEOMETRY
if centre_tfm_model=='moments':
    translation_mode = sitk.CenteredTransformInitializerFilter.MOMENTS
        initial_transform = sitk.CenteredTransformInitializer(v1,
                                                                                                              V2,
                                                                                                              sitk.Euler3DTransform(),
                                                                                                              translation_mode)
```

```
def smooth_and_resample(image, shrink_factors, smoothing_sigmas):
        import SimpleITK as sitk
import numpy as np
        if np.isscalar(shrink_factors):
    shrink_factors = [shrink_factors]*image.GetDimension()
if np.isscalar(smoothing_sigmas):
    smoothing_sigmas = [smoothing_sigmas]*image.GetDimension()
        smoothed_image = sitk.SmoothingRecursiveGaussian(image, smoothing_sigmas)
       import SimpleITK as sitk
import numpy as np
        if intensity_diff_threshold is not None:
    registration_algorithm.SetIntensityDifferenceThreshold(intensity_diff_threshold)
       # the generator,
def image_pair_generator(fixed_image, moving_image, shrink_factors, smoothing_sigmas):
    end_level = 0
    start_level = 0
    if shrink_factors is not None:
    end_level = len(shrink_factors)
    for level in range(start_level, end_level):
        f_image = smooth_and_resample(fixed_image, shrink_factors[level], smoothing_sigmas[level])
        m_image = smooth_and_resample(moving_image, shrink_factors[level], smoothing_sigmas[level])
        yield(fixed_image, m_image)
    yield(fixed_image, moving_image)
            if a constraint imposed by near
shrink_factors is not None:
shrink_factors is not None:
original_size = fixed_image.GetSize()
original_size = fixed_image.GetSpacing()
original_spacing = fixed_image.GetSpacing()
original_spacing = fixed_image.GetSpacing()
original_spacing = fixed_image.GetSpacing()
original_size) if np.isscalar(shrink_factors[0]) else shrink_factors[0]

df_size = [int(sz:/float(sf) + 0.5) for sf,sz in zip(s_factors,original_size)]

df_spacing = [((original_sz-1)*original_spc)*(/new_sz-1)
for original_sz, original_spc, new_sz in zip(original_size, original_spacing, df_size)]
               df_size = fixed_image.GetSize()
df_spacing = fixed_image.GetSpacing()
```

```
fixed_image.GetDirection())

else:
    initial_displacement_field = sitk.Image(df_size, sitk.sitkVectorFloat64, fixed_image.GetDimension())
    initial_displacement_field.SetSpacing(df_spacing)
    initial_displacement_field.SetOrigin(fixed_image.GetOrigin())

# Run the registration.
# Start at the top of the pyramid and work our way down.

count = 0

if multiscale_iters is not None:
    multiscale_iters_ = list(multiscale_iters)
    multiscale_iters_.append(0)

for f_image, m_image in image_pair_generator(fixed_image, moving_image, shrink_factors, smoothing_sigmas):
    initial_displacement_field = sitk.Resample (initial_displacement_field, f_image)

if multiscale_iters is not None:
    registration_algorithm.SetNumberOfIterations(multiscale_iters_[count])
    initial_displacement_field = registration_algorithm.Execute(f_image, m_image, initial_displacement_field)
    count+=1

return sitk.DisplacementFieldTransform(initial_displacement_field)
```

The function for warping given a transform (rigid or non-rigid)

```
im_row = ini.copy() * visualisation enly.

infiles = infiles[ini]
inc = seth sensition[ine], multiplies[alse] * multiplies is required to prevent loading of all associated files.

inc = read.tiff(inifiles)
inc = seth sensition[ine], multiplies[alse] * multipli
```

Reconstruction of the vertices from the demons displacement fields for each time point

2. Binary Segmentation and mesh creation

Restoration is skimage.restoration library. Restoration.wiener was extended to allow 3-d deconvolution. PSF was that of meSPIF made available in uShape3D publication.

Modified marching cubes which runs skimage marching cubes after Gaussian smoothing with sigma=1, and then uses pyacvd to remesh equitriangly to 98% of the original vertices

3. Curvature / Intensity measurement

Code for measuring mesh curvature for vertex

```
principal_curvatures = [igl.principal_curvature(vv[...,::-1], f)[:] for vv in v]
# # separate into the directional fields.
principal_curvature_components_vectors = np.array([cc[:2] for cc in principal_curvatures], dtype=np.float32)
principal_curvatures = np.array([cc[:2] for cc in principal_curvatures], dtype=np.float32)
# principal_curvatures_r2 = np.array([igl.principal_curvature(vv[...,::-1], f, radius=2)[2:] for vv in v]) too noisy....
# visualize the curvatures on the surface now in comparison.
prin_kappa_min = (np.max(principal_curvatures, axis=1)) / px_res
prin_kappa_max = np.min(principal_curvatures, axis=1) / px_res
mean_curvatures = .5*(prin_kappa_min+prin_kappa_max)
```

Code for steepest gradient descent into cell i.e. implicit Euler integration

```
def parametrid_mesh_constant_img_flow(mesh, external_img_gradient,
                                                            esh, externat_umg_gradicite,
niters=1,
deltal=5e-4,
step_size=1,
method='implicit',
robust_l=False,
mollify_factor=1e-5,
conformalize=True, gamma=1, alpha=0.2, beta=0.1, eps=1e-12):
               igl
: numpy as np
: scipy.sparse as spsparse
:qdm import tqdm
.Unzipping import unzip_new as uzip
      vol_shape = external_img_gradient.shape[:-1]
v = np.array(mesh.vertices.copy())
f = np.array(mesh.faces.copy())
           import robust_laplacian
L, M = robust_laplacian.mesh_laplacian(np.array(v), np.array(f), mollify_factor=mollify_factor)
L = -L # need to invert sign to be same convention as is!
      if robust L:
            L = igl.cotmatrix(v,f)
      Usteps = np.zeros(np.hstack([v.shape, niters+1]))
Usteps[...,0] = v.copy()
U = v.copy()
      propagation
"""
for ii in tqdm(range(niters)):
           U_prev = U.copy(); # make a copy.
           U_grad = np.array([uzip.map_intensity_interp3(U_prev,
                                                                              grid_shape=vol_shape,
    I_ref=external_img_gradient[...,ch]) for ch in np.arange(v.shape[-1])])
           U_grad = U_grad.T
           if method == 'explicit':
    U_grad = U_grad / (np.linalg.norm(U_grad, axis=-1)[:,None]**2 + eps) # square this.
    U = U_prev + U_grad * step_size #update.
    Usteps[...,ii+1] = U.copy()
           if method == 'implicit':
    U_grad = U_grad / (np.linalg.norm(U_grad, axis=-1)[:,None] + eps)
                  if conformalize:
                                        robust laplacian
                              __, M = robust_laplacian.mesh_laplacian(U_prev, f, mollify_factor=mollify_factor)
                              M = igl.massmatrix(U_prev, f, igl.MASSMATRIX_TYPE_BARYCENTRIC) # -> this is the only matrix that doesn't degenerate.
```

```
# # implicit solve.
S = (M - deltaL*L) # what happens when we invert?
b = M.dot(U_prev + U_grad * step_size)
else:
    # construct the active contour version.
S = gamma * spsparse.eye(len(v),len(v)) - alpha * L + beta * L.dot(L)
b = U_prev + U_grad * step_size

# get the next coordinate by solving
U = spsparse.linalg.spsolve(S,b)
Usteps[...,ii+1] = U.copy()

# return all the intermediate steps.
return Usteps
```

For external edge gradient computation use gradient of signed distance transform

```
def sdf_distance_transform(binary, rev_sign=True, method='edt'):
    import numpy as np

pos_binary = binary.copy()
    neg_binary = np.logical_not(pos_binary)

if method == 'edt':
    from scipy.ndimage import distance_transform_edt
    res = distance_transform_edt(neg_binary) * neg_binary - (distance_transform_edt(pos_binary) - 1) * pos_binary

if method =='fmm':
    import skmm
    res = skmm.distance(neg_binary) * neg_binary - (skmm.distance(pos_binary) - 1) * pos_binary

if rev_sign:
    res = res * -1

return res
```

```
def surf_normal_sdf(binary, return_sdf=True, smooth_gradient)=None, eps=1e-12, norm_vectors=True):
    import numpy as np
    import scipy.ndimage as ndimage

sdf_vol = sdf_distance_transform(binary, rev_sign=True) # so that we have it pointing outwards!.

# compute surface normal of the signed distance function.
sdf_vol_normal = np.array(np.gradient)(sdf_vol))

# smooth gradient) is not None: # smoothing needs to be done before normalization of magnitude.
    sdf_vol_normal = np.array([ndimage.gaussian_filter(sdf, sigma=smooth_gradient)) for sdf in sdf_vol_normal])

if norm_vectors:
    sdf_vol_normal = sdf_vol_normal / (np.linalg.norm(sdf_vol_normal, axis=0)[None,:]+eps)

return sdf_vol_normal, sdf_vol
```

Intensity measurement (actual computation of raw intensity values)

Binary voxelisation of the mesh into a binary and then taking the mean for the volumetric intensity for normalization.

```
volume_intensity_all.append(np.nanmean(rigid_im[vv_vol_binary>0])) # important for normalization!.
```

Setting the 1um distance

```
sample_radius = 1.
# get the barycenter and construct a circle.
sphere_radius = sample_radius/pix_res # 1 um radius as using the same mesh.

def percentile_mean( vals, percent=90) :
    thresh = np.percentile(vals, percent)
    return np.nanmean(vals[vals>=thresh])
```

```
beta=0.1,
eps=1e-12)
 ##### then we simply use this to look up in the image....
##### accumulate the distance along the trajectory and derive a mask to avoid taking deeper than a threshold....
 v_depth_I = uzip.map_intensity_interp3(v_depth.transpose(0,2,1).reshape(-1,3),
                                                                rigid_im.shape,
 I_ref=rigid_im)
v_depth_I = v_depth_I.reshape(-1,v_depth.shape[-1])
\label{eq:depth0} \begin{array}{l} \mbox{dist}\_v\_depth0 = np.linalg.norm(v\_depth - v\_depth[...,0][...,None], \ axis=1) \\ \mbox{valid}\_I = \mbox{dist}\_v\_depth0 \leftarrow sphere\_radius \\ \mbox{v\_depth}\_I[ \ valid\_I == 0 \ ] = np.nan \ \# \ replace \ with nans \\ \end{array}
 inmesh_face_pts_I_mean_ = []
 immesh_face_pts_I_mean_ = []
for sig in v_depth_I:
    thresh = np.percentile( sig[~np.isnan(sig)], 95)
    inmesh_face_pts_I_mean_.append(np.nanmean(sig[sig>thresh]))
inmesh_face_pts_I_mean = np.hstack(inmesh_face_pts_I_mean_)
 immesn_race_pts_I_mean = np.hstack([np.nanmean(xyz_I[ind_ii]) for ind_ii in ind]) # get the mean intensity
inmesh_face_pts_I_mean[np.isnan(inmesh_face_pts_I_mean)] = 0
septin_all_depth1.append(inmesh_face_pts_I_mean)
       I_min_depth1 = np.percentile(inmesh_face_pts_I_mean, 1)
I_max_depth1 = np.percentile(inmesh_face_pts_I_mean, 99)
 # apply coloring percentile? # this is fluctuating a lot?
intensity_colors = vol_colors.get_colors(inmesh_face_pts_I_mean,
                                                          colormap=cm.RdYlBu_r,
vmin=I_min_depth1,
vmax=I_max_depth1) # was 275,400 for 180522, Cell5
# vmin=np.percentile(inmesh_face_pts_I_mean,0), # set this to be absolute scale.
# vmax=np.percentile(inmesh_face_pts_I_mean,99))
```

Actual sampling for a single timepoint.

4. Bleach correction

```
# correct and express as a relative series.
septin_faces_all_correct = septin_faces_all/(septin_vol_intensity_all[:,None] + 1e-12) # to prevent 0 division.
```

5. Spatial mesh smoothing of timeseries

```
def smooth scalar function mesh (mesh, scalar fn, exact False, n_iters 10, weights None, return_weights True, alpha-0):

...

if exact we use it 10 else we use the cotangent laplacian which is super fast with no inversion required.

allow optional usage of weights.

import ig:
import time
import numpy as np
import scalar fn.copy()

scalars = scalar fn.copy()

if exact:

if exact:

if weights is None:

stitution()

weights = spanse.linalg.spolve(N, L) = m inv l = this inversion is alow. the results for me is very similar. but much slower!

stitution in np.arange(n_iters):

scalars = next = (np.squeeze((np.abs(weights)).dot(scalars)) / (np.abs(weights).sum(axis-1)))

scalars = next = (np.squeeze((np.abs(weights)).dot(scalars)) / (np.abs(weights).sum(axis-1)))

scalars = next = (np.squeeze((np.abs(weights)).dot(scalars)) / (np.abs(weights).sum(axis-1)))

scalars = next = np.array(scalars = next.-copy()

scalars = next = np.array(scalars = next.-copy()

scalars = next = np.array(scalars)

scalars = next = np.array(scalars)
```

6. Autocorrelation determination

```
autocorr_kappa = tsa.autocorr_timeseries_set_id(curvature_faces_sll_um_mesh[:,include_vertex].T, norm=True, eps=te-12)
autocorr_kappa = tsa.autocorr_timeseries_set_id(septin_vertex_all[:,include_vertex].T, norm=True, eps=te-12)
autocorr_septin = tsa.autocorr_kappa = np.namena(autocorr_kappa, ords=0)
set_id_ble_autocorr_kappa = np.namena(autocorr_kappa, ords=0)
set_id_ble_autocorr_septin = np.namena(autocorr_septin, oxds=0)
set_id_ble_autocorr_septin = find_peaks(mean_bleb_autocorr_septin, prominence=0.0001, height=0, distance=5) ** must have height 0
** peaks_mean_bleb_autocorr_septin = find_peaks(mean_bleb_autocorr_septin, prominence=0.0001, height=0, distance=5) ** peaks_mean_bleb_autocorr_septin = find_peaks(mean_bleb_autocorr_septin, height=0, distance=5) **
**peaks_mean_bleb_autocorr_kappa = find_peaks(mean_bleb_autocorr_septin, distance=5) ** must have height 0
**peaks_mean_bleb_autocorr_septin = find_peaks(mean_bleb_autocorr_septin, distance=5) **
**peaks_mean_bleb_autocorr_septin = find_peaks(mean_bleb_autocorr_septin, distance=5) **
**peaks_mean_bleb_autocorr_kappa, idbet=r*is\kappa [1/um]*)
**plit.figure()
```

7. Spatial correlation determination

Utility functions:

Converting vertex timeseries to face timeseries (igl.average_onto_faces)