jaxFlowSim

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Introduction

What is jaxFlowSim?

- 1D-haemodynamics solver
- written in JAX
- differentiable

Motivation

Use and Novelty

- towards personalised medicine
- parameter inference
- sensitivity analysis

$$\frac{\partial \mathbf{U}}{\partial t} + \frac{\partial \mathbf{F}(\mathbf{U})}{\partial z} = \mathbf{S}(\mathbf{U}), \ t > 0, \ z \in [0, l],
\mathbf{U}(z; 0) = \mathbf{U}_0(z), \ z \in [0, l],
\mathbf{U}(0; t) = \mathbf{U}_L(t), \ t > 0,
\mathbf{U}(l; t) = \mathbf{U}_R(t), \ t > 0,$$
(1)

$$\mathbf{U} := \begin{bmatrix} A \\ Q \end{bmatrix}, \ \mathbf{F}(\mathbf{U}) := \begin{bmatrix} Q \\ \frac{Q^2}{A} + \frac{\beta A^{\frac{3}{2}}}{3\rho\sqrt{A_0}} \end{bmatrix}, \ \mathbf{S}(\mathbf{U}) := \begin{bmatrix} 0 \\ -22\frac{\mu}{\rho}\frac{Q}{A} \end{bmatrix}. \quad (2)$$

 $\mathbf{U}_0 \triangleq$ initial condition, $\mathbf{U}_1 \triangleq$ left boundary values, $\mathbf{U}_0 \triangleq$ right boundary values, $A \triangleq$ cross-section, $A_0 \triangleq$ reference cross-section, $Q \triangleq$ volumetric flow-rate, $\beta \triangleq$ elasticity coefficient, $\rho \triangleq$ blood density, $\mu \triangleq$ blood dynamic viscosity.

$$P(z;t) := P_{\text{ext}}(z;t) + \beta \left(\sqrt{\frac{A(z;t)}{A_0(z)}} - 1 \right), \tag{3}$$

$$\beta(z) := \frac{\sqrt{\pi} E h_0(z)}{(1 - \nu^2) \sqrt{A_0(z)}}.$$
 (4)

 $P \hat{=}$ pressure, $P_{ext} \hat{=}$ external pressure,

 $E = \text{Young's modulus}, h_0 = \text{reference vessel wall thickness}, \nu = \text{Poisson's ratio (elasticity parameter)}.$

Initial Conditions

$$u(z;0) \equiv 0,$$
 $z \in [0, I],$ (5)
 $A(z;0) = A_0(z),$ $z \in [0, I],$ (6)
 $Q(z;0) = u(z;0)A(z;0) \equiv 0,$ $z \in [0, I].$ (7)

Inlets, Juntions, Outlets

Inlets

set P from data \rightarrow set u, Q, A, c through linear extrapolation of charateristics set Q from data \rightarrow set u, A, c, P through linear extrapolation of charateristics

Junctions

solve linear system of equations consisting of:

- conservation of mass,
- conservation of pressure,
- extrapolation of charateristics

Outlets

0D-/ lumped parameter model: three element Windkessel (RCR) model

Numerical Methods

1D-Model

FV method: MUSCL scheme with Lax-Friedrichs Flux

Junctions & Outlets

Newton method

Code Structure

```
def runSimulation(config_filename, J)
         config = loadConfig(config_filename)
         simulation_data = buildArterialNetwork(config)
        P t = [0]
         converged = False
         while not converged:
           P_t_{emp} = P_t
12
             dt = computeDt(simulation_data)
             simulation_data = setBoundaryValues(simulation_data, dt)
14
15
             simulation data = muscl(simulation data, dt)
16
             P t[i.:] = savePressure(simulation data)
             t = t + dt
18
           if i >= J:
19
20
             break
21
           converged = checkConv(P_t, P_t_temp)
```

Listing: dt = timestep(CFL), setBoundaryValues=inlet(from data), outlet(Windkessel), junctions(conservation laws), muscl=Monotonic Upstream-centered Scheme for Conservation Laws(Finite Volume)

Padding

without padding

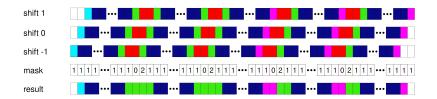


with padding



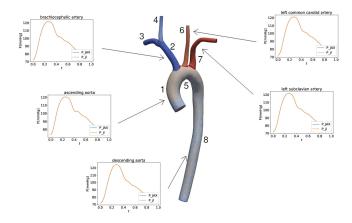


Masking

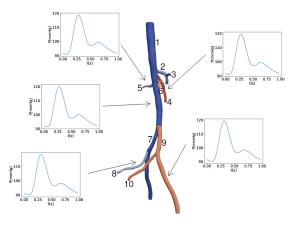




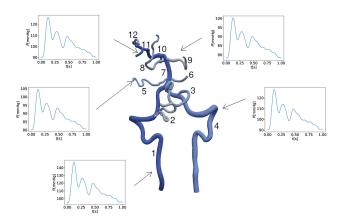
Model: Aorta (0007_H_AO_H)



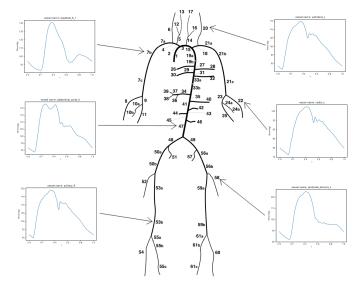
Model: Abdominal Arteries (0029_H_ABAO_H)



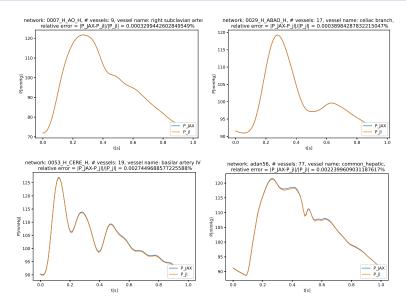
Model: Cerebellar Arteries (0053_H_CERE_H)



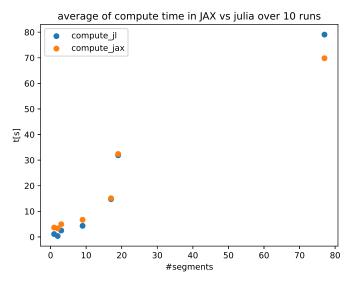
Model: ADAN56



Validation



Comparison



Inference

Demo

inferring an outlet resistance parameter from precomputed data

Future Work

Main Points of Interest

- improving performance (GPU optimization)
- fine tuning parameter inference
- sensitivity analysis

Questions?

Thank you for your attention!