

We want to solve the optimal control problem given by

$$\min J(v, p, u) = \frac{1}{2} \int_{\Gamma_{obs}} |v - v_d|^2 ds + \frac{\alpha_1}{2} \int_{\Gamma_C} |\nabla_t u|^2 ds + \frac{\alpha_2}{2} \int_{\Gamma_C} |u|^2 ds$$

s.t.

$$\begin{cases} -\nu \Delta v + \nabla p = f & \text{in } \Omega \\ \operatorname{div} v = 0 & \text{in } \Omega \\ v = g & \text{on } \Gamma_{in} \\ v = 0 & \text{on } \Gamma_w \\ pn - \nu \partial_n v = u & \text{on } \Gamma_C \end{cases} \quad (1)$$

We want to solve this configuration by considering a 2D realistic representation of an arterial bifurcation, parametrized as shown in Fig. 1. We consider an inverse problem in hemodynamics, focusing on a simplified model of an arterial bifurcation. The computational domain is parametrized, with an inflow boundary denoted as  $\Gamma_{in}$ , two outflow boundaries  $\Gamma_C$ , and the physical vessel wall represented by  $\Gamma_D$ . The primary variables of interest are the velocity  $\vec{v}$  and pressure  $p$ , which are assumed to satisfy (1).

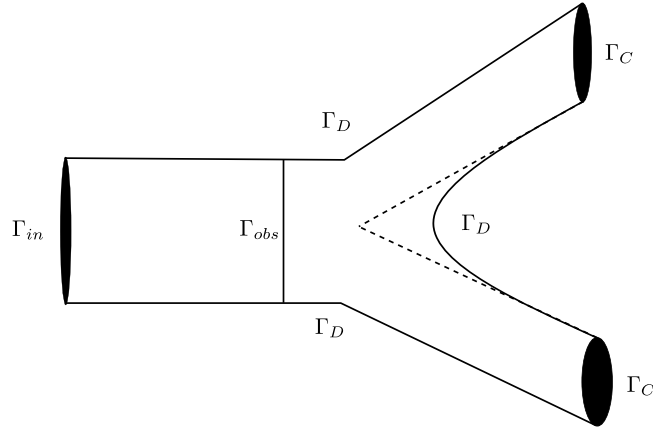


Figure 1: 2D representation of the arterial bifurcation considered for this implementation.

We assume that the velocity profile is known along a segment of the inflow boundary  $\Gamma_{in}$ , but no direct measurements of the Neumann flux at the outflow boundaries  $\Gamma_C$  are available. The control variable in this problem is the unknown Neumann flux at  $\Gamma_C$ . The goal is to deduce this control variable using the velocity data along  $\Gamma_{in}$ , and consequently, to recover the velocity and pressure fields across the entire domain.

The problem involves several parameters, including geometric parameters  $\mu_{geom}$ , which describe the dimensions of the bifurcation (e.g., the length of each branch, the angle of the bifurcation), a parametrized velocity profile  $\mu_{meas}$ , and a parametrized inflow velocity profile  $g(\mu_{in})$ . These parameters together influence the flow field that we aim to reconstruct. This formulation represents a simplified version of the more complex hemodynamic flow problem, assuming two-dimensional geometry, steady-state conditions, and simplified constitutive laws. We further assume that the measured velocity profile can be approximated by a simple analytical function, parametrized for the data assimilation process.