

ENHANCING SEIZURE DETECTION USING DEEP LEARNING

A PROJECT REPORT

Submitted by

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BONAFIDE CERTIFICATE

Certified that this project report “ENHANCING SEIZURE DETECTION USING DEEP LEARNING” is the bonafide work of “Dipin Raj, Rashaz Rafeequ, Jeevan A.J, Akshay S, Rhishitha T.S” who carried out the project work under our supervisor ‘Ms. Merry K P’.

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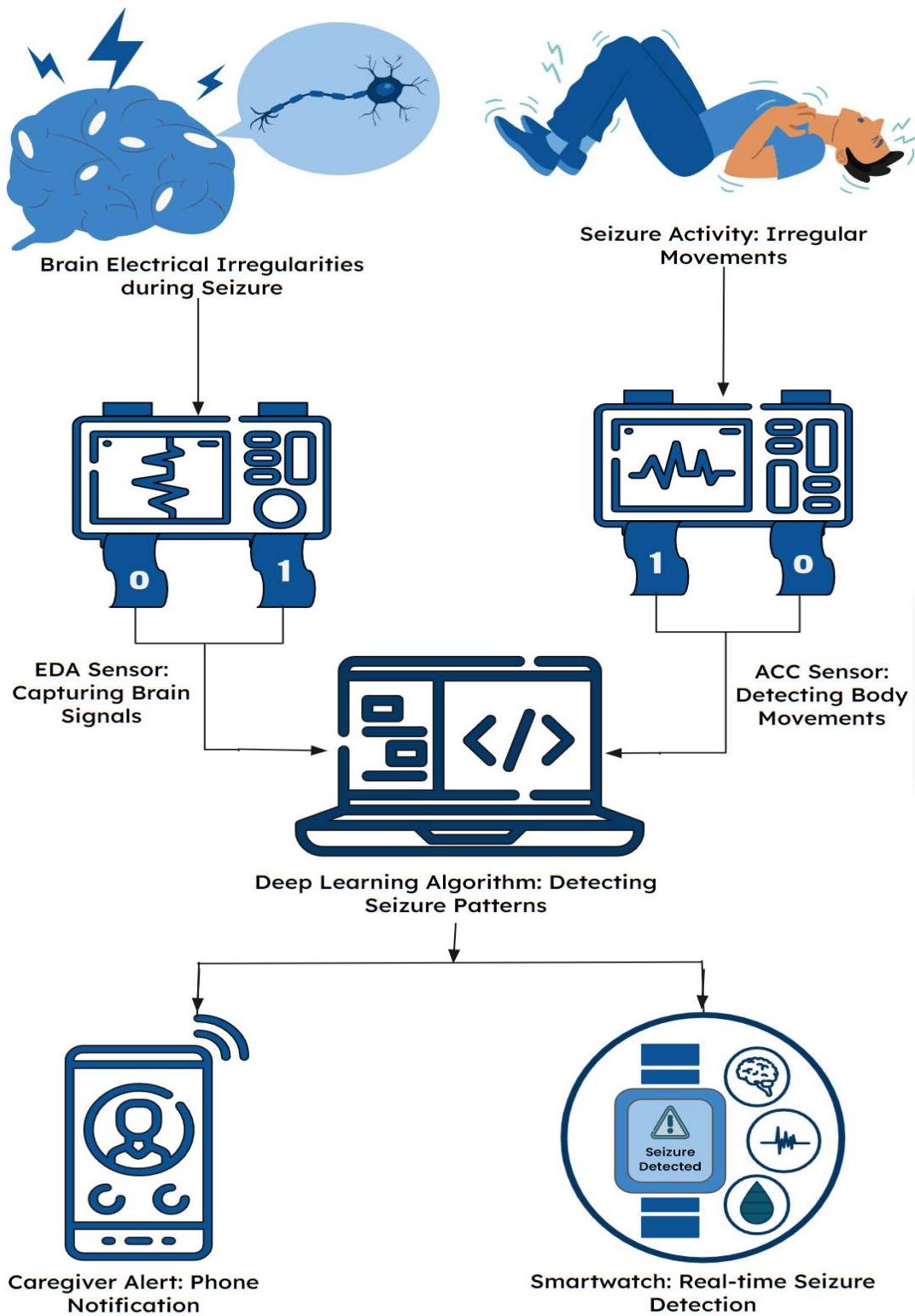
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ABSTRACT

Epilepsy presents significant risks, including Sudden Unexpected Death in Epilepsy (SUDEP), making reliable seizure detection critical. Wearable devices capable of automatic seizure identification and prediction could transform the lives of epileptic individuals, potentially reducing SUDEP risk and improving overall health outcomes. Traditional seizure detection methods, reliant on EEG analysis, face limitations due to signal variability and noise. This study explores the application of deep learning, to enhance seizure detection accuracy. The proposed approach integrates multimodal sensors like ACC and EDA, enabling the model to analyze skin conductivity and erratic heartbeats, offering insights into imminent seizures. Utilizing a diverse dataset with seizure and non-seizure recordings, the deep learning models are trained and evaluated based on sensitivity, specificity, and overall accuracy. Preliminary findings exhibit promising advancements in seizure detection accuracy compared to conventional methods. Deep learning's integration into seizure detection systems holds immense potential. Not only can it enhance diagnostic precision, but it also enables real-time monitoring and early intervention in epilepsy management. These advancements have the capacity to significantly impact the lives of individuals with epilepsy by minimizing risks, improving prognosis, and revolutionizing how seizures are managed and addressed.

Keywords—Seizure, Electrodermal Activity (EDA), Accelerometer (ACC), Deep Learning, Wearable Technology, SUDEP.

GRAPHICAL ABSTRACT



ABBREVIATIONS

ABBREVIATION	MEANING
SUDEP	Sudden Unexpected Death in Epilepsy
ACC	Accelerometer
EDA	Electrodermal Activity
HR Sensor	Heart Rate Sensor
BVP	Blood Volume Pulse
EEG	Electroencephalogram
ECG	Electrocardiogram
PCG	Phonocardiography
TEMP	Temperature Sensor
FNN	Feed Forward Neural Network
XGB	XG Boost
GNB	Gaussian Naïve Bayes
MLP	Multi-layer Perceptron
RNN	Recurrent Neural Network
ROC	Receiver Operating Characteristic Curve

CHAPTER – 1

INTRODUCTION

1.1. Problem Identification

Seizure detection using wearable devices represents a significant technological advancement with the potential to transform the management of epilepsy. However, several challenges persist in achieving accurate and timely detection, particularly when integrating deep learning into the system. It is a technology whose purpose is to detect and alert when a person is experiencing a seizure episode. It seeks for easier detection of seizures and prevention of SUDEP with a system that makes use of sensors such as EDA, ACC, HR and BVP. It also makes use of various machine learning and deep learning algorithms to provide the most efficient result.

One primary challenge arises from the variability in seizure manifestations. Seizures can present in diverse ways, making it difficult to design a universally applicable detection algorithm. The variability in seizure types, durations, and intensities necessitates a sophisticated model capable of adapting to these nuanced characteristics. Ambiguity in sensor data further complicates the problem. Wearable devices commonly use sensors such as Electrodermal Activity (EDA) and Accelerometer (ACC) to capture physiological and movement data. Distinguishing normal daily activities, such as exercising or sleeping, from seizure events proves challenging, as both may exhibit similar sensor patterns. Patient-specific variations add to the complexity. Individuals with epilepsy may have unique physiological and behavioral characteristics. Designing a deep learning model that accommodates these individual variations to achieve high sensitivity and specificity across diverse user profiles is a complex problem. Privacy and ethical concerns are important considerations in the deployment of wearable devices for continuous monitoring. Balancing the need for accurate seizure detection with the protection of user privacy and maintaining ethical considerations becomes paramount.

Addressing these challenges requires a multi-faceted approach that involves not only the refinement of sensor technology but also the development of advanced deep learning algorithms tailored for seizure detection. The integration of deep learning should focus on creating models that are not only accurate but also adaptable, patient-specific, and capable of real-time processing to ensure the effectiveness of seizure detection using wearable devices.

1.2. Seizures & its Types

Seizures are neurological events characterized by abnormal electrical activity in the brain, often resulting in a variety of physical and behavioral manifestations. The classification of seizures is crucial for understanding their diverse nature and tailoring appropriate interventions. Seizures are broadly categorized into two main types: focal (partial) seizures and generalized seizures.



Fig 1.1: Seizure

1.2.1. Focal(Partial) Seizures

Focal seizures originate in a specific region of the brain. They are a type of seizure that focuses on one hemisphere of the brain. They can end up affecting different regions of the brain, and the symptoms that occur can vary depending on the location and extent of the seizure. There are mainly two types of seizures:

1.2.1.1. Simple Focal Seizures

These seizures do not impair consciousness on the individuals. The ones who experience simple focal seizures may display unusual sensations, emotions or movement, which is often localized to one part of the body.

1.2.1.2. Complex Focal Seizures

Complex focal seizures, on the other hand, result in altered consciousness or awareness. People undergoing complex focal seizures may exhibit repetitive behaviors, confusion, or engage in semi-purposeful activities without clear awareness of their surroundings.

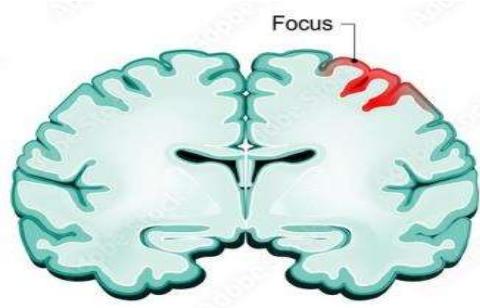


fig 1.2: Focal Seizure

1.2.2. Generalized Seizures

Generalized seizures are a type of seizure in which brain activity happens in both hemispheres of the brain at the same time. Generalized seizures involve abnormal electrical activity throughout the entire brain from the onset and are further categorized into various types.

1.2.2.1. Absence Seizures

Absence seizures are ones that involve a brief loss of consciousness. The loss of consciousness usually lasts for a few seconds. During this, the person might stare blankly without any response to stimuli. It was formerly known as "petit mal" seizures.

1.2.2.2. Tonic-Clonic Seizures

Tonic-clonic seizures involve the loss of consciousness while having convulsive movements and stiffening of the body. These are also known as grand mal seizures. Tonic seizures cause muscle stiffness, typically affecting the muscles of the arms, legs, or back. These seizures can result in a person falling if they occur while standing.

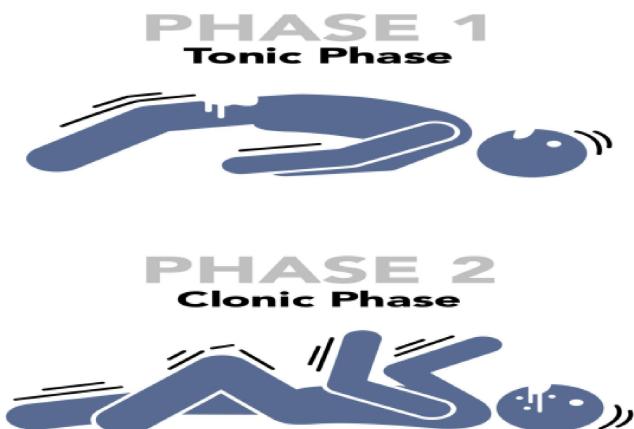


fig 1.3: Tonic-Clonic Seizure

1.2.2.3. Myoclonic Seizures

Myoclonic seizures involve brief, involuntary muscle jerks or twitches. These jerks can affect a specific muscle group or the entire body.



fig 1.4: Myoclonic Seizure

1.2.2.4. Atonic Seizures

Atonic seizures, also known as "drop attacks," lead to a sudden loss of muscle tone. This can result in the person collapsing or falling to the ground.

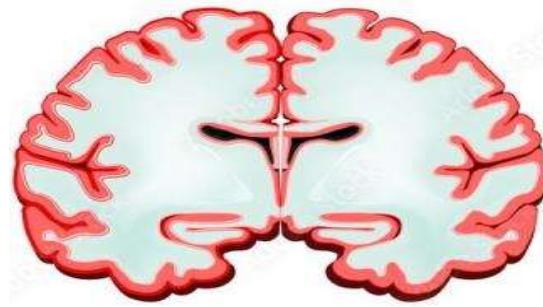


fig 1.5: Atonic Seizure

1.2.2.5. Clonic Seizures

Clonic seizures are characterized by repetitive, rhythmic jerking movements. These movements usually involve both sides of the body.

1.2.2.6. Tonic Seizures

Tonic seizures cause muscle stiffness, typically affecting the muscles of the arms, legs, or back. These seizures can result in a person falling if they occur while standing.



fig 1.6: Tonic Seizure

1.3. Sensors

In order to accurately detect seizures and differentiate between true and false seizures, we require a variety of sensors. These sensors are such as EDA, ACC, HR, BVP, TEMP.

1.3.1. EDA

The skin's electrical conductance, which is mostly determined by sweat gland activity, is measured by the Electrodermal Activity (EDA) sensor, also referred to as a galvanic skin response sensor. EDA is a useful tool for tracking stress levels and emotional arousal since it is sensitive to both physiological and emotional changes. This sensor is frequently utilized in systems like stress management and biofeedback that depend on knowing the user's psychological condition.

1.3.2. ACC

The accelerometer sensor measures movement and orientation changes by detecting changes in acceleration. It is extensively utilized in wearable technology to track steps, measure physical activity, and examine sleep patterns. An accelerometer can record bodily movements in the context of seizure detection, which aids in differentiating between regular everyday activities and atypical motions linked to a seizure episode. This sensor is essential for contextualizing the user's overall physiological status.

1.3.3. HR

The Heart Rate sensor measures the number of heart beats per minute, providing valuable information about cardiovascular health and stress levels. In the context of wearable devices, it plays a key role in fitness monitoring, stress management, and overall health tracking. Monitoring heart rate can be relevant in the context of seizures, as certain types of seizures may lead to changes in heart rate. Integrating a heart rate sensor can contribute to a comprehensive understanding of the physiological responses during a seizure event.

1.3.4. BVP

Changes in blood volume are detected by the Blood Volume Pulse sensor, usually in the skin's microvasculature. The photoplethysmogram (PPG), which depicts the pulsatile blood flow, is typically obtained using it. BVP sensors are frequently used in wearable technology to measure cardiovascular health and monitor heart rate. Changes in blood volume and pulsatile flow may offer more information about the physiological reactions that occur during a seizure episode and enhance the detection system's overall accuracy in the context of seizure detection.

1.3.5. TEMP

A Temperature sensor measures the ambient temperature or, in some cases, the body temperature of the user. In wearable devices, monitoring body temperature can provide insights into various health parameters, including fever or changes in metabolic activity. In the context of seizure detection, abnormal temperature fluctuations may be indicative of a seizure event, especially if it is associated with physiological stress responses. Integrating a temperature sensor adds a valuable dimension to the overall physiological data captured by wearable devices for comprehensive health monitoring.

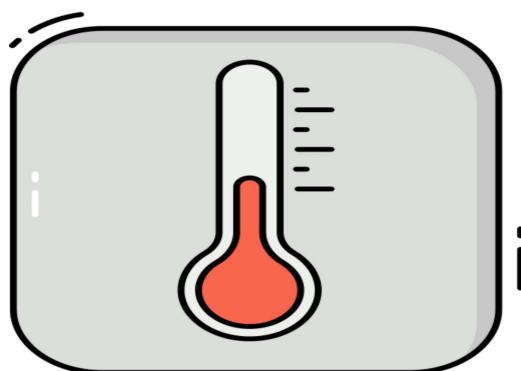


fig 1.7: Temperature Sensor

1.4. Algorithms

1.4.1. Machine Learning Algorithms

1.4.1.1. Logistic Regression

Logistic Regression is a classic machine learning algorithm used for binary and multi-class classification tasks. Despite its name, it is a linear model that estimates the probability of an instance belonging to a particular class. Logistic Regression is widely employed in various fields due to its simplicity and interpretability. It is suitable for situations where a linear decision boundary is sufficient for the given problem.

1.4.1.2. K-Nearest Neighbors (KNN)

K-Nearest Neighbors (KNN) is a simple and effective machine learning algorithm used for classification and regression tasks. It works by assigning a data point the majority class of its k-nearest neighbors in the feature space. KNN is considered a non-parametric and instance-based learning algorithm because it makes predictions based on the local distribution of data points without assuming a specific functional form. It is particularly useful when dealing with datasets with clear clusters or when the decision boundary is nonlinear.

1.4.1.3. XGBoost

XGBoost, short for eXtreme Gradient Boosting, is a machine learning algorithm known for its high performance in supervised learning tasks. It belongs to the family of gradient boosting algorithms and is designed to optimize predictive model performance. XGBoost sequentially adds decision trees to correct the errors of the previous ones, achieving impressive accuracy in tasks like classification and regression. Although XGBoost is not a neural network, it falls under the category of machine learning algorithms.

1.4.1.4. Gaussian Naïve Bayes

Gaussian Naive Bayes is a probabilistic machine learning algorithm based on Bayes' theorem. It assumes that features are conditionally independent given the class label, and it models the distribution of each class using Gaussian (normal) distributions. This algorithm is particularly effective for classification tasks, especially in situations where the feature independence assumption holds.

1.4.1.5. Decision Tree

A Decision Tree is a versatile machine learning algorithm used for both classification and regression tasks. It represents a flowchart-like structure where each internal node represents a decision based on a feature, each branch corresponds to the outcome of that decision, and each leaf node represents the final predicted class or value. Decision Trees are interpretable and can capture complex relationships in the data, making them valuable for various applications.

1.4.1.6. Random Forest

Random Forest is an ensemble learning method that builds multiple decision trees during training and outputs the mode of the classes (classification) or the mean prediction (regression) of the individual trees. It is an extension of the decision tree algorithm, and the "random" aspect comes from training each tree on a random subset of the data and using random subsets of features. Random Forest is known for its robustness and high accuracy, making it a popular choice in machine learning.

1.4.2. Deep Learning Algorithms

1.4.2.1. Feedforward Neural Network (FNN)

A Feedforward Neural Network (FNN) is a fundamental architecture in artificial neural networks, representing a network where information moves in one direction—from the input layer to the output layer. It consists of three main types of layers: the input layer, one or more hidden layers, and the output layer. In the FNN, each layer contains nodes (or neurons), and connections between nodes are associated with weights. The input layer receives the initial data, and through a series of weighted connections and activation functions, information is processed and propagated through the hidden layers to produce an output in the final layer.

1.4.2.2. Multi-Layer Perceptron (MLP)

A Multi-Layer Perceptron (MLP) is a specific type of FNN that comprises multiple layers, including an input layer, one or more hidden layers, and an output layer. Each node in the input layer represents a feature, and connections with adjustable weights transmit information to the hidden layers. The hidden layers contain nodes that use activation functions to process incoming information. The final layer produces the network's output. Training an MLP involves adjusting the weights of connections to minimize the difference between predicted and actual outputs, typically using techniques like backpropagation. MLPs excel in learning complex, nonlinear relationships in data, making them suitable for tasks such as image recognition, natural language processing, and other pattern recognition applications.

1.4.2.3. Recurrent Neural Network (RNN)

Recurrent Neural Network (RNN) is a type of neural network designed for sequence data, where information is retained in the network's memory. Unlike feedforward networks, RNNs have connections that form cycles, allowing them to capture temporal dependencies in data. RNNs are particularly useful in tasks involving sequential information, such as natural language processing and time-series prediction. They have the ability to consider the context of previous inputs, making them well-suited for applications where the order of data is crucial.

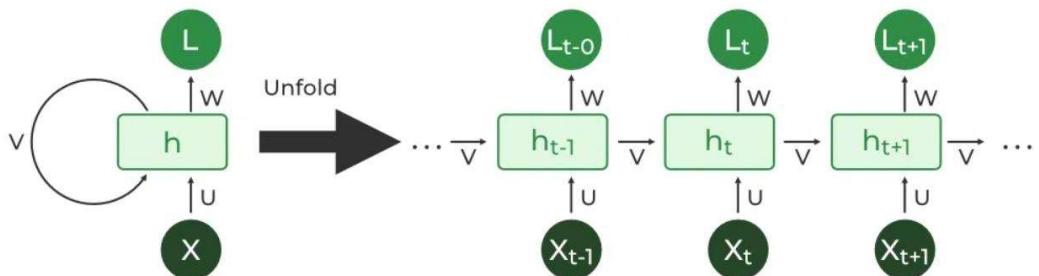


Fig 1.8: RNN Architecture

CHAPTER – 2

LITERATURE REVIEW

- **SEIZURE AND ITS CLASSIFICATIONS:**

Seizure and its classifications are the main topics of the study article. To recognize the physical or chemical characteristics connected to epileptic episodes, sensors are used. Data classification and localization are performed using machine learning classifiers. This theory refers to the categorization of epileptic episodes, according to the new terminology of the International League Against Epilepsy.

- **DEEP LEARNING:**

Deep learning, a powerful facet of machine learning, has been applied to develop an advanced two-channel EEG seizure detection model. The model efficiently identifies seizures in EEG recordings from 590 patients. It addresses data scarcity challenges and accommodates various seizure types using 10-20 electrode array data without spatial information. The study utilizes diverse hospital data, with potential for improvement through additional datasets. The research highlights deep learning's transformative potential in EEG-based seizure detection. CNN and Bi-LSTM models demonstrated the efficiency of deep learning for seizure identification in EEG data (for both epileptic and non-epileptic patients).

- **ELECTROENCEPHALOGRAM (EEG):**

Electroencephalogram (EEG), a key tool in neurology, is vital for diagnosing seizures and neurological issues. The passage highlights the need for accurate epilepsy diagnosis, especially in pediatric patients, and introduces a novel deep-learning method. This method uses a two-dimensional deep convolution autoencoder (2D-DCAE) and a neural network-based classifier to detect seizures in EEG data. The study tested various EEG data segment lengths and employed 10-fold cross-validation, finding that the supervised deep convolutional autoencoder (SDCAE) model outperformed others based on five metrics. This research advances the use of EEG for precise seizure detection, particularly in pediatric cases.

- **ELECTRODERMAL ACTIVITY (EDA):**

The evaluation of changes in skin's electrical conductivity, which can act as a stand-in for both mental and physical states, is referred to by this term. In the framework of the study article, EDA is evaluated during epileptic convulsions to better understand their physiological effects. The experiment was successful in demonstrating that the EDA response increased both during the ictal and postictal phases of the seizure. Focal seizures were found to have a weaker EDA response than other types. Despite the promise of EDA sensors as a seizure detection tool, a number of problems still need to be fixed. EDA sensors, for instance, may be impacted by sweating, movement, and other factors that may affect skin conductance.

- **GENERATIVE ADVERSARIAL NETWORK (GAN):**

Generative Adversarial Networks (GANs) are a breakthrough in deep learning, consisting of two neural networks—the generator and discriminator. GANs have revolutionized various fields by creating highly realistic synthetic data. In the research paper, GANs help address imbalanced EEG data for seizure detection by generating synthetic seizure examples, improving the performance of a one-dimensional Convolutional Neural Network (1DCNN). This highlights GANs' versatility in improving classification, especially in complex medical data analysis.

- **GRAPH GENERATIVE NEURAL NETWORK (GGN):**

In the realm of neurological diagnosis, the study introduces a game-changing tool: the graph-generative neural network (GGN) model. This innovative model is tailored to analyze scalp electroencephalogram (EEG) signals from diverse regions of a patient's scalp, uncovering dynamic brain functional connections. Using a validated dataset of over 3047 epileptic seizure cases, the GGN model has been trained to provide neuroscientists and specialists with a powerful tool for identifying and understanding neurological disorders, particularly epilepsy.

- **AI-BASED TREATMENT PLANS FOR SEIZURES:**

The study article discusses the use of technology for seizure detection and categorization, AI-based treatment plans for seizures, and algorithms. This idea relates to the use of AI technology to the automated diagnosis and prognosis forecasting of specific epilepsy patients. In order to determine the best course of therapy for each patient, the study article explores the use of computer studies that apply AI and ML approaches.

2.1. LITERATURE REVIEW SUMMARY TABLE

Year and Citation	Article/ Author	Tools/ Software	Technique	Source	Evaluation Parameter
Regalia, G., Onorati, F., Lai, M., Caborni, C. and Picard, R.W., 2019. Multimodal wrist-worn devices for seizure detection and advancing research: focus on the Empatica wristbands. Epilepsy research, 153, pp.79-82.	Regalia, Onorati, Lai, Caborni and Picard	Multimodal Sensors (EDA, ACC)	Machine Learning	Science Direct	Furthermore, research is still needed to reduce the FAR and improve the accuracy of seizure detection using multimodal sensors.
Ortega, M.C., Bruno, E. and Richardson, M.P., 2022. Electrodermal activity response during seizures: A systematic review and meta-analysis. Epilepsy & Behaviour, 134, p.108864.	Ortega, M.C., Bruno, E. and Richardson	Electrodermal Activity Sensor	Machine Learning	Science Direct	Further research is indeed needed deep understanding EDA response during epileptic seizures.
Tang, J., El Atrache, R., Yu, S., Asif, U., Jackson, M., Roy, S., Mirmomeni, M., Cantley, S., Sheehan, T., Schubach, S. and Ufongene, C., 2021. Seizure detection using wearable sensors and machine learning: Setting a benchmark. Epilepsia, 62(8), pp.1807-1819.	Tang, J., El Atrache, R., Yu, S., Asif, Jackson, M., and Ufongene	ECG, EDA, PCG	Machine Learning	Epilepsia	The use of ML algorithms and biosensors would be of great help in determining the type of seizure a patient is having.
Zangróniz, R., Martínez Rodrigo, A., Pastor, J.M., López, M.T. and Fernández-Caballero, A., 2017. Electrodermal activity sensor for classification of calm/distress condition. Sensors, 17(10), p.2324.	Zangróniz, R., Martínez-Rodrigo, A., Pastor, J.M., López, M.T. and Fernández-Caballero	ElectrodermalActivity Sensor	Machine Learning	MDPI	The usage of EDA sensors in wearable devices turned out to be of great importance in the health industry, notably in the epilepsy section.

Humairah Tabasum, Nikita Gill, Rahul Mishra and Saifullah Lone. Wearable microfluidic- based eskin sweat sensors – Article.	Humairah Tabasum, Nikita Gill, Rahul Mishra and Saifullah Lone	ElectrodermalActivity Sensor (EDA)	Machine Learning	Royal Society of Chemistry	Developing new cell subtypes, organ-specific microbiomes, biochemical and biophysical gradients across organ & mimicking physiological responses are crucial.
Xu Zeng, Hai-Tao Deng, Dan- Liang Wen, Yao-Yao Li, Li Xu and Xiao-Sheng Zhang. Wearable Multi-Functional Sensing Technology for Healthcare Smart Detection –Article.	Xu Zeng, Hai-Tao Deng, Dan-Liang Wen, Yao-Yao Li, Li Xu and Xiao-Sheng	Accelerometer (ACC)	Machine Learning	MDPI	Wearable sensor has made sprogress but still face challenges such as high integration, fitting human skin, achieving high resolution.
Rosales, M.A., Bandala, A.A., Vicerra, R.R. and Dadios, E.P., 2019, November. Physiological Based Smart Stress Detector using Machine Learning Algorithms. In 2019 IEEE 11 th International Conference on Humanoid, Nanotechnology, Information Technology, Communication and Control, Environment, and Management (HNICEM) (pp. 1-6). IEEE.	Rosales,M.A., Bandala,A.A., Vicerra, R.R. and Dadios	Galvanic Skin Response	Machine Learning, SVM classifiers	IEEE	The GSR sensor can detect changes in sweat gland activity that are reflective of the intensity of the person's emotional state.
Adwitiya, A.Y., Hareva, D.H. and Lazarusli, I.A., 2017, September. Epileptic Alert System on Smartphone. In 2017 International Conference on Soft Computing, Intelligent System and Information Technology (ICSIIT) (pp. 288- 291). IEEE.	Adwitiya,A.Y., Hareva, D.H. and Lazarusli	Accelerometer (ACC)	Fall Detection Algorithm	IEEE	The research consists of negatives such as the placement of smartphones, as it is not convenient to place the device on the upper arm or the head.

Sarmast, S.T., Abdullahi, A.M. and Jahan, N., 2020. Current classification of seizures and epilepsies: scope, limitations and recommendations for future action. <i>Cureus</i> , 12(9).	Sarmast, S.T., Abdullahi, A.M. and Jahan	-	-	Cureus	The classification system can help patients understand their condition and describe their symptoms to healthcare providers very easily which helps in better communication.
Siddiqui, M.K., Morales-Menendez, R., Huang, X. and Hussain, N., 2020. A review of epileptic seizure detection using machine learning classifiers. <i>Brain informatics</i> , 7(1), pp.1-18.	Siddiqui, M.K., Morales-Menendez, R., Huang, X. and Hussain	Electroencephalogram (EEG), Electrocorticography (ECOG)	Machine Learning classifiers Blackbox and non-Blackbox methods	Brain Informatics	Black-box classifiers may achieve high predictive accuracy, but they cannot generate interpretable logicrules. Detecting seizures from large volumes of EEG data is a major challenge in epilepsy diagnosis.
Beniczky, S., Wiebe, S., Jeppesen, J., Tatum, W.O., Brazdil, M., Wang, Y., Herman, S.T. and Ryvlin, P., 2021. Automated seizure detection using wearable devices: A clinical practice guideline of the International League Against Epilepsy and the International Federation of Clinical Neurophysiology. <i>Clinical Neurophysiology</i> , 132(5), pp.1173-1184.	Beniczky, S., Wiebe, S., Jeppesen, J., Tatum, W.O., Brazdil, M., Wang, Y., Herman, S.T. and Ryvlin, P.	-	-	Science Direct	Furthermore, the growth in this research field can result in precise and accurate detection of epileptic seizures, which can effectively support patients with epilepsy.
Chen, F., Chen, I., Zafar, M., Sinha, S.R. and Hu, X., 2022. Seizures detection using multimodal signals: a scoping review. <i>Physiological Measurement</i> .	Chen, F., Chen, I., Zafar, M., Sinha, S.R. and Hu, X.	Multimodal sensors	Machine Learning, SVM Classifiers, Random Forest	PubMed	Furthermore, research is indeed needed to rectify the FAR signals.

Falco-Walter, J.J., Scheffer, I.E. and Fisher, R.S., 2018. The new definition and classification of seizures and epilepsy. <i>Epilepsy research</i> , 139, pp.73-79.	Falco-Walter, J.J., Scheffer, I.E. and Fisher, R.S.	Electroencephalogram (EEG)	Machine Learning	Science Direct	Research in artificial intelligence and machine learning can help improve imaging of EEGs, resulting in better understanding and diagnosis of epileptic seizures.
Posada-Quintero, H.F. and Chon, K.H., 2020. Innovations in electrodermal activity data collection and signal processing: A systematic review. <i>Sensors</i> , 20(2), p.479.	Posada-Quintero, H.F. and Chon, K.H.	Electrodermal activity (EDA)	Machine Learning	ResearchGate	There are tools available for detecting and removing corrupted signals of EDA, but their sensitivity is a factor that needs to be further evaluated.
Van Andel, J., Ungureanu, C., Aarts, R., Leijten, F. and Arends, J., 2015. Using photoplethysmography in heart rate monitoring of patients with epilepsy. <i>Epilepsy & Behavior</i> , 45, pp.142-145.	Van Andel, J., Ungureanu, C., Aarts, R., Leijten, F. and Arends, J.	Photoplethysmography (PPG)	Machine learning	PubMed	In ambulatory heart rate monitoring of patients diagnosed with epilepsy, the heart rate measured with OHR sensor seemed to be equivalent to the heart rate received from automatic ECG analysis.
Mustafa Halimeh, Yonghua Yang, Theodore Sheehan, Solveig Viieluf, Michele Jackson, Tobias Laddenkemper, Christian Meisel. Wearable device assessments of antiseizure medication effects on diurnal patterns of electrodermal activity, heart rate, and heart rate variability - Article preview.	Mustafa Halimeh, Yonghua Yang, Theodore Sheehan, Solveig Viieluf, Michele Jackson, Tobias Laddenkemper, Christian Meisel.	Electrodermal Activity (EDA)	Machine Learning	Science Direct	The multimodal assessment of different data modalities provided by wearable devices may offer a more comprehensive evaluation of antiseizure medications' effects on the ANS, leading to better seizure detection, forecasting, and treatment monitoring in the ambulatory setting.

Jonas Munch Nielsen, Ivan C. Zibrandtsen, Paolo Masulli, Torben Lykke Sørensen, Tobias S. Andersen, Troels Wessenberg Kjær. Towards a wearable multi-modal seizure detection system in epilepsy: A pilot study.	Jonas Munch Nielsen, Ivan C. Zibrandtsen, Paolo Masulli, Torben Lykke Sørensen, Tobias S. Andersen, Troels Wessenberg Kjær.	Electroencephalogram (EEG), Electrocardiogram (ECG), Accelerometer (ACC)	Machine Learning	Science Direct	Visualizations of EEG and ECG features were found to be useful for supplementing manual data review.
Lockman J, Fisher RS, Olson DM. Detection of seizure-like movements using a wrist accelerometer. Epilepsy Behav. 2011 Apr;20(4):638-41. doi: 10.1016/j.yebeh.2011.01.019. Epub 2011 Mar 29. PMID: 21450533.	Lockman J, Fisher RS, Olson DM.	Accelerometer (ACC)	-	Science Direct	This study shows tonic-clonic seizure detection based on wrist-worn motion detector with a Bluetooth link to a computer.
Affanni, A., 2020. Wireless sensors system for stress detection by means of ECG and EDA acquisition. Sensors, 20(7), p.2026.	Affanni, A.	Electrodermal activity (EDA) sensor Electrocardiogram (ECG) sensor	Machine Learning, SVM Classifier	ResearchGate	The researchers designed a wearable sensors system for measuring two channels SPR (Skin Potential Response) from the hands and two channels ECG from chest.
Majumder, A.K.M., ElSaadany, Y.A., Young, R. and Ucci, D.R., 2019. An energy efficient wearable smart IoT system to predict cardiac arrest. Advances in Human-Computer Interaction, 2019.	Majumder, A.K.M., ElSaadany, Y.A., Young, R. and Ucci, D.R.	Heart Rate, Body Temperatures	IoT System	ResearchGate	In this paper, researchers designed and developed an integrated smart IoT system to predict and monitor heart abnormality in patients.

Moodbidri, A. and Shahnasser, H., 2017, January. Child safety wearable device. In 2017 International Conference on Information Networking (ICOIN)(pp. 438-444).IEEE.	Moodbidri, A. and Shahnasser, H.	Real-time location, surrounding temperature, UV radiation index, Distress alarm buzzer	IoT System	Researc hGate	It provides parents with the real-time location, surrounding temperature, UV radiation index and Distress alarm buzzer functionality locate their child or alert bystanders to rescue or comfort the child.
Chen, Y.H., Chiou, H.Y., Lin, H.C. and Lin, H.L., 2009. Affect of seizures during gestation on pregnancy outcomes in women with epilepsy. Archives of neurology, 66(8), pp.979-984.	Chen, Y.H., Chiou, H.Y., Lin, H.C. and Lin, H.L.	-	-	PubMed	The paper found that women who had seizures during pregnancy had higher odds of preterm birth, LBW, and SGA infants than women without epilepsy.
Bornoiu, I.V. and Grigore,O., 2013, May. A study about feature extraction for stress detection. In 2013 8th International Symposium on Advanced Topics in Electrical Engineering (ATEE) (pp. 1-4). IEEE.	Bornoiu, I.V. and Grigore, O	Electromyography (EMG), Electrocardiogram (ECG), Electroencephalogram (EEG)	-	Semant ic Scholar	Overall, it seems like this paper may be of interest to researchers studying EDA signals and their relationship to stress and other physiological responses.
Sai Manohar Beeraka, Abhash Kumar, Mustafa Sameer, Sanchita Ghosh, Bharat Gupta. Accuracy Enhancement of Epileptic Seizure Detection: A Deep Learning Approach with Hardware Realization of STFT.	Sai Manohar Beeraka, Abhash Kumar, Mustafa Sameer, Sanchita Ghosh, Bharat Gupta.	Electroencephalogram (EEG)	Deep Learning models STFT, CNN, Bi-LSTM	Researc hGate	The study Demonstrates the potential of deep learning-based approaches for EEG analysis and seizure detection, providing a promising direction for future research in this field

<p>Hartmann, Manfred, Johannes Koren, Christoph Baumgartner, Jonas Duun-Henriksen, Gerhard Gritsch, Tilman Kluge, Hannes Perko, and Franz Fürbass. "Seizure detection with deep neural networks for review of two-channel electroencephalogram." <i>Epilepsia</i> (2022).</p>	<p>Hartmann, Manfred, Johannes Koren, Christoph Baumgartner, Jonas Duun-Henriksen, Gerhard Gritsch, Tilman Kluge, Hannes Perko, and Franz Fürbass</p>	<p>Electroencephalogram (EEG)</p>	<p>Deep Learning Model – Neural Network</p>	<p>Epilepsia</p>	<p>This approach offers flexibility, high accuracy, and computational efficiency. It also works for detecting absence and focal seizures. The validation and training data used in the study came from independent hospitals, and the authors hypothesize that additional independent data for training could improve performance, robustness, and generalization capability.</p>
<p>Gao, Bin, Jiazheng Zhou, Yuying Yang, Jinxiu Chi, and Qi Yuan. "Generative adversarial network and convolutional neural network-based EEG imbalanced classification model for seizure detection." <i>Biocybernetics and Biomedical Engineering</i> 42, no. 1 (2022): 1-15.</p>	<p>Gao, Bin, Jiazheng Zhou, Yuying Yang, Jinxiu Chi, and Qi Yuan</p>	<p>Electroencephalogram (EEG)</p>	<p>Deep Learning Model – CNN</p>	<p>Science Direct</p>	<p>This paper proposes a novel epileptic seizure detection method combining GAN and 1DCNN, generating more seizure data for a small data set. The method demonstrated good classification results across three EEG databases, demonstrating its generalizability.</p>

Ahmad, I., Wang, X., Zhu, M., Wang, C., Pi, Y., Khan, J.A., Khan, S., Samuel, O.W., Chen, S. and Li, G., 2022. EEG-based epileptic seizure detection via machine/deep learning approaches: A Systematic Review. Computational Intelligence and Neuroscience, 2022.	Ahmad, I., Wang, X., Zhu, M., Wang, C., Pi, Y., Khan, J.A., Khan, S., Samuel, O.W., Chen, S. and Li, G.	Electroencephalogram (EEG)	Machine Learning and Deep Learning	Hindawi	In this research, a comprehensive review of ML and DL models was performed using feature extraction and selection. This study mainly focused on the usage of ANN, SVM, and KNN machine learning models and CNN, RNN, and LSTM deep learning models.
Jemal, I., Mezghani, N., Abou-Abbas, L. and Mitiche, A., 2022. An interpretable deep learning classifier for epileptic seizure prediction using EEG data. IEEE Access, 10, pp.60141-60150	Jemal, I., Mezghani, N., Abou-Abbas, L. and Mitiche, A.,	Electroencephalogram (EEG)	Deep Learning	IEEE Xplore	The study can be strengthened using larger amounts of data and using different databases. Furthermore, the proposed architecture can be applied to other EEG-based classification tasks helping in improving the quality of life of the patients.
Abdelhameed, Ahmed, and Magdy Bayoumi. "A deep learning approach for automatic seizure detection in children with epilepsy." Frontiers in Computational Neuroscience 15 (2021): 650050.	Abdelhameed, Ahmed, and Magdy Bayoumi.	Electroencephalogram (EEG)	Deep Learning	Frontiers	The new method makes use of a two-dimensional deep convolution autoencoder (2D-DCAE) linked to a neural network-based classifier to create a unified system that is trained in a supervised manner to achieve the best classification accuracy between the ictal and interictal brain state signals.

<p>Li, Zhengdao, Kai Hwang, Keqin Li, Jie Wu, and Tongkai Ji. "Graph-generative neural network for EEG-based epileptic seizure detection via discovery of dynamic brain functional connectivity." <i>Scientific Reports</i> 12, no. 1 (2022): 18998</p>	<p>Li, Zhengdao, Kai Hwang, Keqin Li, Jie Wu, and Tongkai Ji.</p>	<p>Electroencephalogram (EEG)</p>	<p>Deep Learning – Graph-generative Neural Network</p>	<p>-</p>	<p>Using a clinically validated dataset of more than 3047 cases of epileptic seizures, they have trained the GGN model, helping it to design the model architecture and operational processes.</p>
<p>Böttcher, S., Bruno, E., Epitashvili, N., Dümpelmann, M., Zabler, N., Glasstetter, M., Ticcinelli, V., Thorpe, S., Lees, S., Van Laerhoven, K. and Richardson, M.P., 2022. Intra-and inter-subject perspectives on the detection of focal onset motor seizures in epilepsy patients. <i>Sensors</i>, 22(9), p.3318.</p>	<p>Böttcher, S., Bruno, E., Epitashvili, N., Dümpelmann, M., Zabler, N., Glasstetter, M., Ticcinelli, V., Thorpe, S., Lees, S., Van Laerhoven, K. and Richardson,</p>	<p>Electrodermal Activity (EDA)</p>	<p>Machine Learning Algorithms</p>	<p>National Library of Medicine</p>	<p>The authors came to the conclusion that although wearable sensors can be utilised to identify focal onset motor seizures, unique patient models are required. They added that their outcomes outperformed those of previous research that employed intra-subject models.</p>
<p>Gaurav, G., Shukla, R., Singh, G. and Sahani, A.K., 2022. A Machine Learning Approach to the Smartwatch-based Epileptic Seizure Detection System. <i>IETE JOURNAL OF RESEARCH</i>.</p>	<p>Gaurav, G., Shukla, R., Singh, G. and Sahani, A.K.,</p>	<p>Photoplethysmography (PPG), electrodermal activity (EDA), accelerometry, and temperature sensors</p>	<p>Machine Learning Model - SVM</p>	<p>IETE Journal Of Research</p>	<p>They come to the conclusion that the suggested technique is a potential method for detecting seizure activity and pre-seizure conditions. They contend that further study is required to increase the system's accuracy and assess how well it functions in practical situations.</p>

<p>Beeraka, S.M., Kumar, A., Sameer, M. et al. Accuracy Enhancement of Epileptic Seizure Detection: A Deep Learning Approach with Hardware Realization of STFT. Circuits Syst Signal Process 41, 461–484 (2022).</p>	<p>Beeraka, S.M., Kumar, A., Sameer, M. et al</p>	<p>Electroencephalogram (EEG)</p>	<p>Deep Learning Models – CNN, Bi-LSTM, STFT</p>	<p>Springer Link</p>	<p>The study used the Bonn EEG dataset and produced a maximum error of around 0.13% when compared to the output obtained using STFT. CNN and Bi-LSTM models demonstrated the efficiency of deep learning for seizure identification in EEG data (for both epileptic and non-epileptic patients) with average accuracies of 93.9% and 97.2%, respectively.</p>
<p>M. Shamim Hossain, Syed Umar Amin, Mansour Alsulaiman, Ghulam Muhammad ACM Transactions on Multimedia Computing, Communications, and Applications Volume 15 Issue 1 Article No.: 10pp 1–17. “Applying Deep Learning for Epilepsy Seizure Detection and Brain Mapping Visualization”</p>	<p>M. Shamim Hossain, Syed Umar Amin, Mansour Alsulaiman, Ghulam Muhammad</p>	<p>Electroencephalogram (EEG)</p>	<p>Deep Learning Models - CNN</p>	<p>-</p>	<p>This system also developed a visual spectral amplitude feature that employed correlational maps to offer medical specialists with timely and appropriate brain mapping pictures for future inquiry. Overall, this model demonstrated its efficacy in robust seizure identification and feature visualization in EEG data.</p>

Table 2.1: Literature Review Summary Table

2.2. EXISTING SYSTEM

Wearable technologies hold immense potential as a transformative tool for individuals grappling with epileptic seizures. The Embrace E4 watches, in particular, have emerged as a groundbreaking solution, demonstrating the capability to detect and predict seizures well in advance of their onset. Leveraging various physiological parameters such as electrodermal activity (EDA), heart rate, blood pressure, and acceleration, these watches employ sophisticated machine learning techniques to learn and evaluate patterns.

The utilization of machine learning and deep algorithms allows for the analysis of sensor responses and seizure frequency, resulting in significantly improved detection accuracy and minimal false alarm rates. The integration of EDA, ACC, and BVP sensors contributes to the success rates of the Embrace E4 watches, ranging from 92% to 100%. Notably, the device's sensitivity approaches 100%, presenting a promising avenue for reducing the risk of Sudden Unexpected Death in Epilepsy (SUDEP) by predicting seizures. Additionally, the incorporation of a location feature adds an extra layer of functionality, enabling caregivers to receive alerts when a potential epileptic seizure is detected.



Fig 2.1: Empatica E4 Wristband

2.3. PROBLEM FORMULATION

The occurrence of seizures, characterized by a sudden burst of electrical activity in the brain, constitutes a significant neurological challenge. Epilepsy, a condition stemming from recurrent seizures with unidentified triggers, affects approximately 50 million individuals globally, ranking among the most prevalent neurological disorders. While seizures are typically non-life-threatening, the experience is unsettling for both the individual and those in close proximity. However, with proper care and support, many individuals with epilepsy can lead healthy lives. Efforts to develop monitoring systems for seizure patients and enhance seizure detection have been ongoing. Traditional methods involve identifying seizures through ECG or EEG waves, but these sensor systems are often impractical and lack portability. The introduction of wrist-worn devices has emerged as a promising solution due to their mobility and convenient size.

To make this model practical and effective, the incorporation of sensors capable of detecting seizures is crucial. Given the limitations of relying on a single sensor, a multimodal sensor approach is proposed. Among the most practical sensors for this purpose are the Accelerometer (ACC) and the Electrodermal Activity (EDA) sensors.

The ACC sensor enables precise positioning of the device and tracking sudden movements, while the EDA sensor measures variations in skin conductivity resulting from increased sweat gland activity. Addressing this problem requires the utilization of deep learning algorithms to train models using data gathered from these sensors. The objective is to develop a robust model capable of accurately detecting seizures. Furthermore, there is a proposal to enhance and implement this model into wristwear devices, endowing them with the capability to alert caregivers when seizures are detected.

In integrating these advancements, it's imperative to ensure data privacy, ethical considerations, and seamless user experience. The implementation of such devices necessitates not only accurate detection but also user-friendly interfaces and secure data management. Collaborative efforts between technologists, healthcare professionals, and individuals with epilepsy are vital to refine these technologies, ensuring they are not just functional but also intuitive and supportive for those who rely on them daily.

2.4. PROPOSED SYSTEM

The envisioned system is a sophisticated deep learning model designed to achieve precise and real-time seizure detection in individuals with epilepsy. The system incorporates wearable sensors to capture crucial data on various parameters, including movement and heart rate. The primary objective of this system is to create an exceptionally sensitive and specific deep learning model capable of accurately identifying seizures. Central to the research is the utilization of a substantial dataset containing labeled seizure and non-seizure data. This extensive dataset enables the model to discern intricate patterns and characteristics associated with seizures, enhancing its learning capabilities. A paramount focus of the investigation is the enhancement of the overall performance of the deep learning model, thereby elevating its accuracy.

The ultimate goal is to provide individuals with epilepsy the benefit of timely interventions, mitigating the risk of injury or other severe consequences associated with seizures. Beyond individual impact, the technology holds promise in delivering valuable insights to caregivers and medical professionals. This information can significantly inform treatment decisions and contribute to an improved overall management of epilepsy, underscoring the potential transformative impact of the proposed deep learning-based seizure detection system.

While the current emphasis remains on refining the deep learning model for seizure detection, the long-term vision involves seamless integration into wearable devices. By prioritizing the development of a robust and accurate model, we lay the groundwork for future implementation into portable, user-friendly devices. These devices could provide real-time monitoring and alerts, offering individuals with epilepsy a sense of security and enabling timely intervention by caregivers or medical professionals. Moreover, the concentrated focus on the deep learning model allows for scalability and adaptability. As technology evolves, advancements in hardware and sensor systems can be integrated with the existing model. This approach ensures flexibility, enabling the incorporation of newer sensors or improved device capabilities without altering the fundamental algorithm, thereby future-proofing the system against technological advancements. The aim is to create a model that can seamlessly adapt to diverse hardware configurations, fostering longevity and versatility in application.

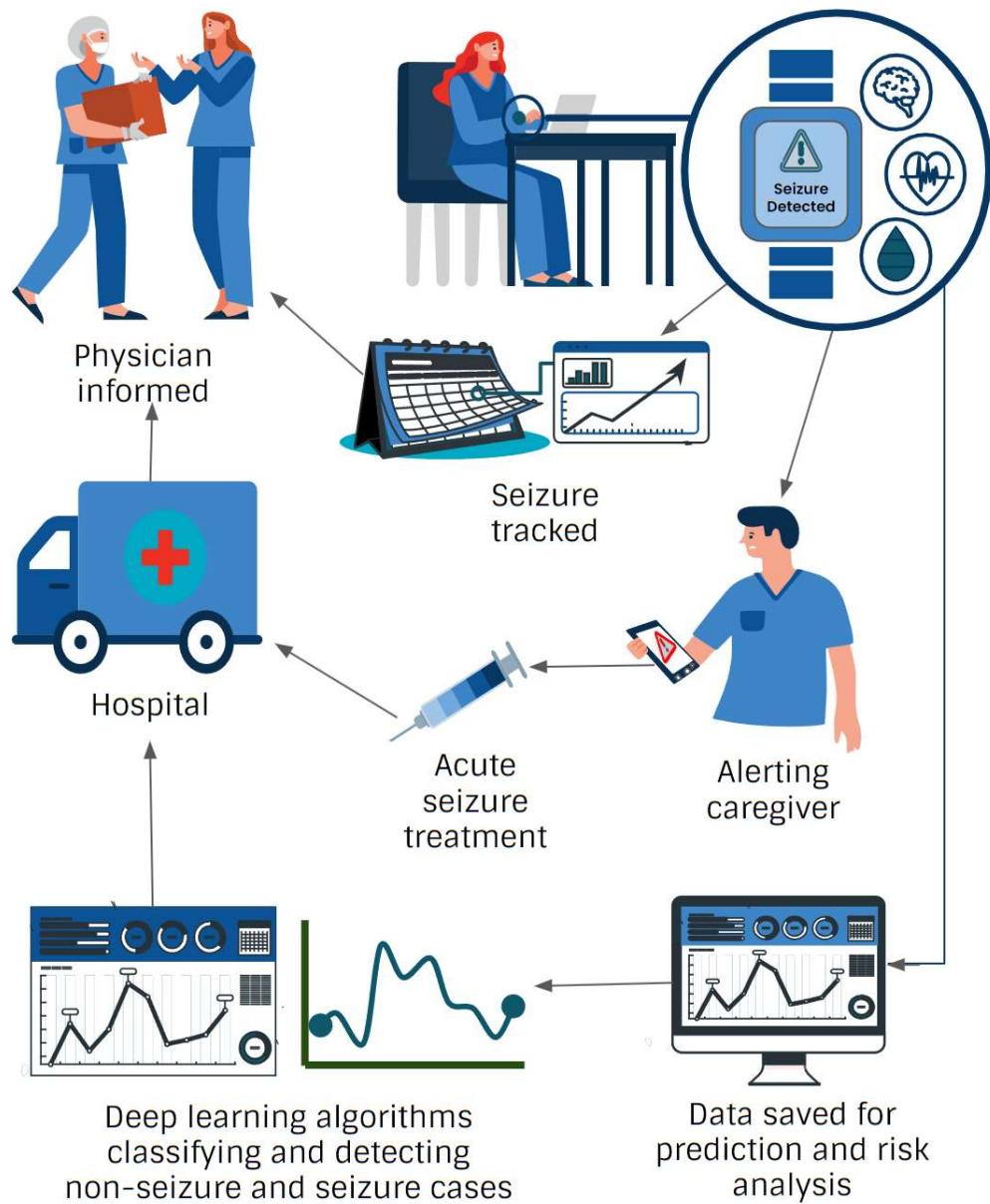


Fig 2.2: Proposed System

2.5. OBJECTIVES

- To properly evaluate the performance of the seizure detection system.
- To develop an accurate detection system algorithm using deep learning
- To optimize and validate the seizure detection system
- To understand the clinical application of the seizure detection system.

CHAPTER – 3

DESIGN FLOW / METHODOLOGY

The methodology for seizure detection in this study involved leveraging data obtained from the My Seizure Gauge Seizure Forecasting Challenge. This dataset encompassed recordings from wrist-worn Empatica E4 devices and NeuroPace RNS implants, spanning from UTC-2020_02_26-23_10_00 to UTC-2020_08_12-17_30_00.

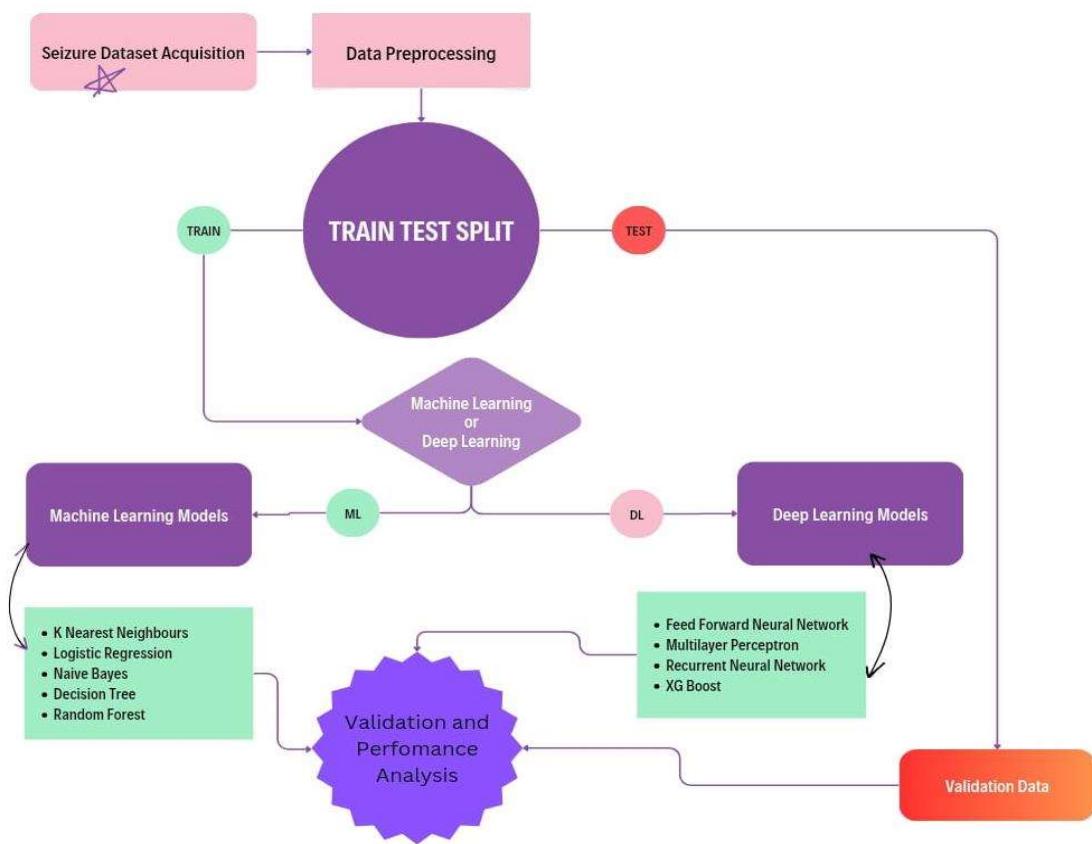


Fig 3.1: Methodology Flowchart

Data Collection and Monitoring:

The patients in the dataset were monitored using Empatica wristwatches, which were equipped with a suite of biosensors capturing essential physiological parameters. These sensors included:

- EDA (Electrodermal Activity)
- ACC (Accelerometer)
- BVP (Blood Volume Pulse)
- HR (Heart Rate)

These sensors provided a comprehensive view of the patients' physiological status, offering insights into their activities, movements, and physiological responses. The recorded data from these sensors served as the foundation for the seizure detection process.

	acc_mag	bvp	eda	hr	temp	Target
0	62.481546	-62.665309	0.332887	48.305214	35.339849	1
1	62.455042	-63.849821	0.332887	48.305214	35.339849	1
2	62.470944	-64.343368	0.332887	48.305214	35.339849	1
3	62.497448	-64.047240	0.332887	48.303558	35.339849	1
4	62.529252	-62.566599	0.332887	48.303558	35.339849	1
...
921595	53.571602	304.373979	0.100176	89.972695	32.179991	0
921596	52.569762	297.347952	0.101434	89.972695	32.179991	0
921597	51.774651	290.891602	0.102692	89.974904	32.179991	0
921598	51.186269	285.194823	0.103881	89.974904	32.179991	0
921599	52.930213	281.966648	0.105139	89.977113	32.179991	0

921600 rows × 6 columns

	utc_timestamp	acc_x	acc_y	acc_z	acc_mag	bvp	eda	hr	temp	Target
0	1.583668e+09	7.311602	-28.998363	-55.994954	62.481546	-62.665309	0.332887	48.305214	35.339849	1
1	1.583668e+09	7.057167	-28.998363	-55.994954	62.455042	-63.849821	0.332887	48.305214	35.339849	1
2	1.583668e+09	7.194986	-28.998363	-55.994954	62.470944	-64.343368	0.332887	48.305214	35.339849	1
3	1.583668e+09	7.444120	-28.998363	-55.994954	62.497448	-64.047240	0.332887	48.303558	35.339849	1
4	1.583668e+09	7.698555	-28.998363	-55.994954	62.529252	-62.566599	0.332887	48.303558	35.339849	1
...
921595	1.583807e+09	28.403681	-27.068579	37.929114	53.571602	304.373979	0.100176	89.972695	32.179991	0
921596	1.583807e+09	27.158007	-29.321395	35.676299	52.569762	297.347952	0.101434	89.972695	32.179991	0
921597	1.583807e+09	25.907032	-31.568909	33.428784	51.774651	290.891602	0.102692	89.974904	32.179991	0
921598	1.583807e+09	24.656057	-33.821724	31.175969	51.186269	285.194823	0.103881	89.974904	32.179991	0
921599	1.583807e+09	26.511317	-35.830705	30.359655	52.930213	281.966648	0.105139	89.977113	32.179991	0

921600 rows × 10 columns

Fig 3.2: Dataset

Data Preprocessing:

The dataset initially consisted of 100 parquet files per patient. A subset was selected based on seizure instances, guided by a separate CSV file detailing target labels mapping seizure presence to specific parquet file names. These selected parquet files were then converted to CSV format, incorporating the associated target labels. The dataset was structured to include both seizure and non-seizure instances, forming the training dataset.

Rigorous preprocessing techniques were applied to the dataset. This included:

- Data cleaning to handle missing or anomalous values.
- Normalization to standardize the data and bring all features to a common scale.
- Feature engineering to extract relevant information from the physiological signals.

```
▶ import pandas as pd
  import numpy as np

[ ]:
  data = pd.read_csv('/kaggle/input/seizure-dataset/szdata.csv')
  df = pd.DataFrame(data)
  df

[ ]:
  columns_to_drop = ['utc_timestamp', 'acc_x', 'acc_y', 'acc_z']
  df.drop(columns_to_drop, axis=1, inplace=True)

[ ]:
  x = df.iloc[:,0:5]
  y = df.iloc[:, -1]

[ ]:
  from sklearn.model_selection import train_test_split
  x_train,x_valid,y_train,y_valid = train_test_split(x,y,test_size=0.2,random_state=15)
```

Fig 3.3: Data Preprocessing

Machine Learning and Deep Learning Models:

A diverse range of machine learning algorithms and deep learning models were employed for seizure detection. These included:

- K-Nearest Neighbors (KNN)

KNN is an instance-based learning algorithm that classifies data points based on the majority class of their k-nearest neighbors in the feature space. The algorithm's sensitivity to local patterns, determined by the choice of 'k,' makes it effective for simple classification tasks, especially when decision boundaries are non-linear. It relies on distance metrics, such as Euclidean distance, to measure the proximity of data points, offering flexibility in capturing local trends.

- Logistic Regression (LogR)

Logistic Regression is a linear model designed for binary classification. It models the probability that a given instance belongs to a particular class using the logistic function. The decision boundary, a linear combination of input features transformed into a probability between 0 and 1, is particularly suitable for cases where the relationship between features and the binary outcome is assumed to be linear.

- Gaussian Naive Bayes (GaussNB)

GaussNB is a probabilistic model based on Bayes' theorem, assuming feature independence given the class. It calculates class probabilities using Gaussian distributions. This model is efficient for tasks like text classification and is advantageous when dealing with high-dimensional data due to its simplifying independence assumption.

- Multi-Layer Perceptron (MLP)

MLP, a type of Feedforward Neural Network (FNN), is composed of multiple layers of nodes with non-linear activation functions. Its architecture allows it to learn complex patterns in data through the forward pass, involving weighted sums and non-linear activations. With depth and non-linearities, MLP is a versatile model suitable for various tasks, including image and speech recognition.

- Feedforward Neural Networks (FNN)

Similar to MLP, FNN is a feedforward neural network without feedback connections between layers. Each layer processes input independently, making it suitable for tasks where the sequence of data is less critical. It is commonly employed in image classification and scenarios where the order of features is less significant.

- eXtreme Gradient Boosting (XGB)

XGB is a gradient boosting framework that builds an ensemble of weak learners, typically decision trees, sequentially. Each tree corrects errors of the previous ones, contributing to improved overall predictive accuracy. Known for its speed and accuracy, XGB is highly effective for structured/tabular data, often used in classification and regression tasks.

- Recurrent Neural Networks (RNN)

RNN is a neural network with recurrent connections, maintaining hidden states to capture information across time steps. This makes it suitable for sequence data with temporal dependencies, such as time series analysis and natural language processing. RNNs excel in tasks where the context or order of input data is crucial for understanding and prediction.

Model Training and Evaluation:

- **Training:**

Models were trained on the preprocessed dataset with the aim of capturing intricate patterns indicative of seizures.

The diverse set of models allowed for the exploration of different learning approaches and their suitability for the given task.

- **Evaluation:**

Robust metrics were employed for model evaluation, ensuring a comprehensive assessment of their performance.

Thorough cross-validation was conducted to validate the models' effectiveness and generalizability across different subsets of the data.

Model Optimization:

- **Hyperparameter Tuning:**

Further optimization involved adjusting model hyperparameters to enhance performance.

The goal was to strike a balance between capturing nuanced patterns and avoiding overfitting.

- **Ensemble Methods:**

Exploration of ensemble methods aimed to combine the strengths of multiple models, enhancing overall predictive power.

This step focused on improving robustness and ensuring the models could generalize well to unseen data.⁵

In summary, the methodology integrated comprehensive data collection, thorough preprocessing, and the utilization of a variety of machine learning and deep learning models to detect seizures in patients. The process involved careful selection of relevant data, rigorous preprocessing, and extensive model evaluation and optimization to achieve accurate and generalizable results in seizure detection.

3.1. Implementation:

3.1.1. Deep Learning Models:

3.1.1.1. Feed Forward Neural Network:

```
[ ]: from tensorflow import keras
      from tensorflow.keras import layers

      model = keras.Sequential([
          layers.Dense(4, activation='relu', input_shape=[5]),
          layers.Dense(4, activation='relu'),
          layers.Dense(1, activation='sigmoid'),
      ])

[ ]: model.compile(
      optimizer='adam',
      loss='binary_crossentropy',
      metrics=['binary_accuracy'],
  )

[ ]: early_stopping = keras.callbacks.EarlyStopping(
      patience=25,
      min_delta=0.001,
      restore_best_weights=True,
  )
```

Fig 3.4: FFNN

The provided code implements a binary classification neural network using TensorFlow and Keras. The model consists of three layers with ReLU and sigmoid activation functions. It is compiled with the Adam optimizer, binary crossentropy loss, and binary accuracy as the evaluation metric.

Early stopping is implemented with a patience of 25 epochs, a minimum delta of 0.001, and restoration of the best weights for efficient model training. This script serves as a concise and effective foundation for binary classification tasks, with detailed documentation for future reference.

```
[ ]: history = model.fit(
    x_train, y_train,
    validation_data=(x_valid, y_valid),
    batch_size=52,
    epochs=50,
    callbacks=[early_stopping],
)

[ ]: history_df = pd.DataFrame(history.history)

history_df.loc[5:, ['loss', 'val_loss']].plot()
history_df.loc[5:, ['binary_accuracy', 'val_binary_accuracy']].plot()

print(("Best Validation Loss: {:.4f}" +\
      "\nBest Validation Accuracy: {:.4f}").format(
          history_df['val_loss'].min(),
          history_df['val_binary_accuracy'].max()))

+ Code + Markdown

[ ]: y_pred1 = model.predict(x_valid)
y_pred_binary = np.round(y_pred1)

[ ]: y_pred1
```

Fig 3.5: Validating The Model

The code initiates the training of a neural network model using the fit method, employing a batch size of 52, training for 50 epochs, and incorporating early stopping for efficiency. The model is evaluated on validation data to assess performance. The code outputs crucial metrics regarding the model's performance on the validation set. Specifically, it provides information on the best achieved validation loss and accuracy during the training process. Finally, the code leverages the trained model to make predictions on the validation data (x_valid). It computes continuous predictions (y_pred1) and binary predictions (y_pred_binary), providing insights into the model's predictive capabilities.

```

history_df = pd.DataFrame(history.history)

history_df.loc[5:, ['loss', 'val_loss']].plot()
history_df.loc[5:, ['binary_accuracy', 'val_binary_accuracy']].plot()

print("Best Validation Loss: {:.4f}\n"
      "\nBest Validation Accuracy: {:.4f})".format(
          history_df['val_loss'].min(),
          history_df['val_binary_accuracy'].max())

```

[79]

... Best Validation Loss: 0.2625
Best Validation Accuracy: 0.9123

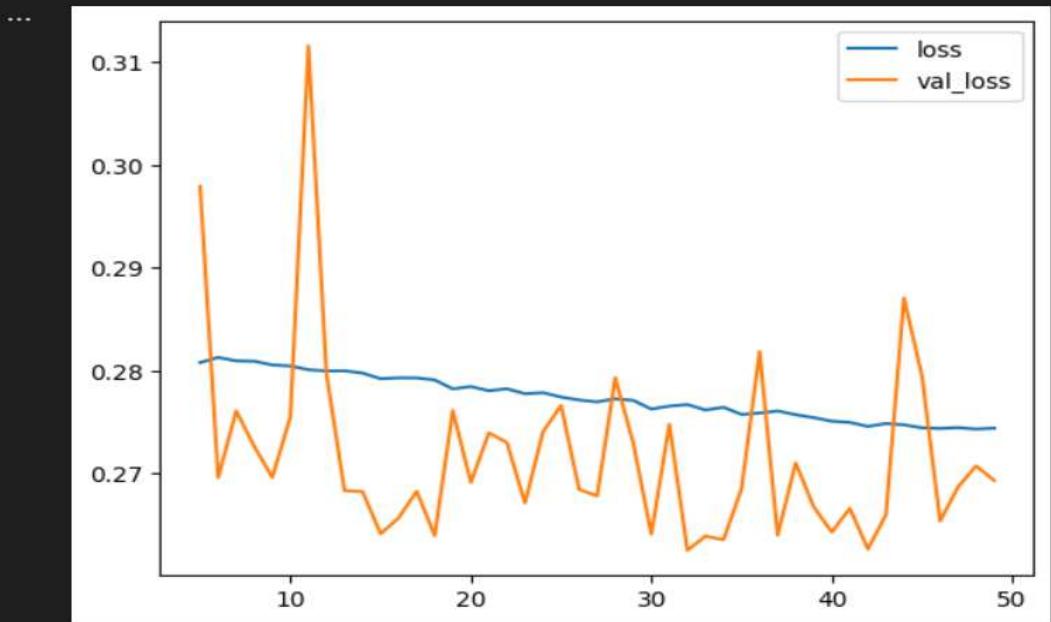


Fig 3.6: Validation Loss

```

from sklearn.metrics import precision_score, recall_score, f1_score

precision1 = precision_score(y_valid, y_pred_binary)
recall1 = recall_score(y_valid, y_pred_binary)
f11 = f1_score(y_valid, y_pred_binary)

print(f'Precision: {precision1:.4f}')
print(f'Recall: {recall1:.4f}')
print(f'F1 Score: {f11:.4f}')

```

Precision: 0.8677
Recall: 0.9525
F1 Score: 0.9081

Fig 3.7: Evaluation Metrics

3.1.1.2. Multi-Layered Perceptron:

```
[ ]: from sklearn.neural_network import MLPClassifier  
  
mlp = MLPClassifier(hidden_layer_sizes=(9,8),  
                     random_state=15,  
                     verbose=True,  
                     learning_rate_init=0.01)  
  
mlp.fit(x_train,y_train)
```

```
[ ]: ypred2=mlp.predict(x_valid)  
  
from sklearn.metrics import classification_report  
  
classification_report(y_valid,ypred2)
```

```
print(accuracy_score(y_valid,ypred2))  
print(precision_score(y_valid,ypred2))  
print(recall_score(y_valid,ypred2))  
print(f1_score(y_valid,ypred2))  
  
0.9637966579861111  
0.9488117386140279  
0.9804174993483361  
0.9643557269604885
```

Fig 3.8: Evaluation Metrics for MLP

The code utilizes the MLPClassifier from the scikit-learn library for neural network based classification. The code evaluates the MLPClassifier's performance on validation data and generates a classification report using scikit-learn's classification_report. This comprehensive report provides precision, recall, F1-score, and support for each class, offering insights into the model's classification performance on the validation set. The MLPClassifier is configured with two hidden layers of sizes 9 and 8, a random seed of 15 for reproducibility, verbose output during training, and an initial learning rate of 0.01.

3.1.1.3. Recurrent Neural Network:

```
[ ]:
from tensorflow.keras.models import Sequential
from tensorflow.keras.layers import SimpleRNN, Dense, Dropout
seq_length = 5
model_rnn = Sequential()
model_rnn.add(SimpleRNN(64, input_shape=(seq_length, 1), return_sequences=True))
model_rnn.add(Dropout(0.2))
model_rnn.add(SimpleRNN(32, return_sequences=True))
model_rnn.add(Dropout(0.2))
model_rnn.add(SimpleRNN(32))
model_rnn.add(Dropout(0.2))
model_rnn.add(Dense(1, activation='sigmoid'))

model_rnn.compile(loss='binary_crossentropy', optimizer='adam', metrics=['accuracy'])
model_rnn.summary()
```

```
[ ]:
history_1 = model_rnn.fit(
    x_train, y_train,
    validation_data=(x_valid, y_valid),
    batch_size=52,
    epochs=50,
    callbacks=[early_stopping]
)
```

Fig 3.9: RNN Model

The code defines a Sequential model for a Recurrent Neural Network (RNN) using TensorFlow and Keras. The RNN model is compiled with binary crossentropy loss, the adam optimizer, and accuracy as the evaluation metric. The model is trained on the provided training data (`x_train` and `y_train`) with validation on a separate dataset (`x_valid` and `y_valid`). The training process involves a batch size of 52, running for 50 epochs, and early stopping as a callback. This RNN architecture includes three SimpleRNN layers with dropout regularization, followed by a dense layer with sigmoid activation for binary classification. The training history (`history_1`) is stored for further analysis.

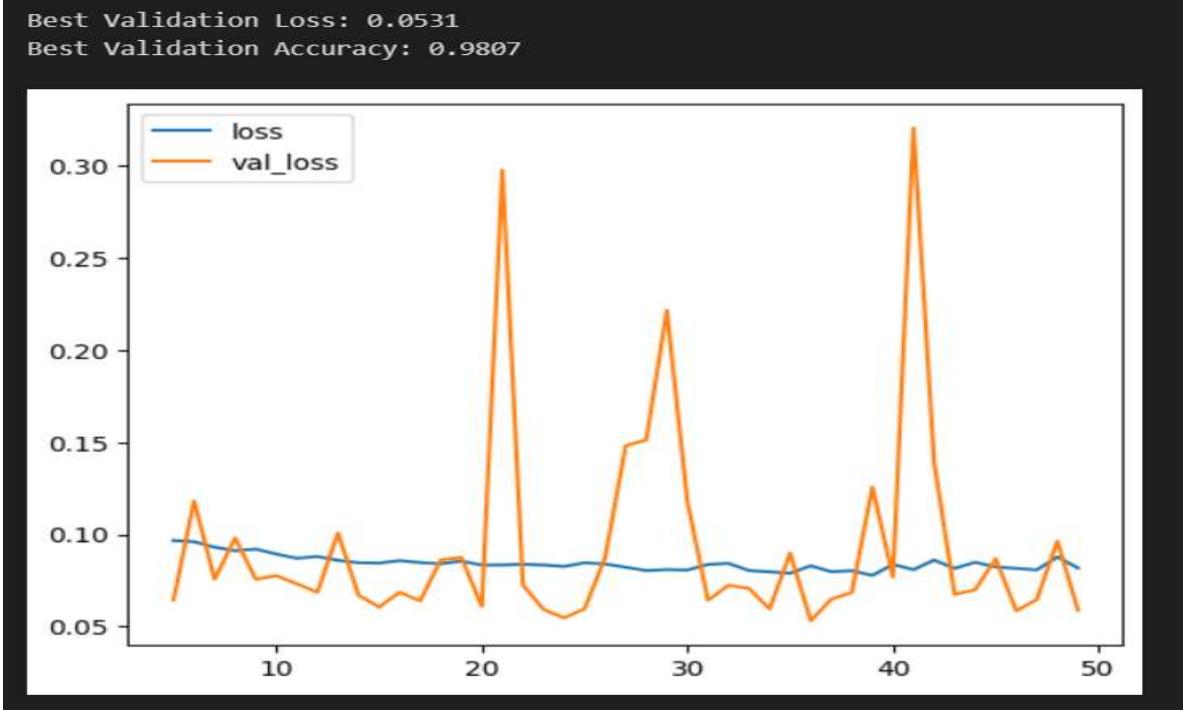


Fig 3.10: Validation Loss and Accuracy of RNN Model

```

precision2 = precision_score(y_valid, y_pred_binary2)
recall2 = recall_score(y_valid, y_pred_binary2)
f12 = f1_score(y_valid, y_pred_binary2)

print(f'Precision: {precision2:.4f}')
print(f'Recall: {recall2:.4f}')
print(f'F1 Score: {f12:.4f}')

]

Precision: 0.9758
Recall: 0.9794
F1 Score: 0.9776

]

acc2 = accuracy_score(y_valid, y_pred_binary2)
print(f'Accuracy: {acc2:.4f}')

]

Accuracy: 0.9776
    
```

Fig 3.11: Evaluation Metrics of RNN Model

The code reports key evaluation metrics for the RNN model trained and validated previously. This section prints the best achieved validation loss and accuracy during the training process. Precision, recall, and F1 score are calculated using scikit-learn's metrics functions for binary classification. The code prints the precision, recall, F1 score, and accuracy for the model on the validation set. These metrics provide a comprehensive understanding of the model's performance in binary classification tasks.

3.1.1.4. eXtreme Gradient Boosting:

```
[ ]: import xgboost as xgb

[ ]: hyperparameters = {
    'n_estimators': 200,
    'max_depth': 5,
    'learning_rate': 0.1,
}

[ ]: modelx = xgb.XGBClassifier(**hyperparameters)
modelx.fit(x_train, y_train)

[ ]: y_predx = model.predict(x_valid)
```

Fig 3.12: XGBoost Model

The code implements an XGBoost classifier for binary classification tasks. This section configures an XGBoost classifier with specified hyperparameters, including the number of estimators, maximum depth, and learning rate.

The model is then trained on the provided training data (`x_train` and `y_train`). Predictions are made on the validation data (`x_valid`). The continuous predictions (`y_predx`) are then binarized based on a threshold of 0.5 to obtain binary predictions (`y_pred_binaryx`).

```
threshold = 0.5
y_pred_binaryx = np.where(y_predx >= threshold, 1, 0)

from sklearn.metrics import accuracy_score

accuracyx = accuracy_score(y_valid, y_pred_binaryx)
precisionx = precision_score(y_valid, y_pred_binaryx)
recallx = recall_score(y_valid, y_pred_binaryx)
f1x = f1_score(y_valid, y_pred_binaryx)

print(f'Accuracy: {accuracyx:.4f}')
print(f'Precision: {precisionx:.4f}')
print(f'Recall: {recallx:.4f}')
print(f'F1 Score: {f1x:.4f}')

Accuracy: 0.9067
Precision: 0.8754
Recall: 0.9482
F1 Score: 0.9103
```

Fig 3.13: Evaluation Metrics of XGBoost Model

3.1.2. Machine Learning Models:

3.1.2.1. K-Nearest Neighbour (KNN):

```
[ ]:  
from sklearn.neighbors import KNeighborsClassifier  
knn= KNeighborsClassifier(n_neighbors=5000)  
knn.fit(x_train, y_train)  
  
[ ]:  
knn_pred= knn.predict(x_valid)
```

Fig 3.14: KNN Model

The code implements a K-Nearest Neighbors (KNN) classifier for binary classification. This section configures the KNN classifier with a specified number of neighbors (5000 in this case) and trains it on the provided training data (`x_train` and `y_train`).

Predictions are then made on the validation data (`x_valid`) using the trained KNN model, and the results are stored in the variable `knn_pred`.

```
print(classification_report(y_valid,knn_pred))  
accuracy = accuracy_score(y_valid, knn_pred)  
print("Accuracy = ",accuracy)  
  
precision    recall   f1-score   support  
0            0.83      0.78      0.80     92248  
1            0.79      0.84      0.81     92072  
  
accuracy                           0.81    184320  
macro avg       0.81      0.81      0.81    184320  
weighted avg    0.81      0.81      0.81    184320  
  
Accuracy =  0.8086100260416667  
  
print(precision_score(y_valid, knn_pred))  
print(recall_score(y_valid, knn_pred))  
print(f1_score(y_valid, knn_pred))  
  
0.7924231034589284  
0.835791554435659  
0.8135297569020472
```

Fig 3.15: Evaluation Metrics of KNN Model

3.1.2.2. Logistic Regression:

```
[ ]: from sklearn.linear_model import LogisticRegression  
lr = LogisticRegression()  
lr.fit(x_train, y_train)  
lr_pred= lr.predict(x_valid)  
  
[ ]: + Code + Markdown  
  
[ ]: print(classification_report(y_valid,lr_pred))  
  
[ ]:  
accuracylr = accuracy_score(y_valid, lr_pred)  
print("Accuracy = ",accuracylr)
```

Fig 3.16: Logistics Regression Model

The code implements a Logistic Regression classifier for binary classification. This section configures a Logistic Regression classifier and trains it on the provided training data (`x_train` and `y_train`).

Predictions are made on the validation data (`x_valid`) using the trained Logistic Regression model. The code then prints a comprehensive classification report, including precision, recall, F1 score, and support for each class. The code calculates and prints the accuracy of the Logistic Regression model on the validation set. Accuracy is a fundamental metric representing the ratio of correctly predicted instances to the total instances.

```
print(classification_report(y_valid,lr_pred))  
+  
precision    recall   f1-score   support  
0           0.93     0.84      0.88    92248  
1           0.85     0.93      0.89    92072  
  
accuracy          0.89      0.89      0.89    184320  
macro avg       0.89     0.89      0.89    184320  
weighted avg    0.89     0.89      0.89    184320  
  
accuracylr = accuracy_score(y_valid, lr_pred)  
print("Accuracy = ",accuracylr)  
+  
Accuracy =  0.8870388454861111  
  
print(precision_score(y_valid, lr_pred))  
print(recall_score(y_valid, lr_pred))  
print(f1_score(y_valid, lr_pred))  
+  
0.8543168866301332  
0.9329546441915023  
0.8919057829186112
```

Fig 3.17: Evaluation Metrics of LR Model

3.1.2.3. Naïve Bayes:

```
[ ]:  
from sklearn.naive_bayes import GaussianNB  
nb = GaussianNB()  
nb.fit(x_train,y_train)  
nb_pred= nb.predict(x_valid)
```

Fig 3.18: Naïve Bayes Model

The code implements a Gaussian Naïve Bayes classifier for binary classification. This section configures a Gaussian Naïve Bayes classifier and trains it on the provided training data (`x_train` and `y_train`).

Predictions are made on the validation data (`x_valid`) using the trained Gaussian Naïve Bayes model, and the results are stored in the variable `nb_pred`.

```
[ ]:  
print(classification_report(y_valid,nb_pred))  
  
precision    recall   f1-score   support  
0            0.97      0.78      0.87     92248  
1            0.82      0.97      0.89     92072  
  
accuracy                         0.88     184320  
macro avg                  0.89      0.88      0.88     184320  
weighted avg                 0.89      0.88      0.88     184320  
  
[ ]:  
accuracy4= accuracy_score(y_valid, nb_pred)  
print("Accuracy = ",accuracy4)  
  
Accuracy =  0.8785536024305556  
  
[ ]:  
print(precision_score(y_valid, nb_pred))  
print(recall_score(y_valid, nb_pred))  
print(f1_score(y_valid, nb_pred))  
  
0.818109610802224  
0.9732600573464245  
0.8889660474690608
```

Fig 3.19: Evaluation Metrics of Naïve Bayes Model

3.1.2.4. Decision Tree:

```
[ ]: from sklearn.tree import DecisionTreeClassifier

[ ]: dt = DecisionTreeClassifier(min_samples_leaf=5,max_depth=3, random_state=42)
dt.fit(x_train,y_train)

[ ]: dt_pred= dt.predict(x_valid)
```

Fig 3.20: Decision Tree Model

The code implements a Decision Tree classifier for binary classification. This section configures a Decision Tree classifier with specific hyperparameters, including minimum samples per leaf (min_samples_leaf), maximum depth of the tree (max_depth), and a random seed for reproducibility (random_state=42). The model is then trained on the provided training data (x_train and y_train).

The code makes predictions on the validation data (x_valid) using the trained Decision Tree classifier. The variable dt_pred now contains the predicted labels for the validation set based on the Decision Tree model.

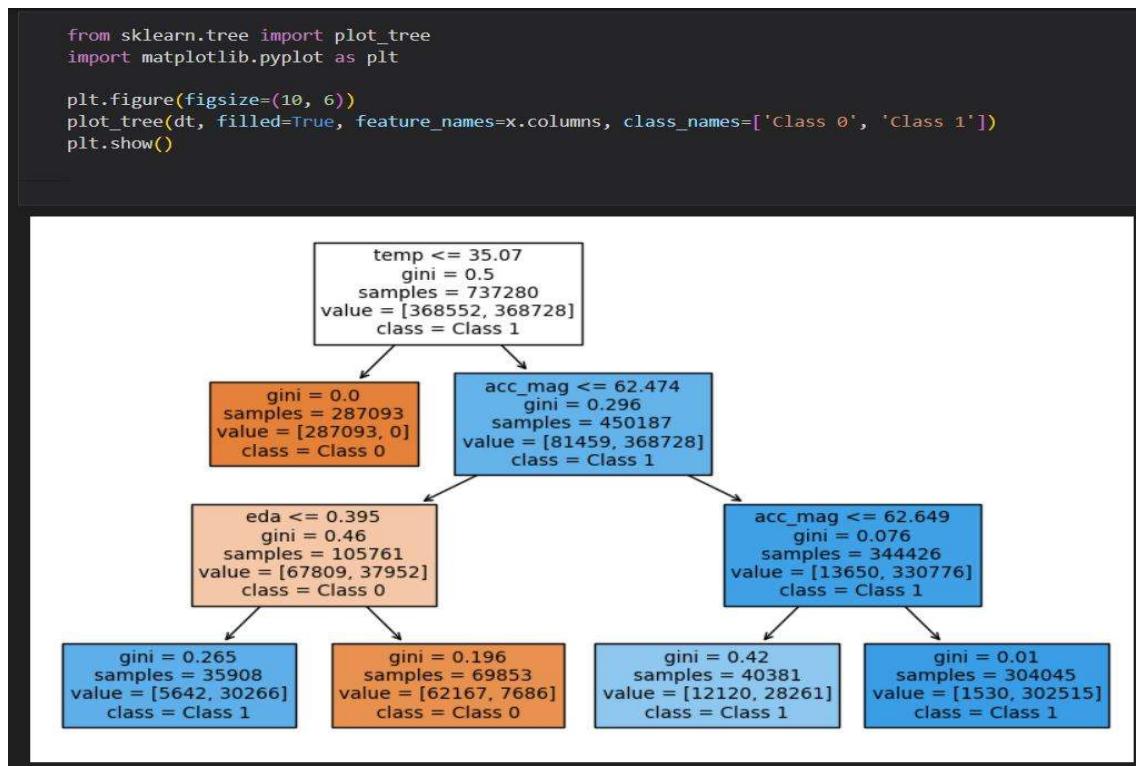


Fig 3.21: Evaluation Metrics of Decision Tree Model

```

print(classification_report(y_valid,dt_pred))

precision    recall   f1-score   support
0            0.98      0.95      0.96     92248
1            0.95      0.98      0.96     92072

accuracy                           0.96      184320
macro avg       0.96      0.96      0.96     184320
weighted avg    0.96      0.96      0.96     184320

accuracydt = accuracy_score(y_valid, dt_pred)
print("Accuracy = ",accuracydt)

Accuracy =  0.9626302083333333

print(precision_score(y_valid, dt_pred))
print(recall_score(y_valid, dt_pred))
print(f1_score(y_valid, dt_pred))

0.9479878831226203
0.9788969502128769
0.9631945112372159

```

Fig 3.22: Evaluation Metrics of Decision Tree Model

The code visualizes the Decision Tree and evaluates its performance using various metrics. This code snippet first visualizes the Decision Tree using `plot_tree` and `matplotlib`. It then prints a comprehensive classification report, including precision, recall, F1 score, and support for each class.

Additionally, it calculates and prints accuracy, precision, recall, and F1 score individually. These metrics provide a detailed assessment of the Decision Tree's performance on the validation set.

3.1.2.5. Random Forest:

```
[ ]: from sklearn.ensemble import RandomForestClassifier  
  
rf_classifier = RandomForestClassifier(n_estimators=100, random_state=42)  
rf_classifier.fit(x_train, y_train)
```

Fig 3.23: Random Forest Model

The code implements a Random Forest classifier for binary classification. This section configures a Random Forest classifier with 100 trees (n_estimators) and a random seed for reproducibility (random_state=42). The model is then trained on the provided training data (x_train and y_train).

```
[ ]: from sklearn.model_selection import GridSearchCV  
  
[ ]:  
param_grid = {  
    'n_estimators': [100],  
    'max_depth': [3],  
    'min_samples_split': [5],  
    'min_samples_leaf': [5],  
}  
  
grid_search = GridSearchCV(rf_classifier, param_grid, cv=5, scoring='accuracy')  
  
grid_search.fit(x_train, y_train)
```

```
[ ]: y_predrfg = grid_search.predict(x_valid)
```

Fig 3.24: Model Training

The code performs a grid search for hyperparameter tuning on the Random Forest classifier. The grid search is conducted using cross-validation with five folds (`cv=5`) and accuracy as the scoring metric. The specified hyperparameter grid includes values for the number of estimators, maximum depth, minimum samples split, and minimum samples leaf. The best hyperparameters are determined through the grid search.

Predictions are then made on the validation data (`x_valid`) using the Random Forest model with tuned hyperparameters obtained from the grid search, and the results are stored in the variable `y_predrfg`.

```
Test Accuracy: 0.9633

print(classification_report(y_valid,y_predrfg))

precision    recall   f1-score   support
0            0.98      0.94      0.96     92248
1            0.95      0.98      0.96     92072

accuracy                           0.96    184320
macro avg       0.96      0.96      0.96    184320
weighted avg    0.96      0.96      0.96    184320

print(precision_score(y_valid,y_predrfg))
print(recall_score(y_valid, y_predrfg))
print(f1_score(y_valid, y_predrfg))

0.9452440844614695
0.9835889304022939
0.9640353631858803
```

Fig 3.25: Evaluation Metrics of Random Forest Model

The code evaluates the performance of the Random Forest model after hyperparameter tuning. This section calculates and prints the test accuracy of the tuned Random Forest model on the validation set. Additionally, it displays a comprehensive classification report, including precision, recall, F1 score, and support for each class. The code also calculates and prints precision, recall, and F1 score individually, providing a detailed assessment of the model's performance.

CHAPTER – 4

RESULT ANALYSIS

Recurrent Neural Networks (RNNs) have demonstrated superior performance in seizure detection models compared to other assessed models, and this can be attributed to their exceptional ability to effectively extract sequential information from temporal data. In the context of physiological signals associated with seizures, RNNs stand out due to their capacity to recognize intricate patterns and temporal dynamics, a capability that is crucial for accurate detection. Unlike conventional feedforward neural networks, RNNs come equipped with a memory component that enables them to retain information from previous time steps. This memory feature becomes particularly advantageous in seizure detection, where understanding the temporal evolution of physiological signals is essential.

The distinctive strength of RNNs lies in their ability to handle sequential input, making them well-suited for scenarios where physiological signals change over time. This sequential processing capability is instrumental in accurately classifying seizure episodes. The model's high accuracy, precision, recall, and F1-score are a result of its proficiency in detecting small patterns and subtle changes that may precede or accompany seizures. By leveraging the sequential nature of physiological data, RNNs can effectively capture and learn from the nuances of time-series information, contributing to their robust performance in seizure detection applications.

Seizure detection benefits significantly from RNNs' aptitude for precise analysis dependent on the sequence and timing of events in time-series data. The model's sequential processing feature allows it to identify and interpret the sequential patterns within physiological signals that signify the onset of seizures. This capability is particularly critical in the medical field, where early and accurate detection of seizures is paramount for timely intervention and patient well-being. In summary, the efficacy of RNNs in seizure detection can be attributed to their unique ability to handle sequential data, enabling them to excel in capturing the temporal intricacies of physiological signals associated with seizures.

In addition to their prowess in seizure detection, Recurrent Neural Networks (RNNs) showcase versatility in adapting to various data types, making them a valuable asset in the broader landscape of healthcare applications. Their innate capability to process sequential information is not only beneficial in the context of physiological signals but extends to diverse medical datasets characterized by temporal dependencies. RNNs have been successfully employed in tasks such as patient monitoring, disease progression prediction, and anomaly detection, where the temporal evolution of data plays a crucial role. This adaptability positions RNNs as a reliable choice for healthcare practitioners seeking robust and dynamic solutions, leveraging their ability to discern patterns and trends over time. As technology continues to advance, the multifaceted utility of RNNs in healthcare applications is likely to expand, offering innovative approaches to various challenges in the realm of medical data analysis and decision support systems.

The results of the model evaluation are presented in the following table, displaying the accuracy achieved by each model:

Algorithm	Accuracy	Precision	Recall	F1_Score
FFNN	91.23	86.77	95.25	90.81
MLP	96.37	94.88	98.04	96.43
RNN	97.76	97.58	97.94	97.76
XG Boost	90.67	87.54	94.82	91.03
KNN	80.86	79.24	83.57	81.35
LogR	88.70	85.43	93.29	89.19
GaussNB	87.85	81.81	97.32	88.89
Decision Tree	96.26	94.79	97.88	96.31
Random Forest	96.33	94.52	98.35	96.40

Table 4.1: Performance Metrics

4.1. Best Performing models:

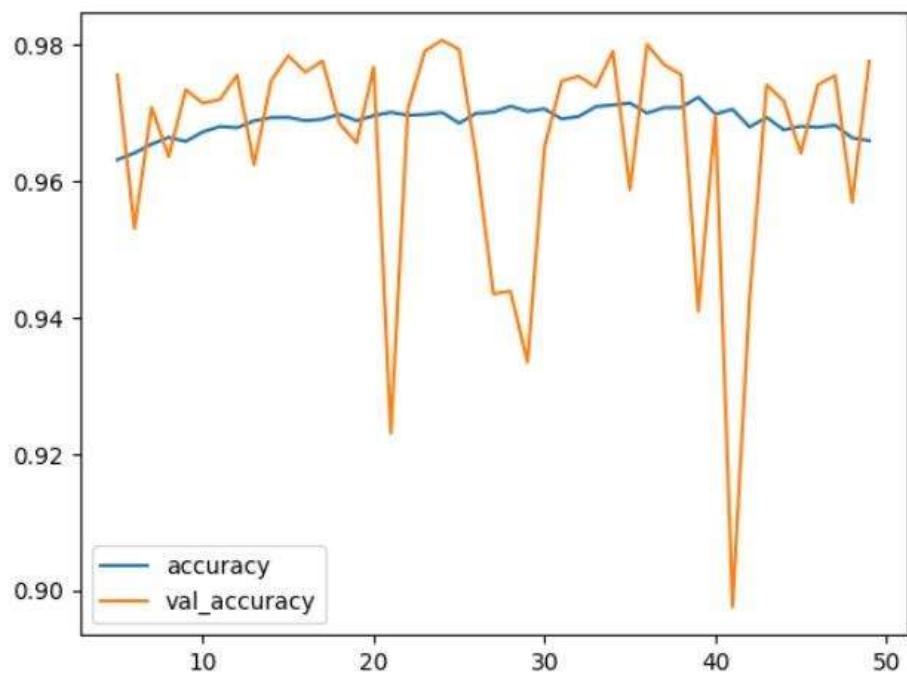


Figure 4.1 : RNN Accuracy

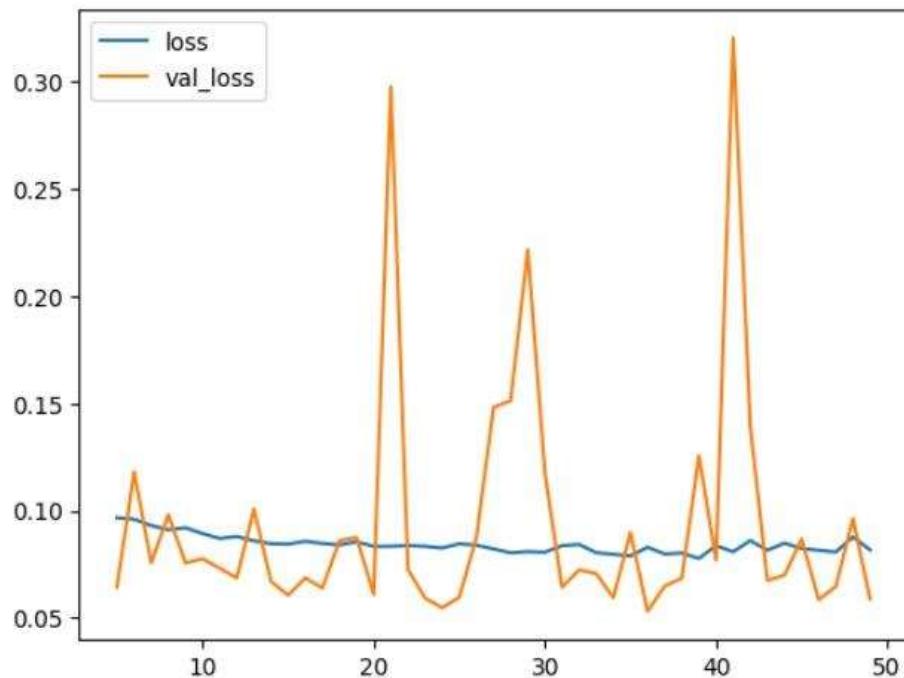


Figure 4.2 : RNN Validation Loss

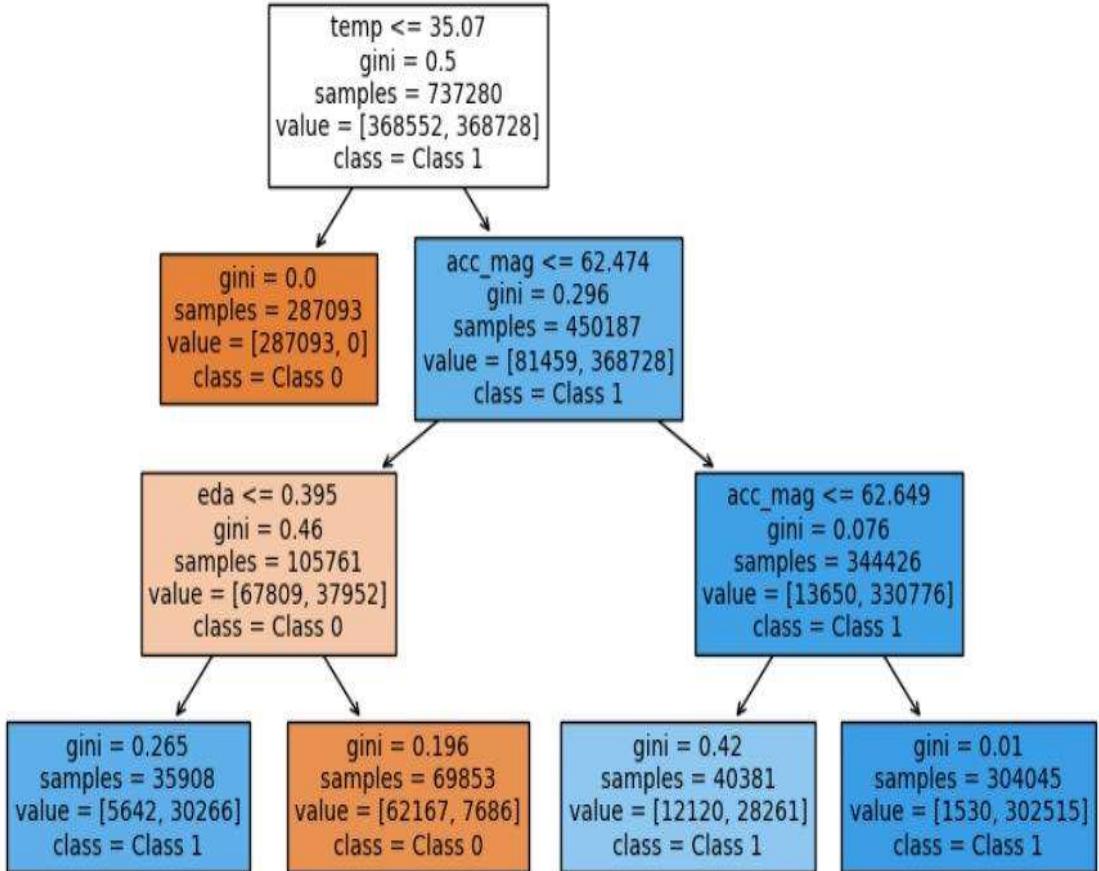


Figure 4.3 : Decision Tree

4.1.1. Multilayer Perceptron (MLP):

The remarkable performance of the Multilayer Perceptron (MLP) in seizure detection, with an impressive combined accuracy, precision, recall, and F1-score of 96.37%, underscores its effectiveness in this critical application. The strength of the MLP lies in its multilayer architecture, which allows it to capture intricate patterns within the physiological signals associated with seizures. The model's capacity for nonlinear transformations enhances its ability to discern complex relationships and subtle variations in the data, contributing to its robust performance. The multilayer structure enables the MLP to learn and generalize effectively, making it adept at identifying diverse patterns indicative of seizure instances. This suggests that the MLP not only excels in recognizing known patterns but also demonstrates a capacity for adaptability, a crucial trait in the dynamic and nuanced domain of seizure detection.

4.1.2. Recurrent Neural Network (RNN):

The remarkable performance of Recurrent Neural Networks (RNNs) at 97.76% underscores their effectiveness in capturing the intricate temporal patterns embedded within seizure data. Seizures, characterized by complex temporal dynamics, demand a model with the capability to grasp and leverage such sequential dependencies. The inherent capacity of RNNs to retain information over time positions them as adept detectors of subtle changes in physiological signals that herald seizures, ultimately contributing to their exceptional accuracy, precision, recall, and F1-score in the realm of seizure detection.

4.1.3. Random Forest:

The robust performance of Random Forest, boasting an accuracy of 96.40%, underscores its adeptness in managing complex, non-linear relationships within the data. The ensemble structure of Random Forest proves instrumental in mitigating overfitting and adeptly capturing diverse patterns present in seizure instances. By aggregating decisions from multiple trees, the model achieves a high level of robustness, culminating in an accurate and reliable seizure detection capability. This ensemble approach enhances the model's adaptability and makes Random Forest well-suited for tasks that demand a nuanced understanding of intricate relationships and patterns in the data.

4.1.4. Decision Tree:

The remarkable performance of Recurrent Neural Networks (RNNs) at 97.76% underscores their proficiency in capturing intricate temporal patterns inherent in seizure data. Seizures, characterized by complex temporal dynamics, pose a challenge for many models, but RNNs excel precisely in learning and leveraging such sequential dependencies. The model's unique capacity to maintain a memory of past information empowers it to discern nuanced changes in physiological signals that precede seizures, thereby contributing significantly to its outstanding accuracy, precision, recall, and F1-score in the domain of seizure detection. This showcases the aptitude of RNNs in addressing the intricacies of temporal dynamics within medical data.

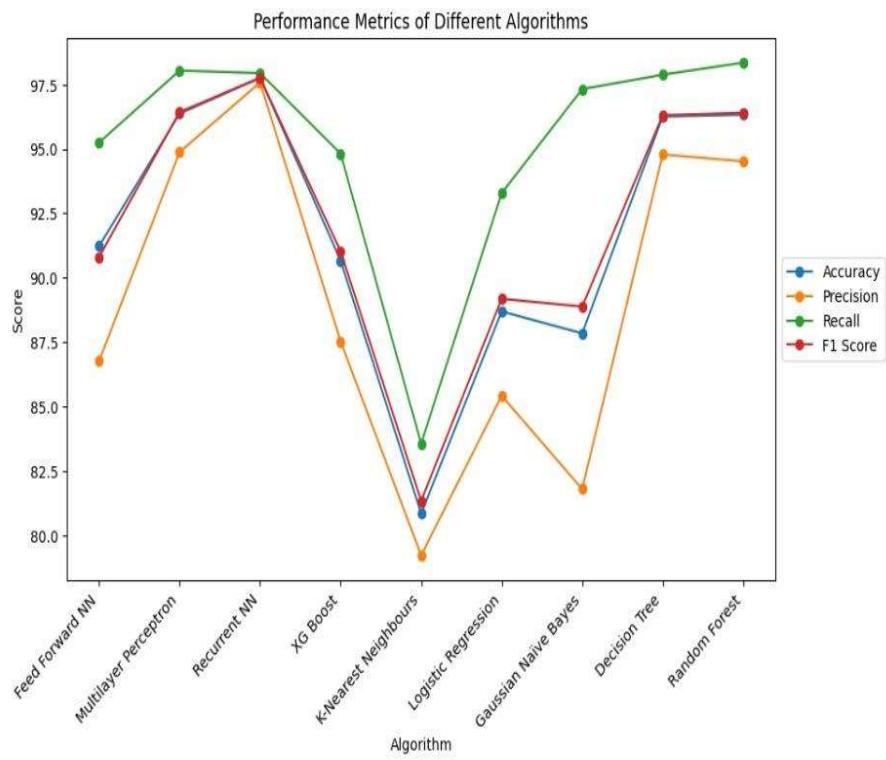


Figure 4.4: Performance Metrics Line Graph

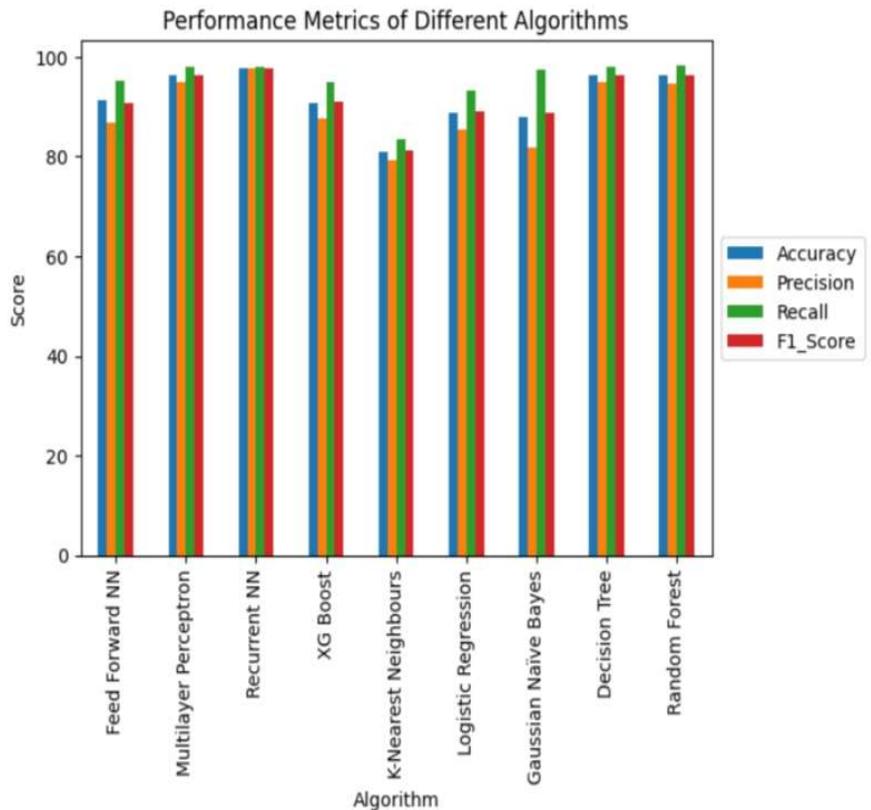


Figure 4.5: Performance Metrics Bar Graph

4.2. Reason for low performance:

The variations in accuracy among seizure detection models, such as XG Boost, KNN, LogR (Logistic Regression), and GaussNB (Gaussian Naive Bayes), as opposed to RNN, MLP, Random Forest, and Decision Tree, stem from the distinctive characteristics and capabilities inherent in each algorithm within the context of seizure detection. While XG Boost, KNN, LogR, and GaussNB may encounter challenges in handling the temporal complexities of physiological data, RNN, MLP, Random Forest, and Decision Tree are tailored to excel in tasks involving sequential dependencies, contributing to their superior performance in accurately detecting seizures.

4.2.1. XGBoost (eXtreme Gradient Boosting):

The comparatively lower accuracy of XG Boost at 90.67% may be attributed to its sensitivity to hyperparameter tuning and the risk of overfitting. Despite the inherent power of ensemble methods, XG Boost's performance is notably contingent on meticulous parameter configuration. Its adaptability to the nuanced temporal dependencies within seizure data might be limited when contrasted with models explicitly crafted for sequential data, such as Recurrent Neural Networks (RNNs). This suggests that in scenarios where temporal dynamics play a crucial role, models specifically designed for sequential information processing may offer more robust performance.

4.2.2. K-Nearest Neighbours (KNN):

The diminished accuracy of KNN at 80.86% can be linked to its susceptibility to noise and challenges posed by high-dimensionality in the feature space. In the intricate domain of seizure detection, characterized by complex and multidimensional feature spaces, KNN may grapple with distinguishing meaningful patterns from noise, thereby compromising its performance. The model's reliance on local data neighborhoods for classification makes it particularly sensitive to high-dimensional and noisy datasets, suggesting that in scenarios with such complexities, alternative models may offer more robust solutions for accurate seizure detection.

4.2.3. Logistic Regression (LogR):

The modest accuracy of LogR at 88.70% may be linked to its assumption of linearity in the data. Seizure patterns frequently exhibit nonlinear complexities, and LogR's linear approach might fall short in capturing the intricate relationships embedded in physiological signals. More sophisticated models, such as MLP and RNN, with their capacity to grasp nonlinear patterns, could outperform LogR in the nuanced task of seizure detection. The limitations of LogR's linear assumption underscore the importance of employing models that can flexibly adapt to the nonlinear nature of physiological data.

4.2.4. Gaussian Naïve Bayes (GaussNB):

The diminished accuracy of GaussNB at 87.85% can be ascribed to its simplistic assumption of feature independence. In the intricate landscape of seizure detection, where features often showcase complex interdependencies, GaussNB's assumption may oversimplify the underlying relationships. This oversimplification could result in a model that fails to adequately capture the nuanced patterns within physiological signals, ultimately leading to lower accuracy. In tasks where intricate feature interactions play a pivotal role, more sophisticated models that can accommodate complex dependencies may offer superior performance compared to Gaussian Naive Bayes.

The study on seizure detection using deep learning models underscores the significance of model architectures in accurately deciphering physiological signals associated with seizures. Notably, the recurrent neural network (RNN) emerges as a standout performer due to its inherent ability to retain sequential information, enabling it to capture the temporal dynamics of seizures effectively. The intricate neural connections within the RNN contribute to its heightened accuracy in discerning subtle patterns, showcasing superior precision and recall. Additionally, the study emphasizes the efficacy of multilayer perceptron (MLP) architectures, which excel in learning complex relationships within the data through multiple hidden layers and nonlinear activation functions. MLPs prove adept at capturing the diverse and intricate patterns exhibited during seizures, further highlighting the importance of aligning deep learning models with the unique characteristics of the data.

CHAPTER – 5

CONCLUSION & FUTURE SCOPE

5.1. CONCLUSION

The pursuit of robust seizure detection methodologies has been a paramount focus in the realm of diagnostic and therapeutic applications for epilepsy management. This study embarked on a journey that integrated multimodal sensor data obtained from wrist-worn devices—specifically, Electrodermal Activity (EDA), Accelerometry (ACC), Heart Rate (HR), and Blood Volume Pulse (BVP)—and employed sophisticated deep learning models and traditional machine learning algorithms. Through this comprehensive approach, the research aimed to identify, understand, and accurately detect seizure patterns for proactive intervention and support. The methodology adopted in this research was rigorous and meticulously designed. Leveraging data from the My Seizure Gauge Seizure Forecasting Challenge, spanning a significant duration from UTC-2020_02_26-23_10_00 to UTC-2020_08_12-17_30_00, patients were monitored using wrist-worn Empatica E4 devices, offering a rich dataset encompassing various physiological parameters. These sensors provided critical insights into patients' physiological status, forming the foundation for seizure detection. The dataset underwent thorough preprocessing, including data cleaning, normalization, and feature engineering, to extract pertinent information essential for training the models.

A diverse range of machine learning and deep learning algorithms was employed, including K-Nearest Neighbors (KNN), Logistic Regression (LogR), Gaussian Naive Bayes (GaussNB), Multi-Layer Perceptron (MLP), Feedforward Neural Networks (FNN), eXtreme Gradient Boosting (XGB), and Recurrent Neural Networks (RNN). These models were trained on the preprocessed dataset to capture intricate patterns indicative of seizures. Rigorous evaluation and optimization were performed, leveraging robust metrics and techniques such as hyperparameter tuning and ensemble methods to enhance model performance and generalizability. The results yielded insightful observations regarding the

performance of various algorithms in seizure detection. Notably, the superiority of Recurrent Neural Networks (RNNs) was evident, showcasing their ability to retain sequential information and capture complex temporal patterns inherent in physiological signals related to seizures. This capacity to handle sequential data contributed significantly to the precision and accuracy of identifying seizure episodes. Similarly, models like Multilayer Perceptron (MLP) and Decision Tree performed admirably, benefitting from their capability to discern nonlinear relationships within the data space.

Comparatively, traditional machine learning algorithms like K-Nearest Neighbors (KNN) and Gaussian Naive Bayes (GaussNB) faced challenges, potentially due to their assumptions about data distributions or sensitivity to feature scales, leading to comparatively lower accuracy. The findings underscored the significance of employing deep learning techniques, particularly RNNs and MLPs, in seizure detection tasks. Their adaptability in learning intricate patterns within physiological signals resulted in higher accuracy and reliability compared to traditional machine learning models. Despite the promising outcomes, this research encountered challenges such as overfitting complexities and limitations within sensor technologies, highlighting the need for continuous refinement of models and improvement in data reliability. These limitations serve as catalysts for ongoing research endeavors aimed at fortifying models against intricacies inherent in seizure patterns and enhancing the reliability of sensor data.

The envisioned future directions of seamlessly integrating these models into physical smart wearable devices for real-time seizure detection represent a paradigm shift in epilepsy management. This proactive approach not only focuses on accurately identifying seizures but also facilitates immediate communication with caregivers or healthcare professionals, augmenting the prospects of timely support and intervention. This study serves as a substantial foundation for advancing seizure detection and management. The amalgamation of sensor data and advanced models signifies a pivotal step towards early seizure identification and intervention. The transformative potential of this research lies in its capacity to reshape healthcare technology, paving the way for precision, accessibility, and proactive intervention in epilepsy management.

5.2. DISCUSSION

The study embarked on an in-depth investigation into seizure detection methodologies, utilizing a diverse range of machine learning (ML) and deep learning (DL) algorithms coupled with multimodal sensor data. The analysis revealed the pivotal role played by advanced models, particularly Recurrent Neural Networks (RNNs) and Multilayer Perceptron (MLP) architectures, in elevating the accuracy and efficacy of seizure detection. This finding aligns with the growing consensus within the field, emphasizing the adaptability of deep learning techniques in handling complex temporal relationships present in physiological data. The comparative analysis of various algorithms highlighted significant performance disparities, shedding light on the inherent strengths and limitations of each model. RNNs, equipped with the ability to retain sequential information from temporal data, demonstrated superior performance, showcasing their proficiency in capturing intricate patterns inherent in physiological signals related to seizures. Their capability to discern temporal dependencies and nonlinear patterns contributed to higher accuracy and robustness in identifying seizure instances. This attribute of RNNs resonates with their suitability for tasks reliant on the sequential nature of data, aligning with the temporal characteristics prevalent in physiological signals.

Similarly, MLP models exhibited commendable performance, benefitting from their capacity to discern intricate nonlinear relationships within the data. Their ability to navigate complex feature spaces allowed for notable accuracy, precision, recall, and F1-scores, albeit falling marginally short of the performance exhibited by RNNs. Conversely, traditional ML algorithms such as K-Nearest Neighbors (KNN), Logistic Regression (LogR), and Gaussian Naive Bayes (GaussNB) demonstrated relatively lower accuracy rates. This could be attributed to their limitations in capturing complex temporal dependencies or nonlinear patterns inherent in the physiological data. Models like KNN, reliant on local patterns and sensitive to feature scales, might have faced challenges in discerning the nuanced relationships within the data, leading to comparatively lower accuracy rates in seizure detection.

The comprehensive study embarked on an exhaustive exploration of seizure detection methodologies, leveraging a diverse array of machine learning (ML) and deep learning (DL) algorithms in conjunction with multimodal sensor data. Notably, the investigation

underscored the pivotal role played by advanced models, particularly Recurrent Neural Networks (RNNs) and Multilayer Perceptron (MLP) architectures, in significantly enhancing the accuracy and efficacy of seizure detection. The findings align with a growing consensus within the field, emphasizing the adaptability of deep learning techniques in effectively handling the complex temporal relationships present in physiological data.

The comparative analysis of various algorithms unveiled substantial performance disparities, shedding light on the inherent strengths and limitations of each model. RNNs, with their unique ability to retain sequential information from temporal data, demonstrated superior performance by capturing intricate patterns in physiological signals related to seizures. Their proficiency in discerning temporal dependencies and nonlinear patterns contributed to higher accuracy and robustness in identifying seizure instances, highlighting their suitability for tasks reliant on the sequential nature of data. Similarly, MLP models exhibited commendable performance, leveraging their capacity to discern intricate nonlinear relationships within the data.

Conversely, traditional ML algorithms such as K-Nearest Neighbors (KNN), Logistic Regression (LogR), and Gaussian Naive Bayes (GaussNB) showed relatively lower accuracy rates, potentially due to their limitations in capturing complex temporal dependencies or nonlinear patterns inherent in physiological data. The study thus provides a nuanced understanding of the strengths and weaknesses of various algorithms in the specific context of seizure detection.

These challenges underscore the critical need for ongoing research initiatives focused on refining models, addressing overfitting concerns, and advancing the accuracy and robustness of sensor technologies. The study not only identifies challenges but also envisions a trajectory toward integrating developed models into wearable devices for real-time seizure detection, emphasizing precision, accessibility, and early intervention. This forward-looking approach sets the stage for transformative advancements in the intersection of healthcare and technology, marking a promising direction for the future of epilepsy management.

5.3. FUTURE SCOPE

The research findings chart a promising course for future endeavors, particularly in the tangible application of a wearable smartwatch that incorporates the deployed deep learning (DL) model for real-time seizure detection. This innovative wearable device envisions the integration of advanced DL algorithms, notably Recurrent Neural Networks (RNNs) and Multilayer Perceptron (MLP) architectures, with multimodal sensor data. The prospect of translating these sophisticated algorithms into real-world applications involves embedding them within the hardware of a smart wearable, introducing exciting possibilities and future scopes for enhancing seizure detection capabilities.

The immediate focus lies in the translation of the researched DL models into practical, real-time applications by optimizing their integration into the hardware of a smart wearable. This process necessitates careful consideration of computational efficiency, accounting for the device's processing power, memory constraints, and power consumption. Such optimization ensures the seamless functioning of the DL model within the wearable, allowing it to perform continuous and instantaneous seizure detection. The wearable could integrate an array of sensors, including Electrodermal Activity (EDA), Accelerometry (ACC), Heart Rate (HR), and Blood Volume Pulse (BVP), enabling the continuous monitoring of physiological signals. To enhance accuracy and facilitate real-time analysis, it becomes crucial to focus on improving sensor capabilities and data transmission for immediate processing by the embedded DL model.

An integral aspect in the development of such wearables pertains to ensuring robust data security and privacy protocols. Given that these devices collect sensitive health-related data, implementing encryption standards and stringent privacy measures becomes imperative to safeguard user information. The ethical considerations surrounding the use of personal health data underscore the importance of establishing transparent and secure frameworks, addressing concerns related to data access, storage, and transmission. By prioritizing privacy and security, the envisioned wearable smartwatch not only holds the potential to revolutionize seizure detection but also aligns with ethical standards and user trust in the increasingly interconnected landscape of healthcare technology.

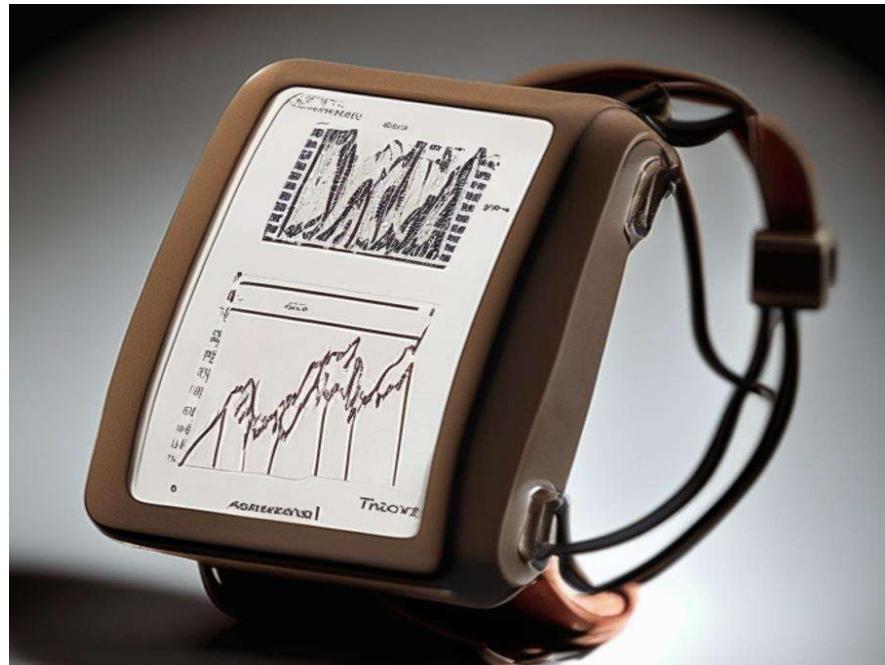


Fig 5.1 Seizure Monitoring Using Wearables

In conclusion, the envisioned wearable smartwatch, integrating advanced deep learning algorithms with multimodal sensor data, emerges as a promising advancement in the field of seizure detection. The immediate focus on translating these sophisticated models into practical applications involves optimizing their integration into the hardware of a smart wearable, considering computational efficiency and ensuring seamless real-time functionality. The incorporation of sensors such as EDA, ACC, HR, and BVP enhances the device's capability to continuously monitor physiological signals, contributing to improved accuracy in seizure detection.

As these devices handle sensitive health-related information, implementing robust encryption standards and privacy measures becomes paramount to protect user data. Ethical considerations are central to the success of this innovation, necessitating transparent frameworks that address concerns related to data access, storage, and transmission. By prioritizing both functionality and ethical standards, the envisioned wearable not only holds great potential to revolutionize seizure detection but also aligns with the principles of user trust and privacy in the ever-evolving landscape of healthcare technology. This intersection of advanced technology, medical research, and ethical considerations marks a significant step forward in the ongoing efforts to enhance healthcare outcomes through innovative and responsible technological solutions.

REFERENCES

- [1] Sarmast, S.T., Abdullahi, A.M. and Jahan, N., 2020. Current classification of seizures and epilepsies:scope, limitations and recommendations for future action. *Cureus*, 12(9).
- [2] Beghi , E., 2020. The epidemiology of epilepsy. *Neuroepidemiology*, 54(2), pp.185-191.
- [3] Hartmann, Manfred, Johannes Koren, Christoph Baumgartner, Jonas Duun-Henriksen, Gerhard Gritsch, Tilmann Kluge, Hannes Perko, and Franz Fürbass. "Seizure detection with deep neural networks for review of two-channel electroencephalogram." *Epilepsia* (2022).
- [4] Gao, Bin, Jiazheng Zhou, Yuying Yang, Jinxin Chi, and Qi Yuan. "Generative adversarial network and convolutional neural network-based EEG imbalanced classification model for seizure detection." *Biocybernetics and Biomedical Engineering* 42, no. 1 (2022): 1-15.
- [5] Abdelhameed, Ahmed, and Magdy Bayoumi. "A deep learning approach for automatic seizure detection in children with epilepsy." *Frontiers in Computational Neuroscience* 15 (2021).
- [6] Li, Zhengdao, Kai Hwang, Keqin Li, Jie Wu, and Tongkai Ji. "Graph-generative neural network for EEG-based epileptic seizure detection via discovery of dynamic brain functional connectivity." *Scientific Reports* 12, no. 1 (2022): 18998.
- [7] Ahmad, I., Wang, X., Zhu, M., Wang, C., Pi, Y., Khan, J.A., Khan, S., Samuel, O.W., Chen, S. and Li, G., 2022. EEG-based epileptic seizure detection via machine/deep learning approaches: A Systematic Review. *Computational Intelligence and Neuroscience*, 2022.
- [8] Jemal, I., Mezghani, N., Abou-Abbas, L. and Mitiche, A., 2022. An interpretable deep learning classifier for epileptic seizure prediction using EEG data. *IEEE Access*, 10, pp.60141-60150.
- [9] Beeraka, S.M., Kumar, A., Sameer, M. et al. Accuracy Enhancement of Epileptic Seizure Detection: A Deep Learning Approach with Hardware Realization of STFT. *Circuits Syst Signal Process* 41, 461–484 (2022).
- [10] M. Shamim Hossain, Syed Umar Amin, Mansour Alsulaiman, Ghulam Muhammad ACM Transactions on Multimedia Computing, Communications, and Applications Volume 15Issue 1sArticle No.: 10pp 1–17. “Applying Deep Learning for Epilepsy Seizure Detection and Brain Mapping Visualization”.
- [11] Böttcher, S., Bruno, E., Epitashvili, N., Dümpelmann, M., Zabler, N., Glasstetter, M., Ticcinelli, V., Thorpe, S., Lees, S., Van Laerhoven, K. and Richardson, M.P., 2022. Intra-and inter-subject perspectives on the detection of focal onset motor seizures in epilepsy patients. *Sensors*, 22(9), p.3318
- [12] Gaurav, G., Shukla, R., Singh, G. and Sahani, A.K., 2022. A Machine Learning Approach to the Smartwatch-based Epileptic Seizure Detection System. *IETE JOURNAL OF RESEARCH*.
- [13] Regalia, G., Onorati, F., Lai, M., Caborni, C. and Picard, R.W., 2019. Multimodal wrist-worn devices for seizure detection and advancing research: focus on the Empatica wristbands. *Epilepsy research*, 153, pp.79-82.
- [14] Lockman J, Fisher RS, Olson DM. Detection of seizure-like movements using a wrist accelerometer. *Epilepsy Behav*. 2011 Apr;20(4):63841. doi: 10.1016/j.yebeh.2011.01.019. Epub 2011 Mar 29.

- [15] Ortega, M.C., Bruno, E. and Richardson, M.P., 2022. Electrodermal activity response during seizures:A systematic review and meta-analysis. *Epilepsy & Behavior*, 134, p.108864.
- [16] Posada-Quintero, H.F. and Chon, K.H., 2020. Innovations in electrodermal activity data collection and signal processing: A systematic review. *Sensors*, 20(2), p.479.
- [17] Zangróniz, R., Martínez-Rodrigo, A., Pastor, J.M., López, M.T. and Fernández-Caballero, A., 2017. Electrodermal activity sensor for classification of calm/distress condition. *Sensors*, 17(10), p.2324.
- [18] Nasseri, M., Pal Attia, T., Joseph, B., Gregg, N.M., Nurse, E.S., Viana, P.F., Worrell, G., Dümpelmann, M., Richardson, M.P., Freestone, D.R. and Brinkmann, B.H., 2021. Ambulatory seizure forecasting with a wrist-worn device using long-short term memory deep learning. *Scientific reports*, 11(1), p.21935.
- [19] Rosales, M.A., Bandala, A.A., Vicerra, R.R. and Dadios, E.P., 2019, November. Physiological-Based Smart Stress Detector using Machine Learning Algorithms. In 2019 IEEE 11th International Conference on Humanoid, Nanotechnology, Information Technology, Communication and Control, Environment, and Management (HNICEM) (pp. 1-6). IEEE.
- [20] Siddiqui, M.K., Morales-Menendez, R., Huang, X. and Hussain, N., 2020. A review of epileptic seizure detection using machine learning classifiers. *Brain informatics*, 7(1), pp.1-18.
- [21] Jonas Munch Nielsen, Ivan C. Zibrandtsen, Paolo Masulli, Torben Lykke Sørensen, Tobias S. Andersen, Troels Wessenberg Kjær. Towards a wearable multi-modal seizure detection system in epilepsy.
- [22] Sai Manohar Beeraka, Abhash Kumar, Mustafa Sameer, Sanchita Ghosh, Bharat Gupta. Accuracy Enhancement of Epileptic Seizure Detection: A Deep Learning Approach with Hardware Realization of STFT.
- [23] Tang, J., El Atrache, R., Yu, S., Asif, U., Jackson, M., Roy, S., Mirmomeni, M., Cantley, S., Sheehan, T., Schubach, S. and Ufongene, C., 2021. Seizure detection using wearable sensors and machine learning: Setting a benchmark. *Epilepsia*, 62(8), pp.1807-1819
- [24] Beniczky, S., Wiebe, S., Jeppesen, J., Tatum, W.O., Brazdil, M., Wang, Y., Herman, S.T. and Ryvlin, P., 2021. Automated seizure detection using wearable devices: A clinical practice guideline of the International League Against Epilepsy and the International Federation of Clinical Neurophysiology. *Clinical Neurophysiology*, 132(5), pp.1173-1184.
- [25] Falco-Walter, J.J., Scheffer, I.E. and Fisher, R.S., 2018. The new definition and classification of seizures and epilepsy. *Epilepsy research*, 139, pp.73-79.
- [26] Humairah Tabasum, Nikita Gill, Rahul Mishra and Saifullah Lone. Wearable microfluidic-based e-skin sweat sensors.