

AI-Driven Artificial Muscle for Cardiac Assist using Hydraulically Amplified Self-Healing Electrostatic Actuators

Issue Statement

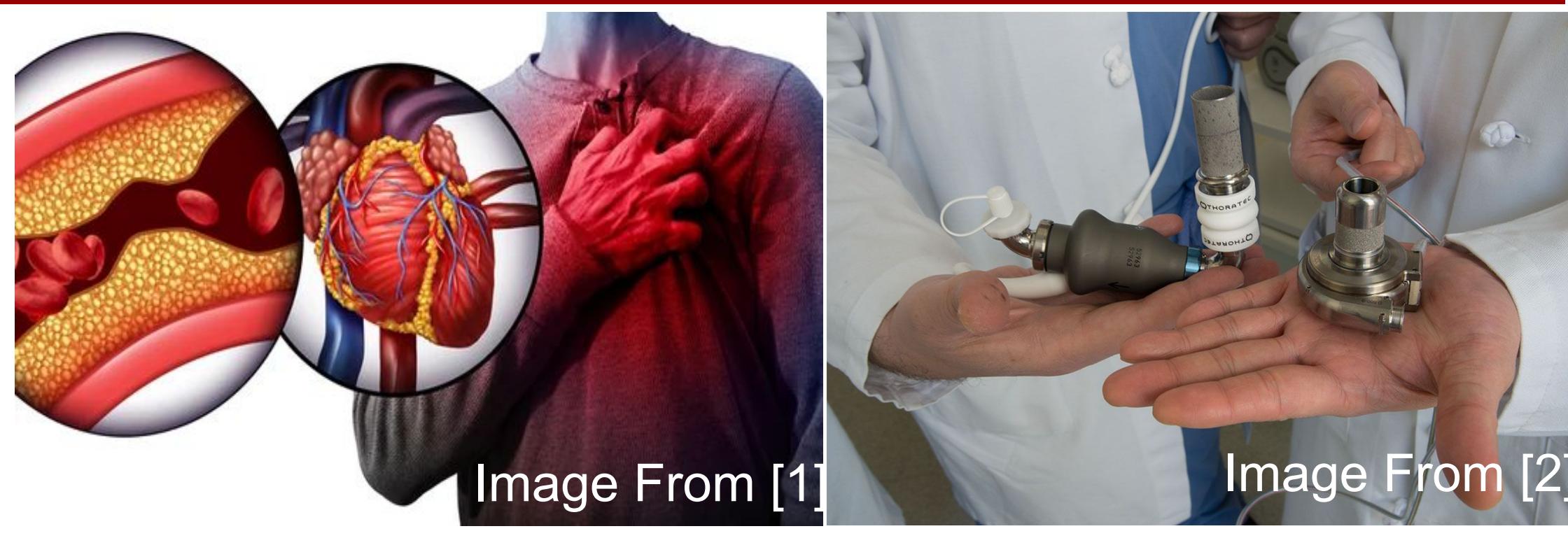


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- Heart Failure (HF) occurs when the heart is unable to pump sufficient blood and oxygen to meet the body's needs, leading to severe health complications.
- It is a major global health crisis, responsible for 17.9 million deaths and affecting 60 million people worldwide each year, making it the leading cause of death worldwide.
- Ventricular Assist Devices (VADs) serve as life-saving interventions for patients ineligible for heart transplants.
- Traditional VADs present significant challenges. These include high rehospitalization rates, mechanical failures, and long-term complications, highlighting the need for improved solutions.

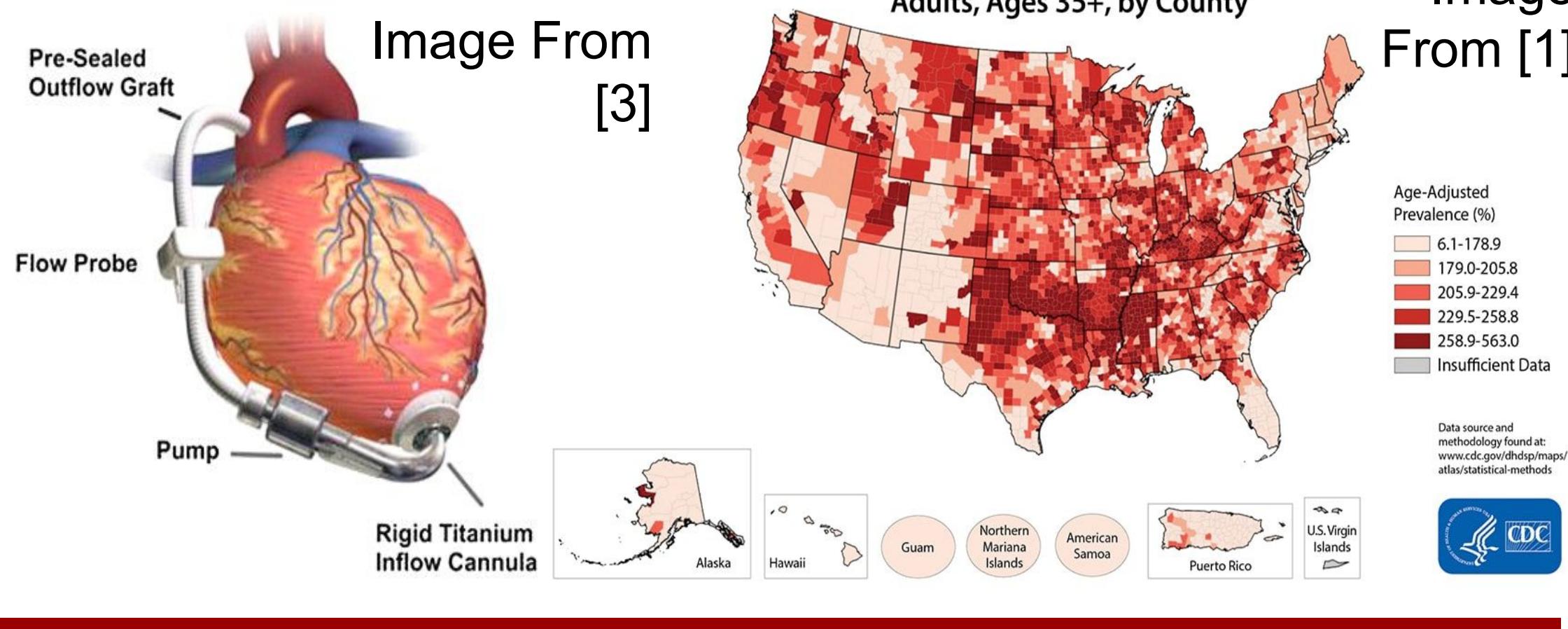
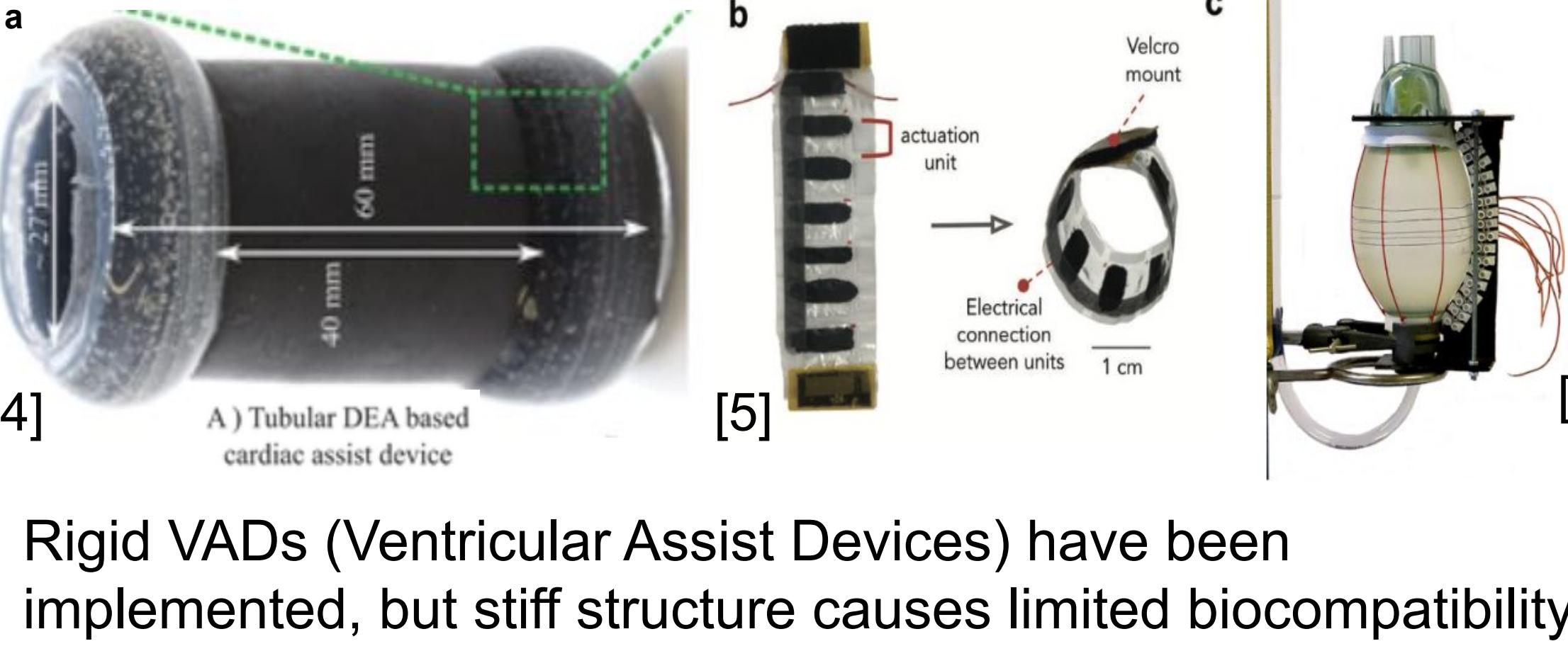


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Previous Research



Rigid VADs (Ventricular Assist Devices) have been implemented, but stiff structure causes limited biocompatibility and high rehospitalization rates (37%) with further complications.

- A. DEA Based VAD - Durability limitations and complete failure after dielectric breakdown. Safety concerns due to actuation geometry with expansion under voltage rather than contraction which risks over-tightening around the heart.
- B. HASEL Based VAD - Lower power output and no real-time control implementation
- C. Pneumatic VAD - Risk of driveline infections due to hydraulic drivelines and poor controllability. Low actuation frequencies.

Research Gap

| | |
|--|---|
| High rehospitalization and complications with rigid VADs | Self-healing, soft HASEL actuators improve biocompatibility |
| Pneumatic drivelines and Limited control of soft devices | Electronically driven HASELs eliminate pneumatic drivelines |
| Poor durability of soft electrically actuated devices | Liquid dielectric allows self-repair after breakdown |
| Complex, nonlinear control of soft actuators | Complex, nonlinear control of soft actuators |
| Fabrication challenges in soft actuator design | Machine learning enables real-time force prediction |
| Lack of real-time control in realistic environments | Tested on phantom heart, integrated pressure sensor |

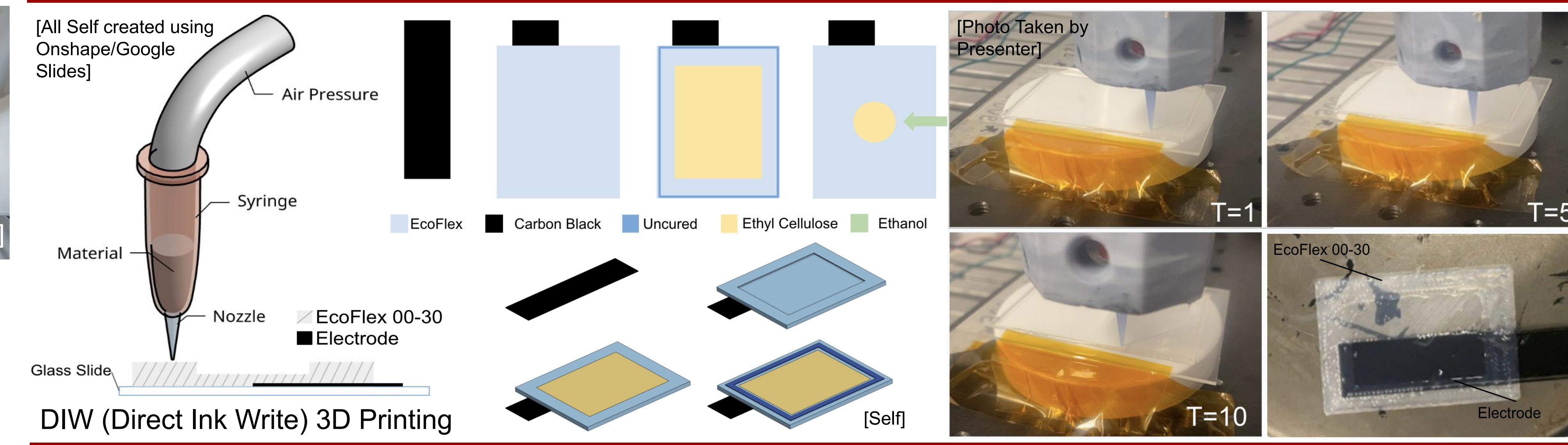
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Design Criteria & Constraints

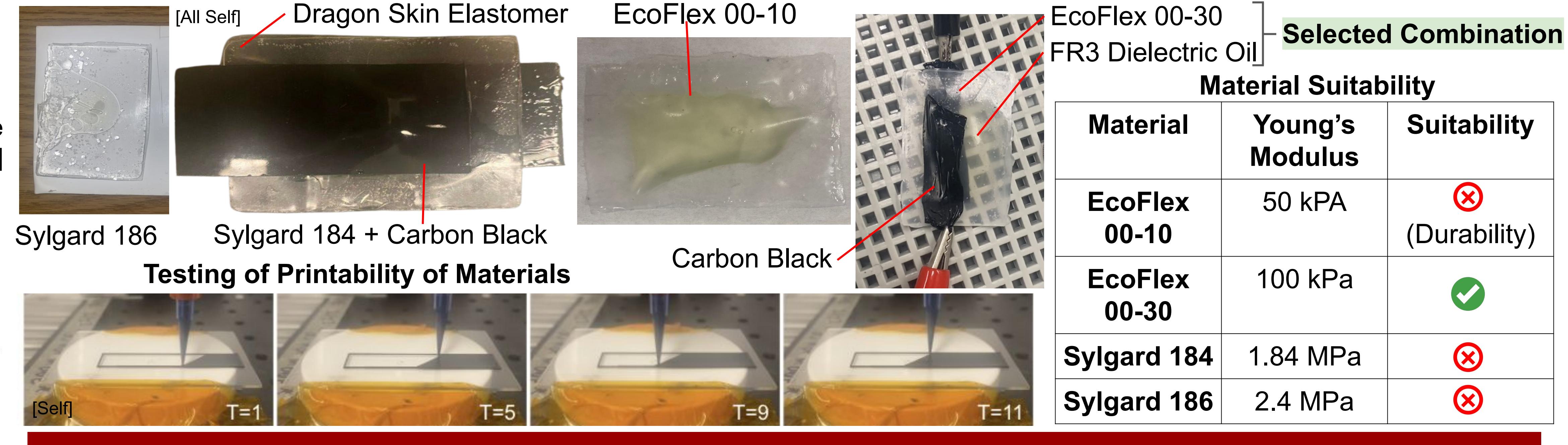
| Metric | Description of Metric | Value |
|----------------|---------------------------------------|----------------|
| Strain | Change in dimensions of the actuator. | >20% |
| Energy | Work generated during actuation | 1 N·mm |
| Directionality | Possible directions of actuation | Unidirectional |
| Frequency | Frequency of Actuation | >=1 Hz |
| Accuracy | Accuracy of control of the actuator | >60% |

[By presenter in Google Slides]

DIW 3D Printing of Ventricular Assist Devices



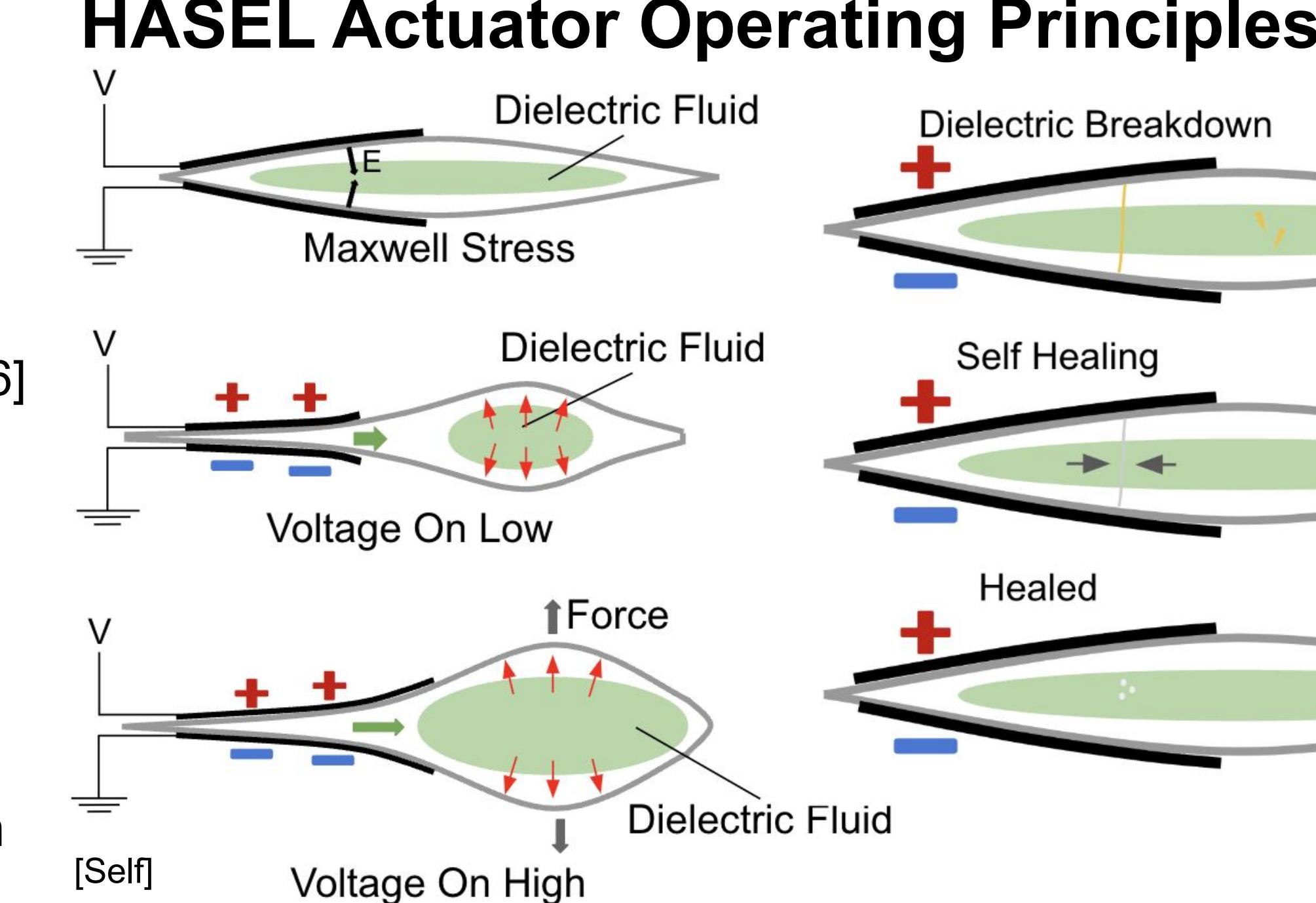
Material Preparation and Experimentation



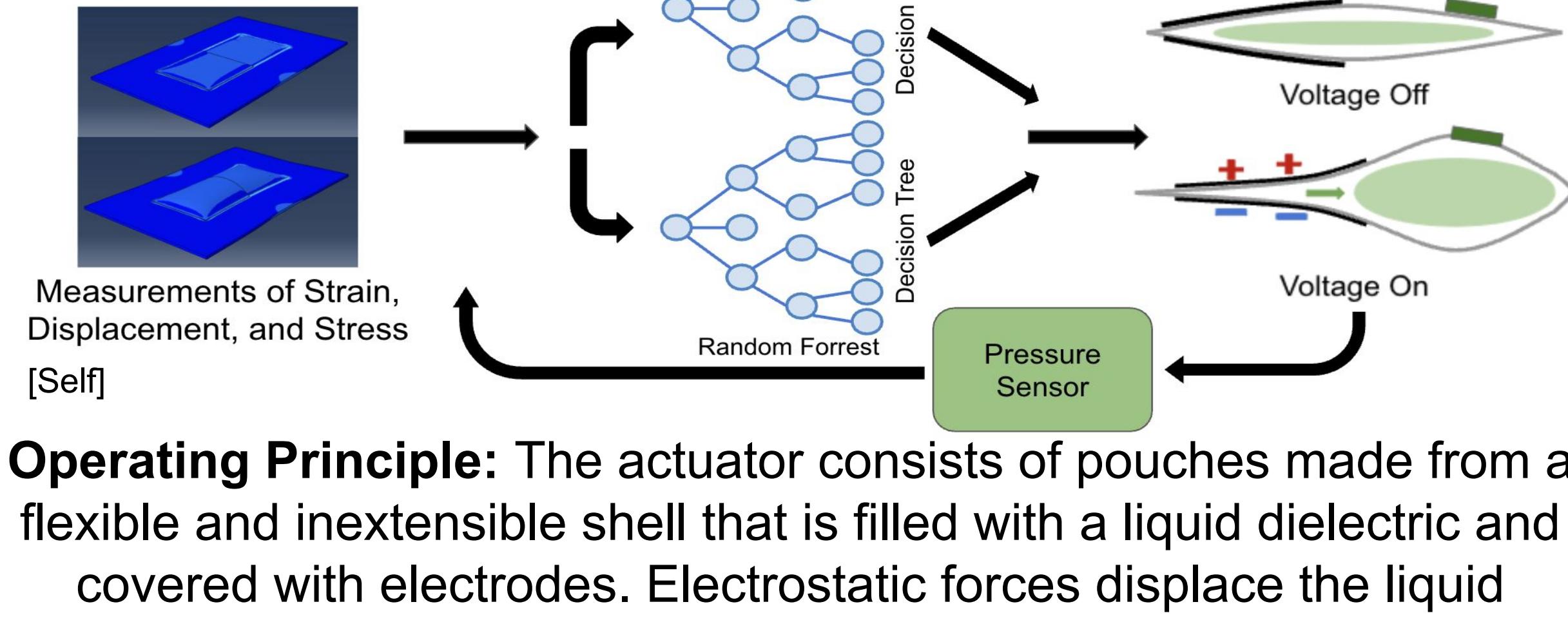
Selected Combination

| Material | Young's Modulus | Suitability |
|---------------|-----------------|----------------|
| EcoFlex 00-10 | 50 kPa | ✗ (Durability) |
| EcoFlex 00-30 | 100 kPa | ✓ |
| Sylgard 184 | 1.84 MPa | ✗ |
| Sylgard 186 | 2.4 MPa | ✗ |

System Design with HASEL Actuators and ML Control

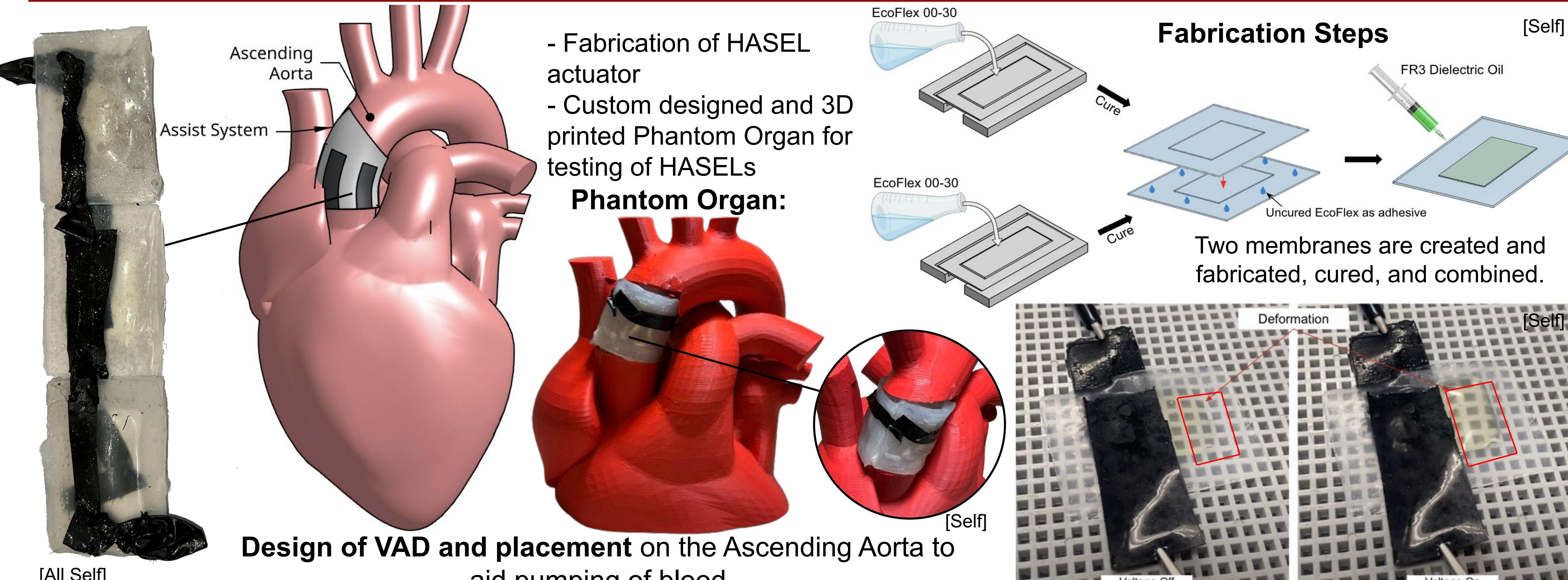


ML Model trained using the FEM data is used to determine the voltage to the HASEL. This determines the output force applied to the heart muscle. A pressure sensor monitors the force applied.

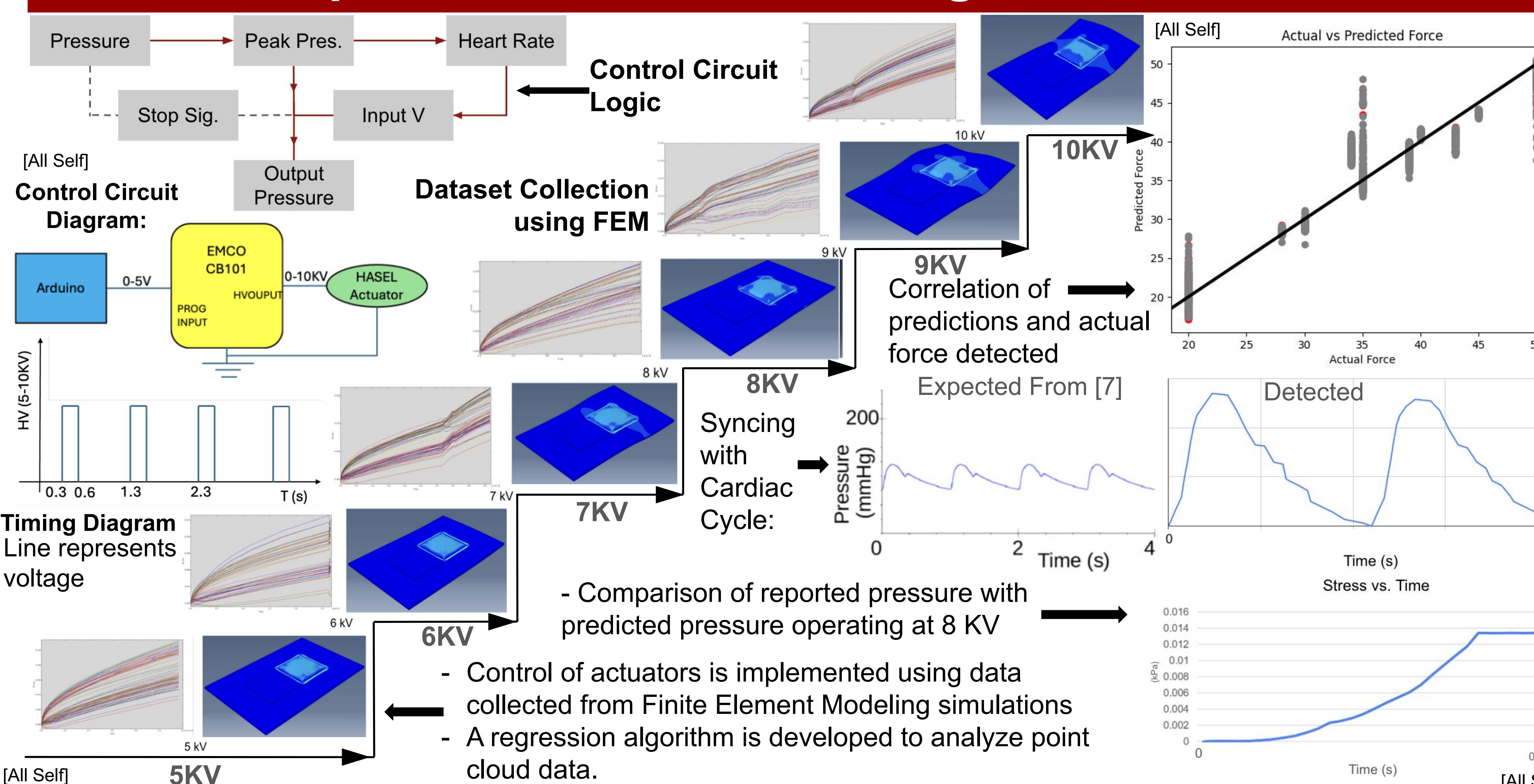


Operating Principle: The actuator consists of pouches made from a flexible and inextensible shell that is filled with a liquid dielectric and covered with electrodes. Electrostatic forces displace the liquid

VAD Design, Fabrication, and Performance



Development of ML Model using FEM Simulations



Theoretical Model

$$p = \epsilon E^2 \text{ where } \epsilon \text{ is the dielectric permittivity of the liquid}$$

$$p \text{ is the electrostatic pressure}$$

$$E \text{ is the electric field } E = \frac{V}{D} \text{ where } V \text{ is applied voltage}$$

$$D \text{ is thickness of dielectric given by}$$

$$\Sigma M = \epsilon E^2 \text{ where } \epsilon \text{ is the dielectric constant}$$

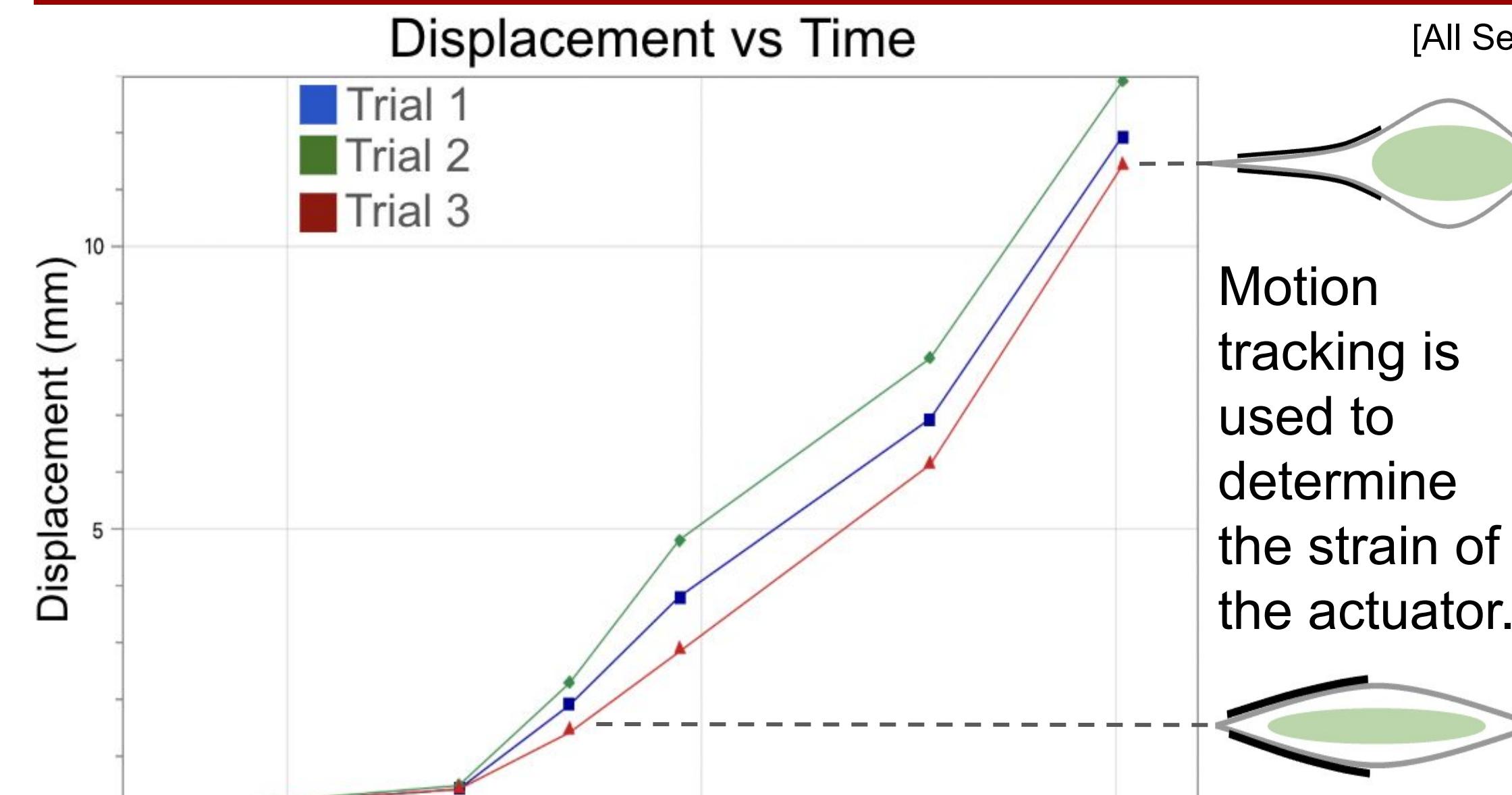
$$\text{Substituting for electric field gives } p = \epsilon \left(\frac{V}{D}\right)^2 \text{ follows}$$

$$\text{which simplifies to the following: } p = \frac{\epsilon V^2}{D^2}$$

$$V = \sqrt{\frac{p D^2}{\epsilon}}$$

Is the relationship used to determine the relationship between the internal pressure of the VAD and the voltage applied for FEM simulations.

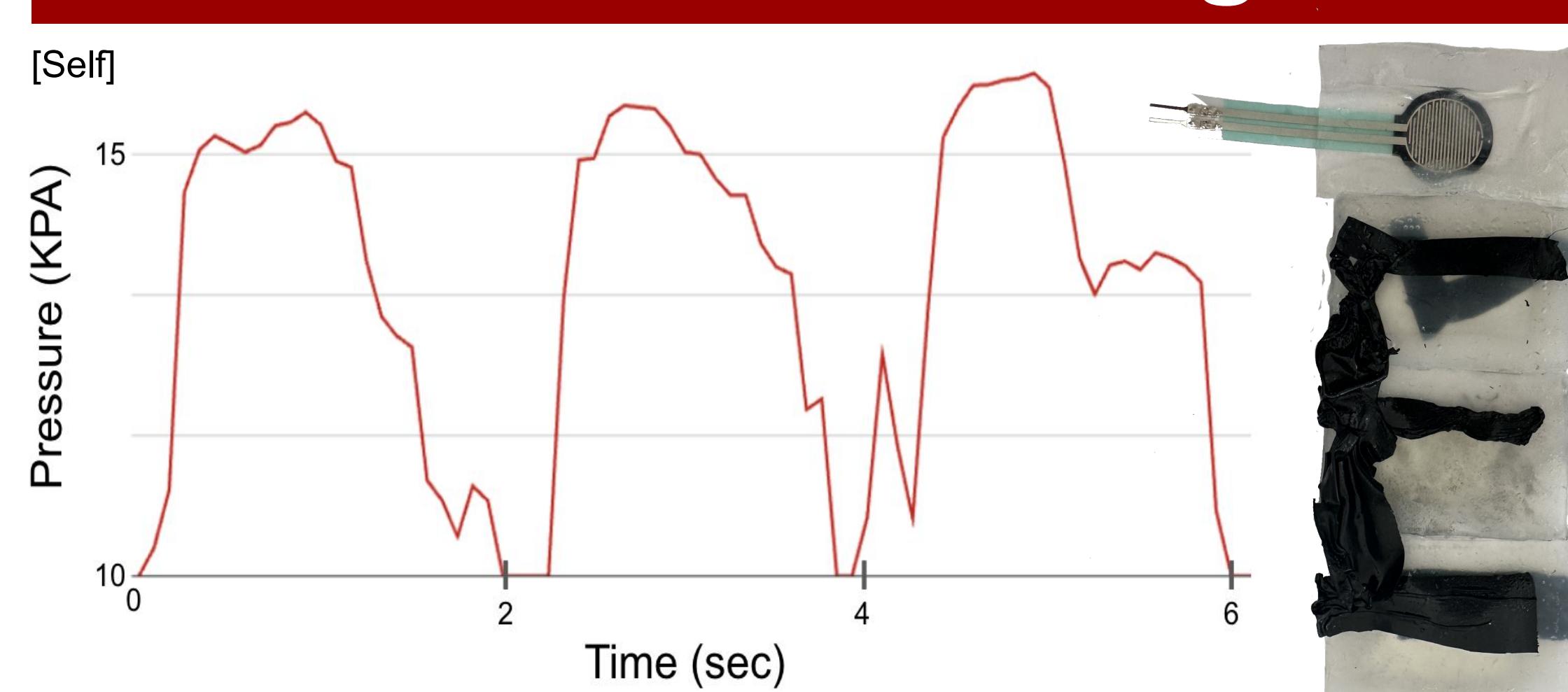
Deformation Characteristics



Assessment of Design Criteria

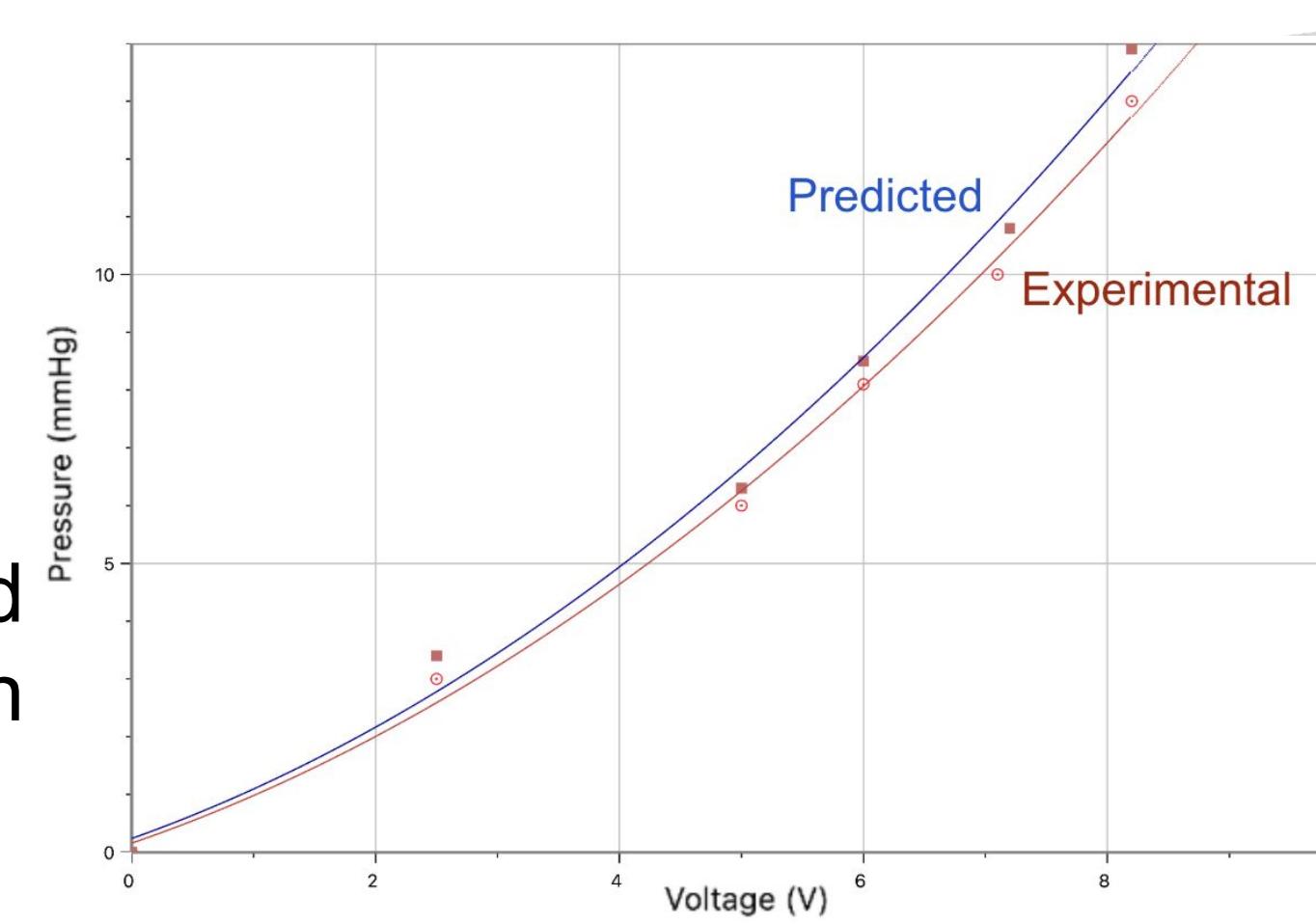
| Strain | 32.9% | Directionality | Unidirectional |
|--------|-----------|----------------|----------------|
| Energy | 5.49 N·mm | Frequency | 3 Hz |

Pressure Sensor Integration



The VAD exhibits consistent pressure output across various trials measured with the pressure sensor.

A force resistive sensor is implemented in the actuator through coating within an elastomer casing.



Conclusions

- Hydraulically Amplified Self-Healing Electrostatic Actuators are implemented for biocompatible, soft ventricular assist devices, reducing complications with rigid solutions and previous soft actuation methods.
- A strain of 32.9% and energy of 5.49 N/mm at an actuation frequency of 2 Hz is achieved for effective cardiac assist.
- An AI algorithm with an accuracy of 91% trained using point cloud data from Finite Element Analysis simulations is developed to provide accurate control predictions of HASEL actuators for use in ventricle assist.
- DIW 3D printing of silicone elastomers is developed for rapid and accurate fabrication of soft elastomer actuators.

Selected References

1. <https://www.cdc.gov/high-blood-pressure/data-research/facts-stats/index.html>
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