

# The Coupleccino Model – Caffeine Effects on Electrically Coupled Retzius Cells using Hodgkin-Huxley Neuron model

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Neu650 Team Project 2024 (Presented on 11.07.2024, supervised by Jutta Kretzberg and Go Ashida)

## Introduction:

The experimental work of this project, alongside other previous findings, show that caffeine may influence the gap junctions of electrically coupled cells. Modifications to the coupling strength of such cells may also lead to variations in the features of the electrophysiological response - such as hyperpolarization amplitude, spike count, spike latency, inter-spike interval (ISI). To gauge the effects of this, a Hodgkin-Huxley (HH) type model was built to simulate coupled Retzius cells.

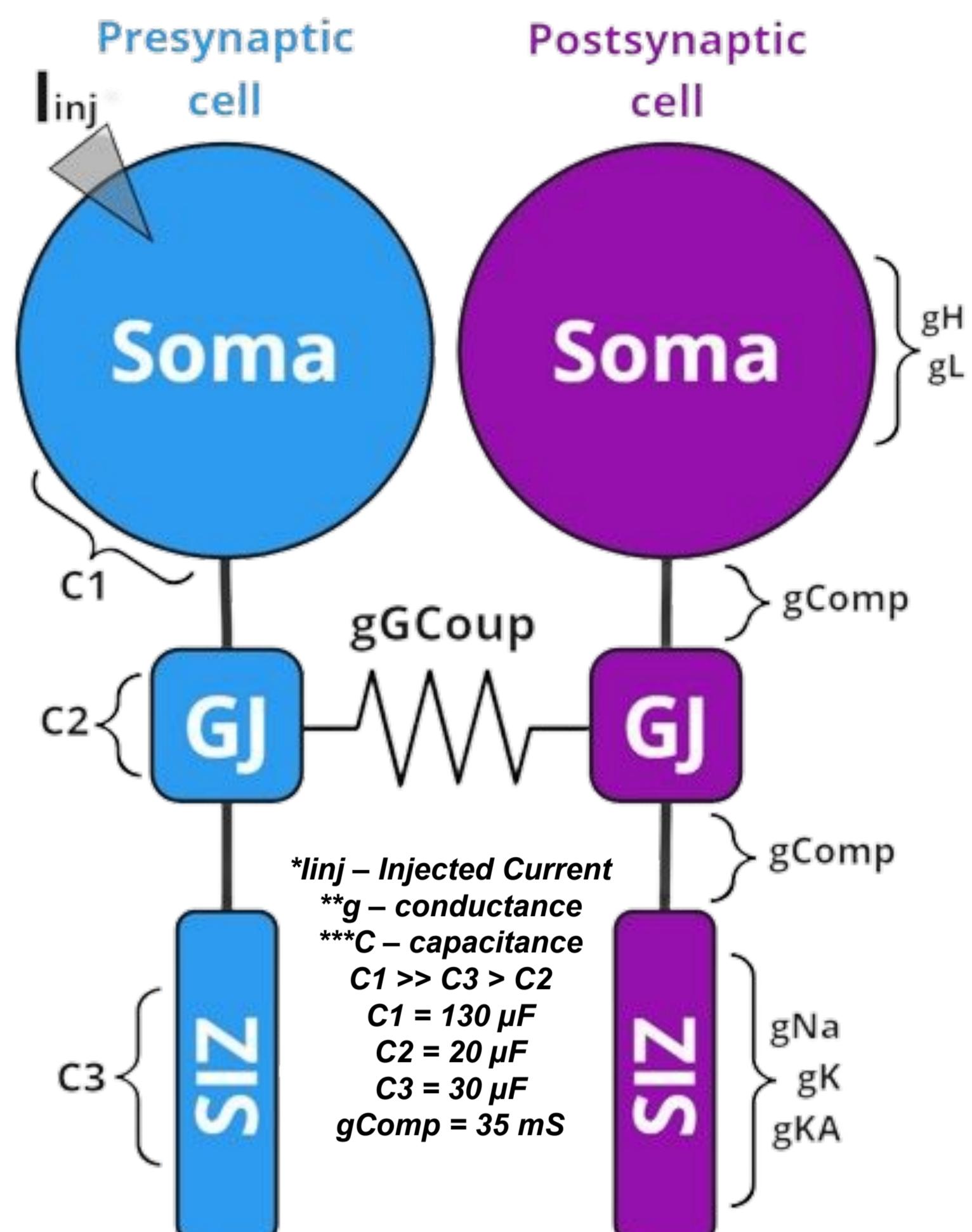
## Methods:

A previous one-cell, two-compartment model was used to build to a three-compartment model, which mathematically represents the soma (compartment 1), gap junction (GJ - compartment 2), and spike initiation zone (SIZ - compartment 3) (figure 1). The soma contains leak and hyperpolarization activated current regulated by  $g_L$  and  $g_H$ , while the spike initiation zone, which is responsible for generating action potentials, has sodium alongside slow and fast potassium activation/inactivation currents, regulated by  $g_A$ ,  $g_K$ ,  $g_{KA}$  respectively. These two identical cells were then combined at the gap junction compartment, and with current ( $I_{inj}$ ) being applied to the soma compartment of the 'presynaptic' cell.

$$I_{GCoup} = g_{GCoup} \times (V_{2Pre} - V_{2Post}) \quad \text{Current between 2 cell compartments regulated by the } g_{GCoup} \text{ parameter}$$
$$\frac{dV_{2Pre}}{dt} = \frac{(I_{C2Pre} - I_{C3Pre} - I_{GCoup})}{C_{2Pre}} \rightarrow \text{Update } V_m \text{ for each time point } \rightarrow V_{2pre(j+1)} = V_{2pre(j)} + \frac{dV_{2Pre}}{dt} \times dt$$
$$\frac{dV_{2Post}}{dt} = \frac{(I_{C2Post} - I_{C3Post} + I_{GCoup})}{C_{2Post}} \rightarrow \text{Update } V_m \text{ for each time point } \rightarrow V_{2post(j+1)} = V_{2post(j)} + \frac{dV_{2Post}}{dt} \times dt$$

Hyperpolarization amplitude, spike count, and latency were fitted to the average range of the experimental datasets of large leech Retzius cells. Passive features were fitted to a 1 s long, -1 nA current based on experimental measurements, while active features were fitted to 1 s long, +1.5 nA current, as it initiated analyzable spike properties.

Figure 1. Graphical representation of HH model for Retzius cells



## Result 1: Parameter Combinations

The simulation aimed to faithfully reproduce key electrophysiological features observed in large leech Retzius cells by strategically adjusting ion channel conductances, capacitances, and activation parameters. Critical combinations included  $g_K$  (58 mS) for precise spike repolarization,  $g_{KA}$  (162 mS) essential for spike frequency adaptation, and  $g_N$  (645 mS) ensuring robust action potential initiation. Additionally,  $g_L$  (10 mS) maintained resting membrane potential stability, while  $g_H$  (1 mS) contributed to membrane potential dynamics during hyperpolarization.

Capacitance parameters, such as  $C_1$  (130  $\mu$ F) influencing soma dynamics, and  $C_2$  (20  $\mu$ F) supporting effective electrical coupling via gap junctions, were crucial. The SIZ capacitance,  $C_3$  (30  $\mu$ F), produced higher spikes at lower values.

Activation times ( $Tau$ ) like  $Tau_H$  (20 ms) for Hyperpolarization channel kinetics and  $Tau_N$  (50 ms) for sodium channel inactivation were pivotal in shaping spike properties. These parameters collectively optimized through simulation, closely mirrored experimental data, capturing membrane potential dynamics, spike features (count, latency, ISI), and responses to current injections accurately.

Certain combinations of activation time parameters can lead to other electrophysiological phenomena, such as chattering and double spikes, which are also noticed in experimental caffeine trials.

*Further parameter calibration could be done over a longer time, or, for example, by an evolutionary classification algorithm.*

Parameter type	Values
Channel Conductance	$g_K = 58 \text{ mS}$ $g_{KA} = 162 \text{ mS}$ $g_N = 645 \text{ mS}$ $g_L = 10 \text{ mS}$ $g_H = 1 \text{ mS}$
Reversal Potentials	$EL = -50 \text{ mV}$ $EH = -20 \text{ mV}$ $EN = +45 \text{ mV}$ $EK = -55 \text{ mV}$
Time Scale in/activation functions	$Tau_H = 20$ $Tau_N = 50$ $Tau_B = 30$ $Tau_Z = 100$
Compartment Conductance	$g_{Comp} = 35 \text{ mS}$ $g_{GCoup} = (5.0:21.5)$

Table 1. Coupled Retzius cell Model Parameters

## Result 2: Comparison to Real Responses

## Result 3: Impact of Coupling Strength

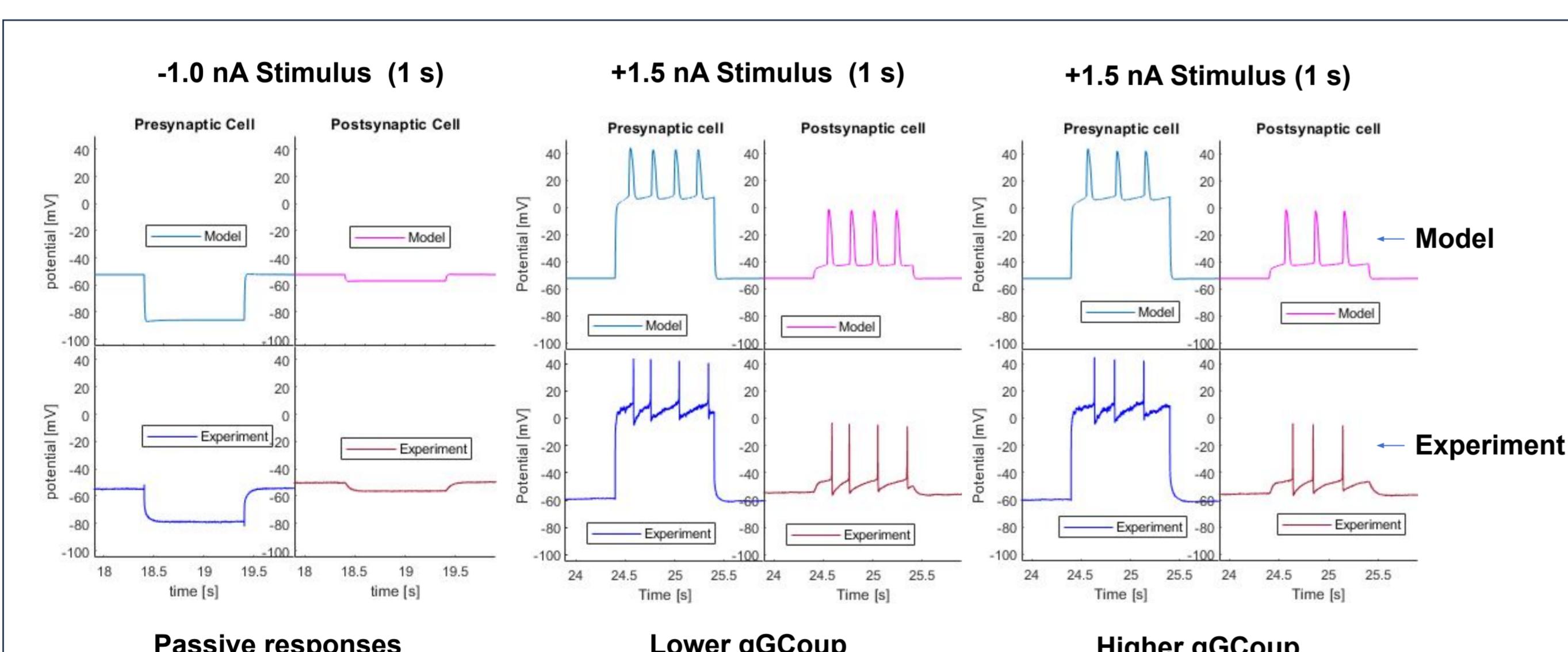


Figure 2. Model and Experimental Cell Responses to Injected Current: Model capabilities of passive and active response generation compared to biological responses. The first plot shows similar amplitude of hyperpolarization (33–35mV) and resting membrane potential (-50 to -55mV) to experimental examples. Second and third plots show active response properties to 1.5 nA stimulus; at lower and higher  $g_{GCoup}$  values respectively, showing that higher  $g_{GCoup}$  causes lower spike counts and higher spike latency as well as Inter-Spike Interval.

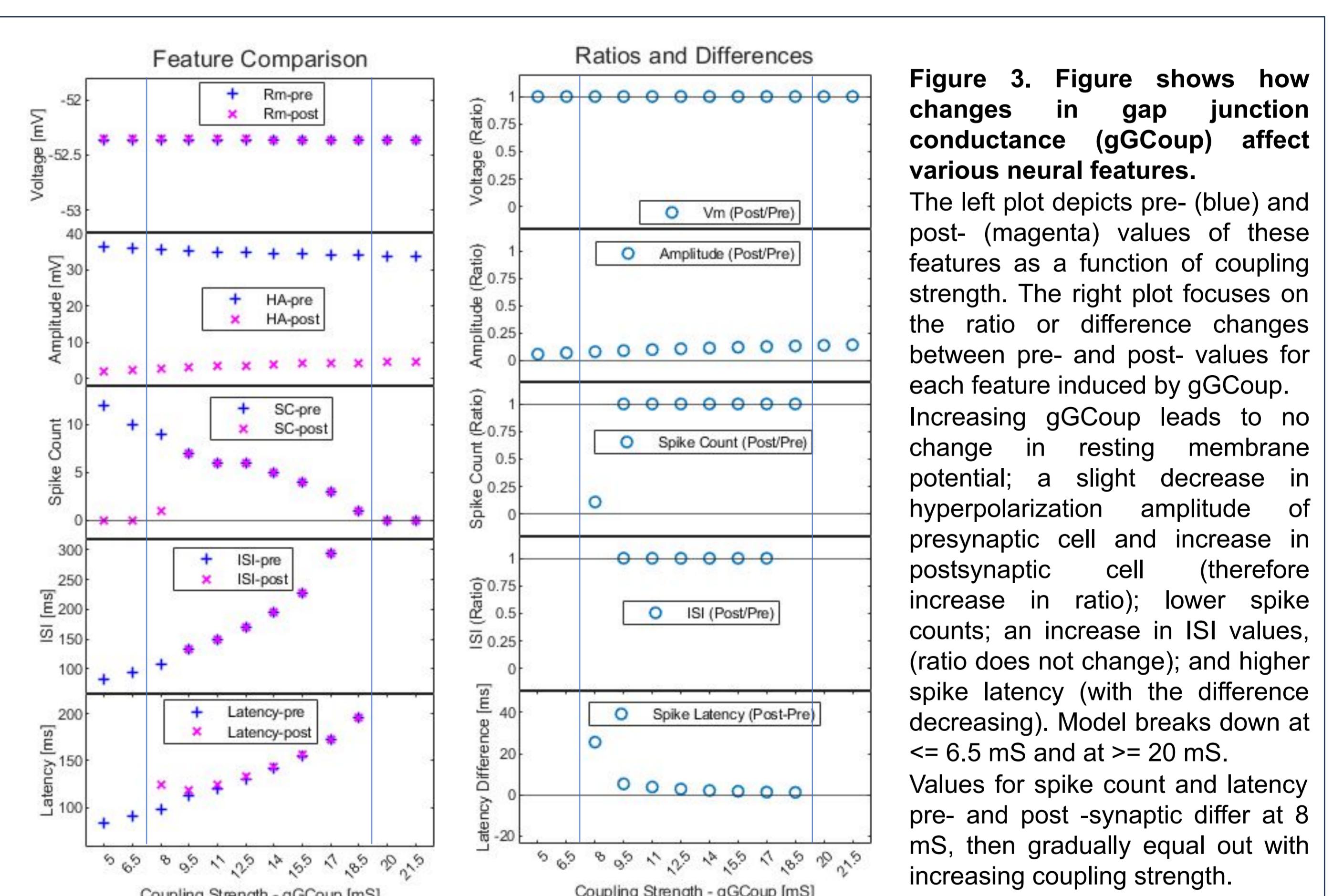


Figure 3. Figure shows how changes in gap junction conductance ( $g_{GCoup}$ ) affect various neural features. The left plot depicts pre- (blue) and post- (magenta) values of these features as a function of coupling strength. The right plot focuses on the ratio or difference changes between pre- and post- values for each feature induced by  $g_{GCoup}$ . Increasing  $g_{GCoup}$  leads to no change in resting membrane potential; a slight decrease in hyperpolarization amplitude of presynaptic cell and increase in postsynaptic cell (therefore increase in ratio); lower spike counts; an increase in ISI values, (ratio does not change); and higher spike latency (with the difference decreasing). Model breaks down at  $<= 6.5 \text{ mS}$  and at  $>= 20 \text{ mS}$ . Values for spike count and latency pre- and post- synaptic differ at 8 mS, then gradually equal out with increasing coupling strength.

## Conclusion:

- Despite not fully representing expected action potential shapes, the model exhibits response features similar to real data. By adhering to Occam's razor—being as simple as possible while still capturing essential response characteristics—the model aids in deciphering which parameters are affected in pharmacological experiments. Further fine-tuning of activation/inactivation parameters could potentially yield the anticipated spike shapes.
- Coupling changes the active response of cells more than passive responses within the range where the model works. Interestingly, when cells are not coupled in a 1:1 ratio but both cells still initiate spikes, there are fewer spikes on the postsynaptic side than on the presynaptic side, and the spike latency difference is significantly higher. This latency difference decreases as coupling strength increases. Additionally, we observe decreasing spike count values and higher latency values with increasing coupling strength, further indicating a negative correlation between these two features in our model.
- Finally, from observing the ratios of around 1 in all parameters produced by the model at specific ranges of  $g_{GCoup}$  values, it can be inferred that caffeine affects not only coupling strength but also the kinetics of each cell. Further optimization of compartments in the future could produce a more robust representation of electrically coupled cells.

## References:

- Prescott, S.A. (2014). Excitability: Types I, II, and III. In: Jaeger, D., Jung, R. (eds)
- Lamb DG, Calabrese RL. Correlated conductance parameters in leech heart motor neurons contribute to motor pattern formation. PLoS One. 2013 Nov 18;8(11)
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