

JOINT ANALYSIS OF X- RAY PTYCHOGRAPHY AND X-RAY FLUORESCENCE



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MULTIMODAL X-RAY DATA

X-Ray Ptychography:

Observations:

- Magnitude/intensities of complex object in Fourier space

Reconstruct:

- Complex object

Goal: Phase retrieval

X-Ray Fluorescence:

Observations:

- photons from fluorescent emission

Reconstruct:

- elemental composition and spatial distribution in an object



“experimental fluorescence map”

Goal: enhance resolution

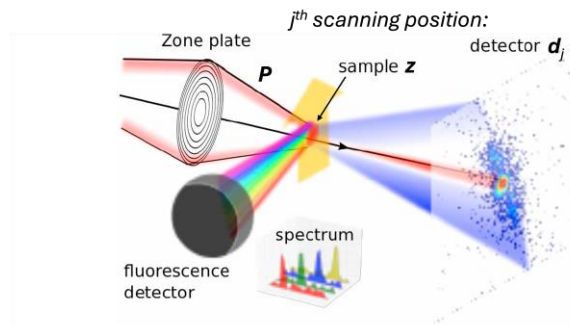


Fig. 1. **Simultaneous ptychographic and fluorescence microscopy.** A focused X-ray beam is scanned across a sample whilst simultaneously recording the X-ray fluorescence spectra and coherent diffraction pattern. [1]

MULTIMODAL APPROACH

⚠ Individually problems are difficult

Our work:

1. Combine problems in a joint framework
 - (Hopefully) better-posed
2. Use a commonality between modalities to simplify problem
3. Explore the conditioning of individual and combined problem
4. Run numerical experiments with various setups

X-RAY PTYCHOGRAPHY

$$d_j = |\mathcal{F}(\mathbf{P}_j \mathbf{z})|^2 + \varepsilon_j,$$

- d_j measurements from probe \mathbf{P} at $j = 1, \dots, N$ position
- \mathbf{z} complex valued object of interest
- \mathcal{F} discrete Fourier

$$\min_{\mathbf{P}, \mathbf{z}} \phi^P = \min_{\mathbf{P}, \mathbf{z}} \frac{1}{2} \sum_{j=1}^N \left| |\mathcal{F}(\mathbf{P}_j \mathbf{z})| - \sqrt{d_j} \right|_2^2$$

- Non-linear
- Non-convex
 - Depends on overlap of \mathbf{P}_j

Common optimization methods:

- PIE
 - Steepest descent step for each j
- Multi-grid
 - Better for large-scale problems

X-RAY PTYCHOGRAPHY

Lack of complex-differentiability \Rightarrow use Wirtinger calculus

$$\nabla(|\mathcal{F}(\mathbf{P}_j \mathbf{z})| - \sqrt{d_j}) = \mathbf{J}_j^P = \frac{1}{2} \overline{\text{diag}(\mathcal{F}(\mathbf{P}_j \mathbf{z}) / |\mathcal{F}(\mathbf{P}_j \mathbf{z})|)} \mathcal{F} \mathbf{P}_j$$

Gradient of objective function ϕ^P :

$$\nabla \phi^P = \sum_{j=1}^N (\mathbf{J}_j^P)^* (|\mathcal{F}(\mathbf{P}_j \mathbf{z})| - \sqrt{d_j})$$

Jacobian:

$$\mathbf{J}^P = \begin{bmatrix} \mathbf{J}_1^P \\ \vdots \\ \mathbf{J}_N^P \end{bmatrix}$$

Approximate Hessian:

$$\mathbf{H}^P = (\mathbf{J}^P)^T \mathbf{J}^P$$

X-RAY FLUORESCENCE

$$D_e = |\mathbf{P}|^2 * \mathbf{w}_e + \hat{\epsilon}_e$$

- Have experimental fluorescence map D_e of element $e = 1, \dots, N_e$
- Can use \mathbf{P} from ptychography to enhance resolution

$$\min_{\mathbf{P}, \mathbf{w}_e} \phi^F = \min_{\mathbf{P}, \mathbf{w}_e} \sum_{e=1}^{N_e} || |\mathbf{P}|^2 * \mathbf{w}_e - D_e ||_2^2$$

- Blind-deconvolution

Current approach:

1. Solve blind ptychography and obtain probe \mathbf{P}
2. Use \mathbf{P} to deconvolve D_e

X-RAY FLUORESCENCE

First note:

$$|\mathbf{P}|^2 * \mathbf{w}_e = \hat{\mathbf{P}} \mathbf{w}_e$$

- $\hat{\mathbf{P}}$ is the matrix representation of the ‘same’ convolution (preserves dimension)

Gradient of objective function ϕ^F :

$$\nabla \phi^F = \sum_{e=1}^{N_e} \hat{\mathbf{P}}^T (\hat{\mathbf{P}} \mathbf{w}_e - D_e)$$

Jacobian:

$$J_e^F = \hat{\mathbf{P}}, \quad J^F = \begin{bmatrix} \hat{\mathbf{P}} \\ \vdots \\ \hat{\mathbf{P}} \end{bmatrix} \}_{N_e \text{ times}}$$

Hessian:

$$\mathbf{H}^F = (\mathbf{J}^F)^T \mathbf{J}^F$$

JOINT FRAMEWORK

Introduce joint objective for a better-posed problem

$$\min_{\mathbf{w}, \mathbf{P}, \mathbf{z}} \alpha \sum_{e=1}^{N_e} \left\| |\mathbf{P}|^2 * \mathbf{w}_e - D_e \right\|_2^2 + \frac{1}{2} \sum_{j=1}^N \left\| |\mathcal{F}(\mathbf{P}_j \mathbf{z})| - \sqrt{d_j} \right\|_2^2$$

- α balances the two objectives

Commonality between modalities:

$$\mathbf{z} = \boldsymbol{\delta} + i\boldsymbol{\beta}, \quad \boldsymbol{\delta} = \sum_e \mathbf{w}_e \mu_e \quad (\text{assume } \mu_e = 1)$$

$$\phi = \min_{\mathbf{w}, \mathbf{P}, \boldsymbol{\beta}} \alpha \sum_{e=1}^{N_e} \left\| |\mathbf{P}|^2 * \mathbf{w}_e - D_e \right\|_2^2 + \frac{1}{2} \sum_{j=1}^N \left\| |\mathcal{F}(\mathbf{P}_j (\sum_e \mathbf{w}_e + i\boldsymbol{\beta}))| - \sqrt{d_j} \right\|_2^2$$

JOINT APPROACH

Gradient of objective function ϕ :

$$\nabla\phi = \alpha\nabla\phi^F + \nabla\phi = \alpha \sum_{e=1}^{N_e} \hat{\mathbf{P}}^T (\hat{\mathbf{P}}\mathbf{w}_e - D_e) + \sum_{j=1}^N (\mathbf{J}_j^P)^* (|\mathcal{F}(\mathbf{P}_j\mathbf{z})| - \sqrt{d_j})$$

Jacobian:

$$\mathbf{J} = \begin{bmatrix} \alpha\mathbf{J}^F \\ \mathbf{J}^P \end{bmatrix}$$

Approximate Hessian:

$$\mathbf{H} = \alpha(\mathbf{J}^F)^T \mathbf{J}^F + (\mathbf{J}^P)^T \mathbf{J}^P$$

Question: Is the joint system better conditioned?

NUMERICAL EXPERIMENTS

- To simplify problem
 - fix probe at ground truth
 - Set $N_e = 1$
- Truncated newton (TN) optimization solver
 - Hessian-free
 - Uses finite difference of Jacobians to approximate \mathbf{H}
- Vary probe overlap, problem size, and element channel

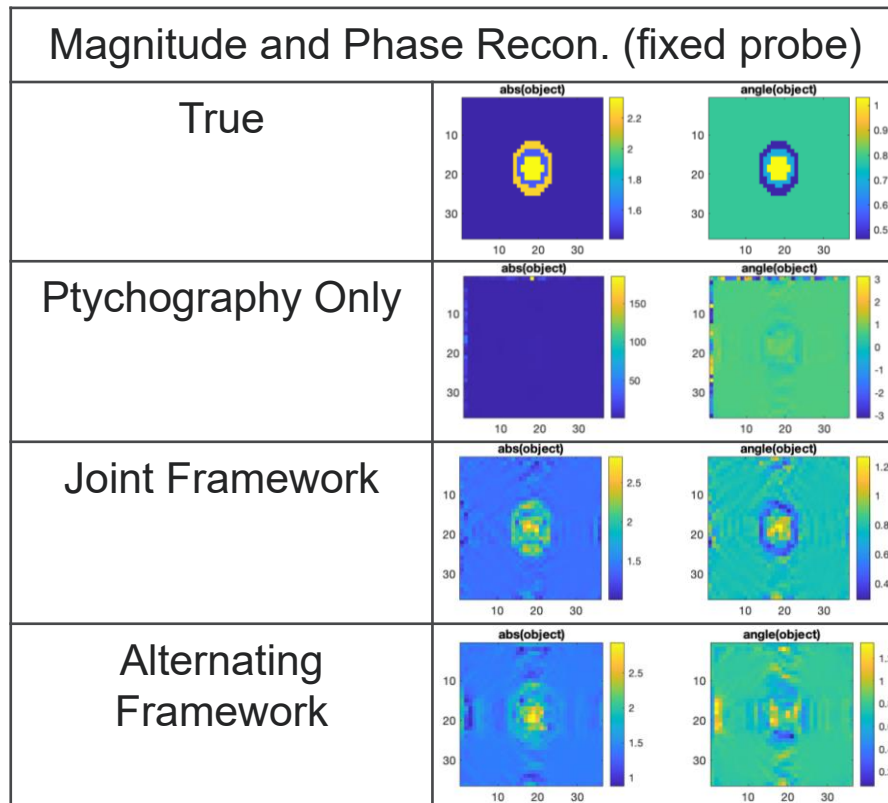
Two Experiment Setups:

1. Alternate between TN for ptychography ϕ^P and TN for fluorescence ϕ^F
2. Use TN for full joint problem ϕ

RESULTS: SMALL EXAMPLE

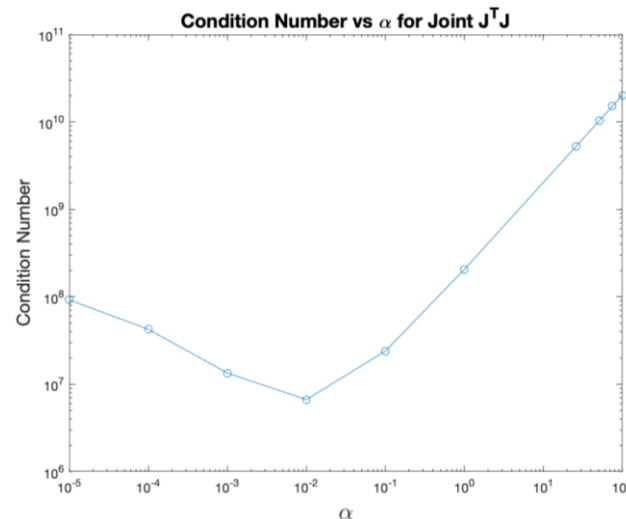
Experimental Setup:

- Probe:
- 9 scanning locations
- Overlap:
- 600 objective function eval



HESSIAN ANALYSIS: SMALL EXAMPLE

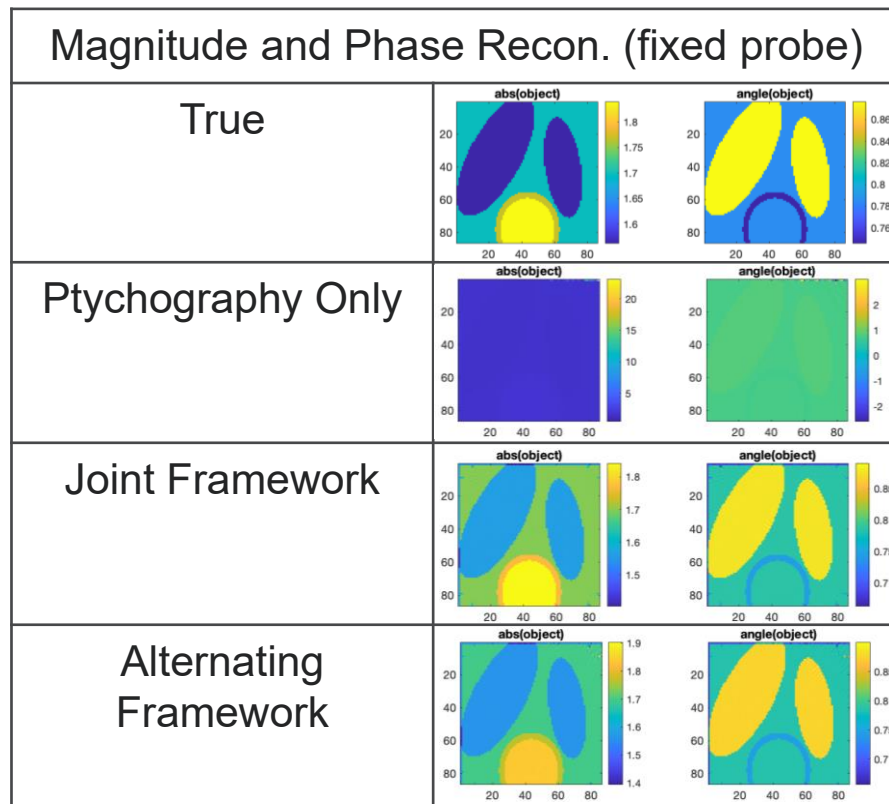
Analysis of $J^T J$	
	Cond. Num.
Ptychography	8.80e+11
Fluorescence	3.75e+19
Combined	6.68e+06



RESULTS

Experimental Setup:

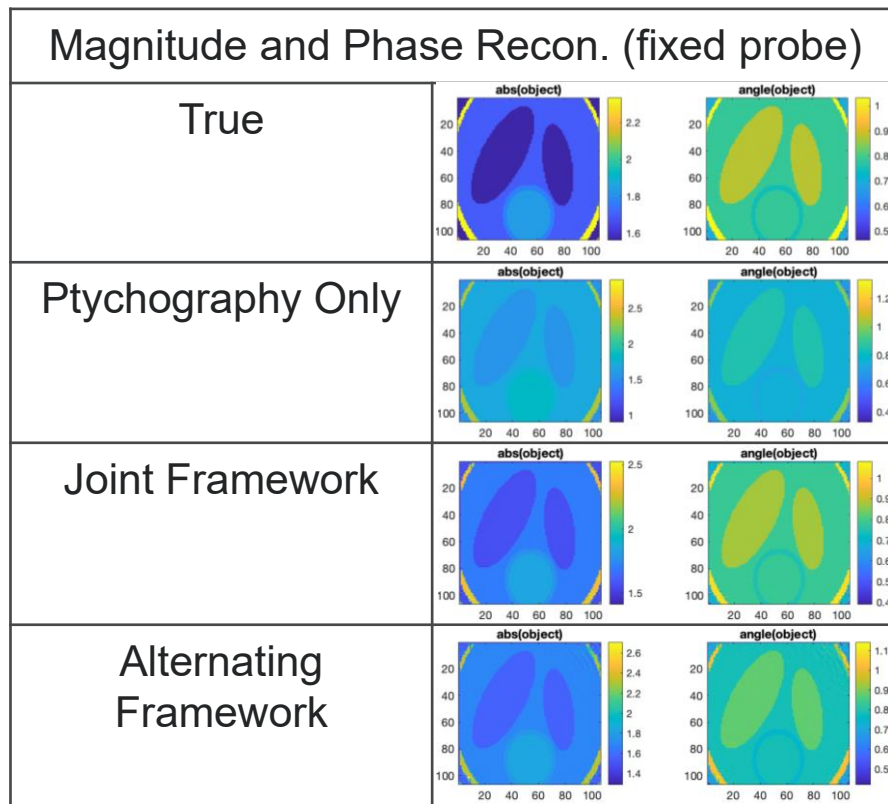
- Probe: 36x36
- 36 scanning locations
- Overlap: 72%
- 600 objective function eval



RESULTS:

Experimental Setup:

- Probe: 64x64
- 36 scanning locations
- Overlap: 84%
- 600 objective function eval



CONCLUSIONS

- Combining modalities can improve the conditioning of the system
- Joint approach may lead to better reconstructions

Future Directions:

- Numerical tests on various experimental configurations
 - Problem size
 - Scanning overlap
 - Noise level
- Rigorous quantification of multimodal benefit

THANK YOU!!! QUESTIONS?



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