

# Hello...

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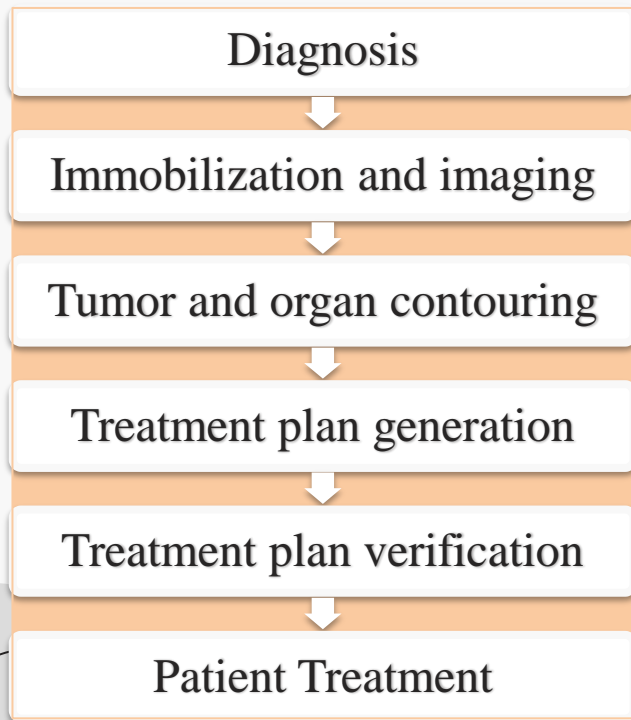
# AI Driven Auto Contouring and Planning for Breast Cancer Radiotherapy: A Feasibility Study on Geometric and Dosimetric Accuracy

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## EBRT Workflow



# Introduction

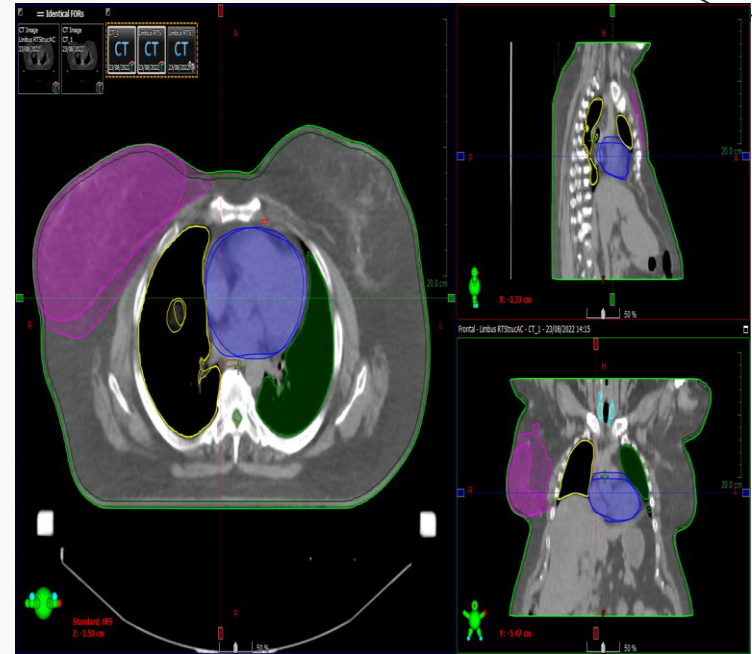
- ❑ Quality of EBRT treatment planning depends on:
  - Target coverage
  - Normal tissue sparing
- ❑ One of the main challenges in EBRT:
  - Accurate and efficient contouring and Planning
- ❑ Workload
  - About 10 million new diagnoses each year globally
  - Many of cases need re-contouring during the treatment

***Workload effects quality of Radiation Therapy***

# Introduction (cont.)

## Manual Contouring

- Radiation oncologists create structure sets
  - Based on anatomical and/or functional information
  - Following consensus guidelines
- Organ sparing and plan optimization depend on:
  - Definition and standardization of OARs
  - Appropriate consideration of movements
- Inter and intra-observer variability in contour delineation is a common issue
  - Affect the resulting plan quality
  - Patient outcomes



**Figure:** Structures contouring of Breast case for radiotherapy

# Introduction (cont.)

## Auto Contouring



A

- ❖ Simplest basic approach for auto segmenting CT scans
- ❖ A voxel is allocated to a ROI if its Hounsfield units exceeds a predefined threshold value

**Intensity  
Analysis**

B

- ❖ Place an initial contour or surface close to the ROI to be segmented
- ❖ Deform image based on image information, such as intensity gradients, and internal constraints.

**Shape Modeling**

C

- ❖ Use of manually segmented reference image.
- ❖ Image registration specifies how a segmented image should be adjusted using mutual information

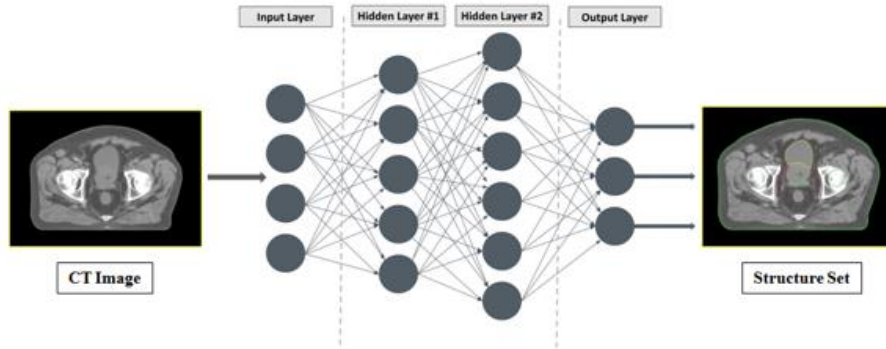
**Atlas Based Auto  
Segmentation**

D

- ❖ Unsupervised-learning algorithms may find areas of comparable voxels but cannot name these regions
- ❖ Supervised-learning systems requires manually segmented images for image segmentation

**Non-deep Machine  
Learning**

# Deep Learning



**Figure:** A simple artificial neural network for anatomy contouring

- Early CNNs were used to segment a two-dimensional image pixel by pixel.
- FCNN, replace the fully connected layers of a CNN with convolutional layers for more effective segmentation.
- Now the U-net CNN architecture is the state-of-the-art auto-contouring method in image contouring.

Helps to minimize:

- **Variability**
- **Clinical workload**

# Automatic contours = Clinically used contour ?

❑ Evaluation according to literature:



**Geometric metrics**



**Dosimetric metrics**

❑ But dosimetry performance is influenced :

- Not only by geometric precision,
- But also by spatial dose distribution and gradient

❑ Each dosimetric parameter (i.e., Dmax, Dmean, Dv%) has a distinct reliance and sensitivity to geometric change



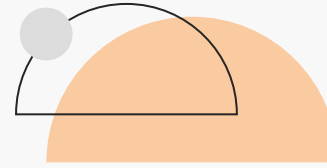
*Geometric impact into dose domain and plan quality remains elusive.*

# Aim of the Study

- ❖ To measure time savings in anatomy contouring using AI based auto-contouring software
- ❖ To gather subjective feedback of physicians on contouring quality of auto-contouring tool
- ❖ To quantitatively investigate the quality and accuracy of structure contours generated either wholly and partially by auto-contouring.
- ❖ To investigate the dose metrics and quality of radiation therapy treatment plans derived from reviewed auto-contouring structures.
- ❖ To evaluate the impact of the variations performed by radiation oncologists starting from the auto-segmentations.



# Materials & Methods



## Materials

- GE LightSpeed 16 Slice CT simulator
- Auto Contour, v2.5 and EZFluence v2.4.4 Software from RAD formation
- Varian Eclipse v 13.6
- MATLAB program for data analysis
- 20 Breast Cancer Cases
- 3DCRT planning



**Version 2.5.0 Rev 1.0**

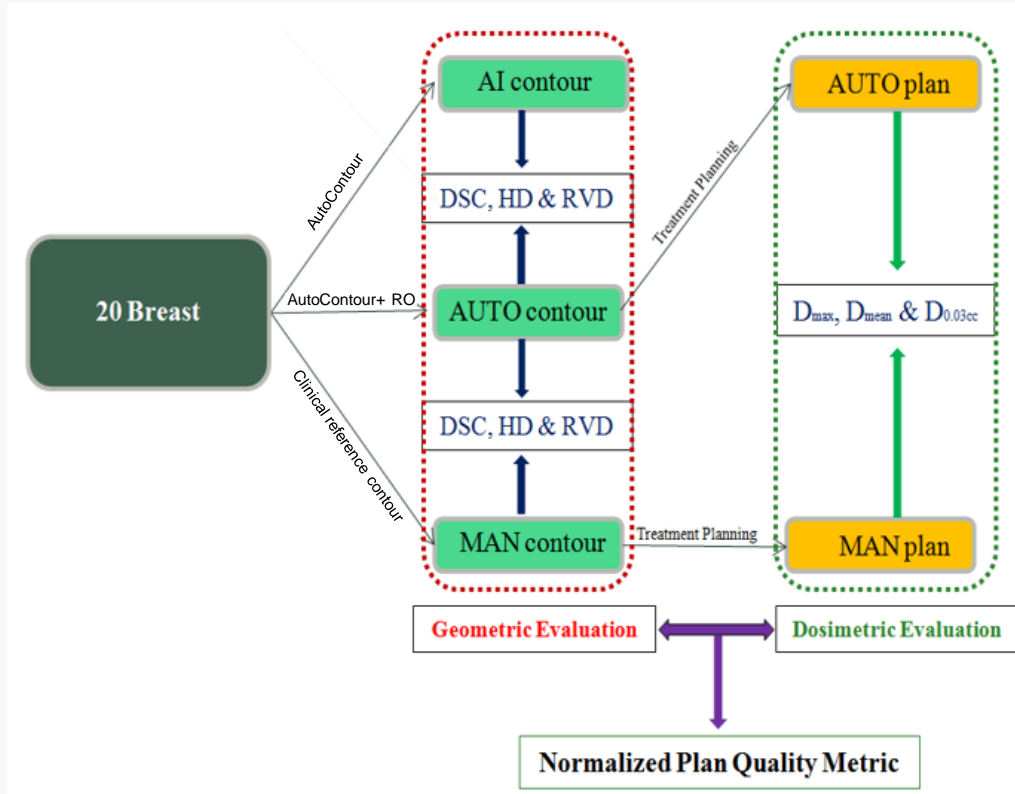
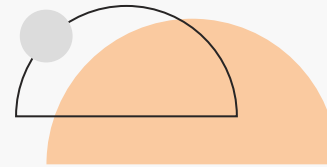


**V2.4.3**



# Materials & Methods

## Workflow of the Study



## Statistical analysis parameters

Condition	H <sub>0</sub>	Difference
$P > \alpha$	Accept/No reject	No
$P < \alpha$	No accept/Reject	Yes
$-CI < 0 < CI$	Accept/No reject	No

## Time Evaluation

$T_{\text{MAN}} \rightarrow$  Contouring time approximated by physicians with their previous experiences

$T_{\text{AUTO}} \rightarrow$  Auto Contour time ( $T_{\text{AIC}}$ ) together with RO editing times ( $T_{\text{RO}}$ ) including DICOM file export and import time



$T_{\text{MAN}}$



$T_{\text{AIC}} + T_{\text{RO}} = T_{\text{AUTO}}$

$$\text{Time savings} = \frac{T_{\text{MAN}} - T_{\text{AUTO}}}{T_{\text{MAN}}}$$

## Qualitative Evaluation

Severe Correction	: Require correction $\rightarrow$ Large and obvious errors
Medium Correction	: Require correction $\rightarrow$ Minor errors that need a small amount of editing
Slight Correction	: Accepted $\rightarrow$ Minor errors but these are clinically not significant
No Correction	: Accepted $\rightarrow$ Contour is very precise

# Geometric Evaluation

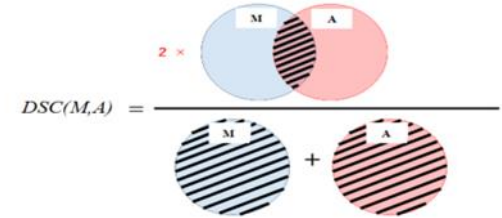
## Dice Similarity Coefficient

- A measure of the volumetric overlap of two contours of a structure

No overlay  $\rightarrow 0$

Total overlay  $\rightarrow 1$

$$DSC(M, A) = \frac{2|M \cap A|}{|M| + |A|}$$



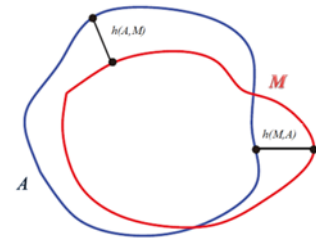
## Hausdorff Distance

- A bi-directional measure of distance between two contour surfaces

No overlay  $\rightarrow > 1 \text{ mm}$

Total overlay  $\rightarrow 0 \text{ mm}$

$$HD(M, A) = \max [h(M, A), h(A, M)]$$



## Relative Volume Difference

- Absolute size difference between the regions in terms of reference size

No overlay  $\rightarrow 1 \text{ and more}$

Total overlay  $\rightarrow 0$

$$RVD = \left| \frac{|A| - |M|}{|M|} \right|$$

# Dosimetric Evaluation



## OAR Dose Metrics

- For generic description : Integrated  $D_{\max}$ ,  $D_{\text{mean}}$  and also  $D_{0.03\text{cc}}$  in terms of absolute dose

$$\Delta D_X = \frac{(D_X)_{\text{AUTO}} - (D_X)_{\text{MAN}}}{(D_X)_{\text{MAN}}}$$

## PTV Dose Metrics

- Homogeneity Index (HI): to evaluate the dose uniformity within the PTV

$$\Delta HI = \frac{|HI_{\text{AUTO}} - HI_{\text{MAN}}|}{|HI_{\text{MAN}}|} \quad \text{Where, } HI = \frac{(D_{2\%} - D_{98\%})}{D_{50\%}}$$

- Conformity Index (CI): to obtain a quantitative evaluation of the PTV coverage by the prescribed dose

$$\Delta CI = \frac{|CI_{\text{AUTO}} - CI_{\text{MAN}}|}{|CI_{\text{MAN}}|} \quad \text{Where, } CI = \frac{(TV_{PV})^2}{V_{PTV} \times V_{TV}}$$

- Serial organs  $\rightarrow D_{\max}$  and  $D_{\text{mean}}$
- Parallel organs  $\rightarrow D_{\text{mean}}$  and/or  $D_{x\%}$

$D_X \rightarrow D_{\max}, D_{\text{mean}} \text{ or } D_{0.03\text{cc}}$

# Normalized Plan Quality Metric



➤ nPQM works as a hypothetical **virtual physician**

$$nPQM = \frac{PQM}{PQM_{max}} \times 100$$

## ❑ Threshold Score:

- No points → objective is not achieved
- Maximum points → accomplished objective

## ❑ Linear Score:

- No points → does not exceed the “minimally acceptable threshold”
- Maximum points → satisfies the constraint's “ideal threshold”
- Linear interpolated score → between the two thresholds

Plan quality metric for evaluation of treatment plans:

Structure	Constraint	Function	Thresholds	Max Score
PTV	D99%	Linear	>6000 cGY (100%) ; >5700cGy (95%)	5 ; 4
	D0.1 cc	Linear	<6300cGy(105%) ; <6420cGy(107%)	5 ; 4
Rectum	V4500 cGy	Threshold	<15%	3
	V2800 cGy	Threshold	<35%	3
	V900 cGy	Threshold	<80%	3
Bladder	V4500 cGy	Threshold	<25%	3
	V2800 cGy	Threshold	<50%	3
Anal Canal	V4500 cGy	Threshold	<15%	3
	V2800 cGy	Threshold	<35%	3
	V900 cGy	Threshold	<80%	3
Femur Right	V3500 cGy	Threshold	<1%	2
Femur Left	V3500 cGy	Threshold	<1%	2

# Results & Discussions

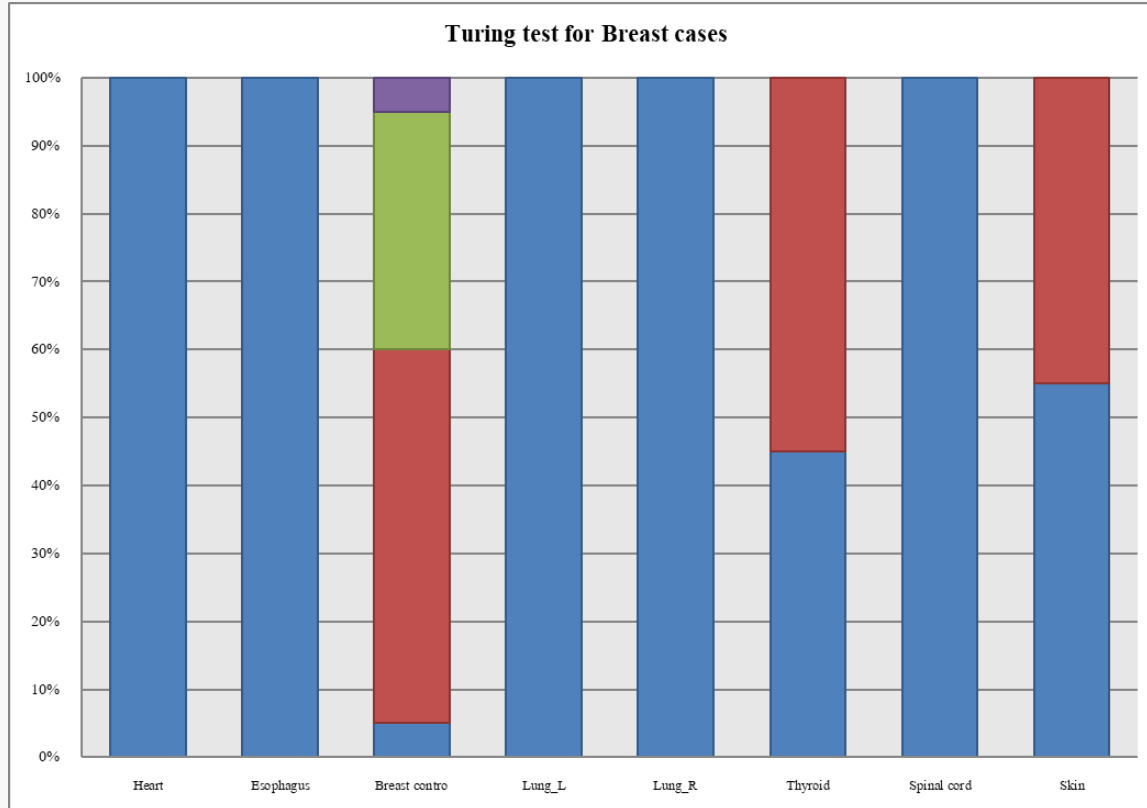


## Time Savings

Procedure	$T_{\text{MAN}}(\text{avg})$	$T_{\text{AUTO}}(\text{avg})$	Time Savings	Saved Time (%)
Contouring	28 min	9.8 min	18.2 min	65%
Planning	40 min	10.9 min	29.1 min	73%

- ❑ More than 65% of contouring time can be saved.
- ❑ More time saving is possible by implementing a fully integrated system.

# Qualitative Evaluation



**Breast:**

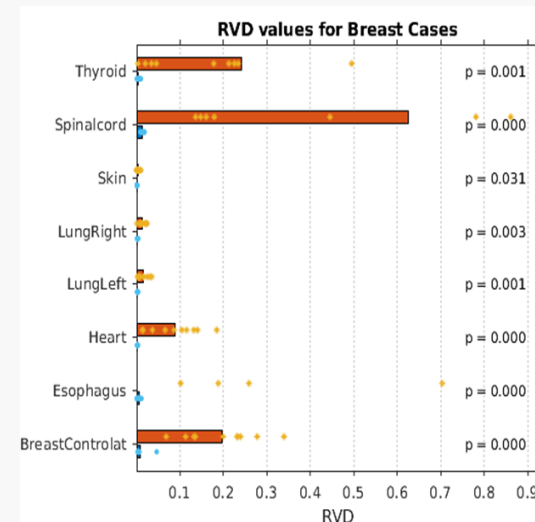
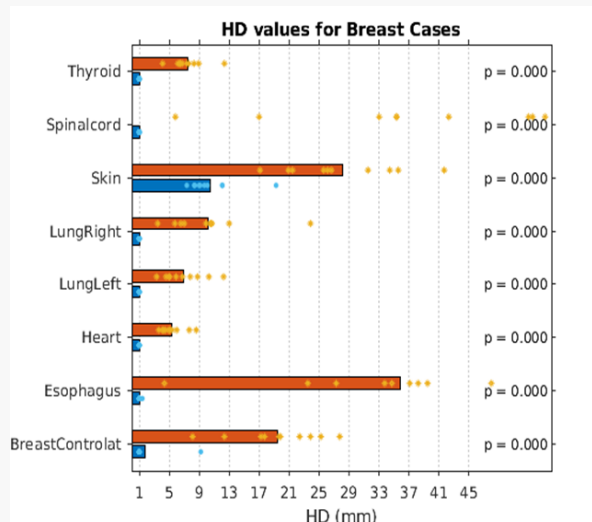
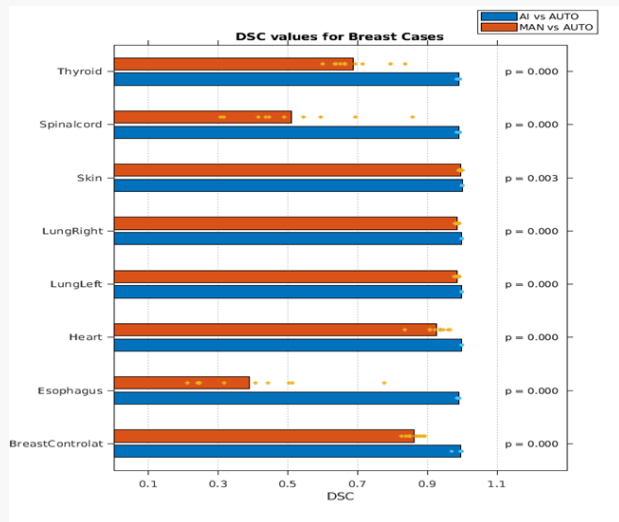
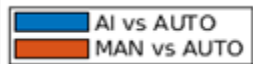
No correction

Accepted → 95%

Corrected → 5%



# Geometric Comparison (Breast)

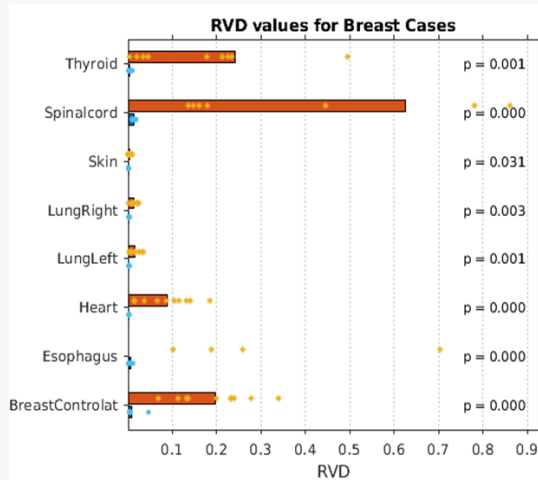
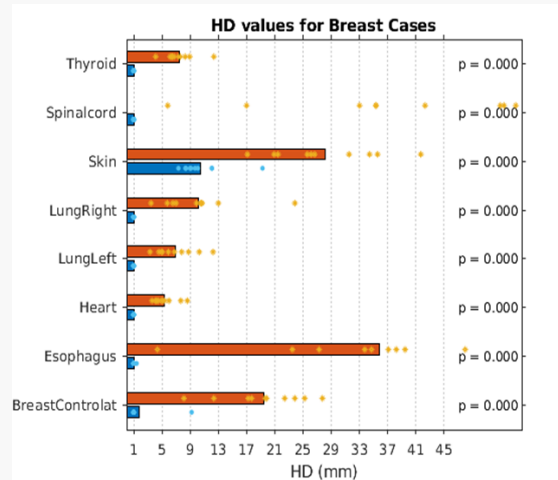
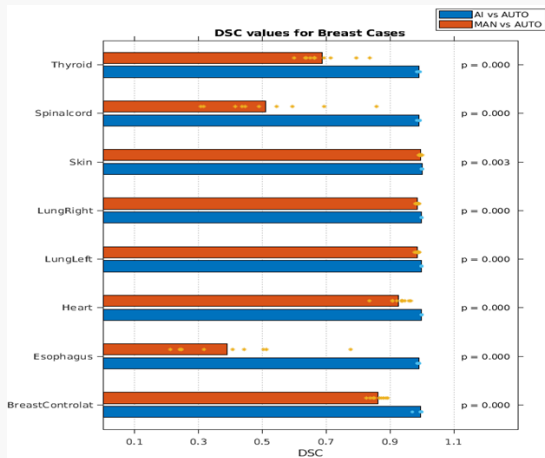


## AI vs AUTO:

- More than 95% similarity
- Skin showed upto 12 mm HD
- Almost no volume difference

# Geometric Comparison (Breast)

AI vs AUTO  
MAN vs AUTO

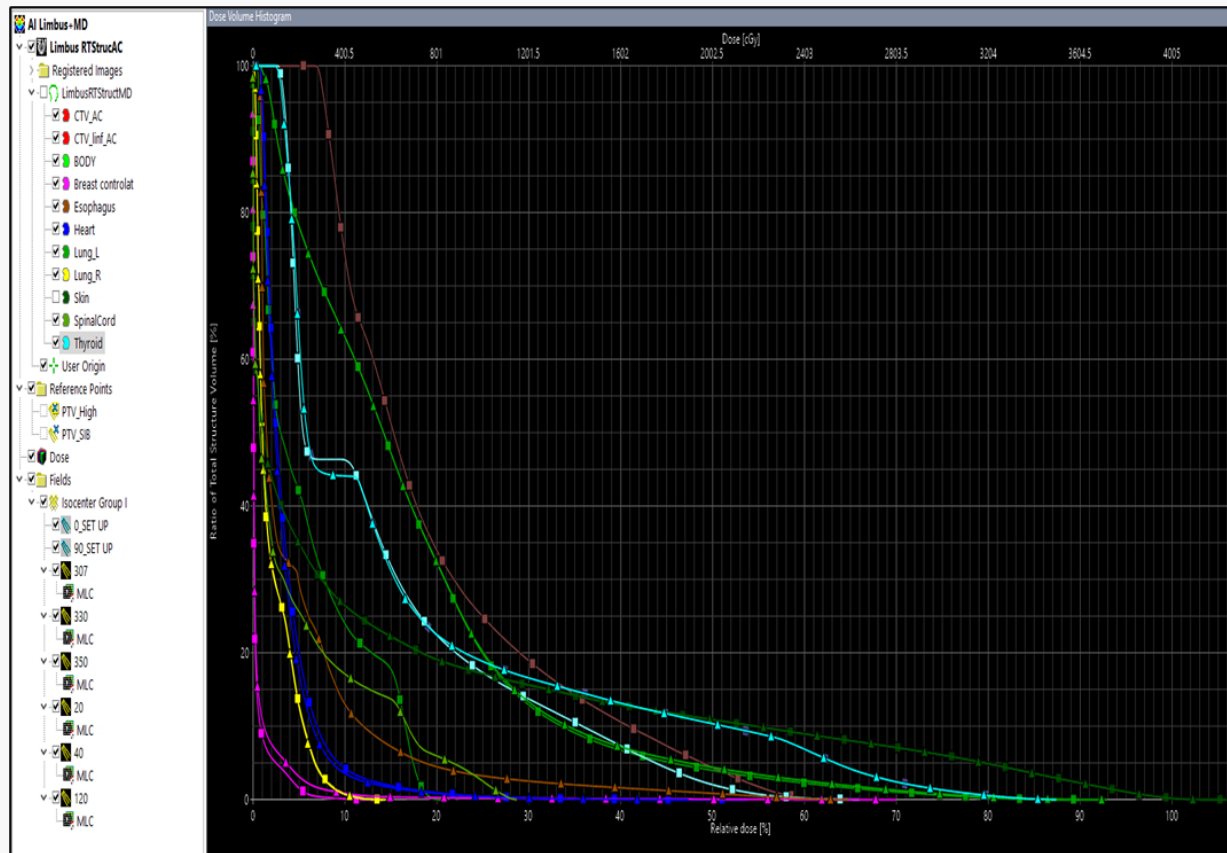


## AI vs AUTO:

- More than 95% similarity
- Skin showed upto 12 mm HD
- Almost no volume difference

## MAN vs AUTO:

- Spinal cord → DSC<0.50 & 61% RVD
- Contralateral breast → 20% volume difference
- Thyroid → 69% DSC & 24% RVD
- High HD: Esophagus, contralateral breast and skin



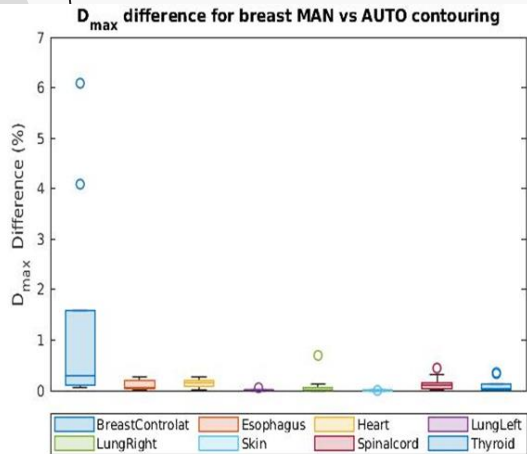
Structural contours  
has influence on:

- Plan optimization
- Plan assessment
- Decision-making process for plans

Breast : DVH for MAN & AUTO contours

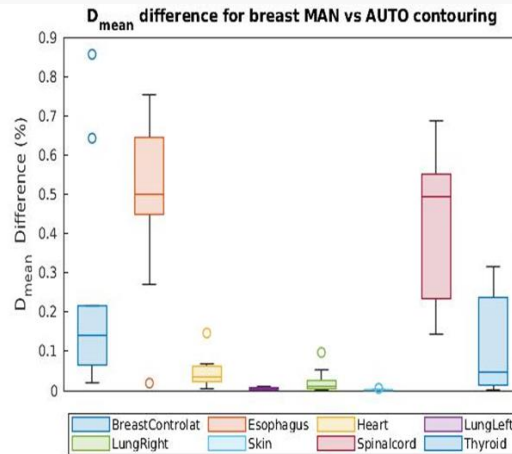


# Dosimetric Comparison (Breast)



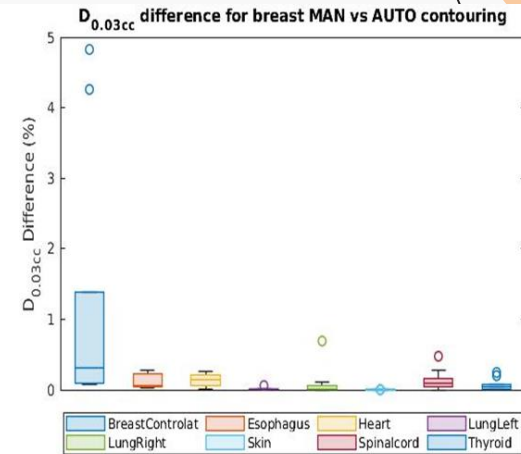
**$\Delta D_{max}$**

- Contralateral Breast: 30%
- Spinal cord: 12%
- Heart: 14%



**$\Delta D_{mean}$**

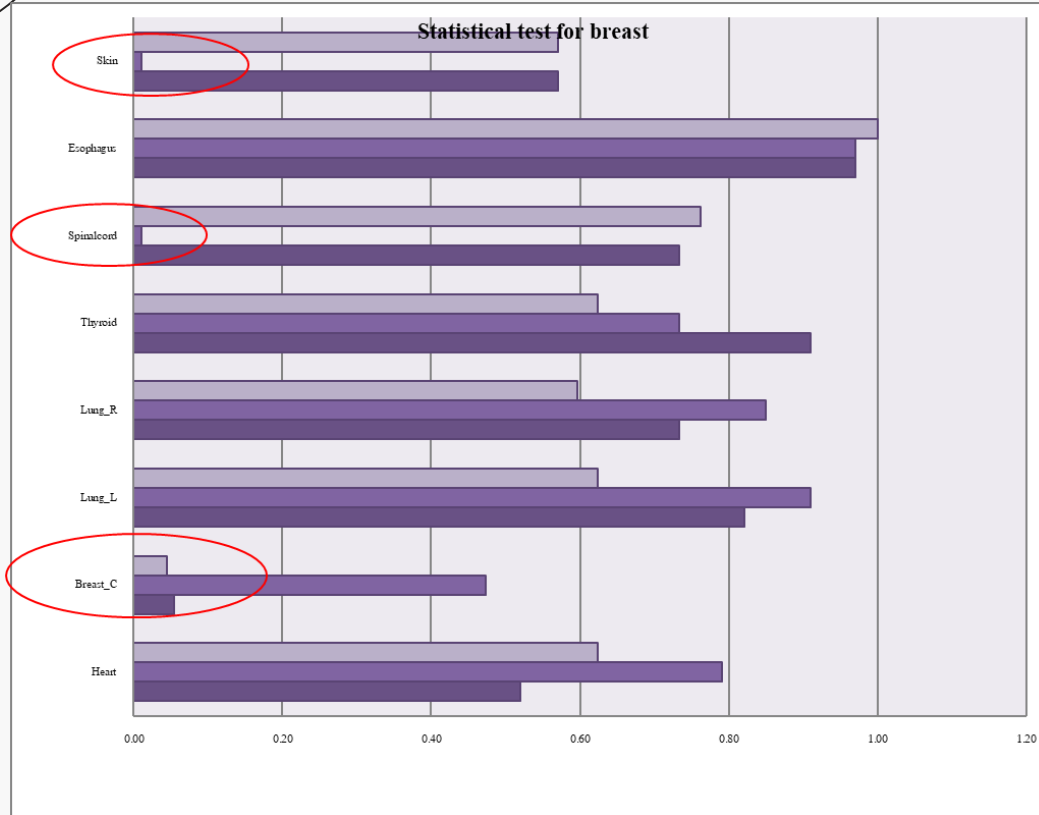
- Contralateral Breast : 14%
- Spinal cord: 49%
- Esophagus : 49%



**$\Delta D_{0.03cc}$**

- Contralateral Breast: 31%
- Spinal cord: 10%
- Heart: 14%

# Statistical Analysis



None of the OAR dose has been found to be statistically significant (  $p \geq 0.05$  ) except the following:

## Breast:

Contralateral Breast,

$D_{0.03cc} \rightarrow p = 0.045$

Spinal cord & Skin,

$D_{mean} \rightarrow p = 0.011$

# Geometry vs Dosimetry

Study Site	OAR	DSC	HD	RVD	Dmax	Dmean	D0.03
Breast	Breast Contralat	0.87	19.75	0.22	0.30	0.14	0.31
	Heart	0.94	5.00	0.09	0.14	0.03	0.14
	Thyroid	0.66	7.03	0.19	0.04	0.05	0.04
	Spinal Cord	0.47	35.34	0.61	0.12	0.49	0.10
	Esophagus	0.36	35.91	1.22	0.06	0.50	0.06

Yellow

→ Significant Difference

Red

→ Higher Difference

# Geometry vs Dosimetry

Study Site	OAR	DSC	HD	RVD	Dmax	Dmean	D0.03
Breast	Breast Contralat	0.87	19.75	0.22	0.30	0.14	0.31
	Heart	0.94	5.00	0.09	0.14	0.03	0.14
	Thyroid	0.66	7.03	0.19	0.04	0.05	0.04
	Spinal Cord	0.47	35.34	0.61	0.12	0.49	0.10
	Esophagus	0.36	35.91	1.22	0.06	0.50	0.06

Yellow

→ Significant Difference

Red

→ Higher Difference

# Normalized Plan Quality Metric



Study Site	Mean (SD)	Median (Range)
Breast	0.077 (0.160)	<b>0.000</b> (0.00-0.500)

- nPQM as a virtual physician
- Integrates both geometry and dosimetry assessment.

Plan Quality Difference

- Breast: 0%



# Conclusions



- Although auto-contouring system achieved state-of-the-art geometrical and dosimetric performance, human review is still unavoidable
- AI driven auto contouring would be improvement to speed up the contouring process over present clinical practice.
- Plans based on automatically generated contours do not overdose nearby OARs
- AI based auto-contouring may help to establish a standard starting point for radiation therapy treatment.
- This study offers a proof-of-concept methodology to investigate the impact of including an auto-contouring and planning software in the RT workflow.



# Thanks!

Do you have any questions?

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