

EMGInformedCMC - Microsoft Visual Studio

```
// Set output file names so that files are flushed regularly in case we fail
ID::makeDir(getResultsDir()); // Create directory for output in case it doesn't exist
manager.getStateStorage().setOutputFileName(getResultsDir() + "/" + getName() + "_states.sto");
try {
    manager.integrate(s);
} catch (const OpenSim::Exception& x) {
    // TODO: eventually might want to allow writing of partial results
    x.print(cout);
    ID::makeDir(savingWorkingDirectory);
    // close open files if we die prematurely (e.g. Out fail)
    manager.getStateStorage().print(getResultsDir() + "/" + getName() + "_states.sto");
    return false;
} catch (...) {
    // TODO: eventually might want to allow writing of partial results
    ID::makeDir(savingWorkingDirectory);
    // close open files if we die prematurely (e.g. Out fail)
    manager.getStateStorage().print(getResultsDir() + "/" + getName() + "_states.sto");
    return false;
}
time(&finishTime);
cout << "Finished tracking the specified kinematics!\n";
if (_verbose) {
    std::cout << "states" << s.getY() << std::endl;
}
cout << "=====!\n";
localTime = localtime(&startTime);
cout << "Start time" << asctime(localTime);
localTime = localtime(&finishTime);
```

Error List

Code	Description	Project	File	Line	Suppression St...
0	Errors	0	Warnings	0	Messages

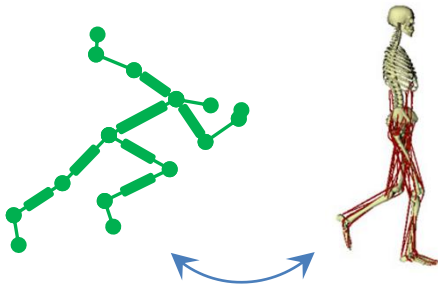


EMG Based Motion Capture [Project]

From Motion Capture to Musculoskeletal Simulation and (not quite) back Felix Laufer

Recap: Why EMG Based Activation Estimation?

wearHEALTH

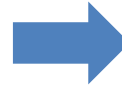


muscular redundancy

What about ...

- co-contraction
- fine motor tasks with higher muscle tension
- extreme (fast) movements
- (temporal / pathological) muscle fatigue ... ?

neurophysiological redundancy /
activation patterns



$$\sum_{i=1}^{N_m} (a_i)^2 \longrightarrow \min$$

$$\text{s.t. } \forall c_j := f_j^* - f_{j, \text{exp}} \approx 0$$

classical stress minimization approach



$$\sum_{i=1}^{N_m} (a_i)^2 \longrightarrow \min$$

$$\text{s.t. } \forall c_j := f_j^* - f_{j, \text{exp}} \approx 0$$

Seminar: Approach 1

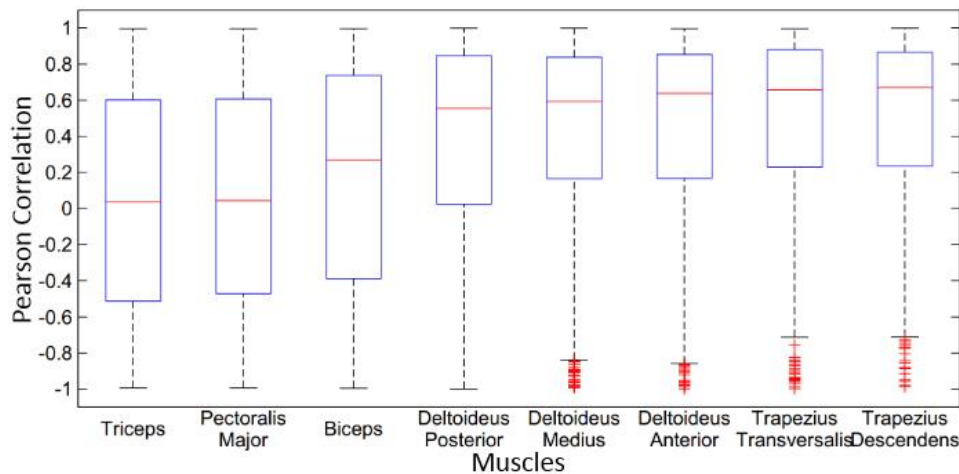
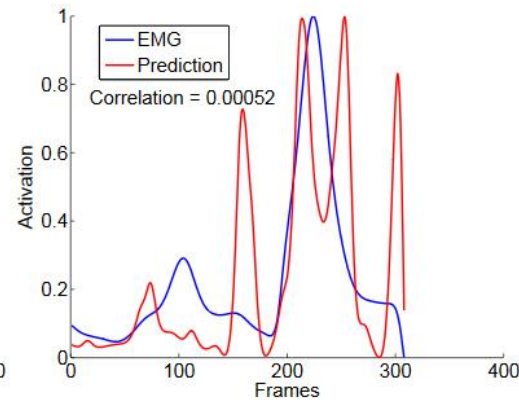
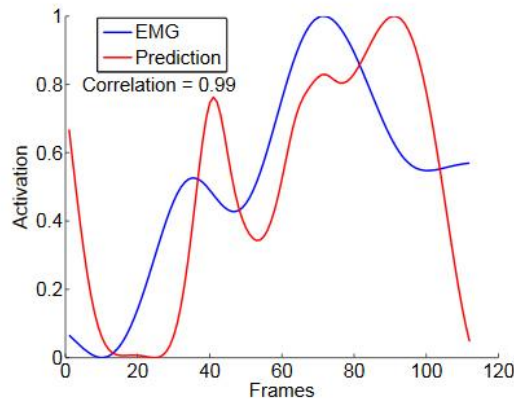
$$\forall c_k := a_k - a_{k, \text{exp}} \approx 0$$

EMG informed minimization approach

Project: Is surface EMG data (sEMG) a valid estimator for computed muscle activation in practice?

$$\forall c_k := a_k - a_{k, \text{exp}} \approx 0$$

?



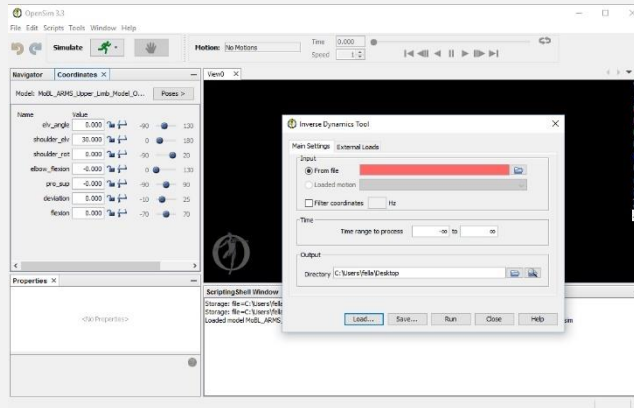
sEMG (8 muscles)

MPI study suggests that sEMG is a useful predictor for muscle activation

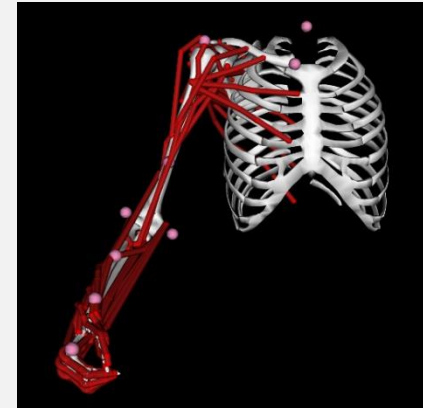
Goal := Verify that, reproduce results!

Project Plan – Overview

OpenSim



Arm model (musculoskeletal)



Inverse **K**inematics
joint angles



Inverse **D**ynamics
forces, torques



Musculoskeletal **S**imulation
muscle activation and forces

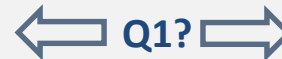
MPI data



- pointing movements
(joint kinematics)



- sEMG measurements
(8 muscles)



- computed muscle activations
(classical minimization approach)

Project Plan – A Look at the Source Data

MPI data



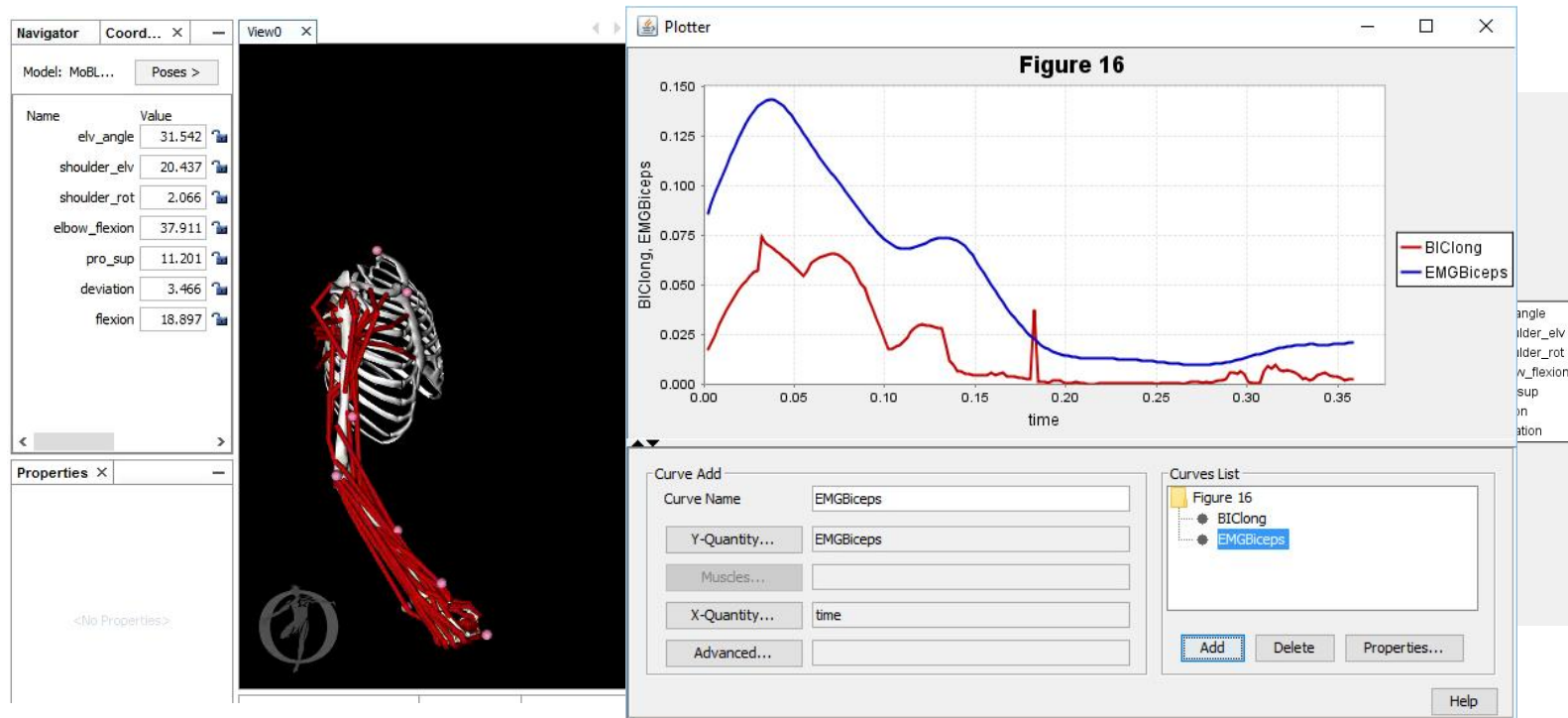
- pointing movements (joint kinematics)



- sEMG measurements (8 muscles)



- computed muscle activations (classical minimization approach)



Actual Project – "Flowchart"

MPI study used commercial full-body model (SIMM)

Choose open source full-body model

Conflicts with latest OpenSim version

Downgrade to earlier version

Different inverse dynamics algorithms

There are only antiquated free full-body models!

Choose a free partial arm model

Complex mapping between full-body model data vs. partial arm model requirements ... finally works!

Classical minimization algorithm doesn't converge!

Partial arm model has been updated!

New model release requires new data mapping

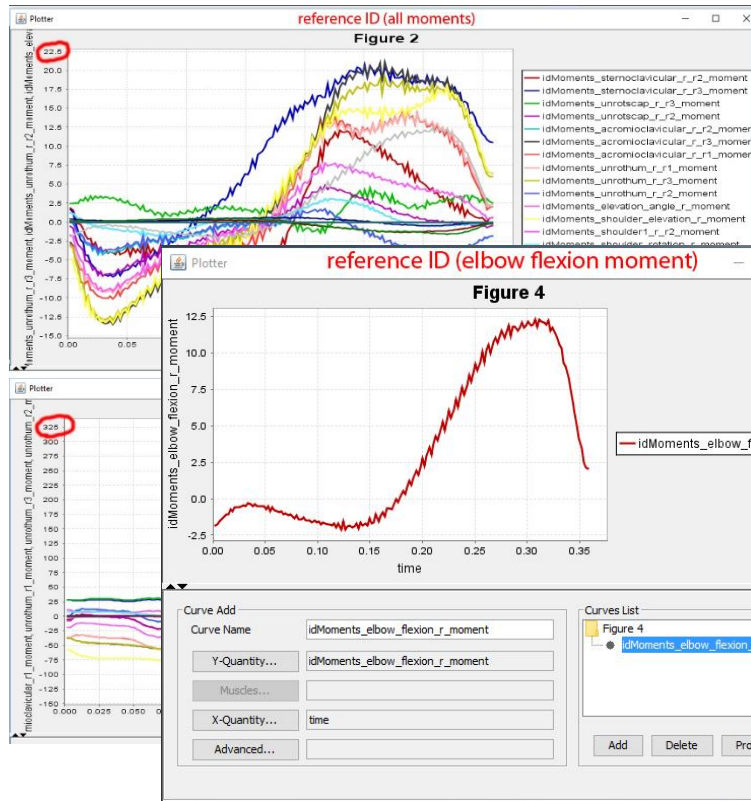
Classical minimization algorithm converges ... but ...

Intermediate inverse dynamics results (joint torques) are totally different from study results!

Trial and error phase, change any parameter randomly



Problem: Inconsistent Dynamics



Inconsistent inverse dynamics solution:
proximal joint torques very different!

But: distal joint torques (e.g. elbow) quite similar!

Main Problem = Different Models



Discussion with ...

Myroslav Bachynskyi
(MPI study)

Kate Saul (partial
arm model dev.)

OpenSim community
(simtk.org)

"Inertial properties of the SIMM full-body model might be [systematically] different to the partial arm model." (M. Bachynskyi)

Subject specific scaling of inertial properties is **not possible**.
(No participant information (mass, scale factors) contained in MPI data)

Inverse Kinematics
joint angles ✓



Inverse Dynamics
forces, torques ⚡



Musculoskeletal Simulation
muscle activation and forces ⚡



Workaround: Restrained Movements

Alternative plan: Consider **only elbow** movement, **restrain all other joints!**

(1 free and 6 fixed DOFs)

→ Compare only those computed activations vs. sEMG measurements related to elbow joint actuation: **biceps, triceps**

But ...

Restrained kinematics → different dynamics (elbow torque cannot be considered in isolation)

different dynamics → different computed muscle activations (stress minimization approach)

... and ...

elbow actuated by **biceps, triceps**, ~~brachialis, pronator teres, anconeus, ...~~ } muscular
biceps / triceps actuate **elbow**, ~~wrist (supination) / shoulder (adduction)~~ } redundancy!

Thus ...

full movement sEMG
measurements

valid for ...?

restrained elbow
movement

yields ...?

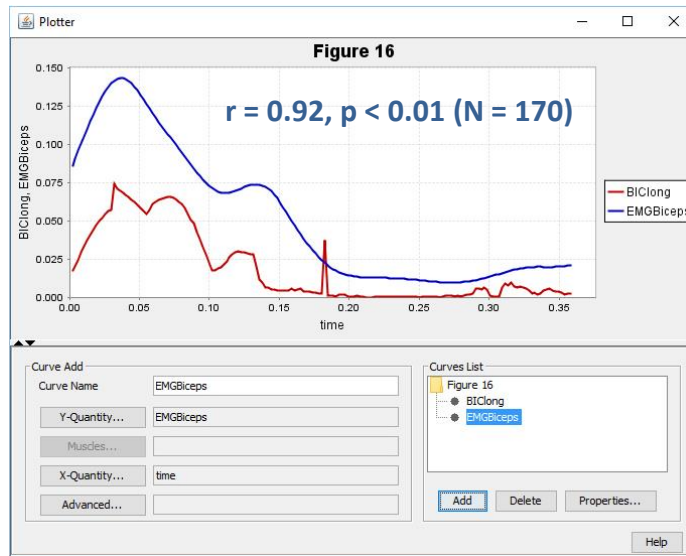
similar computed
muscle activations

still comparable ...?

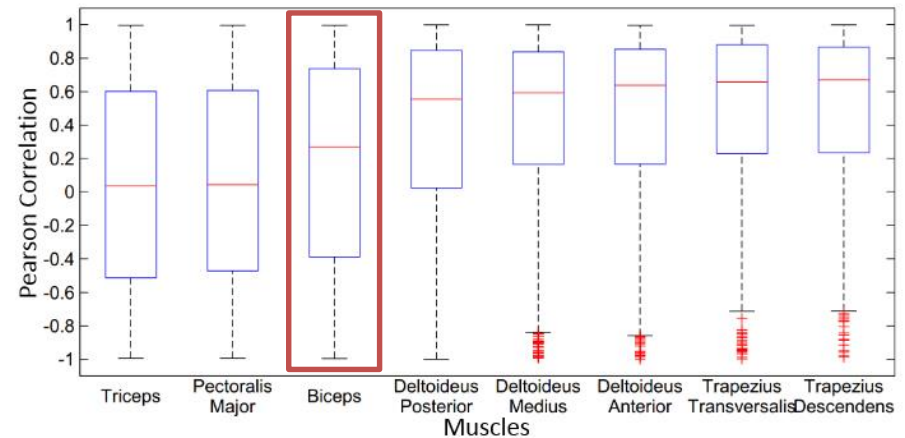
How comparable (w.r.t. study) are results under these restraints / assumptions?

(Spurious) Results

biceps correlation: computed vs. sEMG



MPI study: correlations boxplot



Authenticity of correlations "generated" with ...

- different model
(inertia, internal forces, muscle properties, ...)
- restrained kinematics

But there are also "spurious" correlations contained in the actual study results!

Correlate totally unrelated muscles:
e.g. *pronator teres* vs. *deltoid* → $r = 0.74$



Project Difficulties and Sources of Error

wearHEALTH

marker placement & tracking

- real vs. virtual markers
- tracking accuracy
- repeatability

Motion Capture
marker trajectories

inverse kinematics

- drift of markers
- joint modelling
- numerical errors

Inverse Kinematics
joint angles

inverse dynamics

- measure of external forces
- distribution of body mass
- numerical errors

Inverse Dynamics
forces, torques

Musculoskeletal Simulation
muscle activation and forces

model scaling

- marker points
- distribution of body mass
- ...

MTU modelling

- tendon slack length, optimal fiber length and maximum isometric force
- ...

generalizability (subject \leftrightarrow model)

- individual neural drive and activation strategies
- MTU params highly dependent on subject

(neuro)muscular redundancy

- **muscular** := several muscles for one joint or muscles spanning multiple joints
- **neurophysiological** := task-dependent activation strategies or multiple neurons innervating the same muscle
- **co-contraction**

EMG \leftrightarrow muscle activation \leftrightarrow muscle forces

- mapping poorly understood,
- no reliable models

Motion Simulation
marker trajectories

Forward Kinematics
joint angles

Forward Dynamics
forces, torques

Musculoskeletal Modelling
muscle activation and forces

EMG extraction and processing

- surface EMG only (no deeper MTUs)
- characterizing frequency bandwidths
- \rightarrow generalizability?

Theory



Seminar

vs.

vs.

Practice



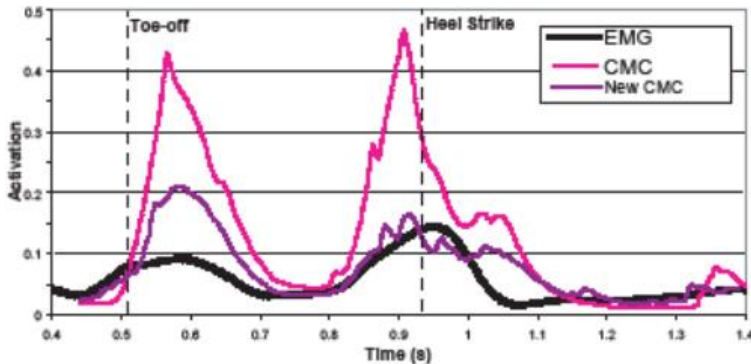
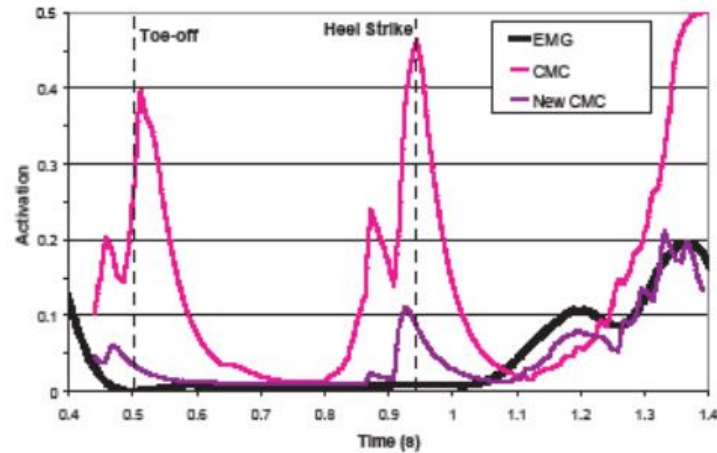
Project

Questions?

Thanks for your attention!

From Motion Capture to Musculoskeletal Simulation and (not quite) back

Assuming that sEMG is a valid estimator ...



$$+ \sum_{k=1}^{N_{c_k}} \omega_k (a_k - a_{k,emg})^2 \longrightarrow \text{min}$$



$$\sum_{k=1}^{N_{c_k}} \omega_k \text{Corr}(a_k, a_{k,emg}) \longrightarrow \text{max}$$



$$- \sum_{k=1}^{N_{c_k}} \omega_k \text{Corr}(a_k, a_{k,emg}) \longrightarrow \text{min}$$