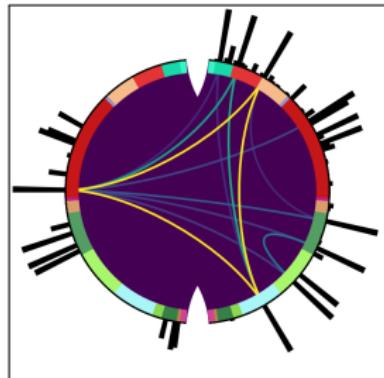
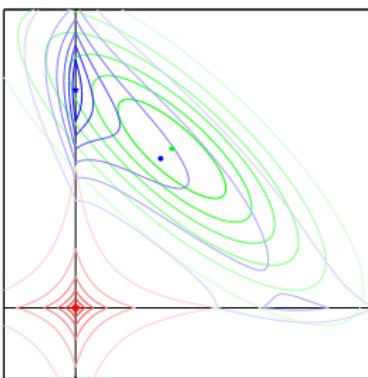
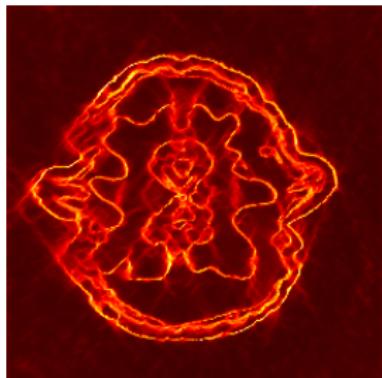


Sparse Bayesian Inference & Uncertainty Quantification for Inverse Imaging Problems



Felix Lucka

Centrum Wiskunde & Informatica
University College London
Felix.Lucka@cwi.nl

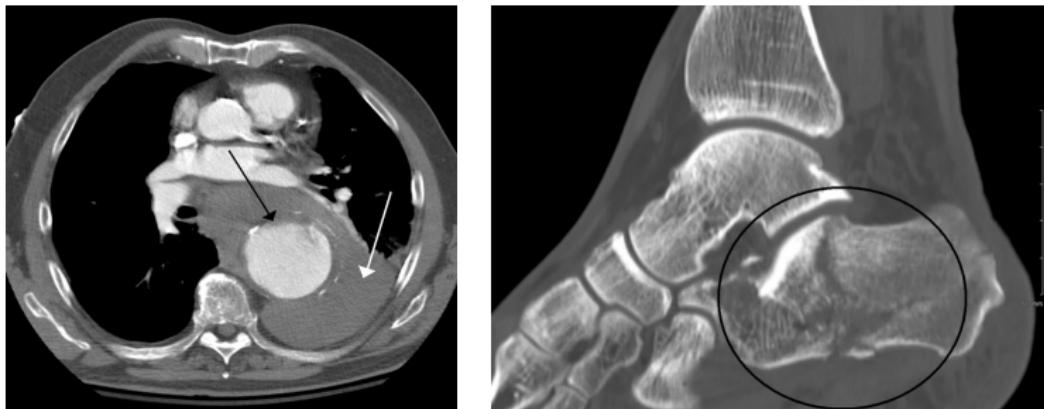
Statistics for Structures Seminar
Leiden

October 20, 2017

Big Picture: From Qualitative to Quantitative Imaging

Traditional task: Produce results to be interpreted by trained experts
⇒ Qualitative usage of the reconstructed information.

Example: Conventional computer tomography (CT).



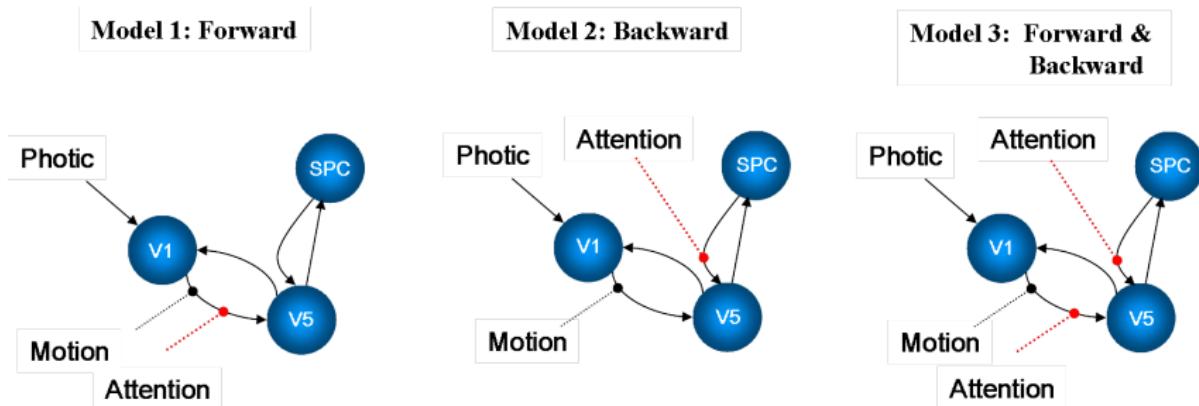
Source: Wikimedia Commons

Big Picture: From Qualitative to Quantitative Imaging

Traditional task: Produce results to be interpreted by trained experts
⇒ *Qualitative* usage of the reconstructed information.

New demand: Produce results for automatized analysis procedures /
hypothesis testing; multimodal imaging.
⇒ *Quantitative* usage of the reconstructed information.

Example: *Dynamical causal modeling (DCM)*.



Source: Andre C. Marreiros et al. (2010), Scholarpedia, 5(7):9568.

Bayesian Inversion and Uncertainty Quantification

Noisy, ill-posed inverse problems:

$$f = N(\mathcal{A}(u), \varepsilon)$$

Example: $f = Au + \varepsilon$

$$p_{\text{like}}(f|u) \propto$$

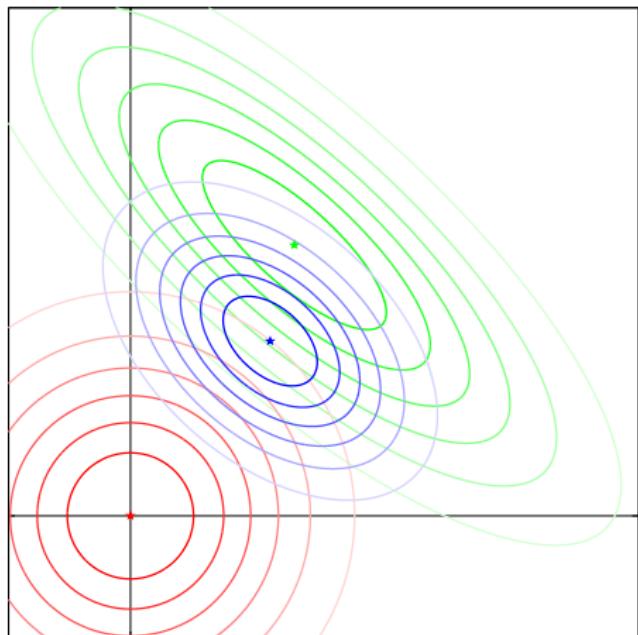
$$\exp\left(-\frac{1}{2}\|f - Au\|_2^2\right)$$

$$p_{\text{prior}}(u) \propto$$

$$\exp\left(-\lambda \|D^T u\|_2^2\right)$$

$$p_{\text{post}}(u|f) \propto$$

$$\exp\left(-\frac{1}{2}\|f - Au\|_2^2 - \lambda \|D^T u\|_2^2\right)$$



Probabilistic representation allows for rigorous **quantification of solution's uncertainties**.

Bayesian Inversion and Uncertainty Quantification

Noisy, ill-posed inverse problems:

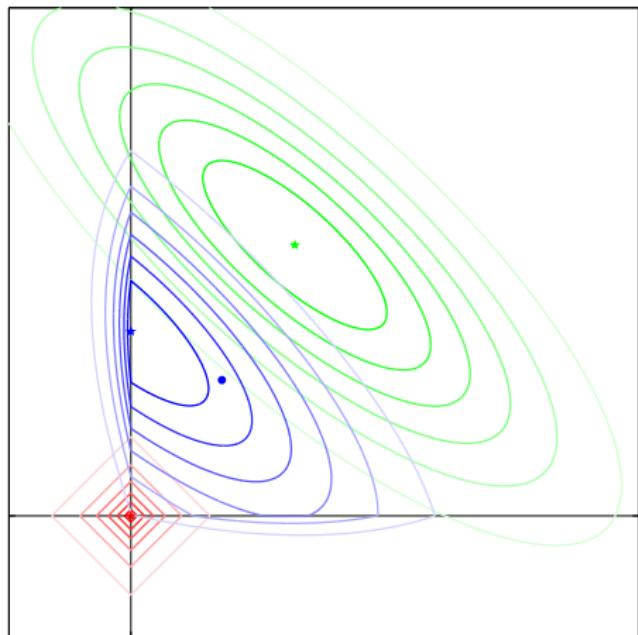
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$$\begin{aligned} p_{\text{like}}(f|u) &\propto \\ &\exp\left(-\frac{1}{2}\|f - Au\|_2^2\right) \end{aligned}$$

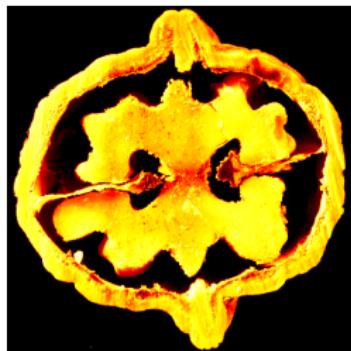
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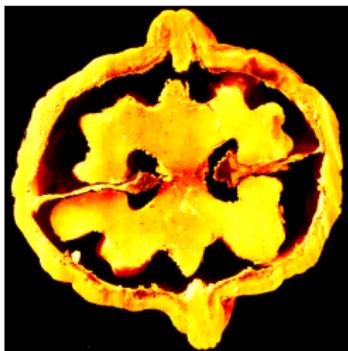


Probabilistic representation allows for rigorous **quantification of solution's uncertainties**.

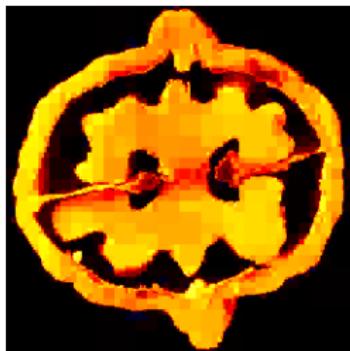
Sparsity / Compressible Representation



(a) 100%



(b) 10%



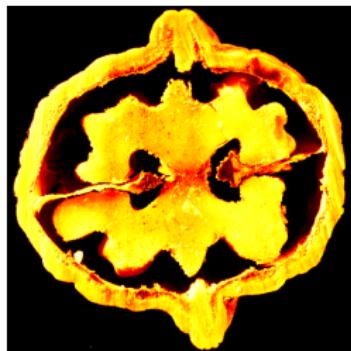
(c) 1%

Sparsity as a-priori constraints are used in variational regularization, compressed sensing and variable selection:

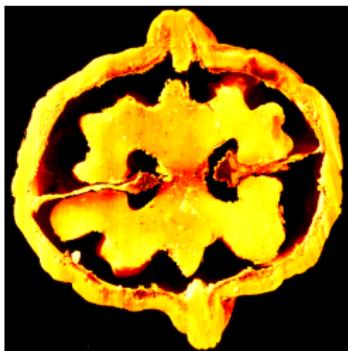
$$\hat{u}_\lambda = \underset{u}{\operatorname{argmin}} \left\{ \frac{1}{2} \|f - Au\|_2^2 + \lambda \|D^T u\|_1 \right\}$$

(e.g. *total variation*, *wavelet shrinkage*, *LASSO*,...)

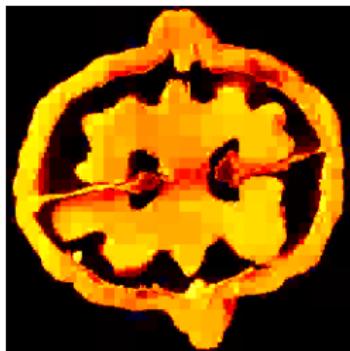
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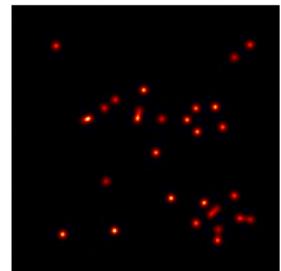
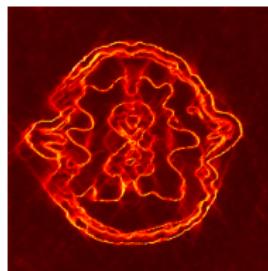
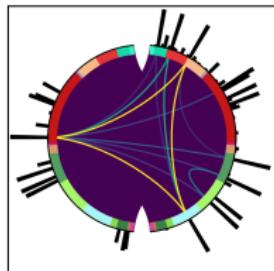
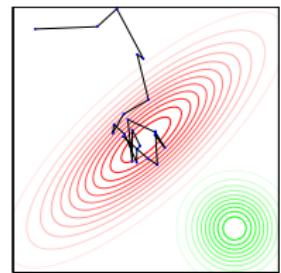
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(e.g. *total variation*, *wavelet shrinkage*, *LASSO*,...)

Sparse Bayesian inversion?

Uncertainty Quantification for Sparse Bayesian Inversion

- How to model sparsity?
 - ℓ_1 -norm priors.
 - Gaussian scale mixture (hierarchical Bayesian)
 - ℓ_p -norm scale mixture (hierarchical Bayesian)
- How to we compute estimators / UQ measures?
- What can we say about estimators?
- Meaningful UQ measures for sparse inversion/imaging?

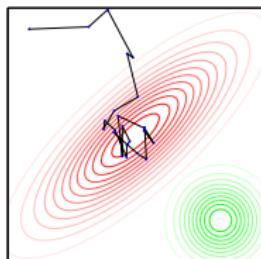


Efficient MCMC for Sparse Image Reconstruction

Task: Monte Carlo integration by samples from

$$p_{post}(u|f) \propto \exp\left(-\frac{1}{2}\|f - A u\|_{\Sigma_{\varepsilon}^{-1}}^2 - \lambda \|D(u)\|_1\right)$$

Problem: Standard [Markov chain Monte Carlo \(MCMC\)](#) sampler ([Metropolis-Hastings](#)) inefficient for large n or λ .



Efficient MCMC for Sparse Image Reconstruction

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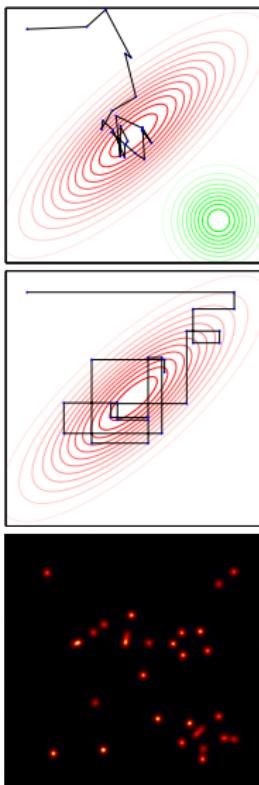
Problem: Standard [Markov chain Monte Carlo \(MCMC\)](#) sampler ([Metropolis-Hastings](#)) inefficient for large n or λ .

Contributions:

- Development of different [Gibbs samplers](#).
- Efficient for high-dim. imaging ($n > 10^6$).

 **F.L, 2016.** Fast Gibbs sampling for high-dimensional Bayesian inversion, *Inverse Problems*.

 **F.L, 2012.** Fast Markov chain Monte Carlo sampling for sparse Bayesian inference in high-dimensional inverse problems using L1-type priors, *Inverse Problems*.



Efficient MCMC for Sparse Image Reconstruction

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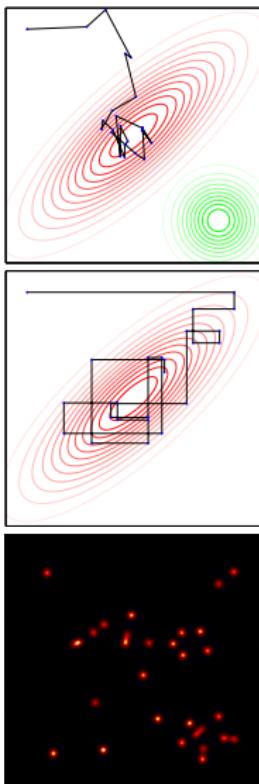
Problem: Standard [Markov chain Monte Carlo \(MCMC\)](#) sampler ([Metropolis-Hastings](#)) inefficient for large n or λ .

Work by Marcelo Pereyra et al.:

- Unadjusted Langevin algorithm applied to Moreau-Yoshida envelopes of posterior energy.
- As easy to implement as proximal gradient descent.



Durmus, Moulines, Pereyra, 2016. Efficient Bayesian computation by proximal Markov chain Monte Carlo: when Langevin meets Moreau, [arXiv:1612.07471](#).

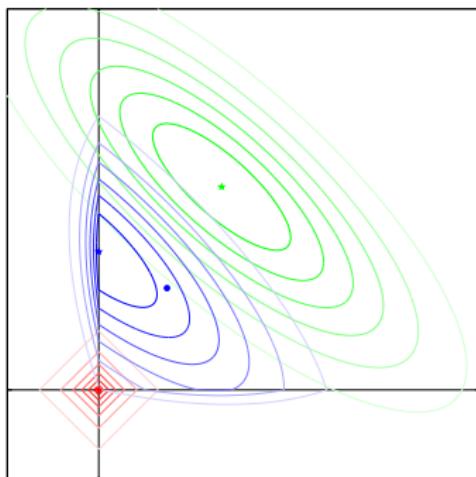


Point Estimators in Bayesian Inference for Imaging

$$\hat{u}_{\text{MAP}} := \underset{u \in \mathbb{R}^n}{\operatorname{argmax}} \{ p_{\text{post}}(u|f) \} \quad \text{vs.} \quad \hat{u}_{\text{CM}} := \int u \, p_{\text{post}}(u|f) \, du$$

State in imaging ~5 years ago:

- CM preferred in theory, inaccessible in practice.
- MAP discredited by theory, accessible in practice.



Point Estimators in Bayesian Inference for Imaging

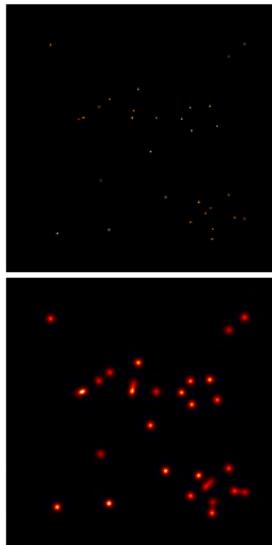
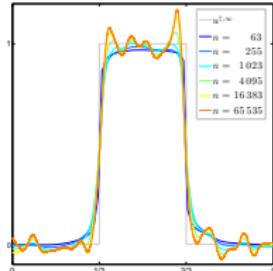
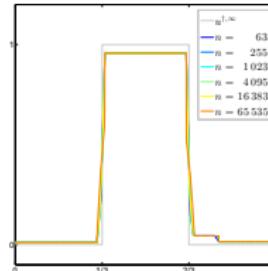
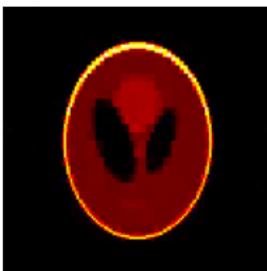
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State in imaging ~5 years ago:

- CM preferred in theory, inaccessible in practice.
- MAP discredited by theory, accessible in practice.

However:

- MAP results looks/perform better or similar to CM.
- Gaussian priors: $\text{MAP} = \text{CM}$. Funny coincidence?
- Theoretical argument has a logical flaw.



Point Estimators in Bayesian Inference for Imaging

$$\hat{u}_{\text{MAP}} := \underset{u \in \mathbb{R}^n}{\operatorname{argmax}} \{ p_{\text{post}}(u|f) \} \quad \text{vs.} \quad \hat{u}_{\text{CM}} := \int u \, p_{\text{post}}(u|f) \, du$$

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Contributions:

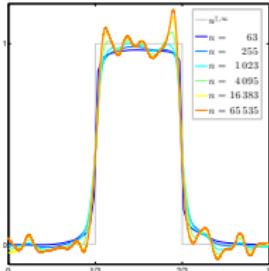
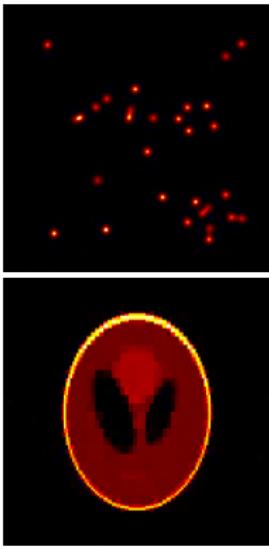
- Theoretical rehabilitation of MAP.
- Key: Bayes cost based on Bregman distances.
- Gaussian case consistent in this framework.



Burger & L, 2014. Maximum a posteriori estimates in linear inverse problems with log-concave priors are proper Bayes estimators, *Inverse Problems*, 30(11).

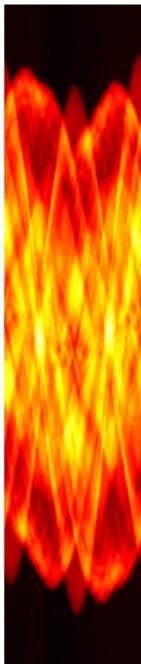
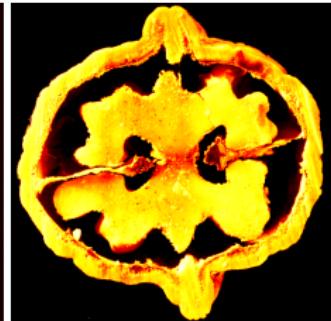
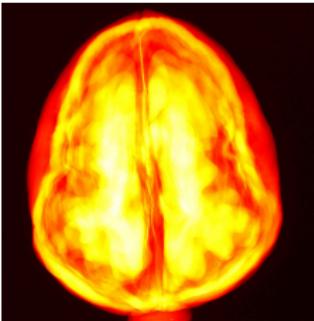
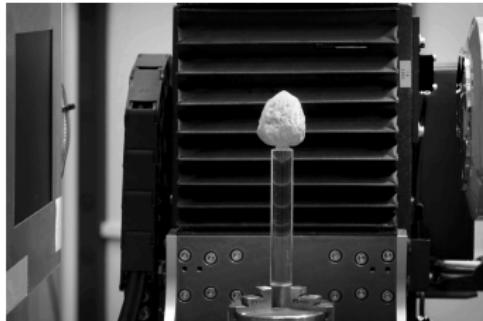


Helin & Burger, 2015. Maximum a posteriori probability estimates in infinite-dimensional Bayesian inverse problems, *Inverse Problems*, 31(8).



Experimental Data: Limited-Angle CT

- Cooperation with [Samuli Siltanen, Esa Niemi et al.](#)
- Besov and TV prior; non-negativity constraints.
- Stochastic [noise modeling](#).
- Uncertainty quantification for [limited angle CT](#).



Use the data set for your own work: arXiv:1502.04064)

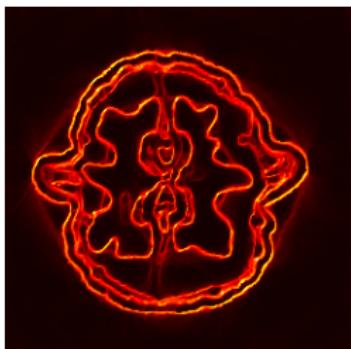
Walnut-CT with TV Prior: Full vs. Limited Angle



(a) MAP, full



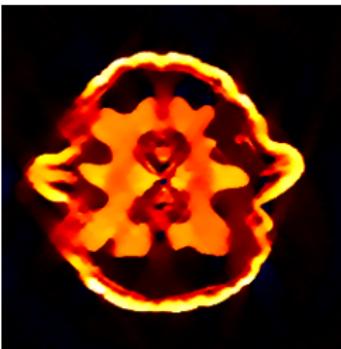
(b) CM, full



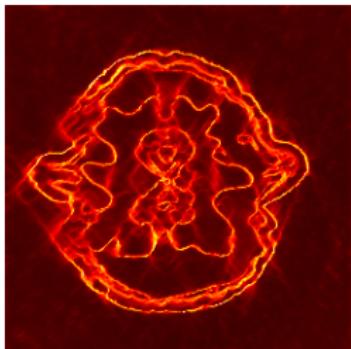
(c) CStd, full



(d) MAP, limited

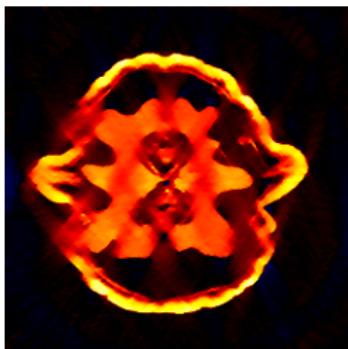


(e) CM, limited

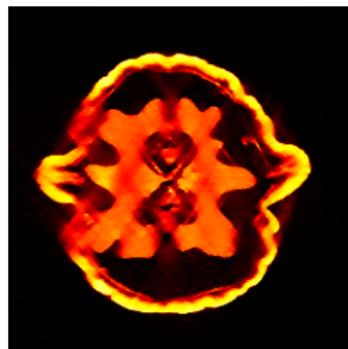


(f) CStd, limited

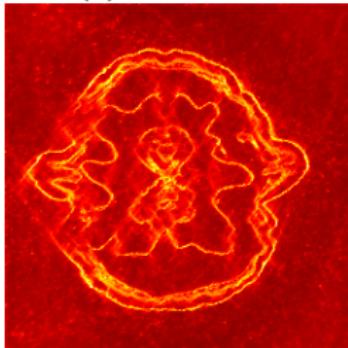
TV Prior, Non-Negativity Constraints, Limited Angle



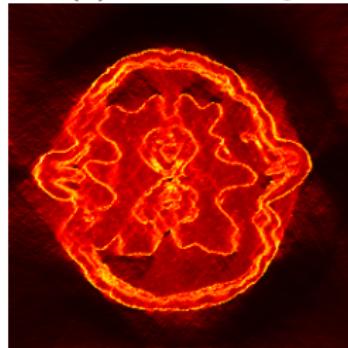
(a) CM, uncon



(b) CM, non-neg

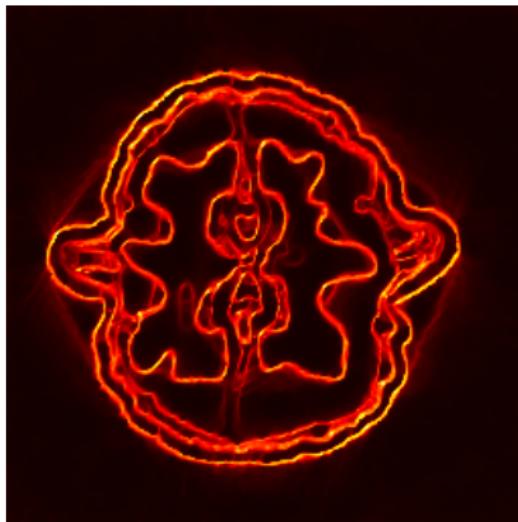


(c) CStd, uncon

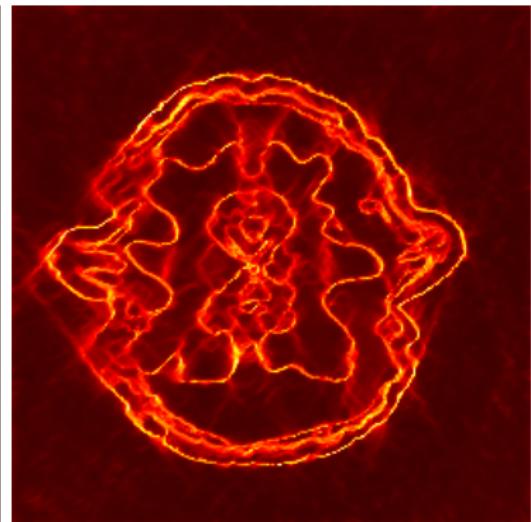


(d) CStd, non-neg

However...



(a) CStd, full



(b) CStd, limited

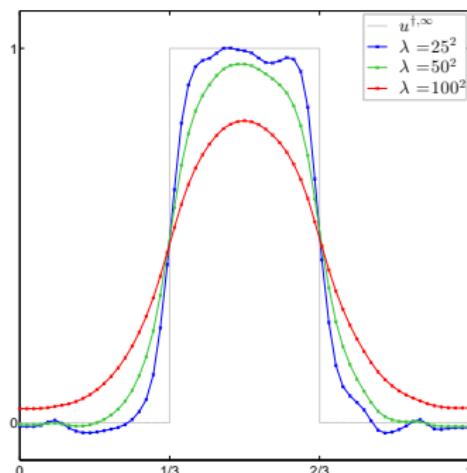
- What does it really tell me?
- Does the uncertainty decrease?!

Hierarchical Bayesian Modeling (HBM) of Sparsity

Gaussian increment prior:

$$p_{prior}(u) \propto \prod_i \exp\left(-\frac{(u_{i+1} - u_i)^2}{\gamma}\right)$$

- Gaussian variables live on characteristic scale, determined by γ .
- Similar amplitudes are likely, sparsity (= outliers) is unlikely.



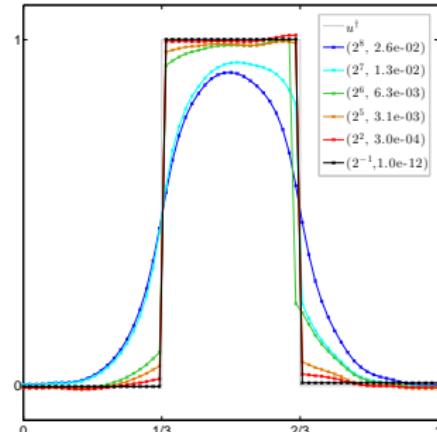
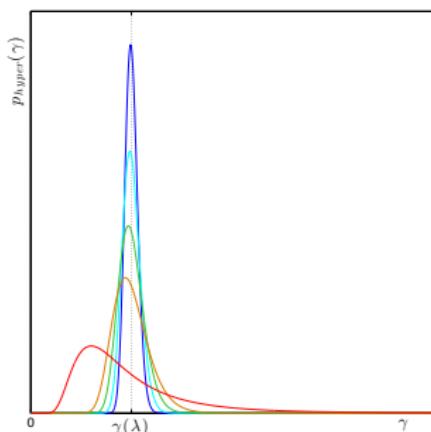
Hierarchical Bayesian Modeling (HBM) of Sparsity

Conditionally Gaussian increment prior:

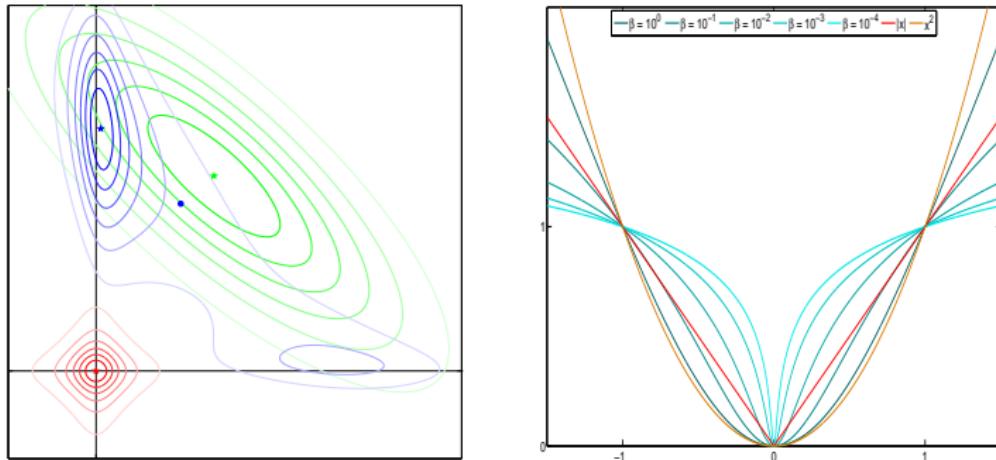
$$p_{prior}(u|\gamma) \propto \prod_i \exp\left(-\frac{(u_{i+1} - u_i)^2}{\gamma_i}\right)$$

Scale-invariant hyperprior to approximate un-informative γ_i^{-1} prior:

$$p_{hyper}(\gamma_i) \propto \gamma_i^{-(\alpha+1)} \exp\left(-\frac{\beta}{\gamma_i}\right), \quad \text{inverse gamma distribution}$$



The Implicit Energy Functional behind HBM

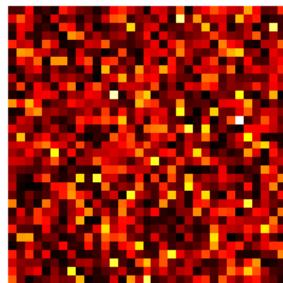
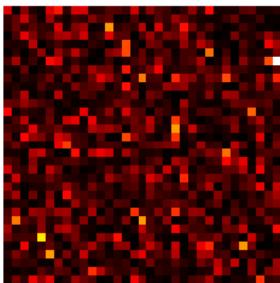
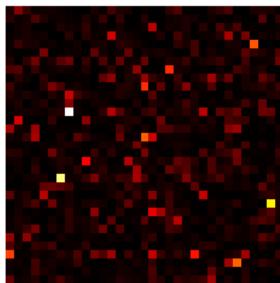
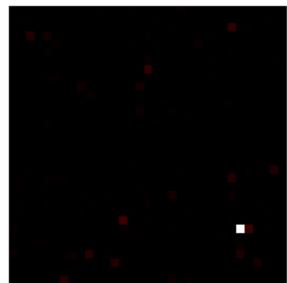


Implicit prior is a Student's t -prior with $\nu = 2\alpha, \theta = \beta/(2\alpha)$:

$$p_{prior}(u) \propto \prod_i \left(1 + \frac{u_i^2}{\nu\theta}\right)^{-\frac{\nu-1}{2}}$$

$$p_{post}(u|f) \propto \exp \left(-\frac{1}{2} \|f - A u\|_{\Sigma_\varepsilon^{-1}}^2 - \frac{\nu-1}{2} \sum_i \log \left(1 + \frac{u_i^2}{\nu\theta}\right) \right)$$

Prior Samples

(a) ℓ_2 (b) ℓ_1 (c) $\ell_{1/2}$ 

(d) Cauchy

$$p_{prior}(u_i) \propto \exp(-|u_i|^p) \quad vs. \quad p_{prior}(u_i) \propto \frac{1}{1 + u_i^2}$$

Why HBM? EEG/MEG Source Reconstruction

Aim: Reconstruction of brain activity by **non-invasive** measurement of induced electromagnetic fields outside of skull.



source: Wikimedia Commons

source: Wikimedia Commons

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Aim: Reconstruction of brain activity by **non-invasive** measurement of induced electromagnetic fields outside of skull.



source: Wikimedia Commons



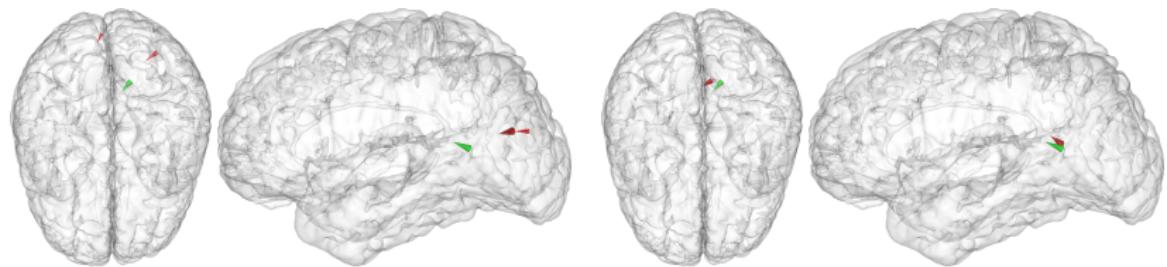
source: Wikimedia Commons



Notoriously ill-posed problem!

HBM for EEG/MEG Source Reconstruction

- Inversion with log-concave priors (e.g., ℓ_1 -type) suffers from systematic depth miss-localization, HBM does not.
- HBM shows promising results for focal brain networks with simulated and real data and EEG-MEG combination.



L., Pursiainen, Burger, Wolters, 2012. Hierarchical Bayesian inference for the EEG inverse problem using realistic FE head models: Depth localization and source separation for focal primary currents, *NeuroImage*, 61(4):1364–1382.

Comparison: Two Approaches to Sparsity

feature	ℓ_p prior	HBM
$\mathcal{J}(u)$	$\ u\ _p^p$	$\frac{\nu+1}{2} \sum \log \left(1 + \frac{u^2}{\nu\theta}\right)$
sparsifying parameter	$p > 0$	$\nu > 0$
quadratic limit	$p = 2$	$\nu \rightarrow \infty$
sparse limit	$p \rightarrow 0$	$\nu \rightarrow 0$
limit functional	$ u _0$	$\sum_i^n \log(u_i)$ if all $u_i \neq 0$, -∞ else
solutions	sparse	compressible
differentiable	$p > 1$	always
convex	everywhere for $p \geq 1$	$\ u\ _\infty < \sqrt{\nu\theta}$
homogeneous	yes	no

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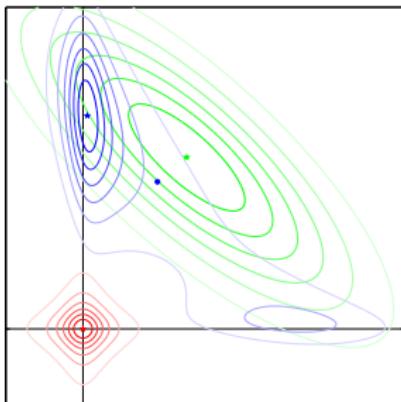
Combine them to get best (worst?!) of both worlds?

ℓ_p -hypermodels with generalized Gamma hyperpriors

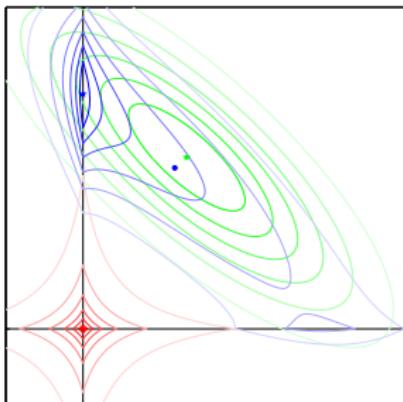
$$p_{prior}(u, \gamma) \propto \exp \left(- \sum_i \left(\frac{|D_i^T u|^p}{\gamma_i} + \frac{\gamma_i^r}{\beta} - (r\alpha - 1 - 1/p) \log(\gamma_i) \right) \right)$$

Implicit prior with inverse gamma hyperprior:

$$\prod_i \left(1 + \frac{|D_i^T u|^p}{\beta} \right)^{-\alpha-1/p}$$



(a) $p = 2$



(b) $p = 1$

ℓ_p -Hypermodels & Majorization-Minimization

Posterior with gamma hyperprior ($r = 1$), $p = 1$, and $\alpha = 2$:

$$p_{post}(u|f) \propto \exp \left(-\frac{1}{2} \|f - A u\|_2^2 - \sum_i \left(\frac{|D_i^T u|}{\gamma_i} + \frac{\gamma_i}{\beta} \right) \right)$$

Computational scheme for full-MAP estimation equivalent to majorization-minimization scheme for $\ell_{1/2}$ regularization (Adaptive Lasso):

$$u^{(k)} = \operatorname{argmin}_u \left\{ \frac{1}{2} \|f - A u\|_{\Sigma_\varepsilon^{-1}}^2 + \frac{1}{\sqrt{\beta}} \sum_i \frac{|D_i^T u|}{\sqrt{|D_i^T u|^{(k-1)}}} \right\}$$



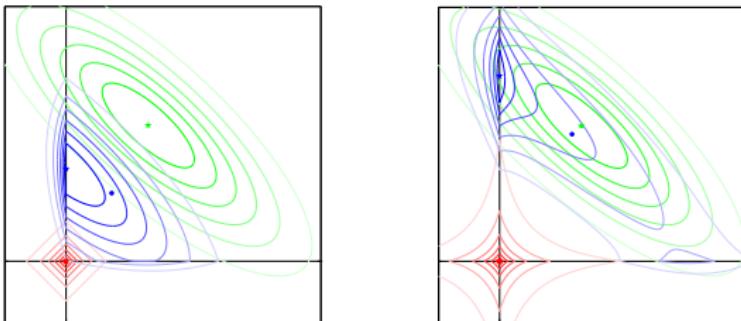
Bekhti, L, Salmon, Gramfort, 2017. A hierarchical Bayesian perspective on majorization-minimization for non-convex sparse regression: application to M/EEG source imaging, *almost submitted*.

Uncertainty Quantification for Non-Convex Sparse Recovery

Severely under-determined problems $f = Au$:

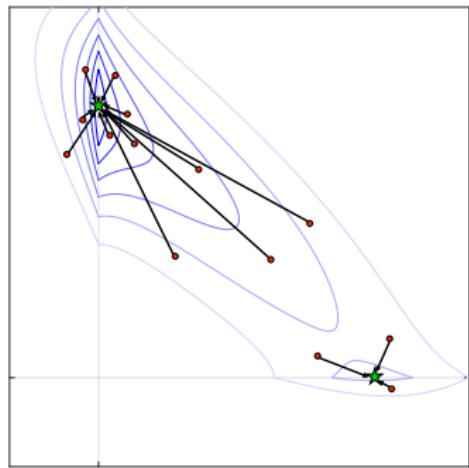
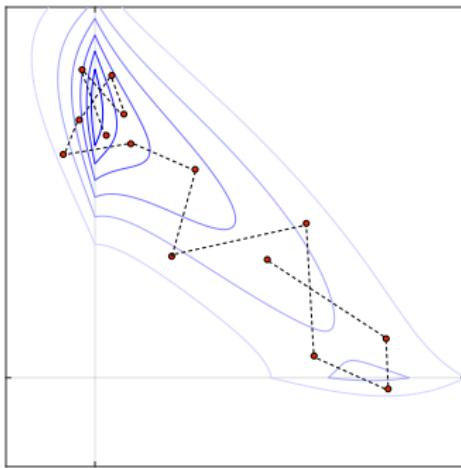
Many sparse solutions consistent with data!

- Log-concave priors erase this ambiguity and yield single result.
- HBM posteriors get multi-modal.
- Traditional UQ measure do not capture these aspects.
- Can we preserve but quantify, structure and visualize ambiguity?



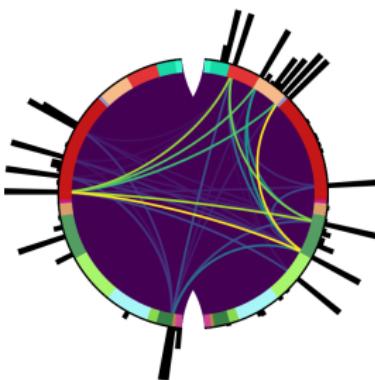
Mode Analysis with MCMC & Optimization

- Generate MCMC chain of posterior samples.
- Use every sample as initialization of gradient-based optimization.
- Analyse resulting chain of modes.

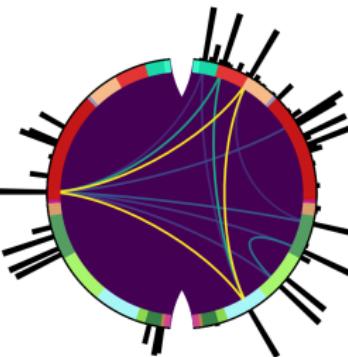


Sparse Source Network Analysis for EMEG Auditory Data

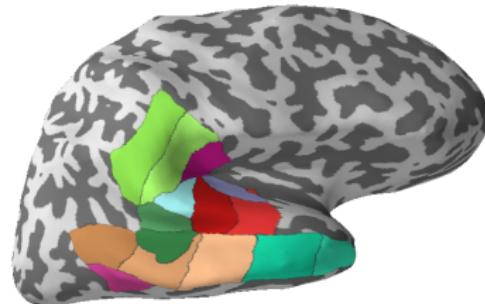
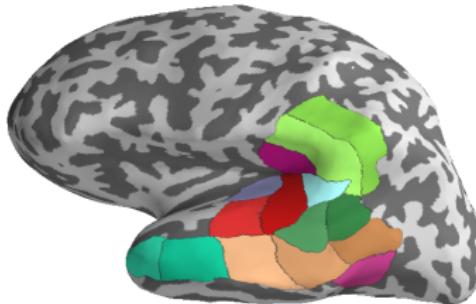
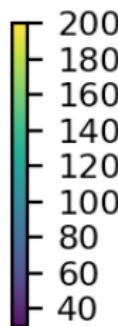
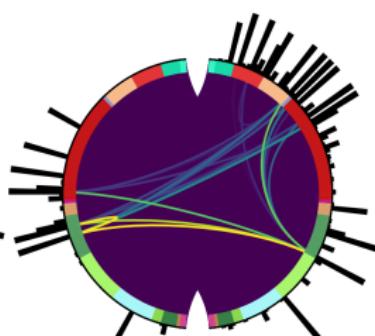
all 364 EEG+MEG



all 306 MEG



182 MEG+EEG



Summary, Outlook & Open Questions

- ℓ_p -norm and HBM road to sparsity: Neither perfect but (somewhat) computationally tractable. ↵ spike-and-slab priors?
- MAP estimates are proper Bayes estimators, modes are meaningful.
- However: Everything beyond point estimation is what's really interesting.
- Meaningful and interpretable UQ measures for sparse inversion / imaging that can complement variational approaches?
- Does it really make sense?
(over confidence in ill-posed problems, prior domination)

-  **Bekhti, L, Salmon, Gramfort, 2017.** A hierarchical Bayesian perspective on majorization-minimization for non-convex sparse regression: application to M/EEG source imaging, *almost submitted*.
-  **L, 2016.** Fast Gibbs sampling for high-dimensional Bayesian inversion, *Inverse Problems*.
-  **L, 2014.** Bayesian Inversion in Biomedical Imaging, *PhD Thesis, University of Münster*.
-  **Burger, L, 2014.** Maximum-A-Posteriori Estimates in Linear Inverse Problems with Log-concave Priors are Proper Bayes Estimators, *Inverse Problems*.
-  **L, 2012.** Fast Markov chain Monte Carlo sampling for sparse Bayesian inference in high-dimensional inverse problems using L1-type priors, *Inverse Problems*.
-  **L, Pursiainen, Burger, Wolters, 2012.** Hierarchical Bayesian inference for the EEG inverse problem using realistic FE head models: Depth localization and source separation for focal primary currents, *NeuroImage*.

Thank you for your attention!

-  **Bekhti, L, Salmon, Gramfort, 2017.** A hierarchical Bayesian perspective on majorization-minimization for non-convex sparse regression: application to M/EEG source imaging, *almost submitted*.
-  **L, 2016.** Fast Gibbs sampling for high-dimensional Bayesian inversion, *Inverse Problems*.
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MAP vs. CM Estimates: The Classical View

A theoretical argument "decides" the conflict: The **Bayes cost formalism**.

- An estimator is a random variable, as it relies on f and u .
- How does it **perform on average**? Which estimator is "best"?
- \rightsquigarrow Define a **cost function** $\Psi(u, v)$.
- Bayes cost is the expected cost:

$$BC(\hat{u}) = \iint \Psi(u, \hat{u}(f)) p_{like}(f|u) df p_{prior}(u) du$$

- Bayes estimator \hat{u}_{BC} for given Ψ minimizes Bayes cost. Turns out:

$$\hat{u}_{BC}(f) = \operatorname{argmin}_{\hat{u}} \left\{ \int \Psi(u, \hat{u}(f)) p_{post}(u|f) du \right\}$$

MAP vs. CM Estimates: The Classical View

Main classical arguments pro CM and contra MAP estimates:

- CM is Bayes estimator for $\Psi(u, \hat{u}) = \|u - \hat{u}\|_2^2$ (MSE).
- Also the **minimum variance estimator**.
- The mean value is intuitive, it is the "center of mass", the known "average".
- MAP estimate can be seen as an **asymptotic** Bayes estimator of

$$\Psi_\epsilon(u, \hat{u}) = \begin{cases} 0, & \text{if } \|u - \hat{u}\|_\infty \leq \epsilon \\ 1 & \text{otherwise,} \end{cases}$$

for $\epsilon \rightarrow 0$ (uniform cost). \implies It is not a proper Bayes estimator.

- MAP and CM seem theoretically and computationally fundamentally different \implies one should decide.
- *"A real Bayesian would not use the MAP estimate"*
- People feel "ashamed" when they have to compute MAP estimates (even when their results are good).

A False Conclusion

"A real Bayesian would not use the MAP estimate as it is not a proper Bayes estimator".

"MAP estimate can be seen as an asymptotic Bayes estimator of

$$\Psi_\epsilon(u, \hat{u}) = \begin{cases} 0, & \text{if } \|u - \hat{u}\|_\infty < \epsilon \\ 1 & \text{otherwise,} \end{cases}$$

for $\epsilon \rightarrow 0$.

??=?? It is not a proper Bayes estimator."

"MAP estimator is asymptotic Bayes estimator for some degenerate Ψ "
≠ "MAP can't be Bayes estimator for some proper Ψ " !!!

Two New Bayes Cost Functions

Define

$$(a) \Psi_{\text{LS}}(u, \hat{u}) := \|A(\hat{u} - u)\|_{\Sigma_{\varepsilon}^{-1}}^2 + \beta \|L(\hat{u} - u)\|_2^2$$

$$(b) \Psi_{\text{Brg}}(u, \hat{u}) := \|A(\hat{u} - u)\|_{\Sigma_{\varepsilon}^{-1}}^2 + \lambda D_{\mathcal{J}}(\hat{u}, u)$$

for a regular L and $\beta > 0$.

Properties:

- Proper, convex cost functions
- For $\mathcal{J}(u) = \beta/\lambda \|Lu\|_2^2$ (Gaussian case!) we have $\lambda D_{\mathcal{J}}(\hat{u}, u) = \beta \|L(\hat{u} - u)\|_2^2$, and $\Psi_{\text{LS}}(u, \hat{u}) = \Psi_{\text{Brg}}(u, \hat{u})$!

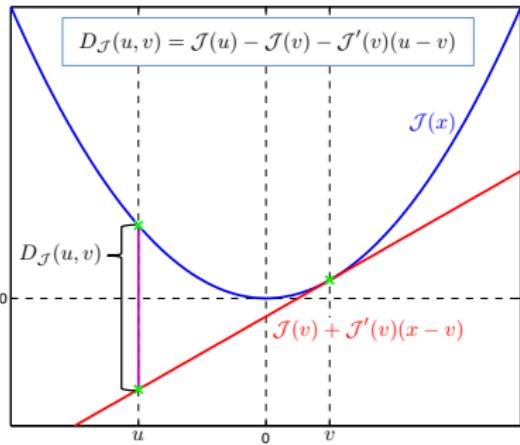
Theorems:

- (I) The CM estimate is the Bayes estimator for $\Psi_{\text{LS}}(u, \hat{u})$
- (II) The MAP estimate is the Bayes estimator for $\Psi_{\text{Brg}}(u, \hat{u})$

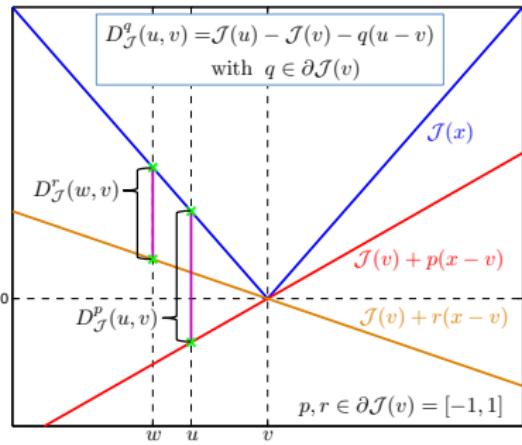
Bregman distances

For a proper, convex functional $\Psi : \mathbb{R}^n \rightarrow \mathbb{R} \cup \{\infty\}$, the *Bregman distance* $D_\Psi^p(f, g)$ between $f, g \in \mathbb{R}^n$ for a subgradient $p \in \partial\Psi(g)$ is defined as

$$D_\Psi^p(f, g) = \Psi(f) - \Psi(g) - \langle p, f - g \rangle, \quad p \in \partial\Psi(g)$$



(c) $J(x) = x^2$



(d) $J(x) = |x|$

Basically, $D_\Psi(f, g)$ measures the difference between Ψ and its linearization in f at another point g