scientific reports



OPEN

Impact of stain variation and color normalization for prognostic predictions in pathology

Siyu Lin¹, Haowen Zhou¹, Mark Watson², Ramaswamy Govindan³, Richard J. Cote² & Changhuei Yang¹⊠

In recent years, deep neural networks (DNNs) have demonstrated remarkable performance in pathology applications, potentially even outperforming expert pathologists due to their ability to learn subtle features from large datasets. One complication in preparing digital pathology datasets for DNN tasks is the variation in tinctorial qualities. A common way to address this is to perform stain normalization on the images. In this study, we show that a well-trained DNN model trained on one batch of histological slides failed to generalize to another batch prepared at a different time from the same tissue blocks, even when stain normalization methods were applied. This study used sample data from a previously reported DNN that was able to identify patients with early-stage non-small cell lung cancer (NSCLC) whose tumors did and did not metastasize, with high accuracy, based on training and then testing of digital images from H&E stained primary tumor tissue sections processed at the same time. In this study, we obtained a new series of histologic slides from the adjacent recuts of the same tissue blocks processed in the same lab but at a different time. We found that the DNN trained on either batch of slides/images was unable to generalize and failed to predict progression in the other batch of slides/images (AUC_{cross-batch} = 0.52 - 0.53 compared to AUC_{same-batch} = 0.74 - 0.81). The failure to generalize did not improve even when the tinctorial difference corrections were made through either traditional color-tuning or stain normalization with the help of a Cycle Generative Adversarial Network (CycleGAN) process. This highlights the need to develop an entirely new way to process and collect consistent microscopy images from histologic slides that can be used to both train and allow for the general application of predictive DNN algorithms.

The past decade has witnessed wide applications of deep neural network (DNN) models in biomedical and digital pathological analysis due to the growing complexity and training techniques of DNN models. There are increasing examples of the ability of DNN-based methods succeeding in tasks that are simply beyond the scope of even expert pathologists. For example, Bychkov et al. demonstrated that their trained DNN model for analyzing H&E stained colorectal cancer tumor tissue microarray digital images was able to classify patient risk more accurately than human pathologists¹. Hekler et al. showed that their trained DNN outperformed 11 pathologists in the classification of histopathological images between benign nevi and malignant melanoma² and Tschandl et al. demonstrated that DNNs consistently outperform expert pathologists in classifying pigmented skin lesions³. Bejnordi, et al. showed that trained deep learning models outperformed expert pathologists in simulated time-constrained settings for detecting lymph node metastases in breast cancer tissue sections⁴. We recently completed a pilot study that showed that DNN can be trained to predict the subsequent development of brain metastases in patients with early-stage NSCLC based on images obtained from Hematoxylin-and-Eosin (H&E) stained slides of their primary tumors⁵ - a task that human pathologists can do little or no better than a random guess. This clearly demonstrates that DNN training can detect subtle features in these images that are simply not recognizable by even expert pathologists. In our pilot study, the DNN was trained based on a ResNet⁶ model pretrained on ImageNet with naturalistic objects. Recently new foundational models have been developed that are pre-trained and specialized for pathology tasks⁷⁻¹⁰. These foundational models may have even greater potential to capture minute relevant features for digital pathology tasks.

However, DNN's capability to detect and use these subtle features is tempered by DNN's vulnerability to fixate on extraneous variations, in particular variations in tinctorial qualities that are a well-recognized and inherent aspect of the staining of histologic tissue sections with vital stains, a problem that is amplified when training is

¹Department of Electrical Engineering, California Institute of Technology, Pasadena, CA 91125, USA. ²Department of Pathology and Immunology, Washington University School of Medicine, St. Louis, MO 63110, USA. ³Department of Medicine, Washington University School of Medicine, St. Louis, MO 63110, USA. [∞]email: chyang@caltech.edu

done on small, homogeneous, well-qualified data sets that would otherwise be ideal for DNN training^{11,12}. The most straightforward way to force the model to ignore these extraneous variations in staining qualities is to train the DNN with an enormous and varied amount of data (i.e., images) such that, ideally, the model will see these different variations and eventually learn to ignore them^{13,14}. This method is well suited for everyday tasks such as ImageNet classification networks where there are a lot of public-domain images available for training. However, this †big data' AI training approach is not well suited for histopathology prediction applications. Prospective large histopathology image data sets with known disease outcomes are difficult and costly to assemble, especially for rare diseases. This is especially true as the "best" source of histologic images that would be useful for training a potential predictive algorithm is from a clinical trial with known treatment and outcomes, which is inherently limited or simply does not exist. Even where the data exists and is accessible, the data format and collection methodology can vary widely across the data collection sites. An alternate strategy to this †big data' approach is to curate or modify the data set to reduce variations prior to DNN training and usage. This approach is well-suited for pathology applications, as far more control can be exerted over the sample and data preparation process in pathology than in most other image-based applications. However, this approach has the disadvantage of being reliant on a smaller data set, more prone to being unable to factor in variations in alternative histology preparations, and thus far less generalizable.

Towards this end, color normalization of digital pathology data is an active area of research. One common image processing-based normalization method that performs stain normalization proposed by Vahadane et al¹⁵ is purely based on image analysis so that it can learn the stain strengths from one sample image or a collection of example images and normalize all other images towards this staining (Fig.1b). This method performs sparse non-negative matrix factorization to separate different staining in the source and target images and then color-normalize the images while preserving the structures in the images¹⁵. Other image-processing-based stain normalization methods include Macenko¹⁶ and Reinhard¹⁷. They work in a similar way - extract stain strengths from some reference images and then color-tune any given image towards the stain characteristics.

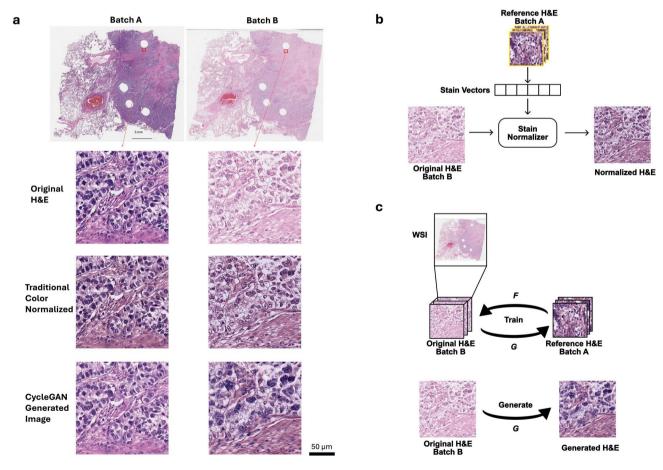


Fig. 1. (a) Stain variations in H&E-stained adjacent non-small cell lung cancer (NSCLC) histology slides. The left and right slides (top row) are adjacent cuts from the same tissue block from the same patient. Zoomin regions show original H&E-stained images (top row) as well as their color-normalized images with a traditional Vahadane method (middle row) and CycleGAN generative method (bottom row) demonstrating the effects of different color-normalization schemes. (b) Illustration of the traditional Vahadane method for color normalization of an image where batch B images are normalized to batch A images. (c) Illustration of a generative method for color normalization via CycleGAN.

The limitation of such methods is that they require the sample images to be representative of the whole dataset in terms of the staining and cellular contents. More recent machine learning-based methods allow the algorithm to take morphological structures and cellular context into account^{4,18}. Normalization can also be achieved through a generative model like a Cycle Generative Adversarial Network (CycleGAN) which has demonstrated success relative to other normalization methods¹⁹. After training, such generative networks can take an image from one color space and transfer it into a different color space or they can paint an unstained image with pseudostainings^{20,21}. Color normalization can be performed this way by projecting all images to one single color space (Fig.1c) specified by a set of reference images. CycleGAN-based method allows the potential change of cell morphology in the normalized image whereas the traditional method preserves the structures in the images.

Figure 1a shows a pair of example images of non-small cell lung cancer (NSCLC) tissue slides that are adjacent cuts from the same tissue block from the same patient. They were cut and stained in the same laboratory but at a different time. The distances between the adjacent cuts are 10–20 µm. Since the two cuts were next to each other, one would expect the cellular content to be similar. However, in the original (batch A) H&E images, the staining in the slide was heavier/darker (more basophilic) than in the second set of stains on the adjacent cut (batch B), leading to a contrast difference between the image pair. The traditional Vahadane method ¹⁵ was able to reduce the contrast difference somewhat, but the remaining differences are apparent, and one can easily appreciate that batch A is still darker than batch B, a difference that can be especially appreciated in the nuclei, where nuclear detail in batch B is more apparent (note easily identifiable nucleoli) compared to batch A, where nuclear detail is obscured due to the darker (more basophilic) staining (Fig. 1a). Using a CycleGAN-base method, the tinctorial qualities between batch A and B appeared more similar; however, in this case, note that the cellular morphology between the batches has altered, most notably in the nuclei, where the nuclei in batch B appear larger and more pleomorphic than in the images for batch A.

In this study, we have set out to determine the impact of staining variation on the generalizability of a predictive DNN algorithm. We have explored key issues inherent in DNN-driven analysis, including whether predictive algorithms, especially those derived from smaller data sets, "work" simply because of overfitting of data, whether advanced color normalization schemes can address the inherent and pervasive impact of stain variability, and if there might be alternative approaches to this important barrier to DNN training and general use.

Materials and methods

Patient cohort and whole-slide imaging

The cohort of patients were all diagnosed with stage I-IV NSCLC all diagnosed and treated at Washington University School of Medicine with long-term follow-up (> 5 years or until metastasis)⁵. This is the same cohort as was used in Ref.⁵. A total of 198 patients was included in the study and one representative block of tumor tissue from each patient was used to create a fresh H&E slide which was then scanned at 40 × magnification with an Aperio/Leica AT2 slide scanner (Leica Biosystems, Deer Park, IL, USA). The original cuts, denoted batch A, and the recuts, denoted batch B, were prepared in the same laboratory at a different time (separated by 8 months) where the original cuts and the recuts are separated by 10-20 μ m. Each batch was prepared within a relatively short time window. All slides were initially subject to blind review to assess tumor adequacy by an expert pathologist and annotated for ROI by circling an approximate contour of the primary tumor, including the entirety of the tumor microenvironment. Forty-four cases were disqualified as being non-representative or insufficient for adequate evaluation or had a missing recut slide. The remaining 154 cases were used for this study with 63 of them developing metastasis (Met+) to the central nervous system and 91 with no recurrence (Met-). The median time to progression or the follow-up time of these cohorts was 12.2 and 106 months, respectively. Detail information of the stages and the histology of the tumors are summarized in Table 1. The DNN model is blind to the clinical parameters such as stage and histology.

Data preprocessing

The data preprocessing procedure used for this study is similar to the one in Ref.⁵. The Otsu thresholding method²² was used on the annotated regions to further exclude the empty areas for each whole-slide image (WSI) and to form the ROI on each slide. Then 1000 image tiles were randomly sampled from each WSI, each with 256 x 256 pixels or 130 x 130 μ m² under 20× magnification, digitally down-sampled from a 512 × 512 pixels 40x magnification image. In the training process, random rotations, random flips, and random crops to 224 × 224 pixels were performed as data augmentation.

Deep learning study design

The DNNs were based on the ResNet-18 convolutional neural network pretrained on the ImageNet dataset⁶. The models were initialized with the pretrained weights, and all model layers were unfrozen during the training process. A linear layer was attached at the end of the model followed by a sigmoid activation function that generated a normalized prediction score from each individual tile. The prediction scores were then supervised with the known Met+/Met- outcome. Finally, the progression risk prediction of a WSI was given by the median of the prediction scores of all the individual image tiles associated with the slide.

Since the total number of patients in the study was only 154, to avoid potential bias in the testing set selection from a single experiment, we used a 3-fold experiment format with different training-testing splits where the training set and testing set will be comprised of data from different patients. No color normalization was performed in these control experiments (no color correction involved). The entire cohort of patients was randomized and numbered from 1 to 154. The randomized patient sequence was used to divide the cohort into a training/validation set (n = 118; Met+ n = 45, Met- n = 73) and a testing set (n = 36; Met+ n = 18, Met- n = 18) in each experiment fold. Specifically, in the first fold of this experiment, the model will be trained on original

| | No progression (n = 91) | Progression (n = 63) |
|-------------------------------|-------------------------|----------------------|
| Gender | | |
| Male | 46 | 25 |
| Female | 45 | 38 |
| Average age at DX | 60 (47–78) | 57 (25-73) |
| Histology | , | |
| Adenocarcinoma | 47 | 45 |
| Squamous cell | 31 | 11 |
| Large cell | 2 | 0 |
| BAC | 4 | 0 |
| Poorly differentiated | 1 | 5 |
| Mixed | 5 | 5 |
| Grade | | |
| 1 | 12 | 4 |
| II | 47 | 26 |
| II | 23 | 28 |
| IV | 0 | 1 |
| ND | 8 | 7 |
| Stage | | |
| 1 | 82 | 29 |
| II | 3 | 12 |
| III | 0 | 10 |
| IV | 0 | 1 |
| ND | 5 | 11 |
| Median follow-up time (month) | 106 | 12.2 |

Table 1. Clinical characteristics of the cohort in this study.

cuts (batch A) data of patient 1-118 and then tested on batch A and adjacent recuts (batch B) data of patient 119-154. Figure 2a illustrates this particular experiment. In the other folds of this experiment, we used batch A and batch B data subjects 83-118 and 47-82 as their respective testing set and trained on batch A data of the rest of the subjects.

A similar experiment was then repeated with the Vahadane color normalization method. We extracted 100 random image tiles for each slide in the training set. As shown in Fig. 1b, the staining vectors of each selected tile were computed based on the algorithm outlined by Vahadane et al. 15, and the mean of the staining vectors was used to perform structural-preserving normalization for every image tile in the testing set. The experiments followed the same format as the control experiments. Figure 2b shows an example data flow chart and the placement of the color normalization step in the process.

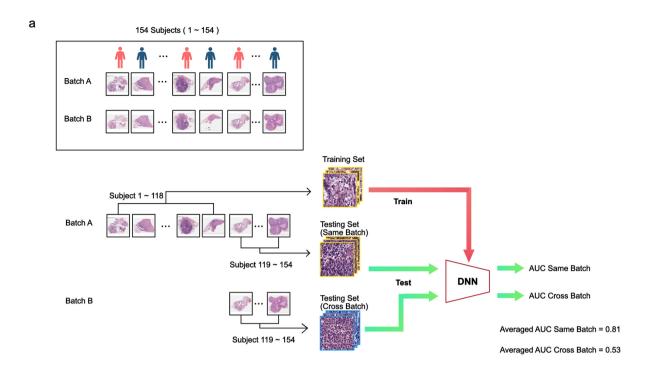
Finally, the experiments were repeated with generative color normalization. For every slide from the testing set, regardless of whether it was from batch A or batch B, we trained a CycleGAN with unpaired data that alternatively projected between the images from the testing slide and images from the slides in the entire training set until the generated images from the testing slide are indistinguishable from the training set images to the model discriminator. We then fed the generated images into the trained models to test the model performance. Once again, the experiments followed the same format as the control experiments. Figure 2c shows an example data flow chart and the placement of the CycleGAN color normalization step in the process.

Statistical analysis

To assess the effectiveness of our DL-based classifier in predicting progression risk, the area under the receiver operating characteristic (ROC) curve (AUC) was calculated to provide a measure of the overall performance of the model. To compare the model outputs with the ground-truth clinical progression outcomes, we binarized the model prediction scores and reported the accuracy metric. p values were calculated to show the performance difference of the model tested with color-normalized images compared with the model tested with original H&E images.

Color analysis

The effectiveness of the color-normalization schemes can not only be seen from their impact on DNN performance but also assessed through the resulting pixel intensity distributions. Specifically, we performed different stain normalization schemes for every whole slide image and generated the histogram distribution for red, green, and blue channels for every slide. The slide-to-slide variation in pixel intensity histogram can then be compared among the resulting images from different stain-normalizing methods as well as the original H&E images.



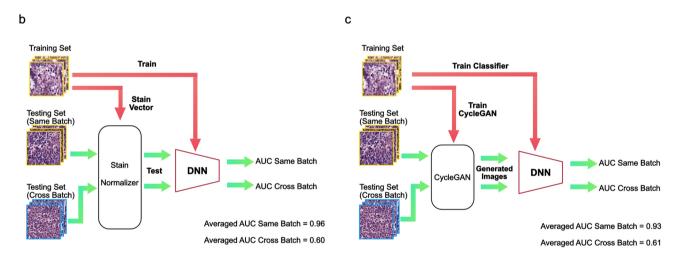


Fig. 2. Training and testing flow charts. (a) The cohort consists of 154 subjects, randomized and labeled with indices 1-154. The subject's biopsy histopathology slides were prepped and scanned on two separate occasions, resulting in two separate pathology image sets denoted by batch A and batch B. In the example illustrated above, we reserved slides of subject 119-154 of batch A as the same-batch testing set, and the rest of the batch A as the training set. The slides of the same subject (subject 119-154) from batch B served as the cross-batch testing set. The trained DNN was then be used to analyze the same-batch testing set slides to yield an AUC_{same-batch} value. We performed the same DNN classification on the cross-batch testing set slides to yield an AUC_{cross-batch} value. This whole training-and-analysis process was repeated three-fold by using different subjects as the test subjects. Specifically, fold-2 would use subject 83-118 as test subjects and fold-3 would use subject 47-82 as test subjects. The average AUC_{same-batch} and AUC_{cross-batch} from the 3-fold experiment are reported above. (b) Training and testing flow chart for a traditional color normalization method. The processing sequence is similar to that for the standard training and testing flow chart. Here, we performed traditional color normalization on the testing set images prior to feeding them through the trained DNN for classification. (c) Training and testing flow chart. Here, we performed generative color normalization on the testing set images prior to feeding them through the trained DNN for classification.

Results

Overall Scheme: Our goal was to study the impact of color variation on DNN generalizability and whether traditional or generative normalization techniques can improve DNN model generalizability both within and across batches of data with different staining. We have recently reported on the successful use of DNN to predict NSCLC metastasis based on the original diagnostic histology and used this as the model DNN case. That study used a batch of H&E stained slides (batch A) that were prepped and scanned within a small time window (one day) in a single lab. This created a data set that was fairly uniform in its tinctorial qualities. We speculated that this homogeneity, in part, explained why the training set required in that study was remarkably small (200 slides), and yet the trained DNN was able to perform its prediction task with remarkable accuracy (AUC = 0.96, p<0.0001). In other words, the data set appeared to have few extraneous variations that would otherwise distract the DNN.

For our current study, we additionally collected a second batch of H&E stained slides (batch B) that were prepped from adjacent cuts from the same cohort's tissue blocks. This batch of slides was also prepped and scanned within a small time window (one day) in the same lab and was prepped \sim 8 months after batch A. We expected that this data set would be fairly uniform in its stain contrast as well, but that the overall stain contrast profile would differ from that of batch A (as is evident in Fig. 1a).

We then trained separate DNN models using Batch A data and Batch B data and compared the performance when the models were used to analyze test slides that were set aside from the training processes. The test slides were either from the same batch or were the corresponding adjacent slides in the other batch. Next, we repeated the experiment where we used a traditional color normalization method to color-tune the images in the testing set towards the training set and assess the model testing performance. Last, we repeated the experiment where the color normalization was done through a CycleGAN method.

The above-described study design allowed us to generate an AUC score for when a DNN was trained on training data from a batch and tested on a set-aside collection of test slides from the same batch. We labeled this AUC score as AUC_{same-batch}. We can also generate a different AUC score - AUC_{cross-batch}, for when a DNN was tested on corresponding slides from the same subjects but from the other batch. As we performed each experiment in 3-fold, we can compute the average of these AUC scores. As noted in Fig. 2a, when the model was trained on training data from batch A and tested on set-aside data from batch A, the model was able to successfully predict metastatic outcome with an average AUC_{same-batch} of 0.81. This corresponded well with the results reported in Ref.⁵. (We noted that the results are not identical because some slides used in Ref.⁵ were excluded due to lack of corresponding adjacent cuts in batch B, and Vahadane¹⁵ color normalization was performed in Ref.⁵.) The predictive power of this model was statistically significant compared to a no-prediction-value null hypothesis with a p-value < 0.0001. Interestingly, the model trained on training data from batch A failed to generalize when tested on testing set data from batch B yielding an average AUC_{cross-batch} scores of 0.53 with a p-value > 0.05 compared to a no-prediction-value null hypothesis. In summary, in a control experiment with no color normalization, a DNN can be trained to make statistically meaningful predictions when the training set and testing set data originated from the same batch (but did not contain overlapping slides), but the same trained DNN failed to generalize to the other batch.

The traditional color normalization experiment with the Vahadane 15 method (see Fig. 3) yielded an averaged $AUC_{\text{same-batch}}$ of 0.96. However, the model trained on training data from batch A failed to generalize when tested on testing set data from batch B yielding an average $AUC_{\text{cross-batch}}$ score of 0.60 with a p-value> 0.05 compared to a no-prediction-value null hypothesis.

In the final experiment where CycleGAN color normalization was employed, the DNN achieved an averaged $AUC_{same-batch}$ of 0.93. In addition, the model trained on training data from batch A failed to generalize when tested on testing set data from batch B yielding an average $AUC_{cross-batch}$ score of 0.61 with p-value > 0.05 compared to a no-prediction-value null hypothesis.

In all the experiments described above, the models were trained with batch A data and evaluated on batch A and batch B data of the patients in the testing sets. We can also swap the role of Batch A and B and repeat all of the experiments, with the only difference being that we train the models on batch B instead and we color normalize the testing images towards the training set of the batch B data. All the results are summarized in Table 2. When we train on batch B, we see similar trends in that when the model was tested cross-batch (on batch A), the model failed to generalize.

With regards to color normalization impact on DNN's performance on same batch data, the slightly improved $AUC_{same-batch}$ scores suggest there may be some improvements. However, when checking the associated p-value with a Bonferroni multi-comparison corrected alpha of 0.05/4, we found that in all cases except one, the increased $AUC_{same-batch}$ did not rise above statistical significance. The sole exception is that the increased $AUC_{same-batch}$ for the experiment where Vahadane color normalization method was used for the DNN trained on the training set data from batch A and tested on the testing set data from batch A. That case gave a p-value of 0.010 which is lower than the Bonferroni corrected alpha of 0.0125. However, the p-value is so close to the alpha that we would caution against overreading the statistical significance of that result.

We further evaluated DNN's performance with other traditional normalization schemes such as the Macenko¹⁶ and Reinhard¹⁷ methods. Specifically, we repeated the experiments outlined in Fig. 2b, but with Macenko and Reinhard methods to normalize all image tiles. These normalization approaches did not yield AUC results that were substantially different from what Vahadane color normalization method provided (see Supplemental Table S1 for details.)

Additionally, we also investigated whether a pathology foundational model would provide better performance with or without color normalization. Specifically, we repeated all the experiments with a trained pathology foundational model Prov-GigaPath⁸ and analyzed the effects of color normalization schemes on the model performances. The overall performances with the Prov-GigaPath model were similar to those with the ResNet

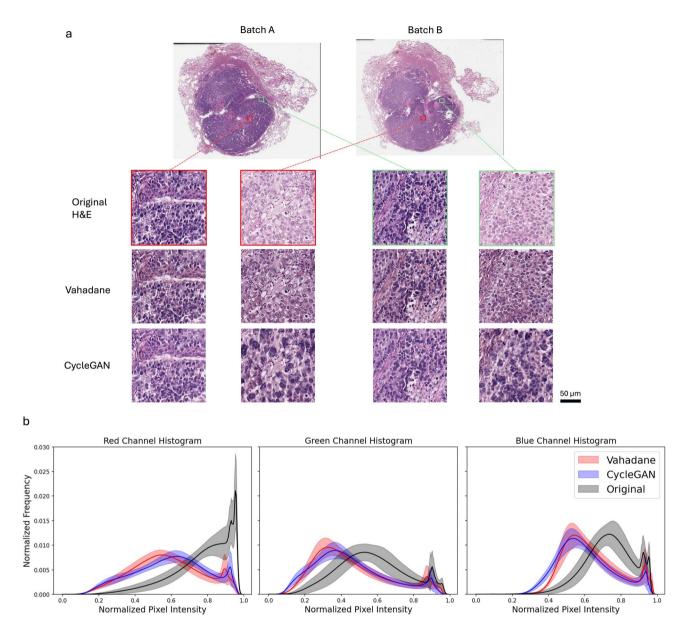


Fig. 3. (a) Example images of H&E stained tissues from adjacent cuts as well as the results of various traditional and generative color normalization methods. Red and green boxes indicate two pairs of images from neighboring tissue regions. (b) Slide-level histograms of normalized pixel intensities of red, green, and blue channel of the original H&E as well as color-normalized images from the testing set of one experiment. The shaded area indicates the \pm 1 standard deviation in slide-to-slide variations.

model. Prov-GigaPath DNN was able to discern features in the histologic slides that were predictive of metastatic outcome, and this performance was enhanced by color normalization schemes. However, the Prov-GigaPath DNN was also unable to generalize across batches. (see Supplemental Table S2 for details.)

The failure of color normalization to help DNN generalize in this case study points to the fact that current color normalization methods are not capable of fully mapping subtle stain variations with sufficient fidelity between data sets with different staining contrasts. This lack of fidelity is in fact visible to the expert human eyes, as further seen in Fig. 3a. We note that the tinctorial qualities of Batch A and B are different, with greater basophilia in batch A. Using Batch A H&E images as the baseline for normalization, we can appreciate that the Vahadane color normalization corrects this to some extent, although there are clear differences between the Batch A and normalized Batch B; for example, note that the nuclei in Batch A are more basophilic, and there is greater nuclear detail in normalized Batch B, such as the clear presence of nucleoli (arrow). The CycleGAN-generated Batch B images appear to have somewhat more consistent tinctorial qualities with Batch A (baseline); however, the CycleGAN process appears to have resulted in distinct morphological changes, particularly notable in the nuclei, which appear more basophilic and pleomorphic compared to Batch A baseline (arrow).

We can further assess the effectiveness of the Vahadane and generative color-normalization schemes through the resulting pixel intensity distributions. We plot the pixel-intensity histograms of the testing slides of batch A

| Testing set | Batch A | Batch B | |
|--------------------|----------------|----------------|--|
| Train on Batch A | | | |
| Original H&E | 0.81 | 0.53 | |
| Traditional method | 0.96(p=0.010) | 0.60 | |
| Generative method | 0.93 (p=0.069) | 0.61 | |
| Train on Batch B | | | |
| Original H&E | 0.52 | 0.74 | |
| Traditional method | 0.58 | 0.88 (p=0.033) | |
| Generative method | 0.52 | 0.87 (p=0.033) | |

Table 2. Results summary of all experiments where we train the models on either batch and test the models within the same-batch or cross-batch. We perform hypothesis testing where the null hypothesis states that the model testing accuracy with color normalization is the same as using just the original H&E images and the alternative hypothesis as the model testing performance with color normalization is better than with the original H &E images. p-values are indicated in the parenthesis. H_0 : The model testing accuracy with color normalization is the same as using the original H&E data H_1 : The model testing accuracy with color normalization is better than using the original H&E data.

in the first experiment in Fig. 3b where the solid line indicates the mean histogram distribution, and the shaded area indicates ±1 standard deviation in slide-to-slide variations. We observe that the histogram distribution of the color-normalized images for both normalization schemes show a different shape than the original color distribution rather than reducing the slide-to-slide variation, indicating that none of the methods work well to generate a homogeneous color distribution for the whole slide images.

Discussion

We have demonstrated that when histologic slides are prepared consistently, within a short timeframe within the same lab, using the same batches of staining reagents and under similar conditions (e.g., temperature, humidity), DNN can be trained to predict subsequent metastasis based on an assessment of the original diagnostic histology. We have further shown that this process is generalizable, in that slides prepared at two different times can be used to train the DNN to perform this task. However, we have also shown that when slides processed at one time are used for training, the subsequent predictive algorithm is unable to predict metastasis on slides processed at a different time. Thus, while there is clearly information present in the diagnostic histology that allows for prediction, it cannot be generalized to slides processed at a different time, even in the same lab. In our study, the slides processed at two different times in the same lab have tinctorial differences that a human pathologist can appreciate, which we suspect is the root cause of the lack of generalizability between batches. Despite the use of four different color normalization schemes, we have found that tinctorial differences between batches remain that can be distinguished by a human pathologist. However, we have now also demonstrated that the use of two different color normalization schemes is unable to make the DNN algorithms more generalizable and have further noted that with both normalization schemes we used, traditional structure-preserving method and CycleGAN-based generative method, the normalized images continue to have tinctorial and morphologic differences from the reference batch. Moreover, the conclusion is the same for both the ResNet model as well as the Prov-GigaPath foundational model. In addition, none of the color normalization methods work well to reduce the variation across different slides with different stain strengths.

Perhaps the important finding from this study is that despite the fact that the DNN algorithms were not useful when applied to different batches of slides, two different types of DNN were able to derive highly predictive algorithms within each batch of slides, indicating that the information necessary to derive the prediction is present in the slides, but that staining differences do not allow generalization of the algorithms. This suggests that in order to make DNN algorithms more generalizable across histologic preparations not only across time but also location, we need to move away from vital staining, and to other ways to analyze histologic slides and images.

The implication for digital pathology and DNN is that for more common tasks where large amounts of diverse data can be easily obtained, the big data approach remains the most viable option to mitigate the effects of unwanted variations. Our study demonstrates that color normalization schemes are in effective in allowing a DNN algorithm trained on one set of slides to be used across other batches of slides processed at different times or in different labs. This study also indicates that there is another way forward - improve the imaging and sample processing protocols to yield more consistently stained histopathology slides. For instance, it is worth considering circumventing the use of H&E staining altogether and implementing microscopy techniques to collect label-free images for downstream DNN analysis. While a human pathologist may spend years training and specializing in reading H&E stained slides well, DNN can be readily trained on different contrasts as long as consistent data are available. The options for label-free imaging are abundant and growing in numbers. For example, Fourier Ptychographic Microscopy (FPM)^{23,24} and more recent technology Angular Ptychographic Imaging with Closed-Form solution (APIC)^{25,26} is able to provide aberration-free, quantitative phase imaging. Other label-free methods can utilize autofluorescence signals, or ultraviolet light to elicit more molecular

specificity^{27,28}. These approaches may yield DNN algorithms that can be used on preparations across time and location and are an area we are now actively pursuing.

Data availability

Part of the processed data is available at CaltechData https://doi.org/10.22002/dw66e-mbs82.

Received: 11 September 2024; Accepted: 12 December 2024

Published online: 18 January 2025

References

- 1. Bychkov, D. et al. Deep learning based tissue analysis predicts outcome in colorectal cancer. Sci. Rep. 8, 3395. https://doi.org/10.10 38/s41598-018-21758-3 (2018).
- 2. Hekler, A. et al. Deep learning outperformed 11 pathologists in the classification of histopathological melanoma images. *Eur. J. Cancer* 118, 91–96. https://doi.org/10.1016/j.ejca.2019.06.012 (2019).
- 3. Tschandl, P. et al. Comparison of the accuracy of human readers versus machine-learning algorithms for pigmented skin lesion classification: an open, web-based, international, diagnostic study. *Lancet Oncol.* 20, 938–947. https://doi.org/10.1016/S1470-2045 (19)30333-X (2019).
- 4. Ehteshami Bejnordi, B. et al. Stain specific standardization of whole-slide histopathological images. *IEEE Trans. Med. Imaging* 35, 404–415. https://doi.org/10.1109/TMI.2015.2476509 (2016).
- 5. Zhou, H. et al. AI-guided histopathology predicts brain metastasis in lung cancer patients. J. Pathol. 263, 89–98. https://doi.org/10.1002/path.6263 (2024).
- He, K., Zhang, X., Ren, S. & Sun, J. Deep Residual Learning for Image Recognition. CVPR https://doi.org/10.48550/ARXIV.1512.0 3385 (2015). Publisher: [object Object] Version Number: 1.
- 7. Lu, M. Y. et al. A multimodal generative AI copilot for human pathology. *Nature* **634**, 466–473. https://doi.org/10.1038/s41586-02 4-07618-3 (2024).
- 8. Xu, H. et al. A whole-slide foundation model for digital pathology from real-world data. *Nature* **630**, 181–188. https://doi.org/10.1038/s41586-024-07441-w (2024).
- 9. Wang, X. et al. A pathology foundation model for cancer diagnosis and prognosis prediction. *Nature* https://doi.org/10.1038/s415 86-024-07894-z (2024).
- Huang, Z. et al. A pathologist-AI collaboration framework for enhancing diagnostic accuracies and efficiencies. Nat. Biomed. Eng. https://doi.org/10.1038/s41551-024-01223-5 (2024).
- Niazi, M. K. K., Parwani, A. V. & Gurcan, M. N. Digital pathology and artificial intelligence. *Lancet Oncol.* 20, e253–e261. https://doi.org/10.1016/S1470-2045(19)30154-8 (2019).
- Bilgin, C., Rittscher, J., Filkins, R. & Can, A. Digitally adjusting chromogenic dye proportions in brightfield microscopy images. J. Microsc. 245, 319–330. https://doi.org/10.1111/j.1365-2818.2011.03579.x (2012).
- 13. Ström, P. et al. Artificial intelligence for diagnosis and grading of prostate cancer in biopsies: a population-based, diagnostic study. *Lancet Oncol.* 21, 222–232. https://doi.org/10.1016/S1470-2045(19)30738-7 (2020).
- 14. Pantanowitz, L. et al. An artificial intelligence algorithm for prostate cancer diagnosis in whole slide images of core needle biopsies: a blinded clinical validation and deployment study. *Lancet Digit. Health* 2, e407–e416. https://doi.org/10.1016/S2589-7500(20)301 59-X (2020).
- 15. Vahadane, A. et al. Structure-preserving color normalization and sparse stain separation for histological images. *IEEE Trans. Med. Imaging* 35, 1962–1971. https://doi.org/10.1109/TMI.2016.2529665 (2016).
- Macenko, M. et al. A method for normalizing histology slides for quantitative analysis. In booktitle2009 IEEE International Symposium on Biomedical Imaging: From Nano to Macro, 1107–1110, https://doi.org/10.1109/ISBI.2009.5193250 (IEEE, 2009).
- 17. Reinhard, E., Adhikhmin, M., Gooch, B. & Shirley, P. Color transfer between images. IEEE Comput. Graph. Appl. 21, 34–41. https://doi.org/10.1109/38.946629 (2001).
- Khan, A. M., Rajpoot, N., Treanor, D. & Magee, D. A nonlinear mapping approach to stain normalization in digital histopathology images using image-specific color deconvolution. *IEEE Trans. Biomed. Eng.* 61, 1729–1738. https://doi.org/10.1109/TBME.2014.2 303294 (2014).
- 19. Shen, Y. et al. A federated learning system for histopathology image analysis with an orchestral stain-normalization GAN. *IEEE Trans. Med. Imaging* 42, 1969–1981. https://doi.org/10.1109/TMI.2022.3221724 (2023).
- Kang, H. et al. StainNet: a fast and robust stain normalization network. Front. Med. https://doi.org/10.3389/fmed.2021.746307 (2021).
- 21. Rivenson, Y. et al. PhaseStain: the digital staining of label-free quantitative phase microscopy images using deep learning. *Light Sci. Appl.* 8, 23. https://doi.org/10.1038/s41377-019-0129-y (2019).
- Otsu, N. A threshold selection method from gray-level histograms. IEEE Trans. Syst. Man Cybern. 9, 62–66. https://doi.org/10.11 09/TSMC.1979.4310076 (1979).
- Zheng, G., Horstmeyer, R. & Yang, C. Wide-field, high-resolution Fourier ptychographic microscopy. Nat. Photonics 7, 739–745. https://doi.org/10.1038/nphoton.2013.187 (2013).
- 24. Horstmeyer, R., Ou, X., Zheng, G., Willems, P. & Yang, C. Digital pathology with Fourier ptychography. *Comput. Med. Imaging Graph.* 42, 38–43. https://doi.org/10.1016/j.compmedimag.2014.11.005 (2015).
- Cao, R., Shen, C. & Yang, C. High-resolution, large field-of-view label-free imaging via aberration-corrected, closed-form complex field reconstruction. Nat. Commun. 15, 4713. https://doi.org/10.1038/s41467-024-49126-y (2024).
- 26. Zhao, S., Zhou, H., Lin, S., Cao, R. & Yang, C. Efficient, gigapixel-scale, aberration-free whole slide scanner using angular ptychographic imaging with closed-form solution. *Biomed. Opt. Express* https://doi.org/10.1364/BOE.538148 (2024).
- You, S. et al. Intravital imaging by simultaneous label-free autofluorescence-multiharmonic microscopy. Nat. Commun. 9, 2125. https://doi.org/10.1038/s41467-018-04470-8 (2018).
- 28. Tu, H. et al. Stain-free histopathology by programmable supercontinuum pulses. *Nat. Photonics* 10, 534–540 https://doi.org/10.10 38/nphoton.2016.94 (2016)

Acknowledgements

This study was supported by U01CA233363 from the National Cancer Institute (RJC) and by the Washington University in St. Louis School of Medicine Personalized Medicine Initiative (RJC). S.L., H.Z. and C.Y. are also supported by Heritage Research Institute for the Advancement of Medicine and Science at Caltech (Grant No. HMRI-15-09-01) and the Caltech Rothenberg Innovation Initiative A4188-Yang-3-A1. M.W. and R.G. are also supported 5R01CA182746 from the National Cancer Institute.

Author contributions

C.Y. and S.L. designed the experiments. S.L. conducted all experiments and analysis. S.L., H.Z., and C.Y. designed the figures. R.J.C. conducted pathology analysis. M.W. and R.G. prepared experimental data. All authors contributed to the writing and preparation of the manuscript as well as figures.

Declarations

Competing interests

The authors declare no competing interests.

Additional information

Supplementary Information The online version contains supplementary material available at https://doi.org/10.1038/s41598-024-83267-w.

Correspondence and requests for materials should be addressed to C.Y.

Reprints and permissions information is available at www.nature.com/reprints.

Publisher's note Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.

Open Access This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons licence, and indicate if changes were made. The images or other third party material in this article are included in the article's Creative Commons licence, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons licence and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this licence, visit https://creativecommons.org/licenses/by/4.0/.

© The Author(s) 2025