

Limited-angle Multi-energy CT using Joint Clustering Prior and Sparsity Regularization

Huayu Zhang, Yuxiang Xing

Tsinghua University, University of Wisconsin-Madison



Outline

- Introduction
- Methodology
- Experiments
- Summary

Introduction

Motivation

- **Spectral (Multi-energy CT)**

- ▷ differentiates materials
- ▷ wide applications: extracting veins and kidney stones, detecting chemical elements (iodine, barium)

- **Problems**

- ▷ The data required for reconstruction is multiplied
- ▷ longer scan time, more cost, more dose

- **Goal**

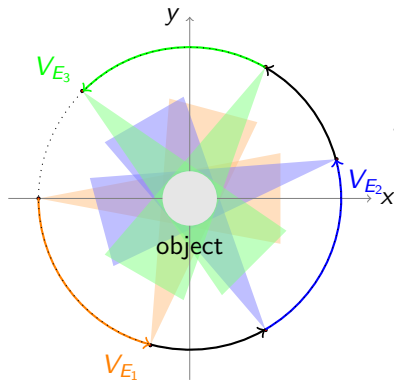
- ▷ Design an easy-to-implement scanning strategy
- ▷ Lower dose, cost and acquisition/reconstruction time (less angular views)
- ▷ mitigate limited-angle artifacts

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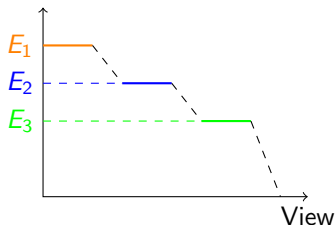
Methodology

Proposed data acquisition strategy: Multi-arc scan



(a) Scanning trajectory

Tube Voltage (KeV)



(b) Voltage switching

Requirement: The angular coverage of all X-ray beams is no less than 180° plus fan beam angle.

Methodology

Main Difficulty: Severe limited-angle Problem

- Limited-angle problem:
 - ▷ violates data sufficient condition: 180° plus fan beam angle coverage
 - ▷ severe artifacts
 - ▷ hard to eliminate the artifacts using compressed sensing
- Solutions:
 - ▷ Independent reconstruction will unavoidably encounter limited-angle artifacts.
 - ▷ Leverage the structural coherence of images at all energies
 - ▷ jointly reconstruct images at all energy channels



Methodology

Pre-reconstruction

Combine the projection data from all energies to pre-reconstruct a prior image.

$$\mu_p = \arg \min_{\mu} \|\mathbf{H}\mu - \mathbf{p}\|_2^2$$

where

$$\mathbf{H} = \begin{pmatrix} \mathbf{H}_1 \\ \mathbf{H}_2 \\ \vdots \\ \mathbf{H}_{N_E} \end{pmatrix} \quad \mathbf{p} = \begin{pmatrix} \mathbf{p}_1 / \|\mathbf{p}_1\|_1 \\ \mathbf{p}_2 / \|\mathbf{p}_2\|_1 \\ \vdots \\ \mathbf{p}_{N_E} / \|\mathbf{p}_{N_E}\|_1 \end{pmatrix}$$

Each independent \mathbf{H}_i is ill posed,
but the combined \mathbf{H} not.



Figure : Prior image

L. Shen and Y. Xing, Medical physics, 42(1): 282, 2015

Methodology

Clustering

- Assumption:
 1. The number of tissues within the object is limited;
 2. Each tissue is spatially continuous;
 3. The pixels within one tissues share an identical value.
- Clustering:
 1. k —means clustering on the prior image;
 2. choosing features $(x, y, \mu(x, y))$.
 (x, y) : coordinates, $\mu(x, y)$: pixel values;
 3. The image is divided into k patches;
 4. These k patches keep some structural details.

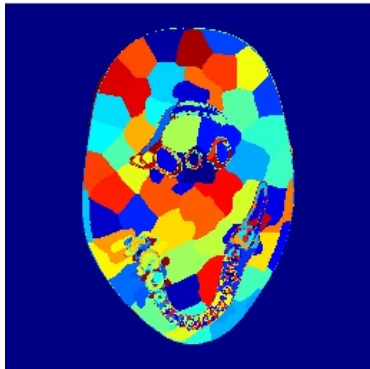


Figure : Clustering

Methodology

Structural information and constraint

Construct a constraint from the clustering

- k patches: $\Omega_c = \{(x, y) \mid \text{labeled with } c\}, c = 1, 2, \dots, k.$
- construct a dictionary

$$\mu = \Phi \mathbf{a} = \sum_{c=1}^k a_c \varphi_c \quad (1)$$

where

$\Phi = (\varphi_1, \varphi_2, \dots, \varphi_k) \in \mathcal{R}^{N \times k}$ dictionary matrix

φ_i basis vector (element)

$$\varphi_{ij} = \mathbf{1}_{i \in \Omega_j} = \begin{cases} 1 & i \in \Omega_j \\ 0 & i \notin \Omega_j \end{cases}$$

Methodology

Reconstruction Model

Joint Clustering Prior and Sparsity Regularization (CPSR) model

$$\arg \min_{\mu} \frac{1}{2} \|\mathbf{H}\mu - \mathbf{p}\|_2^2 + \lambda \|\mathbf{W}\mu\|_1 \quad s.t. \quad \mu = \Phi \mathbf{a} \quad (2)$$

Incorporates the structural constraint into general compressed sensing frame.

- $\|\mathbf{H}\mu - \mathbf{p}\|_2^2$ linear projection model
- $\|\mathbf{W}\mu\|_1$ sparse constraint. \mathbf{W} denotes wavelet transform.
- $\mu = \Phi \mathbf{a}$ structural constraint

Augmented Lagrangian Function:

$$L(\mu, \mathbf{a}, \mathbf{z}, \mathbf{y}_1, \mathbf{y}_2) = \underbrace{\frac{1}{2} \|\mathbf{H}\mu - \mathbf{p}\|_2^2}_{\text{fidelity}} + \underbrace{\frac{\rho_1}{2} \|\mu - \Phi \mathbf{a} + \mathbf{y}_1\|_2^2}_{\text{structural constraint}} + \underbrace{\lambda \|\mathbf{z}\|_1 + \frac{\rho_2}{2} \|\mathbf{z} - \mathbf{W}\mu + \mathbf{y}_2\|_2^2}_{\text{sparse constraint}}$$

Solution: Alternating direction method of multipliers (ADMM)

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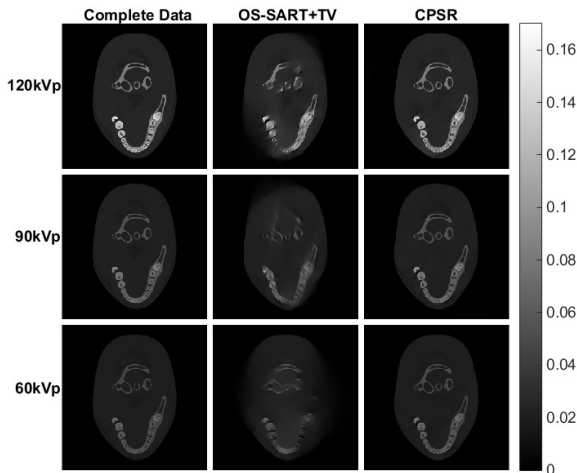
Numerical Experiments

Settings

- Scan
 - modality: Fan beam
 - X-ray energies: 120kVp, 90kVp, 60kVp
 - Projection data for each energy: 75 (views) \times 320 (detectors)
- Reconstruction
 - Image size: 256×256
 - Clustering number: $k = 100$
 - Reconstruction algorithm: OS-SART
 - Sparse constraint: Total variation in wavelet space

Numerical experiments

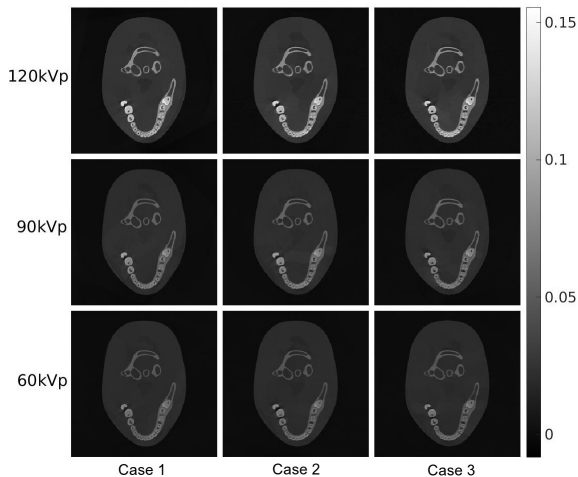
Reconstruction results



- Complete Data: Independent reconstruction from 180° plus fan beam angle projection data
- OS-SART: Independent reconstruction using OS-SART + TV constraint from 75° angular coverage projection data.
- View 3: CPSR method from 75° angular coverage projection data.

Numerical experiments

Impact of view selection on reconstruction



Compare results from different view configurations:

Case 1: $V_{120kVp} = [0^\circ, 75^\circ]$

$V_{90kVp} = [120^\circ, 195^\circ]$

$V_{60kVp} = [240^\circ, 315^\circ]$

Case 2: $V_{120kVp} = [30^\circ, 105^\circ]$

$V_{90kVp} = [150^\circ, 225^\circ]$

$V_{60kVp} = [270^\circ, 345^\circ]$

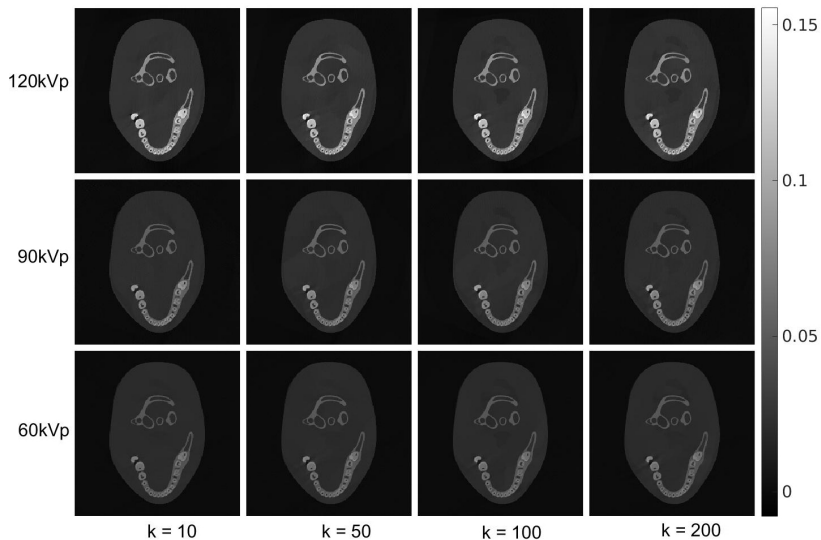
Case 3: $V_{120kVp} = [60^\circ, 135^\circ]$

$V_{90kVp} = [180^\circ, 255^\circ]$

$V_{60kVp} = [300^\circ, 375^\circ]$

Numerical experiments

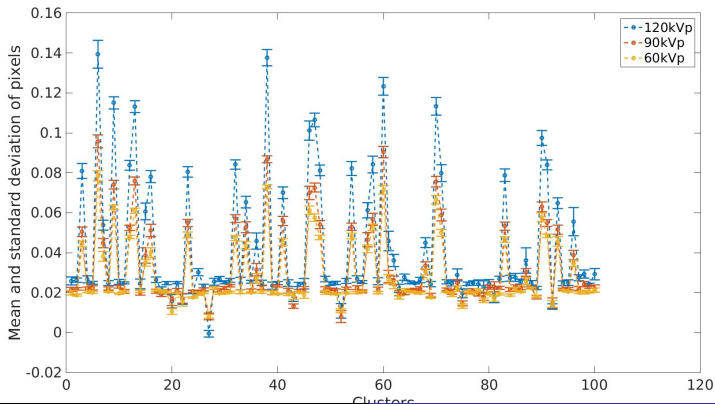
Impact of the clustering number on reconstruction



Numerical experiments

Impact of the clustering constraint on reconstruction

- Assumption of identical pixel value within one cluster may be too strong.
- Our method is flexible and tolerates some variation within each cluster by assigning a weight on the prior structural constraint term.



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Related works

- Multi-energy CT scan and reconstruction [Shen and Xing 2015]
- Compressed sensing
 1. sparsity[Sidky, Kao, and Pan 2006; Sidky and Pan 2008]
 2. low rank[Gao et al. 2011]
- Limited-angle CT[Jin et al. 2012]
- Sparse dictionary learning[Cao and Xing 2013]

Summary

Contributions

- Largely reduce the projection data required.
From 180° plus fan beam angle to at least 75° .
- Design and implement a reconstruction approach using joint clustering prior and sparsity in wavelet space.
- Solve the limited angle problem by leveraging the coherence among all data at different energies.
- Our method enable flexible angular configuration and broaden spectral CT system design.

Main References



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