

# Self-supervised deep learning to improve quantification of blood-brain barrier permeability from MRI data

Friday 22nd March 2024
Photo adapted from D koi on Unsplash[1]



- Blood-brain barrier (BBB)
  - Selectively permeable barrier <sup>1</sup> [2]
  - Maintains homeostasis in brain and CNS [3]



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  - Maintains homeostasis in brain and CNS [3]
- Dysfunction: Pathogens and toxins leak from blood to brain [2]
  - Stroke
  - Multiple sclerosis
  - Tumours
  - Can occur early in disease
- Biomarker

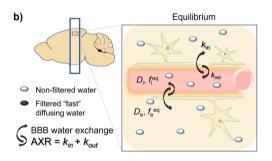


Figure: Adapted from [4]

- FEXI (Filtered exchange imaging) dMRI (Diffusion MRI) technique
  - Originally used to track water exchange across cell membranes
  - Can be used to track water exchange across the BBB



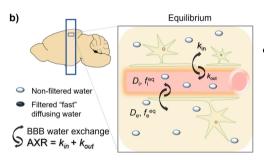


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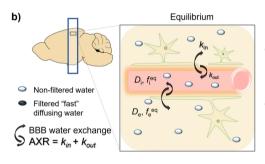


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- Existing method: Non-linear least squares fit (NLLS)
  - Suffers from bias and noise.
- New method: Neural networks (NN) show promise in other dMRI methods
  - ssVERDICT A model of Prostate tumours
  - Reduced bias compared to existing NLLS method [5]
  - Side effect: Slow to train but quicker once implemented
    - 10s of minutes for NLLS
    - Fractions of a second



# Aims and objectives



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## **Objectives:**

- Simulate the MRI signal in Python using NumPy.
- Implement a baseline Non-linear least squares (NLLS) estimation to FEXI.
  - Previously made in MATLAB
- Create a self supervised deep learning model in PyTorch to estimate FEXI parameters.

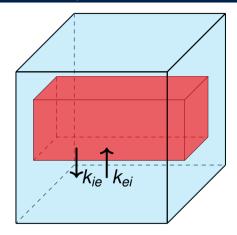


Figure: A FEXI voxel, extra-vascular compartment in blue and intra-vascular compartment in red.

- FEXI assumes a 2 compartment model in every voxel (Volume Element)
- FEXI tracks the water in each compartment. (Blood-water in the intra-vascular compartment)
- The main parameter of interest is the apparent exchange rate
   AXR = k<sub>ie</sub> + k<sub>ei</sub> between the compartments.

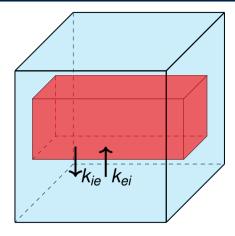


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- Other estimated parameters:
  - Apparent diffusion coefficient ADC
  - Filter efficiency  $\sigma$

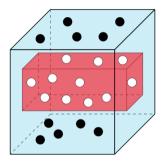


Figure: Exchange of water between intraand extra-vascular compartments during mixing time

- The FEXI MRI sequence contains a mixing time
- There is water exchange between the 2 compartments during this time
- This is what AXR measures

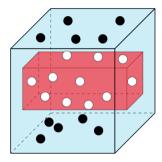


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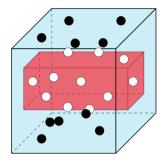


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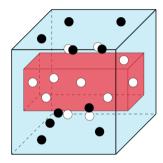


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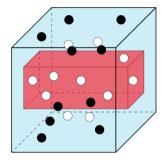


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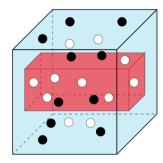


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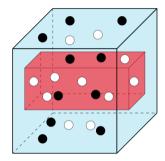


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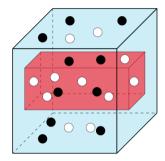


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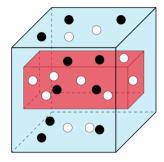


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#### Simulations

- Simulate 10.000 voxels
  - Random distribution of underlying model parameters ADC, σ and AXR
- Calculate the signal produced by each voxel
- Add rician noise<sup>2</sup> (SNR=50) to the signals
  - The ground truth

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#### NLLS and Neural network

- Input noisy MRI signal
- Estimate underlying model parameters ADC, σ and AXR
- Calculate the mean squared error between the estimated signal and the ground truth (with noise added).
- Iterate

<sup>2&</sup>quot;Rician is the thermal noise found in MRI due to the thermal agitation of electrons."[6]

# Non-linear Least squares theory

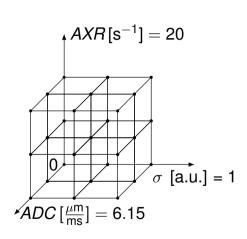


- The scipy.optimize.minimize() function [7] within Python was used to make the estimations.
  - Minimising the sum of squares error between the estimated signal and the noisy ground truth signal.

# Non-linear Least squares theory

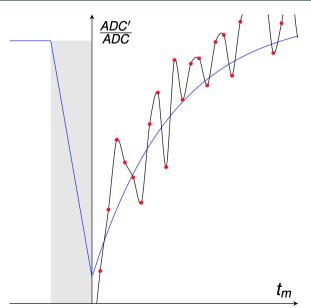


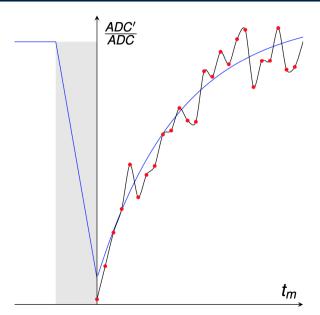
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  - Minimising the sum of squares error between the estimated signal and the noisy ground truth signal.
- The function requires an initial value
  - 3 equally spaced initial values for each parameter (ADC,  $\sigma$  and AXR) were used, producing  $3^3 = 27$  initial starting points.
  - The best estimation from these 27 starting points was used
- Each parameter is bounded within the simulation range.

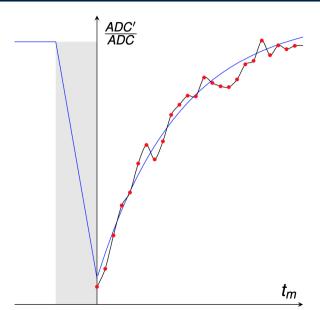


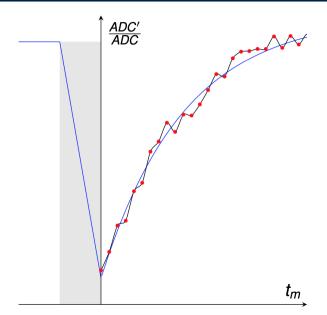
<sup>&</sup>lt;sup>3</sup>Using the Limited-memory Broyden-Fletcher-Goldfarb-Shanno with Bounds algorithm 🕡 📳 🗦 🛫 🛷 🤊











# Neural network theory



- Input: 8 image volumes
- Passed through the weights of each layer
- 3 outputs: ADC, σ and AXR. (Known as the forward model)
- Each parameter is bounded by the same bounds as the simulation.
- Mean squared error calculated between the ground truth noisy signals and estimated signals

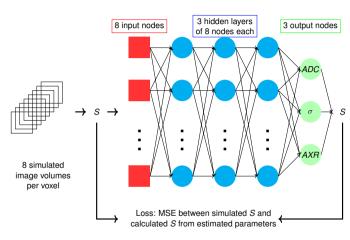


Figure: Neural network

# Neural network theory



- The gradients of the weights are calculated.
- If error improves, then the weights in the model are updated, with gradients giving the most efficient change (Known as backpropagation)
- This process (one epoch) is repeated, and stops after 100 epochs in a row where there is no improvement to the loss.

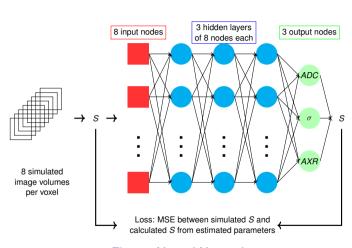
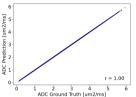
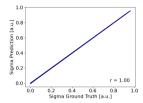


Figure: Neural Network





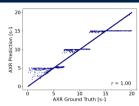
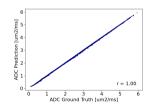
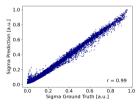


Figure: NLLS estimations





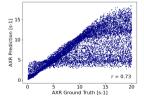


Figure: NN estimations

## Results continued

MSE			
Method	ADC	$\sigma$	AXR
NLLS	$1.75 \times 10^{-7}$	$1.03 \times 10^{-8}$	0.331
NN	2.53	0.104	56.3
Bias			
Method	ADC	$\sigma$	AXR
NLLS	$-3.02  imes 10^{-5}$	$-6.70 \times 10^{-6}$	$3.33 \times 10^{-3}$
NN	$3.57 \times 10^{-3}$	- 3.09 ×10 <sup>-3</sup>	-2.52
Variance			
Method	ADC	$\sigma$	AXR
NLLS	1.27	$5.27 \times 10^{2}$	32.2
NN	1.26	$5.07\times10^2$	23.3

Table: Comparing NLLS to NN (Best results are bolded)

$$\mathsf{MSE} = \frac{1}{N} \sum_{i=0}^{N} (O_i - E_i)^2$$

$$\mathsf{Bias} = \frac{1}{N} \sum_{i=0}^{N} (O_i - E_i)$$

$$Varience = \frac{1}{N} \sum_{i=0}^{N} (O_i - \overline{O})$$

Where *O* is ground truth parameter value, *E* is estimated value, and *N* is number of samples.

- NLLS fit outperforms NN in MSE and Bias for all parameters
- NN outperforms NLLS in variance for all parameters
- AXR is hardest parameter to estimate in both methods
  - ADC and  $\sigma$  have a linear relationship to the signal, but AXR has a exponential relationship.

#### Future work

- Use other variations hyper-parameters of NN.
- Calculate the loss on a per parameter basis.
- Physics informed network Calculate AXR from other parameters rather than estimating in NN
- · Apply to in-vivo data

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- [3] Gerard J. Tortora and Bryan H. Derrickson. *Introduction to the Human Body*. 11th ed. Wiley, 2017-12-15. ISBN: 978-1-119-39273-6. URL: https://bibliu.com/app/#/view/books/9781119392736/epub/0PS/c10. html#page\_393 (visited on 2024-03-07).

- [4] Yolanda Ohene et al. "Filter exchange imaging with crusher gradient modelling detects increased blood—brain barrier water permeability in response to mild lung infection". In: Fluids and Barriers of the CNS 20.1 (2023-04-03), p. 25. ISSN: 2045-8118. DOI: 10.1186/s12987-023-00422-7. URL: https://doi.org/10.1186/s12987-023-00422-7 (visited on 2024-03-21).
- [5] Snigdha Sen et al. ssVERDICT: Self-Supervised VERDICT-MRI for Enhanced Prostate Tumour Characterisation. 2023-09-27. DOI: 10.48550/arXiv.2309.06268. arXiv: 2309.06268 [cs,eess]. URL: http://arxiv.org/abs/2309.06268 (visited on 2024-03-21).

- [6] Divya Pankaj, Govind D., and Narayanankutty K.a. "A novel method for removing Rician noise from MRI based on variational mode decomposition". In: Biomedical Signal Processing and Control 69 (2021-08-01), p. 102737. ISSN: 1746-8094. DOI: 10.1016/j.bspc.2021.102737. URL: https://www.sciencedirect.com/science/article/pii/S1746809421003347 (visited on 2024-03-22).
- [7] scipy.optimize.minimize SciPy v1.12.0 Manual. URL: https://docs.scipy.org/doc/scipy/reference/generated/scipy.optimize.minimize.html (visited on 2024-03-14).

# Thank you for listening



Thank you for listening! Any questions?



$$S(b_f, t_m, b) = S_0(b_f, t_m)e^{-b \cdot ADC'(t_m)}$$
(1)

where:

$$ADC'(t_m) = ADC(1 - \sigma e^{-t_m \cdot AXR})$$