Developing an Affective Point-of-Care Technology

Pedro H. F Bacchini[3], Erlan C. Lopes[3], Marco Aurélio G. de A. Barbosa[2], José O. Ferreira[3], Olegário C. da Silva Neto[3], Adson F. Da Rocha[1] and Talles Marcelo G de A. Barbosa[3].

[1]*UnB-Gama Faculty, University of Brasilia, Gama, Brazil.*
[2]*Santa Casa de Misericórdia de Goiânia Hospital, Goiânia, Brazil*
[3]*Department of Computing, Pontifical Catholic University of Goiás, PUC-Goiás, Goiânia, Brazil.*

Abstract— **Mobile intelligent clinical monitoring systems provide mobility and out of hospital monitoring. It can be used in the follow-up of high-risk patients in out of hospital situations and to monitor "healthy" persons to prevent medical events. The inherent characteristics of local diagnosis and actuation permit an improvement and advance in the diagnosis and emergency decision support. Additionally, Affective Systems have been used in different applications, such as stress monitoring in aircraft seats and managing sensitivity in autism spectrum disorder. Although many scientific progresses have been made there are many computational challenges in order to embedded affectivity into traditional user interfaces. For example, context-sensitive algorithms, low-complexity pattern recognition models and hardware customizations are requirements to support the simplification of user's experience becoming more intuitive, transparent and less obstructive. In this paper a multiparametric affective monitor is presented. The Emopad acquisition system has been developed to analyze user's biofeedback particularly when they are playing games. It is able to capture Galvanic Skin Response (GSR), Temperature, Force, Heart Rate (HR) and its variability (HRV) while complementary algorithms are executed to recognize events related to user's emotional states. Also, in this paper a sliding window-based algorithm is presented and evaluated to detect specific events related to emotional responses. The success of multiparametric affective monitors can lead to a paradigm shift, establishing new scenarios for the Point-of-Care technologies applications.**

Keywords—affective gamepad, affective systems, point-of-care technology, multiparametric affective monitor.

I. INTRODUCTION

The development of computer systems including new user's requirements, such as emotional states has been largely discussed for the last two decades [1] [2] [3] [4], since Rosalind Picard coined the term Affective Computing at MIT Media Labs in 90's. The ability of machines to recognize emotions is an important step to improve the Human-Computer Interactions (HCI). Thus, decision-making could become more intuitive and simplified [36]. Many effort has been applied to recognize emotions through facial expressions, voice and physiological signals in different applications, e.g., embedded in aircraft seats [5], smartphones [6] [9], wearable computers [7][8], cars [11], [12], [16], robots [17] and even embedded in a bathroom's mirror [10]. Recently, more interest in clinical, educational and entertainment applications have been observed [13],[14],[15].

The game industry has special interest in affective games because all video games have the ability to affect a player and the result can be seen in changes of his or her focus or concentration, arousal and stress levels. Virtual stimuli can produce angry, anguish, sadness, panic, fear, happiness, joy, well-being and etc. Most of these emotional states can be expressed directly or indirectly on physiological signals, e.g., Heart Rate (HR) and its variability (HRV), Galvanic Skin Response (GSR), Respiration, Cutaneous Temperature, Movement, Force, ECG, EEG and etc. In the last decade, there has been increased commercial interest in using physiological input in digital games, not only for biofeedback training, but also to enhance immersion and engagement for players [21].

Schaaf and Adam [18] have used an HRV sensor as indicator of emotional arousal for mobile games. For some features, it is possible to use ultra-short term window sizes (shorter than 5 minutes) for short term HRV analysis. Parnandi *et al.* [19] have experimented electrodermal activity (EDA) as a physiological correlate of arousal on car-racing games. Kennedy *et al.* [20] have developed a low-cost rehabilitation instrument suite centered around the Nintendo Wii Balance Board that has the potential to enhance rehabilitation for patients with balance disorders. Balance retraining is a critical part of rehabilitation for many individuals following neuro-trauma such as stroke. Nacke *et al.* [21] propose taxonomy based on direct and indirect physiological sensor input to expand traditional game control. *Direct physiological control* establishes that any user can manipulate and control directly (e.g., muscle flexion, eye gaze) and should be mapped intuitively to reflect an action in the virtual world. *Indirect physiological inputs* are excellent at helping users train themselves to relax precisely because they are indirectly controlled, such as GSR and HRV signals. In May 2014 was launched a game entitled "Throw Trucks". According to [29] it allows users that use NeuroSky's MindWave to give them telekinetic super-powers controlled with their thoughts. NeuroSky's MindWave is one-channel acquisition headset able to capture and process electroencephalogram (EEG). In Throw Trucks, users can crush their enemies by throwing trucks with their minds. Recently, a posted headline at IEEE Spectrum website announces the development of a modified Xbox controller for sensing players' excitement levels at Stanford University [22]. However, they have not submitted any paper for peer review yet.

In this paper an intelligent biofeedback device is presented. Also, a complete description about its components. It has been developed to operate as a user's affective interface, able to deal with implicit and explicit biofeedback processing. Consequently, it has been called Emotional Gamepad or Emopad. Furthermore, energy-efficient and platform-independent requirements were required. Hence, a generic game controller has been redesigned to embed sensors, processor and algorithms able to capture, filter, recognize and classify events, especially those related to users emotional states when they are playing video games. Hence, the proposed game controller device should transform a generic gamepad into a point-of-care technology bringing a personal health monitor system at or near the site of patient care.

II. Materials and Methods

A. Development Process

In order to develop Emopad a bottom-up and successive refinements development methodology was applied. This sort of process is recommended when most of requirements cannot be completely elicited. These requirements are partially observed. Thus, basic and low-level components should be built. As soon as possible they should be customized and fused to arrange high complex and more precise components. Fig. 1 synthetizes applied methodology.

The *Acquisition Systems* were the first component implemented. Their developments were essentials to evaluate, select and handle with physiological signal processing requirements, such as patterns of interests, dimensions, costs, computational complexity and ergonomics aspects. In a preliminary version of Emopad, Galvanic Skin Response (GSR), Cutaneous Temperature, Force, Heart Rate (HR) and its variability (HRV) have been captured and analyzed. In addition, outside of the proposed gamepad, HD Webcam, voice (from each player participant), ambient temperature, ambient humidity and game sequence (in video format) should be also recorded. Fig. 5 shows external variables. Moreover, many DSP technologies were tested and evaluated to support non-functional requirements, such as low cost, platform-independence, ergonomics aspects (short dimensions) and energy efficiency, very important for battery-operated devices.

After the first activity (Fig. 1) two parallels activities were initiated. The development of *Analysis, Visualization and Dataset Tools* activity was responsible for organizing acquired data preparing it for analyzing and visualizing. Both functionalities are indispensable to design algorithms qualified to perform filter noise, recognize interests patterns and classify events. In this activity, all parameters related to embedded algorithms were defined, e. g., window size, resampling rate, outlier's references and decision rules. The *Redesign Gamepad* activity was executed to establish ergonomic parameters to accommodate physical interfaces and their related circuitry. Hence, 3-D modeling was executed based on traditional gamepad models. Before to produce 3-D software models and their artifacts, some 3-D models sculpted with epoxy putty were created. They were built to be touched and assessed by selected user's set at preliminary usability testing.

Consequently, the new gamepad surface, colors, curves, sensors and actuators could be tangibly evaluated. In this activity many hypothesis were tested and final version was inspired in a bike handlebar from italian bianchi, circa 1940. At the end of *Redesign Gamepad* activity a 3-D plastic model was printed at Shapeways spin-off in New York City [28].

After to design and evaluate certain algorithms and heuristics, the best performance solutions have been selected and embedded in a microcontroller platform. The best performance choice was based on a compromise between algorithms hit rate, time/space complexity and energy efficiency. Thus, at the end of *Algorithm Implementation* activity at least one feasible hardware-software solution was achieved.
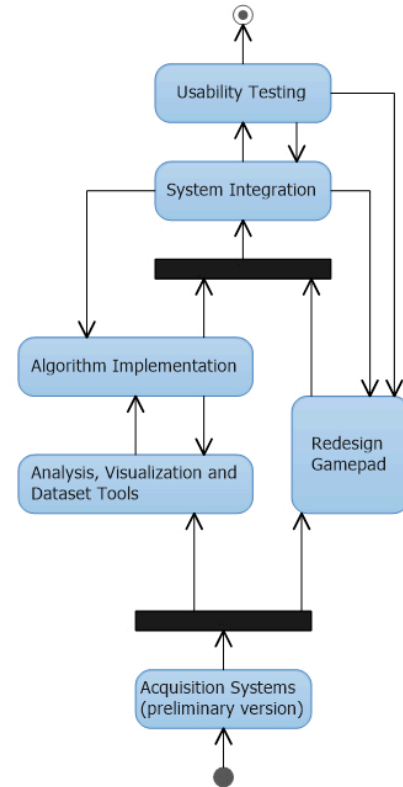

Fig.1. Emopad Development Process [36].

The last two activities in Fig. 1 are related to production and evaluation of an operational prototype version. They should embrace hardware-software artifacts embedded in the Gamepad enclosure and usability testing to verify user's reactions. Most of performed activities required feedback for refactoring non-conforming modules, e.g, programs, electronic circuits, 3-D models, algorithms simulations and analysis. These hypotheses were considered in the proposed development process by each arrow directions in Fig. 1.

B. Acquisition Systems

The EmoPad acquisition's systems were first prepared to deal with four analog signals: GSR, Cutaneous Temperature, Force and PPG. Four different analog interfaces were built and

connected to Analog/Digital (A/D) converter embedded in MSP430 TI microcontroller. Fig. 2 shows the block diagram to clarify Emopad hardware organization and Fig. 5 shows the first prototype version built according to Fig. 2.
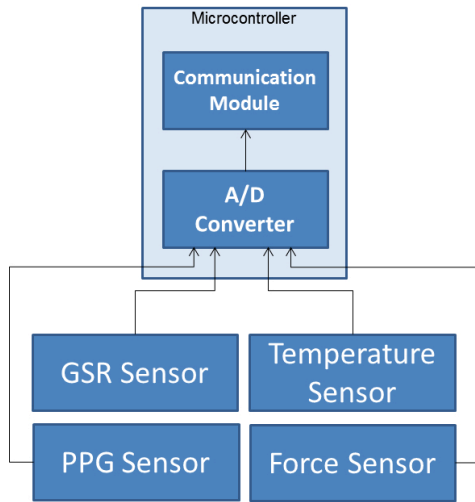

Fig. 2. Emopad Block Diagram.

According to [24][25] GSR reflects psychological stimuli and it has linear correlation with arousal, exposing some user's emotional states. Fig. 3 shows the GSR circuitry developed to embedded it into Emopad. It has been described in previous papers [4], [36], and it works as a voltage divisor, useful to compare a known resistance value with the skin resistance at each time. In the calibration phase, the "2.7MΩ" resistance should be fine-tuned according to the maximum skin resistance for each person at each moment. Buffers are implemented by two ampops and two analog filters, and they were applied to remove undesired artifacts (specially those related to high frequency noise), to avoid the lost of signal strength and to limit the bandwidth, preventing aliasing. In this paper the GSR circuitry has been designed to be embedded in a gamepad, enabling it to capture GSR data using only two fingers on left hand. Although a recent Picard's paper [30] suggests the need to capture GSR in many and different body parts, we argue that a Sensor Network based solution is not feasible to Emopad because that approach could become obstructive and CPU bound. Most entertainment applications related to affective interfaces are concerning in capture the event occurrences (at low level) and fuse them with the other events from different sensors. Next, data should be prepared for pattern recognizing and decision-making (at high level algorithms), commonly executed outside of the microprocessor embedded into affective interfaces. This situation counteracts platform independence because these functionalities should be implemented at driver level on game consoles.

Fig 4 shows the cutaneous temperature circuitry. It has been designed to avoid first-degree burns when the current through the thermistor increases. In order to reach this objective the REF200 from Texas Instruments was chose. It implements a high precision dual current source. This approach prevents the self-heating error from thermistor [26]. Other functional blocks

used in Fig. 4 are: one buffer, one active filter, one passive filter and one thermistor. This circuit was adjusted to operate at 5V and the total sink current is less than 4mA. Thus, the same microcontroller's power supply can be used. Temperature range is regulated from 10ºC to 40ºC. Also the B57861S0103F045 was used, and arrows on Fig. 5 point it. This thermistor is manufactured by Epcos [27] and has a short response time, 1% tolerance resistance. It is very small and therefore easy to fit in the gamepad. Its leads are insulated what prevent current to flow to the body. Different from the circuitry proposed in [26], this circuitry uses just one current source per channel. Thus, just one REF200 is necessary for every two channels, reducing costs and energy consumption when more than one channel for cutaneous temperature is required. In the first version of Emopad, two channels were used to capture data related to cutaneous temperature.
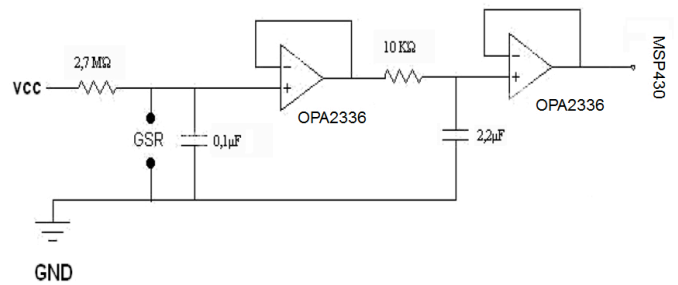

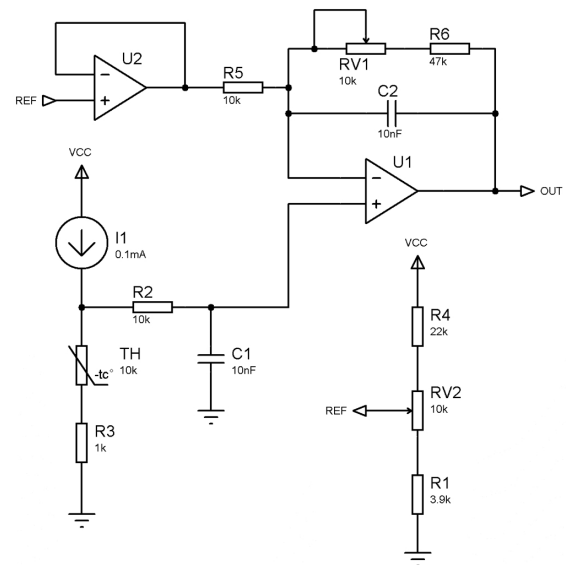Fig. 3. Galvanic Skin Response Sensor [4].

Fig. 4. Temperature Sensor

The force sensor proposed on Fig. 2, one Force Sensing Resistor (FSR) with a round, 0.5" diameter, sensing area from Interlink Electronics was selected. It varies its resistance depending on how much pressure is being applied to the sensing area. The greater the force, the lower the resistance. When no pressure is being applied to the FSR, its resistance will be larger than 1MΩ. This FSR can sense applied force anywhere in the range of 100g-10kg. In Emopad this sensor is

used for detecting weight shift and relative force and correlating them with sympathetic reactions, particularly those related with the flight-or-fight response, e.g., stress. The analog interface for the FSR implements a voltage divider. The value of fixed resistance should be chosen to give the output voltage the greatest "sweep" from 0-3.3V, assuming that the sensing range (resistance sweep) of the sensor is 0-100kΩ. The Emopad circuitry is able to execute dynamic adjusts on the resistance value according to the voltage source adopted, using a digital potentiometer.

The heart rate and its variability are captured by PPG sensor SEN-11574 [28]. It combines a simple optical heart rate sensor with amplification and noise cancellation circuitry. Also, it sips power with 4mA current. It can be applied to the earlobe or on the finger surface. Emopad embeds SEN-11574 to be used on the finger surface contact, without any obstructive artifact. Fig 5. shows SEN-11574 on Emopad prototype.

The A/D converter was set up to multichannel sampling, enabling MSP430's Low Power Mode 0 (LPM0) at 500 Hz sampling rate. This sampling rate was defined based on PPG and HVR requirements, according to [31].

C. Dataset Storage and Usability Tests

Fig. 6 shows CollectPhys user interface running while a usability testing was applied. In order to support data exchange between Emopad Acquisition Systems (Fig.2) and PC software systems, a Matlab application was developed. It was called CollectPhys. CollectPhys enables Matlab's Data Acquisition Toolbox and its real-time plotter to receive, plot and save data from MSP430's USART module, embedded into Emopad hardware. Thus, wired and wireless serial communication can be configured to interconnect Emopad to videogame consoles. In the first Emopad version, a BlueSMiRF technology has been used to support wireless communication. The BlueSMiRF is the Bluetooth wireless serial cable replacement from SparkFun Electronics [32]. This modem works as a serial (RX/TX) pipe. Any serial stream from 2400 to 115200bps can be passed seamlessly from Emopad to videogame console. CollectPhys is also responsible to synchronize all sensors including those outside of Emopad, such as webcam, microphone, ambient temperature and humidity. On Fig. 7 is presented a structural description about data set sensor blocks.

In order to apply usability tests certain elements should be chosen, including those related to the protocol requirements. The game choice was based on gameplay parameter. A linear gameplay allows reproducibility and, consequently, short time tests. A horror game was chosen because of its inherent and most common effect, the scare. Fright condition can be easily perceived in physiological markers and it can be verified and correlated with video recordings, e.g., those obtained from webcam. For each participant the maximum gameplay was 30 minutes and Death Unknown software [33] was used for usability tests. Death Unknown was supported by Intel Core i5 processor, AMD Radeon 7750 video board and 6GB RAM memory. At the same PC console Death Unknown and CollectPhys were run. Fig. 8 shows the usability-testing environment.
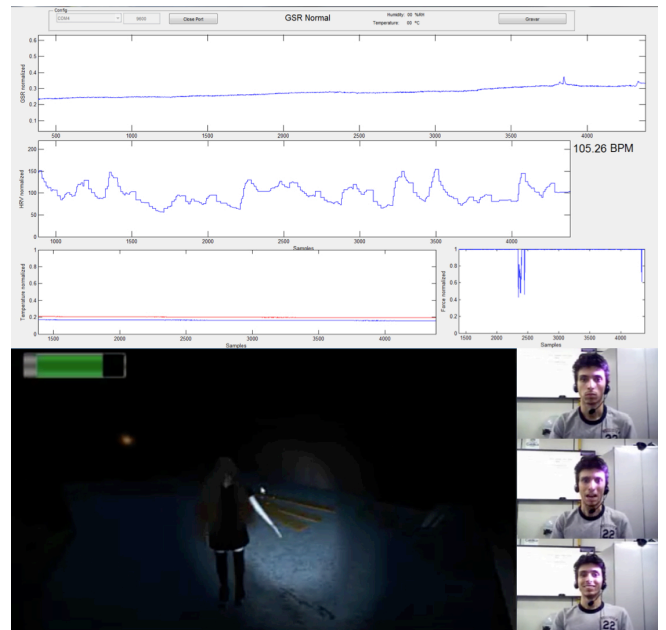

Fig. 5. Emopad – Preliminary Version.

Fig. 6. CollectPhys User Interfaces.

D. The Analysis Tools

Fig. 10 shows one screenshot obtained from analysis tools. They were conceived to evaluate and customize algorithms for real-time applications and are embedded in CollectPhys, presented in Section II-C (Fig. 6). Also, they are useful in visualizing sensors data on Matlab's environment and implements functionalities such as plotting, markers, labeling

Emopad acquired data. These tools can be very convenient in clinical application of the Emopad.
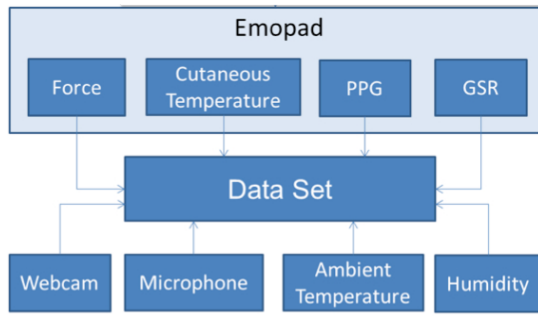

Fig. 7. Dataset Sensor Diagram Blocks.

Fig. 8. Usability Testing Envirolment.

E. Emopad's Window-based Algorithm

The event detection algorithm applied in acquired physiological signals is described in Fig. 9. It shows the filling and sliding of the window, presented in C language available to MSP430 TI microcontroller. In this example, each current signal sample is stored into array called "window". The best WINDOW_SIZE and SHIFT values were adjusted after the algorithm evaluation described in Section III.

For each new signal sample the "__interrupt void USCI0TX_ISR(void)" function is invoked, which is responsible to detect alterations (abnormalities) on each window. The proposed algorithm can be analyzed as a modified version of the hill-climbing algorithm. Fig. 10 illustrates Emopad's Window-based Algorithm when it was applied to process a GSR channel while an instance of the usability testing was executed.

The variable "currentDifference" computes the difference between the maximum and minimum samples stored in each "window". Next, "AvarageSum" and "currentDifference" are incremented in order to establish the threshold level, which corresponds to arithmetic mean, moving on each window. It is important to filter many false positive and to detect peaks. Thus, if "currentDifference" is minor than

"previousDifference" and "previousDifference" is major than threshold level ("currentAvarange"), the search algorithm has to "climb", else it has to come down, meaning "isClimb" should receive and return 0.

```
#define WINDOW_SIZE 110
#define SHIFT 10

unsigned int gsrValue;
unsigned int window[WINDOW_SIZE];
unsigned int indexWindow = 0;
unsigned int AverageSum = 0;
unsigned int currentAverage = 0;
unsigned int countAverage = 0;
unsigned short isClimb = 1;
unsigned int previousDifference = 0;
unsigned short alteredWindow = 0;

#pragma vector=USCIAB0TX_VECTOR
__interrupt void USCI0TX_ISR(void){
unsigned int indexWindow = 0;
unsigned int maximum, minimum  = 0;

if(indexWindow==WINDOW_SIZE){
maximum  = window[0]; minimum = window[0];

for(int i=0;i<WINDOW_SIZE;i++)  {
      if(window[i]>maximum)
            maximum = window[i];
      if(window[i]<minimum)
            minimum = window[i]; }

int currentDifference = maximum-minimum;
AverageSum = AverageSum + currentDifference;
currentAverage = AverageSum/++countAverage;

if(isClimb) {
      if (currentDifference < previousDifference &&
previousDifference > currentAverage){
      alteredWindow = 2;
      isClimb = 0;}
      else{alteredWindow = 1;}
      } else { alteredWindow = 1;
            if(currentDifference >
previousDifference) isClimb = 1;}
previousDifference = currentDifference;
indexWindow = SHIFT; int j = SHIFT;
for(i = 0;j<WINDOW_SIZE;i++,j++){
      window[i] = window[j];}}}
window[indexWindow++] = gsrValue;}
```

Fig. 9. The MSP430's Event Detection Algorithm.

In Fig. 10 the blue line plots the normalized GSR raw signal in the time domain (indexing sample number) while red line plots filtered GSR. The proposed algorithm reduces data

dimensionality defining only one data sample to represent each window, highlighted in gray columns. This data sample is defined based on the difference between maximum and minimum encountered values. Also, it acts as rectifier preparing GSR signal to next stage. After that, hill-climbing algorithm can be applied in order to detect GSR peak points.
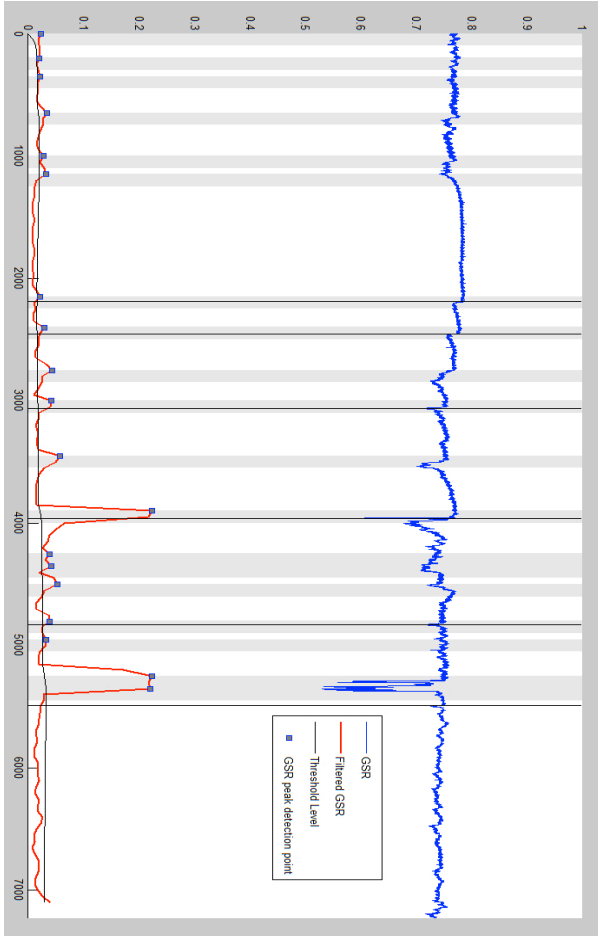

Fig. 10. Analysis Tools Screenshot.

III.   PRELIMINARY EVALUATION AND RESULTS

The Emopad evaluation methodology was based on [34]. The usability tests were carried out in the 505E room in the Embedded Systems Laboratory, Department of Computing at Pontifical Catholic University of Goiás. The main aim of this activity was to collect and process physiological signals using the first version of Emopad prototype, presented in Fig. 5. Thus, the proposed window-based algorithm (Section 2.E) could be evaluated in real conditions. Also, ergonomic features have been assessed.

The participants were students from Computing Department, with a total of 31, 15 female individuals of ages from 19 to 25 years old (21.5 ± 1) and 16 male individuals of ages from 19 to 25 years (21.5 ± 1.5). As described in Section 2.C, this paper proposes to induce fright in order to obtain a proper arousal in terms of physiological signals and simulate real conditions of using proposed technology. Female and

male individuals differs have similar responses when the stress stimuli consist of specific actions in a very short period of time, e.g., an accident, an armed robbery, and the like [34]. Thus, we argue that the same horror game was a good choice for provoking scare in real conditions, although the 20 minutes (on average) for each gameplay.

Depending on the threshold level defined to window-based algorithm described in Section 2E is necessary to differ True Scare Detection (TSD) rate from True non-Scare Detection (TNSD) rate. TSD corresponds to sensitivity statistical measurement while TNSD to the specificity. To compute TSD:

TSD = True Positive/(True Positive + False Negative)

Where a True Positive means classifying as scared an individual GSR window which is indeed represents a real scare (seen on Webcam and correlated with HR peak), and False Negative means classifying as normal a GSR window which is corresponding to real scare. To compute FSD:

TNSD = True Negatives/(True Negatives + False Positives)

Where a True Negative means classifying as non-scare an individual GSR window which is indeed represents a normal window (without GSR peaks) and False Positives means classifying as scared a GSR window which contains only normal samples, eg., relaxed. Fig. 11 shows TSD and TNSD for the ten better window size/displacement size of the window, called "shifting size", showed in Table I while Table II presents the Confusion Matrix corresponding to the best configuration encountered in Table I.

TABLE I.   BEST TSD AND FSD RATES OBTAINED DURING THE EMOPAD USABILITY TESTING FOR PROPOSED WINDOW-BASED ALGORITHM .

Window Size	Shifting Size	TSD(%)	TNSD(%)
140	30	100	92.4
120	20	100	93.9
120	**10**	**100**	**95.5**
110	40	100	90.5
110	**10**	**100**	**95.5**
90	10	100	94.3
80	10	100	93.6
70	10	100	92.8
60	10	100	92.3
50	10	100	91.7

Clearly, TSD and TNSD depend on threshold level, highlighted in Fig. 9. If threshold decreases the algorithm considers every output as an event related to scare. Thus, if threshold increases TSD increases while TNSD decreases. The threshold level is computed based on arithmetic mean. Thus, a compromise must be reached by finding the best configuration of window size versus shifting size, when TSD are close to TSND. These indexes indicate where the errors in detecting false positives and false negatives are close. Fig. 11 shows

TSD and TNSD performance related to the window size, when the shifting size is fixed, equals to 10 while Fig. 12 shows the same indexes when the displacement size of the window is changed to twenty samples. Both graphics are selected based on evidences encountered in Table I. Blue line represents TSD percentage while red line describes TNSD performance.
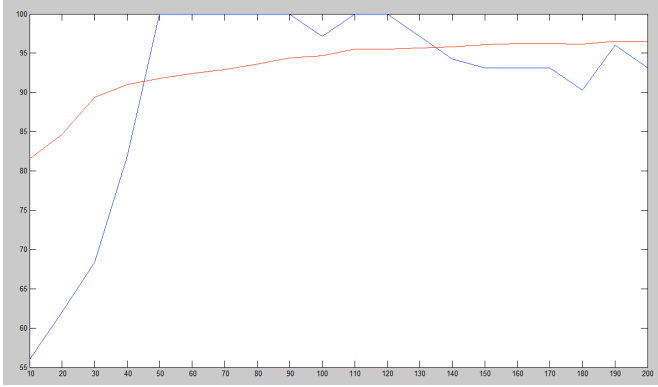

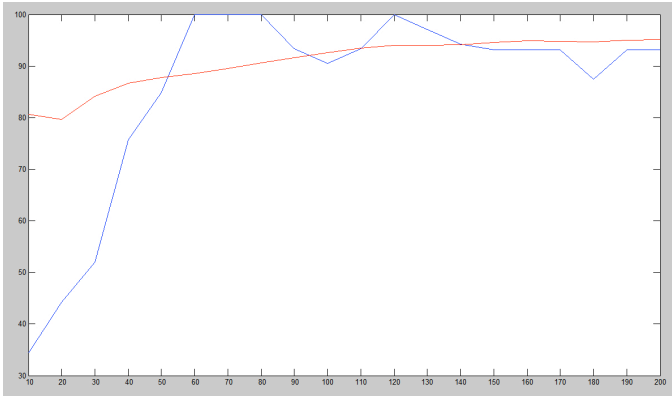Fig. 11. TSD and TSND performance for shifting size equals to ten samples.

Fig. 12. TSD and TSND performance for shifting size equals to twenty samples.

When the window size is very short errors become greater, even if the shifting size is changed to 20 samples (Fig. 12). The best performance is encountered when the window size is setup to 110 and the shifting size is setup to 10 samples (Fig.11), and window size equals to 120, shifting size equals to 20, in Fig. 12. When the window size is bigger, more memory amount is required from embedded hardware. This is the assumption required for evaluating the performance of minors' window sizes. Fig. 11 and Fig. 12 reveal that the performance obtained from the window size when it is equals to 110 is almost the same (only 3% more) when compared to the windows size when it is equals to 50. Table II shows the confusion matrix related to the best configuration obtained from Table I while Table III shows the confusion matrix when window size is halved. The "Scare" label counts the number of strong abnormalities for each processed window while "Non-Scare" label counts the number of processed windows without

any strong abnormalities (high peaks). As it was verified in manual classification, almost always (95%) there is a scare when a high peak occurs.

TABLE II.   CONFUSION MATRIX CORRESPONDING TO THE BEST CONFIGURATION (WINDOW SIZE=110/SHIFITING SIZE=10) ACCORDING TO TABLE I.

		Actual	
		Scare	Non-Scare
Predicted	Scare	*33*	*0*
	Non-Scare	*472*	*9605*

TABLE III.   CONFUSION MATRIX CORRESPONDING TO THE CONFIGURATION (WINDOW SIZE=50/SHIFITING SIZE=10) .

		Actual	
		Scare	Non-Scare
Predicted	Scare	*32*	*0*
	Non-Scare	*828*	*9280*

IV.   CONCLUSION AND FUTURE WORK

A Sony registered patent[1] became public on 2014 revealing a framework that should be developed for emotion recognition. It was called Multi-modal Sensor based Emotion Recognition And Emotional Interface [35]. "If the emotional state of the user or game player is known, a game or machine can dynamically adapt accordingly. For example, in a simple case, a game can become easier or harder for the user depending on the detected emotional state of the user". Sony's framework shares many hypotheses with Emopad project, although neither technology or algorithm solution was revealed or evidenced based on Sony's patent description. Thus, this paper proposes and presents a feasible platform, describing a complete solution and arguing that this sort of technologies can be used remote clinical monitoring.

The proposed scare-detection system that is embedded in traditional gamepad can be useful not only to entertainment applications, but its inherent characteristics, such as non-invasiveness and non-obstructiveness become it adequate to point-of-care monitoring. Thus, a multiparametric affective monitor is proposed.

Future works will concentrate in many aspects of Emopad, especially those related to data fusion algorithms in order to improve the pattern recognition accuracy based on multi-modal sensor feature available on proposed platform. At this moment a classification algorithm is been developing to inform the game engine about arousal related to scare and other relevant emotional states. Also, a study involving many participants aims to reveal how temperature variations can be useful to recognize and classify emotional states.

---

[1] Patent number US20140112556.

REFERENCES

[1] R. Picard, "Affective computing", MIT Press. Boston, 1997.

[2] M. F. A. Carvalhaes, A. F da Rocha, M. F. Vieira and T. M. G. de A. Barbosa, "Affective embedded systems: a requirement engineering aproach", International Journal of Computer Trends and Technology (IJCTT), v. 8, pp. 70-75, Feburary 2014.

[3] D. Bersak, G. McDarby, N. Augenblick, et al., "Intelligent biofeedback using an immersive competitive environment," in Proceedings of the UbiComp Workshop on Designing Ubiquitous Computing Games, 2001.

[4] V. H. M. Gomide, P. A. Valle, J. O. Ferreira, J. R. G. Barbosa, A. F. da Rocha and T. M. G. de A. Barbosa, "Affective crowdsourcing applied to usability software", International Journal of Computer Science and Information Technologies (IJCSIT), Vol. 5 (1), 2014, 575-579. doi: 10.14445/22312803/IJCTT-V8P113.

[5] J. Schumm, C. Setz, M. Bächlin, M. Bächler, B. Arnrich, G. Tröster, "Unobtrusive physiological monitoring in an airplane seat", Personal and Ubiquitous Computing, V. 14 (6), 2010, pp. 541-550. doi: 10.1007/s00779-009-0272-1.

[6] M. Z. Poh, k. Kim, K., A. D. Goessling,N. C. Swenson, R. W. Picard, "Heartphones: sensor earphones and mobile application for non-obtrusive health monitoring," Proceedings of the 13th IEEE International Symposium on Wearable Computers, Linz, Austria, 2009, pp. 153-154.

[7] R. Fletcher, K. Dobson, M. S. Goodwin, H. Eydgahi, D. Wilder-Smith, D. Fernholz, Y. Kuboyama, E. Hedman, M. Z. Poh, R. W. Picard, "iCalm: wearable sensor and network architecture for wirelessly communicating and logging autonomic activity," IEEE Transactions on Information Technology in Biomedicine, vol.14, no.2, pp.215-223, March 2010. doi: 10.1109/TITB.2009.2038692.

[8] F. Arafsha, K. M. Alam and A. El Saddik, "EmoJacket: consumer centric wearable affective jacket to enhance emotional immersion", Proceedings of International Conference on Innovations in Information Technology (IIT), 2012, pp. 350-355.

[9] M. Z. Poh, D. J. McDuff and R. Picard, "Advancements in Non-contact, Multiparameter Physiological Measurements Using a Webcam," IEEE Transactions on Biomedical Engineering, vol.58, no.1, pp. 7-11, Jan 2011. doi: 10.1109/TBME.2010.2086456.

[10] M. Z. Poh, D. J. McDuff and Picard, R.W., "A Medical Mirror for Non-Contact Health Monitoring," ACM SIGGRAPH Emerging Technologies, Aug 2011.

[11] R. Fernandez and R.W. Picard (2003), "Modeling Driver's Speech under Stress," Speech Communication, Volume 40, pp. 145-159.

[12] J. Hernandez, D. McDuff, X. Benavides, J. Amores, P. Maes and R. Picard, "AutoEmotive: Bringing Empathy to the Driving Experience to Reduce Stress," To appear as a provocative work in Designing Interactive Systems (DIS), Vancouver, Canada 2014.

[13] J. Hernandez, I.Riobo, A. Rozga, G. D. Abowd and R. W. Picard, "How Easy Are Children to Engage during Child-Adult Play? Using Electrodermal Activity as Identifier", To appear in the Extended Abstract of IMFAR, Alanta, USA, 2014.

[14] T. Teixeira, T. Kaliouby and R. Picard, "Why, When and How Much to Entertain Consumers in Advertisements? A Web-based Facial Tracking Field Study," Marketing Science (To Appear) 2014.

[15] M. Eckhardt, C. Ferguson and R. W. Picard, "A Platform for Creating Stories Across Digital and Physical Boundaries," Proceedings of the 8th International Conference on Tangible, Embedded and Embodied Interaction. ACM, 2014.

[16] K. Williams, J. Peters and C. Breazeal, "Towards Leveraging the Driver's Mobile Device for an Intelligent, Sociable In-Car Robotic Assistant," IEEE Intelligent Vehicles Symposium, 23-26 Jun. 2013.

[17] S. O. Adalgeirsson and C. Breazeal, "MeBot: A robotic platform for socially embodied telepresence" Proceedings of 5th ACM/IEEE International Conference on Human-Robot Interaction (HRI), 2010.

[18] K. Schaaff and M. T. P. Adam, "Measuring Emotional Arousal for Online Applications: Evaluation of Ultra-Short Term Heart Rate Variability Measures" Proceedings of Humaine Association Conference on Affective Computing and Intelligent Interaction, 2013.

[19] A. Parnandi, Y. Son amd R. Gutierrez-Osuna, "A Control-Theoretic Aproach to Adaptive Physiological Games" Proceedings of Humaine Association Conference on Affective Computing and Intelligent Interaction, 2013.

[20] M. W. Kennedy, J. P. Shimiedeler, C. R. Crowell, M. Villano, A. D. Striegel and J. Kuitse, "Enhanced Feedback in Balance Rehabilitation using the Nintendo Wii Balance Board" Proceedings of 13th IEEE International Conference on e-Health Networking, Applications and Services, 2011.

[21] L. E. Nack, M. Kalyn, C. Lough and R. L. Mandryk Biofeedback Game Design: Using Direct and Indirect Physiological Control to Enhance Game Interaction" Proceedings of ACM Conference on Human Factors in Computing Systems (CHI), 2011.

[22] J. Hsu, "Game Controller Senses Players' Excitement Levels", online: http://spectrum.ieee.org/tech-talk/consumer-electronics/gaming/game-controller-senses-players-excitement-levels, April, 2014.

[23] W. Wolf. Computers as Components, Principles of embedded computing System design, ELSEVIER, 2nd edition, 2008.

[24] STERN, R.M., RAY, W.J.& QUIGLEY, K.S., Psychophysiological Recording. (2nd ed.), Oxford University Press, New York, 2001.

[25] Lang, P. J.The Emotion Probe. American Psychologist, 50(5), pp.372-385, 1995.

[26] J. Bishop, "Thermistor temperature transducer-to-ADC application" in Analog Applications Journal, Texas Instruments Incorporated.

[27] Epcos, "NTC thermistors for temperature measurement", Mar 2013.

[28] Shapeways. Online: http://www.shapeways.com.

[29] Neurosky – Body and Mind: Throw Trucks. Oline: http://store.neurosky.com/products/throw-trucks-with-your-mind?mc_cid=6c3dfb6fe0&mc_eid=53dde7647e.

[30] R. W. Picard, S. Fedor and Y. Ayzenberg, "Multiple Arousal Theory and Daily-Life Electrodermal Activity Asymmetry" Emotion Review, (To Appear) 2014.

[31] J. G. Webster, "Medical Instrumentation Application and Design", 4th ed., Wiley, 2009.

[32] Sparkfun, "Bluetooth Modem – BlueSMiRF".Online: https://www.sparkfun.com/products/12582.

[33] Game Jolt, "Death Unknown". Online http://gamejolt.com/games/other/death-unknown-v-1-2/16329/"

[34] A. S. Sierra, C. S. Ávila, J. G. Casanova and G. B. del Pozo, "A Stress-Detection Based on Physiological Signals and Fuzzy Logic", IEEE Transactions on Industrial Electronics, v. 58, n. 10, october 2011.

[35] O. Kalinli-Akbacak, "Multi-modal sensor based emotion recognition and emotional interface". Online: http://www.google.com/patents/US20140112556.

[36] P. H. F. Bacchini, J. O. Ferreira and T. M. G. de A. Barbosa, "Emopad: An Affective Gamepad", International Journal of Computer Applications, vol. 102, no. 15, pp.6-12, Sept. 2014. doi: 10.5120/17889-8885