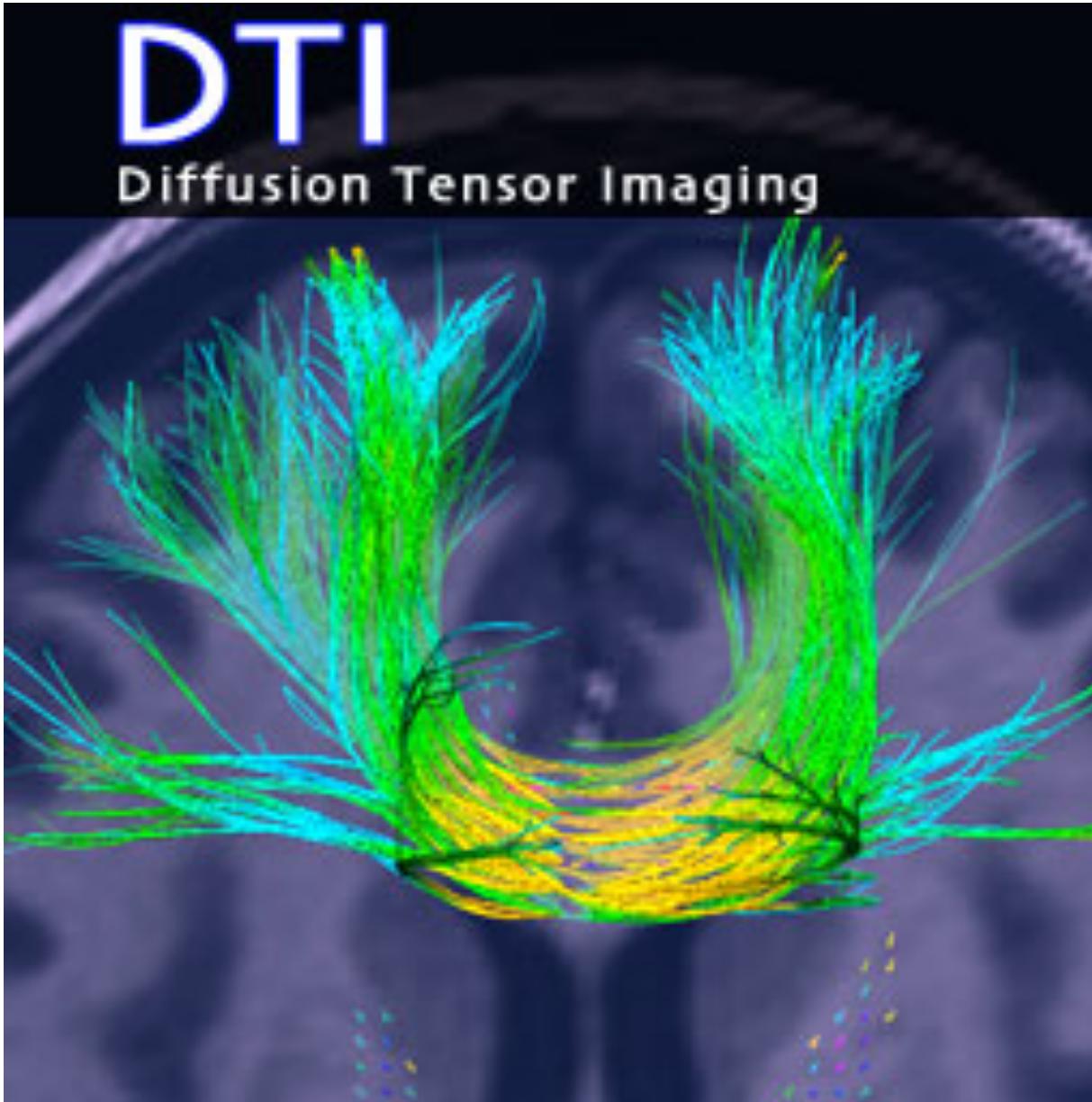


# DTI

Diffusion Tensor Imaging



# Diffusion tensor imaging (Part 2)

Valentina Giunchiglia



v.giunchiglia20@imperial.ac.uk

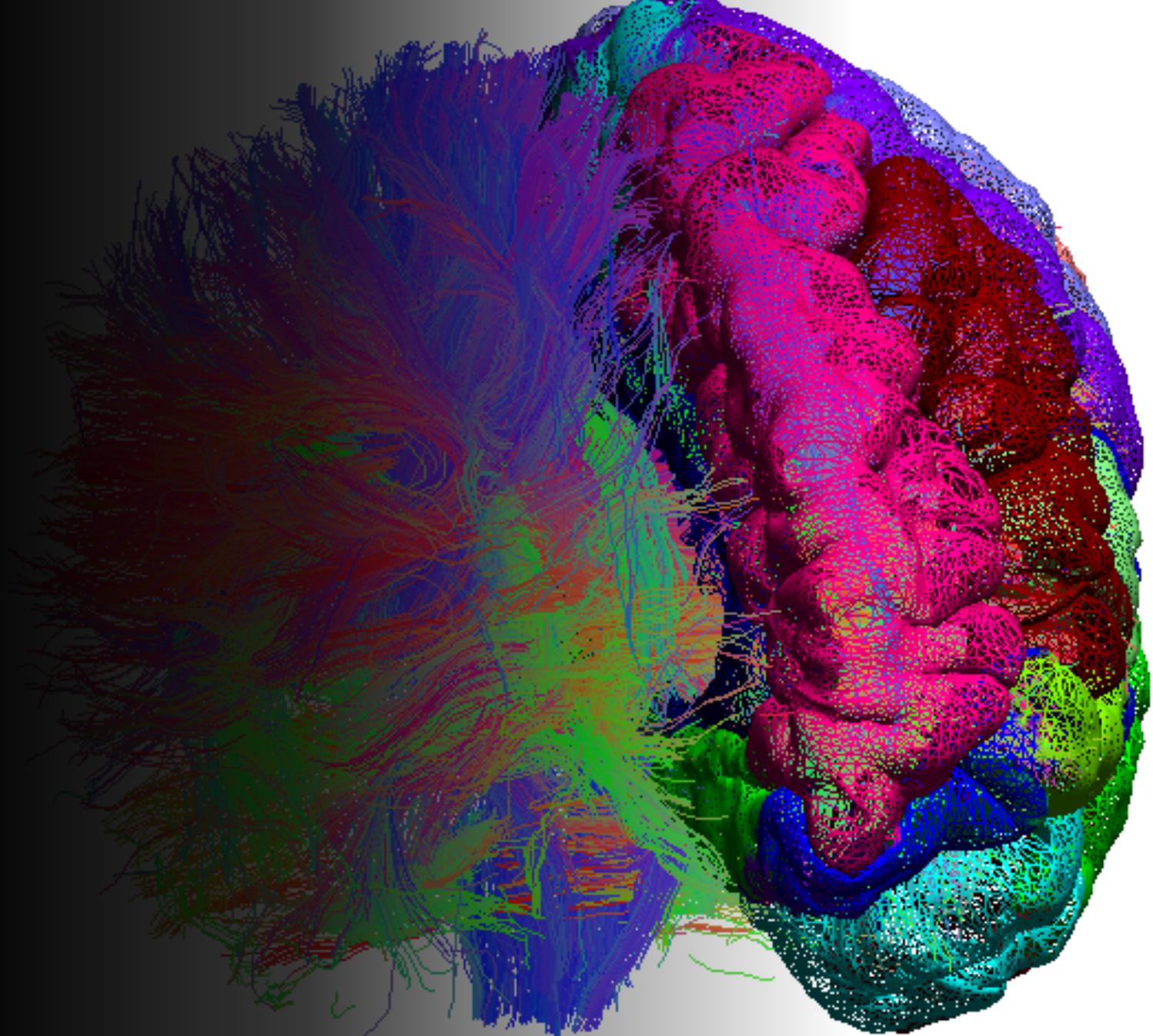


@valegiunca

# What you will learn from this talk

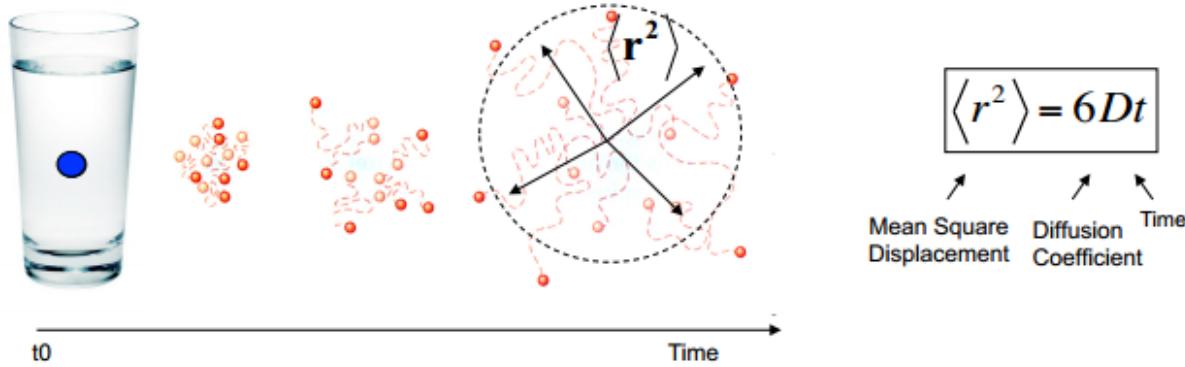
---

- What diffusion is
- How we acquire brain images sensitive to diffusion
- Diffusion tensor imaging
- Imaging metrics
- Tractography
- Limitations
- Spherical deconvolution

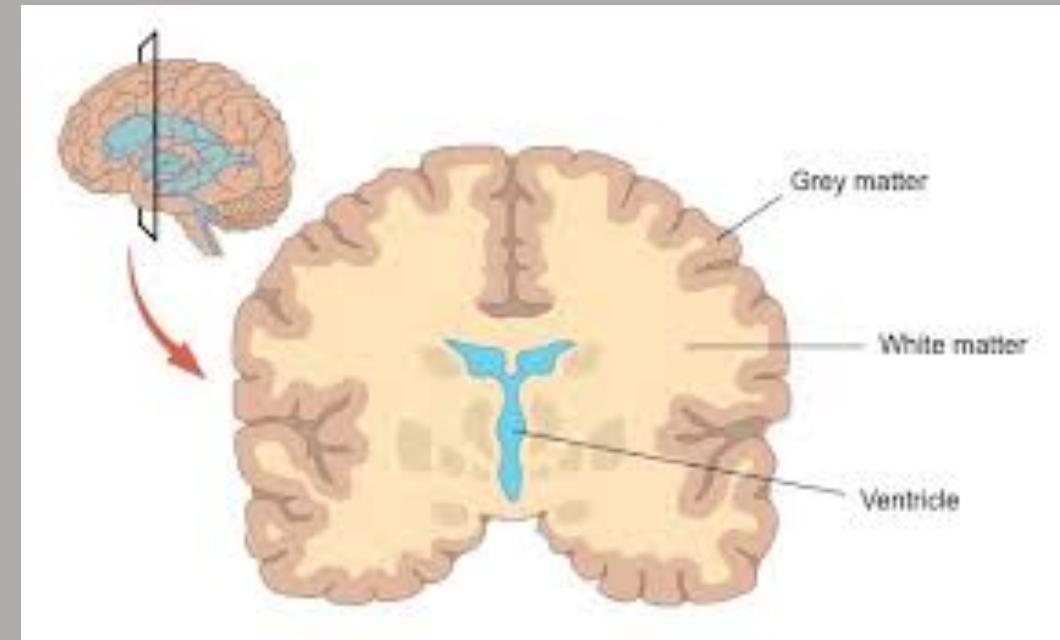


# Diffusion

**Diffusion is a random walk process**  
(e.g. Random motion of water molecules)



**Displacement** is proportional to the Diffusion Coefficient and the Time.

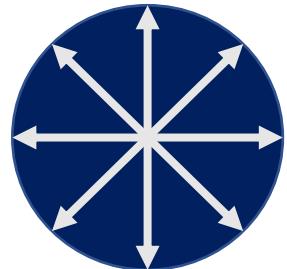
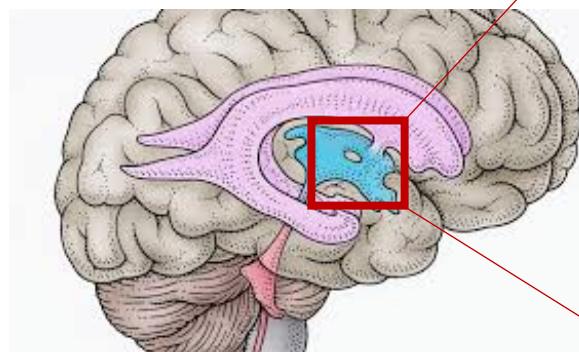


Different parts of the brain will have different diffusion properties due to their structure

# Diffusion in the brain

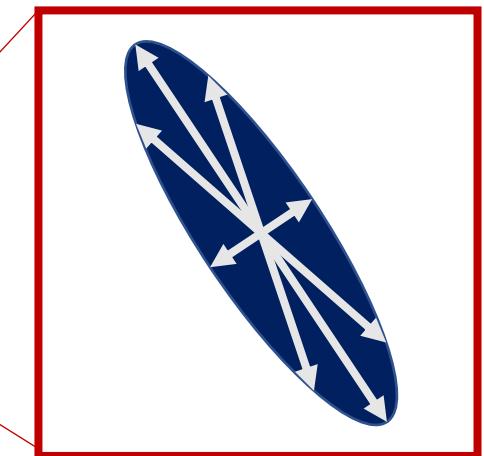
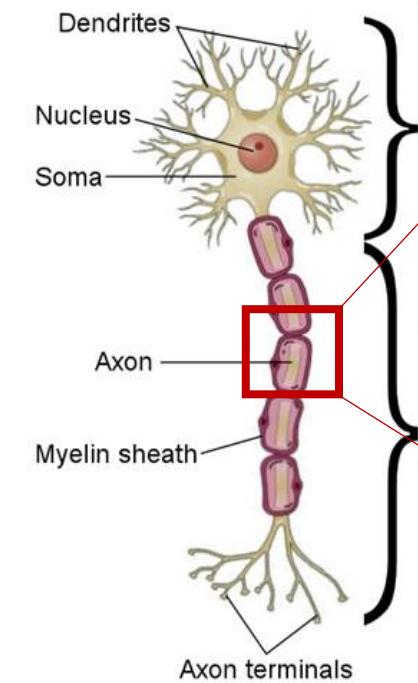
## Isotropy

Unconstrained diffusion



## Anisotropy

Restricted diffusion



# Clinical benefits of diffusion weighted imaging

NOW

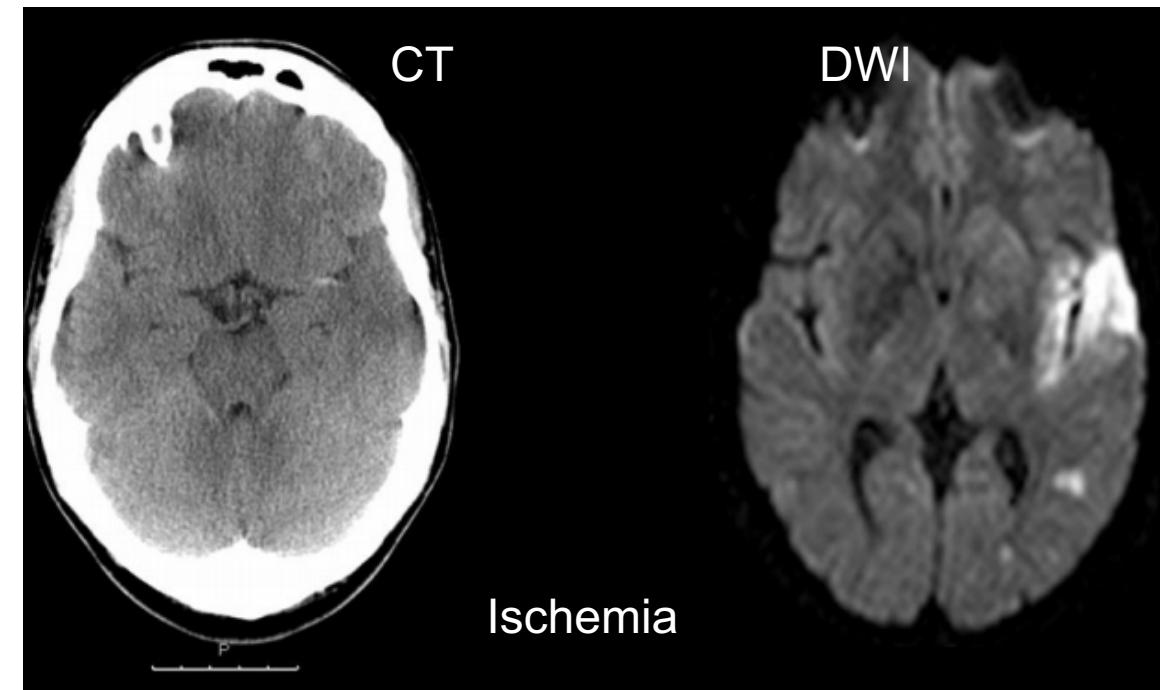
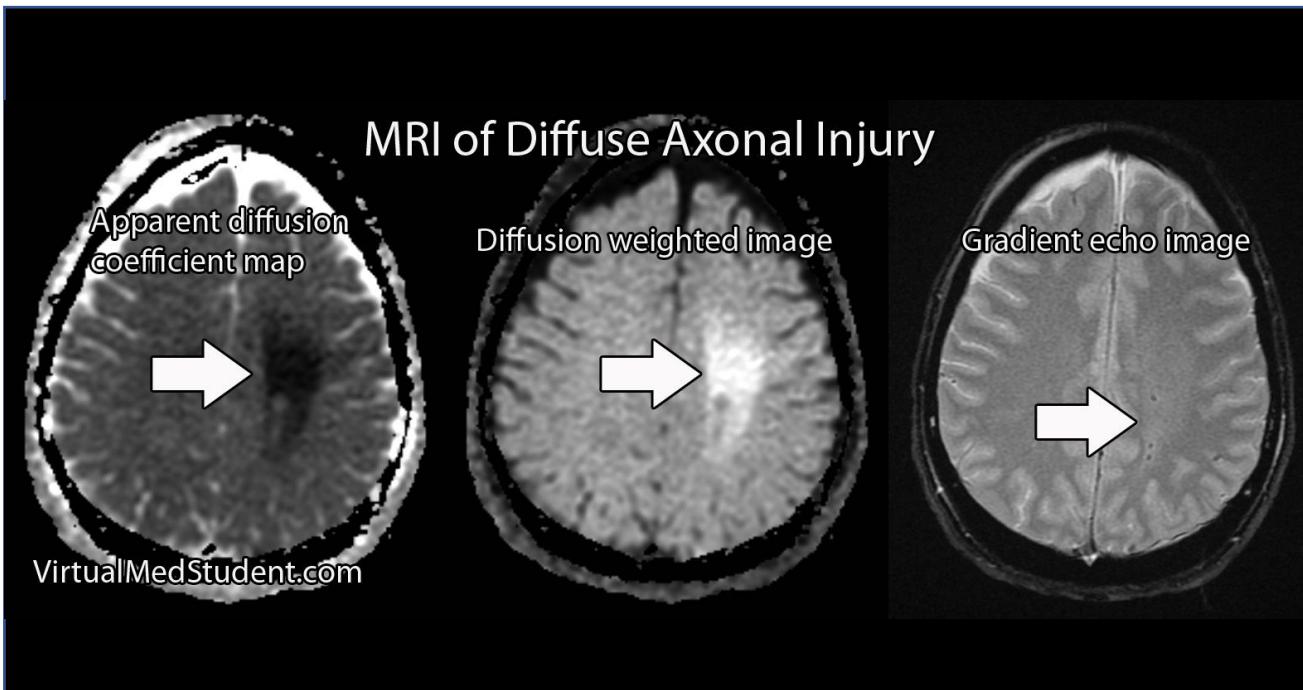


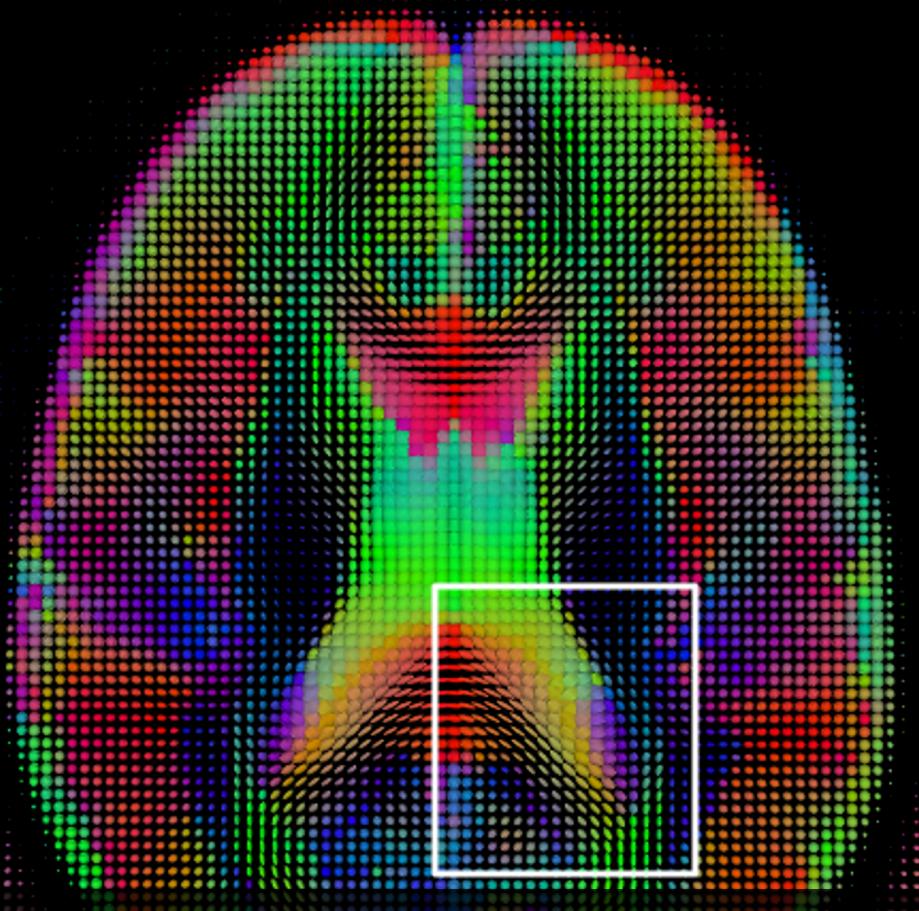
CT scans are used to examine white matter damage and ischemia.

BUT

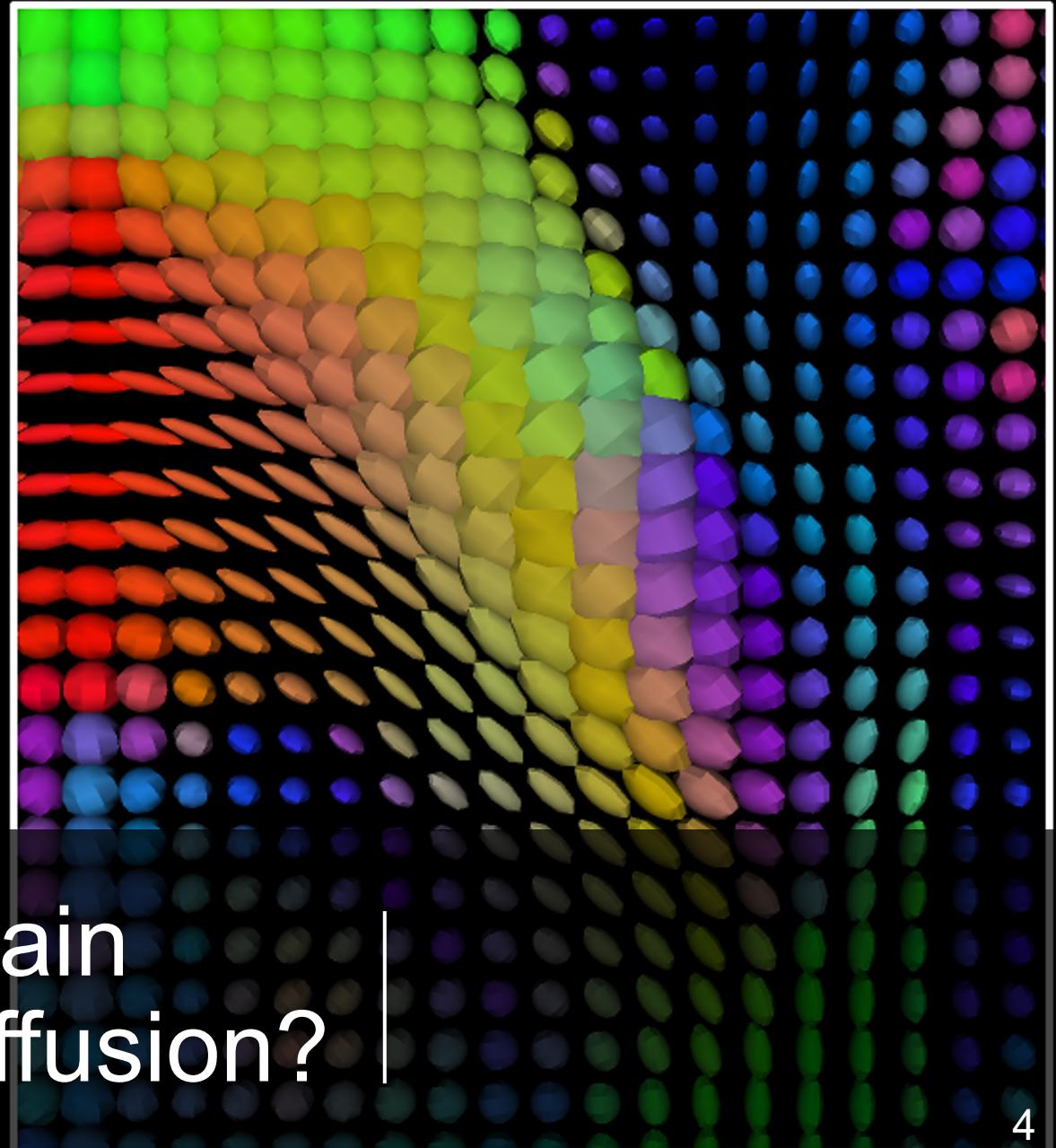


Huge applications for diffusion weighted imaging in clinical practice.



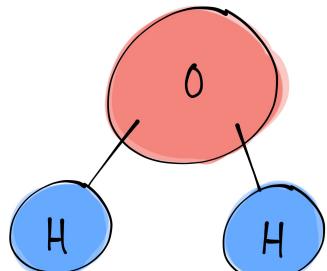


How do we acquire brain  
images sensitive to diffusion?

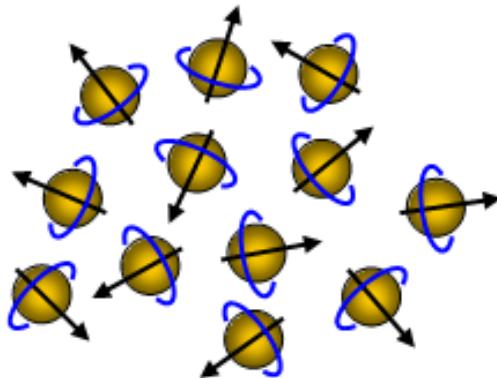


# MRI summary

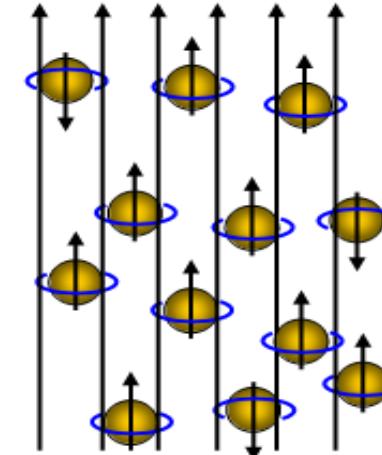
a. The body is 60% H<sub>2</sub>O



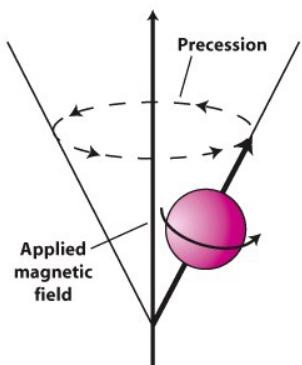
bi. Protons normally dance around



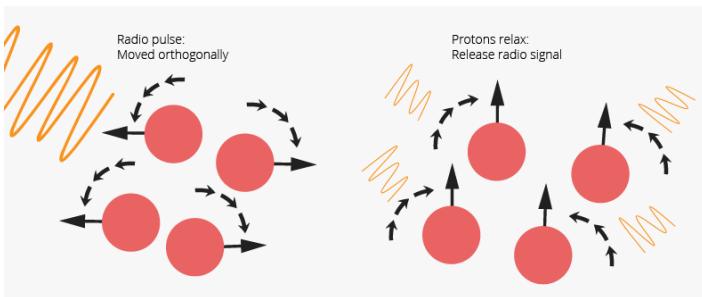
bii. Protons align inside a magnetic field



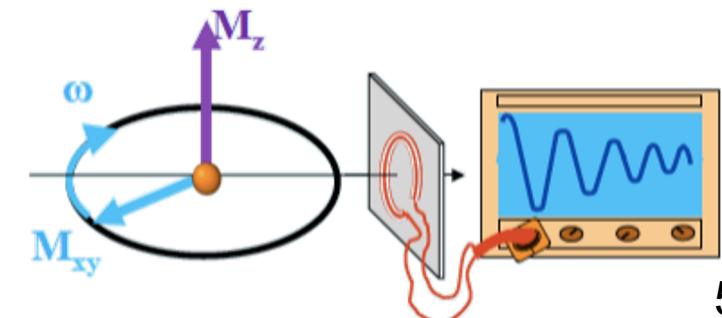
c. Precession



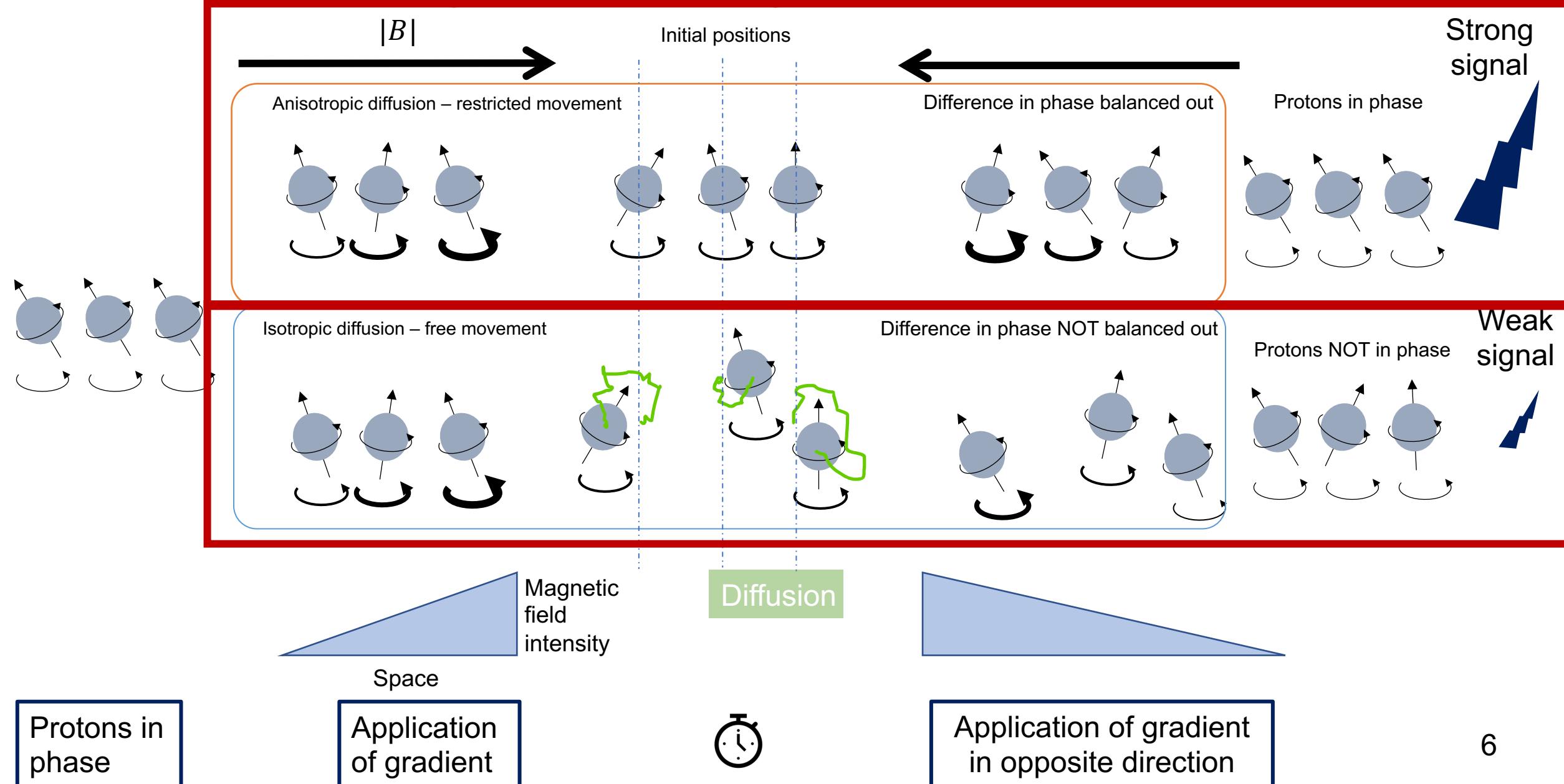
d. RF pulses give energy to the protons.



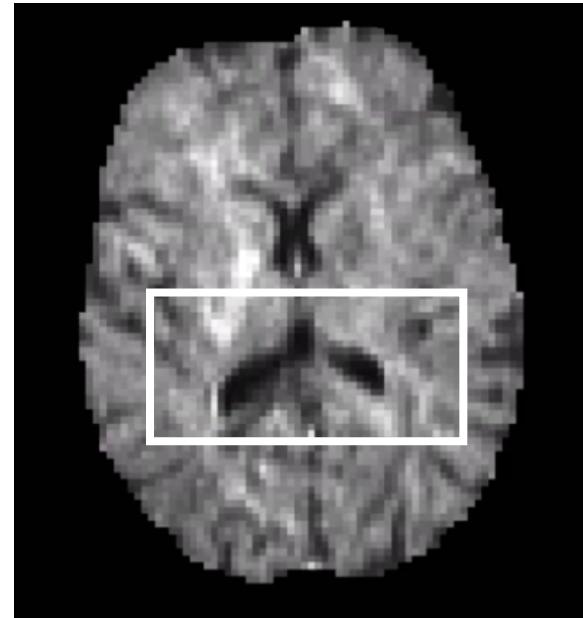
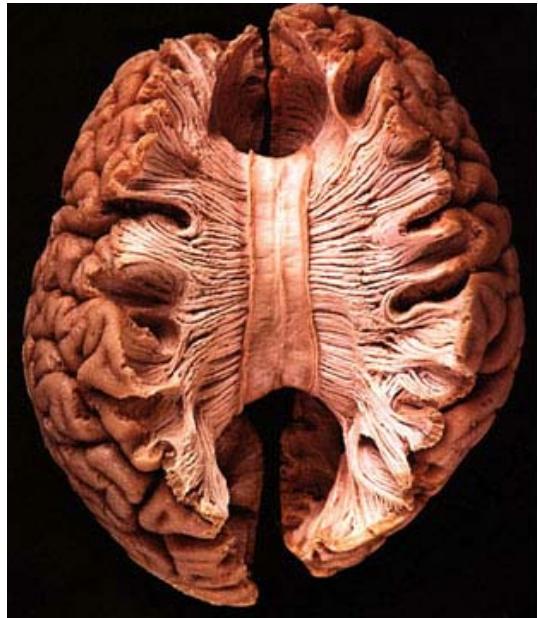
e. MRI measures the energy released



# Diffusion weighted images



Diffusion is along the direction of the gradient...

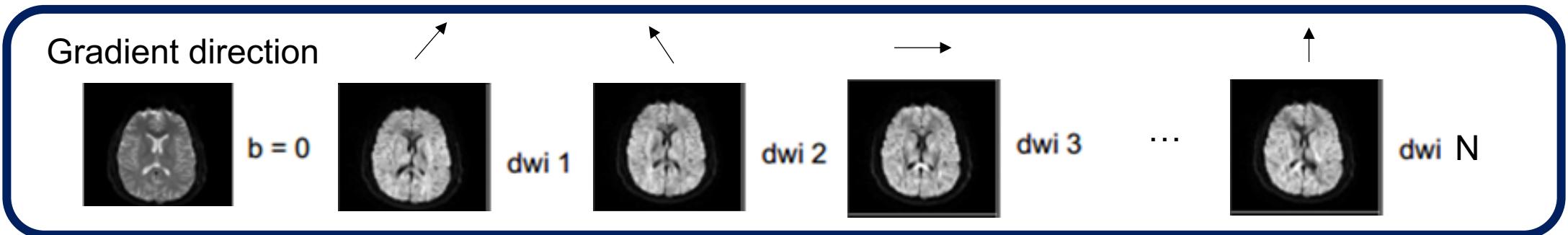


Corpus Callosum

# Diffusion MRI encoding

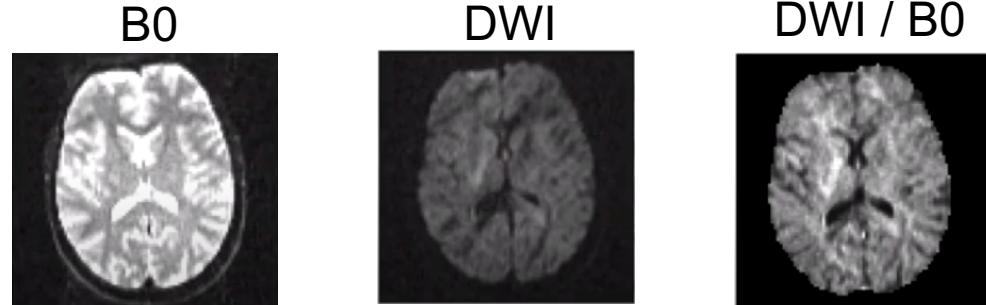
1

- Acquisition of multiple DWI with different gradient directions
  - Directions must be uniform through space
  - Minimum: 6, Quality data  $> 30$
  - We normally use 64 directions



2

- Diffusivity calculated relative to the  $b=0$  image



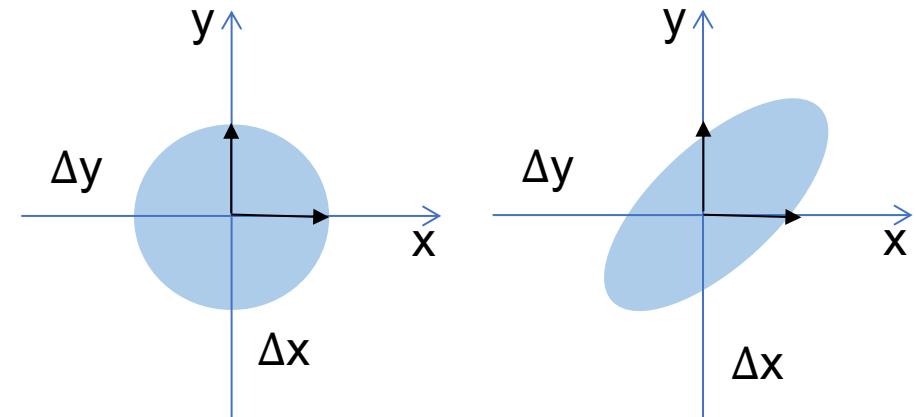
# The diffusion tensor and array

$$\begin{bmatrix} D_{xx} & D_{xy} & D_{xz} \\ D_{xy} & D_{yy} & D_{yz} \\ D_{xz} & D_{yz} & D_{zz} \end{bmatrix}$$

Diagonal elements (D<sub>xx</sub>, D<sub>yy</sub> and D<sub>zz</sub>) diffusion coefficients along x,y and z axis.

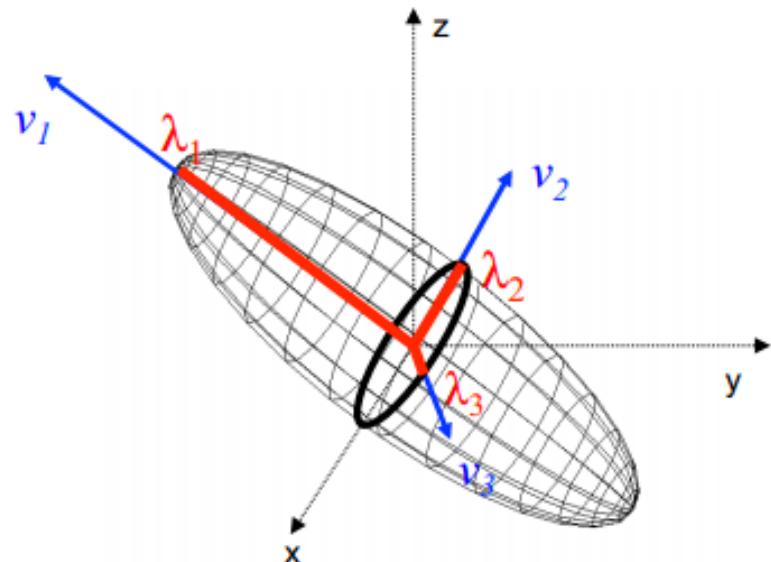
Off-diagonal elements correlation of motions between each pair of directions.

**DIFFUSION TENSOR:** 3x3 symmetric matrix that represents the diffusion rates in each combination of directions.



According to  $\Delta x$  and  $\Delta y$ , they look the same

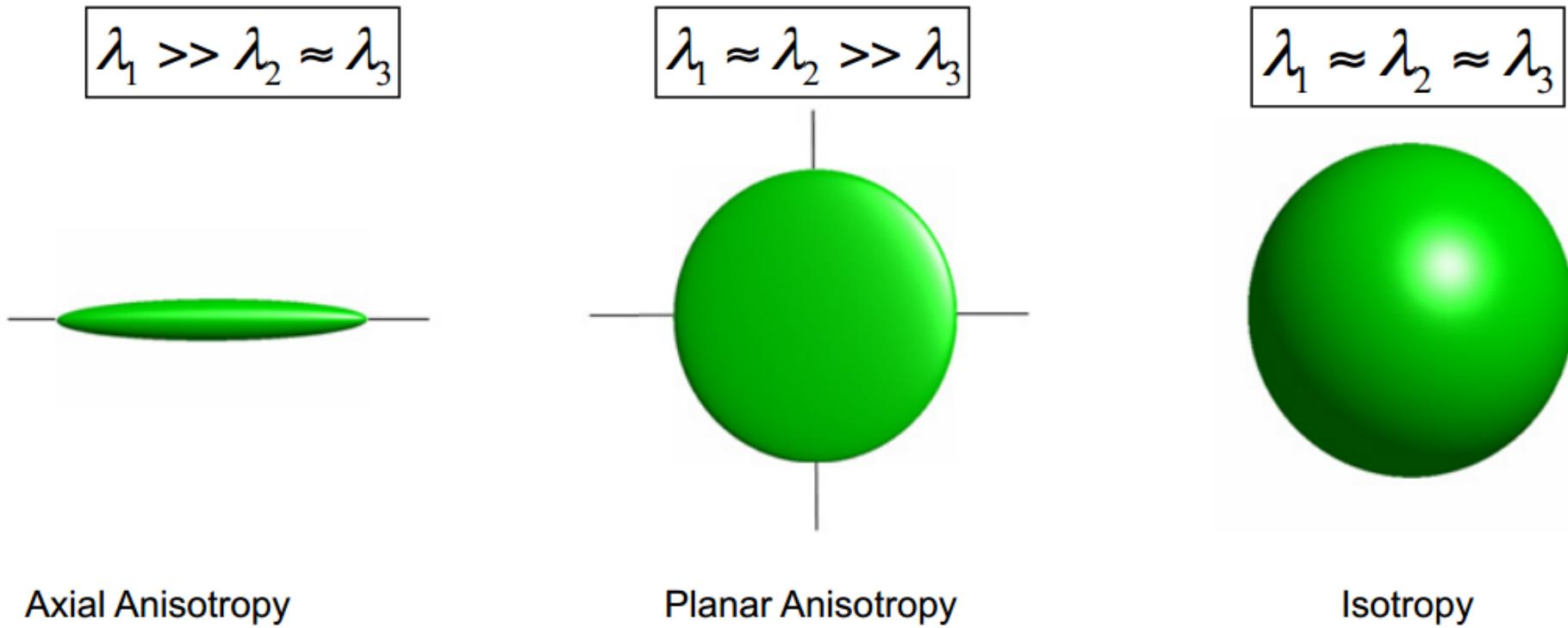
# How to get a more interpretable coordinate system?



## Eigenvalue decomposition

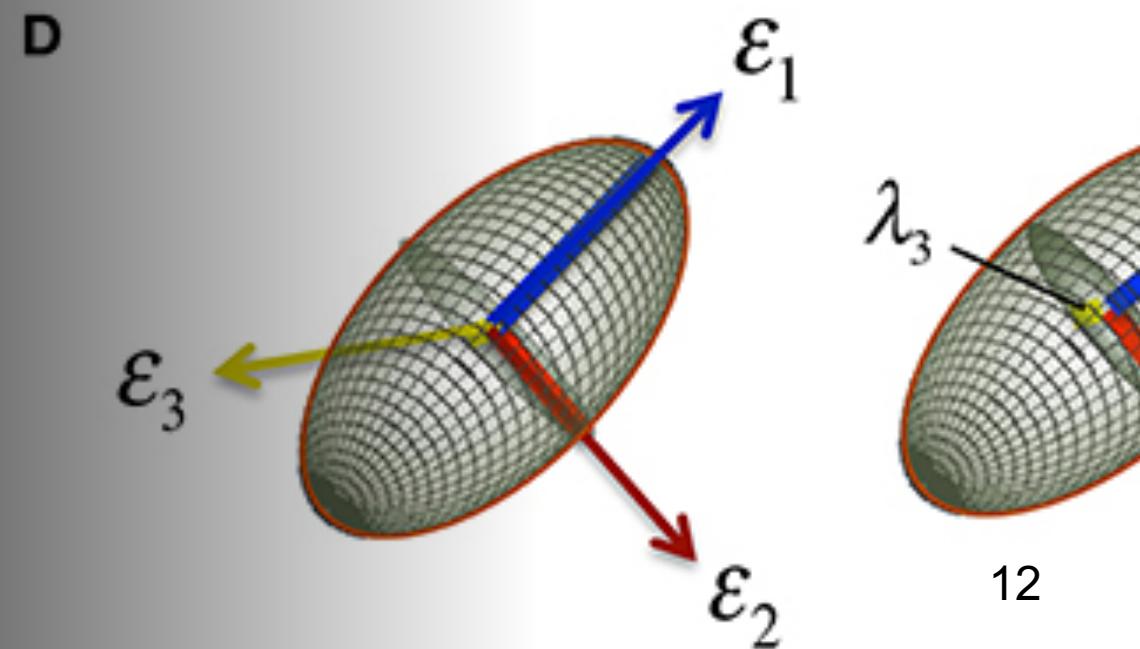
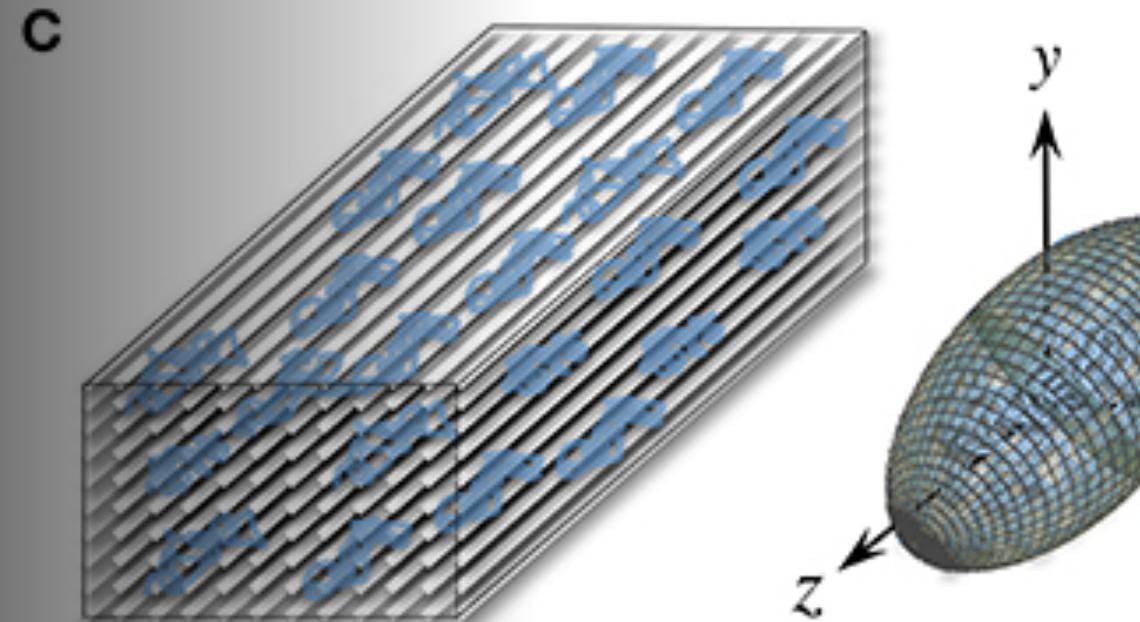
- 3 Eigenvectors –
  - Represent the **direction** of diffusion
  - First eigenvector = preferred direction
- 3 Eigenvalues -
  - Represent the **magnitude** of diffusion.

# Ellipsoid tensors provide 3D characterisations of water diffusivity

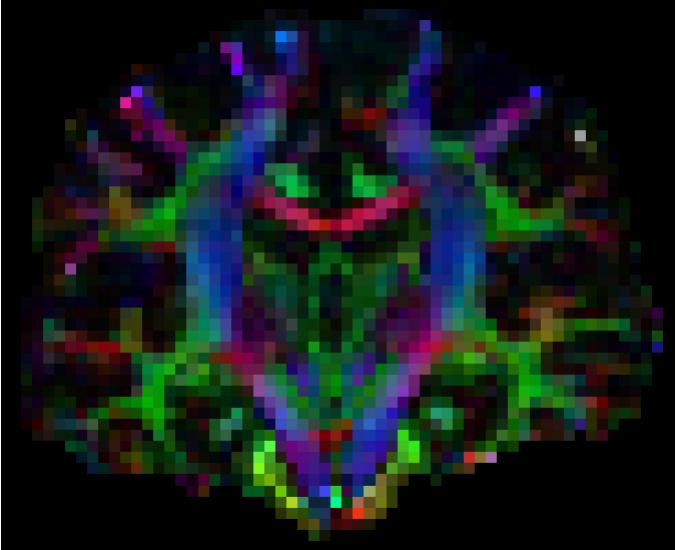
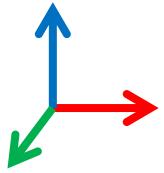


How do we  
represent 3D  
diffusion?

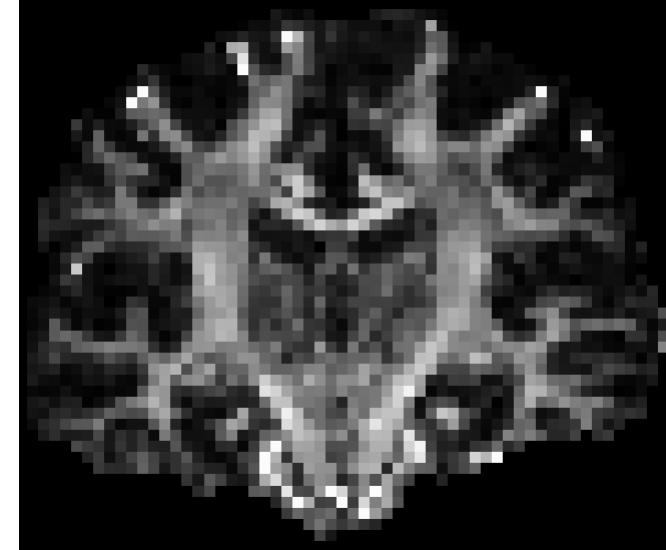
$N_d=30$



# 3D diffusion



**RGB** maps represent the orientation of each voxels tensor

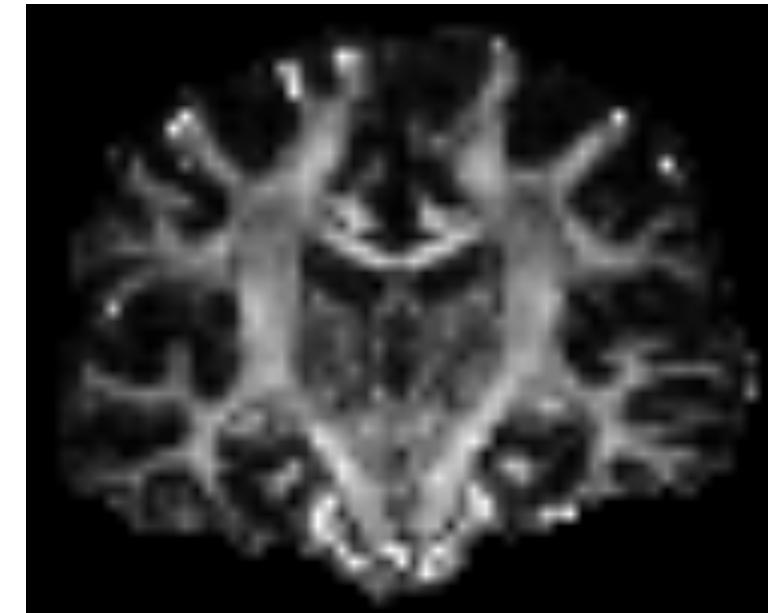
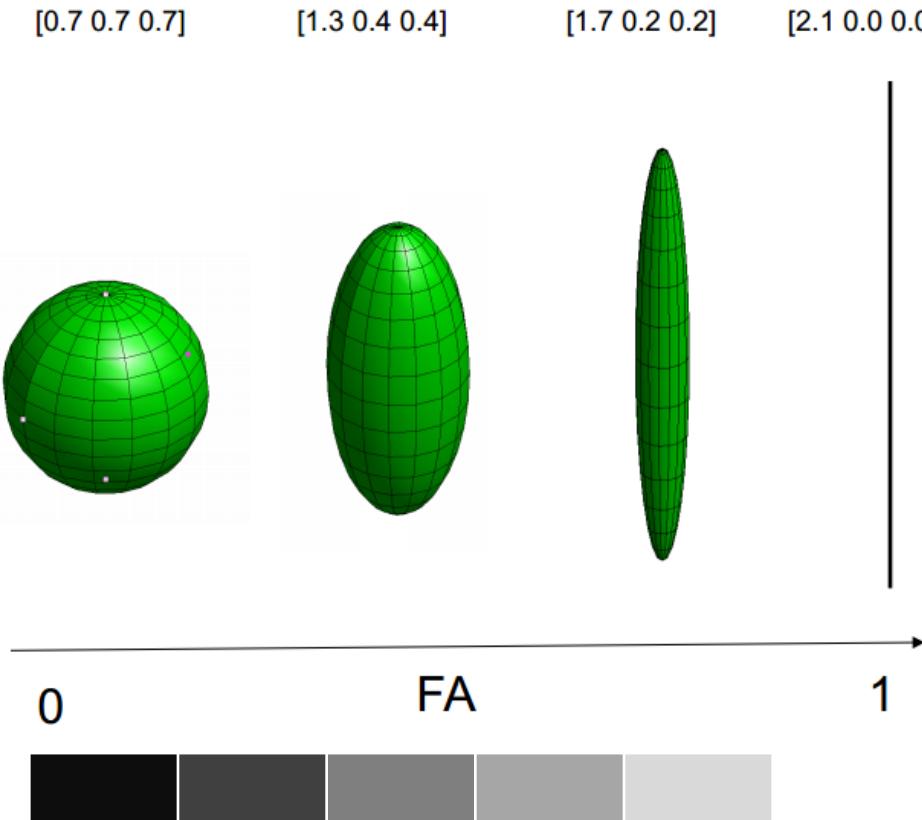


Maps based on different measures of diffusivity:

- Fractional Anisotropy
- Mean Diffusivity

# Fractional Anisotropy

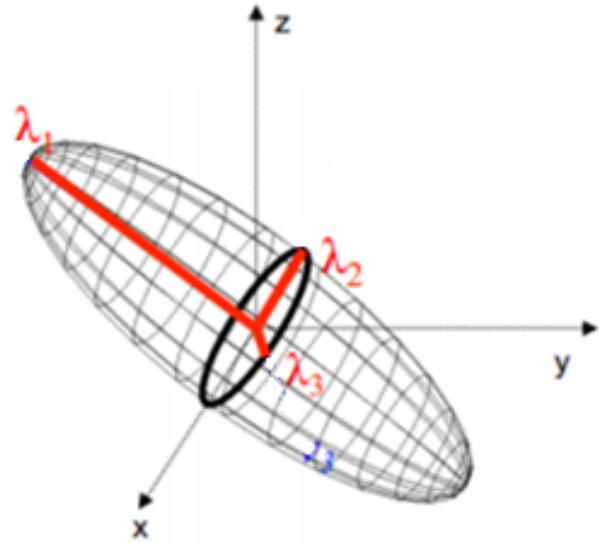
Eigenvalues' variance



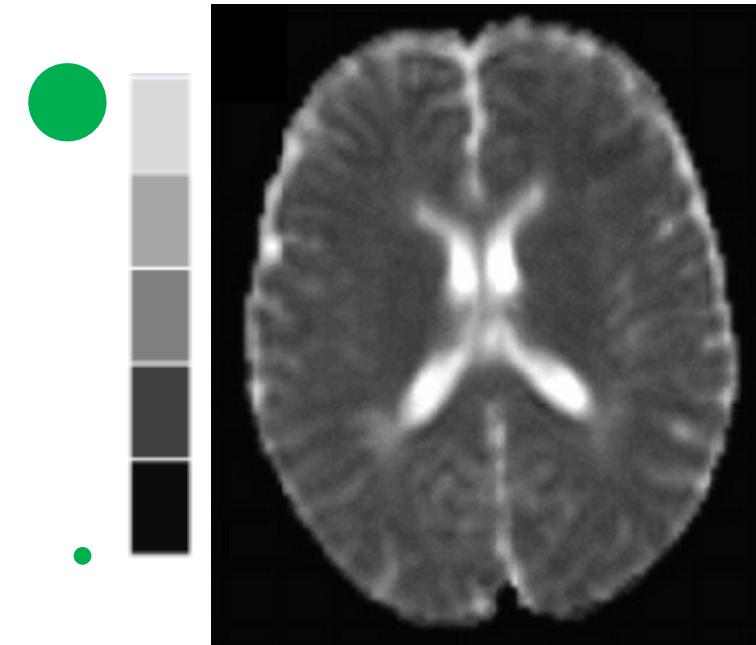
$$FA = \sqrt{\frac{3 \sum_{i=1}^3 (\lambda_i - \bar{\lambda})^2}{2 \sum_{i=1}^3 \lambda_i^2}}, \quad FA \text{ in } [0,1]$$

# Mean Diffusivity

Eigenvalues' mean



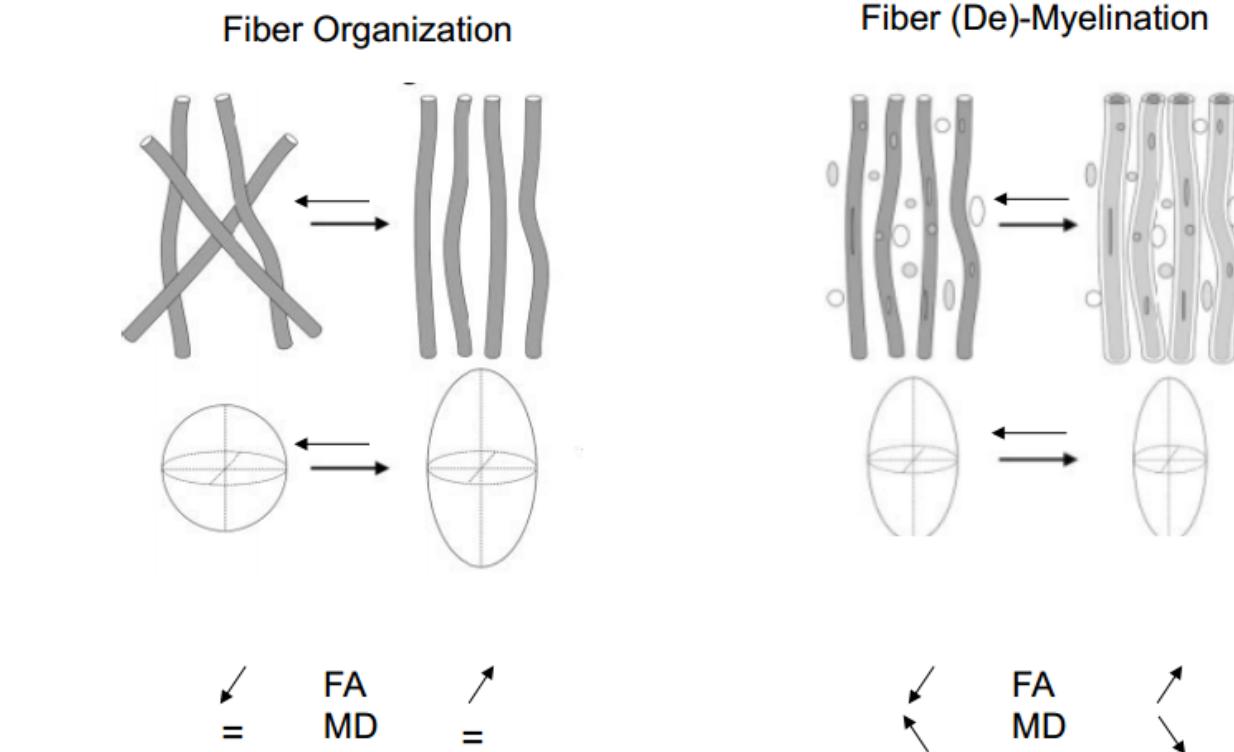
- Average mobility of the tissue.
- The bigger the sphere, the greater the overall diffusion.



$$MD = (\lambda_1 + \lambda_2 + \lambda_3)/3$$

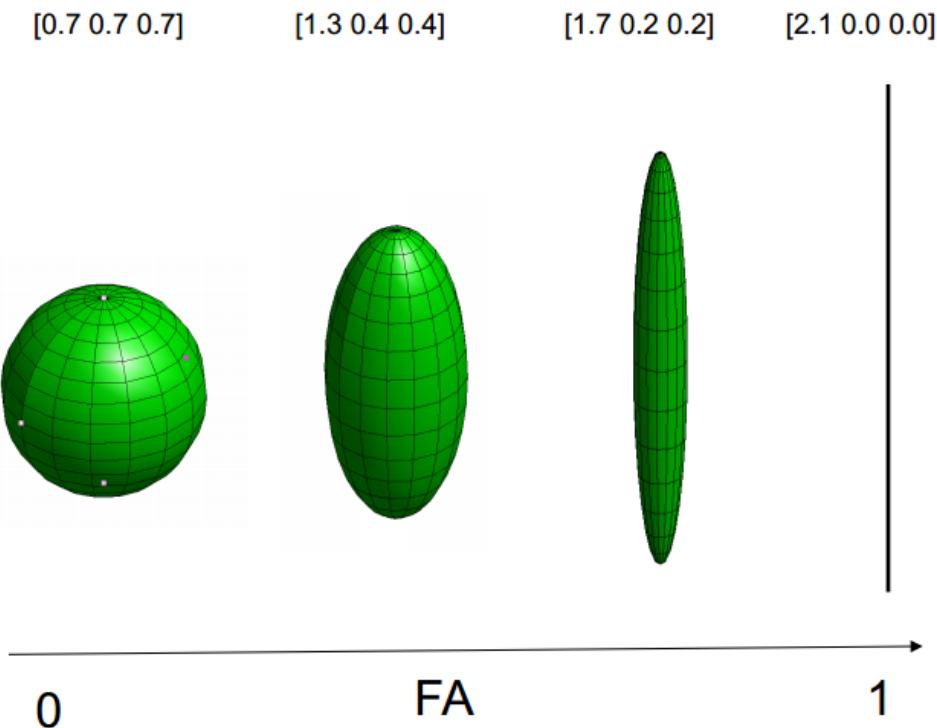
# Different measures provide different information about white matter microstructure

	FA	MD	AD	RD
		$(\lambda_1 + \lambda_2 + \lambda_3)/3$	$\lambda_1$	$(\lambda_2 + \lambda_3)/2$
FA is a summary measure of microstructural integrity. While FA is highly sensitive to microstructural changes, it is less specific to the type of change.	MD is an inverse measure of the membrane density, is very similar for both GM and WM and higher for CSF. MD is sensitive to cellularity, edema, and necrosis.	AD tends to be variable in WM changes and pathology. In axonal injury AD decreases. The ADs of WM tracts have been reported to increase with brain maturation.	RD increases in WM with de- or dys-myelination. Changes in the axonal diameters or density may also influence RD.	
Gray Matter	↓	—	↓	↑
White Matter	↑	—	↑	↓
CSF	↓	↑	↑	↑
High myelination	↑	↓	—	↓
Dense axonal packing	↑	↓	—	↓
WM Maturation	↑	↓	↑	↓
Axonal degeneration	↓	↑	↓	↑
Demyelination	↓	↑	—	↑
Low SNR	↓	↑	↓	—



J.Dubois et al Human Brain Mapping 29:14–27 (2008)

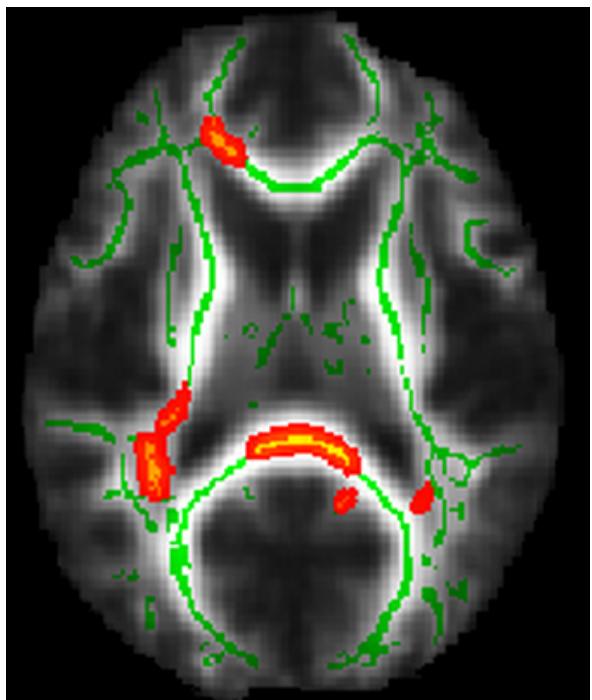
# Which ellipsoid has the greatest MD?



.....they all have the same MD!

# Whole brain vs ROI measures

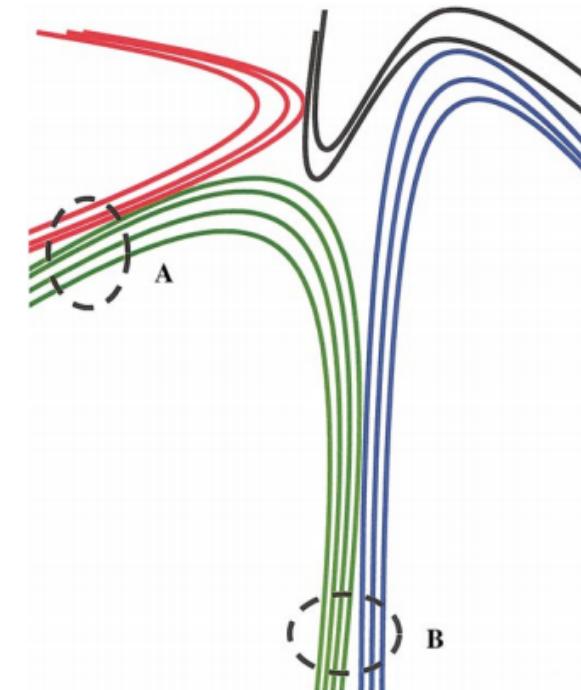
- Whole brain TBSS



(Smith et al., 2006)

<http://fsl.fmrib.ox.ac.uk/fsl/fsl4.0/tbss/index>

- ROI tractography

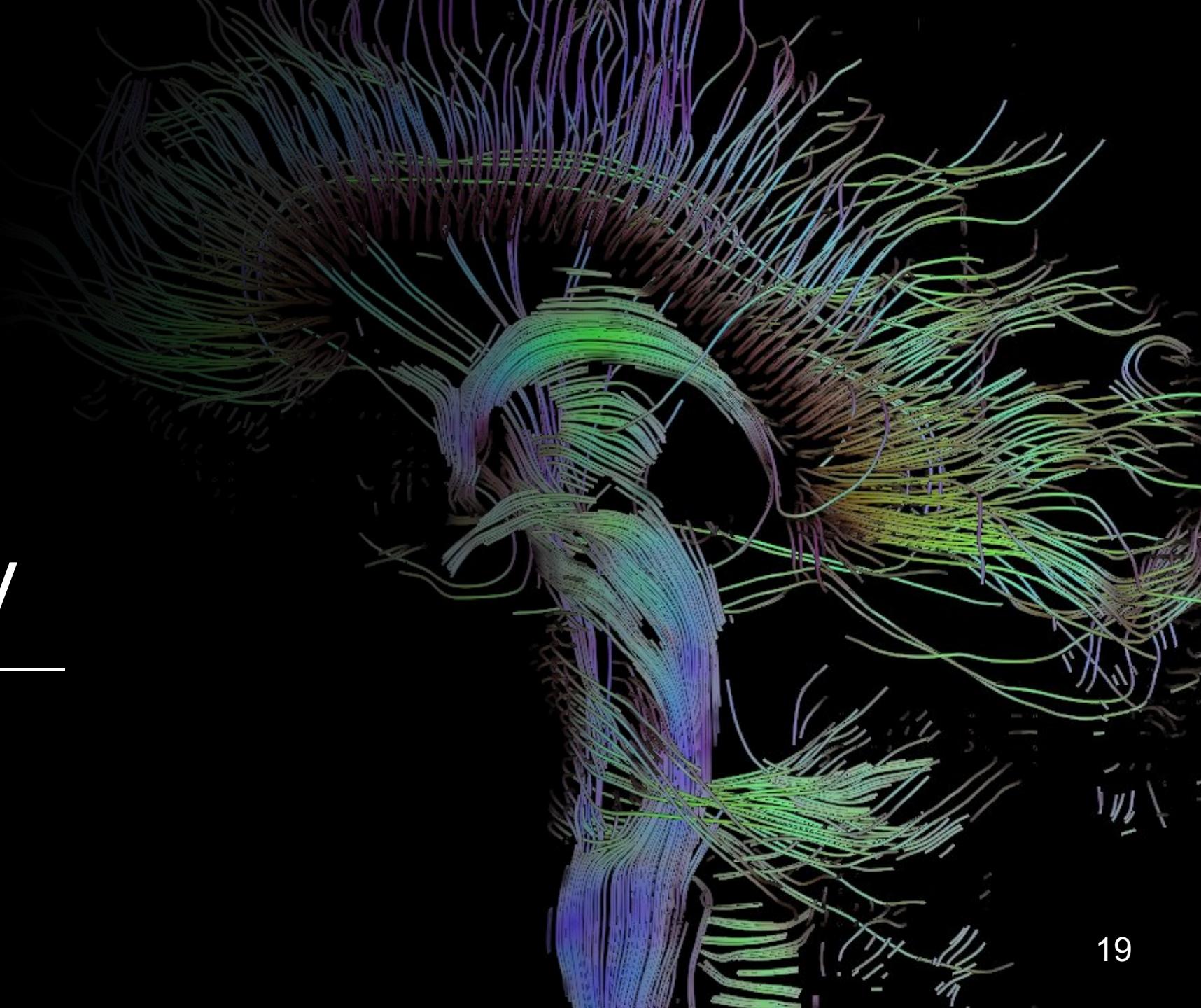


(Catani et al., 2002)



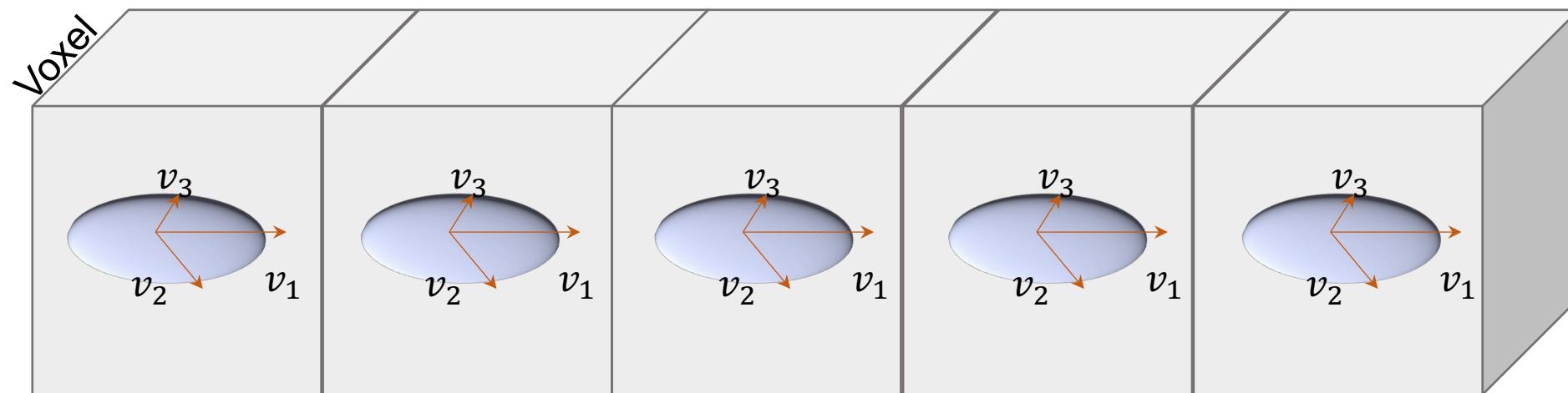
# Tractography

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# Tractography

Indirect reconstruction of the white matter anatomy based on the diffusion of water molecules



Assumption:  
Main eigenvalue tangential to the white matter trajectory  
(Mori et al., 1999)



Streamline

# There are limitations!

1

Stopping rules	
FA thresholds	Curvature
< 0.2 FA	>45 degrees

2

Data quality	
SNR	Spatial resolution

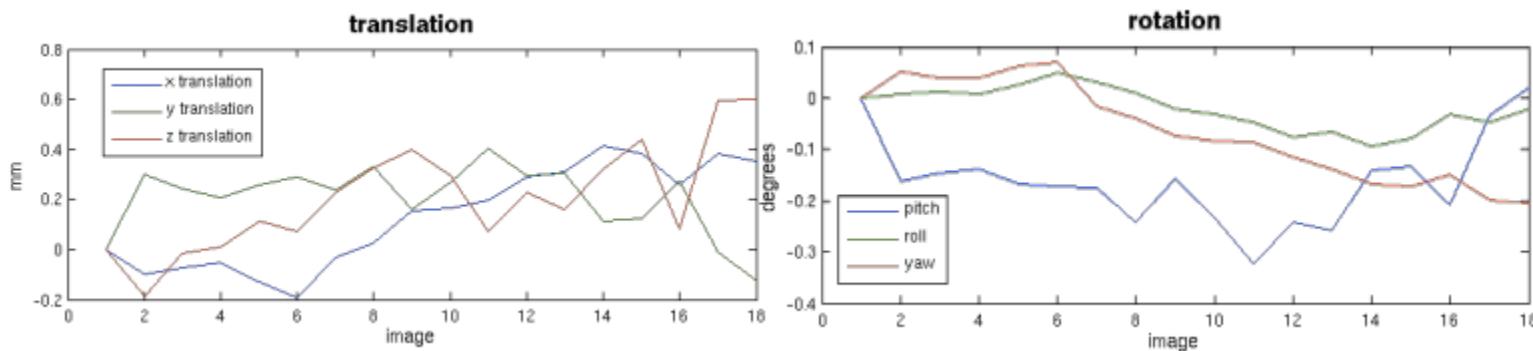
3

Model limitations	
Partial Volume	Crossing
bending	kissing

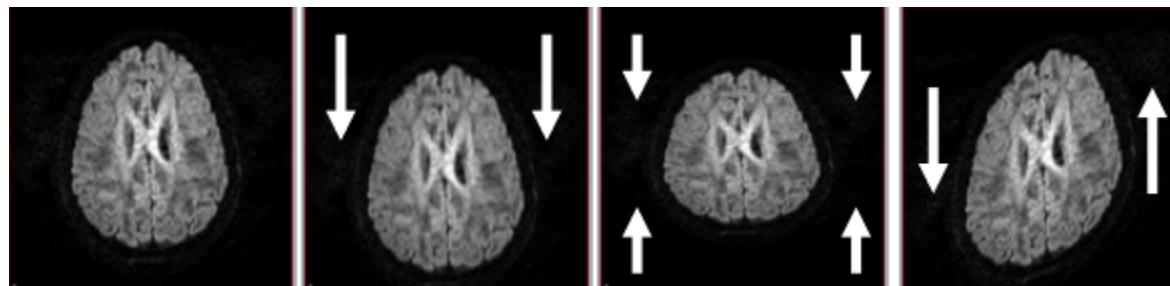


# Data quality is essential!

- Head motion

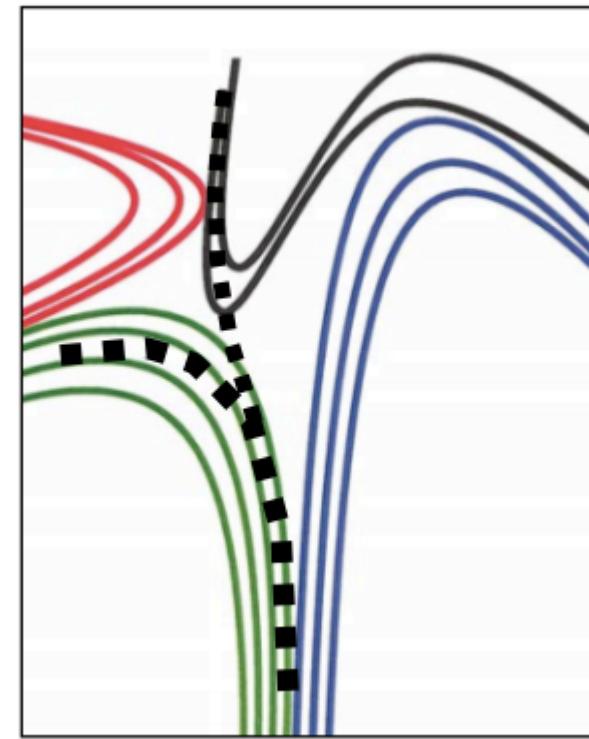
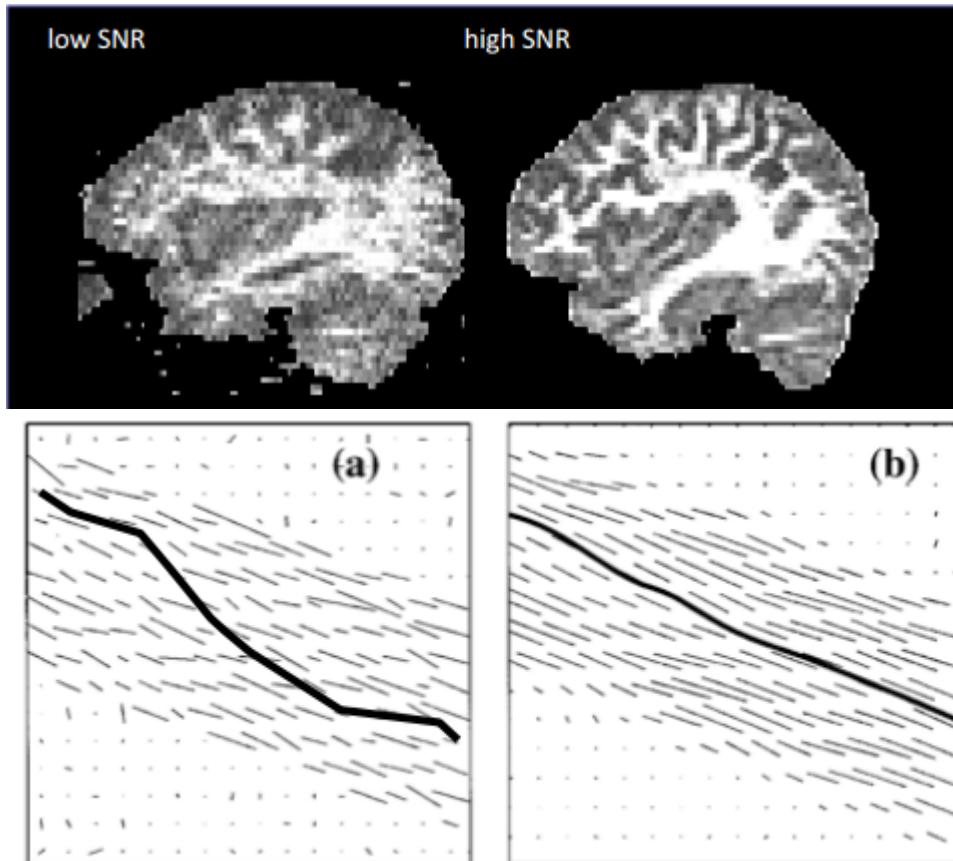


- Eddy current distortion



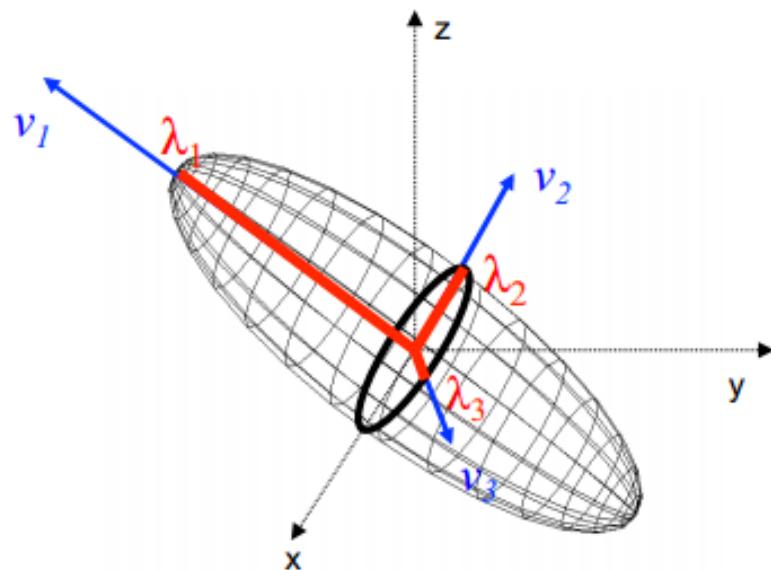
## 2

# Data quality



SNR  
↓  
Trajectory estimation accuracy

# Model limitations

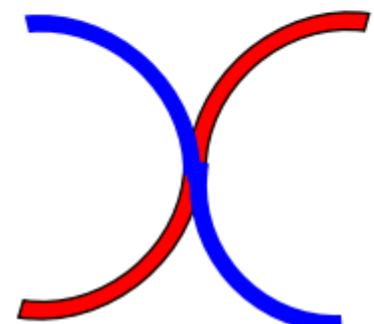
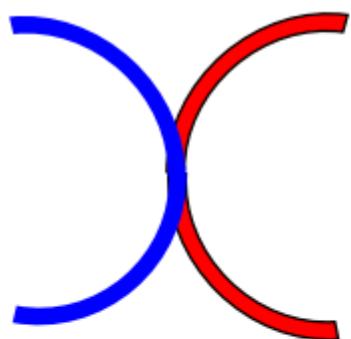


Diffusivity based on 3 Eigenvalues ( $\lambda_1, \lambda_2, \lambda_3$ )

- Compact Description
- Oversimplified Description

# Model limitations

“Real” Fibres



Kissing

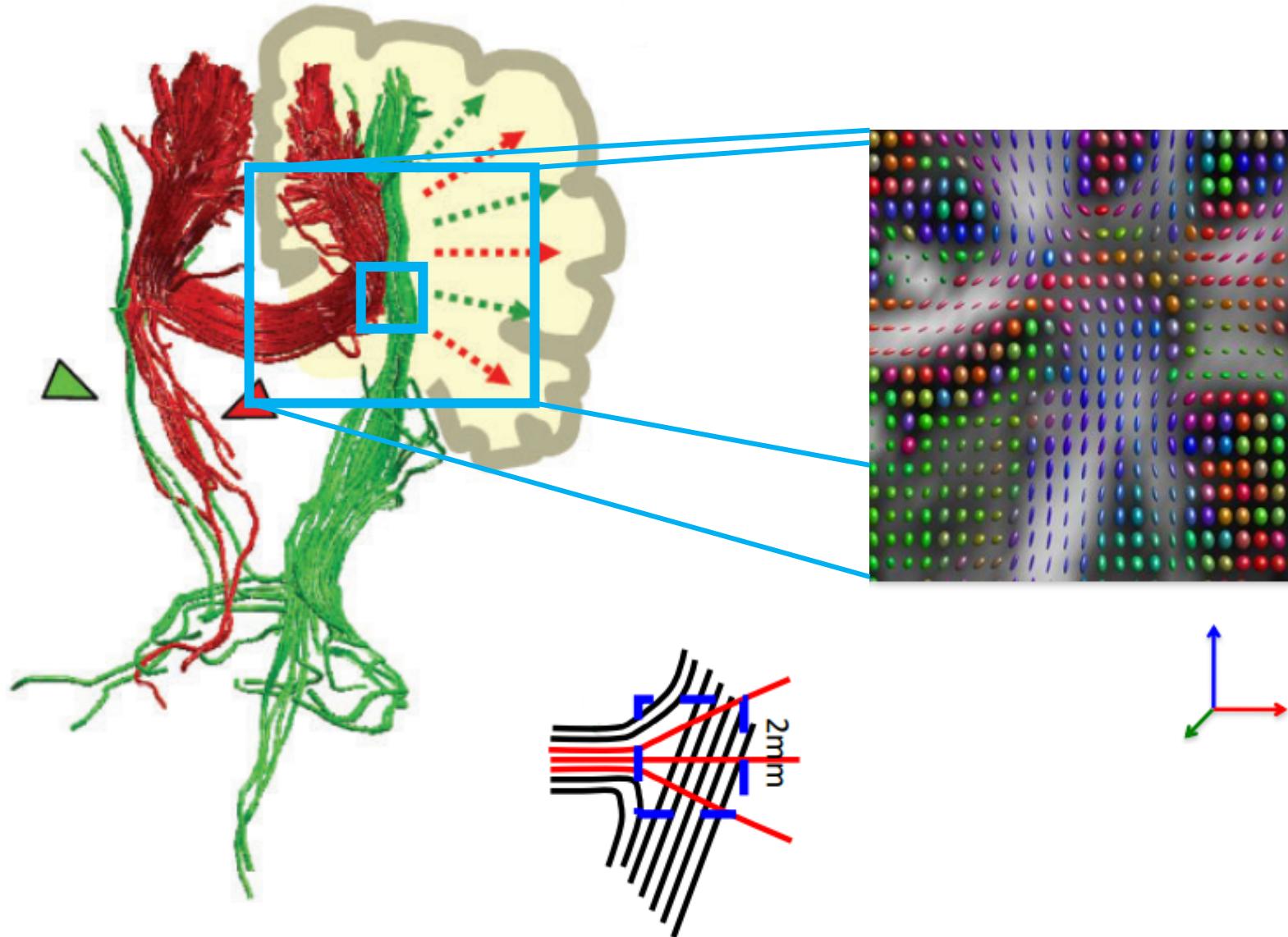
Crossing

...with Diffusion MRI



3

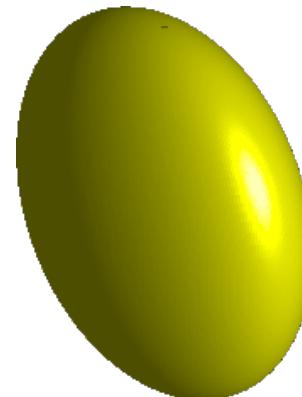
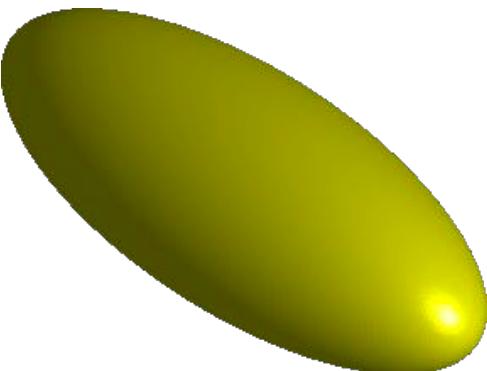
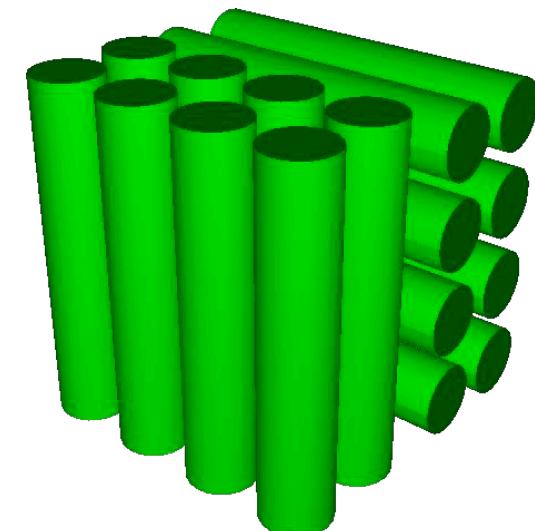
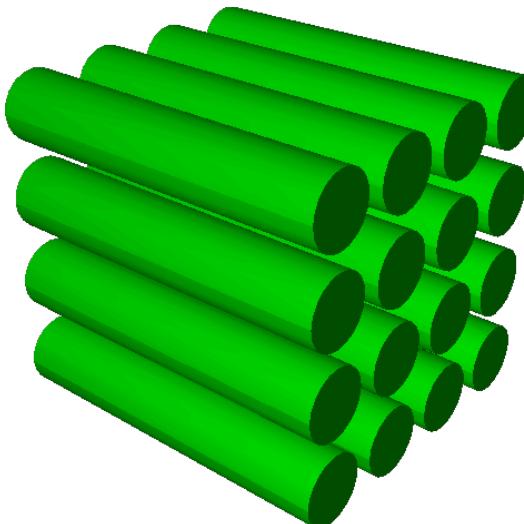
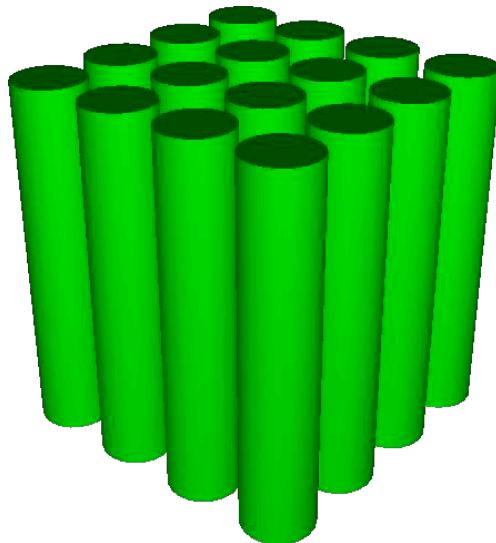
# Model limitations



**CROSSING  
FIBERS...**

# Crossing fibers

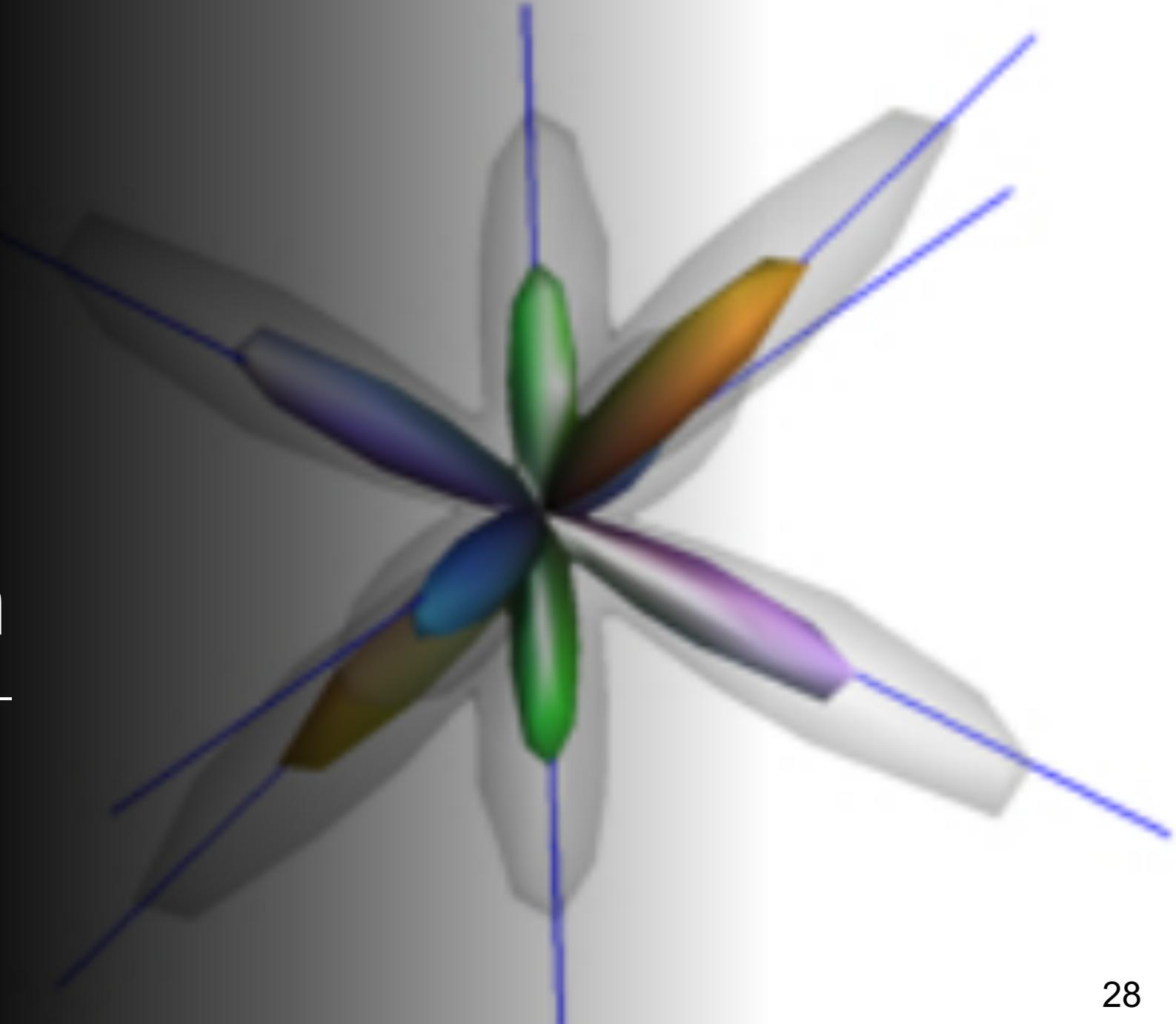
# How to address the problem?



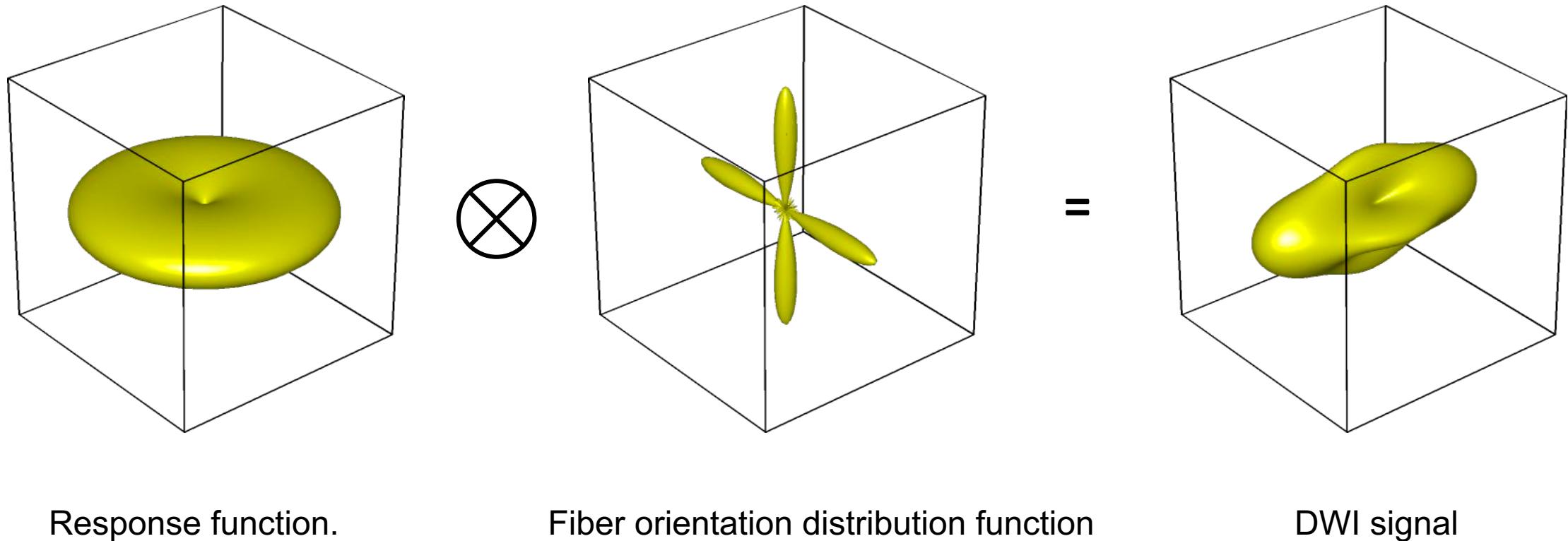


# Spherical Deconvolution

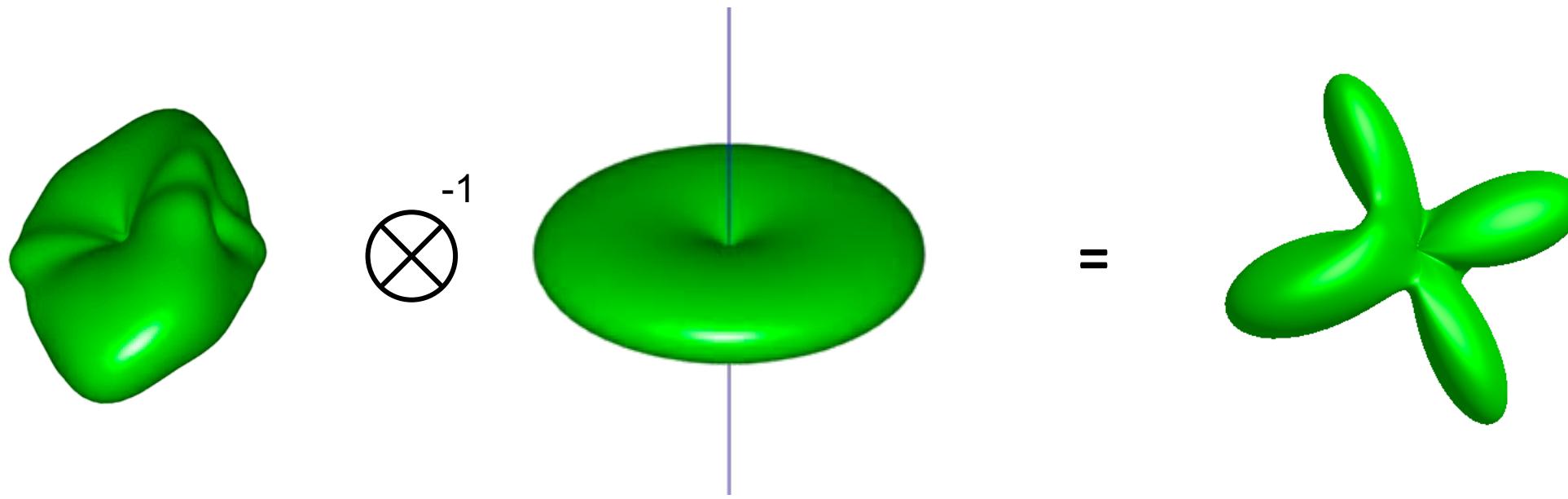
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# Convolution



# Deconvolution

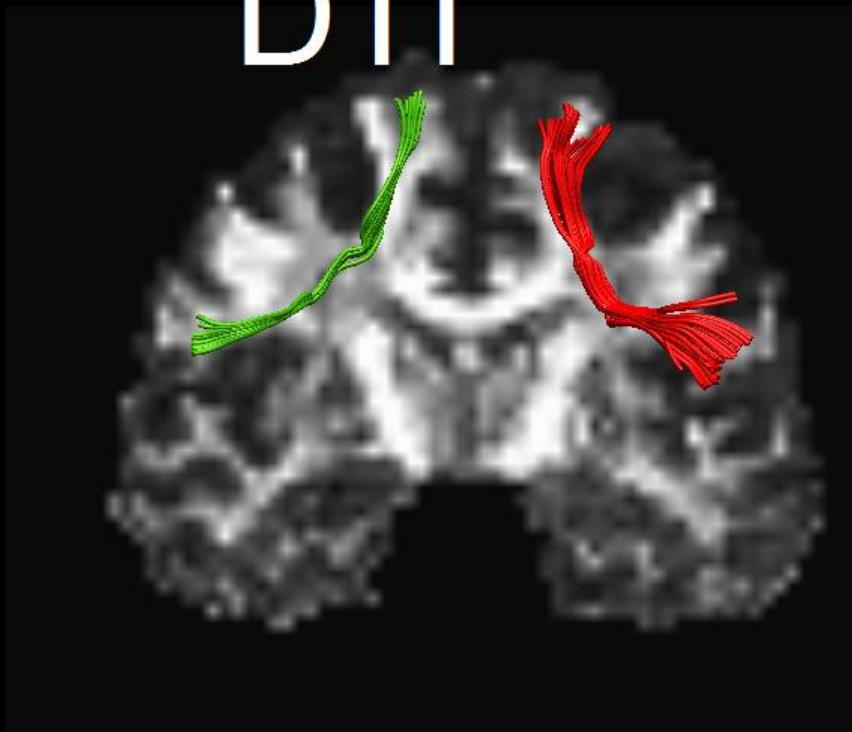


DWI signal

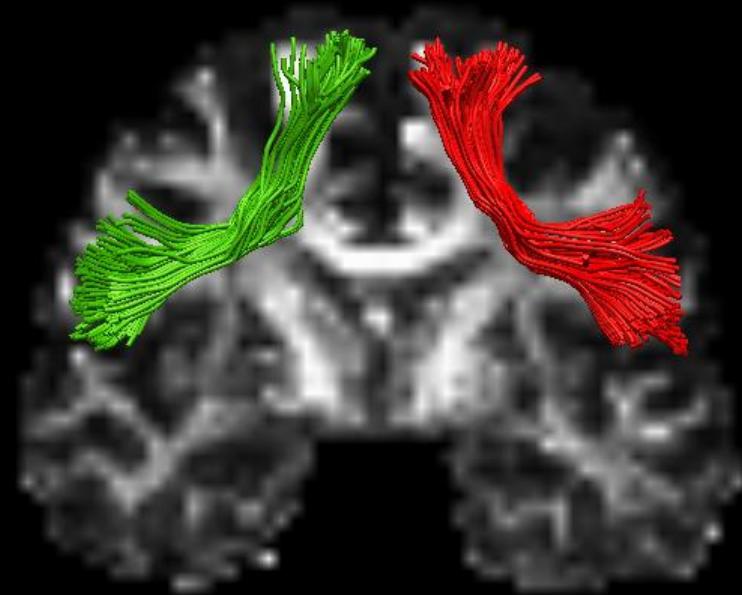
Response function.

Fiber orientation distribution function

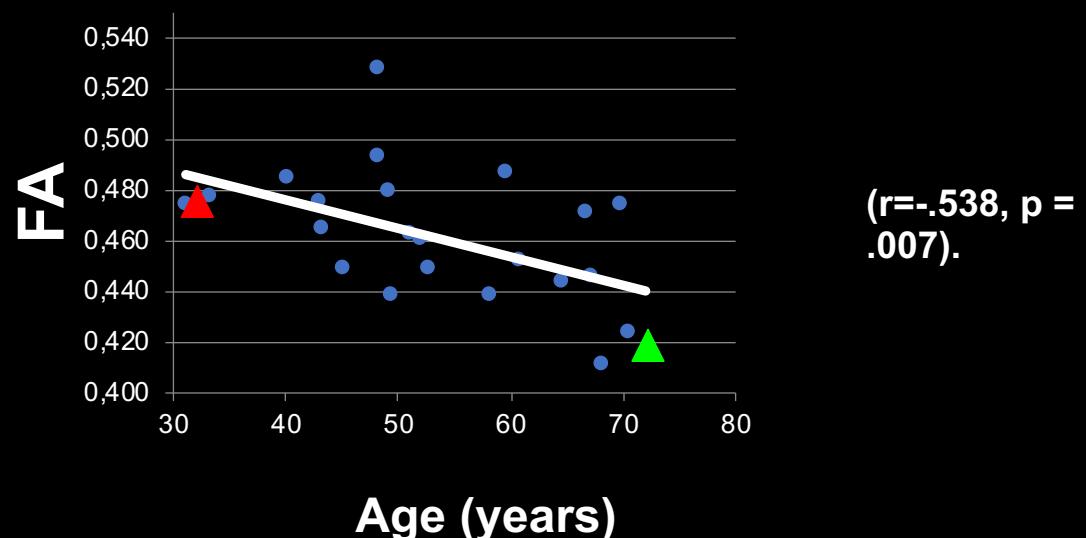
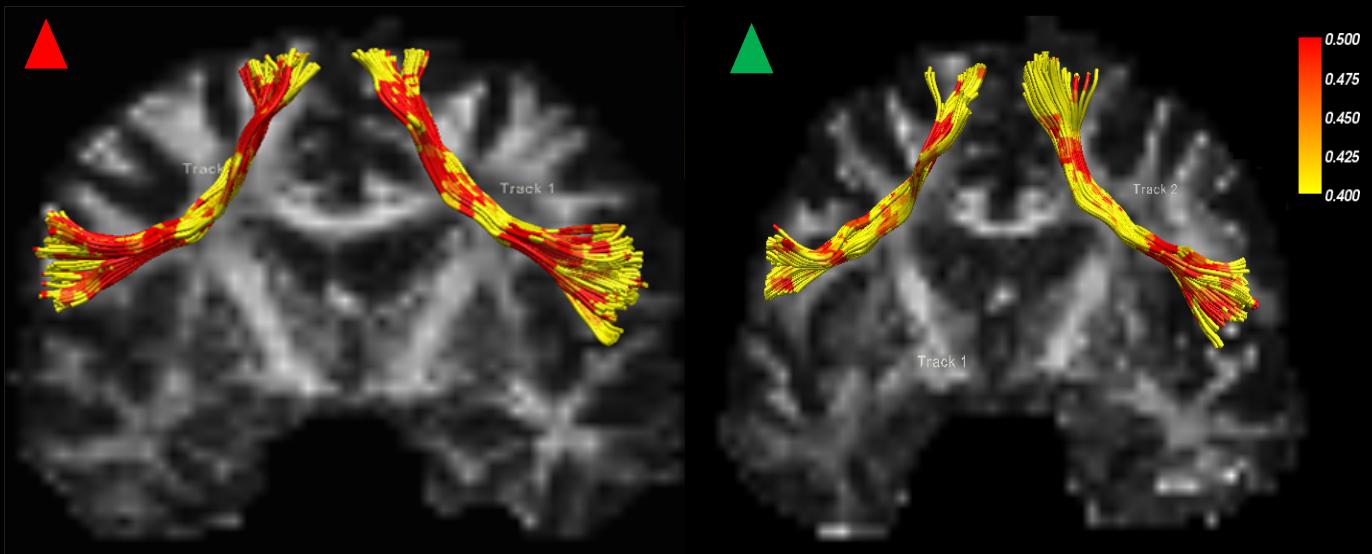
DTI



SD



# Application?



# Questions?

With thanks to Richard Daws and Amy Jolly for help with slides