CFD Simulation and Validation of a Redesigned Paediatric Inhaler Spacer

GROUP: HEALTHCARE 1

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Project Brief

Background:

• Computational Fluid Dynamics is carried out to explore the trajectory of drug particles from the inhaler to the throat. This is performed on a pressurised metered-dose inhaler targeted towards children.

Aims:

- Evaluate the effect of changing the size/shape of the inhaler spacer.
- Analyse the efficiency of the inhaler through the particles that travel to the throat.

Inhaler Spacers and Asthma.

- Metered-Dose Inhaler's (MDIs) are a way of providing a standardized dose of medication during an asthma attack.
- The medicine is typically a corticosteroid or bronchodilator and is absorbed via the lungs.
- A spacer improves the efficiency of the MDI by reducing the amount of medicine wasted in the throat and mouth.
- Spacers do require constant cleaning, with soap and water and there is a misunderstanding regarding the target audience for a spacer – any age can benefit from them.

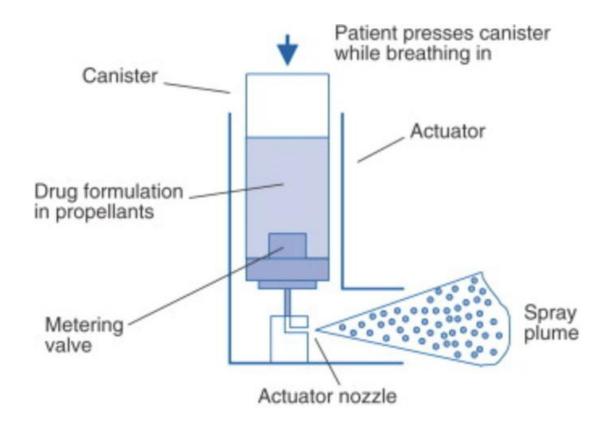


Figure 1: Pediatric Inhaler Delivery

Geometry of Initial Design of Inhaler Spacer



Dimensions	Value
Length of Spacer	119 mm
Spacer Diameter	48 mm
Mask Insertion Diameter	24 mm

Geometry of Initial Design



Geometry of Redesigns

Design 1 – Tapered Spacer (Skyler)



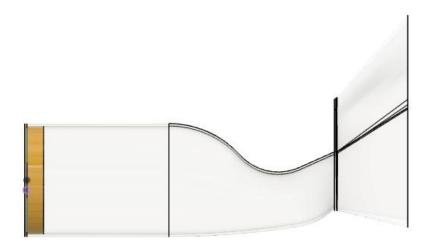
Design 2 – Pear-shaped Spacer (Brandon)



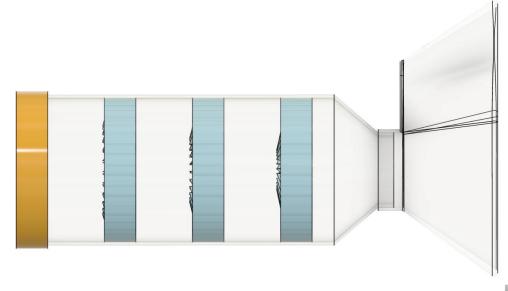


Geometry of Redesigns

Design 3 – Inclined Outlet Spacer (Diljit)



Design 4 – Internal Guide Vanes Spacer (Harkirat)





Concept for Redesign 4

Design is inspired by: Stator blades in turbine jet engines

Usually act to diffuse air, however in some cases they can act as compressors

The geometry of the compressive ring is loosely based on two diagrams below

- Key points:
 - Curved blade > Straight Blade
 - Equally spaced thin blades

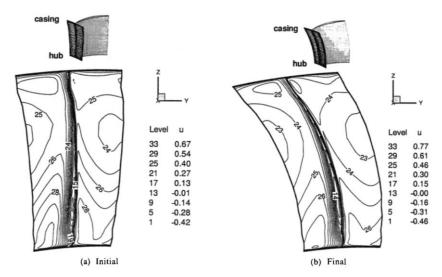


Figure 2: Initial and final designs for a stator blade (Lee S.Y and Kim K.Y, 2000)

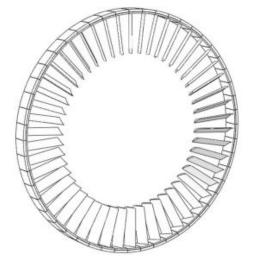
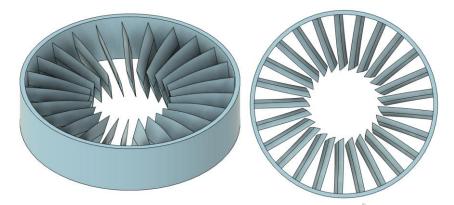


Figure 3: Full circle compressor stator blade ring model (Ma J, Liu Z, Zhang D and Xie Y, 2023)



Mouth Anatomy

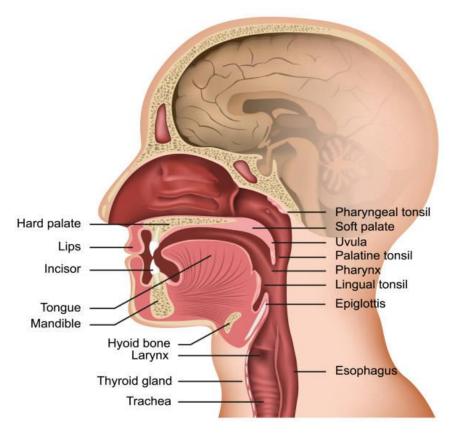
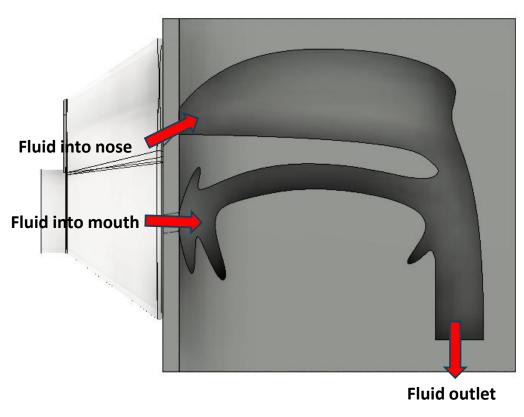


Figure 5: Mouth and Tongue Anatomy



Direction of Fluid Into and Out of the Cavity of Mouth and Nose.

Regulations

- The National Institute for Health and Care Excellence (NICE) guideline emphasises the importance of using Pressure Metered Dose Inhalers with a spacer device for young children.
- They also highlight the need to select the right device to ensure consistent drug dosing.



Fluid and Material Properties

• Due to insufficient information around the properties of salbutamol except density, air properties from Ansys Fluent are used to replace the missing ones.

Property	Salbutamol / Air
Density	1.07 kg/m ³
Specific Heat	1006.43 J/kgK
Thermal Conductivity	0.0242 W/mK
Dynamic Viscosity	1.7894 x 10 ⁻⁵ kg/ms

Property	Polycarbonate
Density	63.987 kg/m ³
Specific Heat	1198.5
Thermal Conductivity	0.034606 W/mK



Governing Equations

• Assuming that density is constant: $\nabla \cdot (\rho \vec{v}) \equiv \rho \nabla \cdot \vec{v} + \vec{v} \cdot \nabla \rho$

• Assuming that momentum is constant:
$$x$$
-component: $\frac{\partial(\rho u)}{\partial t} + V \cdot (\rho u \vec{V}) = -\frac{\partial p}{\partial x} + \frac{\partial \tau_{xx}}{\partial x} + \frac{\partial \tau_{yx}}{\partial y} + \frac{\partial \tau_{zx}}{\partial z} + \rho f_x$

y-component:
$$\frac{\partial(\rho v)}{\partial t} + \nabla \cdot (\rho v \vec{V}) = -\frac{\partial p}{\partial y} + \frac{\partial \tau_{xy}}{\partial x} + \frac{\partial \tau_{yy}}{\partial y} + \frac{\partial \tau_{zy}}{\partial z} + \rho f_y$$

z-component:
$$\frac{\partial(\rho w)}{\partial t} + \nabla \cdot (\rho w \vec{V}) = -\frac{\partial p}{\partial z} + \frac{\partial \tau_{xz}}{\partial x} + \frac{\partial \tau_{yz}}{\partial y} + \frac{\partial \tau_{zz}}{\partial z} + \rho f_z$$

• Energy is conserved:

$$\begin{split} &\frac{\partial}{\partial t} \left[\rho \left(e + \frac{V^2}{2} \right) \right] + V \cdot \left[\rho \left(e + \frac{V^2}{2} \right) \vec{V} \right] \\ &= \rho \dot{q} + \frac{\partial}{\partial x} \left(k \frac{\partial T}{\partial x} \right) + \frac{\partial}{\partial y} \left(k \frac{\partial T}{\partial y} \right) \\ &+ \frac{\partial}{\partial z} \left(k \frac{\partial T}{\partial z} \right) - \frac{\partial (up)}{\partial x} - \frac{\partial (vp)}{\partial y} - \frac{\partial (wp)}{\partial z} + \frac{\partial (u\tau_{xx})}{\partial x} \\ &+ \frac{\partial (u\tau_{yx})}{\partial y} + \frac{\partial (u\tau_{zx})}{\partial z} + \frac{\partial (v\tau_{xy})}{\partial x} + \frac{\partial (v\tau_{yy})}{\partial y} \\ &+ \frac{\partial (v\tau_{zy})}{\partial z} + \frac{\partial (w\tau_{xz})}{\partial x} + \frac{\partial (w\tau_{yz})}{\partial y} + \frac{\partial (w\tau_{zz})}{\partial z} + \rho \vec{f} \cdot \vec{V} \end{split}$$



Governing Equations

Computational approach: Reynolds-Averaged Navier Stokes (RANS) with k-epsilon model.

Navier-Stokes –Body and Surface forces present:

$$-\rho\left(\frac{D\vec{v}}{Dt}\right) = \rho\nabla\Phi + \nabla p + \eta\nabla^2\vec{v} \qquad \qquad \frac{D}{Dt} \equiv \frac{\partial}{\partial t} + (\vec{v}\cdot\nabla)$$

• Turbulence – For internal flow: $Re \ge 2300$

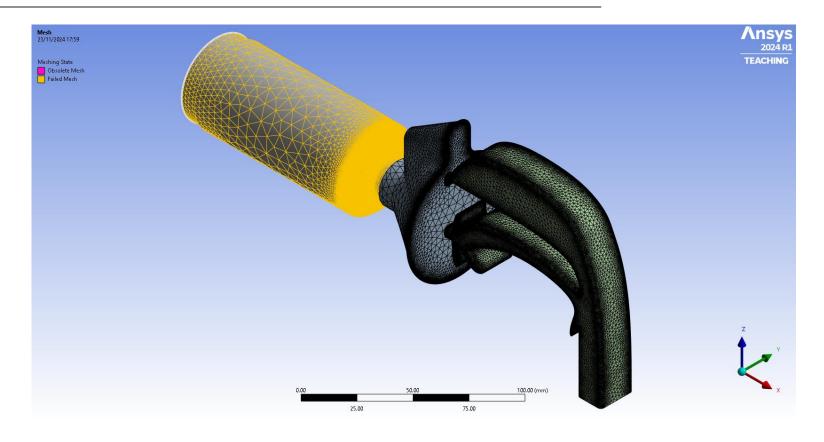
•
$$Re_{Salbutamol/Air} = \frac{\rho uL}{\mu} = \frac{1.07 \times 1.724 \times 119 \times 10^{-3}}{1.7894 \times 10^{-5}} = 12269$$



Default Mesh for Initial design

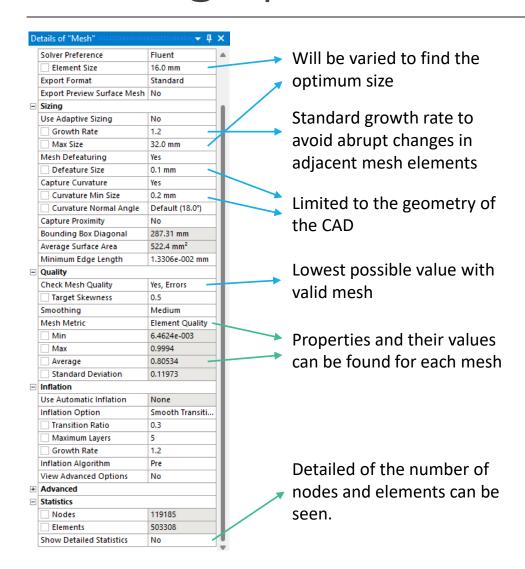
The default meshing option is inadequate:

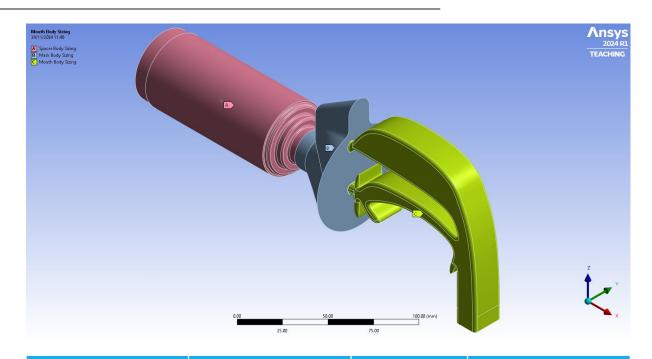
- High number of Elements
- The Mesh fails



Mesh Size (mm)	Number of Elements	Aspect Ratio	Skewness	Orthogonal Quality	Element Quality
Default	1,141,767	1.9014	0.2419	0.7568	0.8274

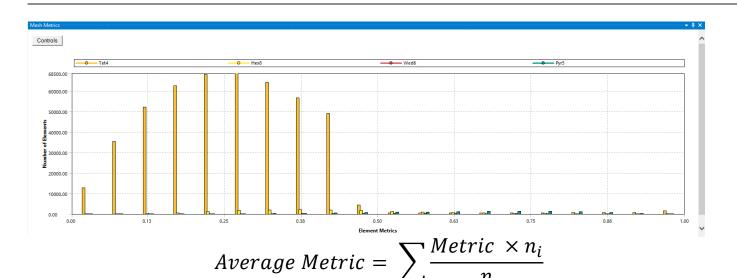
Finding optimum Mesh Size – Method

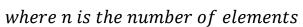




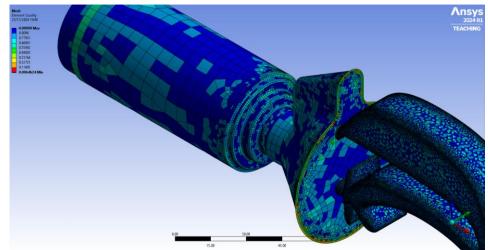
Location	Mesh Method	Defeature size	Local Minimum Size
Spacer Volume	Hex Dominant	0.75 mm	1.2 mm
Mask Volume	Hex Dominant	0.5 mm	0.8 ram
Mouth Volume	Patch Conforming	0.3 mm	0.5 mm

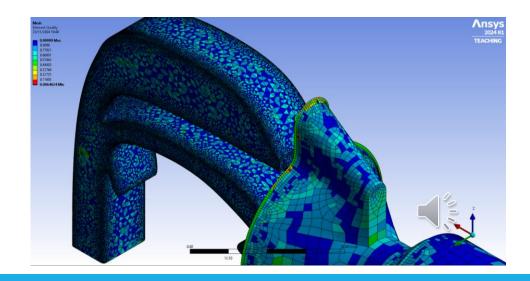
Varying Mesh Size for Initial Design

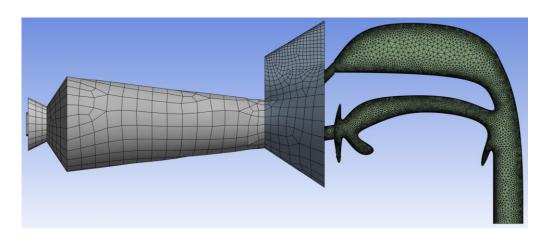


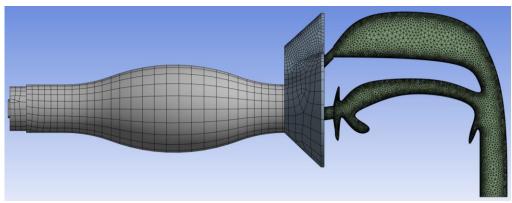


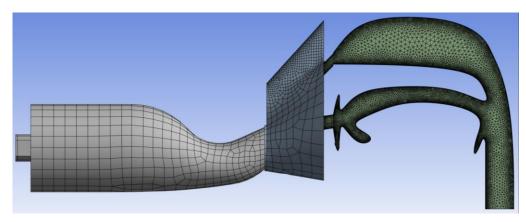
Mesh Size (mm)	Number of Elements	Aspect Ratio	Skewness	Orthogonal Quality	Element Quality
16	503,308	2.0772	0.2730	0.7334	0.8053
12	503,456	2.1290	0.2747	0.7318	0.8042
8	503,813	2.0613	0.2731	0.7331	0.8056
4	507,966	2.1024	0.2742	0.7334	0.8030

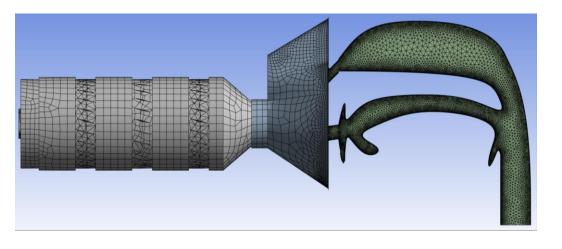








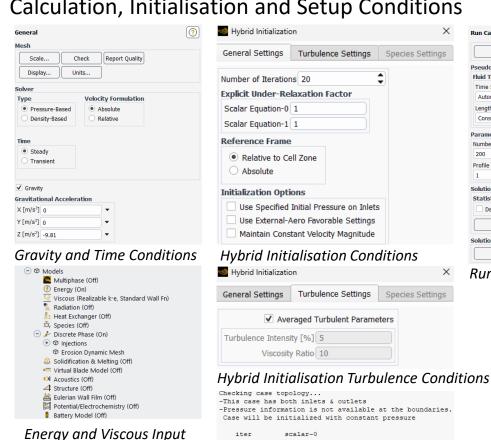




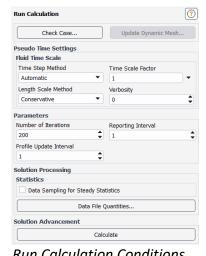
Design	Number of Elements	Aspect Ratio	Skewness	Orthogonal Quality	Element Quality
Tapered	481,829	1.9265	0.25776	0.74292	0.81704
Pear Shape	486,293	1.9434	0.25948	0.74178	0.81528
Inclined Outlet	488,125	1.9409	0.25942	0.74207	0.81565
Guide Vanes	508,911	2.2861	0.27787	0.72855	0.80159



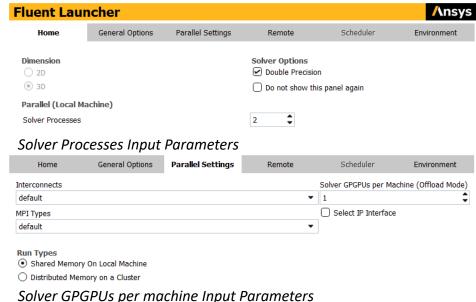
Calculation, Initialisation and Setup Conditions

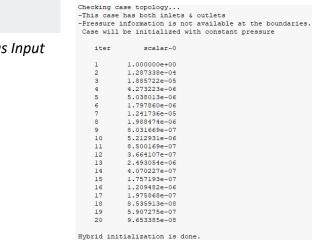


Parameters



Run Calculation Conditions





Hybrid Initialisation Iterations

Boundary Conditions

Inlet Conditions			
Velocity Magnitude (m/s)	1.724		
Specification Method	Intensity and Viscosity Ratio		
Turbulent Intensity (%)	5		
Turbulent Viscosity Ratio	10		
Temperature (°C)	25		
Discrete Phase Type	Escape		

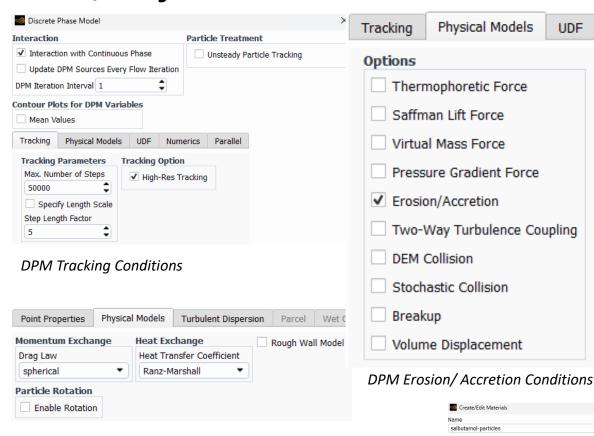
Outlet Conditions			
Backflow Reference Frame	Absolute		
Gauge Pressure (Pa)	0		
Specification Method	Intensity and Viscosity Ratio		
Turbulent Intensity (%)	5		
Turbulent Viscosity Ratio	10		
Backflow Total Temp (°C)	25		
Discrete Phase Type	Escape		

Wall Conditions			
Wall Motion	Stationary		
Shear Condition	No Slip		
Roughness Model	Standard		
Roughness Height (m)	0		
Roughness Constant	0.5		
Temperature (°C)	25		
Discrete Phase Type	Trap		

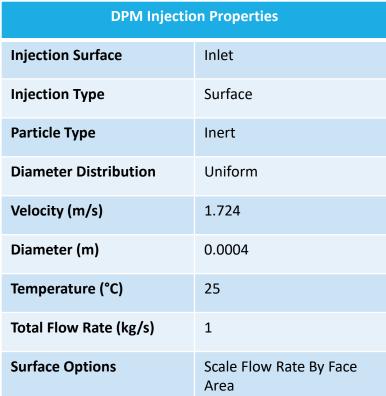
Average number of breaths for 3-5 year olds = 28 breaths per minute Inspiratory Flow Rate for 2-12 year olds $(Q_1)=30\frac{L}{min}=0.0005\frac{m^3}{s}$ Inlet Area of Spacer $(A_1)=0.00029$ m^2 Inlet Velocity = $\frac{Q_1}{A_1}=\frac{0.0005}{0.00029}=1.724\frac{m}{s}$



DPM/Injection Conditions



DPM Physical Model Conditions



Point Properties Physical Models Turbulent Dispersion

Stochastic Tracking

Dispersion Model

discrete-random-walk ▼

Random Eddy Lifetime

Number of Tries

5

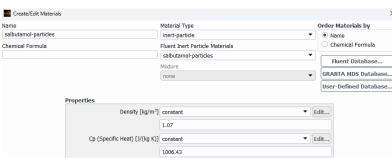
Time Scale Constant

0.15

Length Scale Constant

0.72

DPM Turbulence Conditions

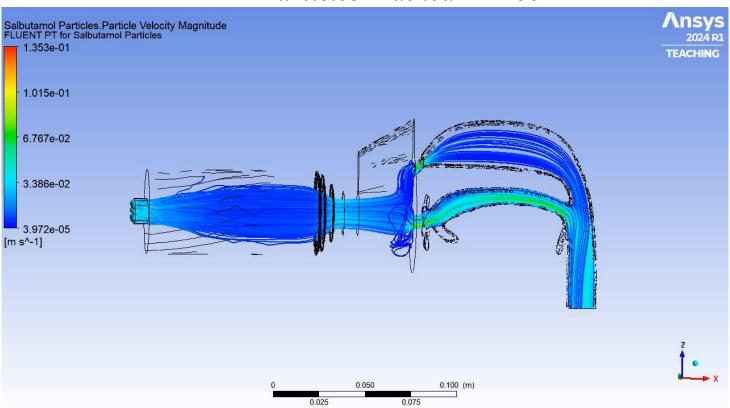


Salbutamol Injection Material Properties



Initial Design Result

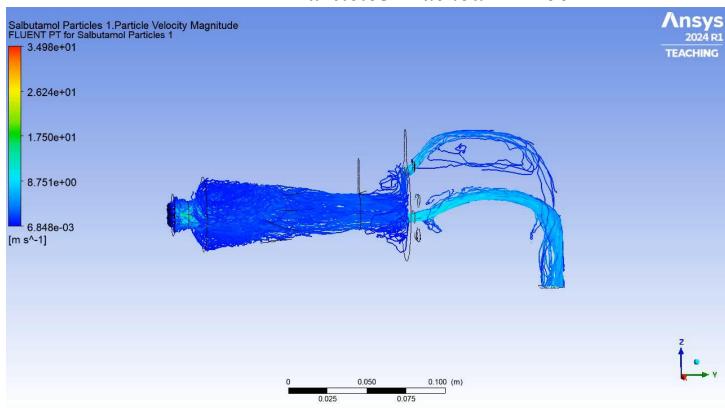
$$Efficiency of Spacer = \frac{Particles Escaped}{Particles Tracked} = \frac{562}{1200} = 46.83\%$$





Tapered Spacer Result

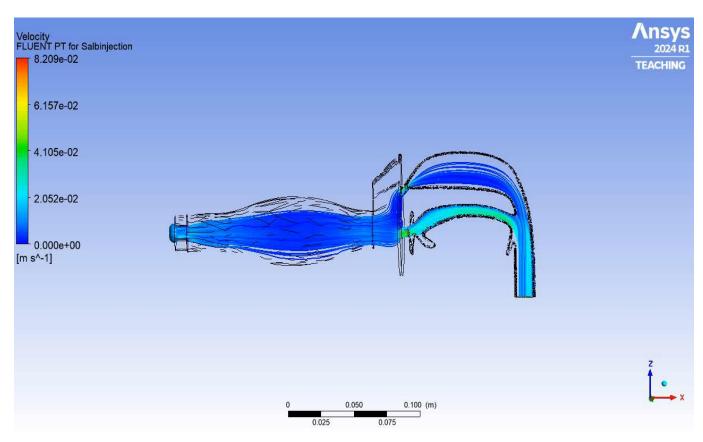
$$Efficiency of Spacer = \frac{Particles Escaped}{Particles Tracked} = \frac{2109}{4400} = 47.93\%$$





Pear-Shaped Spacer Result

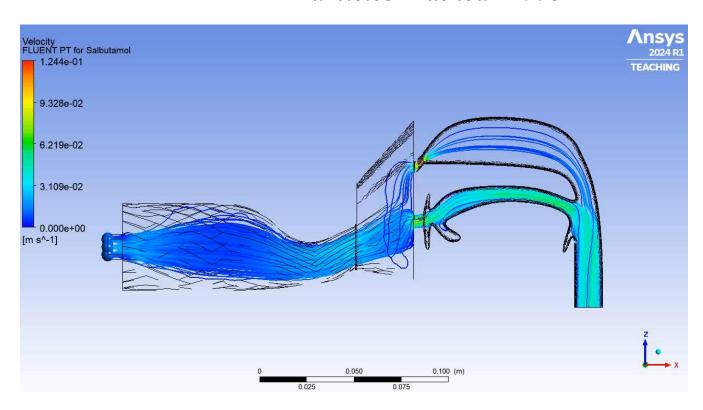
Efficiency of Spacer =
$$\frac{Particles\ Escaped}{Particles\ Tracked} = \frac{658}{900} = 73.11\%$$





Inclined Outlet Spacer Result

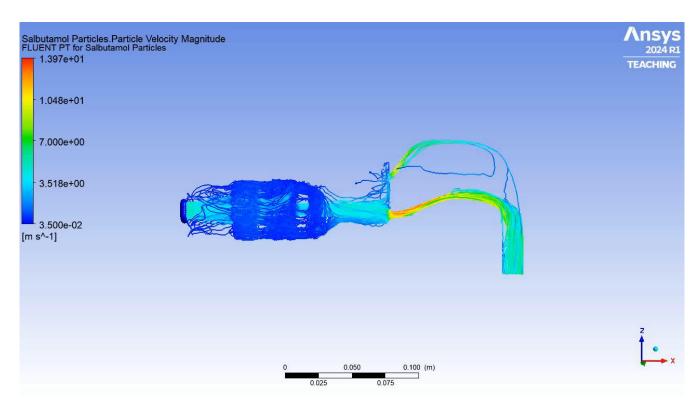
Efficiency of Spacer =
$$\frac{Particles\ Escaped}{Particles\ Tracked} = \frac{686}{990} = 69.29\%$$





Internal Guide Vanes Spacer Result

$$Efficiency \ of \ Spacer = \frac{Particles \ Escaped}{Particles \ Tracked} = \frac{283}{1120} = 25.27\%$$



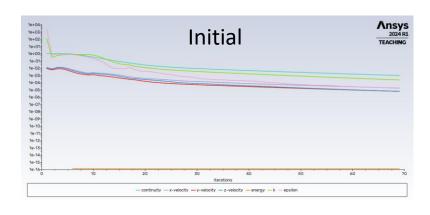


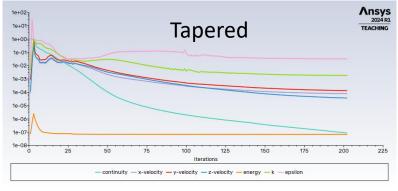
Comparison of Results

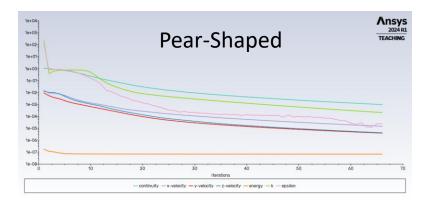
Spacer Type	Tracked Particles	Escaped Particles	Efficiency (%)
Initial	1200	562	46.83
Tapered	4400	2109	47.93
Pear-shaped	900	658	73.11
Inclined Outlet	990	686	69.29
Internal Guide Vanes	1120	283	25.27

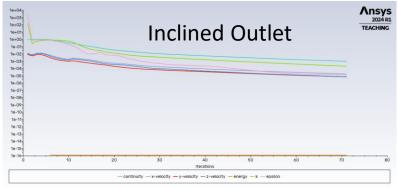


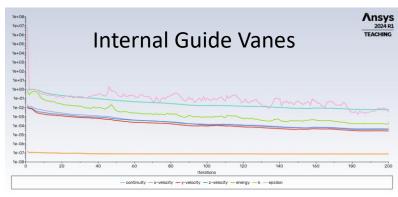
Solver













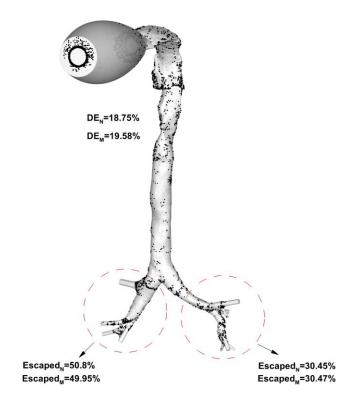
Validation

Advantages:

- Complies with regulations
- •Turbulent model k epsilon
- Mesh Resolution default meshing

Things to Consider:

- Accuracy of human anatomy
- Using transient model instead of steady state
- Material and fluid properties





Limitations of model

- The computational cost of a transient model is too high (simulations take hours or crash). To address this, the model is simplified by choosing the steady-state option.
- The model for the mouth makes simplifications in CAD. We could outsource a more anatomy-correct model.
- The material for the wall boundary was chosen to be "honeycomb polycarbonate plastic" and modelled as smooth. Ideally, the mouth should be another material and have the associated roughness model.
- The fluid properties are mainly accounting for air instead of salbutamol, which slightly affects our efficiency values when solving.

