



Advanced Robot Control and Learning

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Advanced Robot Control - Outline

Differential Geometry in Robotics
Basics of Task Space Modeling and Control
Redundant Robots
Modern Methods of Robot Control
Port-Hamiltonian Systems in Robotics
Linear Parametrization and Identification of Robot Dynamics

Bio-Inspired Robot Control

- Bio-Inspired Formulation
- Adaptive Impedance Control for a Manipulator





Chapter 7: Bio-Inspired Robot Control



Bio-Inspired Formulation





Motivation

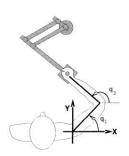
- Unlike animals, humans take a long while to learn to control even basic movements of their body
- But eventually, we learn to do sophisticated movements
 (e.g. dealing with novel environments such as steep ski slopes!)

But, how can human adapt to these environments?

→ Experimental research on Neuromechanics and Motor Control

Task (Shadmehr et al 1994):

Reaching movements in presence of external forces imposed from mechanical environment







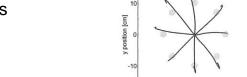
Adaption to Novel Dynamics

Experiments:

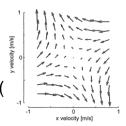
- Point-to-point (PTP) movements on a horizontal plane: Null force field ((figure C: Easy!)
- PTP movements on a horizontal plane under a stable force field: e.g. Velocity-dependent force field (*VF*) (figure D: first trial, figure E: later trials)
- PTP movements on a horizontal plane under VF, then suddenly NF (What would happen?)

Figure F: big trajectory disturbances in the *opposite* direction

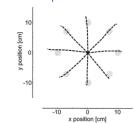
- → subjects learned to compensate for the forces!
- → controller did not just simply stiffen the joints¹ but the learned compensation has feedforward characteristics



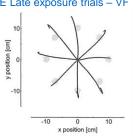
A Velocity dependent force field



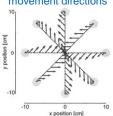
C Pre-exposure trials - NF



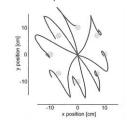
E Late exposure trials - VF



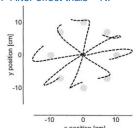
B Forces experienced in the movement directions



D Initial exposure trials - VF



F After effect trials - NF



Shadmehr et al 1994

¹ otherwise straighter movements would occur





Adaption to Novel Dynamics

Experiment: Point-to-point movements on horizontal plane under different VF's (Kinematic error not systematically reduced!)

- → Controller compensates for the approximate mean of the random distribution of the force fields,
- → primarily by the strength of the force field on the most recent trials

Suggested *feedforward* output of the adaptation process²:

$$z^{k+1} = \vartheta z^k + \alpha e^k$$
, $\vartheta, \alpha > 0$

where e^k is the last trial error and z^k is the previously learned output

Consequently, as learning progresses and error is reduced, the feedback sensory signals appear to shift forward in time!

² Known as *autoregressive* adaption model





Motor Learning under Unstable and Unpredictable Conditions

Adaptation to novel stable dynamics ↔ Learning the appropriate feedforward forces for each state

Are all novel environments stable?

Opening a door with high resistance vs. Using a screwdriver (inherently unstable!)

Is instability the only problem? NO!

- Unpredictability
- Unrepeatability

How about noise? (both in perception and action)

- Error in state of the body
- Error in state of the world
- Leading to wrong feedforward command

Noise in opening a door with high resistance vs. in using a screwdriver

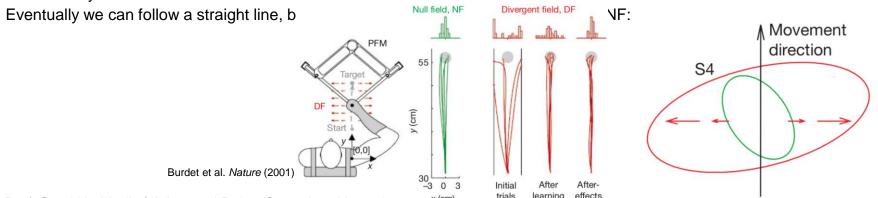


Unstable Interaction

Experiment:

PTP movements on a horizontal plane under an unstable position-dependent divergent force field (DF) of $F_x = K_x x$ and $F_y = 0$, where x is the perpendicular distance to the PTP straight line, F_x and F_y are the forces applied respectively perpendicular and in parallel to the straight line, and K_x is the field constant. (What would happen?)

- Co-contraction will increase the stiffness and viscosity of the joints and consequently the endpoint of limb
- Posture modification will changes the effective mass of the limb and the postural contributions to endpoint stiffness and viscosity







Adapted Impedance

Limb's endpoint impedance is tuned:

- To exactly compensate for the imposed instability → *Scalability*
- In direction of instability → Directionality

Limb's endpoint impedance tuning can be done by:

- Co-contraction: Fast but high metabolic cost (e.g. when someone hits you and your eyes are open)
- Feedback tuning: Slow but low metabolic cost (e.g. when someone hits you and your eyes are closed)





Change of Impedance and Force During Learning

- In both stable and unstable novel environments → An early co-contraction³ in learning
- Unstable force field → Co-contraction decays in a selective manner to final level of sufficient endpoint stiffness
- Stable force field → After compensation for position error, co-contraction will turn to a feedforward torque, leaving the task to the directly responsible muscles



Eventual decrease in energy consumption for both cases

³ known as wasted contraction



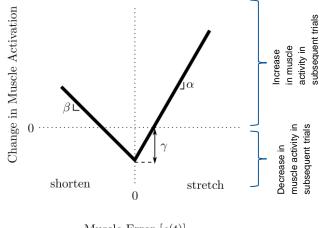
Principles of Motor Adaption

 Motor commands are composed of feedforward and feedback commands

Principles of motor adaptation:

- Errors stretching a muscle along desired trajectory
 - \rightarrow increment in *feedforward* activity, proportional to the size of the error (α)
- > Errors shortening a muscle along desired trajectory
 - increment in *feedforward* activity,
 proportional to the size of the error
 (with lower proportionality constant) (β)
- Muscle activation is reduced as error decrease with practice
 - $\rightarrow \gamma$ determines vertical offset, acts to minimize activation

V-shaped learning function (learning parameters $\alpha > \beta$ determine the slope)



Muscle Error [e(t)]





Error-Based Learning Algorithm

CNS Learns Stable, Accurate, and Efficient Movements Using a Simple Algorithm, David W. Franklin et al., Journal of Neuroscience, 2008

• Assumption: each motor command $\mathbf{w} \equiv (w_1, w_2, ..., w_M)$ for m muscels

$$w = u + v$$

with:

- u: feedforward term, corresponding to learned dynamics
- − v: feedback term, corresponding to feedback responses from unlearned dynamics
- Feedforward motor command u_i^k for each muscle i is updated from trial k to k+1:

$$\Delta u_i^k(t) = \alpha \left[\varepsilon_i^k(t) \right]_+ + \beta \left[-\varepsilon_i^k(t) \right]_+ - \gamma, \qquad \alpha > \beta > 0, \quad \gamma > 0$$

$$u_i^{k+1}(t) = \left[u_i^k(t) + \Delta u_i^k(t+\zeta) \right]_+, \qquad [.]_+ = \max\{., 0\}$$

$$\varepsilon_i^k(t) = e_i^k(t) + \delta \dot{e}_i^k(t), \qquad \delta > 0$$

with:

- $-e_i^k(t)$: stretch/shortening in muscle i at time t
- $-\Delta u_i^k$ is shifted forward in time by $\zeta > 0$
- ζ: feedback delay
- $-\alpha$, β , γ : as shown in slide 13

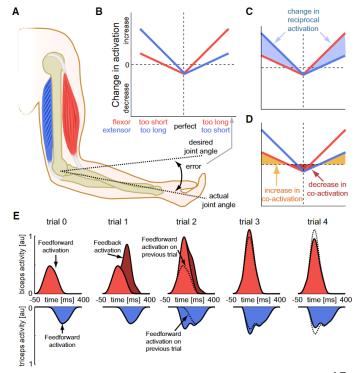


Error-Based Learning Algorithm

Computational Mechanisms of Sensorimotor Control, David W. Franklin et al., Neuron, 2008

Consider single joint motion

- A:
 - elbow joint is controlled by two antagonist muscles, biceps and triceps.
- B:
 - each error measure used by V-shaped update rule to determine change in muscle activation for next repetition of movement,
 - change is shifted forward in time to compensate for delays,
 - V-shaped learning rule for each muscle has different slope depending on whether muscle too long or too short (indicated by error)
- C:
 - different slopes for stretch/shortening of each muscle lead to appropriate change in reciprocal muscle activation
 - drives compensatory changes in the joint torques and endpoint forces





Adaptive Impedance Control for a Manipulator





Motivation and Control Formulation

 Ultimate goal of impedance control is the following task space closed-loop behavior (see lecture 4 Modern Methods of Robot Control)

$$F_{\rm ext} = M\Delta \ddot{x} + D\Delta \dot{x} + K\Delta x$$

Control law:

$$\boldsymbol{\tau}_{\text{in}}(t) = \boldsymbol{J}^{T}(\boldsymbol{q}) \left(-\boldsymbol{F}(t) - \boldsymbol{K}(t) \Delta \boldsymbol{x}(t) - \boldsymbol{D}(t) \Delta \dot{\boldsymbol{x}}(t) \right) + \boldsymbol{\tau}_{r}(t)$$

where

- $\Delta x(t) = x(t) x_d(t)$: position error
- F(t): feedforward generalized force
- K(t): stiffness matrix
- D(t): damping matrix
- $\tau_r(t)$: rest of control law including gravity term
- J(q): Jacobian matrix of the manipulator

Following the same idea as for human's limb, one can find an adaption law for the stiffness, damping and feedforward generalized force



Adaption Goal

Considering $\phi(t)$ as the vector of the values which are to be adapted, and $\phi^*(t)$ as the vector of desired values with which we can reach to the desired behaviour, our goal is to see that $\phi(t)$ approaches $\phi^*(t)$ while the error is being minimized

$$\phi(t) \equiv [\operatorname{vec}(\mathbf{K}(t))^T, \operatorname{vec}(\mathbf{D}(t))^T, \mathbf{F}^T(t)]^T$$

$$\phi^*(t) \equiv [\operatorname{vec}(\mathbf{K}_E(t))^T, \operatorname{vec}(\mathbf{D}_E(t))^T, \mathbf{F}_E^T(t)]^T$$

Considering $\tilde{\phi}(t) \equiv \phi(t) - \phi^*(t)$, reaching to the goal would be equivalent to minimize the following two cost functions:

$$V_p(t) = \frac{1}{2} \boldsymbol{\varepsilon}^T(t) \boldsymbol{M}_C(\boldsymbol{q}) \boldsymbol{\varepsilon}(t)$$

$$V_c(t) = \frac{1}{2}\widetilde{\boldsymbol{\phi}}^T(t)\boldsymbol{Q}^{-1}(\boldsymbol{q})\widetilde{\boldsymbol{\phi}}(t)$$

where

- $M_{\mathcal{C}}(q)$: mass matrix in task space
- $\varepsilon(t) \equiv \Delta \dot{x}(t) + \Lambda \Delta x(t)$: tracking error
- Q: matrix made by the positive definite matrices Q_K , Q_D and Q_τ , corresponding to the learning rate of K, D and τ





Adaption Law

Minimization of $V(t) = V_p(t) + V_c(t)$ can be done by the adaption laws, similar to what we saw for human's limb

Adaption law for each time step can be defined as:

$$F(t_{i+1}) = F(t_i) + Q_{\tau}(\varepsilon(t_i) - \gamma(t_i)F(t_i))$$

$$K(t_{i+1}) = K(t_i) + Q_{K}(\varepsilon(t_i)\Delta x^{T}(t_i) - \gamma(t_i)K(t_i))$$

$$D(t_{i+1}) = D(t_i) + Q_{D}(\varepsilon(t_i)\Delta \dot{x}^{T}(t_i) - \gamma(t_i)D(t_i))$$

where $\gamma(t_i)$ is the forgetting factor of learning which can be defined as follows

$$\gamma(t_i) = \frac{a}{1 + b||\boldsymbol{\varepsilon}(t_i)||^2}$$

with positive parameters a and b