



Brain Imaging in Alzheimer Disease

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Imaging has played a variety of roles in the study of Alzheimer disease (AD) over the past four decades. Initially, computed tomography (CT) and then magnetic resonance imaging (MRI) were used diagnostically to rule out other causes of dementia. More recently, a variety of imaging modalities including structural and functional MRI and positron emission tomography (PET) studies of cerebral metabolism with fluoro-deoxy-D-glucose (FDG) and amyloid tracers such as Pittsburgh Compound-B (PiB) have shown characteristic changes in the brains of patients with AD, and in prodromal and even presymptomatic states that can help rule-in the AD pathophysiological process. No one imaging modality can serve all purposes as each have unique strengths and weaknesses. These modalities and their particular utilities are discussed in this article. The challenge for the future will be to combine imaging biomarkers to most efficiently facilitate diagnosis, disease staging, and, most importantly, development of effective disease-modifying therapies.

THE CHANGING ROLES AND SCOPE OF NEUROIMAGING IN ALZHEIMER DISEASE

There has been a transformation in the part played by neuroimaging in Alzheimer disease (AD) research and practice in the last decades. Diagnostically, imaging has moved from a minor exclusionary role to a central position. In research, imaging is helping address many of the scientific questions outlined in Selkoe et al. (2011): providing insights into the effects of

AD and its temporal and spatial evolution. Furthermore, imaging is an established tool in drug discovery, increasingly required in therapeutic trials as part of inclusion criteria, as a safety marker, and as an outcome measure.

Concomitantly the potential of brain imaging has expanded rapidly with new modalities and novel ways of acquiring images and of analysing them. This article cannot be comprehensive. Instead, it addresses broad categories of structural, functional, and molecular imaging in AD. The specific modalities included are

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magnetic resonance imaging (MRI; both structural and functional) and positron emission tomography (PET; for assessment of both cerebral metabolism and amyloid). These modalities have different strengths and limitations and as a result have different and often complementary roles and scope.

Imaging in the Diagnosis and Prognosis of AD

The uncertainty inherent in a clinical diagnosis of AD has driven a search for diagnostic imaging markers. A definitive diagnosis still requires histopathological confirmation and the inaccessibility of the brain means imaging has a key role as a “window on the brain.” Historically, imaging—first computed tomography (CT) and then MRI—was used only to exclude potentially surgically treatable causes of cognitive decline. Now its position in diagnosis also includes providing positive support for a clinical diagnosis of AD in symptomatic individuals by identifying characteristic patterns (signatures) of structural and functional cerebral alterations. We can now also visualize the specific molecular pathology of the disease—amyloid deposits—with amyloid imaging. Alongside this increasing specificity for AD, imaging also contributes to differential diagnosis in practice by identifying alternative and/or contributory pathologies. Imaging is central to identifying vascular and non-AD degenerative pathologies and has helped in the recognition of the prevalence of mixed pathology in dementia.

In the setting of mild cognitive impairment (MCI) (Petersen 2004), the determination of underlying pathology carries immediate prognostic importance. Only a fraction of patients with MCI progress to clinical AD over 5–10 years (Petersen et al. 1999; Ritchie et al. 2001; Visser et al. 2006) and a recent meta-analysis concluded that most people with MCI will not progress to dementia even after 10 years of follow-up (Mitchell and Shiri-Feshki 2009). Two community-based studies have shown over one-third of patients diagnosed with MCI at baseline may eventually return to normal cognition (Larrieu et al. 2002; Ganguli

et al. 2004). Obviously, it would be of great value to be able to predict which MCI subjects were destined to progress to a clinical diagnosis of AD. This is true even in the absence of disease-modifying treatments, but will be especially critical when disease-modifying treatments become available.

Looking to the future, imaging has helped establish that there is a long preclinical and presymptomatic period where the pathological effects of AD are detectable. Although more data are needed, imaging is starting to provide prognostic information at this early preclinical stage. The need for an earlier and more certain diagnosis will only increase as disease-modifying therapies are identified. This will be particularly true if, as expected, these therapies work best (or only) when initiated at the preclinical stage.

Understanding the Biology of AD

Importantly, imaging has a major role to play in improving our understanding of this disease (or diseases). Uniquely, imaging is able to delineate in life the location within the brain of the effects of AD. Together with this topographical information imaging can quantify multiple different aspects of AD pathology and assess how they relate to each other and how they change over time. The clinical correlations of these changes and their relationships to other biomarkers and to prognosis can be studied. Ultimately the role of imaging in improving our understanding of the biology of AD underpins all its applications and is a theme that runs through the following sections of this article.

STRUCTURAL MRI IN AD

Basics of Structural MRI as Applied to AD

MRI utilizes the fact that protons have angular momentum which is polarized in a magnetic field. This means that a pulse of radiofrequency can alter the energy state of protons and, when the pulse is turned off, the protons will, on returning to their energy stage, emit a radiofrequency signal. By a combination of different gradients and pulses, “sequences” can be designed

to be sensitive to different tissue characteristics. In broad terms structural MRI in AD can be divided into assessing atrophy (or volumes) and changes in tissue characteristics which cause signal alterations on certain sequences such as white matter hyperintensities on T2-weighted MRI as a result of vascular damage. A number of MR sequences that are sensitive to micro-structural change (e.g., magnetization transfer or diffusion) have shown alterations in AD. These sequences are already important research tools; however, they have not yet found a place in routine clinical practice in AD and they will not be considered further here.

Utility of Structural MRI in the Study of AD

Atrophy in AD

Progressive cerebral atrophy is a characteristic feature of neurodegeneration that can be visualized in life with MRI (best with T1-weighted volumetric sequences; see Fig. 1). The major contributors to atrophy are thought to be

dendritic and neuronal losses. Studies of regional (e.g., hippocampal) MRI volumes have shown these are closely related to neuronal counts at autopsy (Bobinski et al. 2000; Gosche et al. 2002; Jack et al. 2002). The pattern of loss differs between diseases reflecting selective neuronal vulnerability and/or regional disease expression. AD is characterized by an insidious onset and inexorable progression of atrophy that is first manifest in the medial temporal lobe (Scahill et al. 2002). The entorhinal cortex is typically the earliest site of atrophy, closely followed by the hippocampus, amygdala, and parahippocampus (Lehericy et al. 1994; Chan et al. 2001; Dickerson et al. 2001; Killiany et al. 2002). Other structures within the limbic lobe such as the posterior cingulate are also affected early on. These losses then spread to involve the temporal neocortex and then all neocortical association areas usually in a symmetrical fashion. This sequence of progression of atrophy on MRI most closely fits histopathological studies that have derived stages for the spread of neurofibrillary tangles (Braak and Braak 1991).

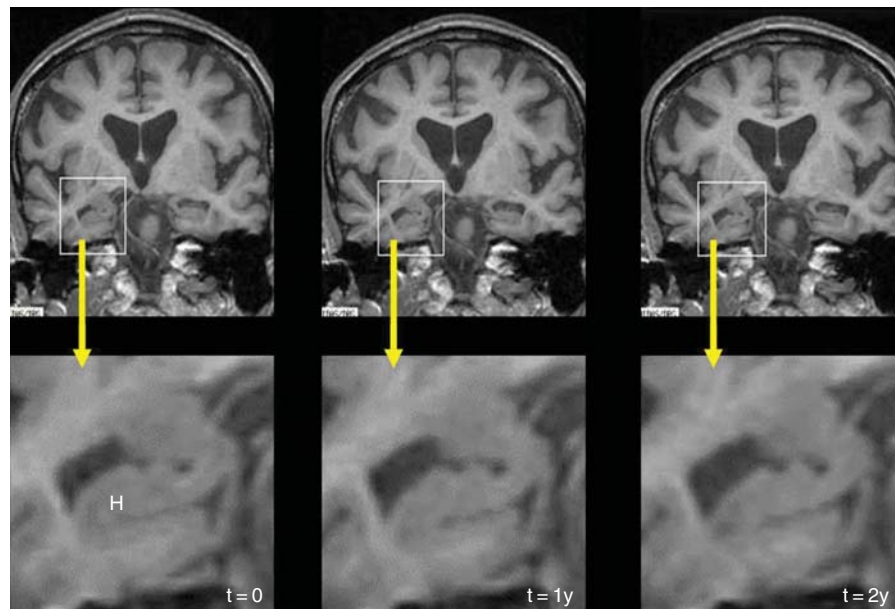


Figure 1. This series of three coronal T1-weighted studies, from an individual with autopsy-proven Alzheimer disease (AD), were each acquired ~1 yr apart and show progressive hippocampal (H) atrophy as the individual progressed from memory complaints (*left column*, $t = 0$) to MCI (*center*, $t = 1y$) and on to fulfill criteria for AD.

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Nonetheless, a significant minority of AD cases have atypical presentations and in these cases the pattern of atrophy accords with clinical phenotype: with language presentations particularly having left temporal atrophy and visual variants having posterior cortical atrophy.

It is increasingly clear that by the time a typical AD patient comes to diagnosis atrophy is well established. Even in mildly affected individuals (e.g., mean MMSE of $\sim 24/30$) entorhinal volumes are already reduced by $\sim 20\text{--}30\%$ and hippocampal volumes by $\sim 15\text{--}25\%$ (Chan et al. 2001; Dickerson et al. 2001; Schuff et al. 2009). Because rates of hippocampal atrophy in mild AD are $\sim 3\text{--}5\%$ per year (Barnes et al. 2009) this suggests that there must have been a period of several years before diagnosis where medial temporal lobe atrophy was already in process. Longitudinal MRI studies of individuals who are initially asymptomatic but who subsequently develop AD support this suggestion and find that hippocampal volumes are already reduced by about 10% 3 years before receiving a diagnosis of dementia due to AD and that rates of hippocampal atrophy increase gradually some 5 years before diagnosis. By the time a clinical diagnosis is made, atrophy is also quite widespread with whole brain volumes down by $\sim 6\%$; rates of loss having gradually accelerated (at $\sim 0.3\%/yr^2$) in the 2–4 years up to a diagnosis (Chan et al. 2003; Ridha et al. 2006; Jack et al. 2008b).

Assessment of medial temporal atrophy on MRI has been shown to have positive predictive value for AD. Visual assessment differentiates mild AD from normal aging with a sensitivity and specificity of $\sim 80\text{--}85\%$ (Scheltens et al. 1992; Duara et al. 2008; Burton et al. 2009). Differentiating MCI subjects who will progress to AD in the near future from those who will not is a more difficult task: Medial temporal atrophy on MRI is still a very significant predictor of progression with sensitivity and specificity of $\sim 50\text{--}70\%$ for distinguishing individuals who will progress to AD from those who will not (Korf et al. 2004; DeCarli et al. 2007). For these reasons medial temporal lobe atrophy now forms one of the biomarkers of AD included in proposed criteria for diagnosing

(prodromal) AD at a pre-dementia stage (Dubois et al. 2007). The severity of hippocampal atrophy tends to be greater in AD than in dementia with Lewy bodies (DLB) or vascular dementia (VaD)—when matched for clinical severity. Nonetheless, hippocampal atrophy is a feature of DLB and VaD, and in frontotemporal dementia (FTD) can be more severe anteriorly than in AD (Barber et al. 2000; Chan et al. 2001; McKeith et al. 2005; Burton et al. 2009). The differential diagnosis of AD therefore needs to take into account the overall pattern of imaging (and other) features of these dementias: for instance, focal frontal/temporal lobar atrophy on MRI would point to a diagnosis of FTD, whereas marked signal changes in white matter may suggest VaD (Chan et al. 2001; Scheltens et al. 2002; Likeman et al. 2005; Rabinovici et al. 2007; Frisoni et al. 2010). The overall pattern of atrophy is used in clinical practice and there is interest in automated pattern classification of MRI to predict AD at an early stage and to distinguish it from other dementias (Kloppel et al. 2008; Misra et al. 2009; Vemuri et al. 2009).

Measuring Progression in AD with Structural MRI

The fact that pathologically increased cerebral atrophy starts early (even presymptomatically), continues relentlessly, at least until individuals are severely affected, and correlates with clinical decline has led to atrophy on MRI being suggested as a marker of disease progression and a potential outcome measure in trials. The amount, distribution, and rate of cerebral atrophy are all closely correlated with cognitive deficits (Hua et al. 2008; Ridha et al. 2008; Cardenas et al. 2009; Fox et al. 1999b). In the absence of an intervention cerebral volume loss in AD has clear, direct, and profound negative clinical consequences. Epidemiological-autopsy studies of individuals with and without dementia showed that, whereas plaques, tangles, and atrophy are all associated with dementia, atrophy was the factor that most strongly correlated with dementia at all ages (Savva et al. 2009). It appears that histopathological



hallmarks of AD are markers of disease process whereas the clinical state is captured by the extent of neurodegeneration—for which atrophy may be considered an *in vivo* measure. Rates of regional and/or global atrophy on MRI have as a result been proposed as outcome measures in trials seeking to show a disease-modification effect in AD; the motivation for this is the potentially increased power to detect a disease-slowness effect. Sample size calculations based on natural history studies would support this with only ~20% as many patients being expected to be needed for the same effect using MRI measures than if clinical scales were used (Fox et al. 2000; Jack et al. 2008a; Ridha et al. 2008; Schuff et al. 2009). Rates of hippocampal and whole brain atrophy on MRI have to date been the most widely included imaging measures in trials; however, other MRI measures show promise, including cortical thickness or composites of change (Lerch et al. 2005; Hua et al. 2008; Jack et al. 2008a; Vemuri et al. 2009). The validation of this approach, however, awaits the discovery of disease-modifying therapies particularly as therapies may have an effect on progression of volume loss through mechanisms other than reduced rates of neuronal loss (e.g., hydration, inflammatory, and anti-inflammatory effects) (Fox et al. 2005a). It is likely that multiple imaging and fluid biomarkers will be included in trials that seek to understand as well as measure effects on disease progression.

Availability and Utility of Structural MRI

An obvious strength of MRI is its availability. A testament to its value in diagnosis in dementia is the fact that European and U.S. guidelines recommend that all subjects with cognitive decline undergo structural imaging (MRI or CT) and that it is part of proposed diagnostic criteria for AD and for other dementias (Waldemar et al. 2000; Knopman et al. 2001; McKeith et al. 2005; Dubois et al. 2007). In most centers, MRI is regarded as an essential investigation in dementia—a marker of its utility. Although not as rapid as CT, a typical high-resolution volumetric sequence can be acquired in 5–10

min and more basic sequences in considerably less time. MRI is safe and as it does not involve ionizing radiation individuals can be imaged serially without concerns about carcinogenicity. MRI offers a range of different sequences that can probe different tissue characteristics providing multiple clinical and research measures in the same session. Atrophy as an outcome measure has strengths over clinical measures because it is not subject to practice effects or (realistically) to floor or ceiling effects, and it theoretically has a greater ability to detect disease slowing. MRI measures of atrophy reflect cumulative neuronal damage which in turn is directly responsible for clinical state. When compared with other imaging markers (and other biomarkers) cerebral atrophy has, as a strength, its strong correlation with cognitive decline.

Limitations of Structural MRI in AD

Structural MRI lacks molecular specificity. It cannot directly detect the histopathological hallmarks of AD (amyloid plaques or neurofibrillary tangles) and as such it is downstream from the molecular pathology. Cerebral atrophy is a nonspecific result of neuronal damage and, whereas certain patterns of loss are characteristic of different diseases, they are not entirely specific. Atrophy patterns overlap with other diseases and unusual forms of AD have atypical patterns of atrophy too. In more severely affected individuals and those with claustrophobia, MRI may not be tolerated whereas a rapid CT scan may be more feasible. In terms of measuring progression, volume changes on MRI may be produced by factors other than the progression of neuronal loss and as such assessment of disease modification may be obscured, at least in the short term, by such spurious effects. As the name implies, structural MRI cannot assess function; this is provided with increasing sophistication by functional MRI and PET.

Overall the availability, ease of use, and multiple applications of structural MRI in AD mean it will play a central role in research and practice for some years to come. Increasingly, the other (complementary) modalities described in this article will address the weaknesses of MRI.

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FUNCTIONAL MRI IN AD

Basics of Functional MRI as Applied to AD

Functional MRI (fMRI) is being increasingly used to probe the functional integrity of brain networks supporting memory and other cognitive domains in aging and early AD. fMRI is a noninvasive imaging technique which provides an indirect measure of neuronal activity, inferred from measuring changes in blood oxygen level-dependent (BOLD) MR signal (Ogawa et al. 1990; Kwong et al. 1992). Whereas fluoro-deoxy-D-glucose (FDG)-PET is thought to be primarily a measure of synaptic activity, BOLD fMRI is considered to reflect the integrated synaptic activity of neurons via MRI signal changes because of changes in blood flow, blood volume, and the blood oxyhemoglobin/deoxyhemoglobin ratio (Logothetis et al. 2001). fMRI can be acquired during cognitive tasks, typically comparing one condition (e.g., encoding new information) to a control condition (e.g., viewing familiar information or visual fixation on a cross-hair), or during the resting state to investigate the functional connectivity (fc-MRI) within specific brain networks. Fc-MRI techniques examine the correlation between the intrinsic oscillations or time course of BOLD signal between brain regions (Fox et al. 2005b), and have clearly documented the organization of the brain into multiple large-scale brain networks (Damoiseaux et al. 2006; Vincent et al. 2006). Both task-related and resting fMRI techniques have the potential to detect early brain dysfunction related to AD, and to monitor therapeutic response over relatively short time periods; however, the use of fMRI in aging, MCI, and AD populations thus far has been limited to a relatively small number of research groups.

Utility of Functional MRI in the Study of AD

Much of the early fMRI work in MCI and AD used episodic memory tasks, and was focused on the pattern of fMRI activation in hippocampus and related structures in the medial temporal lobe. In patients with clinically diagnosed AD, the results have been quite

consistent, showing decreased hippocampal activity during the encoding of new information (Small et al. 1999; Rombouts et al. 2000; Kato et al. 2001; Gron et al. 2002; Machulda et al. 2003; Sperling et al. 2003; Remy et al. 2004; Golby et al. 2005; Hamalainen et al. 2007). Several studies have reported increased prefrontal cortical activity in AD patients (Grady et al. 2003; Sperling et al. 2003; Sole-Padullés et al. 2009), suggesting that other networks may increase activity as an attempted compensatory mechanism during hippocampal failure.

A relatively small number of fMRI studies have been published in subjects at risk for AD, including MCI subjects and genetic at-risk individuals yielding somewhat discrepant findings. Several studies have reported decreased mesial temporal lobe (MTL) activation in MCI (Small et al. 1999; Machulda et al. 2003; Johnson et al. 2006; Petrella et al. 2006) and genetic at-risk subjects (Smith et al. 1999; Lind et al. 2006a,b; Trivedi et al. 2006; Borghesani et al. 2007; Mondadori et al. 2007; Ringman et al. 2010). Interestingly, several fMRI studies have reported evidence of *increased* MTL activity in at-risk subjects, particularly among very mild MCI subjects (Dickerson et al. 2004, 2005; Celone et al. 2006; Hamalainen et al. 2006; Heun et al. 2007; Kircher et al. 2007; Lenzi et al. 2009), and cognitively intact individuals with genetic risk for AD (Bookheimer et al. 2000; Smith et al. 2002; Wishart et al. 2004; Bondi et al. 2005; Fleisher et al. 2005; Han et al. 2007; Filippini et al. 2009). It is likely that these discrepant results are related to specific paradigm demands, stage of impairment, and behavioral performance. A common feature of the studies reporting evidence of increased fMRI activity is that the at-risk subjects were able to perform the fMRI tasks reasonably well. In particular, the event-related fMRI studies have found that hyperactivity was observed specifically during successful memory trials, which suggested that hyperactivity might represent a compensatory mechanism in the setting of early AD pathology (Dickerson and Sperling 2008; Sperling et al. 2009).

Cross-sectional studies suggest that the hyperactivity may be present only at early stages

of MCI, followed by a loss of activation in late stages of MCI, similar to the pattern seen in AD patients (Celone et al. 2006). Longitudinal studies furthermore suggest that the presence of hyperactivity at baseline is a predictor of rapid cognitive decline (Bookheimer et al. 2000; Dickerson et al. 2004; Miller et al. 2008a), and loss of hippocampal function on serial fMRI (O'Brien et al. 2010). The mechanistic underpinnings of MTL hyperactivation remain unclear; however, these new longitudinal data suggest that hyperactivity may be a marker of impending neuronal failure. This phenomena may reflect cholinergic or other neurotransmitter up-regulation (DeKosky et al. 2002), aberrant sprouting of cholinergic fibers (Masliah et al. 2003), inefficiency in synaptic transmission (Stern et al. 2004), increased calcium influx, and evidence of excitotoxicity (Palop et al. 2007; Busche et al. 2008).

Converging data suggest that memory function is subserved by a network of brain regions, which includes not only the MTL system, but also a set of cortical regions, including the precuneus, posterior cingulate, lateral parietal, lateral temporal, and medial prefrontal regions, collectively known as the “default network” which typically deactivate during memory encoding and other cognitively demanding tasks focused on the processing of external stimuli (Raichle et al. 2001; Buckner et al. 2008). Recent studies have also suggested that the default network shows markedly abnormal responses during memory tasks in clinical AD patients and in subjects at risk for AD (Lustig and Buckner 2004; Celone et al. 2006; Petrella et al. 2007a; Pihlajamaki et al. 2008, 2009). Interestingly, it is the same default network regions that typically show beneficial deactivations in healthy subjects, particularly, the posterior cingulate/precuneus (Daselaar et al. 2004; Miller et al. 2008b), which tend to manifest a paradoxical increase in fMRI activity (or loss of normal default network deactivation) in both at-risk groups and clinical AD patients (Petrella et al. 2007b; Pihlajamaki et al. 2008; Fleisher et al. 2009; Sperling et al. 2010).

There has been a recent emphasis on BOLD fMRI techniques to study spontaneous brain

activity and the interregional correlations during the resting state. These studies have clearly documented the organization of the brain into multiple large-scale brain networks (Damoiseaux et al. 2006; Vincent et al. 2007). Interestingly, both independent component analyses and “seed-based” connectivity techniques have shown the robust intrinsic connectivity between the posteromedial nodes of the default network, in particular the posterior cingulate/precuneus, with the hippocampus. Multiple groups have confirmed impaired intrinsic functional connectivity in the default network during the resting state in MCI and AD (Greicius et al. 2004; Rombouts et al. 2005, 2009; Sorg et al. 2007; Bai et al. 2008; Koch et al. 2010) over and above more general age-related disruption of large-scale networks (Andrews-Hanna et al. 2007; Damoiseaux et al. 2008). One recent study suggests that these resting fMRI techniques may be more readily applied to at-risk clinical populations than task fMRI (Fleisher et al. 2009). Fc-MRI may be particularly advantageous for use in clinical trials, as no special equipment is required, subjects do not have to be able to perform a cognitive task, and a resting run could be added to the end of a safety or volumetric MRI protocol. Additional longitudinal work is needed to determine if longitudinal changes in fc-MRI will parallel clinical decline.

Interestingly, the default network regions showing aberrant task-related fMRI activity and dysconnectivity in MCI and AD also overlap the anatomy of regions with the highest amyloid burden in AD patients (Fig. 2; Klunk et al. 2004; Buckner et al. 2005, 2009; Sperling et al. 2009). Several recent studies in cognitively normal older individuals with evidence of amyloid deposition on PET imaging have shown evidence of disrupted default network activity during memory tasks and at rest (Hedden et al. 2009; Sheline et al. 2009; Sperling et al. 2009), suggesting these markers may be particularly useful to track response to anti-amyloid therapies in preclinical trials.

fMRI, either during cognitive paradigms or during resting state, may hold the greatest potential for the evaluation of novel pharmacological strategies to treat AD. Several studies in

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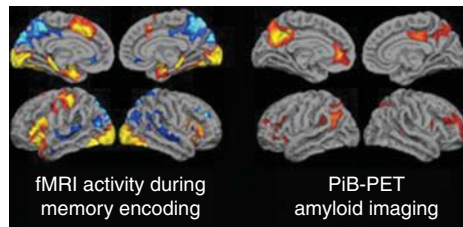


Figure 2. (Left) Group map of fMRI activity showing regions that increase activity (yellow/red) or decrease (blue) activity during successful encoding. (Right) Group map of ^{11}C -PiB retention in a group of non-demented older individuals. Note the anatomic overlap of PiB retention to default network (regions in blue on left).

healthy young and older subjects suggest that fMRI can detect acute pharmacological effects on memory networks (Thiel et al. 2001; Sperling et al. 2002; Kukolja et al. 2009). To date, only a few small fMRI studies have shown enhanced brain activation after acute or prolonged treatment with cholinesterase inhibitors in MCI and AD, although these studies were not conducted as typical double-blind, placebo-controlled trials (Rombouts et al. 2002; Goekoop et al. 2004; Saykin et al. 2004; Shanks et al. 2007; Bokde et al. 2009; Venneri et al. 2009). fMRI is now being incorporated into a small number of investigator-initiated add-on studies to ongoing Phase II and Phase III trials, which should provide some valuable information regarding the potential utility of these techniques in clinical trials.

Limitations of fMRI in AD

There are multiple challenges in performing longitudinal fMRI studies in patients with neurodegenerative dementias. It is likely that fMRI will remain quite problematic in examining patients with more severe cognitive impairment, as these techniques are very sensitive to head motion. If the patients are not able to adequately perform the cognitive task, one of the major advantages of task fMRI activation studies is lost. Resting state fMRI may be more feasible in more severely impaired patients.

It is critical to complete further validation experiments. BOLD fMRI response is known

to be variable across subjects, and very few studies examining the reproducibility of fMRI activation in older and cognitively impaired subjects have been published to date (Clement and Belleville 2009; Putcha et al. 2010). Longitudinal functional imaging studies are needed to track the evolution of alterations in the fMRI activation pattern over the course of the cognitive continuum from preclinical to prodromal to clinical AD. It is also important to evaluate the contribution of structural atrophy to changes observed with functional imaging techniques in neurodegenerative diseases. Finally, longitudinal multimodality studies, including structural MRI, fMRI, and FDG-PET and PET amyloid imaging techniques, are needed to understand the relationship between these markers, and the relative value of these techniques in tracking change along the clinical continuum of AD (Jack et al. 2010).

FLUORODEOXYGLUCOSE (FDG) PET IN AD

Basics of FDG PET as Applied to AD

Brain FDG PET primarily indicates synaptic activity. Because the brain relies almost exclusively on glucose as its source of energy, the glucose analog FDG is a suitable indicator of brain metabolism and, when labeled with Fluorine-18 (half-life 110 min) is conveniently detected with PET. The brain's energy budget is overwhelmingly devoted to the maintenance of intrinsic, resting (task-independent) activity, which in cortex is largely maintained by glutamatergic synaptic signaling (Sibson et al. 1997). FDG uptake strongly correlates at autopsy with levels of the synaptic vesicle protein synaptophysin (Rocher et al. 2003). Hence, FDG PET is widely accepted to be a valid biomarker of overall brain metabolism to which ionic gradient maintenance for synaptic activity is the principal contributor (Schwartz et al. 1979; Magistretti 2006). In this context, a single, specific AD-related alteration in FDG metabolism has not been identified and therefore the FDG-PET abnormalities described below are assumed to be the net result of some combination of processes putatively involved in the

pathogenesis of AD including, but not limited to, expression of specific genes, mitochondrial dysfunction, oxidative stress, deranged plasticity, excitotoxicity, glial activation and inflammation, synapse loss, and cell death.

Utility of FDG PET in the Study of AD

The Pattern of FDG Hypometabolism Is an Endophenotype of AD

A substantial body of work over many years has identified a FDG-PET endophenotype of AD (Fig. 3)—that is, a characteristic or signature ensemble of limbic and association regions that are typically hypometabolic in clinically established AD patients (Foster et al. 1983; Reiman et al. 1996; Minoshima et al. 1997; De Santi et al. 2001). The anatomy of the AD signature includes posterior midline cortices of the parietal (precuneus) and posterior cingulate gyri, the inferior parietal lobule, posterolateral portions of the temporal lobe, as well as the hippocampus and medial temporal cortices. Metabolic deficits in AD gradually worsen throughout the course of the disease. Bilateral asymmetry is common at early stages, more

advanced disease usually involves prefrontal association areas, and in due course even primary cortices may be affected. Interestingly, the regions initially hypometabolic in AD are anatomically and functionally interconnected and form part of the large-scale distributed brain network known as the default mode network (Raichle et al. 2001). We now know in addition that these regions are highly vulnerable to amyloid- β (A β) deposition (Klunk et al. 2004; Buckner et al. 2005).

Less severe or consistent hypometabolism has been identified in MCI patients, some of whom were found on follow-up examination to have converted to AD (Arnaiz et al. 2001; de Leon et al. 2001; Jagust et al. 2002, 2007; Chetelat et al. 2003; Caselli et al. 2008; Langbaum et al. 2009; Landau et al. 2010). Differences in FDG between MCI and normal aging have not typically been large, but the control groups in most of these studies were likely contaminated with a number of individuals who, although clinically normal, were amyloid positive (see below) and possibly in earlier phases of preclinical AD. FDG hypometabolism parallels cognitive function along the trajectory of normal, preclinical, prodromal, and established AD (Minoshima et al. 1997; Furst et al. 2010); however, higher levels of brain and cognitive reserve are well known to attenuate the strength of these correlations and highly intelligent AD patients can be clinically mild, but severely hypometabolic (Stern et al. 1992; Alexander et al. 1997). Coexisting vascular disorders, including ischemia, amyloid angiopathy, and micro-hemorrhage, potentially confound the relation of FDG to clinical phenotype, but the classic AD FDG pattern is well correlated with histopathologic diagnosis of AD at autopsy (Hoffman et al. 2000; Jagust et al. 2007).

FDG Hypometabolism Is Related to Other AD Biomarkers and to Genes

The association between amyloid deposition and brain function in AD has been studied with FDG PET. Longitudinal data has shown that, once the stage of established AD is reached, amyloid deposition in most regions has

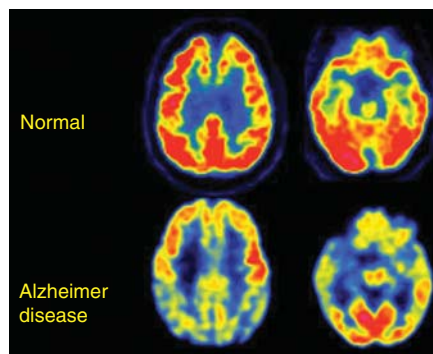


Figure 3. Transaxial FDG-PET images of a normal control subject and a patient with mild AD. Note severe hypometabolism (yellow and blue cortical regions) in association and limbic cortex. These are the typically involved brain regions that define the FDG endophenotype of AD. They include posterior-medial parietal (precuneus), lateral parietal, lateral temporal, and medial temporal lobes. This pattern slowly worsens in parallel with symptoms and is well correlated at autopsy with AD pathologic diagnosis.

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plateaued (Engler et al. 2006; Jack et al. 2009), but FDG continues to decline along with cognitive function (Engler et al. 2006). Several groups have observed high amyloid deposition in parietal regions to be associated with co-localized FDG hypometabolism, possibly indicating a local toxicity (Klunk et al. 2004; Engler et al. 2006; Edison et al. 2007; Cohen et al. 2009). In other groups, this association was not statistically significant, possibly because the amyloid burden in these patients was already at its plateau (Kadir et al. 2008; Furst et al. 2010). An important clue to this relationship could lie in the observation that the relation is consistently weaker in frontal regions, where some of the highest amyloid burdens are found (Klunk et al. 2004; Edison et al. 2007). Interestingly, amyloid-positive MCI patients in one study had preserved FDG metabolism that was *positively* correlated with extensive Pittsburgh Compound-B (PiB) retention, possibly suggesting a mediating role for metabolism, perhaps either as a brain reserve factor or as an accelerant of deposition (Cohen et al. 2009). Additional longitudinal data will be required to clarify these relationships, but clearly FDG metabolism appears to be changing as amyloid is accumulating. It is possible that FDG data could signal an intermediate stage between the initiating pathologic event and the subsequent development of synaptic failure and neurodegeneration (Cohen et al. 2009).

Brain volume loss is also observed in AD hypometabolic areas, but the FDG findings have generally survived MRI-based corrections for cortical atrophy (Meltzer et al. 1996; Ibanez et al. 1998; Jagust et al. 2006; Cohen et al. 2009; Lowe et al. 2009; Rabinovici et al. 2010), suggesting that volume loss and function loss are separable phenomena in AD. Both domains of data are reported to have predictive power: FDG hypometabolism that predicts ultimate development of AD occurs before impairment (de Leon et al. 2001; Jagust et al. 2006) and brain volume loss has also been reported in cognitively normal individuals who go on to develop AD (Fox et al. 1999a; Jack et al. 2004). Systematic comparison of two imaging biomarkers requires caution because of rapidly evolving

technology. For example, recently developed methods for subject-specific MRI segmentation have revealed subtle cortical thinning in a distribution similar to that seen with FDG (Walhovd et al. 2009; Karow et al. 2010). A continuing challenge is presented by the fact that FDG-PET data inherently contains volume information, and PET-based partial volume correction (e.g., with deconvolution [Tohka and Reilhac 2008]), may eventually be useful to disentangle FDG retention and structural loss.

Initial reports associating FDG hypometabolism and AD-related CSF measures have varied, likely due in part to image and fluid sample processing differences. FDG was associated with low CSF A β and increased CSF tau in amyloid-positive clinically normal older individuals (Petrie et al. 2009), but with CSF A β and not tau in an Alzheimer's Disease Neuroimaging Initiative (ADNI) study of AD, MCI, and controls, adjusted for diagnosis (Jagust et al. 2009).

Carriers of the apolipoprotein-E (APOE) ϵ 4 allele have a higher risk of developing AD, and the classic AD pattern of hypometabolism described above is seen in cognitively normal APOE ϵ 4 carriers (Reiman et al. 1996, 2005). A relationship of this FDG pattern to serum cholesterol and to an aggregate cholesterol-related genetic score in middle age has also been reported (Reiman et al. 2008, 2010). Maternal history of dementia has recently been related both to increased PiB retention and to FDG hypometabolism in AD-related areas among asymptomatic individuals (Mosconi et al. 2009, 2010).

FDG PET Is a Valid AD Biomarker

Over the course of three decades of investigation, FDG PET has emerged as a robust marker of brain dysfunction in AD. Its principal value is twofold: first, clinical utility has been documented when confounding conditions (e.g., DLB or frontotemporal lobar degeneration [FTLD]), are in question. Thus, when frontotemporal rather than temporoparietal hypometabolism is prominent, a clinically uncertain AD diagnosis may be changed to FTLD (Foster et al. 2007); when prominent

occipital hypometabolism is found in addition to temporoparietal, the data are highly suggestive of DLB (Albin et al. 1996; Mosconi et al. 2008).

Second, FDG has emerged as a robust biomarker of neurodegeneration with which hypometabolism can be observed to precede the appearance of cognitive symptoms and to predict the rate of progressive cognitive decline in individuals who are later found to have progressed to AD (de Leon et al. 2001; Jagust et al. 2006). FDG hypometabolism is also predictive of the rate of memory decline in APOE ϵ 4 carriers with mild memory loss over 2 years (Small et al. 2000). Most importantly for AD treatment research, a recent analysis of ADNI FDG data found that AD and MCI groups each showed progression of AD-like hypometabolism over 1 year that paralleled changes in a standard clinical endpoint, the clinical dementia rating scale (CDR) sum-of-boxes (Chen et al. 2010). These authors calculated that the use of FDG PET in clinical trials of AD therapy could reduce sample sizes by approximately one order of magnitude.

The Limitations of FDG PET in AD

FDG PET is relatively expensive and, like all PET techniques, has more limited availability, although its use in oncology has dramatically increased availability in the USA over the past decade. It requires intravenous access and involves exposure to radioactivity, although at levels well below significant known risk. Brain FDG retention is a nonspecific indicator of metabolism that can be deranged for a variety of reasons (e.g., ischemia or inflammation) and may in certain individuals be irrelevant or only indirectly related to any AD-related process.

AMYLOID PET IN AD

Basics of Amyloid PET as It Is Applied to AD

An important “first principle” of amyloid imaging in the context of AD is that amyloid PET is intended first and foremost as an in vivo

surrogate for A β pathology, and not necessarily as a surrogate for clinical diagnosis. As discussed below, there are diagnostic applications of amyloid imaging, but these share the same strengths and limitations as postmortem determinations of A β content. Another important principle of amyloid imaging is that the substrate for all currently known A β tracers is fibrillar A β in a beta-sheet conformation (Ikonomovic et al. 2008). When speaking of the binding substrates of amyloid tracers, it is preferable to think in terms of fibrillar and nonfibrillar A β rather than visual descriptions of plaques as fleecy, amorphous, diffuse, compact, cored, neuritic, etc., because there can be varying amounts of fibrillar A β in any of these plaque types. Compact, cored, and neuritic plaques typically have large amounts of fibrillar amyloid and fleecy and amorphous plaque deposits typically have very little (particularly in the cerebellum). However, diffuse plaques are not a precisely defined term and can have widely varying amounts of fibrillar A β from case to case. Along similar lines, cerebrovascular amyloid typically has a high degree of fibrillar A β and appears to be a very good substrate for amyloid tracer binding (Bacskai et al. 2007; Johnson et al. 2007; Lockhart et al. 2007; Ikonomovic et al. 2008). Increasing recognition has been given to the toxicity of oligomeric species of A β and this is described in Mucke and Selkow (2011). Although it is possible that currently available amyloid tracers could bind to oligomers of A β in a beta-sheet conformation once they reach a necessary size (probably at least a trimer or tetramer), the in vivo signal of amyloid tracers is not directly representative of these species because of their low concentration relative to insoluble A β fibrils. However, there may be a relationship between the amyloid PET signal and oligomer concentration based on the existence of an equilibrium between monomers, oligomers, and fibrillar A β . Although claims have been made that some tracers can image neurofibrillary tangles, there have been no validation studies in this regard. To the contrary, there is evidence that some amyloid tracers do not bind neurofibrillary pathology (Klunk et al. 2003; Ikonomovic et al. 2008).

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With regard to specific amyloid imaging agents, this review will discuss “amyloid tracers” in general, while acknowledging that most of the statements are derived from data on the most widely evaluated PET tracer, PiB (Klunk et al. 2004). At the time of writing, there have been one or two, small published studies using each of the fluorine-18-labelled tracers, [F-18]florbetaben (18F-BAY94-9172 or AV-1; Rowe et al. 2008), [F-18]florbetapir (AV-45; Wong et al. 2010; Clark et al. 2011) and [F-18]flutemetamol (3’F-PiB or GE-067; Nelissen et al. 2009; Vandenberghe et al. 2010) in AD patients. Although the PiB PET findings may ultimately be found to extend to these F-18-labeled tracers as well, this cannot be assumed until appropriate studies have been repeated with each individual tracer or until pharmacological equivalency to PiB has been established by direct comparison in the same subjects.

Utility of Amyloid PET in the Study of AD

The obvious strength of amyloid imaging is that it has allowed the determination of brain A β content to be moved from the pathology laboratory into the clinic. Amyloid imaging can detect cerebral β -amyloidosis and appears specific for this type of amyloid pathology, giving negative signals in pathologically confirmed cases of prion amyloid (Villemagne et al. 2009), pathologically confirmed pure α -synucleinopathy (Burack et al. 2010), as well

as in apparently pure cases of tauopathy in semantic dementia (Drzezga et al. 2008).

In the setting of clinical dementia, particularly in clinically atypical presentations, this has important diagnostic utility. Reviewing recent publications from 15 research groups who have performed amyloid PET on clinically diagnosed AD patients, 96% of AD patients were amyloid positive (Fig. 4; Kemppainen et al. 2006; Aizenstein et al. 2008; Edison et al. 2008; Shin et al. 2008; Drzezga et al. 2009; Hedden et al. 2009; Lowe et al. 2009; Maetzler et al. 2009; Wolk et al. 2009; Devanand et al. 2010; Forsberg et al. 2010; Jagust et al. 2010; Rabino-vici et al. 2010; Roe et al. 2010; Rowe et al. 2010; Tolboom et al. 2010). One assumption is that amyloid-negative demented patients diagnosed as AD have been given an incorrect diagnosis. Another possibility is that amyloid imaging was simply not sensitive enough in some patients and these patients would become amyloid positive over time. One follow-up of three amyloid-negative subjects initially diagnosed as AD (Klunk et al. 2004), has shown that all three subjects have remained amyloid negative for 5 years (Kadir et al. 2010), suggesting that sensitivity was not the issue and that these patients are not likely to have AD as the cause of their cognitive deficits. On the other side of the coin are amyloid-positive patients who have been diagnosed with a dementia other than AD. In the case of FTD, it has been assumed that patients who present with a

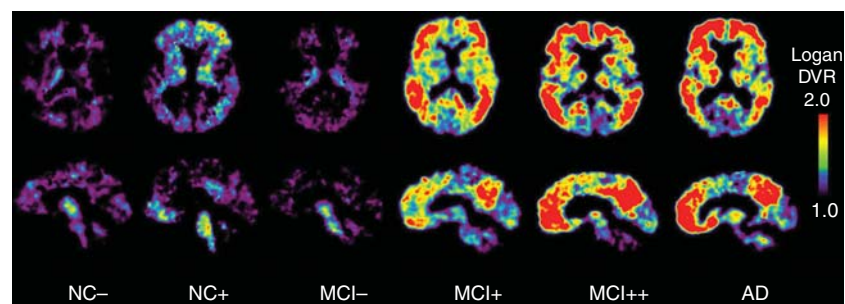


Figure 4. PiB PET Images of normal control, MCI, and AD subjects showing a range of amyloid- β deposition. Most controls show no evidence of amyloid- β deposition (NC-), but a substantial portion (~25%) do (NC+). Most patients with MCI show moderate (MCI+) or severe amyloid- β deposition (MCI++), but as many as 40%–50% show no evidence of amyloid- β pathology (MCI-). The vast majority of clinically diagnosed AD patients show heavy amyloid- β deposition (AD).

clinical FTD syndrome but have AD-like amyloid PET scans are really atypical presentations of AD (Rabinovici et al. 2007, 2008; Engler et al. 2008), but pathological verification remains to be done. These patients will be particularly important to identify when there are effective treatments for AD directed at A β deposition.

In the setting of MCI, combined data from nine amyloid PET studies show that 161 of 272 MCI patients were amyloid positive (59%) (Fig. 4; Forsberg et al. 2008; Koivunen et al. 2008; Lowe et al. 2009; Okello et al. 2009; Tolboom et al. 2009; Wolk et al. 2009; Devanand et al. 2010; Jagust et al. 2010; Rowe et al. 2010). Five of these studies included longitudinal clinical follow-up for 1–3 years on 155 MCI patients and showed that 57 of these 155 progressed to clinical AD (37%) and 53 of these 57 were amyloid positive at baseline (93%); only four of 54 amyloid-negative MCI patients progressed to clinical AD in these studies (7%) (Forsberg et al. 2008; Koivunen et al. 2008; Okello et al. 2009; Wolk et al. 2009; Jagust et al. 2010).

The most substantial contribution of amyloid imaging may come in the setting of the cognitively normal elderly. It is at this clinically “invisible” stage that detection of underlying cerebral β -amyloidosis (the sine qua non of AD pathology) may give us the greatest insights into the very beginnings of this disease. Furthermore, it may be at this asymptomatic stage that our chances are greatest of discovering truly effective treatments. In a series of studies from 13 sites, 155 of 651 (24%) of cognitively normal controls showed evidence of cerebral A β deposition (Fig. 4; Kemppainen et al. 2006; Mintun et al. 2006; Edison et al. 2008; Shin et al. 2008; Hedden et al. 2009; Lowe et al. 2009; Maetzler et al. 2009; Wolk et al. 2009; Devanand et al. 2010; Jagust et al. 2010; Rabinovici et al. 2010; Roe et al. 2010; Rowe et al. 2010; Tolboom et al. 2010). In most cases, the degree of amyloid deposition was fairly easy to distinguish from that typically seen in AD (Aizenstein et al. 2008), but this is not always the case. The prevalence of amyloid positivity is related closely to age and apolipoprotein-E allele status (Morris

et al. 2010; Rowe et al. 2010). Although some subtle cognitive effects of PET amyloid positivity may be discernable in this population (Rentz et al. 2010), in most cases the overriding conclusion is that there is no tight, direct relationship between amyloid PET and cognition at these earliest stages of A β deposition. As discussed above, other protective or vulnerability factors must be invoked to fully explain the connection between early PET amyloid positivity and cognitive impairment. It is possible that the failure to directly assess oligomeric A β concentration could preclude the demonstration of amyloid PET-related cognitive effects, but vulnerability factors (such as subclinical cerebrovascular disease) and brain/cognitive reserve factors are likely to play a role as well (Kemppainen et al. 2008; Roe et al. 2008, 2010; Cohen et al. 2009; Rentz et al. 2010).

In Blennow et al. (2011), CSF biomarkers are discussed. There is clearly a large overlap in the information available from CSF A β 42 levels and amyloid PET, but each technique has its advantages and limitations (see below). The advantages of amyloid PET center around the regional information and in the continuously variable nature of the biological changes. The latter refers to the fact that decreases in CSF A β 42 appear to occur early (at least as early as changes in amyloid PET) and precipitously—achieving its final level very early in the course of the pathophysiological spectrum of AD—probably presymptomatically (Blennow and Hampel 2003; Hansson et al. 2006; Fagan et al. 2007, 2009). That is, the change in CSF appears to be a step-function and longitudinal studies have not shown a progressive decrease in CSF A β 42 over time (Buchhave et al. 2009). This is not surprising given that typical concentrations of A β found in insoluble deposits in AD cortex are approximately 5000 μ g/L (\sim 1 μ M), while typical CSF A β 42 concentrations are around 0.5 μ g/L—or 0.01% of insoluble cortical A β . Thus, it is not surprising that relatively little cortical A β would need to deposit before a new equilibrium would be established with CSF. This has an important implication for clinical trials: As an outcome measure, CSF A β 42 is not likely to normalize

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until the vast majority of cortical A β deposits are removed. Thus, CSF A β 42 and amyloid PET are likely to be equivalent as screening tools for clinical trials, but the more dynamic nature of amyloid PET and the fact that amyloid tracer retention correlates directly with A β load (Ikonomovic et al. 2008) makes this a more suitable outcome measure when the goal is to detect changes in brain A β load. In support of this statement, the ability of amyloid PET to show an amyloid-lowering effect of passive immunotherapy in humans has already been reported (Rinne et al. 2010).

A unique strength of amyloid PET across the entire clinical spectrum is the regionally specific nature of the quantitative data. Although we often reduce imaging data to a single number (e.g., mean cortical retention), we must remember that a strength of any imaging technique is the wealth of regional information that is supplied. Although amyloid PET can quantify amyloid load throughout the brain, it is not clear what pool of brain A β is represented by changes in CSF A β . One study has suggested that CSF A β is most tightly correlated with amyloid retention in brain regions adjacent to CSF spaces (Grimmer et al. 2009).

The Limitations of Amyloid PET in AD

Major deterrents to the widespread use of amyloid PET remain cost and availability. Availability has been improved by the development of F-18-labeled agents that can be distributed to PET scanners not associated with a cyclotron. Cost remains an issue, especially where CSF measurement of A β 42 can provide very similar information when the question is simply the presence or absence of brain A β deposition. Being an early event in the pathogenesis of AD, amyloid PET is not a good surrogate marker of progression during the clinical stage of the disease (Engler et al. 2006; Kadir et al. 2010). This role is filled much better by structural MRI and FDG PET (Jack et al. 2010). Similarly, amyloid imaging gives much more of a binary diagnostic readout than techniques such as MRI and FDG PET. That is, amyloid imaging has a certain specificity for the

pathology of AD, but when that pathology is absent, a negative amyloid PET scan will be identical regardless of the non-AD etiology of the dementia. In contrast, MRI and FDG PET may give an indication of a frontotemporal or vascular pathology when an amyloid PET scan would be ambiguously negative in both cases. The threshold of sensitivity of amyloid PET has yet to be precisely determined, but it is clear that some level of amyloid deposition is histologically detectable prior to the *in vivo* signal becoming “positive” (Cairns et al. 2009).

SUMMARY

State-of-the-(Imaging)-Art

In this chapter we briefly reviewed the most commonly used imaging technologies: structural and functional MRI and FDG and amyloid PET. Other MRI techniques such as diffusion tensor imaging (DTI) and associated tractography technologies, arterial spin labeling measures of cerebral blood flow and PET tracers targeted at the cholinergic system, microglial activation and other tracers in development are also contributing to our basic understanding of AD. A particularly exciting pursuit is PET ligands targeting the other major AD pathologic hallmark, the neurofibrillary tangle. Biomarkers of tau have been a particular challenge because of the need to target binding to something other than the β -sheet fibril dominated by A β deposits and the relatively smaller total mass of tau deposits, but steady progress is being made to achieve sufficient ligand affinity and selectivity. It should be clear from the above discussions that no single imaging technique can provide all of the answers. Fortunately, the strengths and weakness of the available imaging technologies are largely complementary. This has led to a variety of “multi-modal” imaging studies in which several techniques are simultaneously or sequentially applied to the same subjects for the same period of time. These direct comparisons have contributed greatly to our understanding of AD and the strengths and limitations of each technique.

Looking to the Future: The Role of Imaging in the Treatment of AD

The search for therapies that can modify the course of AD—to slow, delay, or prevent it—is clearly our most important challenge. That search has in turn led to a search for imaging markers that can be used as outcomes in drug discovery and trials. The value of any imaging technology will ultimately be determined by its contribution to meeting the challenge of finding and using effective therapies. This value includes contributions toward diagnosis. The large variability, intrinsic to clinical outcomes in AD, means that studies relying purely on clinical measures are necessarily large and consequently very costly. Using clinical outcomes to power studies to establish meaningful disease-slowing effects may require complicated designs and thousands of subjects. A major aim in academia and industry has been to find biomarkers that could identify disease-slowing effects earlier and/or with significantly fewer subjects exposed to treatment. Imaging is being increasingly incorporated into trial designs to measure the effects of a therapy on fibrillary amyloid (with amyloid imaging) on atrophy (with MRI) and on metabolism (PET and fMRI).

As increasingly biologically active therapies are studied, so too have side effects increased. Imaging is emerging as a means of detecting potential adverse effects that can initially be clinically silent or go unrecognized because of a patient's level of cognitive impairment and confusion (Salloway et al. 2009). Particularly with more biologically active therapies, regular monitoring, or so-called safety scans, are now a prerequisite in such trials.

The recognition that it may be necessary to intervene at a very early stage to effect disease modification has led to interest in “prevention” studies. Preclinical intervention studies, almost by definition, are difficult to power on clinical outcomes. Imaging and other biomarkers are likely to be needed to select subjects for these studies and to provide outcome measures that can assess whether therapies are having a disease-modifying effect that could potentially translate into a delay in clinical onset.

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