The Dissipative Particle Dynamics Simulation of Macromolecular Suspension in Micro-channels

ZHOU Lv-Wen¹*, LIU Mou-Bin²

1,2 Institute of Mechanics, CAS, Beijing 100190, China

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Abstract

This paper investigated the transport and conformation of macromolecules in microchannels using the dissipative particle dynamics (DPD) and finite extensible non-linear elastic (FENE) bead spring chains model. The dynamic behavior of macromolecules with different number of beads and different chain length in three kinds of micro-channels, straight quadrate contraction sloping contraction micro-channel are comparatively analyzed. It is found that the macromolecules tend to drag the simple DPD particles, reducing their velocity, and leading to density fluctuations. The dragging effect is more important as the number of macromolecules or the length of the macromolecular chain increases.

1 Introduction

Understanding the dynamic behavior of macromolecules, such as DNA, is very important for fundamental research and practical applications in bio, chemical and medical engineering, especially in the designing micro-devices. Recently, micro-devices enable processing, analyzing, and delivering biochemical materials in a wide range of biomedical and biological applications[1, 2].

2 Methodology of the dissipative particle dynamics

In Dissipative particle dynamics system, a particle is represented a cluster of molecules or small regions of fluid material. The forces between particles are assumed to be pair-wise additive. The motion of DPD particles is governed by Newton's equations of motion. For simple DPD particle i, we have the governing equations

$$\frac{\mathrm{d}r_i}{\mathrm{d}t} = v_i, \quad \frac{\mathrm{d}v_i}{\mathrm{d}t} = \sum_{j \neq i}^{N} f_{ij_i}^{\mathrm{ext}}$$
(1)

^{*}zhou.lv.wen@gmail.com

Where r_i and v_i denote the position and velocity of particle i. The mass of the all DPD particle has been taken to be the same and unity; and f_{ij} denote the total force between particles i and j. f_i^{ext} is the external force, such as the gravity. The inter-particle force f_{ij} consists of three parts, namely: conservative force F_{ij}^C , dissipative force F_{ij}^D and random force F_{ij}^R .

$$\mathbf{F}_{ij}^{C} = \begin{cases} a_{ij} (1 - r_{ij}/r_c) \widehat{\mathbf{r}}_{ij} & r_{ij} < r_C \\ 0 & r_{ij} \ge r_C \end{cases}$$
 (2)

3 Parameters

To construct a working DPD, we need select values of some necessary parameters. In this section, we will talk abut how to select model parameters' values. Table 1 listed the some model parameters that we need determined before we could sufficient to construct a working DPD system. For a simple single component DPD system, we just set all particles' mass to be unity, and cutoff radius is also set to be unity.

Table 1: Model parameters

Model parameters	Symbol	Value
Mass of DPD particle	m	unity
Cutoff radius of DPD particle	r_C	unity
Simulation time step	Δt	
Friction coefficient	γ	$\sigma = 2\gamma k_b T$

4 Channel flow of FENE chain suspension

We use DPD particles and FENE chains to model the suspension of macromolecules in three kinds of micro-channels. Quadrate contraction micro-channel and sloping contraction micro-channel are comparatively analyzed. The conformation evolution of macromolecules passing through quadrate contraction micro-channel and sloping contraction micro-channel at t=4000 are show in figure 1 and figure 2 respectively.

5 Conclusion

Our numerical results show that macromolecules are mainly concentrated in the middle channel. Macromolecules tend to drag simple fluid particles, reducing their velocity, and leading to density and velocity fluctuations. The dragging effect is more important as the number of macromolecules or the length of the macromolecular chain increases.

The conclusions of this paper is very important for fundamental research and practical applications in bio, chemical and medical engineering. By control the flow of macromolecular suspensions, which carried drugs and DNA molecules, we can efficiently and precisely deliver a small amount of drug or DNA into local tissue, skin regions, and even cells.

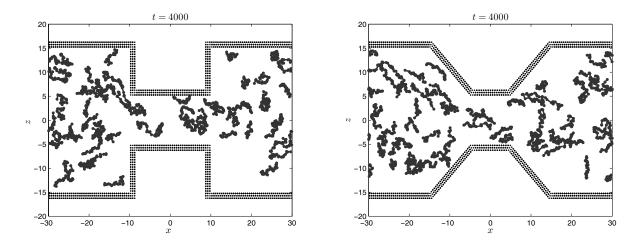


Figure 1: Quadrate contraction micro-channel Figure 2: Sloping contraction micro-channel

Acknowledgements

I would like to thank LIU Mou-Bin.

References

- [1] K. Chun, G. Hashiguchi, H. Toshiyoshi, and H. Fujita, "Fabrication of array of hollow microcapillaries used for injection of genetic materials into animal/plant cells," Jpn. J. Appl. Phys., Part 2 38, L279(1999).
- [2] Fan X, Phan-Thien N, Yong N T, Wu X, Xu D. "Microchannel flow of a macromolecular suspension". Phys Fluids, 2003, 15(1): 11-21

Appendices

A Latex Code

```
1 % copyright by Zhou Lvwen. zhou.lv.wen@gmail.com
2 \documentclass[12pt,a4paper]{article} % 文档说明[字号,纸张类型]{文档类型}
 \usepackage {amsmath, fancyhdr, graphicx, appendix, lastpage, extramarks, array}
5 \usepackage{listings}
6 \usepackage {xcolor}
7 \usepackage{attachfile2}
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                        =1in, \pm = 1.2in, \top = 1in
9 \usepackage [left=0.8in,right=0.8in,top=1.2in,bottom=1in] {geometry}
11 \usepackage {xeCJK}
 %\usepackage{fontspec}
12
13 \setCJKmainfont[BoldFont=simhei.ttf]{simsun.ttf}
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15 \setlength {\parskip} {2pt}
16
17 % 定义页眉: 左页眉{中文姓名, 学号}, 便为老师打分, 所以这里用中文姓名
           中页眉{英语学术论文写作}为课程名称
18 %
           右页眉{第X页,共X页}
19
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21 \chead {英语学术论文写作(排版作业)}
22 \rhead{第\ \thepage\ 页,{~} 共\ \protect\pageref{LastPage} 页}
24 % 注: 各位同学改改页边距, 段落间距及页眉. 别搞得大家版式一样
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 \definecolor{hellgelb}{rgb}{0.96,0.96,0.96}
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43
      showstringspaces=false,%
44
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45
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      numbersep=1em,%
47
      breaklines=true,%
48
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49
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第5页, 共7页

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52
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53
                 xrightmargin=\fboxsep%
54
55 }
56
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59 \title{The Dissipative Particle Dynamics Simulation of Macromolecular
        Suspension in Micro-channels % 论文标题
61 % 作者\\单位
62 \author{ZHOU Lv-Wen$^1$\footnote{zhou.lv.wen@gmail.com}, LIU Mou-Bin$^2$\\
                      \textit{$^{1,2}}$Institute of Mechanics, CAS, Beijing 100190, China}}
63
                                                                                                        % 写作日期,省略则为当前计算机日期
     \date{July 1, 2012}
64
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66
69 \begin{abstract}
                                                                                                       % 摘要
70 This paper investigated the transport and conformation of macromolecules in
        micro-channels using the dissipative particle dynamics (DPD) and finite
         extensible non-linear elastic (FENE) bead spring chains model. The dynamic
         behavior of macromolecules with different number of beads and different
         chain length in three kinds of micro-channels, straight quadrate contraction
           sloping contraction micro-channel are comparatively analyzed. It is found
        that the macromolecules tend to drag the simple DPD particles, reducing
         their velocity, and leading to density fluctuations. The dragging effect is
         more important as the number of macromolecules or the length of the
        macromolecular chain increases.
     \end{abstract}
    % ......
72
73
74 \section{Introduction}
                                                                                                        % 引言
     Understanding the dynamic behavior of macromolecules, such as DNA, is very
           important for fundamental research and practical applications in bio,
           chemical and medical engineering, especially in the designing micro-devices
            . Recently, micro-devices enable processing, analyzing, and delivering % \left( 1\right) =\left( 1\right) \left( 
           biochemical materials in a wide range of biomedical and biological
           applications\cite{KChun,FanX}.
76
77 | %........
78 \section{Methodology of the dissipative particle dynamics} 发文
79 In Dissipative particle dynamics system, a particle is represented a cluster
        of molecules or small regions of fluid material. The forces between
         particles are assumed to be pair-wise additive. The motion of DPD particles
         is governed by Newton's equations of motion. For simple DPD particle $i$,
        we have the governing equations
80 \begin{equation}
81 \frac{d}{r_i}{\mathbf{d}t} = v_i, , , , , , 
82 \left| \frac{d}{v_i}{\mathbf{d}v_j} \right| = \sum_{j=0}^{n} f_{ij_{i}}^{\mathbf{d}v_j}
83 \end{equation}
84 Where $r_i$ and $v_i$ denote the position and velocity of particle $i$. The
        mass of the all DPD particle has been taken to be the same and unity; and $f
         _{ij}$ denote the total force between particles $i$ and $j$. $f_i^{\mathrm{}}
         ext}}$ is the external force, such as the gravity. The inter-particle force
         f_{ij}\ consists of three parts, namely: conservative force F_{ij}^c,
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dissipative force $F {ij}^D$ and random force $F {ij}^R$.
85
  \begin{equation}
86
  \mathbf{F}_{ij}^{C}=\begin{cases}
a_{ij}(1-r_{ij})/r_{c})
89 0 & r_{ij} \neq r_{C}
  \end{cases}
91
  \end{equation}
92
  \section{Parameters}
93
95 To construct a working DPD, we need select values of some necessary parameters
    . In this section, we will talk abut how to select model parameters' values.
    Table \ref{parameters} listed the some model parameters that we need
    determined before we could sufficient to construct a working DPD system. For
     a simple single component DPD system, we just set all particles' mass to be
     unity, and cutoff radius is also set to be unity.
96 \begin{table}[!htb]
97 \centering
  \caption{\label{parameters}Model parameters}
  \begin{tabular}{|1|1|1|}
| 100 | \textbf{Model parameters} & \multicolumn{1}{c|}{\textbf{Symbol}} & \
   multicolumn{1}{c|}{\textbf{Value}} \\
  \hline
101
102 Mass of DPD particle & \multicolumn{1}{c|}{$m$} & \multicolumn{1}{c|}{unity}
103 \hline
Cutoff radius of DPD particle & \multicolumn{1}{c|}{$r_C$} & \multicolumn{1}{c}
   |}{unity} \\
105 \hline
  Simulation time step & \multicolumn{1}{c|}{$\Delta t$} & \multicolumn{1}{c|}{}
  \hline
107
Friction coefficient & \multicolumn{1}{c|}{$\gamma$} & \multicolumn{1}{c|}{$\
   sigma=2\gamma k_bT$} \\
109 \hline
  \end{tabular}
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  \end{table}
111
112
  \section{Channel flow of FENE chain suspension}
113
114
115 We use DPD particles and FENE chains to model the suspension of macromolecules
    in three kinds of micro-channels. Quadrate contraction micro-channel and
    sloping contraction micro-channel are comparatively analyzed. The
    conformation evolution of macromolecules passing through quadrate
    contraction micro-channel and sloping contraction micro-channel at $t =
    4000$ are show in figure \ref{chainT} and figure \ref{chainY} respectively.
116
117 \begin{figure}[!htb]
118 \centering
119 \begin{minipage}[c]{0.5\textwidth}
120 \centering
  \includegraphics[width=0.85\textwidth]{./figures/chainT4000s.pdf}
  \caption{\label{chainT} Quadrate contraction micro-channel}
123 \end{minipage}%
124 \begin{minipage}[c]{0.5\textwidth}
125 \centering
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126 \includegraphics [width=0.85\textwidth] {./figures/chainY4000s.pdf}
  \caption{\label{chainY} Sloping contraction micro-channel}
128 \end{minipage}
  \end{figure}
130
  131
132
133
                                       % 结论
  \section{Conclusion}
134
Our numerical results show that macromolecules are mainly concentrated in the
   middle channel. Macromolecules tend to drag simple fluid particles, reducing
    their velocity, and leading to density and velocity fluctuations. The
   dragging effect is more important as the number of macromolecules or the
   length of the macromolecular chain increases.
136
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   practical applications in bio, chemical and medical engineering. By control
   the flow of macromolecular suspensions, which carried drugs and DNA
   molecules, we can efficiently and precisely deliver a small amount of drug
   or DNA into local tissue, skin regions, and even cells.
138
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139
                                      % 致谢
  \section*{Acknowledgements}
  I would like to thank LIU Mou-Bin.
141
142
144 \begin{thebibliography}{99}
                                     % 参考文献
145 \bibitem {KChun} K. Chun, G. Hashiguchi, H. Toshiyoshi, and H. Fujita, ``
   Fabrication of array of hollow microcapillaries used for injection of
   genetic materials into animal/plant cells,'' Jpn. J. Appl. Phys., Part 2 38,
    L279(1999).
  \bibitem{FanX} Fan X, Phan-Thien N, Yong N T, Wu X, Xu D. ``Microchannel flow
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