

## Non-invasive Brain-Computer Interfaces: Enhancing Applicability using Computational Intelligence and Technological Advances

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## Presentation outline

- State-of-the-art non-invasive BCI
- R&D challenges
- CI approaches to handling challenges
- Laboratory facilities
- EEG-based Post-stroke rehabilitation
- MEG-based Post-stroke rehabilitation
- Conclusions and further R&D challenges

## **Background**

- Brain-computer Interface a direct communication pathway between a human brain and a computer.
- Mainly useful for patients suffering from motor impairments: world-wide about 10M stroke sufferers; approx. 40k SCI patients in UK alone.
- A broad range of promising applications such as alternative augmentative communication (AAC) systems for environmental control, tele-robotics & mobility, and neuro-rehabilitation systems involving prosthetics and/or orthotics/exoskeletons.
- However because of <u>high brain signal non-stationarity</u> and other <u>practical issues</u>, BCI systems have found limited practical use.

## **Types of BCI**

- Invasive techniques
  - Using micro-electrodes or electro-corticogram (ECoG).
  - Electrodes are implanted directly onto a patient's brain.
  - Need for surgery; may cause scar, and materials issues.
  - Ethical issues; risk of infection.
- Noninvasive techniques
  - Using EEG, MEG, NIRS, and/or fMRI.
  - External sensors for availing brain signals.
  - Susceptible to noise.
  - Most widely used is EEG being easy to use, low cost & portable.

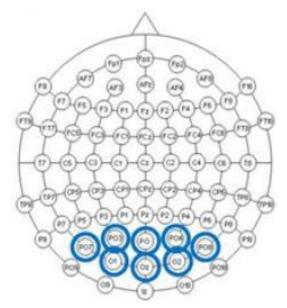


Photo Courtesy: University of Utah Department of Neurosurgery



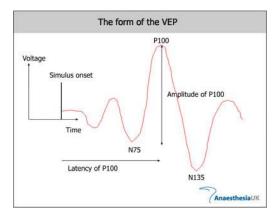
#### Non-invasive BCI Categorisation based on Mental Tasks

- Visually Evoked Potential (VEP): SSVEP most common
- P300
- Sensorimotor activity



Top View of the brain Electrode placement



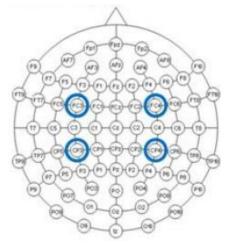


Potential changes of the occipital EEG under stimulation of light

## Non-invasive BCI Categorisation....

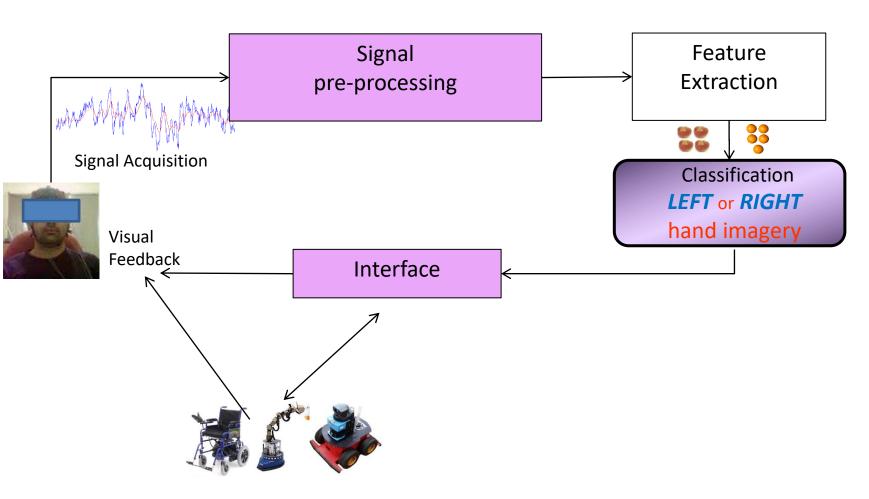
#### Sensorimotor

Sensorimotor rhythm (SMR) (e.g., mu rhythm) gets modulated when a person imagines to move (i.e. motor imagery by a healthy person), intends to move (e.g., by a disable person), or actually moves his/her right and/or left hand, tongue, or foot.



If we can **decode** the information from brain to <u>display human thinking</u>, we can design a very intuitive and natural communication channel.

## Operational Block Diagram of a BCI



### **Critical Performance Limiting Factors**

#### **Human Factors**:

Brain signals change due to mood, fatigue, attention, motivation, medications, sensory stimuli, circadian rhythms, progression of disease, and amount of practice.

Head movements and eye blinking may cause artefacts.

#### *Machine Factors*:

Electromagnetic (EM) noise may affect recordings.

For EEGs, impedance changes due to sweating, drying gel, electrode placement variation, surface metal degradation, and lead wear.

### **Laboratory facilities...**

#### NI Functional Brain Mapping facility

- A joint investment of £5.3M from Invest Northern Ireland (INI) and UU
  equipped with the latest whole head 306 channels Elekta Neuromag MEG
  TRIUX system. First MEG on island of Ireland, about 200 worldwide.
- Magneto-encephalography (MEG) records magnetic field induced by brain activities across the whole scalp while maintaining much higher spatial and temporal resolution.
- Research focus:
  - Improved understanding of dynamics of human brain signal processing;
  - Neurological disorders, stroke, Alzheimer's disease, and epilepsy.
- Outputs:
  - More effective diagnostic tools for early diagnosis;
  - More effective prevention or intervention measures;
  - Collaborative development of Biomarkers;
  - Enhanced software tools for more automated medical image analysis.



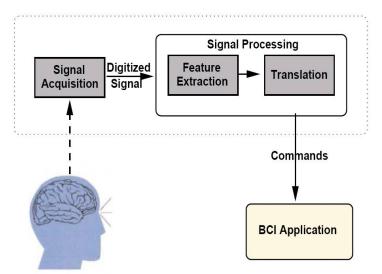
### Some R&D works addressing challenges

- Rapid selection of user-specific parameters and intelligent pre-processing [e.g. data analytics for optimal channel selection (*Roy et al. (2020), J Neural Eng*); signal pre-processing using SOFNN or recurrent Quantum NN (Gandhi et al. (2013), *IEEE T NN & Learning Sys*)]
- Optimal methods for feature extraction [e.g. PSD (Herman et al. (2008), IEEE T Neural Sys Rehab Eng.) & bi-spectrum (Shahid & Prasad (2011), J Neural Eng)];
- Adaptable and robust classifier design and transfer learning [e.g. Interval Type-2 Fuzzy Logic (Herman et al. (2017), IEEE T Fuzzy Sys); Riemannian geometry based tangent Space (Gaur et al. (2019), IJNS), Deep learning (Roy et al. (2020), Frontiers in Neuroscience].
- Multi-modal BCI through multi-sensor integration combining EMG, ECG, and/or eye-tracker [e.g., EEG-EMG Correlation based feature (*Choudhury et al. (2019), J Neuroscience Methods*)]
- Appropriate user interface (visual and auditory) development for neurofeedback and accomplishing tasks such as text entry, web-page access, wheelchair/mobile robot control, and stroke rehabilitation & related game playing [e.g., Auditory NFB (McCreadie et al. (2014) IEEE T Neural Sys Rehab Eng.)]

Integration of BCI and robotic exoskeleton: A way forward

for neuro-rehabilitation

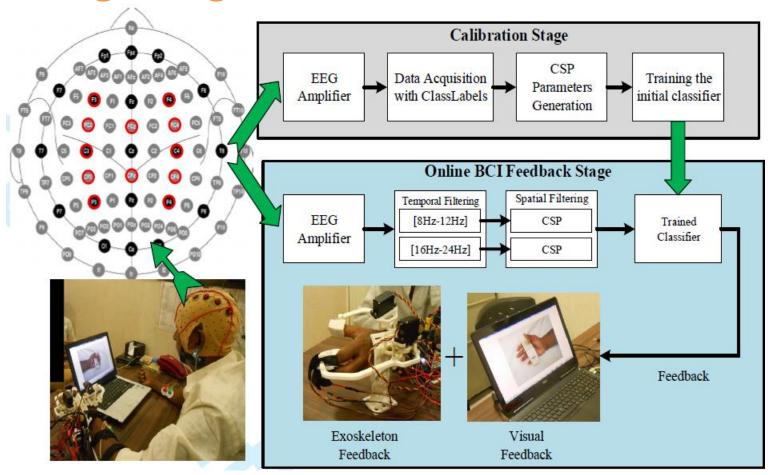
- Robots administer <u>repetitive exercises</u> but may not be sufficiently engaging for neuroplasticity to occur due to:
  - lack of interactive and engaging user interface.
- A symbiotic fusion of BCI and robot can facilitate:
  - Engaging and natural user interface;
  - Capturing of patient's attention while allowing intense repetition of therapeutic task, causing <u>neuroplasticity</u>;
  - Reliable quantification of patient's performance and recovery process;
  - Applicability to wide range of motor impairments.





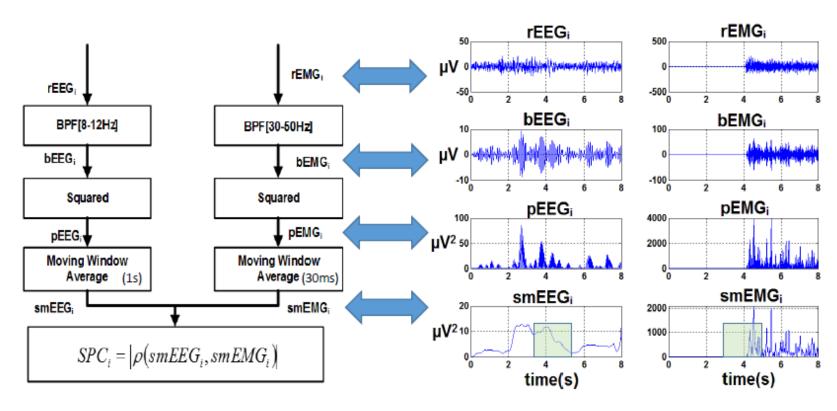
## Completed RTD:

## Integrating EEG-based BCI and Exoskeleton



- Features: CSP; Cortico-muscular coherence (CMC) / EEG-EMG band-limited power time-courses (CBPT) Correlation;
- Feature Classifier: SVM

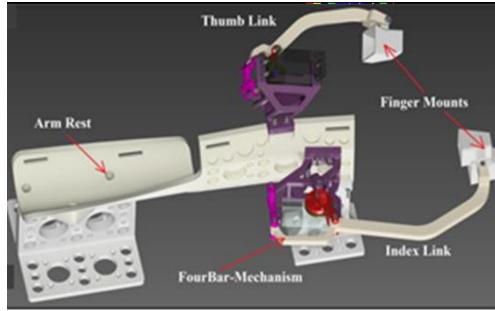
## Cortico-Muscular-Coupling...



EMG signal from the flexor-digitorum-superficialis (FDS) muscle

### A Participant using the Neuro-rehabilitation System





[Chowdhury et al. (2018), IEEE T Cognitive and Developmental Systems]

## **Pilot Clinical Trial**

- > Participant Selection Criteria
  - Stroke patients with partial or full finger motion disability.
  - Time since stroke not less than 6 months.
  - MMSE score more than 21/30.
- > Experimental Protocol [Prasad et al., 2010]
  - Assist-as-needed Physical Practice (30 min).
  - BCI based Mental Practice (30 min).
  - 2/3 therapy sessions per week; Six week long.
  - Four stroke (ischemic) (1 male, 3 females, mean time after stoke:23(4.6) months, MMSE score:28.34(±1.25)).
  - Recovery outcome measures:
    - Action Research Arm Test (ARAT) (1-57): Grip(1-57),
       Pinch(18), Grip(12), Grasp(18), Gross movement(9).
    - Grip Strength.

## Pilot Clinical Trial...

**Demographics of the Patients** 

| Sub id | Age<br>(years) | gender | Imp<br>aired<br>side | Domin<br>ant<br>Side | Time<br>Since<br>Stroke<br>(months) | Minimental<br>State Test<br>Score |
|--------|----------------|--------|----------------------|----------------------|-------------------------------------|-----------------------------------|
| P01    | 61             | F      | R                    | R                    | 22                                  | 30/30                             |
| P02    | 56             | M      | L                    | R                    | 28                                  | 30/30                             |
| P03    | 69             | F      | R                    | R                    | 24                                  | 30/30                             |
| P04    | 59             | F      | L                    | R                    | 19                                  | 30/30                             |

## Pilot Clinical Trial...

#### Physical Practice (PP):

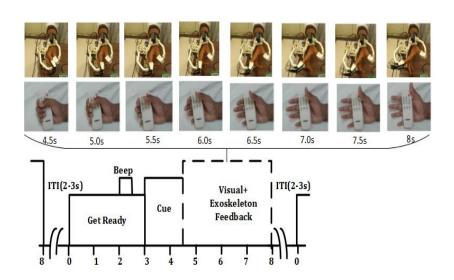
- Repetitive finger flexion and extension exercise in assist-asneeded mode for 30 min
- Strategy implemented by a force threshold based switching between active non-assist and passive assistance mode.
- Participants applied finger-tip force is converted into exoskeleton motion using an impedance model if force is above a certain threshold level (active non-assist mode).
- Switches to passive assistance mode providing full assistance when the applied force is below the threshold.
- The difficulty level of the PP is adjusted by updating the impedance parameters according to the average force generation ability.

## Pilot Clinical Trial...

#### **≻**Mental Practice

BCI system 16 channel EEG/EMG g.USBamp system from

g.tec

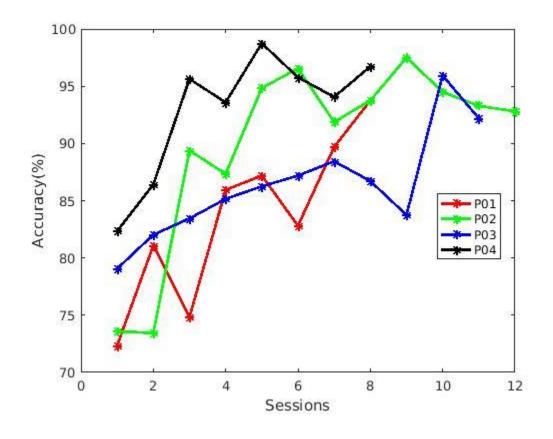


Visual neurofeedback along with paradigm timing diagram.

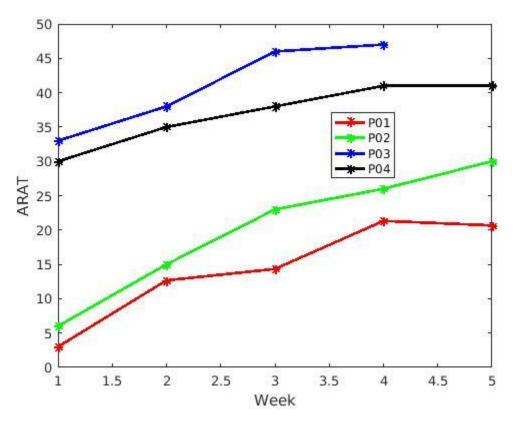


A Patient undergoing the trial

## Change in BCI Classification Accuracy

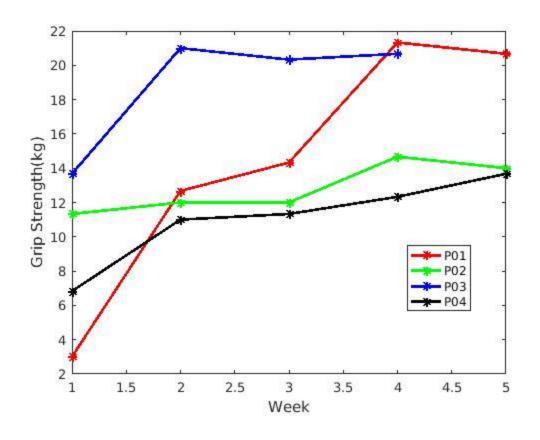


#### **Clinical Outcome Measure: Action Research Arm Test (ARAT)**

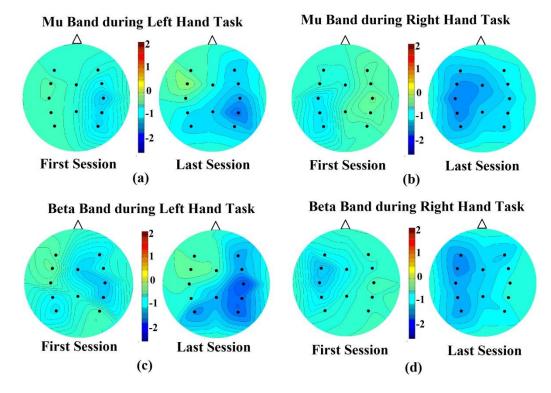


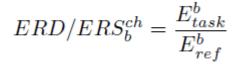
All the participants achieved Minimal clinically important difference (MCID) in their ARAT.

### **Clinical Outcome Measure: Grip Strength**



## Scalp Topoplots for ERD/ERS Changes



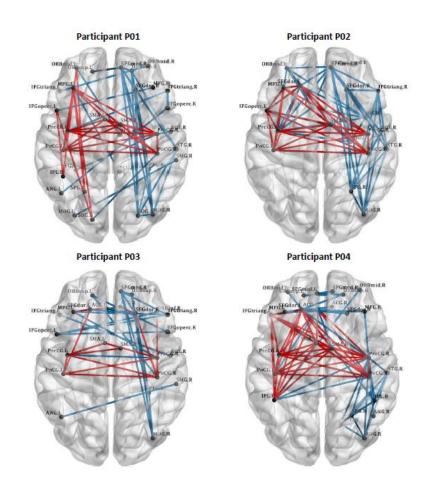


- Both mu and beta band ERD increased from first to the last session
- Significant pre vs post ERD changes in EEG :

Mu band Left Task: CP4; Mu band Right Task: C3, CP3

Beta band Left Task: C4; Beta band Right Task: F3 and FC3

## Resting State beta band connectivity change in MEG – A Neuroplasticity Analysis



Left -> Ipsilesional hemisphere

- Functional connectivity (FC) clusters correlated positively (Red) and negatively (Blue) with the hand functional recovery index for all four participants in beta-low frequency band (15-26 Hz).
- ➤ The intra-hemispherical FC values in M1, S1, and SMA within both ipsilesional and contralesional hemispheres increase with UL functional recovery.
- ➤ The ipsilesional hemisphere possesses larger number of positively correlated clusters.
- ➤ The inter-hemispherical FC analysis showed a stable pattern of positively correlated connections within the motor cortical regions whereas the inter-hemispheric negative cluster is variable across the participants.

### **Advancing MEG-based BCI Supported Neurorehabilitation**

#### -MEG Issues:

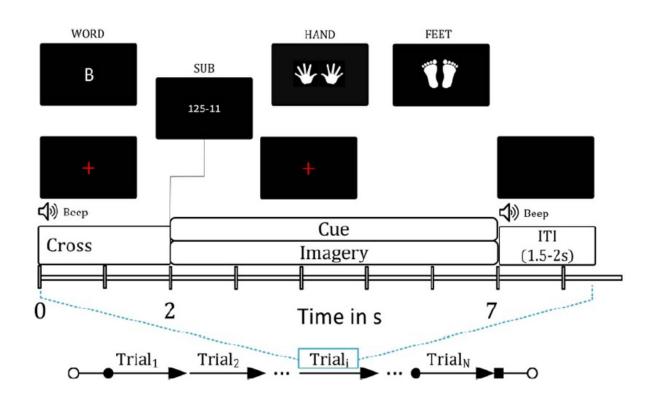
- Highest spatiotemporal resolution (204 gradiometer & 102 magnetometer channels, Triux, Elekta, recorded at 1k Hz) of all neuroimaging modalities.
- Sensors in a dedicated helmet rather than physically placed on subjects' scalps resulting in significant signal attenuation.
- Low decoding accuracy, despite using large number of channels.
- For MEG-based BCI no channel selection methodology has been reported.
  - UKIERI phase-3 project: Advancing MEG-based Brain-Computer Interface Supported Upper Limb Post-Stroke Rehabilitation (DST UKIERI 2016 -17 -128, PI, £145k, 2017 –21).

## Channel Selection Procedure using Cl

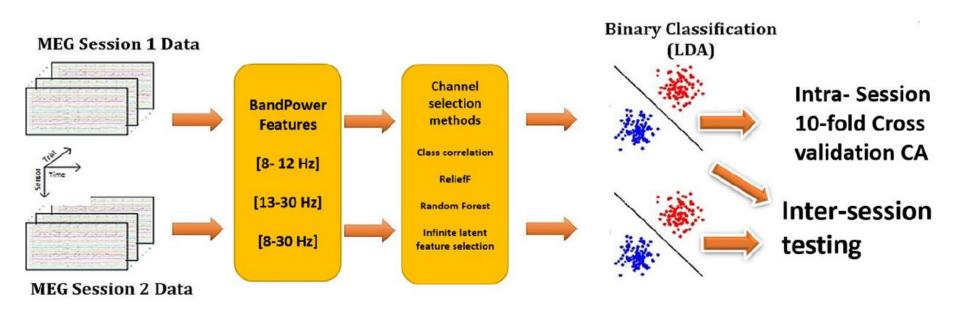
- Timing paradigm design for data recording;
- MEG data recorded for two sessions from 15 healthy participants performing mixed imagery tasks pairs;
- Data preprocessing bad channels removed.
- Channel selection methods Class-Correlation, ReliefF, Random Forest, and Infinite Latent Feature Selection were applied across six binary tasks in three different frequency bands;
- Features: Bandpower and common spatial pattern (CSP)
- Feature classification using Linear Discriminant Analysis (LDA) classifier.

Roy, Rathee, Chowdhury, McCreadie, & Prasad (2020). Assessing impact of channel selection on decoding of motor and cognitive imagery from MEG data. *Journal of Neural Engineering*, 17(5).

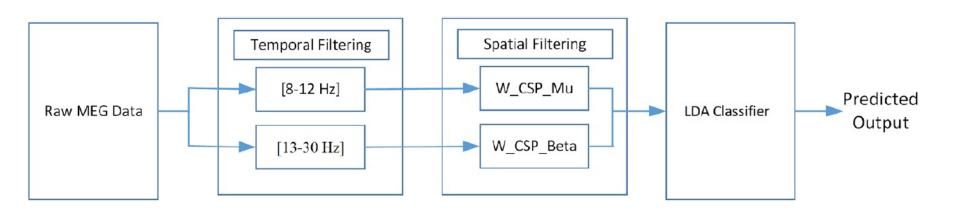
# Timing diagram of MEG-based BCI paradigm



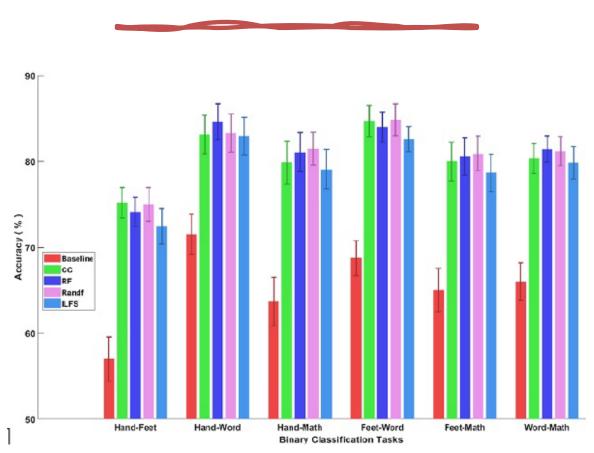
## Schematic diagram of signal processing pipeline using bandpower feature



# The data processing pipeline using CSP

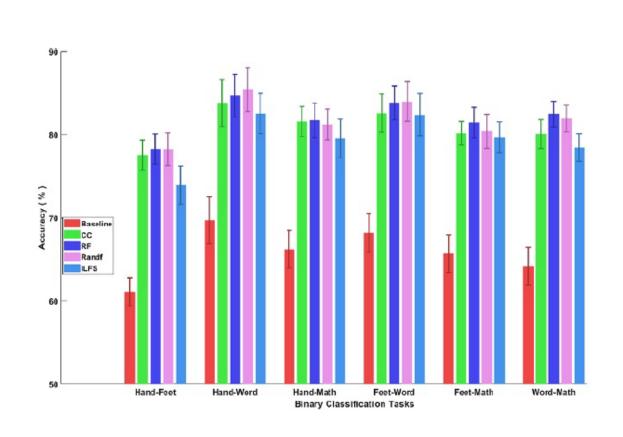


## Mean classification accuracies (CAs) for $\alpha$ band (8-12 Hz) for session-1 using 10-fold cross-validation.

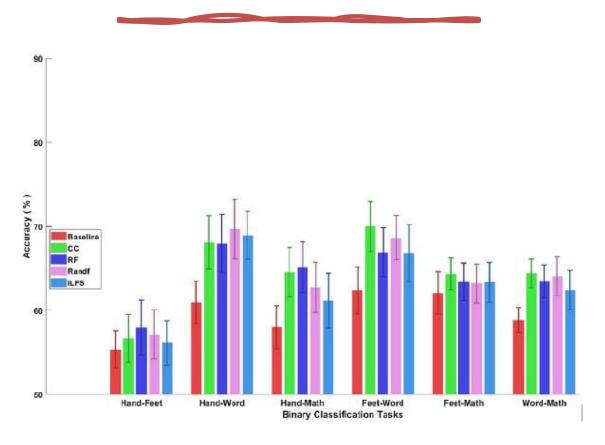


- RandF provided a statistically significant improvement over ILFS in H-F, H-M, W-M, F-W and W-M task pairs (p < 0.05).
- Overall mean CA across subjects using RandF is 81.11% (±6.02), ILFS is 79.30% (±6.51), CC is 81.72% (±6.25), and RF is 81.14% (±6.22) for session 1 whereas baseline was 65.32% (±8.09).

## Mean CAs for the $\alpha$ band (8-12 Hz) for session-2 using 10-fold cross-validation



# Mean classification accuracies (CAs) for α band for a classifier trained on session-1 data and tested on session-2 data

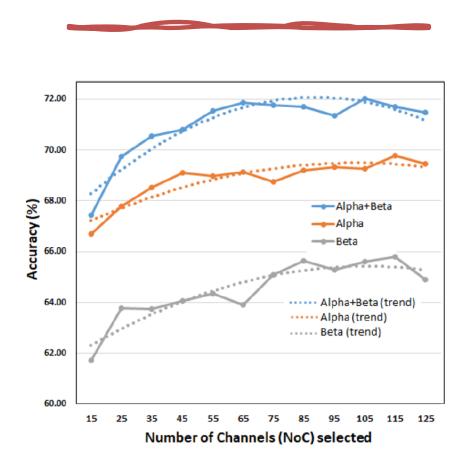


H-W group provided higher accuracy than the MI (H-F) group.

# Number of channels contributing to maximum accuracy using RandF method in $\alpha+\beta$ band using bandpower feature

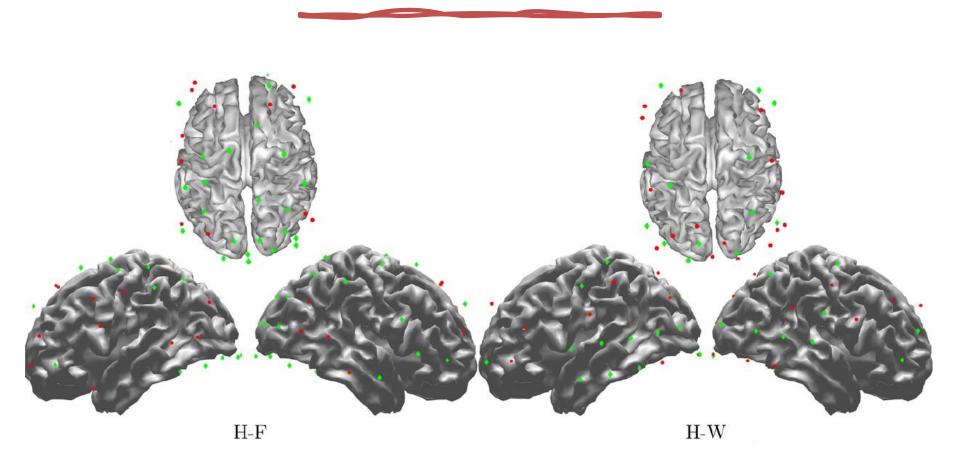
| Participants | Hand vs Foot |      | Hand vs Word |      | Hand vs Math |       | Feet vs Word |             | Feet vs Math |       | Math vs Word |     |
|--------------|--------------|------|--------------|------|--------------|-------|--------------|-------------|--------------|-------|--------------|-----|
|              | S01          | S02  | S01          | S02  | S01          | S02   | S01          | <i>S</i> 02 | S01          | S02   | S01          | S02 |
| P01          | 7            | 7    | 14           | 5    | 16           | 5     | 9            | 7           | 14           | 19    | 11           | 12  |
| P02          | 13           | 11   | 14           | 4    | 23           | 12    | 15           | 12          | 6            | 15    | 9            | 9   |
| P03          | 10           | 8    | 10           | 13   | 10           | 12    | 9            | 9           | 8            | 8     | 14           | 13  |
| P04          | 14           | 11   | 5            | 13   | 8            | 14    | 14           | 16          | 17           | 1     | 12           | 10  |
| P05          | 9            | 9    | 14           | 9    | 7            | 21    | 5            | 6           | 8            | 6     | 16           | 9   |
| P06          | 14           | 6    | 24           | 15   | 11           | 15    | 18           | 17          | 14           | 9     | 18           | 6   |
| P07          | 16           | 6    | 19           | 11   | 14           | 10    | 11           | 10          | 6            | 9     | 14           | 6   |
| P08          | 13           | 12   | 13           | 14   | 9            | 14    | 13           | 10          | 8            | 12    | 10           | 21  |
| P09          | 22           | 12   | 18           | 9    | 13           | 13    | 16           | 9           | 13           | 2     | 13           | 9   |
| P10          | 4            | 13   | 9            | 16   | 10           | 12    | 15           | 18          | 10           | 16    | 18           | 6   |
| P11          | 16           | 11   | 9            | 12   | 14           | 14    | 19           | 18          | 14           | 7     | 12           | 14  |
| P12          | 9            | 19   | 2            | 12   | 3            | 7     | 17           | 12          | 7            | 12    | 9            | 6   |
| P13          | 13           | 11   | 16           | 7    | 10           | 13    | 10           | 11          | 3            | 8     | 5            | 4   |
| P14          | 7            | 5    | 12           | 8    | 15           | 14    | 10           | 5           | 6            | 20    | 7            | 2   |
| P15          | 11           | 18   | 16           | 8    | 9            | 11    | 16           | 18          | 8            | 13    | 11           | 11  |
| Mean         | 11.87        | 10.6 | 13           | 10.4 | 11.47        | 12.47 | 13.13        | 11.87       | 9.47         | 10.47 | 11.93        | 9.2 |

## Mean transfer-session accuracy with the channels selected using CSP in all the three bands



If we feed the CSP with a larger NoC it can optimize the CSP projection matrix very well which could lead to higher discriminability between the two classes.

## Plot of channels common for minimum of three participants' imagery tasks for 8–30 Hz



represents channels in session 01

& represents channel in session 2.

## Main Findings of MEG-based BCI Performance Analysis

- Channel selection improved intra-session BCI CA significantly but intersession CA improvement is marginal.
- The optimal channel number varied not only in each session but also for each participant.
- Reducing the NoC helps to decrease the computational cost and maintain numerical stability in cases of low trial numbers.
- For all combinations, the mixed imagery task pairs (H-W, H-M, F-W & F-M)
  provided higher separability as compared to the H-F and W-M task pairs in
  α band.
- Findings support that the suppression of alpha band power around 10 Hz is a stronger marker for movement planning, execution and imagery than beta band.
- It resulted into substantial channel reduction, from 204 channels to:
  - a range of 1–25 channels using bandpower as a feature and
  - 15-105 channels using common spatial pattern (CSP) features.
- Roy, Rathee, Chowdhury, McCreadie, & Prasad (2020). Assessing impact of channel selection on decoding of motor and cognitive imagery from MEG data. *Journal of Neural Engineering*, 17(5).

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## **Conclusion**

- Neurorehabilitation system integrating BCI and a hand exoskeleton.
- BCI neurofeedback of motor imagery practice enhances rehab effectiveness and patient focus.
- BCI brain activations in EEG/MEG trigger hand exoskeleton to provide active rehab exercises.
- Exoskeleton proprioceptive neurofeedback enhances BCI effectiveness for focused mental practice of rehab tasks.
- Completed Pilot trial demonstrated enhanced effectiveness through a six week clinical trial on four hemiplegic stroke patients; functional recovery gain in terms of GS and ARAT scores and other transformative change in stroke participants.
- Significantly enhanced decoding accuracy obtained on MEG-based BCI using computational intelligence techniques for channel selection.
- Trials are on-going on the Neurorehabilitation System using MEGbased BCI controlled exoskeleton.

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