

Simulations in emission tomography using GATE

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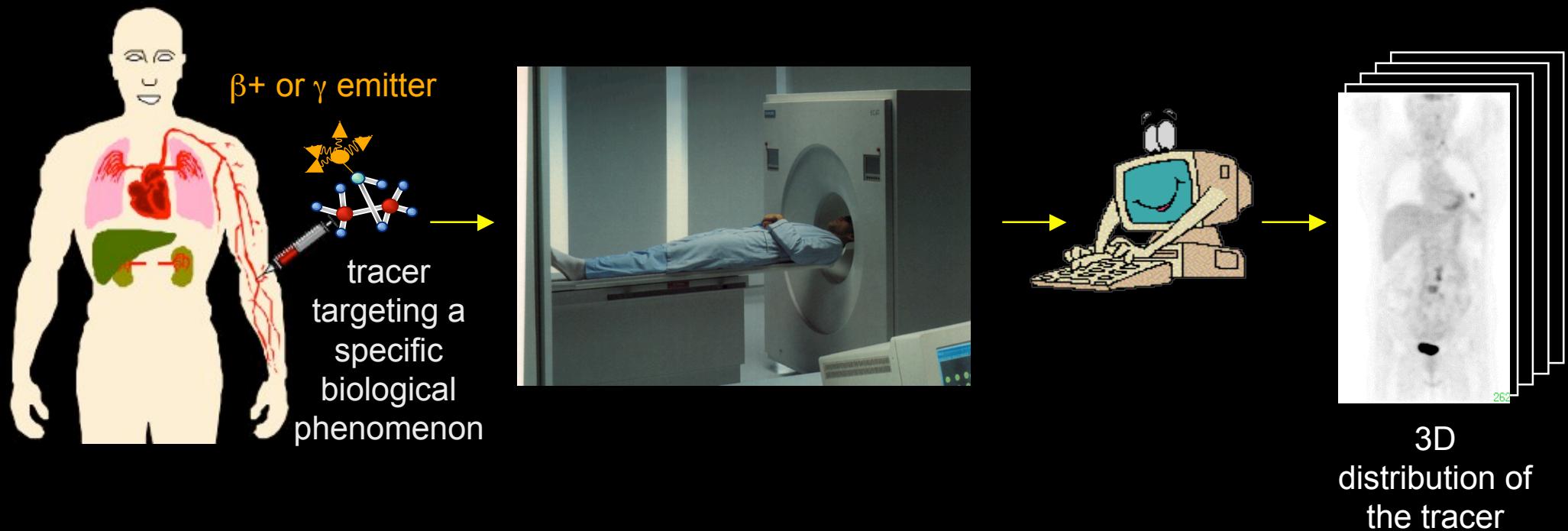
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Outline

- Emission tomography and need for simulations
- GATE short history and main features
- Usefulness of GATE for assisting in detector design :
 - Flexibility
 - Modeling of time dependent processes
 - Modeling the electronic response
 - Others
- Current priorities in the development of GATE
- Conclusion

Emission tomography in functional imaging

Non invasive techniques for assessing the in vivo distribution of a radiotracer administered to a patient



γ emitter: Single Photon Emission Computed Tomography (SPECT)

β^+ emitter: Positron Emission Tomography (PET)

Need for simulations in emission tomography

- Scanner design, protocol optimization, image reconstruction, (scatter) corrections, dosimetry (for image guided radiotherapy), etc
- Monte Carlo simulations are widely used in addition to analytical simulations and phantom experiments
- No standard code, but about 15 different codes, many of them “home made”

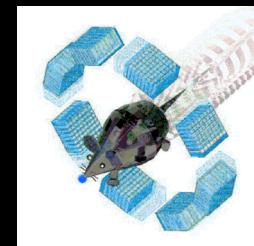


SimSET



SIMIND

Geant 4



GATE

Penelopet
Sorteo
PET-EGS
...

- Various types of users (medical physicists, research scientists...), not necessarily with a strong background in particle physics

GATE short history

- July 2001:
 - 2-day brainstorming meeting on Monte Carlo simulations in Paris involving French and European labs
 - Decision to develop a new code, based on GEANT4, to overcome the limitations of existing codes
- December 2001:
 - First developments of the code, with 4 labs deeply involved at first (EPFL Lausanne, LPC Clermont Ferrand, University of Ghent, U494 Inserm Paris)
- Early 2002:
 - Creation and development of the OpenGATE collaboration
 - More and more labs joined the collaboration, up to 23 today, and worked on the development of the code and the preparation of a public release
- May 2004:
 - First public release of GATE
- Yesterday (March 8th, 2007):
 - 953 registered users

GATE today: technical features

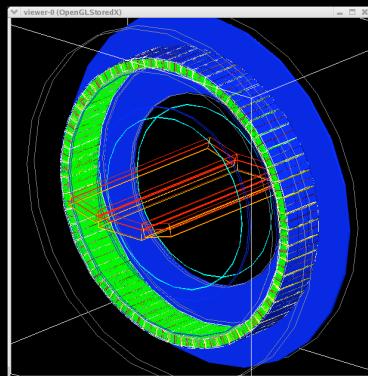
- Based on GEANT 4
- Written in C++
- Can be run on many platforms (Linux, Unix, MacOs)
- User-friendly: simulations can be designed and controlled using macros, without any knowledge in C++
- Appropriate for SPECT and PET simulations
- Flexible enough to model almost any detector design, including prototypes
- Explicit modeling of time (hence detector motion, patient motion, radioactive decay, dead time, time of flight, tracer kinetics)
- Can handle voxelized and analytical phantoms
- Modular design: new extensions easily added

GATE today: practical features

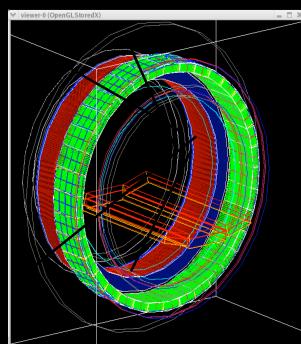
- Can be freely downloaded, including the source codes (registration required, LGPL license)
- On-line documentation, including FAQ and archives of all questions (and often answers) about GATE that have been asked so far
- Help about the use of GATE can be obtained through the gate-user mailing list
- Many commercial tomographs and prototypes have already been modeled and models have been validated
- Developed as a collaborative effort (23 labs worldwide)
- 2 public releases each year
- an official publication:
Jan S, et al. GATE: a simulation toolkit for PET and SPECT. Phys Med Biol 49: 4543-4561, 2004.
- Website: <http://www.opengatecollaboration.org>
- GATE workshops at the IEEE Medical Imaging Conferences (2003, 2004, 2005, 2006)
- GATE training sessions

Usefulness of GATE for assisting in detector design: flexibility

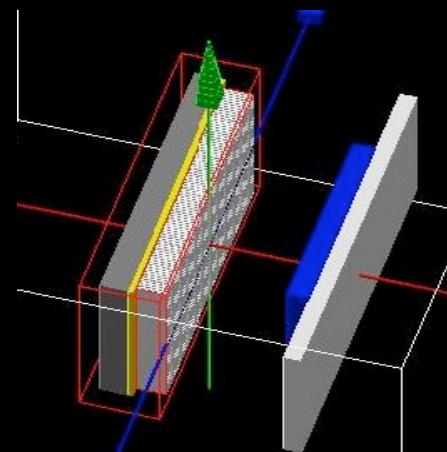
- 8 commercial PET systems, 4 commercial SPECT systems and 5 prototypes have already been modelled, including validation of the models



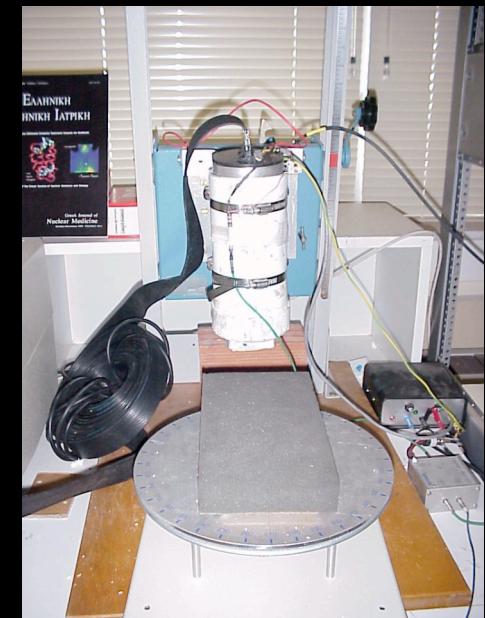
GE Advance/Discovery LS PET scanner
Schmidlein et al, Med Phys 2006



GE Advance/Discovery ST PET, 3D mode
Schmidlein et al. MSKCC



DST Xli camera
Assié et al, Phys Med Biol 2005

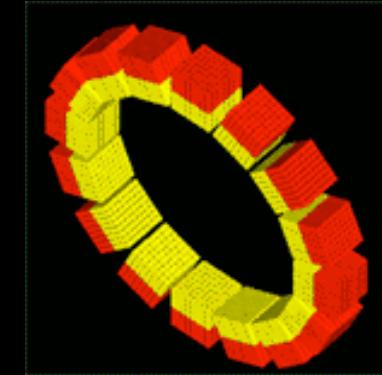


IASA CsI(Tl) gamma camera
Lazaro et al, Phys Med Biol 2004

Modeling time dependent processes in GATE

SPECT and PET intrinsically involves time:

- Change of tracer distribution over time (tracer biokinetic)
- Detector motions during acquisition
- Patient motion
- Radioactive decay
- Dead times of the detector
- Time-of-flight PET



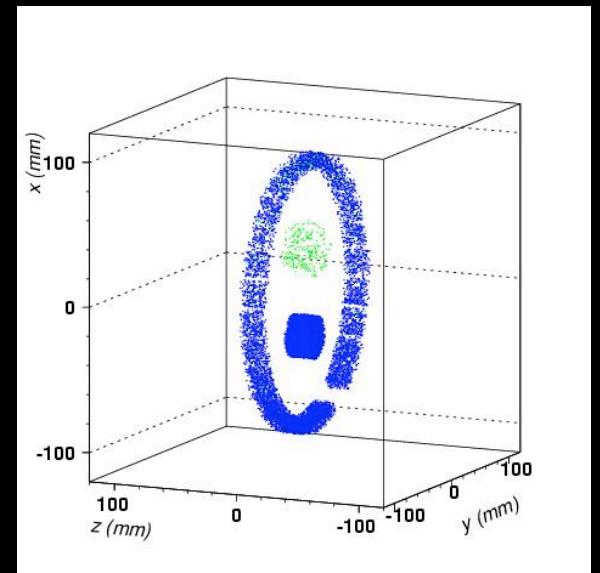
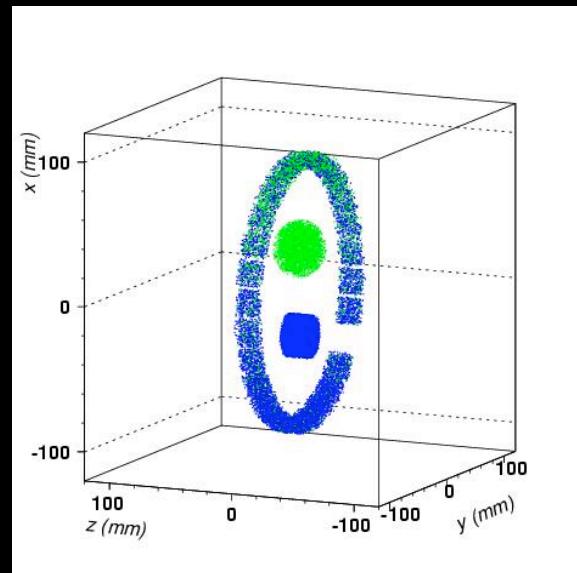
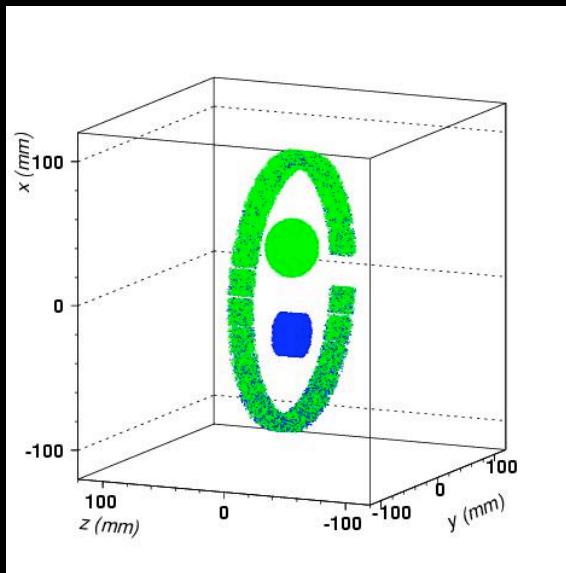
Principle of time modelling in GATE:

- Customized G4 radioactive decay module
- A clock models the time changes during the experiment
- The user defines the experiment timing (time slices)
- Time-dependent and synchronized objects are updated when time changes

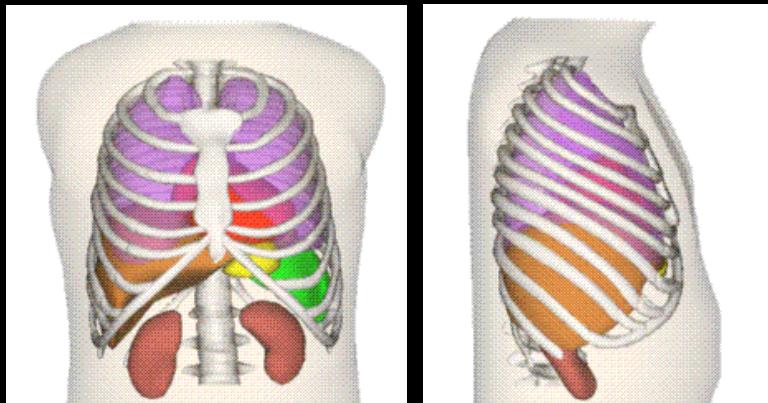
All of the above features can be modeled

Modeling of radioactive decay

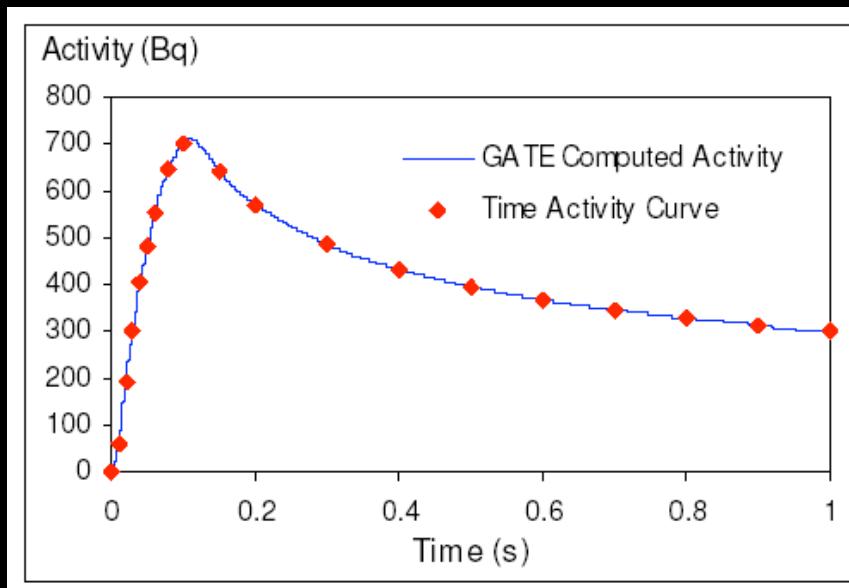
^{15}O (2 min)
 ^{11}C (20 min)



Modeling moving phantoms and change of tracer distribution



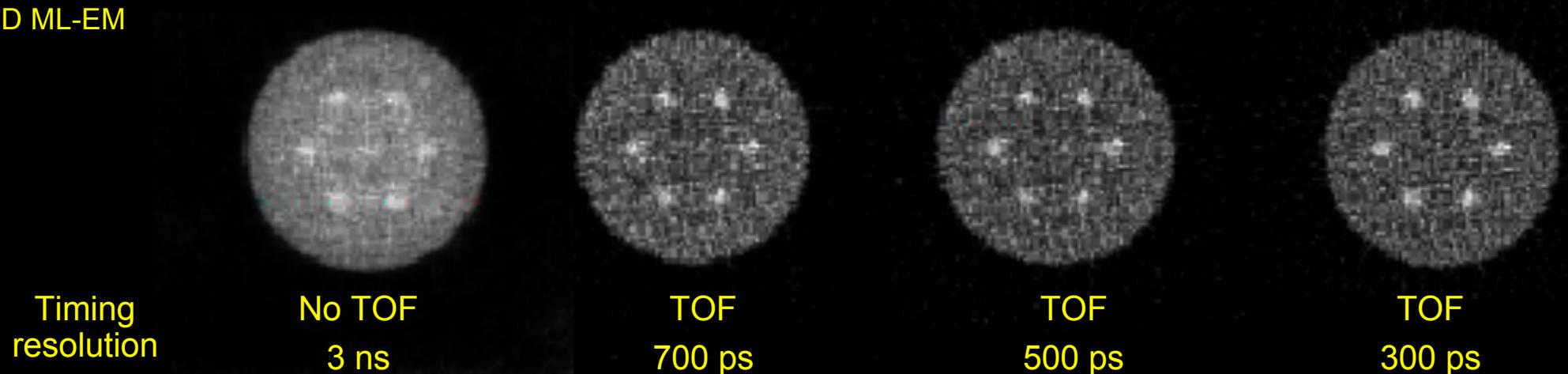
Segars et al, IEEE Trans Nucl Sci 2001



Descourt et al, IEEE MIC Conf Records 2006

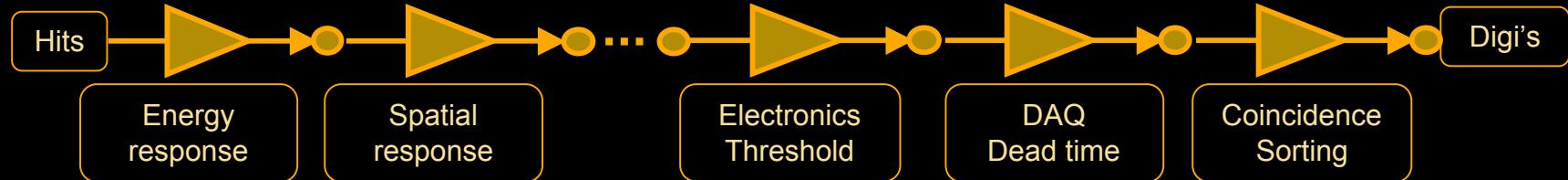
Modeling of time of flight PET

3D ML-EM



Timing resolution	No TOF 3 ns	TOF 700 ps	TOF 500 ps	TOF 300 ps
Type of study	Detector	Energy resolution (FWHM)	Low energy threshold (keV)	Coincidence time window (ns)
No TOF	GSO	15%	410	8
TOF	LaBr3	6.7%	470	6

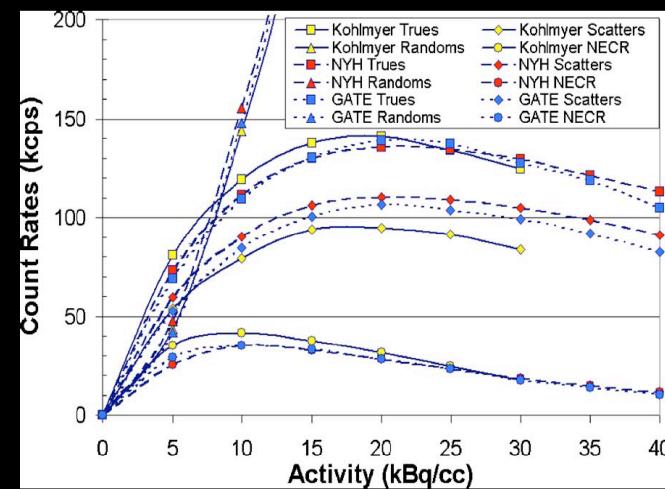
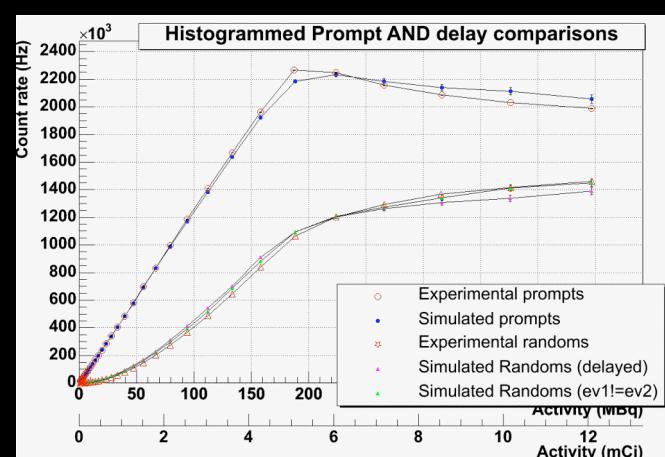
Modeling the electronic response of the system



Using the “digitizer”:

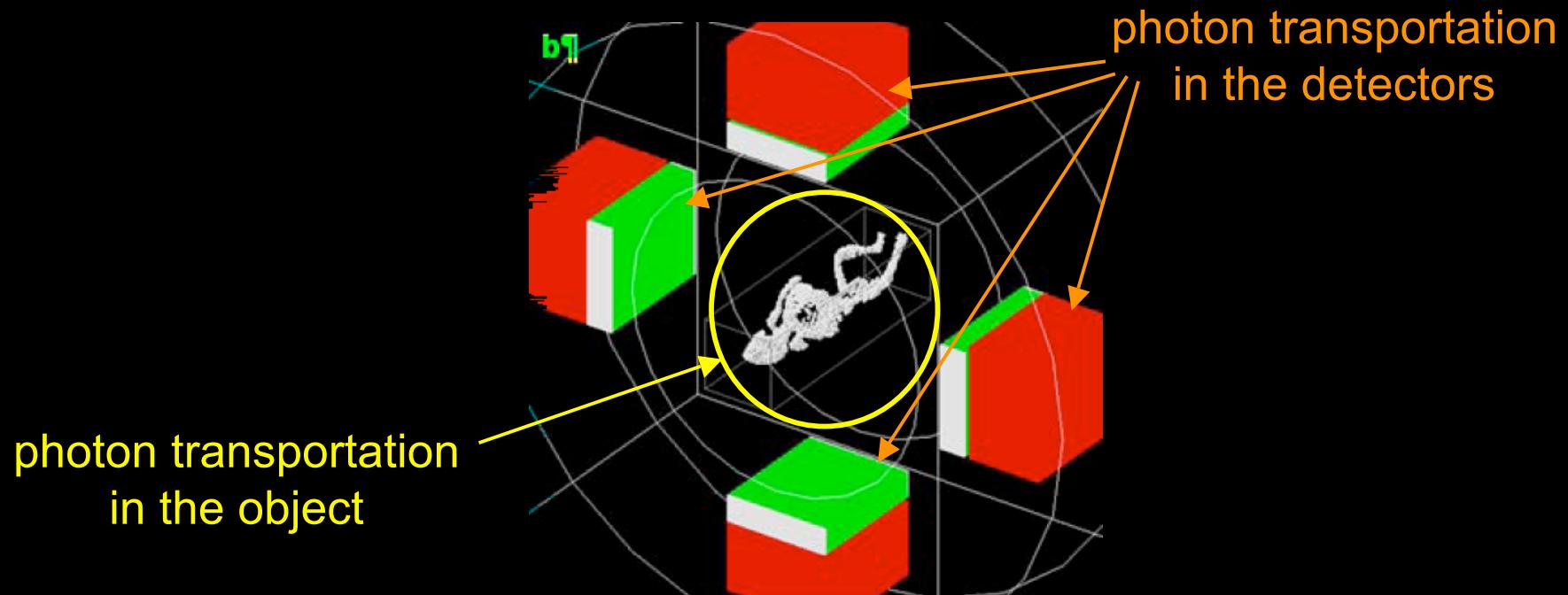
- Linear signal processing
- Modular (set-up via scripting)
- Several dead time models available

Makes it possible to accurately reproduce count rate curves



Other GATE features useful for helping in detector design

A simulation can be broken into 2 simulations*:

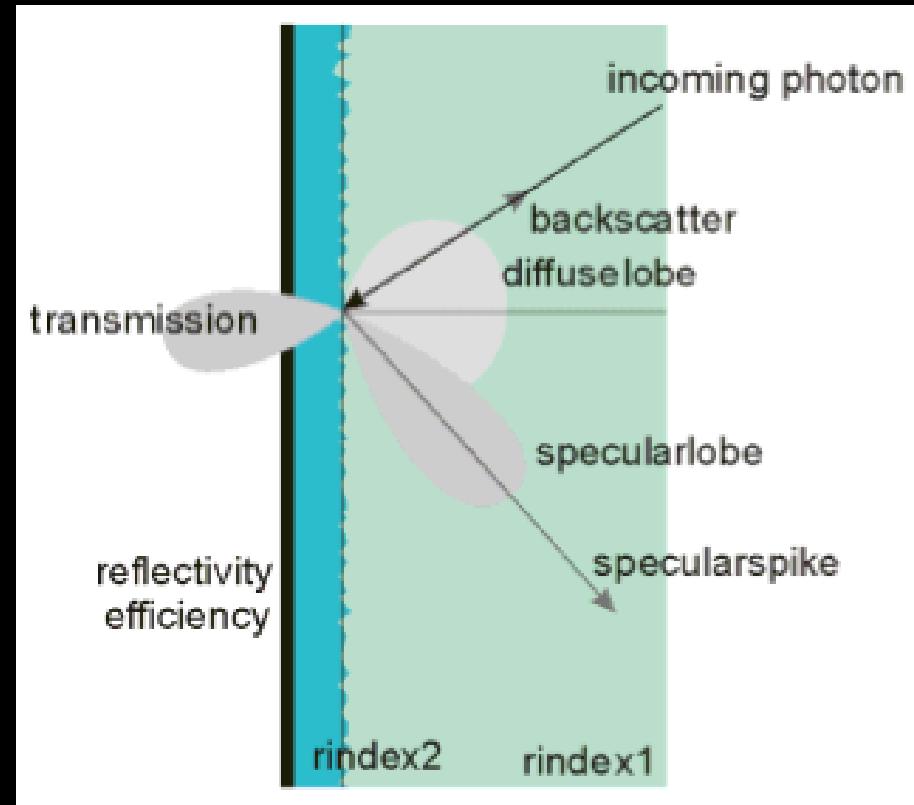
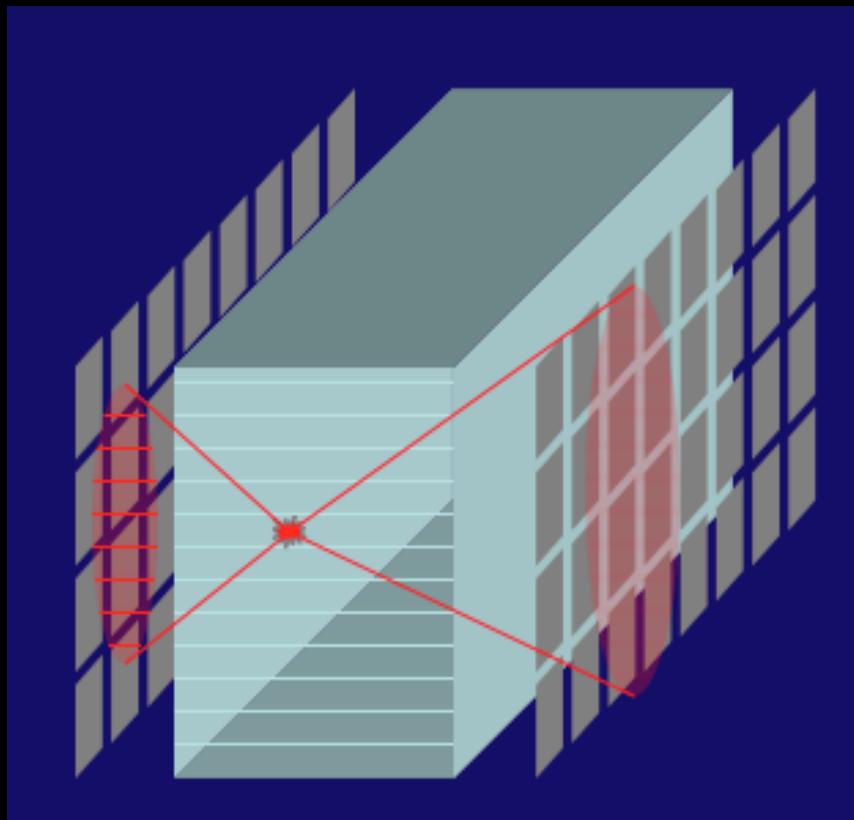


- Output from photon transportation in the object stored in a phase space
- Useful to test several detector designs without having to repeat the whole simulation through the object

* to be released soon

Other GATE features useful for helping in detector design

Tracking of optical photons in the crystal*



- Based on Geant4 classes

* currently available in GATE

Current priorities in GATE developments

- Improving the simulation throughput for efficient production of clinical and preclinical data*

Simulation time is the major problem with GATE and GEANT4

- Big “World”:
 - detectors have a “diameter” greater than 1 m
 - emitting object (e.g., patient) is large (50 cm up to 1.80 m)
 - emitting object is finely sampled (typically 1 mm x 1 mm x 1 mm cells)
 - voxelized objects are most often used
- Large number of particles to be simulated
 - low detection efficiency
 - in SPECT, typically 1 / 10 000 is detected
 - in PET, 1 / 200 is detected

More than 17000 h CPU are needed to model a realistic whole body PET scan

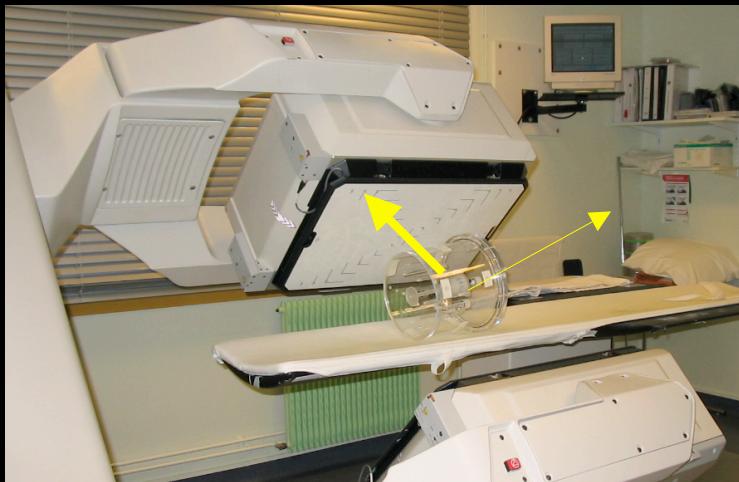
At least 4 approaches can be used to increase the throughput of the simulations

* Funded by the French ANR under contract ANR-06-C/S-004 (2007-2009)

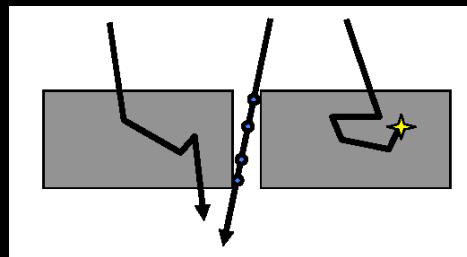
Improvement of simulation efficiency

Acceleration methods

- Variance reduction techniques such as importance sampling (e.g. in SimSET)
→ speed-up factors between 2 and 15



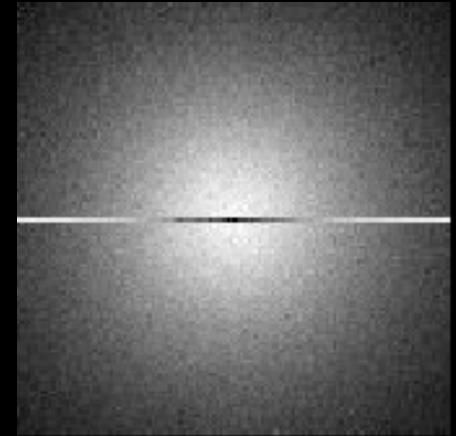
- Fictitious cross-section (or delta scattering)



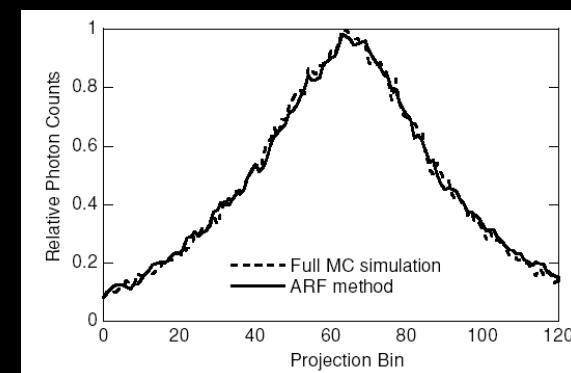
Combining MC with non MC models



Full MC



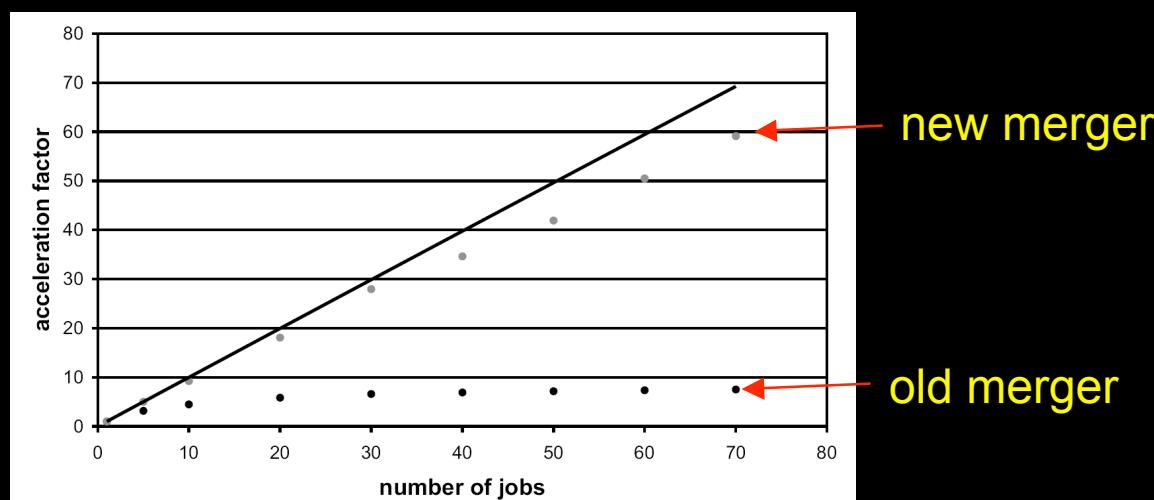
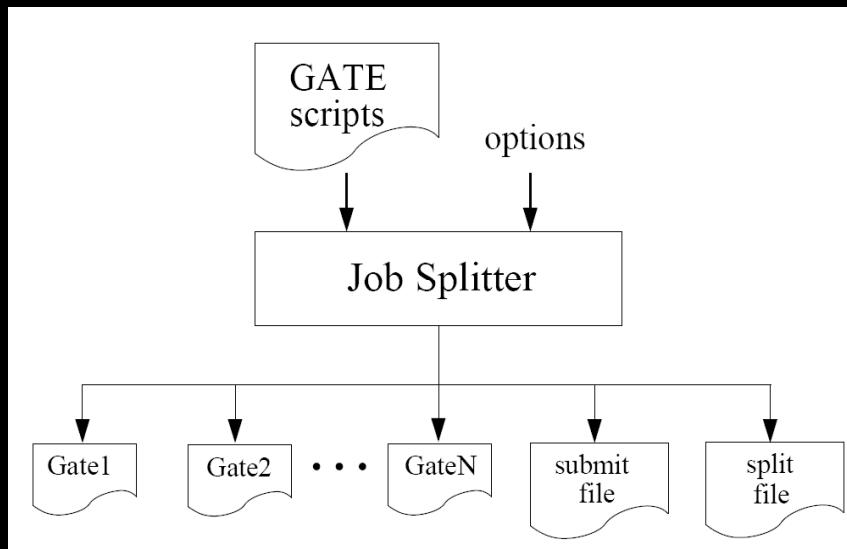
Collimator Angular Response Function



increase in efficiency > 100

Song et al, Phys Med Biol 2005

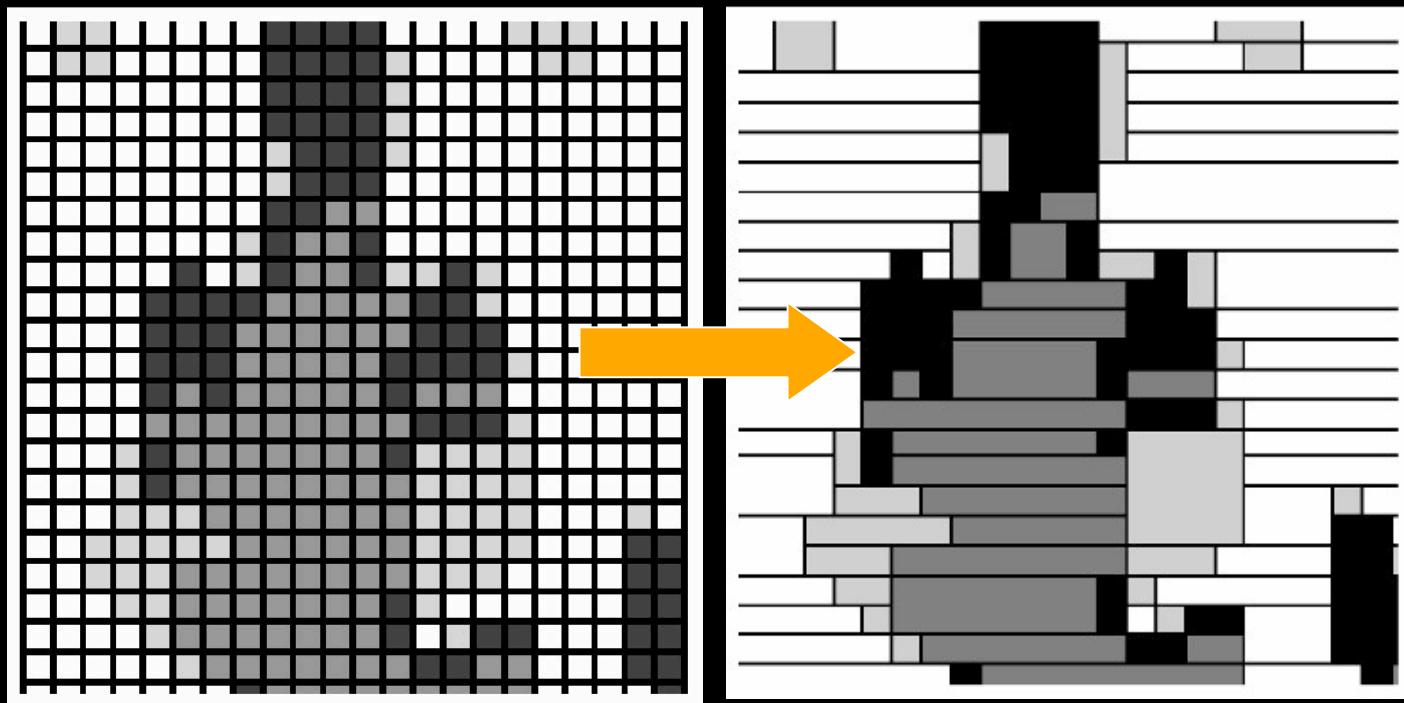
Parallel execution of the code on a distributed architecture



PET

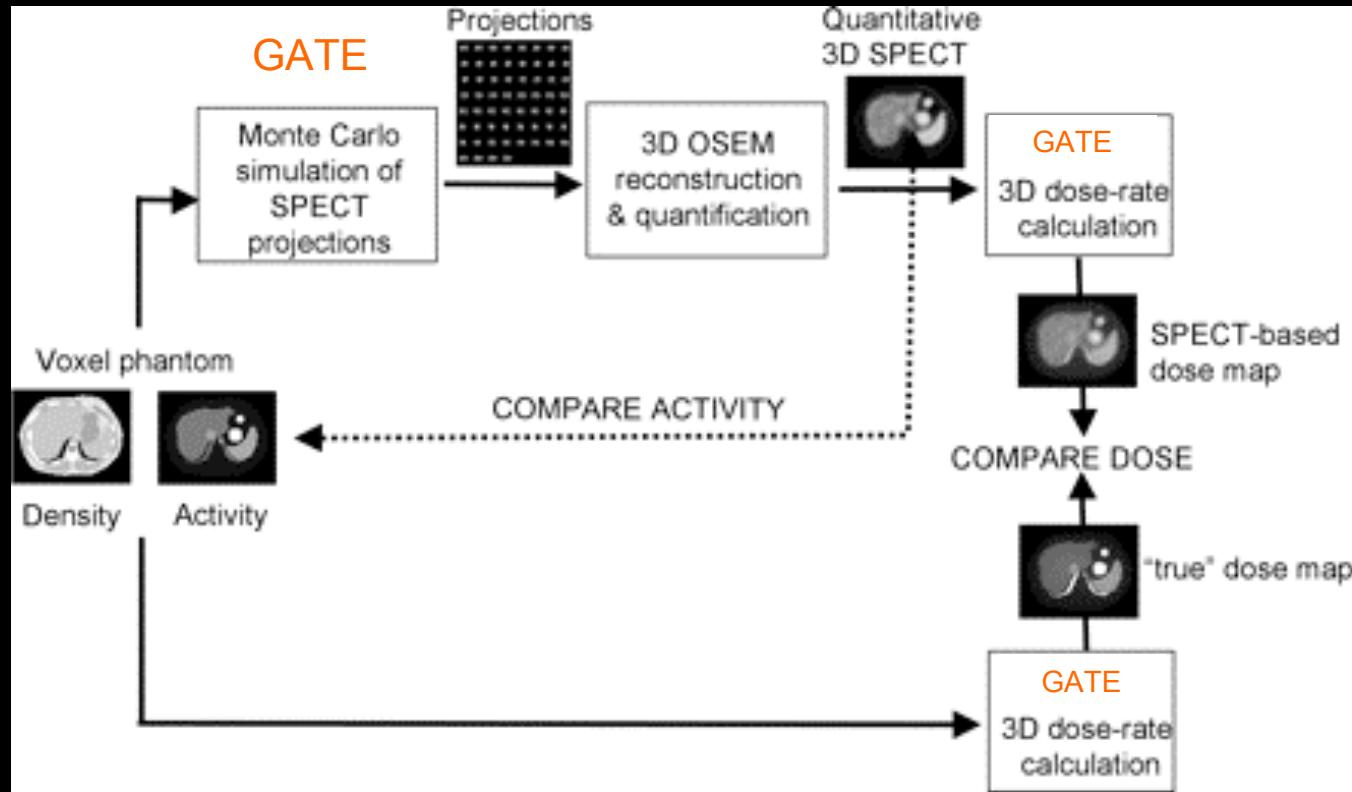
De Beenhouwer et al, IEEE MIC Conf Records 2006

Smart sampling



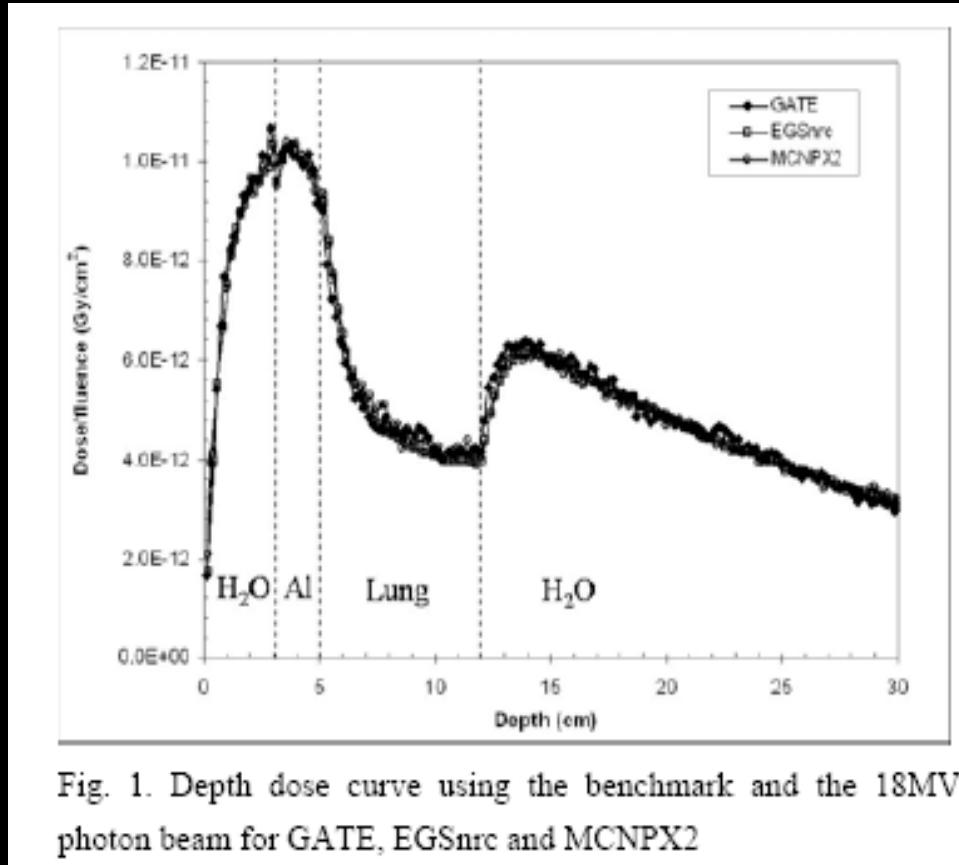
Taschereau et al, Med Phys 2006

Bridging the gap between MC modeling in imaging and dosimetry



- Calculation of dose maps are already possible in GATE
- Further validation studies are still needed (comparison with other dosimetry software)

Using GATE for dosimetry



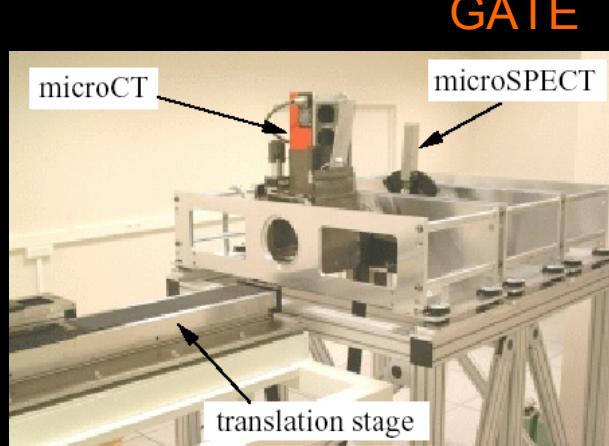
Visvikis et al NIM A 2006

Modeling hybrid machines (PET/CT, SPECT/CT, OPET)

PET/CT

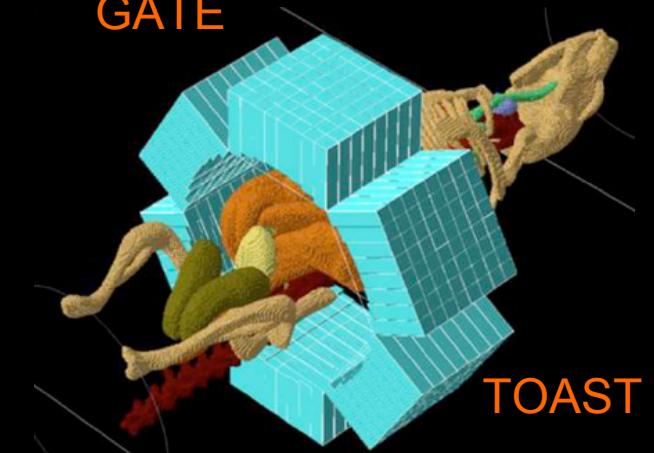


SPECT/CT



Brasse et al, IEEE MIC Conf
Rec 2004

OPET



Alexandrakis et al, Phys Med
Biol 2005

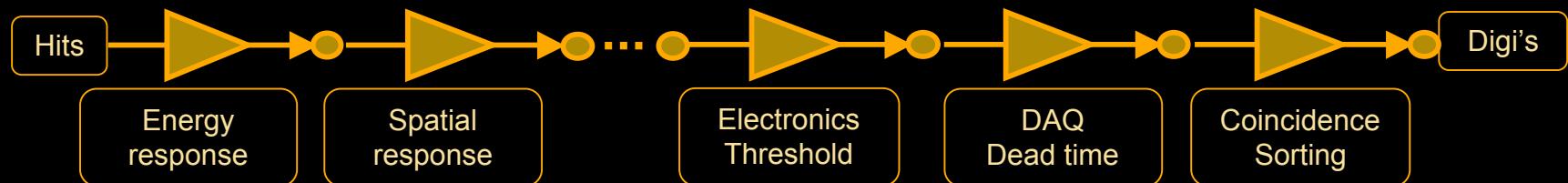
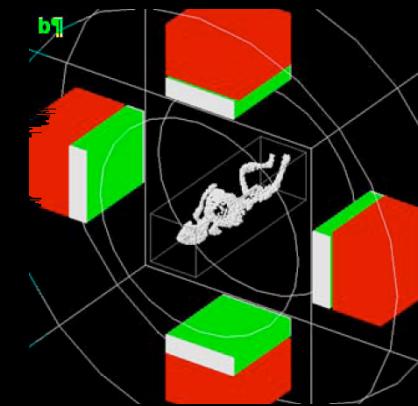
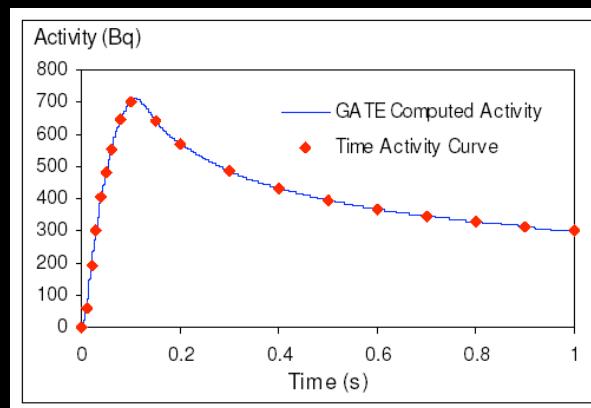
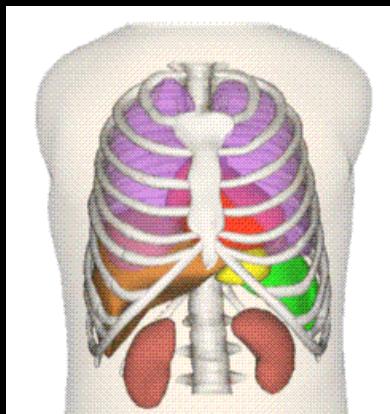
Integrating Monte Carlo modeling tools for:

- common coordinate system
- common object description
- consistent sampling
- convenient assessment of multimodality imaging

On-going studies regarding the use of GATE for CT simulations

Conclusion

- GATE is a relevant tool for Monte Carlo simulations in ET



- GATE is appropriate for studying detector designs and how they impact image quality in very realistic configurations (including movement for instance)

Acknowledgments

The OpenGATE collaboration

To know more about GATE

<http://www.opengatecollaboration.org>

[OpenGate Collaboration](#) [Registered users](#) [OpenGATE Collaboration](#)

GATE - Geant4 Application for Emission Tomography

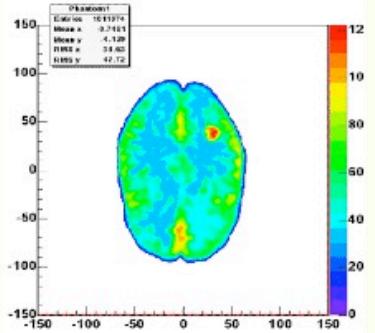
Overview



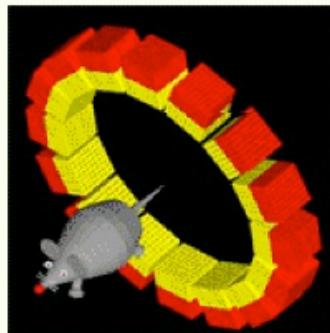
[Introduction](#)
[History](#)
[Source code, user support and documentation](#)
[Training](#)
[Publications](#)
[Systems already modelled with GATE](#)
[Benchmarks](#)
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GATE - Geant4 Application for Emission Tomography

NEW: GATE workshop at the [IEEE Medical Imaging Conference](#)



Diameter: 16.11974
Mean x: -0.7465
Mean y: -4.49
Mean z: 24.40
RMS x: 12.72



Voxelized Hoffmann brain phantom *Small animal PET scanner with movement implementation !*



Introduction

Emission tomography and especially PET has a fast growing importance in modern medicine for both diagnostic and treatment purposes. At the same time there is a demand for higher imaging quality, accuracy and speed. Both result in vast increase of the computational efforts in the field. Enhanced greatly by the wide availability of powerful computer clusters, Monte Carlo simulations

Answers to questions

PET systems already modeled by the OpenGATE collaboration

Scanner type	Studied FOM	Agreement	References
ECAT EXACT HR+, CPS	Spatial resolution Sensitivity Count rates Scatter fraction	about 3 % < 7 % good at activity concentrations < 20 kBq/ml about 3 %	Jan et al 2005
ECAT HRRT, Siemens	Spatial resolution Scatter fraction Scattered coinc profiles Count rates	excellent (<0.2 mm) < 1 % very good (visual) good (about 10%)	Bataille et al 2004
Hi-Rez, Siemens	Scatter fraction Count rates NEC curves	about 1 % good at activity concentrations < 40 Bq/ml good at activity concentrations < 40 Bq/ml	Michel et al 2006
Allegro, Philips	Count rate Scatter fraction	< 8 % 8 %	Lamare et al 2006
GE Advance, GEMS	Energy spectra Scatter fraction	not reported < 1 %	Schmidlein et al 2006
MicroPET P4, Concorde	Spatial resolution Sensitivity Miniature Derenzo phantom	about 7 % < 4 % visual assessment	Jan et al 2003
MicroPET Focus 220, Siemens	Spatial resolution Sensitivity Count rates for mouse phantom	about 5 % about 3 % prompt coinc: < 5.5 % delayed coinc: < 13 %	Jan et al 2005
Mosaic, Philips	Scatter fraction Count rates	about 5 % 4-15 %	Merheb et al 2005

Answers to questions

SPECT systems already modeled by the OpenGATE collaboration

Scanner type	Studied FOM	Agreement	References
IRIX, Philips	None reported	n/a	Staelens <i>et al</i> 2004
AXIS, Philips	Spatial resolution Energy resolution Energy spectra Sensitivity Scatter profiles	< 5 % < 1 % visual assessment < 4.6 % visual assessment	Staelens <i>et al</i> 2003
DST Xli, GEMS	Energy spectra Spatial resolution Sensitivity	excellent < 2 % in air, < 12 % in water < 4 %	Assié <i>et al</i> 2005
Millennium VG Hawk-Eye, GEMS	I131 energy spectra Spatial resolution for I131	excellent (visual) acceptable (<3mm)	Autret <i>et al</i> 2005

Answers to questions

Prototypes already modeled by the OpenGATE collaboration

Scanner type	Studied FOM	Agreement	References
Solstice, Philips	Sensitivity	good with theoretical data	Staelens et al 2003 Staelens et al 2004 Staelens et al 2004
LSO/LuYAP phoswich PET	Sensitivity NEC curves	n/a n/a	Rey et al 2003
ATLAS	Spatial resolution Sensitivity Line phantom	< 6 % < 10 % visual assessment	Chung et al 2004 Chung et al 2005
CsI(Tl) SPECT camera	Energy spectra Energy resolution Spatial resolution Scatter fraction Sensitivity Line phantom	good < 1 % < 1 % < 2 % < 2 % visual assessment	Lazaro et al 2004
OPET	Spatial resolution Sensitivity	n/a n/a	Rannou et al 2004

Answers to questions

The list of systems that have already been modeled by the collaboration can be found on the Web site
<http://www.opengatecollaboration.org>.

The specific macros corresponding to these models are not provided, as they include some parameters the companies do not want us to divulge, so please contact the group that has designed the macro (info on the GATE Web site) to see how you can get the macro.

Answers to questions

Data produced by GATE could be gathered in a public database, so that researchers interested in such data would not have to re-do the simulations. Such databases already exist (see next slide), although the data they contain have not been simulated using GATE, but using other Monte Carlo simulation software.

Using Monte Carlo for feeding database

<http://www.ibfm.cnr.it/mcet/index.html>

The MC-ET database				
#	Description of study	Scanner	Available Data	Total events
► 1	18FDG Brain study: normal subject	GE-Advance	Sinograms	3318047
► 2	18FDG thorax study: thyroid tumour with metastases in the abdomen	GE-Advance	Sinograms	1210779
► 3	18F NEMA uniform cylinder: 20x18 cm	GE-Advance	Sinograms	4500951
► 4	18F hot sphere cylinder: 20x14 cm	GE-Advance	Sinograms	4814214
► 5	18F NEMA 8 cm off-centered line source in water	GE-Advance	Sinograms	2138901
► 6	18F uniform cylinder: 14x75 cm	ADAC-CPET	Sinograms	2144551
► 7	18F uniform cylinder: 35x75 cm	ADAC-CPET	Sinograms	97956
► 8	18F NEMA uniform cylinder: 20x18 cm	ADAC-CPET	Sinograms	19742
► 9	18F NEMA 20 cm off-centered line source in air	CPS-HR+	Sinograms	96010
► 10	18F NEMA centered line source in air	CPS-HR+	Sinograms	78994
► 11	18F NEMA centered line source in water	CPS-HR+	Sinograms	207690
► 12	18F NEMA 8 cm off-centered line source in water	CPS-HR+	Sinograms	293841
► 13	18F NEMA uniform cylinder: NEMA 20x18 cm	CPS-HR+	Sinograms	284759
► 14	18F Zubal phantom: thorax	CPS-HR+	Sinograms, images	1945948
► 15	18F Zubal phantom: abdomen with lesions	CPS-HR+	Sinograms, images	2250675
► 16	18FDG oncological patient without attenuation: liver with lesions (lesions to background 3:1)	CPS-HR+	Sinograms, images	22186058
► 17	18FDG oncological patient :liver with lesions (lesions to background 3:1)	CPS-HR+	Sinograms, images	18026320
► 18	18FDG oncological patient without attenuation: liver with lesions (lesions to background 4:1)	CPS-HR+	Sinograms, images	22787362
► 19	99mTc NEMA centered line source in air	ELSCINT Helix dual-head	Projections	507285
► 20	99mTc NEMA off-centered line source in air	ELSCINT Helix dual-head	Projections	516296

<http://sorteo.cermep.fr>

Downloads [buvato]

Jacob	<input checked="" type="radio"/> MRI
Zubal	<input type="radio"/> Labels
Patient 01	<input type="radio"/> [18F]FDG PET Images
Patient 02	<input type="radio"/> [18F]DOPA PET Images
Patient 03	<input type="radio"/> [11C]Raclopride PET Images
Patient 04	<input type="radio"/> [18F]FDG PET Sino
Patient 05	<input type="radio"/> [18F]DOPA PET Sino
Patient 06	<input type="radio"/> [11C]Raclopride PET Sino
Patient 07	<input type="radio"/> Transmission Sino
Patient 08	Common : Blank
Patient 09	Common : Normalization
Patient 10	
Patient 11	
Patient 12	
Patient 13	
Patient 14	
Patient 15	

Download

Terms of use

Running GATE on a grid

GATE can be run on a grid. It has already been deployed on the EGEE grid with success. See S. Staelens, J. De Beenhouwer, D. Kruecker, L. Maigne, F. Rannou, L. Ferrer, Y. D'Asseler, I. Buvat, I. Lemahieu. GATE: improving the computational efficiency. Nucl. Instr. Meth. A 569: 341-345, 2006.

Tools for running GATE on a distributed architecture will be included in the next release of GATE (March 2007)

GATE and Litrani

The GATE digitizer could be replaced by another module performing a more sophisticated simulation of the electronic processing. This module would have to use the GATE output (events as detected in the crystal and their associated characteristics) as an input. Some interface has to be developed for that, but this is feasible.

The software Litrani (<http://gentit.home.cern.ch/gentit/litrani/>) could also be used to precisely model optical photon tracking in a specific detector, and determine how the GATE digitizer should be set up for accurately reproducing the detector response. A systematic tracking of optical photons in the context of the simulation of a real PET or SPECT scan would be unrealistic in terms of computational time.