#### Imperial College London

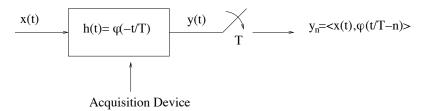


#### Sparse Sampling: Theory and Applications

Pier Luigi Dragotti Imperial College London

## The Sampling Problem

You are given a class of functions. You have a sampling device. Given the measurements  $y_n = \langle x(t), \varphi(t/T - n) \rangle$ , you want to reconstruct x(t).



#### Natural questions:

- ▶ When is there a one-to-one mapping between x(t) and  $y_n$ ?
- What signals can be sampled and what kernels  $\varphi(t)$  can be used?
- What reconstruction algorithm?

#### A few Interesting Applications: Digital Imaging



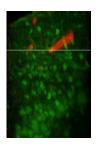
Real Scene

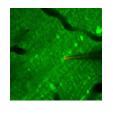
Digital Image

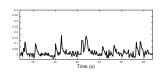
- The real scene is analogue and is turned into a digital image by the camera
- Can we overcome the limitation of the camera and, given the pixels, obtain a sharper image with arbitrary resolution?
- Sparsity: Edges and contours can be modelled using a small number of parameters

## Application: Neuroscience

Goal: Understanding how information processing occurs in neural circuits.

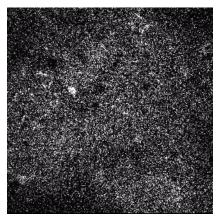






- Brain activity is analogue and it is observed with digital two-photon microscopes
- Neurones communicate through pulses called Action Potentials (AP)
- The problem of reconstructing the activity of a neurone is sparse when the shape of the AP is approximately known.

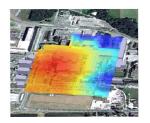
#### Application: Neuroscience



This is a multidimensional problem that requires simultaneously segmentation, denoising and time-resolution enhancement.

**Note:** Video from Simon Peron, Jeremy Freeman, Vijay Iyer, Karel Svoboda (2014); Calcium imaging data from vibrissal S1 neurons in adult mice performing a pole localization task.

#### Application: Estimation of Diffusion Fields





- Can we localise diffusion sources or acoustic sources using sensor networks?
- Application:
  - 1. Monitor dispersion in factories producing bio-chemicals
  - 2.Check whether your government is lying ;-)
- The diffusion field is analogue, spatio-temporal sensor measurements are digital



#### **Problem Statement**

What do all these problems have in common?

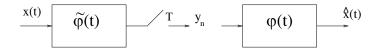
- · The world is analogue, computation is digital
- The source is continuous in time and/or space, measurements are discrete (e.g., pixels in a camera, sensors measurements)
- The data formation process is well understood and involves deterministic smoothing functions normally known a priori (e.g., point spread function in a camera, the diffusion kernel for diffusion fields)
- · Strong priors on the source to be estimated

#### Our Approach

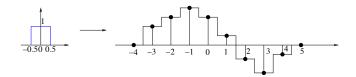
- From the samples, using the knowledge of the observation process, estimate proper integral measurements of the source (e.g., estimate the Fourier transform at specific frequencies, or estimate a few moments of the function)
- Given the integral measurements, solve the inverse/reconstruction problem using proper sparsity priors

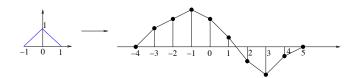
## **Classical Sampling Formulation**

- Sampling of x(t) is equivalent to projecting x(t) into the shift-invariant subspace  $V=\operatorname{span}\{\varphi(t/T-n)\}_{n\in\mathbb{Z}}.$
- If  $x(t) \in V$ , perfect reconstruction is possible.
- Reconstruction process is linear:  $\hat{x}(t) = \sum_n y_n \varphi(t/T n)$ .
- For bandlimited signals  $\varphi(t) = \operatorname{sinc}(t)$ .



# **Classical Sampling Formulation**





#### Signals with Finite Rate of Innovation

Consider a signal of the form:

$$x(t) = \sum_{k \in \mathbb{Z}} \sum_{r=0}^{R-1} \gamma_{k,r} g_r(t - t_k). \tag{1}$$

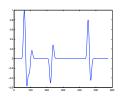
The rate of innovation of x(t) is then defined as

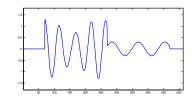
$$\rho = \lim_{\tau \to \infty} \frac{1}{\tau} C_x \left( -\frac{\tau}{2}, \frac{\tau}{2} \right). \tag{2}$$

Definition [VetterliMB:02] A signal with a finite rate of innovation is a signal whose parametric representation is given in (1) and with a finite  $\rho$  as defined in (2).

## Signals with Finite Rate of Innovation

Consider a continuous-time stream of pulses or a piecewise regular signal.





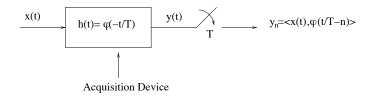
#### These signals

- are not bandlimited.
- are not sparse in a basis or a frame.

#### However:

▶ they are completely determine by a finite number of free parameters.

#### The Sampling Kernel



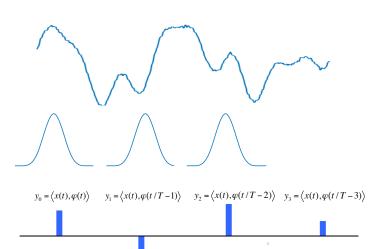
#### Note that

$$y(t) = h(t) * x(t) = \int_{-\infty}^{\infty} x(\tau)h(t-\tau)d\tau$$

$$y_n = y(nT) = \int_{-\infty}^{\infty} x(\tau)h(nT - \tau)d\tau = \int_{-\infty}^{\infty} x(\tau)\varphi(\tau/T - n)d\tau$$
$$= \langle x(t), \varphi(t/T - n)\rangle$$

 φ(t) is the time reversed version of the acquisition device and is called sampling kernel.

#### **Sampling Process**



Possible classes of kernels (we want to be as general as possible):

1. Any kernel  $\varphi(t)$  that can reproduce polynomials:

$$\sum_{n} c_{m,n} \varphi(t-n) = t^{m} \quad m = 0, 1, ..., L,$$

for a proper choice of coefficients  $c_{m,n}$ .

2. Any kernel  $\varphi(t)$  that can reproduce exponentials:

$$\sum_n c_{m,n} \varphi(t-n) = e^{amt} \quad a_m = \alpha_0 + m\lambda \text{ and } m = 0,1,...,L,$$

for a proper choice of coefficients  $c_{m,n}$ .

3. Any kernel with rational Fourier transform:

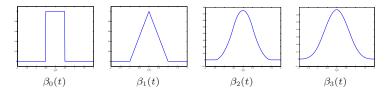
$$\hat{\varphi}(\omega) = \frac{\prod_i (j\omega - b_i)}{\prod_m (j\omega - a_m)} \quad a_m = \alpha_0 + m\lambda \text{ and } m = 0, 1, ..., L.$$

Class 1 is made of all functions  $\varphi(t)$  satisfying Strang-Fix conditions. This includes any scaling function generating a wavelet with L+1 vanishing moments (e.g., Splines and Daubechies scaling functions).

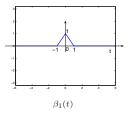
Strang-Fix Conditions:

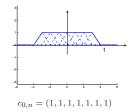
$$\hat{\varphi}(0) \neq 0$$
 and  $\hat{\varphi}^{(m)}(2n\pi) = 0$  for  $n \neq 0$  and  $m = 0, 1, ..., L$ ,

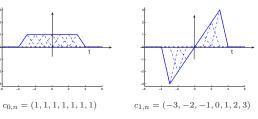
where  $\hat{\varphi}(\omega)$  is the Fourier transform of  $\varphi(t)$ .



B-splines satisfy Strang-Fix conditions since  $\hat{\beta}_n(\omega) = \text{sinc}(\omega/2)^{n+1}$ .

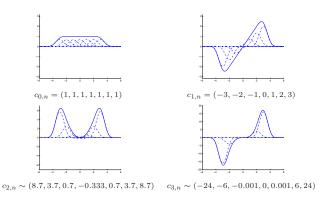






The linear spline reproduces polynomials up to degree L=1:  $\sum_n c_{m,n} \beta_1(t-n) = t^m \quad m=0,1,$  for a proper choice of coefficients  $c_{m,n}$  (in this example n=-3,-2,...,1,2,3).

**Notice**:  $c_{m,n} = \langle \tilde{\varphi}(t-n), t^m \rangle$  where  $\tilde{\varphi}(t)$  is biorthogonal to  $\varphi(t)$ :  $\langle \tilde{\varphi}(t), \varphi(t-n) \rangle = \delta_n$ .

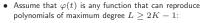


The cubic spline reproduces polynomials up to degree L=3:  $\sum_n c_{m,n} \beta_3(t-n) = t^m \quad m=0,1,2,3.$ 



$$x(t) = \sum_{k=0}^{K-1} x_k \delta(t - t_k).$$

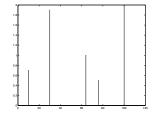
The signal has  $2K\ \mbox{degrees}$  of freedom.



$$\sum_{n} c_{m,n} \varphi(t-n) = t^{m}, \quad m = 0, 1, ..., L,$$

where  $c_{m,n}=\langle \tilde{\varphi}(t-n),t^m\rangle$  and  $\tilde{\varphi}(t)$  is biorthogonal to  $\varphi(t)$ .

• We want to retrieve x(t), from the samples  $y_n=\langle x(t), \varphi(t/T-n)\rangle$  with n=0,1,...,N-1 and  $TN=\tau.$ 



Assume for simplicity that T=1 and define  $s_m=\sum_n c_{m,n}y_n,\, m=0,1,...,L$ , we have that

$$s_{m} = \sum_{n=0}^{N-1} c_{m,n} y_{n}$$

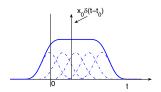
$$= \langle x(t), \sum_{n=0}^{N-1} c_{m,n} \varphi(t-n) \rangle$$

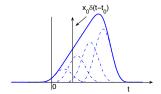
$$= \int_{-\infty}^{\infty} x(t) t^{m} dt$$

$$= \sum_{k=0}^{K-1} x_{k} t_{k}^{m} \quad m = 0, 1, ..., L$$

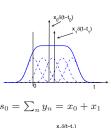
$$(3)$$

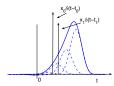
We thus observe  $s_m = \sum_{k=0}^{K-1} x_k t_k^m$ , m=0,1,...,L.



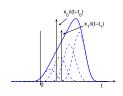


$$\sum_{n} y_n = \langle x_0 \delta(t - t_0), \sum_{n} \varphi(t - n) \rangle = \int_{-\infty}^{\infty} x_0 \delta(t - t_0) \sum_{n} \varphi(t - n) dt = x_0 \sum_{n} \varphi(t_0 - n) = x_0$$
$$\sum_{n} c_{1,n} y_n = \langle x_0 \delta(t - t_0), \sum_{n} c_{1,n} \varphi(t - n) \rangle = x_0 \sum_{n} c_{1,n} \varphi(t_0 - n) = x_0 t_0$$

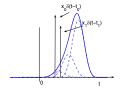




$$s_2 = \sum_n c_{2,n} y_n = x_0 t_0^2 + x_1 t_1^2$$
  $s_3 = \sum_n c_{3,n} y_n = x_0 t_0^3 + x_1 t_1^3$ 



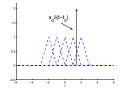
$$s_0 = \sum_n y_n = x_0 + x_1$$
  $s_1 = \sum_n c_{1,n} y_n = x_0 t_0 + x_1 t_1$ 

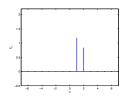


$$s_3 = \sum_n c_{3,n} y_n = x_0 t_0^3 + x_1 t_1^3$$

Example: T=1,  $x(t)=x_0\delta(t-t_0)$  with  $x_0=2$  and  $t_0=\sqrt{2}$ .

The sampling kernel is a linear spline.





In this case

$$y_n = \langle x(t), \varphi(t-n) \rangle = x_0 \varphi(t_0 - n) = \begin{cases} 0 & n \neq 1, 2 \\ 2(2 - \sqrt{2}), & n = 1, \\ 2(\sqrt{2} - 1) & n = 2. \end{cases}$$

and

$$\begin{array}{l} s_0 = \sum_n c_{0,n} y_n = \sum_n y_n = y_1 + y_2 = x_0 = 2, \\ s_1 = \sum_n c_{1,n} y_n = \sum_n n y_n = y_1 + 2y_2 = x_0 t_0 = 2\sqrt{2}. \end{array}$$

# Prony's Method



The quantity

$$s_m = \sum_{k=0}^{K-1} x_k t_k^m, \quad m = 0, 1, ..., L$$

is a power-sum series.

We can retrieve the locations  $t_k$  and the amplitudes  $x_k$  with the annihilating filter method (also known as Prony's method since it was discovered by Gaspard de Prony in 1795).

## Overview of Prony's Method

1. Call  $h_m$  the filter with z-transform  $H(z) = \sum_{i=0}^K h_i z^{-i} = \prod_{k=0}^{K-1} (1 - t_k z^{-1})$ .

We have that

$$h_m * s_m = \sum_{i=0}^K h_i s_{m-i} = \sum_{i=0}^K \sum_{k=0}^{K-1} x_k h_i t_k^{m-i} = \sum_{k=0}^{K-1} x_k t_k^m \underbrace{\sum_{i=0}^K h_i t_k^{-i}}_{0} = 0.$$

This filter is thus called the annihilating filter. In matrix/vector form we have that  ${\bf S}H={\bf H}S=0$  or alternatively using the fact that  $h_0=1$ 

$$\begin{bmatrix} s_{K-1} & s_{K-2} & \cdots & s_0 \\ s_K & s_{K-1} & \cdots & s_1 \\ \vdots & \vdots & \ddots & \vdots \\ s_{L-1} & s_{L-2} & \cdots & s_{L-K} \end{bmatrix} \begin{pmatrix} h_1 \\ h_2 \\ \vdots \\ h_K \end{pmatrix} = - \begin{pmatrix} s_K \\ s_{K+1} \\ \vdots \\ s_L \end{pmatrix}.$$

Solve the above Toeplitz system to find the coefficient of the annihilating filter.

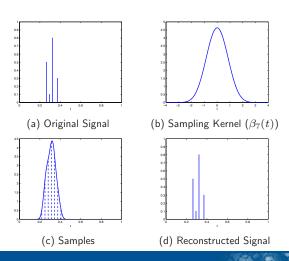
# Overview of Prony's Method

- **2.** Given the coefficients  $\{1, h_1, h_2, ..., h_k\}$ , we get the locations  $t_k$  by finding the roots of H(z).
- 3. Solve the first K equations in  $s_m=\sum_{k=0}^{K-1}x_kt_k^m$  to find the amplitudes  $x_k$ . In matrix/vector form

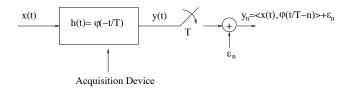
$$\begin{bmatrix} 1 & 1 & \cdots & 1 \\ t_0 & t_1 & \cdots & t_{K-1} \\ \vdots & \vdots & \ddots & \vdots \\ t_0^{K-1} & t_1^{K-1} & \cdots & t_{K-1}^{K-1} \end{bmatrix} \begin{pmatrix} x_0 \\ x_1 \\ \vdots \\ x_{K-1} \end{pmatrix} = \begin{pmatrix} s_0 \\ s_1 \\ \vdots \\ s_{K-1} \end{pmatrix}. \tag{4}$$

Classic Vandermonde system. Unique solution for distinct  $t_k$ s.

#### Sampling Streams of Diracs: Numerical Example



## The Noisy Scenario



- The measurements are noisy
- The noise is additive and i.i.d. Gaussian
- The sampling kernel is the sinc function or B-splines or E-splines.

## **Total Least Squares Algorithm**

The annihilation equation

$$SH = 0$$

is only approximately satisfied.

Minimize:  $\|\mathbf{S}H\|_2$  under the constraint  $\|H\|_2 = 1$ .

This is achieved by performing an SVD of S:

$$\mathbf{S} = \mathbf{U}\lambda \mathbf{V}^{\mathbf{T}}.$$

Then H is the last column of V.

Notice: this is similar to Pisarenko's method in spectral estimation.

# Cadzow's Algorithm

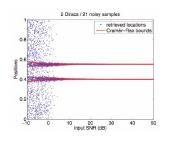
For small SNR use Cadzow's method to denoise S before applying TLS.

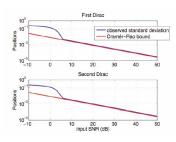
The basic intuition behind this method is that, in the noiseless case, S is rank deficient (rank K) and Toeplitz, while in the noisy case S is full rank.

#### Algorithm:

- SVD of  $\mathbf{S} = \mathbf{U}\lambda\mathbf{V^T}$ .
- $\bullet$  Keep the K largest diagonal coefficients of  $\lambda$  and set the others to zero.
- Reconstruct  $S' = U\lambda'V^T$ .
- This matrix is not Toeplitz, make it so by averaging along the diagonals.
- Iterate.

#### Simulation Results





- Samples are corrupted by additive noise.
- This is a parametric estimation problem.
- Unbiased algorithms have a covariance matrix lower bounded by CRB.
- The proposed algorithm reaches CRB down to SNR of 5dB.

Super-Resolution is a multichannel sampling problem with unknown shifts. Use moments to retrieve the shifts or the geometric transformation between images.







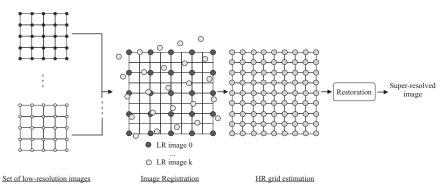
(a)Original (512  $\times$  512)

(b) Low-res.  $(64 \times 64)$ 

(c) Super-res ( PSNR=24.2dB)

- Forty low-resolution and shifted versions of the original.
- Intuition: The disparity between images has a finite rate of innovation and can be retrieved exactly.
- Accurate registration is achieved by retrieving the continuous moments of the 'Tiger' from the samples.
- The registered images are interpolated to achieve super-resolution.

Image super-resolution basic building blocks



- For each blurred image I(x, y):
  - A sample P<sub>m,n</sub> in the blurred image is given by

$$P_{m,n} = \langle I(x,y), \varphi(x/T-n, y/T-m) \rangle,$$

where  $\varphi(t)$  represents the point spread function of the lens.

– We assume  $\varphi(t)$  is a spline that can reproduce polynomials:

$$\sum_{n} \sum_{m} c_{m,n}^{(l,j)} \varphi(x-n,y-m) = x^{l} y^{j} \quad l = 0, 1, ..., N; j = 0, 1, ..., N.$$

- We retrieve the exact moments of I(x,y) from  $P_{m,n}$ :

$$\tau_{l,j} = \sum_{n} \sum_{m} c_{m,n}^{(l,j)} P_{m,n} = \langle I(x,y), \sum_{n} \sum_{m} c_{m,n}^{(l,j)} \varphi(x/2^{J} - n, y/2^{J} - m) \rangle = \int \int I(x,y) x^{l} y^{j} dx dy.$$

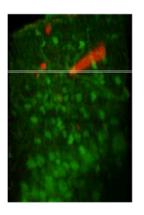
• Given the moments from two or more images, we estimate the geometrical transformation and register them. Notice that moments of up to order three along the x and y coordinates allows the estimation of an affine transformation

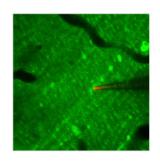


(a)Original ( $128 \times 128$ )

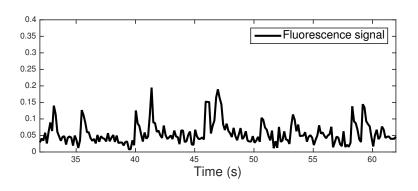


(b) Super-res  $(1024 \times 1024)$ 

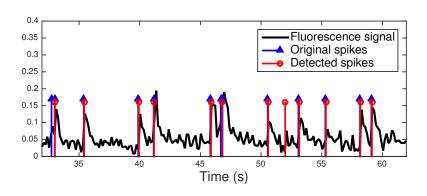


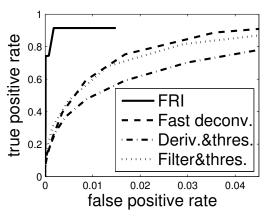


[OnativiaSD:13, ReynoldsSD:17]



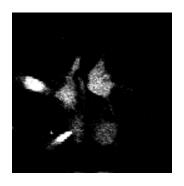
Signal Model: Stream of decaying exponentials

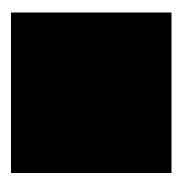




- The algorithm outperforms state-of-the art methods
- Can operate in real-time simultaneously on 80 streams
- Increase in resolution by factor 3

#### Segmentation and Calcium Transient Detection



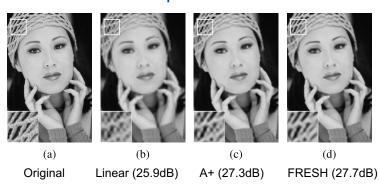


[ReynoldsSD:17]

## Nobel Prizes in Signal Processing ;-)

- · 1908 (phy), Gabriel Lippmann
- 1914 (phy), Max von Laue (X-ray diffraction crystallography)
- 1953 (phy), Frits Zernike (phase-contrast microscopy)
- 1962 (med), Watson, Crick and Wilkins (DNA)
- 1971 (phy), Dennis Gabor (holographic method)
- 1979 (med), Allan M. Cormack, Godfrey N. Hounsfield (CAT)
- 1991 (chem), Richard R. Ernst (high-resolution NMR spectroscopy)
- 2002 (chem), Kurt Wüthrich (3D NMR spectroscopy)
- 2003 (med), Paul C. Lauterbur and Sir Peter Mansfield (MRI)
- 2014 (chem), Eric Betzig, Stefan W. Hell, William E. Moerner (super-resolved fluorescence microscopy)
- 2017 (chem), Jacques Dubochet (cryo-electron microscopy)
- One of the legacy of wavelet and sampling theory is the emergence of computational imaging
  which refers to techniques that combine the design of the hardware layer with
  signal processing techniques in order to go beyond physical limitations of traditional image
  formation systems.
- In computational imaging, computation plays an integral role in the image formation process, for this reason, this research area is intimately related to sampling theory and aspects of sparse representation.

# Single Image Super-Resolution: Numerical Comparisons



#### FRESH Results: Real Data



Low-res input 64 x64 pixels



Final result 256x256 pixels



#### **Conclusions**

#### Sparse Sampling:

- New framework that allows the sampling and reconstruction of continuous-time non-bandlimited signals.
- Use the knowledge of the acquisition process to map discrete measurements to specific integral measurements

#### Key Insights:

- No need to discretize the input signals (use the mathematics of Hilbert and shiftinvariant spaces)
- Non-convex reconstruction algorithms (i.e., structured least-squares methods) often superior to other methods
- Be creative with the notion of sparsity!
- Carve the right solution for the problem at hand: discrete/continuous, convex/nonconvex, noise/no-noise

Outlook: This is the era of inverse problem! Be prepared to witness and contribute to surprising new results and applications!

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