# A Convolutional Neural Network for Enhancing the Detection of SSVEP in the Presence of Competing Stimuli

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### **Outline**

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**Performance Evaluation** 

Methods – Stimulus and Data Acquisition

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Experiment

Discussions

Convolutional Neural Network (CNN) **Future Work** 

Canonical Correlation Analysis (CCA)

#### **Motivation**

Stimulus proximity has been shown to have an influence on the classification performance of a steady-state visual evoked potential based brain-computer interface (SSVEP-BCI)

Multiple visual stimuli placed close to each other compete for neural representations leading to the effect of competing stimuli<sup>1</sup>

This limits the range of flexibility for SSVEP stimulus interface design

<sup>1</sup>Kian B. Ng, Andrew P. Bradley, and Ross Cunnington. Stimulus specificity of a steady-state visual-evoked potential-based brain-computer interface. Journal of Neural Engineering, 2012



## **Proposed Method**

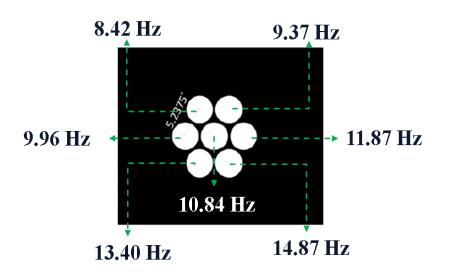
A Convolutional neural network (CNN) based classification to enhance the detection accuracy of SSVEP in the presence of competing stimuli

A 7-class SSVEP dataset from 10 healthy participants was used for evaluating the performance

The results were compared with the canonical correlation analysis (CCA) detection algorithm

## **Methods – Stimulus and Data Acquisition**

#### 7 Class SSVEP



The g.USBamp and Gammabox (g.tec Guger Technologies, Austria) wet electrode (g.Scarabeo) system

Sampling rate - 1200 Hz Channels - O1, O2, Oz, PO3, POz, PO4 and FPz

FPz – ground; right ear lobe – reference

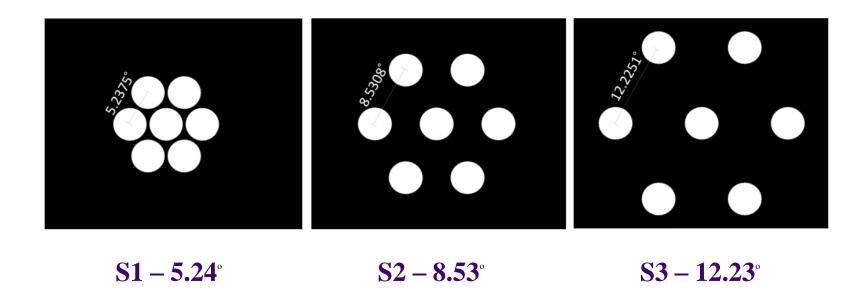
Only O1, O2 and Oz were used in the study

<sup>2</sup>Y. Wang, Y.-T. Wang, and T.-P. Jung. Visual stimulus design for high- rate SSVEP BCI. Electronics Letters, 46(15):1057, 2010.

<sup>3</sup>Masaki Nakanishi, Yijun Wang, Yu Te Wang, Yasue Mitsukura, and Tzyy Ping Jung. Generating visual flickers for eliciting robust steady- state visual evoked potentials at flexible frequencies using monitor refresh rate. PLoS ONE, 2014.



## **Stimulus Designs Evaluated**



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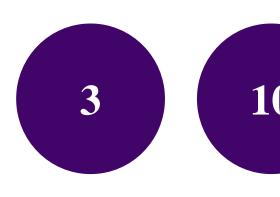
**ENGINEERING** 

<sup>&</sup>lt;sup>3</sup>A. Ravi, S. Pearce, X. Zhang, N. Jiang, and S. Member, "User-Specific Channel Selection Method to Improve SSVEP BCI Decoding Robustness Against Variable Inter-Stimulus Distance," 9th Int. IEEE EMBS Conf. Neural Eng., pp. 283–286, 2019.

## **Experiment**







12 s - Trial Length 2 s – Cue 6 s – Stimulation 4 s – Break

**Total Number of** Trials for each **Stimulus** 

**Total Number** of Trials

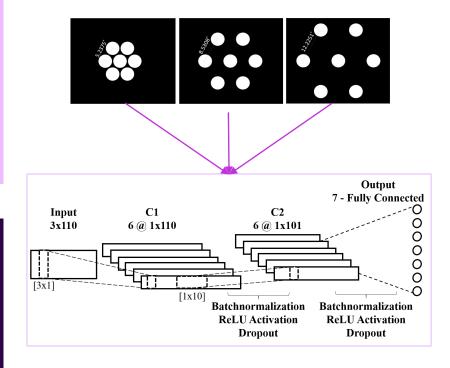
**Total number of** Sessions 1 for each ISD

**Total number of Participants** 



In comparison to the CNNs using time-domain inputs, a CNN using frequency-domain inputs would have a similar but relatively simple network structure and reduced computational complexity (reduced number of tunable parameters)

Investigated whether the CNN parameters learned on one inter-stimulus distance (ISD) can generalize across to other ISDs and sessions



<sup>&</sup>lt;sup>4</sup>No Sang Kwak, Klaus Robert M"uller, and Seong Whan Lee. A convolutional neural network for steady state visual evoked potential classification under ambulatory environment. PLoS ONE, 2017.



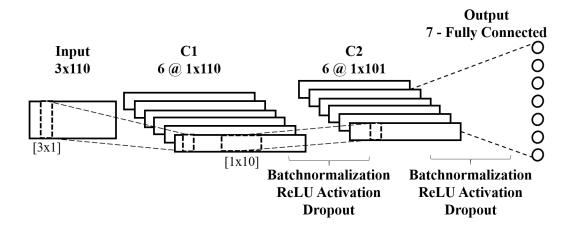
#### **Pre-Processing**

Filter: 4<sup>th</sup> order Butterworth band-pass filter between 1 Hz – 40 Hz

Data Length: 1 s window sliding 100 ms

#### FFT Features (Magnitude Spectrum)

Frequency Resolution: 0.2930 Hz Frequency Components: 3 Hz to 35 Hz



<sup>&</sup>lt;sup>4</sup>No Sang Kwak, Klaus Robert M"uller, and Seong Whan Lee. A convolutional neural network for steady state visual evoked potential classification under ambulatory environment. PLoS ONE, 2017.

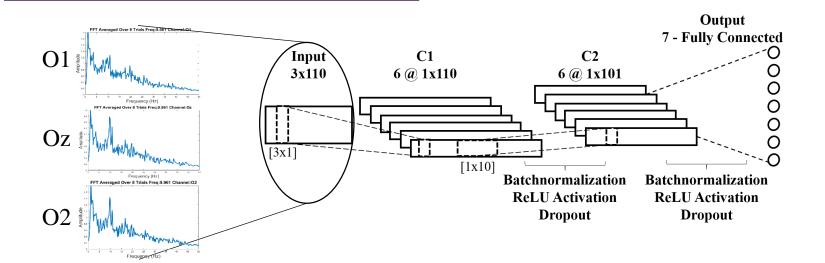
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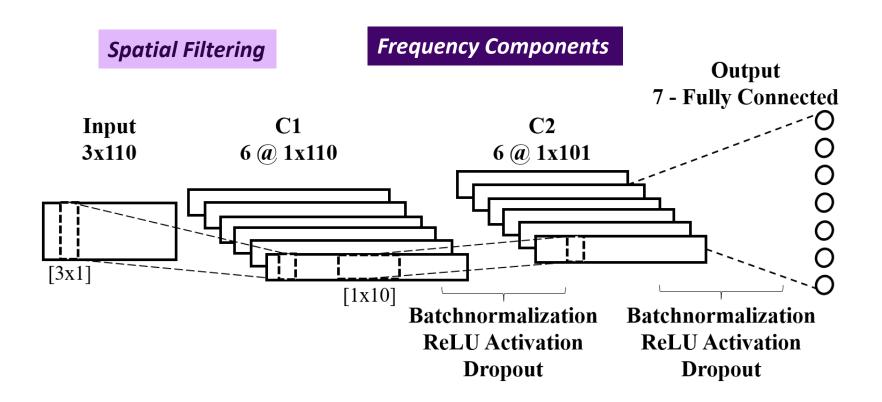
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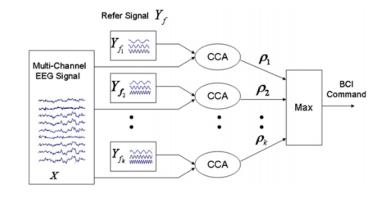
<sup>&</sup>lt;sup>4</sup>No Sang Kwak, Klaus Robert M"uller, and Seong Whan Lee. A convolutional neural network for steady state visual evoked potential classification under ambulatory environment. PLoS ONE, 2017.



## **Canonical Correlation Analysis (CCA)**

$$\rho(x,y) = max_{w_x,w_y} \frac{\mathbb{E}[w_x^T X Y^T w_y]}{\sqrt{\mathbb{E}[w_x^T X X^T w_x] \mathbb{E}[w_y^T Y Y^T w_y]}}$$

$$Y_{n} = \begin{bmatrix} sin(2\pi f_{n}t) \\ cos(2\pi f_{n}t) \\ \vdots \\ sin(2\pi N_{h}f_{n}t) \\ cos(2\pi N_{h}f_{n}t) \end{bmatrix}, t = \begin{bmatrix} \frac{1}{f_{s}}, \frac{2}{f_{s}}, \dots, \frac{N_{s}}{f_{s}} \end{bmatrix},$$



The canonical correlation features  $\rho_{fi}$ , where i=1,2,...,7  $C = \operatorname{argmax}(\rho_{fi})$ 

<sup>&</sup>lt;sup>6</sup>G. Bin, X. Gao, Z. Yan, B. Hong, and S. Gao, "An online multi-channel SSVEP-based brain-computer interface using a canonical correlation analysis method," *J. Neural Eng.*, 2009.



<sup>&</sup>lt;sup>5</sup> Z. Lin, C. Zhang, W. Wu, and X. Gao, "Frequency recognition based on canonical correlation analysis for SSVEP-Based BCIs," *IEEE Trans. Biomed. Eng.*, vol. 54, no. 6, pp. 1172–1176, 2007.

#### **Performance Evaluation**

#### **Offline Analysis**

Simulated Online Analysis

#### **Training**

Hyper-parameters were optimized based on a grid search:

- ❖ Batch size (B):  $2^b$ ,  $b \in \{5,6,7,8,9\}$
- ❖ Dropout Ratio (D): {0.25,0.3.0.35,0.4,0.45,0.5}
- **❖** Number of Epochs (E): {20,30,40,50,60}
- $\Leftrightarrow$  Learning Rate  $\{\alpha\}$ :  $\{0.001, 0.002, 0.005, 0.01, 0.1\}$
- Weights were initialized based on a Gaussian distribution ( $\mu$ =0,  $\sigma$ <sup>2</sup>=0.01)
- **❖ Final Parameters were chosen** based on the **ones that generally resulted in the best** performance for all participants.

#### **Evaluation**

- Case 1: CNN trained on S1 and tested on S2 and S3
- Case 2: CNN trained on S2 and tested on S1 and S3
- Case 3: CNN trained on S3 and tested on S1 and S2

Average accuracies across stimulus-distances were calculated



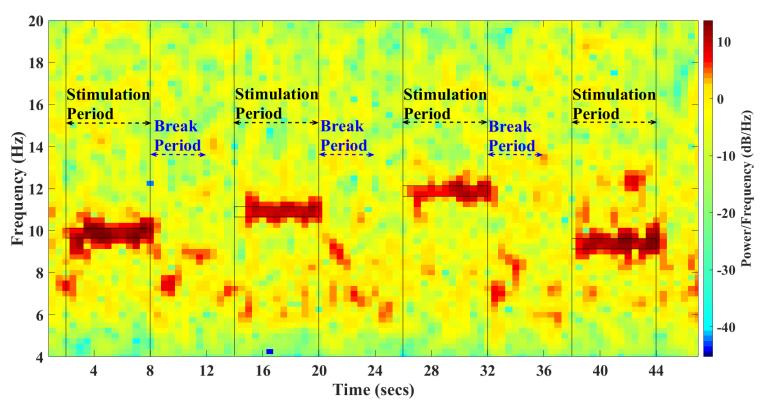
#### **Performance Evaluation**

**Offline Analysis** 

**Simulated Online Analysis** 

- ❖ All three cases as outlined previously were tested
- ❖ For the test data, the initial 1 s of each trial [0.5s 1.5s] from the start of the flickering period was considered, whereas the training data was segmented in the same manner as mentioned earlier
- ❖ The classification accuracies and the information transfer rate (ITR) were calculated for the CCA and the proposed CNN methods individually

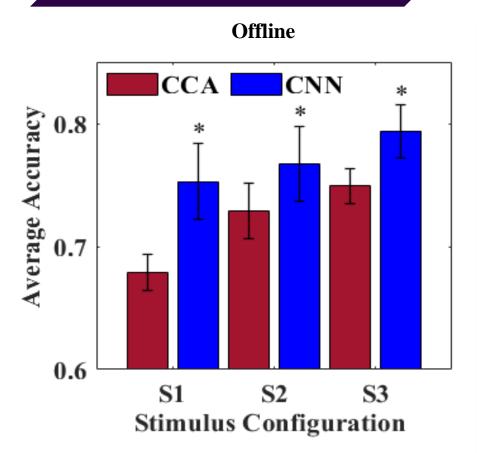
#### **Results**



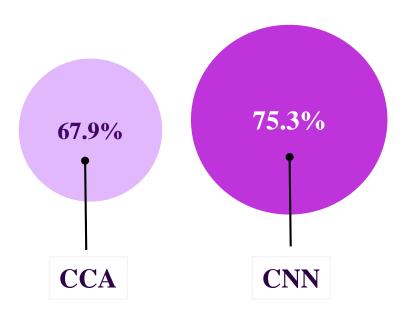
Illustrates an example of the spectrogram of four consecutive trials of SSVEP signals at frequencies 9.961 Hz, 10.84 Hz, 11.87 Hz and 9.375 Hz collected over the channel Oz

### **Results - Performance**

 $S_3 > S_2 > S_1 (p < 0.001)$ 



#### **Offline Analysis**



S1 - Closest ISD (p < 0.001)



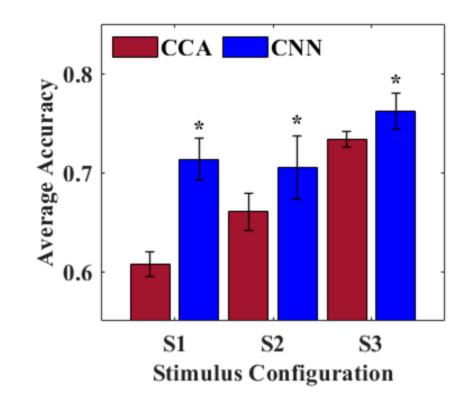
### **Results - Performance**

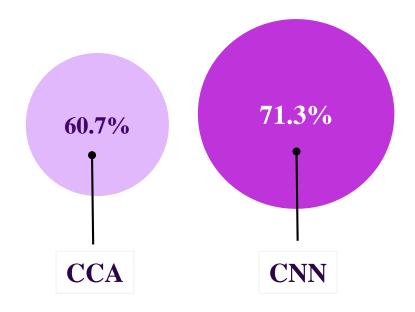
ITR (CNN vs. CCA) - (bits/min)

**Simulated Online Analysis** 

S1 51.0 vs. 34.4 S2 51.3 vs. 42.6 S3 59.0 vs. 52.5

#### **Simulated Online**





S1 - Closest ISD (p < 0.001)



## **Results – Computational Complexity**

The total number of trainable parameters were 4663 Trained on Intel Core i5-8400 CPU @ 2.80 GHz and 8 GB RAM

Overall training time was 6 s

Mean inference time for all segments was found to be 1.3 ms



#### **Discussions**

Average accuracy increased by over 10% using CNN on the closest ISD which is the most challenging case with the most significant completing stimuli

The CNN is robust in **decoding**SSVEP across different ISDs, and can be trained independent of the

ISD resulting in a model that generalizes to other ISDs

Beneficial for practical applications developed on virtual reality or augmented reality platforms where the stimuli would tend to be very closely spaced

Interface Design - Provides more flexibility as newly configured stimulus distances can be easily modified with a simple software update and retain the same CNN weights for inference

Low computational load, short calibration time (approx. 12 minutes) and a 3-channel setup



## **Future Work (In Progress)**

The proposed CNN across time windows and effects on performance when including more channels will be evaluated

Use of complex spectrum features and compare with other variants of CCA

**User-independent training of a CNN** 



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