

An Open Source Rendering Pipeline for Neuroimaging Data

ABSTRACT

Despite the existence of high level technologies available for visualising 3D information, imaging data seems confined to proprietary software linked to DICOM and NIFTI files shipped by manufacturers of costly MRI equipment. Another issue that arises from this is that many of these pieces of software are built purely for stability, opting to forego modern rendering solutions that can drastically increase quality of final renders for use in scientific communication and publication, or are wholly confined to 2D stacked image representations. This report describes a methodology that retains the stability and flexibility of the proprietary programs, but uses open source intermediates and modern 3D software to convert MRI information into 3D files that can be rendered in a path traced engine. It is my aim for this to allow for more efficient and effective scientific communication and outreach of neuroimaging data, and for entities with less funding or necessary expertise in neuroimaging to have the ability to create high-quality figures for communication purposes.

METHODS

MRI Data Acquisition and Formatting

By its very nature, MRI data is often protected information and can be understandably difficult to obtain. Within this report the Yale Longitudinal Dataset of Brain Metastases on MRI with Associated Clinical Data (*Chadha et al, 2025*) was used for versions 1.0 and 1.1 due to their generous open access policies. For version 2.0 onwards, the “Olfactory dysfunction and functional connectivity changes in cognitively normal Parkinson’s disease” published on OpenMRI is used (*Yoneyama et al, 2018*) due to its significantly higher resolution (<20 MRI z-levels versus 255 respectively). This workflow will function for any clinical data obtained in the file formats DICOM (.dcm) or NIFTI (.nii).

The example render used here is of Patient ID YG_04YGLO8ATWRL, from 2013-07-25 and uses the PRE scan information. This dataset, alongside many other imaging sets, provides it’s data in the NIFTI format to preserve patient anonymity and trim out excess information usually preserved in a DICOM file. Unfortunately, InVesalius (the program we use to create the 3D object necessary for the final render) only accepts imports in a DICOM format. Therefore, we must convert the NIFTI file back to DICOM. This is done via the python program *nii2dcm* (*Roberts, 2025*). For further instruction, consult the documentation found on the project’s GitHub repository.

DICOM Masking and .STL Conversion

Now in the DICOM file format, we import the folder of stacked images into InVesalius (Amorim et al, 2015). Following a quality check, the images are masked in order to select desired tissues and remove noise. For the purposes of the example render, the default range preset was used although results may be significantly improved with manual masking. After masking, the generated 3D information can be exported as an .STL file for import into Blender (Blender Team, 2025).

Alternatively to automatic masking, I would strongly recommend using the manual masking feature in InVesalius. This workflow has seen significant improvements to ventricular and cortical detail utilizing this instead of simple automatic selection.

Cleaning and Rendering in Blender

Here all of the steps taken to create the final animated render will be described. However, as many bioscientists have limited familiarity with blender, a template file is provided in this projects repository. Upon loading the template file, you must import the generated .STL of the MRI and align it with the rectangle labelled "Occlusion Plane" by placing it approximately above the origin (0,0,0). After this, I recommend cleaning your mesh both manually and using the tools available in Blender as described. First, manually remove any artefact mesh data present outside of the brain model. Next I would advise decimating the mesh to an appropriate scale factor (e.g. 0.5) to allow dynamic recalculation of topology as the occlusion plane moves through the object. Note that this will modify the raw MRI information, technically rendering it less accurate. It will, however, significantly reduce render times and improve visuals. If using the template, this is all that needs to be done. Here, you can render out your final animation and any images and optionally apply any materials you wish to your brain mesh.

In the case of creating the template, after completing topographic cleanup a camera was created and aligned with the desired final angle. Bidirectional soft lights were also added. Finally, a cube was created and linked via Boolean modifier to the imaging mesh. Crucially, this modifier must be placed on the MRI object, and set to the complex calculator with the "allow holes" option checked. Whilst this does increase render time, this ensures no artefact creation when rendering. This allows rendering the animation of brain slices in 3D. Keyframes were added to the cube, and it was marked non-visible in the render in order for it to occlude the brain mesh. A rudimentary coloured principled BSDF shader was added to the brain mesh and subsurface scattering applied.

fMRI BOLD Visualisation

To co-visualise fMRI BOLD data alongside anatomical data (Fig. 3), the desired frame of the BOLD data must be imported into InVesalius and converted into a mesh using the method detailed above. During this process, you must decide on a masking threshold to determine what level of activity should be visualised. This will be study and machine specific, and for the example in this report any value above 950 was included in the mesh.

After this, import the STL object into Blender, and align it with the anatomical data. It is recommended to use a semi-transparent material for the anatomical data to better see the BOLD mesh.

RESULTS

Anatomical MRI

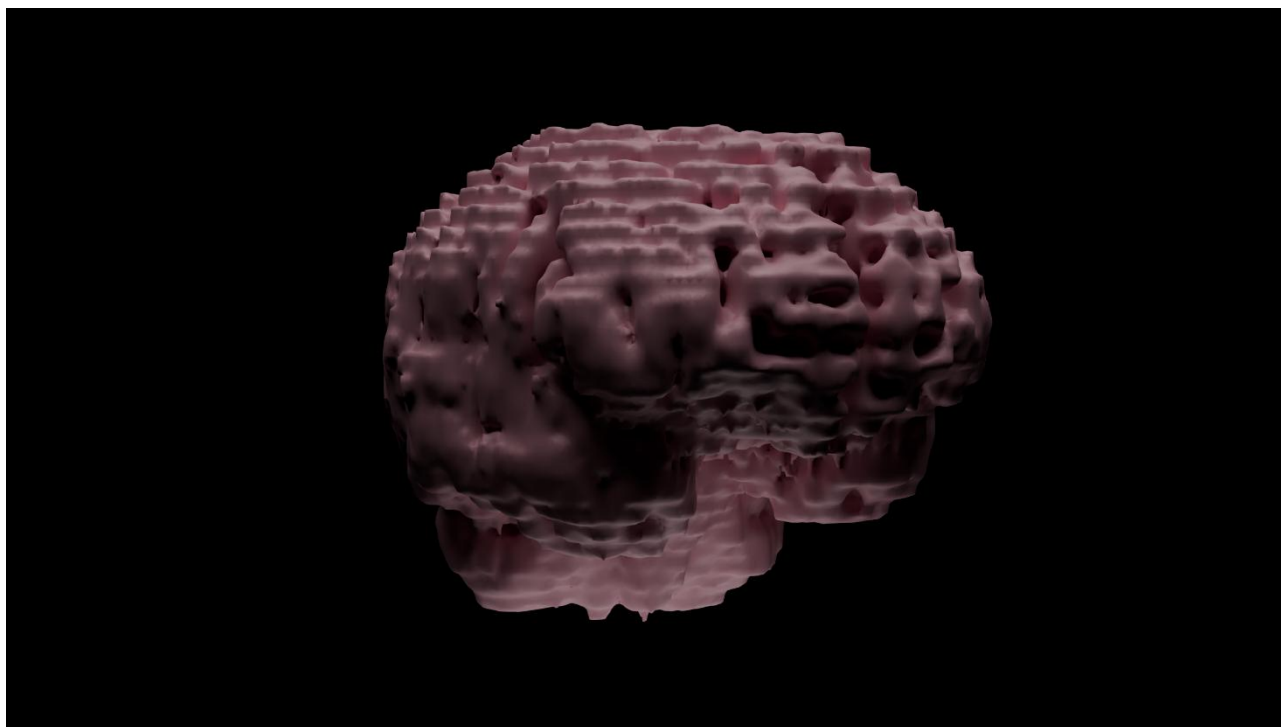


Figure 1: Legacy 3D render of MRI brain scan data from Yale Brain Mets Longitudinal Study. This is from, v1 and v1.1 of the repository. Final render performed in Cycles.

The above image in *Fig. 1* shows the legacy render obtained from the old data pipeline. Note there are artefacts present in the form of horizontal banding seen around the brain. These artefacts are a result of the data being derived from images stacked in the z-axis, and have been entirely removed by updating to a higher resolution dataset.

For the following, refer to the animation found in the GitHub repository, henceforth referred to as *Fig. A1*. In *Fig. A1*, despite still retrieving a render, we see a general smoothness and lack of ventricular and realistic cortical detail. This is likely due to the band-based automatic masking process in InVesalius. This was improved in v1.1 via manual and more aggressive masking in InVesalius, but ultimately did not have as much impact as simply using a higher resolution dataset, as seen in v2.0.

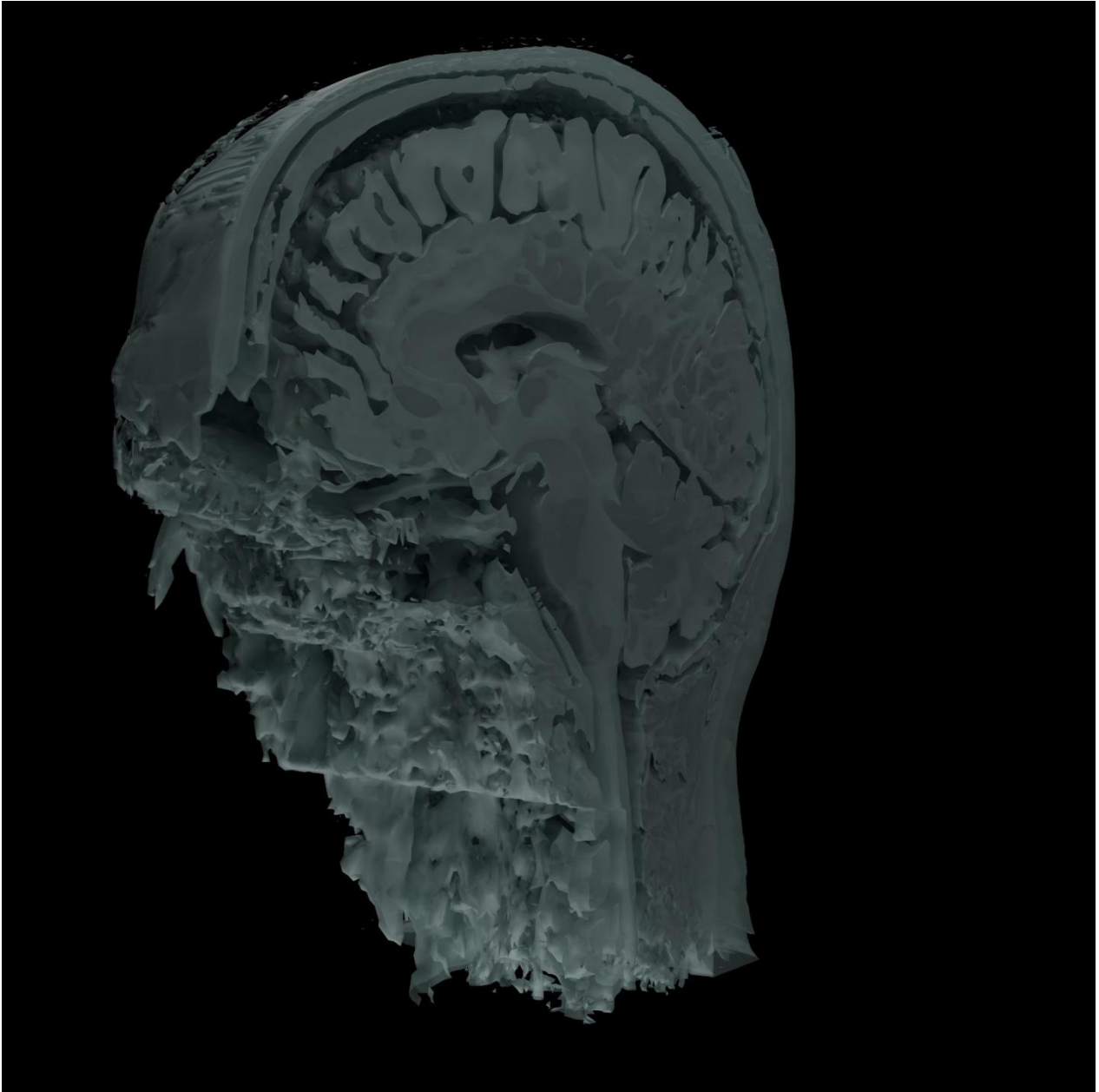


Figure 2: v2 3D render of MRI Anatomical scan data from Yoneyama et al, 2018 bisected in the sagittal plane. Rendered in Blender via Cycles.

As seen in *Fig. 2*, massive resolution improvements have been made. These have been achieved through decimating the mesh instead of remeshing, and using a much higher quality dataset. Note the lack of facial information is a result of the datasets anonymity procedures, not an artefact of the render. A semi-transparent material ($\alpha = 0.7$) has also been used to better show the thickness of the mesh in the sagittal plane as it is cut.

fMRI BOLD

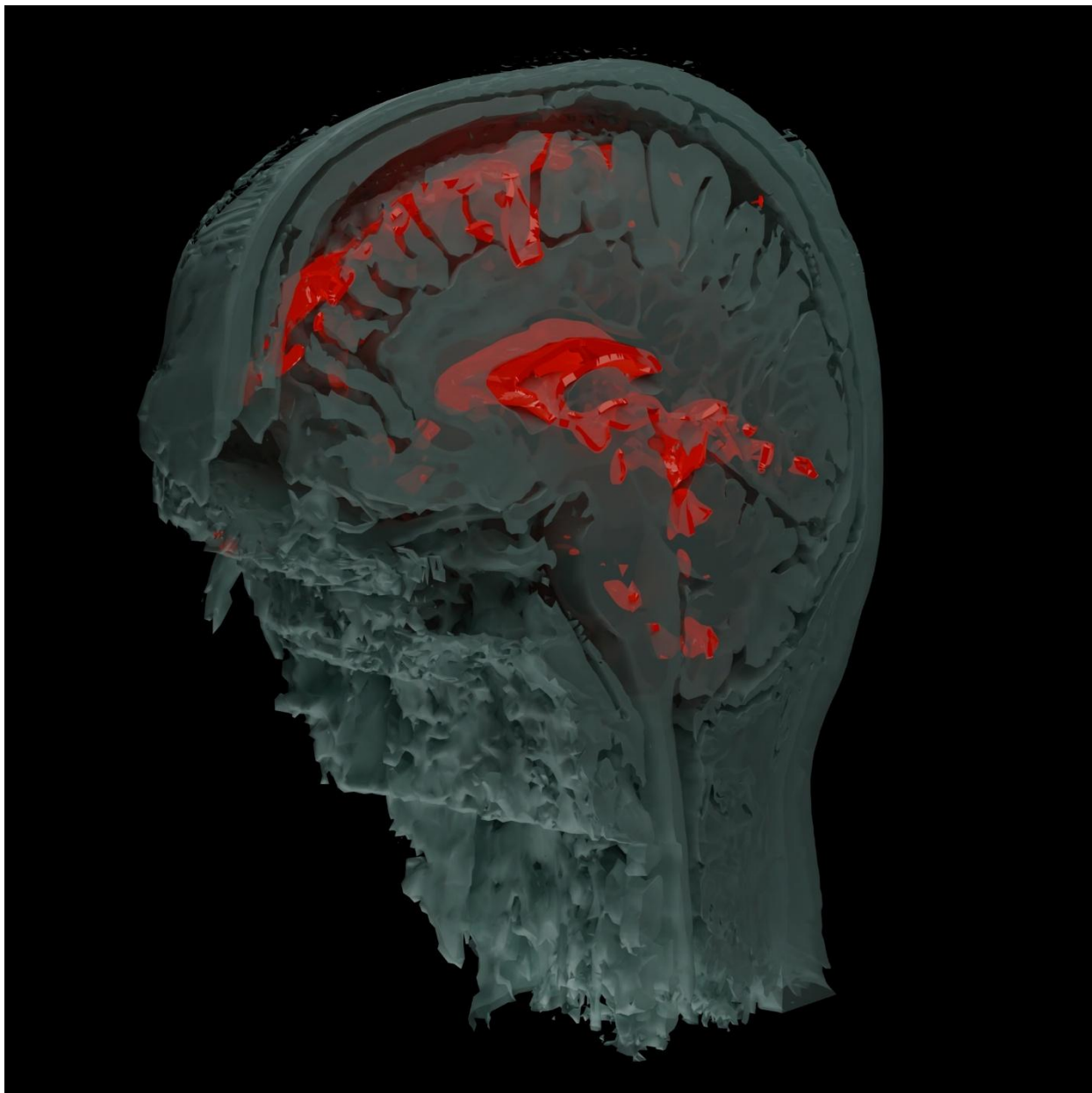


Figure 3: v2.1 3D render of MRI Anatomical scan data from Yoneyama et al, 2018 bisected in the sagittal plane. Shown in red is a single frame of fMRI BOLD data from the same study. Rendered in Blender via Cycles.

Fig.3 shows how the pipeline can be used to render two meshes alongside each other, in this case showing detailed patient anatomical MRI (z-levels = 255), and less detailed fMRI BOLD data. fMRI BOLD mesh is using an emissive texture to better view it through the transparency of the anatomical mesh. Currently the pipeline is limited to displaying only a single frame of this data, but hopefully new techniques introduced in Blender 4.5 may allow for rendering of the full stack of frame data as a 3D animation.

DISCUSSION

With v2.0, the pipeline has demonstrated itself capable of producing much higher quality 3D renders whilst maintaining relatively low render times (approx. 20s/frame at 2160x2160 with an 82 FP32 TFLOPS and 191 FP16 TFLOPS system). As such, I believe it is now in a suitable place to begin iterating and expanding out to other imaging forms, the first of which will be fMRI BOLD data overlayed on anatomical data.

Whilst the expansion of the pipeline into visualising fMRI BOLD data appears promising, it faces two significant challenges. The first is that it is incapable of rendering a true heatmap of BOLD data, instead only rendering a mesh above a threshold. This could theoretically be solved by either SPM integration or potentially a custom scripting or geometry nodes solution, but both would be very time consuming to implement and so will be delayed until further improvements have been made. The second issue is that currently only a single frame of the 198 included for this patient is rendered here. I believe this may be resolvable through new import geometry nodes implemented in Blender 4.5, and will attempt to implement this soon.

Currently under investigation as a significant potential improvements would be integration of SPM to allow for more accurate topological exports. This program would also perfectly fit the aim of this pipeline as it is also open source. For a list of improvements and expansions to the project I aim to make, please consult the repository readme file.

In the meantime, I hope that this provides a method of creating visually appealing renders of anatomical MRI information for scientific communication through a methodology which is entirely free and open source. My sincere acknowledgements to the creators of Blender, InVesalius and nii2dcm for creating the invaluable tools used in this pipeline, and the creators of OpenMRI for dataset access.

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